

# svZeroDSolver: A modular package for lumped-parameter cardiovascular simulations

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## Summary

Computational modeling of cardiovascular blood flow has emerged as a valuable tool in the diagnosis and treatment of cardiovascular disease (Menon, Hu, et al., 2024). While simulations of blood flow can be performed using high and low-fidelity techniques, lumped-parameter or zero-dimensional modeling is a widely used low-order technique in applications which require quick estimation of bulk flow quantities, such as flow and pressure at specific anatomical locations (Pfaller et al., 2024).

We introduce [svZeroDSolver](#), an efficient and modular package for performing lumped-parameter (zero-dimensional) simulations of cardiovascular blood flow. As part of the [SimVascular](#) open-source project, [svZeroDSolver](#) and [SimVascular](#) together allow users to go from medical imaging to fast zero-dimensional evaluations of patient-specific hemodynamics. [svZeroDSolver](#) is written in C++ using a modular object-oriented framework. Simply specifying a .json dictionary of lumped-parameter “blocks” – such as blood vessels, junctions between blood vessels, and boundary conditions (along with their associated parameters) – allows the code to automatically assemble and solve the governing equations corresponding to the user-specified vascular model. In addition, the package includes Python and C++ interfaces to facilitate its use with other software packages. For example, it can be integrated into Python-based optimization and uncertainty quantification applications (Lee et al., 2024; Menon, Zandoni, et al., 2024; Richter et al., 2024; Zandoni et al., 2024). It can also be interfaced with C++/Fortran software for high-fidelity cardiovascular flow simulations, where [svZeroDSolver](#) can conveniently provide physiological lumped-parameter boundary conditions (Menon et al., 2023; Menon, Khan, et al., 2024). [svZeroDSolver](#) includes an application, called [svZeroDCalibrator](#), to automatically calibrate parameters of a given zero-dimensional model based independent hemodynamic measurements or high-fidelity simulations – thus improving the accuracy of zero-dimensional models (Richter et al., 2024). It also includes graphical interfaces to interactively create lumped-parameter models for simulations, as well as to visualize the simulated anatomy and hemodynamics.

## Statement of need

Non-invasive quantification of patient-specific hemodynamics via computational simulations has improved patient outcomes and reduced invasive clinical procedures in large randomized clinical trials (Taylor et al., 2023). Computational modeling is also a promising tool for non-invasive and personalized optimization of clinical treatments and surgery (Marsden, 2014).

Previous work has used several techniques to model cardiovascular blood flow, all of which

can be broadly categorized based on their level of fidelity. High-fidelity models generally involve simulations of the full three-dimensional flow-field within anatomical regions of interest (Menon, Hu, et al., 2024; Updegrove et al., 2017). While these are the most accurate and informative, they are computationally expensive (each simulation can take several hours or days on hundreds of CPU cores) and therefore not practical in typical clinical settings or for applications, such as optimization and uncertainty quantification, which often require thousands of model evaluations. On the other end of the spectrum, lumped-parameter or zero-dimensional models provide information about bulk hemodynamics, such as flow rate and pressure, at specific anatomical regions of interest. While these models are not spatially-resolved, they are valuable in applications which require near real-time quantification of bulk hemodynamics, as well as those that rely on thousands of repeated model evaluations (Lee et al., 2024; Menon, Zanoni, et al., 2024; Richter et al., 2024; Zanoni et al., 2024). They are also commonly used in conjunction with high-fidelity simulations where lumped-parameter models are used as physiological boundary conditions (Menon et al., 2023; Menon, Khan, et al., 2024).

svZeroDSolver, which is a part of the SimVascular open-source project, is a new open-source software package that enables fast evaluation of zero-dimensional hemodynamics. One major challenge in zero-dimensional modeling that svZeroDSolver addresses is that different clinical applications (and individual clinical cases within the same application) often require unique anatomical arrangements of blood vessels, heart valves, etc. Moreover, distinct anatomical configurations are governed by a distinct set of governing equations. Therefore, it is common for users to implement application-specific solvers which simulate the equations governing a specific application or anatomical configuration. In contrast, the modularity of svZeroDSolver allows users to easily create arbitrary anatomical configurations by arranging a library of available “blocks”, following which the software automatically assembles the equations governing the user-specified configuration.

