



Date of experiment: 14 August 2025

Medical Physics Laboratory - I

Name: Souvik Das

Roll No: 241126007



ଚିକିତ୍ସା ଓ ବିକିରଣ ଭୋଟିକୀ କେନ୍ଦ୍ର ଧିକିତ୍ସା ଏବଂ ଵିକିରଣ ଭୌତିକୀ କେନ୍ଦ୍ର
CENTRE FOR MEDICAL AND RADIATION PHYSICS

National Institute of Science Education and Research
Jatani, Odisha, India

Date of submission: November 4, 2025

Contents

1 Objective	1
2 Apparatus	1
3 Theory	2
4 Observation	5
5 Error	7
6 Conclusion	7
7 References	7



1 | Objective

To measure the output of a Telecobalt unit (Co-60 photon beams).

2 | Apparatus

- Telecobalt Unit
- Water/Slab Phantom
- Ionization Chamber
- Electrometer and Connecting cables
- Thermometer and Barometer

Telecobalt Unit

The Telecobalt machine is equipment that houses a Co-60 radioactive source with an activity of 10–12 kCi. The Co-60 source is doubly encapsulated in stainless steel, in a cylindrical shape, and contains Co-60 radioactive sources in the form of pellets. The typical size of this encapsulation is around 3 cm in length and 2–2.5 cm in diameter.

The main components of a telecobalt unit are the gantry, source head, collimator, and patient support assembly or treatment couch. The Co-60 source is placed inside a shielded chamber in the source head. During the time of treatment, the Co-60 source is driven toward the collimator, and the shutter is opened for irradiation. The gantry helps to rotate the unit around the patient. The collimator is a beam-limiting device that defines the radiation beam to a particular area of interest for the patient.

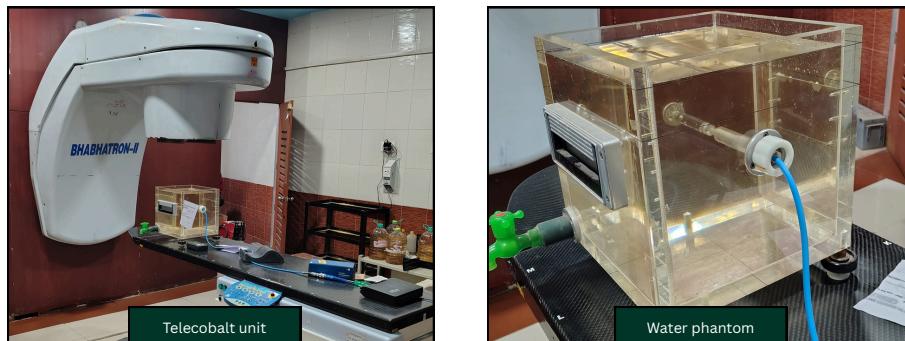


Figure 2.1: Telecobalt unit (Bhabhatron) at AHPGIC

Teletherapy Sources

The most widely used teletherapy source uses ^{60}Co radionuclides contained inside a cylindrical stainless steel capsule and sealed by welding. A double-welded seal is used to prevent any leakage of the radioactive material.

- To facilitate interchange of sources from one teletherapy machine to another and from one isotope production facility to another, standard source capsules have been developed.
- The typical diameter of the cylindrical teletherapy source is between 1 and 2 cm; the height of the cylinder is about 2.5 cm. The smaller the source diameter, the smaller its physical penumbra and the more expensive the source. Often a diameter of 1.5 cm is chosen as a compromise between the cost and penumbra.
- Typical source activities are of the order of 5000–10 000 Ci (185–370 TBq) and provide a typical dose rate at 80 cm from the teletherapy source of the order of 100–200 cGy/min. Often the output of a teletherapy machine is stated in Rmm (roentgens per minute at 1 m) as a rough guide for the source strength.

