

svZeroDSolver: A modular package for lumped-parameter cardiovascular flow simulations

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Summary

Computational modeling of cardiovascular blood flow has emerged as a valuable tool in the diagnosis and treatment of cardiovascular disease (Menon, Hu, et al., 2024). While simulations of blood flow can be performed using various high and low-fidelity techniques, lumped-parameter or zero-dimensional modeling is a low-order technique that is widely used in various applications that require quick estimation of bulk flow quantities, such as flow and pressure at specific anatomical locations.

We introduce svZeroDSolver, an efficient and modular package for performing lumped-parameter (zero-dimensional) simulations of cardiovascular blood flow. svZeroDSolver is written in C++ using an object-oriented framework. It is designed so that a user can simply specify a .json dictionary of lumped-parameter “blocks” – such as blood vessels, valves, heart chambers, junctions between blood vessels, and boundary conditions (along with their associated parameters) – which the code uses to automatically assemble and solve the governing equations corresponding to the user-specified vascular model. In addition, the package includes Python and C++ APIs to facilitate its use with other software packages. For example, it can be integrated into Python-based optimization and uncertainty quantification applications. It can also be interfaced with high-performance C++/Fortran software for high-fidelity cardiovascular flow simulations, where svZeroDSolver can conveniently provide lumped-parameter boundary conditions. svZeroDSolver also includes an application, called svZeroDCalibrator, to automatically calibrate parameters of a given zero-dimensional model to recapitulate independent measurements of hemodynamics at specific anatomical locations from high-fidelity simulations – thus improving the accuracy of zero-dimensional simulations.

Statement of need

The ability to non-invasively quantify patient-specific hemodynamics via computational simulations has been shown to improve patient outcomes and reduce invasive clinical procedures in large randomized clinical trials (Taylor et al., 2023). Computational modeling is also a promising tool for non-invasive and personalized optimization of clinical treatments and surgery (Marsden, 2014).

Previous work has used a variety of techniques to model cardiovascular blood flow, all of which can be broadly categorized based on their level of fidelity. High-fidelity models generally involve simulations of the full three-dimensional flow-field within anatomical regions of interest (Menon, Hu, et al., 2024; Updegrove et al., 2017). While these are the most accurate and informative, they are computationally expensive (each simulation can take several hours or days on hundreds of CPU cores) and therefore not feasible for use within typical clinical settings or for applications, such as optimization, which often require thousands of evaluations.

42 On the other end of the spectrum, lumped-parameter or zero-dimensional models provide
43 information about bulk hemodynamics, such as flow rate and pressure, at specific anatomical
44 regions of interest. While these models are not spatially-resolved, they are very valuable
45 in applications that require near real-time quantification of bulk hemodynamics, as well as
46 applications that rely on thousands of repeated model evaluations, such as optimization and
47 uncertainty quantification (Lee et al., 2024; Richter et al., 2024; Zanoni et al., 2024). They
48 are also used in conjunction with high-fidelity simulations where lumped-parameter models are
49 used as boundary conditions (Menon et al., 2023; Menon, Khan, et al., 2024).

50 svZeroDSolver, which is a part of the Simvascular open-source project, is a new open-source
51 software package that enables fast evaluation of zero-dimensional hemodynamics. One major
52 challenge in zero-dimensional modeling that svZeroDSolver addresses is that different clinical
53 applications (and individual clinical cases within the same application) often require unique
54 anatomical arrangements of blood vessels, heart valves, etc., and each of these anatomical
55 configurations is governed by a distinct set of governing equations. It is therefore common
56 for users to implement application-specific solvers, which simulate the equations governing a
57 specific application or anatomical configuration. In contrast, the modularity of svZeroDSolver
58 allows users to easily create arbitrary anatomical configurations by arranging a library of available
59 “blocks”, following which the software automatically assembles the equations governing the
60 user-specified configuration.

61 Another unique feature of svZeroDSolver is its ability to easily interface with other C++ and
62 Python packages. This has been used in previous work on uncertainty quantification (Lee
63 et al., 2024; Richter et al., 2024; Zanoni et al., 2024) as well as in multi-scale simulations
64 coupling three-dimensional hemodynamics with zero-dimensional representations of downstream
65 circulation (Menon et al., 2023; Menon, Khan, et al., 2024). In particular, the C++ interface
66 has been successfully coupled with high-fidelity multi-physics solvers svSolver and svFSI,
67 which are part of the widely used Simvascular open-source software project for cardiovascular
68 biomechanics simulations (Updegrove et al., 2017; Zhu et al., 2022). svZeroDSolver has
69 also been integrated into the graphical user interface of the Simvascular project. This allows
70 users to leverage the functionality in Simvascular to generate three-dimensional patient-
71 specific anatomical models from medical images, and subsequently perform patient-specific
72 zero-dimensional simulations of blood flow by automatically converting the three-dimensional
73 anatomy into a zero-dimensional model (Pfaller et al., 2022).

