



LCD-Capsule Network for the Detection and Classification of Lung Cancer on Computed Tomography Images

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Abstract

Lung cancer is the second most prominent cancer in men and women, and it is also the leading cause of cancer-related mortality. If lung cancer is diagnosed early, when it is minuscule and has not spread, it is preferable to be adequately treated. A non-invasive low-dose Computed Tomography (CT) scan can detect abnormal patches in the lungs that could be cancerous. It is proposed that machine learning and pattern classification be used to identify and categorize lung cancer from CT scans. Pattern classification algorithms like deep learning can categorize input data into various classes based on the input's characteristic features. A novel deep learning framework formulated by the encapsulation of a Convolutional Neural Network (CNN) and a Capsule Neural Network (CapsNet) called LCD-CapsNet, leveraging the capabilities of these networks to minimize vast amounts of data and achieve spatial invariance for lung cancer detection and classification using CT images is proposed. The primary objective of the proposed method is to create algorithms that would classify and examine images from a dataset to determine whether or not a patient had or posed a danger of developing lung cancer. The Lung Image Database Consortium (LIDC) datasets are utilized to assess this deep learning model, from which 4335 images were collected for the training and testing pipeline. The results demonstrated that LCD-CapsNet outperforms CapsNet, with an average Precision of 95 %, Recall of 94.5 %, F1-Score 94.5 %, Specificity 99.07 %, Area Under the Curve of 0.989, and Accuracy 94 % of benign and malignant data.

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1 Introduction

The world has advanced technologically, yet cancer continues as a chronic disease, with lung cancer being the second most frequent [50]. This is because lung cancer symptoms emerge at the end of the disease's progression, and the patient is no longer able to be rescued. As a result, a person suffering from lung cancer can only be saved if cancer is diagnosed in its initial phases. Because of this, many methodologies were developed as well as computer-aided innovations [54], which are outstanding in their own right. Medical image analysis provides a significant benefit in the realm of health. Different imaging modalities may be used to identify lung cancer [13], and CT [36] is one of the most cost-effective, non-invasive, and efficient methods used in clinics to assess lung health [15]. Manual assessment of lung abnormalities predicted on CT scans is a laborious effort that necessitates the services of a pulmonologist with extensive knowledge. If a computer-assisted approach is used to diagnose a lung abnormality, the evaluation report can be sent to a pulmonary specialist to aid in deciding on a procedure and selecting a course of treatment.

As a result, beginning in the early 1980s, doctors began to use Computer-Aided Diagnostic (CAD) [27] systems to aid in the interpretation of medical images [18]. Such systems investigate images using processes such as preprocessing, segmentation [37], object detection [2, 7], feature extraction, and classification [3]. Extracting features is a crucial part in a CAD framework of machine learning. Lung cancer has been diagnosed using image processing methods in the past [29]. By analyzing CT images obtained with artificial intelligence algorithms, machine learning techniques[1] assist in the diagnosis and classification of lung nodules. In today's fast-paced world of Artificial Intelligence (AI), image processing analytics utilizing Machine Learning [22, 38] and DL [14, 25] technology is highly effective for the accurate diagnosis and detection of lung cancer. DL has evolved tremendously since the advent of the Convolutional Neural Network (CNN) [10, 41] and it has been in use for more than two decades, providing an improved diagnosis.

In traditional CNNs, a certain cost function is utilized in order to measure the global error that builds up at the rear of the network as the training moves forward. On the other hand, if the weight among two neurons is judged to be zero, the activation of a neuron will not develop any further and will cease increasing at that point. This is because the activation of a neuron is dependent on the weight between two neurons. In the process known as recurrent dynamic routing, in addition to the agreement, the information is routed in accordance with the feature specifications. This is done in place of supplying a single size together with the comprehensive cost function.

The problems of vanishing gradient and saturated accuracy can arise if the CNN is trained to an excessive depth. Objects or sub-parts of objects can be represented by capsules, which are collections of neurons whose activity vectors can be used to extract structured features while preserving knowledge of their spatial relationships. An approach used in capsule networks, known as dynamic routing, makes use of the level of agreement among the input capsules to create the final product capsules. For dynamic routing, primary capsules are added together and their weights are adjusted iteratively during the forward based on whether closely their activations match the sum of all the weights. State-of-the-art accuracy can be attained through the use of this routing-by-agreement method.

To solve the aforementioned problems, this paper proposes a Lung Cancer Detection capsule network (LCD-CapsNet) for the diagnosis and categorization of lung cancer. Extracting spatial and temporal features from CT images is facilitated by the capsule network's superior capacity for learning the intrinsic relationship among various features. Accordingly, the capsule network was preferred as the foundational model for lung cancer classification rather than conventional CNNs. The summary of the contributions of this paper are,

- (i) A novel LCD-CapsNet is structured to extract multi-dimensional CT image features to increase classification accuracy and classify lung cancer as either benign or malignant and,
- (ii) The ideation and creation of an effective, highly provable, deep learning neural network based on capsules that is capable of achieving state-of-the-art results on CT images. The proposed LCD-CapsNet combines CNN and CapsNet to outperform state-of-the-art methods on small datasets.