Source	Co-60
Half-life	5.26 days
Specific activity(Ci/g)	1100
Photon energy (MeV)	1.17 and 1.33
Specific γ rate constant $\Gamma[Rm^2/(Ci.h)]$	1.31
Maximum source strength	170 RMM(26-Dec-2017)
HVL (cm Pb)	1.1
Means of Production	$^{59}Co + n$ in reactor

- Teletherapy sources are usually replaced within one half-life after they are installed; however, financial considerations often result in longer source usage.
- The ^{60}Co radionuclides in a teletherapy source decay with a half-life of 5.26 years into ^{60}Ni with the emission of electrons (β^- particles) with a maximum energy of 320 keV and two γ rays with energies of 1.17 MeV and 1.33 MeV. The emitted gamma rays constitute the therapy beam; the electrons are absorbed in the cobalt source or the source capsule, where they produce relatively low energy and essentially negligible bremsstrahlung X-rays and characteristic X-rays.
- Cobalt-60 decays to Nickel-60 plus an electron and an electron antineutrino. The decay is initially to a nuclear excited state of nickel-60, from which it emits either one or two gamma-ray photons to reach the ground state of the nickel isotope. The decay scheme of Co-60 is shown,

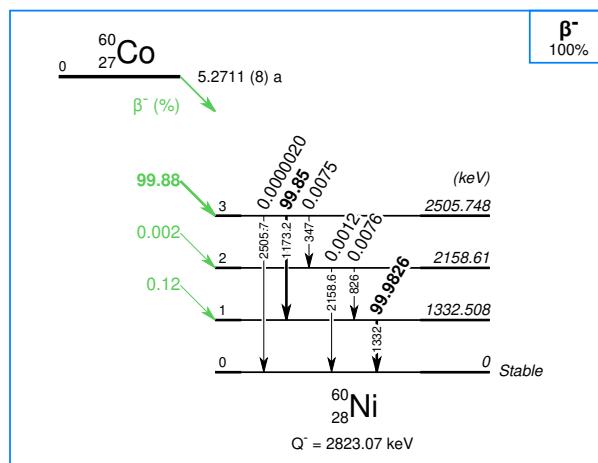


Figure 2.2: Co-60 Decay Scheme

3 | Theory

The output of ionizing radiation beams produced by external beam radiotherapy treatment machines must be determined accurately before the machine is used clinically, and it must also be verified regularly during clinical use to ensure accurate delivery of the prescribed dose to the patient. The output of a Telecobalt machine is the absorbed dose rate to water measured in units of cGy/min at a reference depth in water for a reference field size (e.g., 10 cm \times 10 cm). The output measurement is one of the quality assurance tests that is performed to ensure that the absorbed dose to water for the equipment is within acceptable tolerance, as recommended by the competent authority (AERB).

IAEA TRS 398 — “Absorbed Dose Determination in External Beam Radiotherapy” — is the recommended protocol which is usually followed internationally for the measurement of output from a Telecobalt machine. The protocol and formalism for the measurement of output from a Telecobalt unit are described here. The absorbed dose to water at a point is given by:



$$D_{w,Q} = N_{D,w,Q_0} M_Q k_{Q,Q_0}$$

where

- N_{D,w,Q_0} = Calibration factor (Gy/nC) provided in the calibration certificate,
- M_Q = Corrected meter reading,
- k_{Q,Q_0} = Beam quality correction factor.

Beam Quality Correction Factor (k_{Q,Q_0})

The beam quality correction factor is used when the measurement beam differs from the reference beam in which the chamber was calibrated. The values of this correction factor for various chambers are available in IAEA TRS 398. If both the reference beam and measurement beam are the same, then this factor is taken as 1.