74 In addition, the svZeroDCalibrator application within svZeroDSolver includes functionality
75 to improve the accuracy of zero-dimensional models by optimizing the parameters of blood
76 vessels to recapitulate observed hemodynamics from measurements or high-fidelity simulations.
77 This allows users to build more accurate zero-dimensional models than those typically based
78 on purely the anatomy of the vascular region of interest (Richter et al., 2024). The accuracy
79 of svZeroDSolver is assessed using continuous integration tests and has also been verified by
80 comparing with high-fidelity three dimensional simulations (Pfaller et al., 2022). This combi-
81 nation of features makes svZeroDSolver uniquely applicable to a wide range of applications in
82 cardiovascular biomechanics.



Figure 1: Various zero-dimensional “blocks” included in svZeroDSolver at the time of writing.

Software details

svZeroDSolver relies on a collection of “blocks” to set up the governing equations for a given anatomical configuration. Each block is inherited from a block class, as illustrated in Figure 1, and is governed by a “local” set of equations with associated degrees-of-freedom. The solver parses through an input configuration .json file, which lists the blocks, their parameters, and how they are connected to each other, and then automatically assembles the local equations and degrees-of-freedom for each block into a global system of equations. The governing equations and circuit representation for each block are available in the documentation. For example, see the [documentation for a blood vessel block](#).

The zero-dimensional simulations performed by svZeroDSolver are governed by non-linear differential-algebraic equations. We integrate these equations in time using the implicit generalized-alpha scheme (Jansen et al., 2000), with Newton-Raphson iterations to solve the linearized system. Under the hood, these linearized governing equations for each block are implemented as local contributions to a system of linear (matrix) equations, which are then assembled into a global linear system based on the user-specified configuration. Details on the modular implementation of the blocks, along with their governing equations, are provided in the documentation’s [Developer Guide](#). We use the [Eigen package](#) to represent and solve these sparse linear systems (Guennebaud et al., 2010). Mathematical details on this implementation are provided in the [SparseSystem](#) and [Integrator](#) classes in the documentation.

The input to svZeroDSolver is a .json file which specifies the simulation parameters (number

of time steps, cardiac cycles, etc.), the types of blocks to be included in the specific model, the boundary conditions, and how the blocks are connected (typically using junction blocks). Each of these blocks generally requires several parameters which can be specified using a steady value, a list of time-varying values, or a mathematical function which is parsed using `exprtk`. The solver can either run simulations for a specified number of time steps and cardiac cycles, or until the difference in mean quantities between consecutive cardiac cycles is below a given threshold.

`svZeroDSolver` currently has implementations of different types of blood vessel blocks with non-linear resistors to model vascular stenoses, junctions between blood vessels, a heart valve block modeled using a hyperbolic tangent function, a cardiac chamber block modeled as a time-varying capacitor and inductor, and several different boundary condition blocks including simple flow, pressure and resistors blocks, windkessel boundary conditions, coronary boundary conditions that include the intramyocardial pressure experienced by coronary arteries, as well as closed-loop versions of windkessel and coronary boundary conditions that allow a user to build a closed-loop circulation model (H. Kim et al., 2010; H. J. Kim et al., 2009; Menon et al., 2023; Menon, Khan, et al., 2024).

Examples of configuration files to run `svZeroDSolver` simulations using the various available blocks are in `svZeroDSolver/tests/cases`. The repository also includes examples demonstrating the simple API for interfacing between `svZeroDSolver` and external C++ software packages in `svZeroDSolver/tests/test_interface`. Details on creating zero-dimensional simulations from three-dimensional models using the `Simvascular` graphical interface are available on the [Simvascular documentation](#).

Future development plans include a graphical interface to create circuit representations of existing zero-dimensional models, as well as functionality to create `svZeroDSolver`-compatible .json configuration files directly from graphical (circuit) representations of user-specified circulatory models. We are also expanding the available blocks to more accurately model hemodynamics, such as by using data-driven models for pressure losses at arbitrarily shaped vascular junctions. The development team actively implements new features, blocks and test cases to build on the capabilities of `svZeroDSolver` and ensure its accuracy and speed.