The rest of the manuscript is organized as follows. Section 2 discussed the related works for the lung cancer classification. Section 3 explains the proposed methodology for lung cancer detection. The Capsule Networks and the proposed LCD-CapsNet are also discussed in Section 3. Section 4 presents the dataset that was used to evaluate the proposed LCD-CapsNet, as well as the experiments and findings. Section 5 concludes the paper.

2 Related works

In the field of deep learning, CNNs are a type of multi-layer neural network. Input and output layers, as well as hidden layers, constitute its structure. Most frequently, CNN is applied to images. The CNN will extract the pertinent image features through supervised training. The CNN weights are then determined using the back propagation algorithm version. The hidden layer typically comprises of several multiple stages.

The state-of-the-art CNN architectures [16] are used for image analysis and have produced several satisfying outcomes. It has also made significant progress in lung cancer detection and classification. Song et al. [51] constructed a CNN structure for the detection and classification of lung nodules and yielded an accuracy of 84.15 %. AlexNet is a robust CNN architecture for lung cancer diagnosis, and Hamdalla F. Al-Yasriy et al. [9] examined 110 test CT scans and found it to be 93.54 % accurate. Heng Yu et al. [57] devised a framework for determining lung cancer that uses a deep neural network after segmentation and has comparable accuracy. Abhir Bhandary et al. [15] suggested another deep learning network, a modified AlexNet, for lung cancer classification using the LIDC dataset. For the detection of lung nodules using CT images, H. Polat et al. [42] proposed a CNN model with and P. Wu et al. [55] presented a deep residual network. [33] proposed a 3D lung cancer detection method based on the Active Contour Model, as well as classification using various machine learning algorithms. With the aid of various feature extraction models, Asuntha et al. [12] suggested a deep learning model to detect the cancerous lung nodule.

T. Ghani [20] proposed regression as a machine learning approach for predicting lung cancer survival rates using 2D CT data. An adaptive boosting method was utilized by S. Pang et al. [39] to increase classification performance on a more efficient state-of-the-art CNN architecture, DenseNet, which achieved competent image classification results. A Generative model for lung cancer was established by Salama et al. by using ResNet [45]. G. E. Hinton et al. [44] developed Capsule Network (CapsNet) to alleviate the inadequacies

of CNN, and P. Afshar et al. [5] proposed MIXCAPS network for malignancy prediction in lung nodules based on CapsNet structure. H. J. D. Koresh et al. [26] segmented the major boundaries of the corneal layer and K. Adu et al. [4] proposed a novel method for lung and colon cancer classification based on Capsule Network. Fast CapsNet was used by Aryan Mobiny et al. [31] to suggest a technique for lung screening that was effective for lung nodules. Utilizing the Capsule network, B. Tang et al. [53] used pathological images to detect lung cancer.

Saleh et al. [47] suggested using a CNN in conjunction with the SVM algorithm for the classification of lung cancer. With the assistance of the data from chest CT scans, the CT images of the lungs are classified using a method that is a hybrid of CNN and SVM as either normal, adenocarcinoma, or large cell carcinoma. Squamous cell carcinoma is also a possibility. Kalaivani et al. [24] classified CT scans of the lungs as either normal or malignant using an adaptive boosting algorithm that was implemented using DenseNet Architecture that was trained on Clinical Data. Employing GoogleNet by Huseiny et al. [8] to identify images of malignant nodules found on computed tomography of the lung. The method involves submitting the input images to a pre-processing step that is straightforward and quick. This step extracts regions of interest from the images. The implementation of Harris Hawks optimization techniques, along with the assistance of Cancer Imaging Archive datasets, is used by Guo et al. [21] to improve CNN classifier results. The feature-based classifier was made use of the LBP and Haralick features, which are both relatively well-known. 3D Res U-Net is employed for segmentation, whereas 3D ResNet50 is utilized for the classification of lung cancer by Yu et al. [56] leveraging LIDC-IDRI.

Researchers are also utilizing Capsule Networks for the detection and classification of lung cancer. The concept of a memory-enhanced capsule network that uses LUNA-16 to extract features from high-dimensional input has been proposed by Mobiny et al. [32]. Afshar et al. [6] utilized LIDC-IDRI datasets in the process of implementing a 3D-MCN for lung nodule cancer. The 3D inputs in this method provide information about the 3D nodules, while the multi-scale inputs record the local characteristics. A design based on CapsNet that can handle only a few training samples. Shafi et al. [48] are accountable for the implementation of the Capsule Network with SVM using LIDC-IDRI datasets. Capsule Network is utilized in the process of segmenting lung nodules, while Support Vector Machines are utilized in the process of classifying lung cancer. Ramana et al. [43] utilized LIDC-IDRI datasets to put their Capsule Network and Whale optimization algorithm into action for lung cancer classification. The integration of capsule networks reduces the computational complexity as well as overfitting. The Whale optimization algorithm modifies the pre-trained network's hyperparameters to achieve a higher accuracy rate. The qualitative comparison of earlier methods with the recently proposed method for lung cancer classification leveraging deep neural network is presented in Table 1.

The authors reviewed deep learning-based CT image lung cancer detection and classification models. To improve accuracy, CNN training necessitates a substantial amount of data. CNNs are also sensitive to affine transformation and cannot maintain spatial relationships between image features. The authors use CT scan images to classify lung cancer using the powerful CapsNet. It increases all the performance criteria because the information contained in low-level capsules can be successfully used to determine the poses and the probabilities of high-level capsules, effectively saving a significant number of computational resources while also significantly enhancing the accuracy of image classification. The authors concluded by discussing the difficulties of developing the Capsule Network-based lung cancer detection system.

