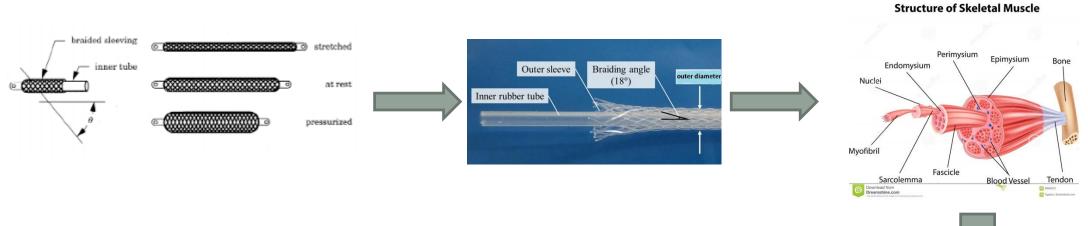
DESIGN OF UPPER-BODY EXOSKELETON WITH MULTIFILAMENT MUSCLE ACTUATION AND BIOMIMETIC SUPPORT

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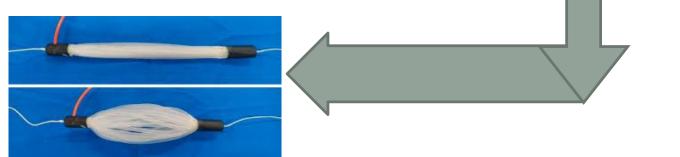
Introduction

• These are smaller McKibben muscles that work on pneumatic actuation.



Main parts:

- 1. Inner tube
 OD=4.34 mm
 ID=3 mm
- 2. Outer Sleeve OD=0.4 mm



Problem Definition

• PAMs are used usually in Exosuits; these are sturdy & provide heavy forces but compromise on flexibility



- To tackle this we use thin Mckibben bundles called Multifilament muscles
- These muscles have been tested to replicate human-like motions in certain robotic designs



• This paper tries to conceptualize the use of such muscles in an Exo-suit to obtain force augmentations

Theoretical Methodology

Mathematical model

$$\mathbf{F}=5.0705\times10^{-4}(\mathbf{P-P_{th}})-5.006\times10^{-10}(\mathbf{P-P_{th}})^2-7.3828\times10^{-16}(\mathbf{P-P_{th}})^3$$

$$P_{app} = 0.7MPa$$

$P_{th} = 0.1441 MPa$

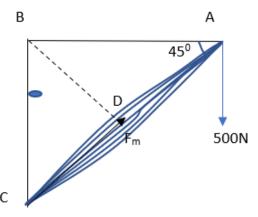
Braid angle =
$$18^{\circ}$$

Bicep Muscles

- Number of muscles = 16
- L= 200 mm
- $F_m = 500 \text{ N}$
- $F_{\text{single}} = 500/16 = 31.25 \text{ N}$
- P = 0.652624MPa

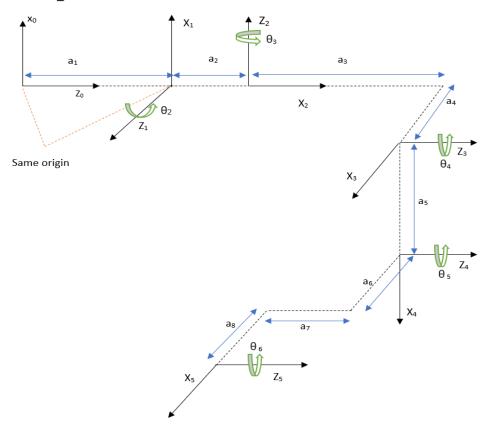
Back Muscles

- Number of muscles = 22
- L= 217.0817 mm
- $F_m = 500/\sin 45 = 707.10672 \text{ N}$
- $F_{\text{single}} = 707.10672/22 = 32.14 \text{ N}$
- P = 0.6510683MPa



Kinematic Modelling

DH parameterization



$${}^{0}T_{5} = A_{1}A_{2}A_{3}A_{4}A_{5}$$

Dynamic Modelling

Rigidbodytree creation

Robot: (5 bodies)

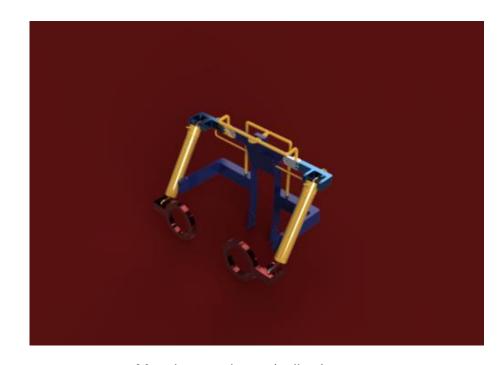
Idx	Body Name	Joint Name	Joint Type	Parent Name(Idx)	Children Name(s
1	body1	jnt1	revolute	base(0)	body2(2)
2	body2	jnt2	revolute	body1(1)	body3(3)
3	body3	jnt3	revolute	body2(2)	body4(4)
4	body4	body4_jnt	fixed	body3(3)	body5(5)
5	body5	jnt5	revolute	body4 (4)	