Another unique feature of svZeroDSolver is its ability to easily interface with other C++ and Python packages. This has been used in previous work on uncertainty quantification (Lee et al., 2024; Menon, Zanoni, et al., 2024; Richter et al., 2024; Zanoni et al., 2024) as well as in multi-scale simulations coupling three-dimensional hemodynamics with zero-dimensional representations of downstream circulation (Menon et al., 2023; Menon, Khan, et al., 2024). The C++ interface has been coupled with the high-fidelity multi-physics solver svFSIplus, which is part of the widely used SimVascular open-source software project for cardiovascular biomechanics simulations (Updegrove et al., 2017; Zhu et al., 2022). svZeroDSolver has also been integrated into the graphical user interface of the SimVascular project. This allows users to leverage the functionality in SimVascular to generate three-dimensional patient-specific anatomical models from medical images, and subsequently perform patient-specific zero-dimensional simulations of blood flow by automatically converting the three-dimensional anatomy into a zero-dimensional model (Pfaller et al., 2022). The automatic conversion of arbitrary patient-specific anatomies to zero-dimensional simulations is possible due to the modular nature of svZeroDSolver. Using this pipeline, previous work has demonstrated accelerated convergence of three-dimensional simulations when using corresponding zero-dimensional simulation results as initial conditions (Pfaller et al., 2021).

In addition, svZeroDSolver includes several applications to augment its functionality. The svZeroDCalibrator application improves the accuracy of zero-dimensional models by optimizing the parameters of blood vessels to recapitulate observed hemodynamics from measurements or high-fidelity simulations. This allows users to build more accurate zero-dimensional models than those typically based purely on the anatomy of the vascular region of interest (Richter et al., 2024). The svZeroDGUI application is a web-based graphical interface that allows users to create zero-dimensional simulations by interactively dragging-and-dropping individual blood vessels, heart chambers, boundary conditions, connections between these blocks, etc. Another graphical application, svZeroDVisualization, is an interface to visualize the lumped-parameter structure of given anatomical models as well as the simulated hemodynamics within each block. Together, these graphical interfaces make svZeroDSolver intuitive for a wide

95 range of users, potentially expanding its use from research to instructional and clinical contexts.  
96 The functionality and accuracy of svZeroDSolver is assessed using continuous integration  
97 tests on GitHub, and has also been verified by comparing with high-fidelity three dimensional  
98 simulations (Pfaller et al., 2022). This combination of features makes svZeroDSolver uniquely  
99 applicable to a wide range of applications in cardiovascular biomechanics.

100 While there are other open-source projects that provide the functionality for cardiovascular  
101 flow modeling, and specifically zero-dimensional flow modeling, svZeroDSolver has several  
102 features that distinguish it from previous work. In particular, prior packages have primarily  
103 focused on multi-physics finite element modeling for cardiovascular biomechanics (Africa et al.,  
104 2024; Arthurs, 2021; Hirschvogel, 2024; Zhu et al., 2022). Although these projects allow the  
105 implementation of simple zero-dimensional models, usually as boundary conditions to three-  
106 dimensional models, the primary focus is on the modeling of full three-dimensional fluid and  
107 tissue mechanics. There are, however, packages aimed specifically at reduced-order modeling  
108 for cardiovascular flows. For example, the SimVascular project includes svOneDSolver for the  
109 purpose of one-dimensional blood flow modeling. Another popular package for one-dimensional  
110 blood flow simulations is Nektar1D (Alastruey et al., 2012). Similarly, Artery.FE implements  
111 one-dimensional blood flow modeling using the FEniCS finite element framework (Agdestein  
112 et al., 2018), the VaMpy toolkit includes a package for modeling one-dimensional blood flow  
113 using the Lax-Wendroff finite difference method (Diem & Bressloff, 2017), and openBF is a  
114 finite volume implementation of one-dimensional blood flow (Benemerito et al., 2024). In  
115 the zero-dimensional modeling context, CRIMSON (Arthurs, 2021) and lifex-cfd (Africa et  
116 al., 2024) include the ability to simulate simple zero-dimensional blood flow models, primarily  
117 as boundary conditions to three-dimensional simulations. However, their focus is on multi-  
118 physics simulations of cardiovascular biomechanics, therefore they are not stand-alone and  
119 modular zero-dimensional flow solvers. The CellML and CVSim packages include a limited set  
120 of stand-alone zero-dimensional flow models for specific anatomies/applications (Clerx et al.,  
121 2020; Heldt et al., 2010), but they do not provide the modular functionality to specify unique  
122 anatomical models. In addition, there have been other packages that use zero-dimensional  
123 modeling techniques with a focus on statistical analysis, cardiac electromechanics, or specific  
124 anatomical models (Huttary et al., 2017; Regazzoni & Quarteroni, 2021; Rosalia et al., 2021).  
125 However, these packages are either not focused on zero-dimensional modeling or use MATLAB  
126 implementations, which require software licenses and are not free to use. In contrast, the  
127 purpose of svZeroDSolver is to provide an open-source framework specifically for simulating  
128 zero-dimensional flows in a variety of simple and complex anatomies that can be designed  
129 in a user-specific and application-specific manner – by leveraging the modular nature of the  
130 code. The unique features listed above allow the use of svZeroDSolver both as a stand-alone  
131 zero-dimensional flow solver for unique and patient-specific anatomies, as well as in conjunction  
132 with the aforementioned multi-physics solvers as boundary conditions, for parameters estimation  
133 and uncertainty quantification, or even as an instructional tool using its graphical interfaces.