Table 1 Comparison of previous methods for Lung Cancer Classification

State-of-the-art Model	Methodology	Benchmarks	Key Points
Saleh et al. [47]	CNN+SVM	Chest CT-Scan images Dataset	lung CT images are classified using a hybrid CNN-SVM method into adenocarcinoma, large cell carcinoma, normal, or squamous cell carcinoma.
Kalaivani et al. [24]	DenseNet	Clinical Data	An adaptive boosting algorithm is used with DenseNet Architecture for lung cancer classification
Huseiny et al. [8]	GoogLeNet	IQ OTH/NCCD	Input images are fed to a simple and rapid pre-processing step that extracts regions of interest
Guo et al. [21]	CNN	Cancer Imaging Archive	Improved Harris Hawks optimization improved CNN classifier results. The feature-based classifier used two well-known Haralick and LBP features
Yu et al. [56]	3D ResNet50	LIDC-IDRI	For segmentation, 3D Res U-Net is used, while 3D ResNet50 is used for classification
Mobiny et al. [32]	Capsule Network	LUNA - 16	memory-enhanced capsule network extract features from high-dimensional input
Mobiny et al. [32]	3D-MCN	LIDC-IDRI	3D inputs provide 3D nodule information, while multi-scale input captures local features.
Shafi et al. [48]	Capsule Network+SVM	LIDC-IDRI	capsule Network is used to segment lung nodules while SVM is used to classify lung cancer
Ramana et al. [43]	Capsule Network+WOA	LIDC-IDRI	Whale optimization algorithm tunes pre-trained network hyperparameters to enhance the accuracy rate

The objective of this article is to develop a DL Architecture for early lung cancer diagnosis and classification using LCD-CapsNet which utilizes the characteristics of both Capsule Network and Convolutional Neural Network. CapsNet is a popular image categorization and detection algorithm. Despite the fact that CapsNet lacks a pooling operation, it still provides good classification accuracy with small datasets. This paper proposes a novel framework for extracting features from CT lung images and classifying them as benign or malignant. Few quantifying parameters namely, Accuracy, Precision, F1-Score, and Recall of the proposed method are also compared with state-of-the-art classifiers.

3 Methodology

The framework of the proposed LCD-CapsNet is shown in Fig. 1. The Inputs are pairs of images labeled as benign or malignant. This dataset is divided into three sections namely train, validation, and test data. The train and validation data are pre-processed before being fed into the feature extractor [23]. In the proposed model, CNN is used as a feature extractor which can extract the deep features of images. These image representative features are fed into the proposed LCD-CapsNet model. In LCD-CapsNet, CNN is utilized to extract the features, and capsule networks are employed to perform classification. Accuracy and Loss in training and validation are performed during model training. The accuracy of a proposed model test can be computed with the help of reserve test data. The predicted label is obtained using the softmax classifier. The classification accuracy is calculated using the measure of quality for both the predicted and true labels.

3.1 Datasets

The LIDC-IDRI Dataset contains 1,018 scans from 1,010 patients and 244,527 images. This dataset contains CT scan images and XML files with case-specific CT scan annotations. Four expert thoracic radiologists annotated these images. Radiologists first classified CT findings by sizes such as nodules less than 3 mm, nodules between 3 and 6 mm, and

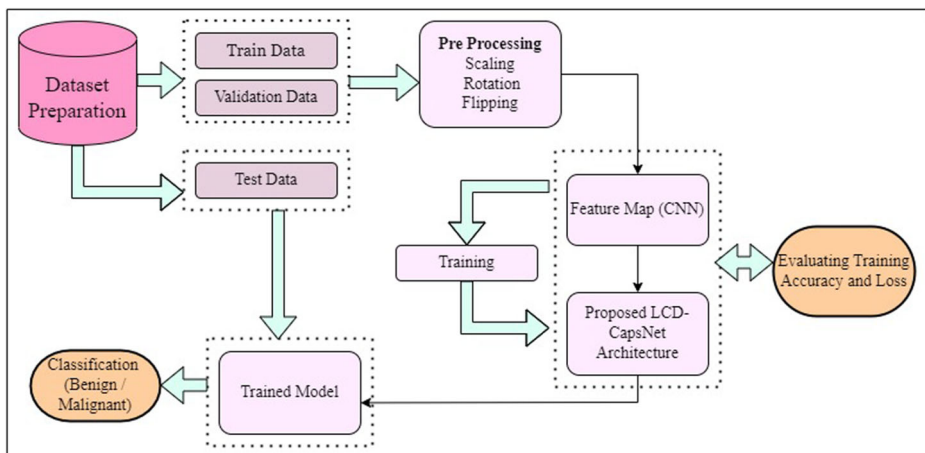


Fig. 1 The Work Flow of the Proposed LCD-CapsNet Model

non-nodules. The second phase involves a covert comparison of radiologist categorizations. Thus, all four radiologists evaluate each dataset nodule independently. This dataset enables nodule and two-label patient diagnosis triage. Each CT scan produces 64 to 764 DICOM images with 512×512 resolution. Unknown, Benign/Non-Cancer, Primary Lung Cancer/Malignant, and Metastatic Lesions are the LIDC-IDRI dataset's four lung nodule categories (Other Primary Cancer). Figure 4 shows LIDC-IDRI datasets of benign and malignant data.