Mechanical Design & Assembly



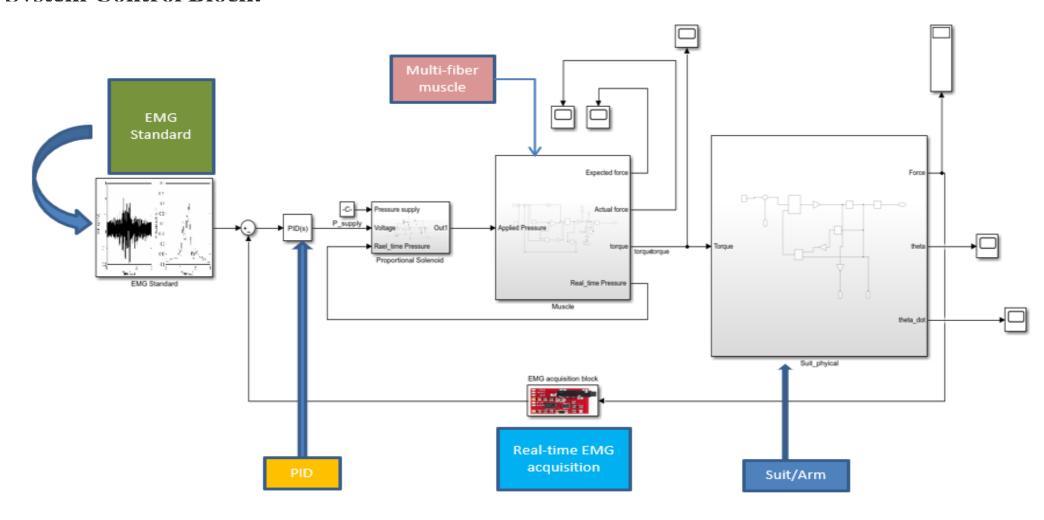
- Four complexes
 - Back Complex
 - Shoulder Complex
 - Elbow Complex
 - Upper Limb part
 - Elbow Joint
 - Forearm Part
 - Hand Complex



- Muscle complexes (yellow)
 - Elbow Muscles
 - Shoulder Muscles

Sensing & Control

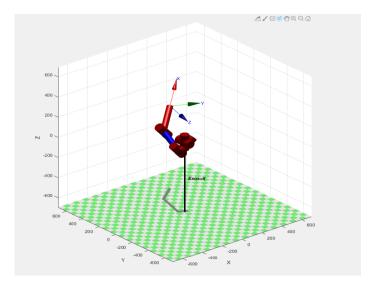
Overall System Control Block:



Results and Discussion

1. Mathematical modelling:

• The observed actual force is less than theoretical force – due to "dead space"



2. Kinematic and dynamic modelling:

- Dynamic modelling was done using MATLAB robotic system toolbox using DH parameters and transformations
- Forward and inverse dynamic analysis were obtained using the inbuilt functions in MATLAB