Correction for Temperature, Pressure, and Humidity ($k_{T,P}$)

Since the ionization chamber used to measure output is open to ambient air, the mass of the air in the cavity volume is affected by the surrounding temperature, pressure, and humidity. No correction for humidity is applied if the humidity range is within 20–80%. The correction due to temperature and pressure is given by

$$k_{T,P} = \frac{273.15 + T}{273.15 + T_0} \times \frac{P_0}{P}$$

where T = temperature at the time of measurement, T_0 = reference temperature (20°C), P = pressure at the time of measurement, and P_0 = reference pressure (1013.2 mbar). T_0 and P_0 are the temperature and pressure, respectively, at which the chamber is calibrated, and are mentioned in the calibration certificate.

Correction for Ion Recombination or Saturation (k_s)

This error arises due to incomplete charge collection inside the ionization chamber. The two-voltage method is usually applied to calculate the recombination error. The protocol recommends that the ratio of the two applied voltages be at least 2.

During the charge collection, charges may be lost due to recombination in the active volume or cavity. This recombination is mainly of three types: columnar recombination (or initial recombination), Volume recombination (or general recombination) and Diffusion loss caused by the diffusion of ions onto the measuring electrode against the electric field. The initial recombination is due to the recombination of ions in a single charge particle track. On the other hand, volume recombination is due to ions formed by separate ionizing particle tracks. So, it is dependent on the dose rate. In continuous radiation beams, the general recombination is by far the most important charge loss mechanism, so that initial recombination and diffusion against the electric field are ignored in comparison to general recombination. Under this condition, Boag theory provides the following expression for the collection efficiency f_{gen}^c for a constant dose rate and an electronegative cavity gas.

$$\begin{aligned} f_{gen}^c &= \frac{Q(V)}{Q_{sat}} = \frac{1}{1 + \frac{\lambda_{gen}^c}{V^2}} \\ \frac{1}{Q(V)} &= \frac{1}{Q_{sat}} + \frac{\lambda_{gen}^c}{V^2 Q_{sat}} \\ \frac{1}{Q(V)} &= \frac{1}{Q_{sat}} + \frac{\lambda_{gen}^c}{V^2} \end{aligned}$$

λ_{gen}^c is a parameter that is proportional to the dose rate but also depends on chamber geometry and properties of ions of the cavity gas. The labels “gen” and “c” stand for “general recombination” and “continuous beam”, respectively. Let, in two voltage method for higher voltage V_1 charge collection is Q_1 and for a lower voltage V_2 charge collection is Q_2 .

$$\frac{1}{Q_1} = \frac{1}{Q_{sat}} + \frac{\lambda_{gen}^c}{V_1^2}$$



$$\lambda_{gen}^c = \frac{V_1^2}{Q_1} - \frac{V_1^2}{Q_{sat}} \quad (3.1)$$

For charge Q_2 at Voltage V_2

$$\frac{1}{Q_2} = \frac{1}{Q_{sat}} + \frac{\lambda_{gen}^c}{V_2^2}$$
$$\lambda_{gen}^c = \frac{V_2^2}{Q_2} - \frac{V_2^2}{Q_{sat}} \quad (3.2)$$

Equating (4) and (5):

$$\frac{V_1^2}{Q_1} - \frac{V_1^2}{Q_{sat}} = \frac{V_2^2}{Q_2} - \frac{V_2^2}{Q_{sat}}$$
$$\frac{V_1^2}{Q_1} - \frac{V_2^2}{Q_2} = \frac{1}{Q_{sat}}(V_1^2 - V_2^2)$$
$$Q_{sat} = \frac{Q_1 Q_2 (V_1^2 - V_2^2)}{Q_2 V_1^2 - Q_1 V_2^2}$$

Now we can put the Q_{sat} value to obtain f_{gen}^c and from its reciprocal value of K_s can be calculated.

$$f_{gen}^c = \frac{Q_1}{Q_{sat}} = \frac{Q_1}{\frac{Q_1 Q_2 (V_1^2 - V_2^2)}{Q_2 V_1^2 - Q_1 V_2^2}}$$
$$f_{gen}^c = \frac{\left(\frac{V_1}{V_2}\right)^2 - \frac{Q_2}{Q_1}}{\left(\frac{V_1}{V_2}\right)^2 - 1}$$

$$k_s = \frac{1}{f_{gen}^c(V_1)} = \frac{\left(\frac{V_1}{V_2}\right)^2 - 1}{\left(\frac{V_1}{V_2}\right)^2 - \frac{Q_1}{Q_2}}$$