3.2 Preprocessing

Pre-processing images reduces network load and computation complexity. An LIDC-IDRI CSV file contains lung CT scan images with labels. Using CSV annotations, the model separates and labels cancerous and noncancerous images. ImageDataGenerator from the Keras library performed data augmentation techniques like rescaling, rotation, and horizontal and vertical flips. Images can be rotated ten degrees from zero. Set range = 1 and use Rescale by 1./255 to scale each pixel value from [0, 255] to [0, 1]. The color mode function of the flow directory of Python can be used to convert grayscale images into color ones. The Images are downsized from 512×512 to 299×299 , and the Keras ImageDataGenerator class enhances images efficiently and quickly.

3.3 Convolutional neural network

CNN has the advantage of less pre-processing than other classification algorithms. CNN retrieves image features [46] using pooling and convolution. These extracted features then train the model and classify images. The proposed model has four convolutional and one pooling layer as shown in Fig. 2. The convolutional layer filters the image in 3×3 pixels. The actual outcome of the convolutional layer is a matrix that is significantly more compact than the initial image. Backpropagation helps train the network by adding nonlinearity to convolutional layer input. Selecting the maximum or minimum value from each group of values in the pooling layer reduces the activation layer matrix size. Finally, Capsule Network classifies CNN output.

3.4 Capsule network

Capsule Networks, also known as CapsNet, are a type of Artificial Neural Network (ANN) [34] that are designed to overcome the information loss that occurs during the pooling

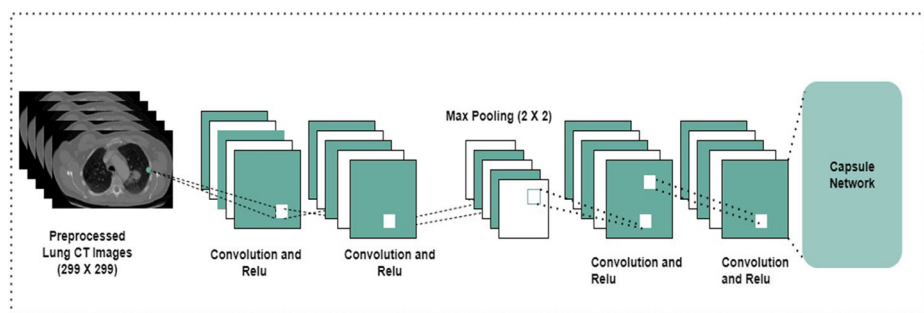


Fig. 2 Block Diagram of Proposed CNN for Feature Extraction

operations carried out by CNN. These networks are able to retrieve spatial information as well as other crucial characteristics. A supervised neural network receives an image as input and outputs a label. The equivariance structure is preferred for tasks that need location-related information, such as segmentation [35] and detection since it preserves the position and its pose across the network. CNN pooling layers downsample the image, which causes the network to gradually lose location-related information. The potential problems of CNN were addressed by Hinton [44] and implemented CapsNet in 2017 as shown in Fig. 3. In a Capsule network, output of each neuron is no longer a scalar, but rather a vector that represents the entity. The angle of the vector represents the entity's properties, and the vector length goes from one to near zero if the entity hardly exists. Otherwise, the closer a vector's length is to one, the more likely it is to exist. The lower layer of the capsule network is connected to the higher layer via a matrix that predicts the whole object based on the recognized part. The weighted sums of all the prediction vectors in a parent capsule are used to calculate the final result vector.

During training, the network employs the routing by agreement technique, in which each prediction vector is a dot product with the output vector, with the results gradually adjusting the connection weights. Let the layers p and $p + 1$ ought to have m and n capsules respectively. Calculating the activations of the capsules at layer $p + 1$ is the objective given the activations at layer p . Initially, the capsules at layer p are used to compute the prediction vectors. The prediction vector $\hat{v}_{j|i}$ for j of layer $p + 1$ by a capsule i of the layer, p is provided by (1).

$$\hat{v}_{j|i} = W_{i,j} v_i \quad (1)$$

where $W_{i,j}$ is the weight matrix and v_i is capsule activations at layer t . The weighted total of all the prediction vectors f_j generated by the capsules of layer t for the capsule j is then used to compute the output vector for the capsule j as shown in (2).

$$f_j = \sum_i C_{i,j} \hat{v}_{j|i} \quad (2)$$

Between capsules i and j , the scalar $C_{i,j}$ stands for a Coupling Coefficient. The capsules of layers p and $p + 1$ are connected by different coupling coefficients $C_{i,j}$, which will be adjusted depending on the image content. It can be established by a dynamic routing algorithm as in (3).