**Figure 1:** Various zero-dimensional “blocks” included in svZeroDSolver at the time of writing.

## Software details

svZeroDSolver relies on a collection of “blocks” to set up the governing equations for a given anatomical configuration. Each block is inherited from a block class, as illustrated in Figure 1, and is governed by a “local” set of equations with associated degrees-of-freedom. The solver parses through an input configuration .json file, which lists the blocks, their parameters, and the blocks’ connectivity, and then automatically assembles the local equations and degrees-of-freedom for each block into a global system of equations. The governing equations and circuit representation for each block are available in the documentation. For example, see the [documentation for a blood vessel block](#).

The zero-dimensional simulations performed by svZeroDSolver are governed by non-linear differential-algebraic equations. We integrate these equations in time using the implicit generalized-alpha scheme (Jansen et al., 2000), with Newton-Raphson iterations to solve the linearized system. Under the hood, these linearized governing equations for each block are implemented as local contributions to a system of linear (matrix) equations, which are then assembled into a global linear system based on the user-specified configuration. Details on the modular implementation of the blocks, along with their governing equations, are provided in the documentation’s [Developer Guide](#). We use the [Eigen package](#) to represent and solve these sparse linear systems (Guennebaud et al., 2010). Mathematical details on this implementation are provided in the [SparseSystem](#) and [Integrator](#) classes in the documentation.

svZeroDSolver currently has implementations of different types of blood vessel blocks with

non-linear resistors to model vascular stenoses, junctions between blood vessels, a heart valve block modeled using a hyperbolic tangent function, a cardiac chamber block modeled as a time-varying capacitor and inductor, and several boundary condition blocks including simple flow, pressure and resistors blocks, windkessel boundary conditions, coronary boundary conditions that include the intramyocardial pressure experienced by coronary arteries, as well as two-sided versions of windkessel and coronary boundary conditions that allow a user to build closed-loop circulation models (H. Kim et al., 2010; H. J. Kim et al., 2009; Menon et al., 2023; Menon, Khan, et al., 2024; Mirramezani et al., 2019; Vignon-Clementel et al., 2006). The input to svZeroDSolver is a .json file which specifies the simulation parameters (number of time steps, cardiac cycles, etc.), the types of blocks to be included in the specific model, the boundary conditions, and how the blocks are connected (typically using junction blocks). Each of these blocks generally requires several parameters which can be specified using a steady value or a list of time-varying values. The solver can either run simulations for a specified number of time steps and cardiac cycles, or until the difference in mean quantities between consecutive cardiac cycles is below a given threshold.