Polarity Correction (k_{pol})

The electrometer reading changes when the polarity of the bias voltage applied to the ionization chamber is reversed. The correction factor for change in meter readings due to polarizing potentials of opposite polarity is given by:

$$k_{pol} = \frac{|M_+| + |M_-|}{2M}$$

where M_+ = meter reading with positive bias voltage, M_- = meter reading with negative bias voltage, and M = meter reading with the usual bias voltage (used for daily output measurement).

Electrometer Calibration (k_{elec})

Usually, the ionization chamber and measuring electrometer are calibrated as a single unit. In that case, the electrometer calibration factor k_{elec} is unity. If the electrometer is calibrated separately, this factor must be multiplied by the uncorrected meter reading to obtain the corrected reading. The corrected meter reading after applying all correction factors is given as:

$$M_Q = M_{Q,unc} k_{T,P} k_{pol} k_s k_{elec}$$



Table 3.1: Reference Conditions for Absorbed Dose to Water in ^{60}Co Gamma Ray Beams [1]

Influence Quantity	Reference Value or Characteristic
Phantom material	Water
Chamber type	Cylindrical or plane parallel
Measurement depth, z_{ref}	5 g/cm ² (or 10 g/cm ²)
Reference point of the chamber	<ul style="list-style-type: none"> ■ Cylindrical: On the central axis at the centre of the cavity volume. ■ Plane parallel: On the inner surface of the front wall.
Position of reference point of chamber	At the measurement depth z_{ref} for both chamber types
Source-surface source-chamber distance	or 80 cm or 100 cm
Field size	10 cm × 10 cm

4 | Observation

The $30 \times 30 \times 30 \text{ cm}^3$ phantom is filled with water; the height of the water is filled to 25 cm, so the chamber cavity comes at the depth of 10 cm. After proper alignment with the levelling instruments the water temperature and ambient pressure is checked.

At first using a $25 \times 25 \text{ cm}^2$ field size a 3-minute warmup is fired. Then for output measurement $10 \times 10 \text{ cm}^2$ field size with an exposure time of 1 minute is fired for each reading.

Bias Voltage(V)	$M_1(nC)$	$M_2(nC)$	$M_3(nC)$	Average ($M_{Q\text{unc}}(nC)$)
400	8.751	8.757	8.756	8.755(M_1^*)
200	8.788	8.803	8.807	8.799
-400	-8.78	-8.773	-8.771	-8.775
Timer error reading(400 V)	8.935	8.956	8.946	8.946(M_2^*)

Table 4.1: Tabulation for output measurement

Calculation:

■ Temperature and pressure correction factor

$$T = 23.05^\circ\text{C}, P = 1007.35 \text{ mbar}$$

$$T = 20^\circ\text{C}, P = 1013.2 \text{ mbar}$$

$$\begin{aligned} K_{T,P} &= \frac{(273.2 + T) \times P_0}{(273.2 + T_0) \times P} \\ &= \frac{(273.2 + 23.05) \times 1013.2}{(273.2 + 20) \times 1007.35} \\ &= \boxed{1.01627} \end{aligned}$$

■ Saturation Correction factor(k_s):

$$V_1 = 400V; Q_1 = 8.755 \text{ nC}$$



$$V_2 = 200V; Q_2 = 8.799 \text{ nC}$$

$$\begin{aligned} k_s &= \frac{\left(\frac{V_1}{V_2}\right)^2 - 1}{\left(\frac{V_1}{V_2}\right)^2 - \frac{Q_1}{Q_2}} \\ &= \frac{\left(\frac{400}{200}\right)^2 - 1}{\left(\frac{400}{200}\right)^2 - \frac{8.755}{8.799}} \\ &= [0.9983] \end{aligned}$$