$$C_{i,j} = \frac{e^{b_{i,j}}}{\sum_k e^{b_{i,k}}} \quad (3)$$

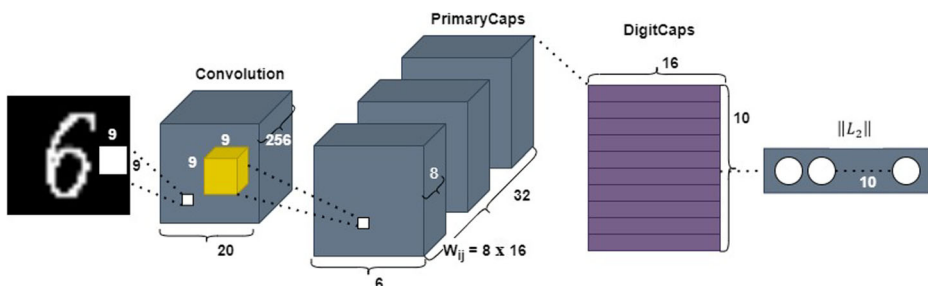


Fig. 3 Basic Capsule Network Model

The output vector f_j is squashed to get the activation s_j of the capsule e_j . The squashing function is applied to make the probability of the magnitude of the output vector between 0 and 1. At the layer $p + 1$, for a capsule j , $s_j = \text{squash}(f_j)$ and is calculated using (4).

$$\text{Squash function}, s_j = \frac{\|f_j\|^2 \cdot f_j}{1 + \|f_j\|^2 \cdot \|f_j\|} \quad (4)$$

where s_j represents the capsule's vector output and f_j represents the capsule's final input. When $\|f_j\| = 0$, the derivative of $\|f_j\|$ is unbounded, and it has the potential to explode during training. Calculating the square root of the sum of squares as well as a small epsilon number ϵ , provides the solution as in (5).

$$\|f_j\| = \sqrt{\sum_i s^2 + \epsilon} \quad (5)$$

Finally, the scalar product a_{ij} is used by (6), to calculate the agreement.

$$a_{i,j} = f_j \cdot \hat{v}_{j|i} \quad (6)$$

During the entire process, the Coupling Coefficient $c_{i,j}$ learns from the input data, whereas the weight matrix $W_{i,j}$ adapts and modifies itself during training in CapsNet based on back propagation.

3.5 LCD-CapsNet

3.5.1 Overview of the architecture

The architecture of the LCD-CapsNet is shown in Fig. 4. The overview of LCD-CapsNet is as follows. There are four convolutional layers and two capsule layers in this network. Input to this is pre-processed lung CT images.

During pre-processing, 512×512 images were sampled down to 299×299 images, to shorten training time and reduce the number of parameters. In addition, each pixel value undergoes a rescaling transformation, shifting it from $[0, 255]$ to $[0, 1]$, as well as a rotation and flipping (both horizontal and vertical) of the image.

The first layer is the convolution layer which learns 64 filters, convolves with a kernel of size 3×3 and stride 1, and produces a feature map of size $297 \times 297 \times 64$. The batch

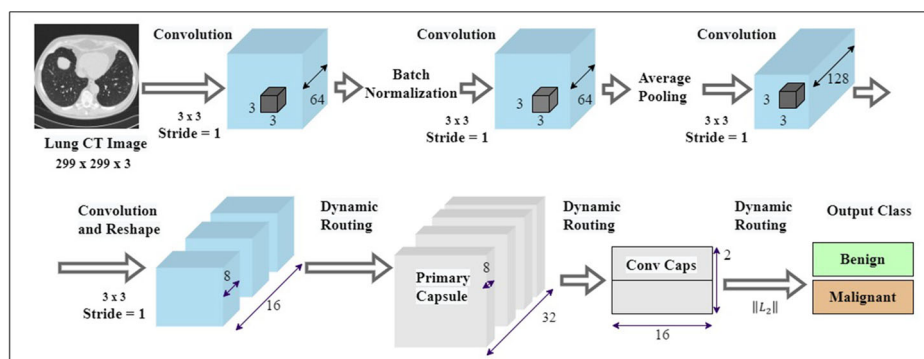


Fig. 4 LCD-CapsNet Architecture for Lung Cancer Detection and Classification

normalization used after the convolution layer, helps to maintain output mean zero and output variance one. The second layer is a convolution $295 \times 295 \times 64$, followed by average pooling that reduces output shape to $147 \times 147 \times 64$. The third and fourth convolution layers learn 128 filters and reshape the output of the fourth layer, which is the input of the Capsule Network. To activate the network, the ReLu function is used across all four convolutional layers.

The LCD-CapsNet contains two Capsule layers that execute the routing by the agreement method explained in Section 5.2. The primary capsule layer comprises 32 capsules of size 8 each. The final Capsule layer named Conv Caps includes the instantiation parameters for the 2 types with a dimension of 16 namely benign and malignant. The squash function is deployed as the non-linear activation function in the capsule network, with the length of these two capsules representing the probability of each category occurring.

3.5.2 Routing by agreement algorithm

Dynamic routing involves transmission of lower capsules data to a higher capsule, which is more appropriate capsule. It is the parent capsule that receives the results from child capsules. Using the agreement and assignment mechanism, which is based on the dot product, expectation-maximization, and mixture models, parent capsules carry out routing. The capsule with the greatest dot product is selected as the parent capsule. A dot product is calculated by multiplying the weight matrix by the prediction vector that was generated by the lower capsule layers.