The documentation for svZeroDSolver is automatically built on GitHub using Doxygen. It includes instructions for installation, user guides for svZeroDSolver and its various applications, as well as mathematical and graphical descriptions of each zero-dimensional block that is implemented in the solver. Examples of configuration files to run svZeroDSolver simulations using the various available blocks are in svZeroDSolver/tests/cases. The repository also includes examples demonstrating the simple API for interfacing between svZeroDSolver and external C++ software packages in svZeroDSolver/tests/test\_interface. Details on creating zero-dimensional simulations from three-dimensional models using the SimVascular graphical interface are available on the SimVascular documentation.

Future development plans include functionality to specify time-varying block parameters as mathematical expressions using the exprtk package. We are also expanding the available blocks to more accurately model hemodynamics, such as by using data-driven models for pressure losses at arbitrarily shaped vascular junctions (Rubio et al., 2025). In addition, we plan to extend the svZeroDGUI application to interactively create custom zero-dimensional boundary conditions for three-dimensional simulations. The development team actively implements new features, blocks and test cases to build on the capabilities of svZeroDSolver and ensure its accuracy and speed.

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## References

- Africa, P. C., Fumagalli, I., Bucelli, M., Zingaro, A., Fedele, M., Dede', L., & Quarteroni, A. (2024). Lifex-cfd: An open-source computational fluid dynamics solver for cardiovascular applications. *Computer Physics Communications*, 296, 109039. <https://doi.org/10.1016/j.cpc.2023.109039>
- Agdestein, S. D., Valen-Sendstad, K., & Diem, A. K. (2018). Artery.FE: An implementation of the 1D blood flow equations in FEniCS. *Journal of Open Source Software*, 3(32), 1107. <https://doi.org/10.21105/joss.01107>
- Alastruey, J., Parker, K. H., & Sherwin, S. J. (2012). Arterial pulse wave haemodynamics. *11th International Conference on Pressure Surges*, 401–443.