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References

- Guennebaud, G., Jacob, B., & others. (2010). *Eigen v3*. <http://eigen.tuxfamily.org>.
- Jansen, K. E., Whiting, C. H., & Hulbert, G. M. (2000). A generalized-alpha method for integrating the filtered navier–stokes equations with a stabilized finite element method. *Computer Methods in Applied Mechanics and Engineering*, 190(3), 305–319. [https://doi.org/10.1016/S0045-7825\(00\)00203-6](https://doi.org/10.1016/S0045-7825(00)00203-6)
- Kim, H. J., Vignon-Clementel, I. E., Figueroa, C. A., Ladd, J. F., Jansen, K. E., Feinstein, J. A., & Taylor, C. A. (2009). On coupling a lumped parameter heart model and a three-dimensional finite element aorta model. *Annals of Biomedical Engineering*, 37(11), 2153–2169. <https://doi.org/10.1007/s10439-009-9760-8>
- Kim, H., Vignon-Clementel, I., Coogan, J., Figueroa, C., Jansen, K., & Taylor, C. (2010). Patient-specific modeling of blood flow and pressure in human coronary arteries. *Annals of Biomedical Engineering*, 38, 3195–3209. <https://doi.org/10.1007/s10439-010-0083-6>
- Lee, J. D., Richter, J., Pfaller, M. R., Szafron, J. M., Menon, K., Zanoni, A., Ma, M.

- 149 R., Feinstein, J. A., Kreutzer, J., Marsden, A. L., & Schiavazzi, D. E. (2024). A
150 probabilistic neural twin for treatment planning in peripheral pulmonary artery steno-
151 sis. *International Journal for Numerical Methods in Biomedical Engineering*, 40(5), e3820.
152 <https://doi.org/https://doi.org/10.1002/cnm.3820>
- 153 Marsden, A. L. (2014). Optimization in cardiovascular modeling. *Annual Review of Fluid*
154 *Mechanics*, 46, 519–546. <https://doi.org/10.1146/ANNUREV-FLUID-010313-141341>
- 155 Menon, K., Hu, Z., & Marsden, A. L. (2024). Cardiovascular fluid dynamics: A journey
156 through our circulation. *Flow*, 4, E7. <https://doi.org/10.1017/flo.2024.5>
- 157 Menon, K., Khan, M. O., Sexton, Z. A., Richter, J., Nguyen, P. K., Malik, S. B., Boyd, J.,
158 Nieman, K., & Marsden, A. L. (2024). Personalized coronary and myocardial blood flow
159 models incorporating CT perfusion imaging and synthetic vascular trees. *Npj Imaging*,
160 2(9). <https://doi.org/10.1101/2023.08.17.23294242>
- 161 Menon, K., Seo, J., Fukazawa, R., Ogawa, S., Kahn, A. M., Burns, J. C., & Marsden, A.
162 L. (2023). Predictors of myocardial ischemia in patients with kawasaki disease: Insights
163 from patient-specific simulations of coronary hemodynamics. *Journal of Cardiovascular*
164 *Translational Research*, 16, 1099–1109.
- 165 Pfaller, M. R., Pham, J., Verma, A., Pegolotti, L., Wilson, N. M., Parker, D. W., Yang, W.,
166 & Marsden, A. L. (2022). Automated generation of 0D and 1D reduced-order models of
167 patient-specific blood flow. *International Journal for Numerical Methods in Biomedical*
168 *Engineering*, 38(10). <https://doi.org/10.1002/cnm.3639>
- 169 Richter, J., Nitzler, J., Pegolotti, L., Menon, K., Biehler, J., Wall, W. A., Schiavazzi, D. E.,
170 Marsden, A. L., & Pfaller, M. R. (2024). *Bayesian windkessel calibration using optimized*
171 *0D surrogate models*. <https://arxiv.org/abs/2404.14187>
- 172 Taylor, C. A., Petersen, K., Xiao, N., Sinclair, M., Bai, Y., Lynch, S. R., UpdePac, A., & Schaap,
173 M. (2023). Patient-specific modeling of blood flow in the coronary arteries. *Computer*
174 *Methods in Applied Mechanics and Engineering*, 417, 116414. <https://doi.org/https://doi.org/10.1016/j.cma.2023.116414>
- 175
176 Updegrove, A., Wilson, N. M., Merkow, J., Lan, H., Marsden, A. L., & Shadden, S. C. (2017).
177 SimVascular: An Open Source Pipeline for Cardiovascular Simulation. *Annals of Biomedical*
178 *Engineering*, 45(3), 525–541. <https://doi.org/10.1007/s10439-016-1762-8>
- 179 Zanoni, A., Geraci, G., Salvador, M., Menon, K., Marsden, A. L., & Schiavazzi, D. E. (2024).
180 Improved multifidelity Monte Carlo estimators based on normalizing flows and dimensionality
181 reduction techniques. *Computer Methods in Applied Mechanics and Engineering*, 429,
182 117119. <https://doi.org/https://doi.org/10.1016/j.cma.2024.117119>
- 183 Zhu, C., Vedula, V., Parker, D., Wilson, N., Shadden, S., & Marsden, A. (2022). svFSI: A
184 multiphysics package for integrated cardiac modeling. *Journal of Open Source Software*,
185 7(78), 4118. <https://doi.org/10.21105/joss.04118>