The classification is formed by computing the length $\|L2\|$ of the capsule vectors in the final layer and allocating the malignant class to those capsule vectors whose magnitude are greater than the threshold, and the benign class to those capsule vectors whose magnitude are less than the threshold. The schematic representation in Fig. 5 explains dynamic routing algorithm. The input vector v_i , also known as the lower-level capsule is subjected to an affine transformation. The prediction vector \hat{v}_i is obtained by multiplying each of these vectors v_i by the weight vector W_{ij} . The weighted sum of these prediction vectors with the coupling coefficient C_{ij} , which is learned through routing by agreement is computed. The

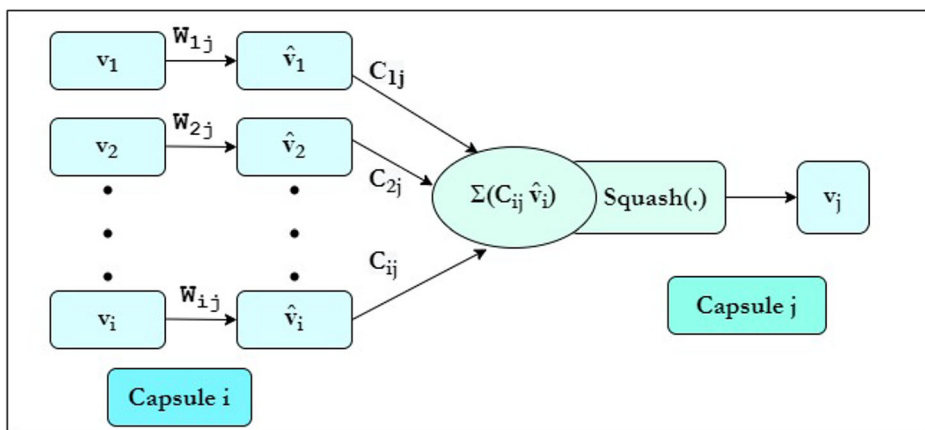


Fig. 5 Schematic Representation of Dynamic Routing Algorithm

weighted sum runs through a non-linearity squash function to ensure that the vector length is between 0 and 1. Algorithm 1 summarizes the pseudocode for LCD-CapsNet agreement routing.