- 201 Arthurs, R. A. M., Christopher J. AND Khlebnikov. (2021). CRIMSON: An open-source  
202 software framework for cardiovascular integrated modelling and simulation. *PLOS Compu-*  
203 *tational Biology*, 17(5), 1–21. <https://doi.org/10.1371/journal.pcbi.1008881>
- 204 Benemerito, I., Melis, A., Wehenkel, A., & Marzo, A. (2024). openBF: An open-source finite  
205 volume 1D blood flow solver. *Physiological Measurement*, 45(12), 125002.
- 206 Clerx, M., Cooling, M. T., Cooper, J., Garny, A., Moyle, K., Nickerson, D. P., Nielsen, P.  
207 M. F., & Sorby, H. (2020). CellML 2.0. *Journal of Integrative Bioinformatics*, 17(2–3),  
208 20200021. <https://doi.org/doi:10.1515/jib-2020-0021>
- 209 Diem, A. K., & Bressloff, N. W. (2017). VaMpy: A python package to solve 1D blood flow  
210 problems. *Journal of Open Research Software*. <https://doi.org/10.5334/jors.159>
- 211 Guennebaud, G., Jacob, B., & others. (2010). *Eigen v3*. <http://eigen.tuxfamily.org>.
- 212 Heldt, T., Mukkamala, R., Moody, G. B., & Mark, R. G. (2010). CVSim: An open-source  
213 cardiovascular simulator for teaching and research. *The Open Pacing, Electrophysiology &*  
214 *Therapy Journal*, 3, 45.
- 215 Hirschvogel, M. (2024). Ambit – a FEniCS-based cardiovascular multi-physics solver. *Journal*  
216 *of Open Source Software*, 9(93), 5744. <https://doi.org/10.21105/joss.05744>
- 217 Huttary, R., Goubergrits, L., Schütte, C., & Bernhard, S. (2017). Simulation, identification  
218 and statistical variation in cardiovascular analysis (SISCA) – a software framework for  
219 multi-compartment lumped modeling. *Computers in Biology and Medicine*, 87, 104–123.  
220 <https://doi.org/https://doi.org/10.1016/j.combiomed.2017.05.021>
- 221 Jansen, K. E., Whiting, C. H., & Hulbert, G. M. (2000). A generalized-alpha method for  
222 integrating the filtered navier–stokes equations with a stabilized finite element method.  
223 *Computer Methods in Applied Mechanics and Engineering*, 190(3), 305–319. [https://doi.org/10.1016/S0045-7825\(00\)00203-6](https://doi.org/10.1016/S0045-7825(00)00203-6)
- 224
- 225 Kim, H. J., Vignon-Clementel, I. E., Figueroa, C. A., Ladisa, J. F., Jansen, K. E., Feinstein,  
226 J. A., & Taylor, C. A. (2009). On coupling a lumped parameter heart model and a  
227 three-dimensional finite element aorta model. *Annals of Biomedical Engineering*, 37(11),  
228 2153–2169. <https://doi.org/10.1007/s10439-009-9760-8>
- 229 Kim, H., Vignon-Clementel, I., Coogan, J., Figueroa, C., Jansen, K., & Taylor, C. (2010).  
230 Patient-specific modeling of blood flow and pressure in human coronary arteries. *Annals of*  
231 *Biomedical Engineering*, 38, 3195–3209. <https://doi.org/10.1007/s10439-010-0083-6>
- 232 Lee, J. D., Richter, J., Pfaller, M. R., Szafron, J. M., Menon, K., Zanoni, A., Ma, M. R.,  
233 Feinstein, J. A., Kreutzer, J., Marsden, A. L., & Schiavazzi, D. E. (2024). A probabilistic  
234 neural twin for treatment planning in peripheral pulmonary artery stenosis. *International*  
235 *Journal for Numerical Methods in Biomedical Engineering*, 40(5), e3820. <https://doi.org/10.1002/cnm.3820>
- 236
- 237 Marsden, A. L. (2014). Optimization in cardiovascular modeling. *Annual Review of Fluid*  
238 *Mechanics*, 46, 519–546. <https://doi.org/10.1146/ANNUREV-FLUID-010313-141341>
- 239 Menon, K., Hu, Z., & Marsden, A. L. (2024). Cardiovascular fluid dynamics: A journey  
240 through our circulation. *Flow*, 4, E7. <https://doi.org/10.1017/flo.2024.5>
- 241 Menon, K., Khan, M. O., Sexton, Z. A., Richter, J., Nguyen, P. K., Malik, S. B., Boyd, J.,  
242 Nieman, K., & Marsden, A. L. (2024). Personalized coronary and myocardial blood flow  
243 models incorporating CT perfusion imaging and synthetic vascular trees. *Npj Imaging*,  
244 2(9). <https://doi.org/10.1101/2023.08.17.23294242>
- 245 Menon, K., Seo, J., Fukazawa, R., Ogawa, S., Kahn, A. M., Burns, J. C., & Marsden, A.  
246 L. (2023). Predictors of myocardial ischemia in patients with kawasaki disease: Insights  
247 from patient-specific simulations of coronary hemodynamics. *Journal of Cardiovascular*