■ **Polarity Correction factor(k_{pol}):**

$$\begin{aligned} k_{pol} &= \frac{|M_+| + |M_-|}{2M} \\ &= \frac{|8.755| + |8.775|}{2 \times 8.755} \\ &= [1.001142] \end{aligned}$$

■ **Timer Error:** t= 1 min; n=2

$$\begin{aligned} \delta t &= \frac{M_2^* - M_1^*}{2M_1^* - M_2^*} \times t \\ &= \frac{8.946 - 8.755}{2 \times 8.755 - 8.946} \times 1 \text{ min} \\ &= 0.0223 \text{ min} \end{aligned}$$

■ **Corrected Meter reading:**

$$\begin{aligned} M_Q &= M_{Qunc} \times k_{T,P} \times k_{pol} \times k_{elec} \\ &= 8.755 \times 1.01627 \times 0.9983 \times 1.001142 \times 1 \\ &= [8.892 \text{ nC}] \end{aligned}$$

■ **The absorbed dose to water at 10 cm depth:**

$$k_{Q,Q_0} = 1$$

$$N_{D,w,Q_0} = 5.374 \times 10^7 \text{ Gy/C}$$

$$\begin{aligned} D_{w,Q(z_{ref})} &= N_{D,w,Q_0} \times M_Q \times k_{Q,Q_0} \\ &= 5.374 \times 10^7 \text{ Gy/C} \times 8.892 \text{ nC} \times 1 \\ &= [47.785 \text{ cGy}] \end{aligned}$$

■ **Absorbed dose rate to water at the depth of dose maximum, Z_{max} :**

Depth of dose maximum: $Z_{max} = 0.5 \text{ g/cm}^2$

80 cm SSD set up PDD at Z_{ref} for a 10 cm \times 10 cm field size:

PDD ($Z_{ref} = 10 \text{ gm/cm}^2$) = 56.74% Absorbed dose rate calibration at Z_{max}

$$\begin{aligned} D_{w,Q_{z_{max}}} &= \frac{D_{w,Q}}{PDD \times (t + \delta t)} \\ &= \frac{47.785 \times 100 \text{ cGy}}{56.74 \times 1.0223 \text{ min}} \\ &= [82.3804 \text{ cGy/min}] \end{aligned}$$



5 | Error

Output measured = 82.380 cGy/min.

The calculated output on the date of the experiment = 84.585 cGy/min.

$$\begin{aligned}\text{Error (\%)} &= \left(\frac{\text{Measured} - \text{Standard}}{\text{Standard}} \right) \times 100 \\ &= \left| \frac{82.380 - 84.585}{84.585} \right| \times 100 \\ &= 2.60\% \text{ (within tolerance} = 3\%) \end{aligned}$$

6 | Conclusion

The telecobalt machine uses a radioactive source with a defined geometry and monoenergetic (or fixed average energy), so there is no change in energy. However, due to exponential activity loss, the source strength decreases, so the exposure at a fixed distance also decreases proportionally. During the treatment time calculation, the initial strength of the source is considered, and the present activity is calculated to prescribe the treatment time. The output of the machine is checked monthly to verify whether it is within tolerance (< 3%) from the calculated value or not.

Our results enhance the overall knowledge regarding dose rate calculations and quality control, reinforcing the importance of safe and accurate radiation therapy for patients. This study underscores the significance of routine monitoring and upkeep of Telecobalt Units to maintain their effectiveness in cancer treatments.

7 | References

- [1] International Atomic Energy Agency. Absorbed dose determination in external beam radiotherapy: An international code of practice for dosimetry based on standards of absorbed dose to water. Technical Report 398 (Rev. 1), International Atomic Energy Agency, Vienna, Austria, 2024. Endorsed by the European Society for Radiotherapy and Oncology (ESTRO).