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procedure Routing ( $\hat{v}_{j|i}$ ,  $z$ ,  $p$ )
for in layer  $p$  and capsule  $j$  in layer  $(p + 1)$ , and for every capsule  $i$ :  $b_{i,j} \leftarrow 0$ .
for  $z$  iterations do
for in layer  $p$ , all capsules  $i$ :  $c_i \leftarrow \text{softmax}(b_i)$ : using Eq. (3)
for in layer  $(p + 1)$  all the capsules  $j$ :
 $f_i \leftarrow \sum_i c_{ij} \hat{v}_{j|i}$ 
for in layer  $(p + 1)$  all the capsules  $j$ :
 $s_j \leftarrow \text{squash}(f_j)$ ; using Eq. (4)
for in layer  $p$  and capsule  $j$  in layer  $(p + 1)$  all the capsules  $i$ :  $b_{i,j} \leftarrow b_{i,j} + f_j \cdot \hat{v}_{j|i}$ 
return  $f_i$ 

```

Algorithm 1 Routing by Agreement between Capsules

3.5.3 Loss function

The loss function is utilized to assess the accuracy of the network's predictions. Equation (7) is used to compute the loss in the LCD-CapsNet:

$$L_m = T_m \max(0, h^+ - \|f_m\|)^2 + \lambda(1 - T_m) \max(0, \|f_m\| - h^-)^2 \quad (7)$$

where L_m - Loss term for one Conv Caps, T_m - Loss function of Conv Caps,

λ is numerical stability coefficient whose value is fixed at 0.5. $T_m \max(0, h^+ - \|f_m\|)^2$, calculates the loss for accurate ConvCaps, when T_m is 1. $\lambda(1 - T_m) \max(0, \|f_m\| - h^-)^2$ computes the loss for erroneous ConvCaps, when T_m is 0.

4 Experimental results and discussion

The proposed system was evaluated using the LIDC dataset [11]. A total of 4335 CT images were utilized in this experiment for evaluation. Of these 2160 are benign and 2175 are malignant data. Four radiologists examined the LIDC data set in depth. This dataset depicts the size of nodules present in the lung using CT scans. If the size of the nodule is less than 3mm, it is deemed benign and if the size of the nodule is larger than 3mm, it is labeled as malignant. Figure 6 shows the samples of benign and malignant data of LIDC datasets. The datasets are broken down into three categories namely training, testing, and validation sets. From the LIDC dataset, 20% of the images (867) are used as test data. Of the remaining 80% of the image, 20% (694) are used for validation which is used to identify the best performing model, and the leftover datasets (2774) are considered as training sets for training the model.

With a learning rate of 10^{-3} , 50 epochs, a fixed batch size of 16, and this system was trained using an Adam optimizer. The non-linear activation function employed in Capsule is the squashing function. It reduces the length of a large vector to near one and the length of a small vector to zero. The experiments were carried out using Python libraries such as Keras and TensorFlow on a GPU NVIDIA-MX450, an i5-1135G7 processor, with Windows as the operating system.

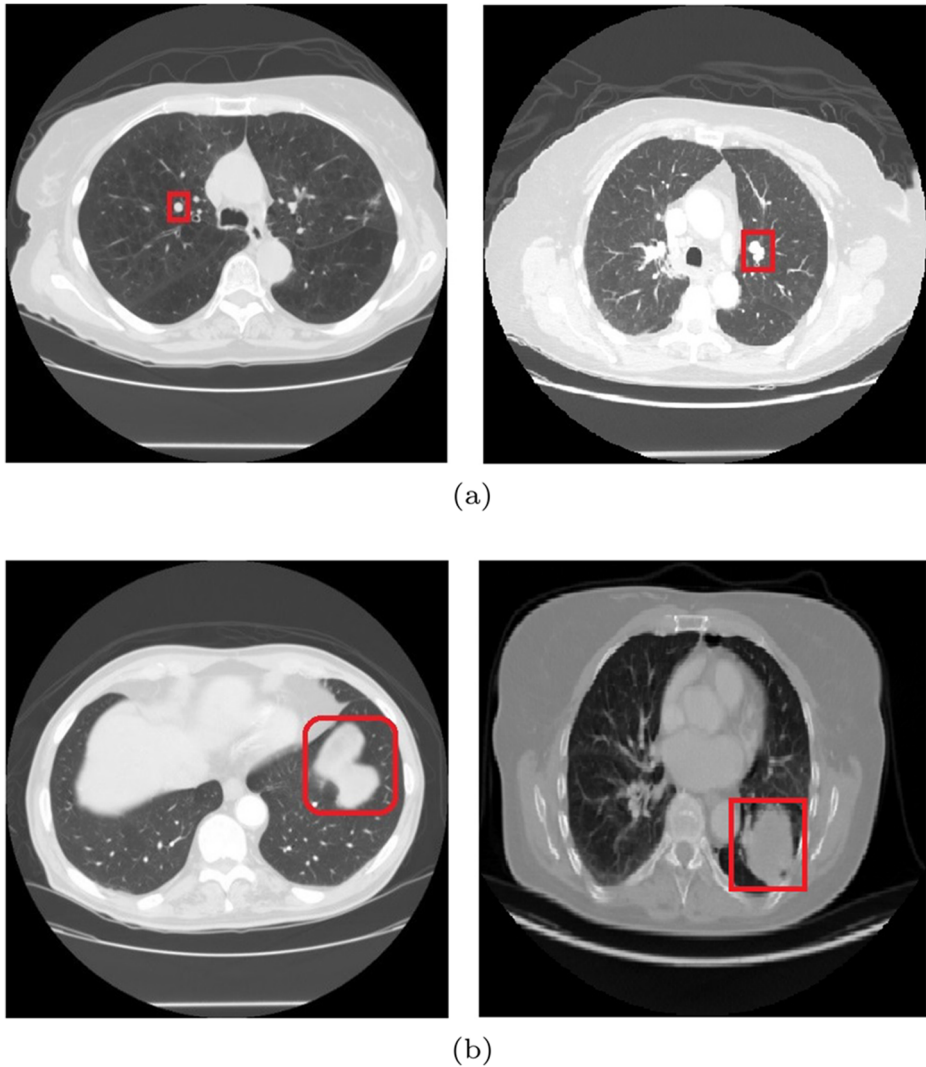


Fig. 6 Sample Lung Images (a) Benign nodule (b) Malignant nodule (Courtesy: LIDC- IDRI Dataset)

Two experiments have been done in this paper. They are detection and classification of Lung cancer using CapsNet, and LCD-CapsNet. In CapsNet, two secondary capsule layers were used after the primary capsule, and the total number of parameters were 295,488. But in the proposed LCD-CapsNet, only one secondary capsule layer is used, therefore the number of parameters could be reduced to 293,440. Feature map in Fig. 7 visualizes an inside story of LCD-CapsNet identifying different features present in lung images, thereby providing a deeper understanding of the algorithm of the proposed model. The abstract features are learned while moving deeper inside the neural network. In the initial stages of a neural network, it is possible to interpret the details that the filter is attempting to extract from the images. However, as the network progresses deeper, the process becomes