- 248 *Translational Research*, 16, 1099–1109.
- 249 Menon, K., Zanoni, A., Khan, O., Geraci, G., Nieman, K., Schiavazzi, D. E., & Marsden, A. L.  
250 (2024). Personalized and uncertainty-aware coronary hemodynamics simulations: From  
251 bayesian estimation to improved multi-fidelity uncertainty quantification. *arXiv*, 2409.02247.  
252 <https://arxiv.org/abs/2409.02247>
- 253 Mirramezani, M., Diamond, S. L., Litt, H. I., & Shadden, S. C. (2019). Reduced Order  
254 Models for Transstenotic Pressure Drop in the Coronary Arteries. *Journal of Biomechanical*  
255 *Engineering*, 141(3), 31005. <https://doi.org/10.1115/1.4042184>
- 256 Pfaller, M. R., Pegolotti, L., Pham, J., Rubio, N. L., & Marsden, A. L. (2024). Chapter  
257 20 - reduced-order modeling of cardiovascular hemodynamics. In T. C. Gasser, S. Avril,  
258 & J. A. Elefteriades (Eds.), *Biomechanics of the aorta* (pp. 449–476). Academic Press.  
259 <https://doi.org/10.1016/B978-0-323-95484-6.00016-6>
- 260 Pfaller, M. R., Pham, J., Verma, A., Pegolotti, L., Wilson, N. M., Parker, D. W., Yang, W.,  
261 & Marsden, A. L. (2022). Automated generation of 0D and 1D reduced-order models of  
262 patient-specific blood flow. *International Journal for Numerical Methods in Biomedical*  
263 *Engineering*, 38(10). <https://doi.org/10.1002/cnm.3639>
- 264 Pfaller, M. R., Pham, J., Wilson, N. M., Parker, D. W., & Marsden, A. L. (2021). On the  
265 periodicity of cardiovascular fluid dynamics simulations. *Annals of Biomedical Engineering*.  
266 <https://doi.org/10.1007/s10439-021-02796-x>
- 267 Regazzoni, F., & Quarteroni, A. (2021). Accelerating the convergence to a limit cycle in 3D  
268 cardiac electromechanical simulations through a data-driven 0D emulator. *Computers in Bi-*  
269 *ology and Medicine*, 135, 104641. [https://doi.org/10.1016/j.combiomed.](https://doi.org/10.1016/j.combiomed.2021.104641)  
270 [2021.104641](https://doi.org/10.1016/j.combiomed.2021.104641)
- 271 Richter, J., Nitzler, J., Pegolotti, L., Menon, K., Biehler, J., Wall, W. A., Schiavazzi, D. E.,  
272 Marsden, A. L., & Pfaller, M. R. (2024). Bayesian windkessel calibration using optimized  
273 0D surrogate models. *arXiv*, 2404.14187.
- 274 Rosalia, L., Ozturk, C., Van Story, D., Horvath, M. A., & Roche, E. T. (2021). Object-  
275 oriented lumped-parameter modeling of the cardiovascular system for physiological and  
276 pathophysiological conditions. *Advanced Theory and Simulations*, 4(3), 2000216.
- 277 Rubio, N. L., Pegolotti, L., Pfaller, M. R., Darve, E. F., & Marsden, A. L. (2025). Hybrid physics-  
278 based and data-driven modeling of vascular bifurcation pressure differences. *Computers in*  
279 *Biology and Medicine*, 184, 109420. <https://doi.org/10.1016/j.combiomed.2024.109420>
- 280 Taylor, C. A., Petersen, K., Xiao, N., Sinclair, M., Bai, Y., Lynch, S. R., UpdePac, A.,  
281 & Schaap, M. (2023). Patient-specific modeling of blood flow in the coronary arteries.  
282 *Computer Methods in Applied Mechanics and Engineering*, 417, 116414. [https://doi.org/](https://doi.org/10.1016/j.cma.2023.116414)  
283 [10.1016/j.cma.2023.116414](https://doi.org/10.1016/j.cma.2023.116414)
- 284 Updegrove, A., Wilson, N. M., Merkow, J., Lan, H., Marsden, A. L., & Shadden, S. C. (2017).  
285 SimVascular: An Open Source Pipeline for Cardiovascular Simulation. *Annals of Biomedical*  
286 *Engineering*, 45(3), 525–541. <https://doi.org/10.1007/s10439-016-1762-8>
- 287 Vignon-Clementel, I. E., Alberto Figueroa, C., Jansen, K. E., & Taylor, C. A. (2006). Outflow  
288 boundary conditions for three-dimensional finite element modeling of blood flow and  
289 pressure in arteries. *Computer Methods in Applied Mechanics and Engineering*, 195(29–32),  
290 3776–3796. <https://doi.org/10.1016/j.cma.2005.04.014>
- 291 Zanoni, A., Geraci, G., Salvador, M., Menon, K., Marsden, A. L., & Schiavazzi, D. E. (2024).  
292 Improved multifidelity Monte Carlo estimators based on normalizing flows and dimensionality  
293 reduction techniques. *Computer Methods in Applied Mechanics and Engineering*, 429,  
294 117119. <https://doi.org/10.1016/j.cma.2024.117119>
- 295 Zhu, C., Vedula, V., Parker, D., Wilson, N., Shadden, S., & Marsden, A. (2022). svFSI: A

296 multiphysics package for integrated cardiac modeling. *Journal of Open Source Software*,  
297 7(78), 4118. <https://doi.org/10.21105/joss.04118>

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