Motion Analysis

Shoulder

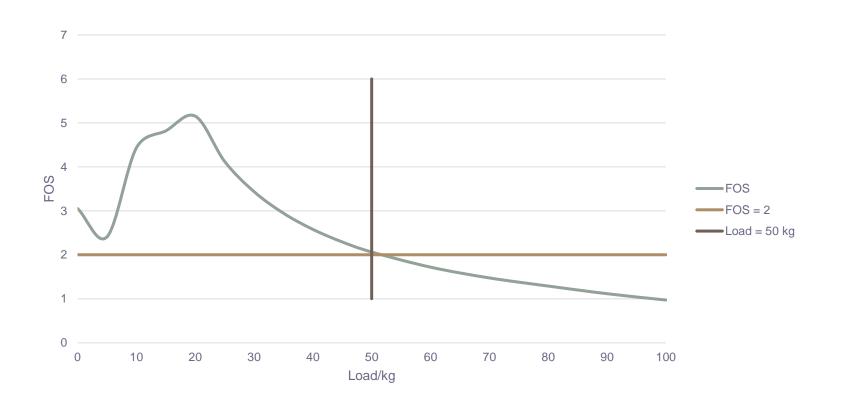


Elbow

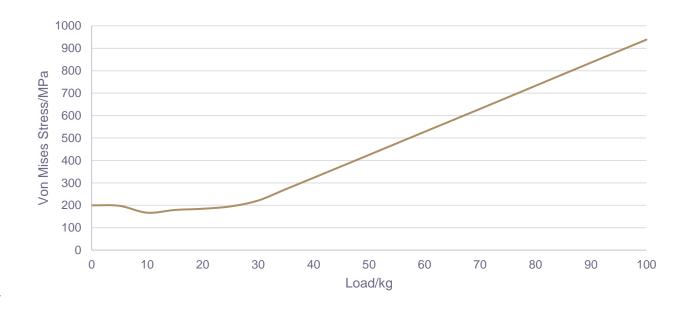


3. Mechanical design:

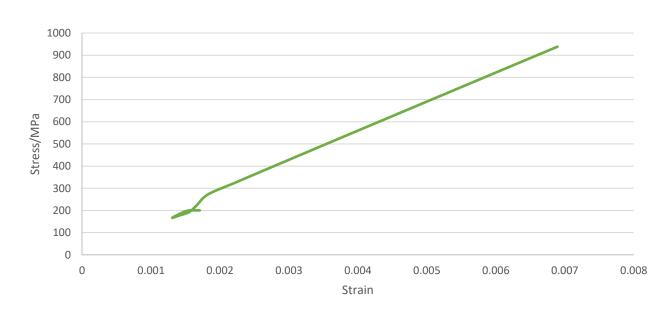
• Variation of FOS w.r.t Load



• Variation in Stress w.r.t Load

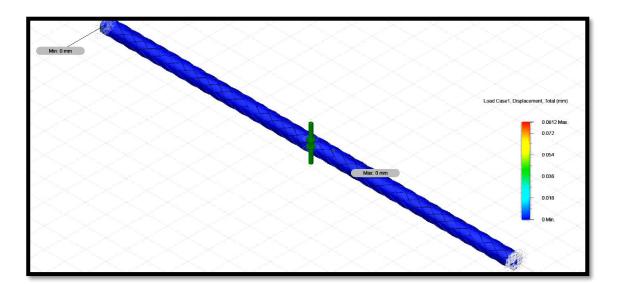


• Stress-Strain Curve of the suit



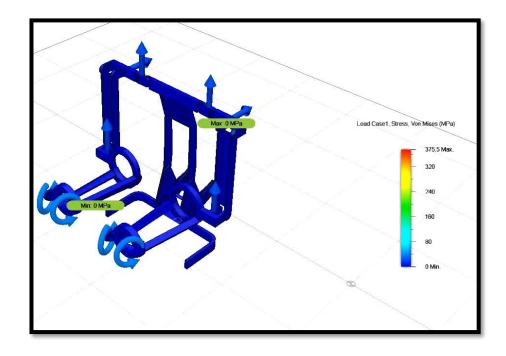
Simulation of Mckibben Fibre

Maximum Displacement observed in a single Fibre is 60 microns



Simulation of Exoskeleton

Minimum Factor of Safety = 2.356



4. Sensing & Control:

- EMG acquisition test: Used to standardize muscle pattern
- Commercial gel electrodes were used which has noise in the input signal. Clinical EMG test will give more accurate results
- Control of the suit was done using a PID model with a proportional valve
- Control variable here is the spool position
- A memory block can be added to counteract any overloads created
- As a safety precaution, include **deadman's switch**

Conclusion

- The concept of dead space present during bundling of fibres reduce the expected force received.
- Although multiple EMG tests were conducted, the absence of precision sensors in turn affects the control of the suit. However, using proper AgCl coated electrodes have been seen to tackle this issue fairly.
- The use of an AFC control would have been able to tackle the noises that arise from the inputs as well as during the working cycle.
- Although the use of a proportional solenoid valve gives better control, the price of such an apparatus much higher than the conventional directional valves and increases complexity.

Scope for future work

- Better design of individual strands and modification of dead space
- Adding more bundles to represent each muscle sector
- Providing a dense energy source to the suit
- The biggest challenge for precision control is precise input acquisition
- Inclusion of ML and/or AI
- Experiments can be done conducted to improve the utility range of use of the suit

References

- 1. Shunichi Kurumaya, Hiroyuki Nabae, Gen Endo, "*Design of thin McKibben muscle and multifilament structure*". Koichi Suzumori Department of Mechanical Engineering, Tokyo Institute of Technology, 2-12-1 Ookayama, Meguro-ku, Tokyo 152-8552, Japan.
- 2. INTRODUCTION TO ROBOTICS ANALYSIS, CONTROL, APPLICATIONS, Second Edition, Saeed Benjamin Niku, Ph.D., P.E. Professor Mechanical Engineering Department California Polytechnic State University San Luis Obispo
- 3. Wan Hasbullah Mohd Isa1, Zahari Taha1, Ismail Mohd Khairuddin1, Anwar P.P., "An intelligent active force control algorithm to control an upper extremity exoskeleton for motor recovery", IOP Conf. Series: Materials Science and Engineering 114 (2016).
- 4. Madeeha Majeed, Khurram Butt, Salman Qureshi, Bilal Majeed, 2013, "Design and Control of Low- Cost Portable EMG Driven Exoskeleton Device for Human Wrist Rehabilitation", INTERNATIONAL JOURNAL OF ENGINEERING RESEARCH & TECHNOLOGY (IJERT) Volume 02, Issue 10 (October 2013).
- 5. A. Salman, J. Iqbal, U. Izhar, U. S. Khan and N. Rashid, "*Optimized circuit for EMG signal processing*," 2012 International Conference of Robotics and Artificial Intelligence, Rawalpindi, 2012 IEEE.
- 6. Amirul Syafiq Sadun, Jamaludin Jalani, Jumadi Abdul Sukor, and Faizal JamiL," Force Control for a 3-Finger Adaptive Robot Gripper by using PID Controller ", Department of Electrical Engineering Technology, Universiti Tun Hussein Onn Malaysia.

THANK YOU