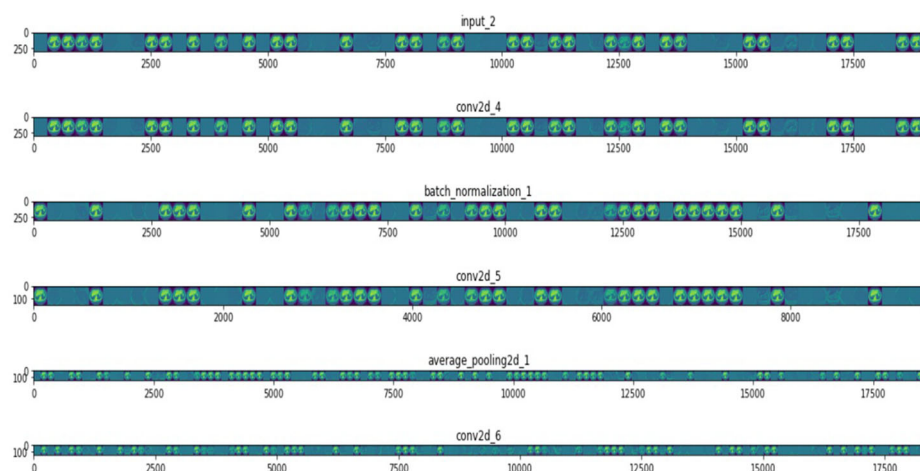


Fig. 7 Feature map for Lung image of LCD-CapsNet

more complex. The developed system was successfully trained and tested. The performance evaluation matrices of accuracy, recall, precision, and F1 score were also determined.

The amount of time necessary to train the models is listed in Table 2, together with the number of network parameters that required to be learned during the training procedure (expressed on the scale of millions). It is clear that the training and testing of the LCD-CapsNet is significantly faster than that of the conventional CapsNet for the data sets.

Figure 8 represents the training progress of CapsNet and LCD-CapsNet in which, Fig. 8 a) depicts the accuracy curve of training and validation of CapsNet, whereas Fig. 8 b) illustrates the training and validation accuracy of LCD-CapsNet. By evaluating these accuracy curves, it is known that the LCD-CapsNet provides improved accuracy than CapsNet. Figure 8c) and d) illustrate the training and validation loss of CapsNet and LCD-CapsNet respectively. The loss was reduced to 0.048 in CapsNet after 50 epochs, whereas the final loss in the proposed LCD-CapsNet is 0.037. Table 3 illustrates the confusion matrices, which indicate the effectiveness of the categorization models CapsNet and LCD-CapsNet.

There are 376 True Positive (TP) instances in CapsNet where the system predicted the existence of malignancy and 428 True Negative (TN) cases where the system predicted the absence of cancer in CapsNet. In addition, 4 False Positive (FP) instances projected malignancy but did not have cancer, indicating a Type 1 error, while 59 False Negative (FN) cases predicted benign but were malignant, indicating a Type 2 error. However, in the LCD-CapsNet system, the instances of TP, TN, FP, and FN are 392, 427, 5, and 43, respectively. From the comparison matrices shows in Table 1 it is understood that LCD-CapsNet provides better classification than CapsNet.

Table 2 Number of parameters and Processing time Comparison of CapsNet and LCD-CapsNet

Method	Parameters	Processing Time (s)
CapsNet	0.295M	1457
LCD-CapsNet	0.293M	1304

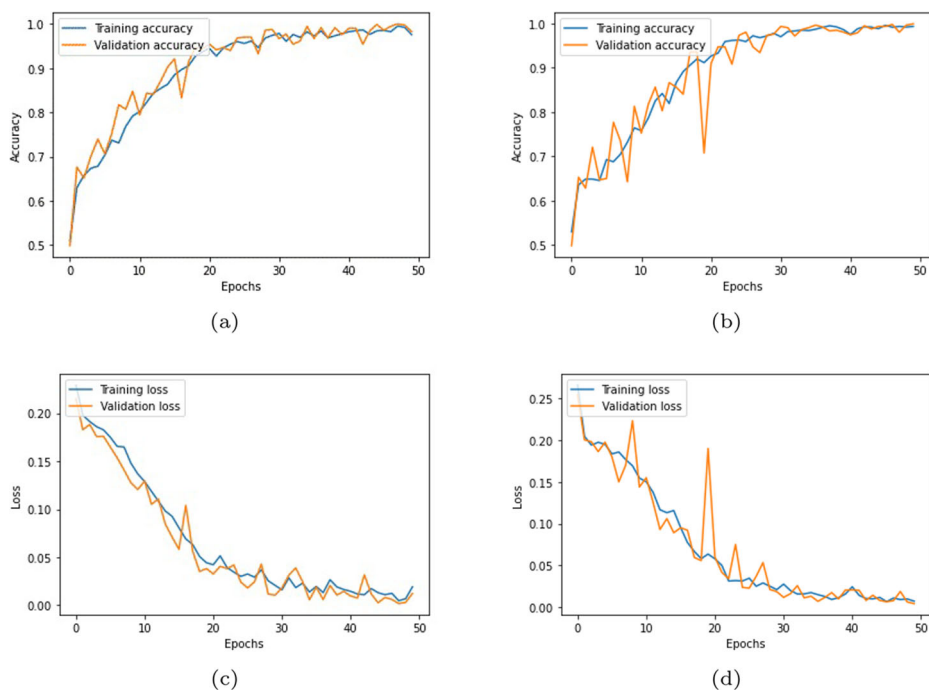


Fig. 8 Training progress of CapsNet and proposed LCD-CapsNet (a) Accuracy of CapsNet (b) Accuracy of LCD-CapsNet (c) Loss of CapsNet (d) Loss of LCD-CapsNet

The performance analysis matrices for the imposed CapsNet and LCD-CapsNet are shown in Tables 4. The inferences from the performance comparison are as follows. In LCD-CapsNet, all the performance metrics have been improved, as shown in Tables 4. Out of 867 test samples, 432 are benign and 435 are malignant. In CapsNet, the value of Recall or sensitivity and F1-Score is 92.5 %, whereas it is 94.5 % in LCD-CapsNet. Precision has increased from 93 % to 95 % and test accuracy has increased from 93 % to 94 %.

Table 5 compares the proposed LCD-CapsNet model with the existing cutting-edge CNN lung cancer classification methods. As shown in Table 5, LCD-CapsNet outperformed other state-of-the-art architectures in terms of accuracy, AUC, sensitivity, and specificity. Over [5], its accuracy is increased by 3.3%, AUC increased by 0.033, sensitivity increased by 4.5%, and specificity increased by 5.67%.

Table 3 Confusion Matrices of CapsNet and LCD-CapsNet

Model	Actual Class	Predicted Class	
		Benign	Malignant
CapsNet	Benign	428	4
	Malignant	59	376
LCD-CapsNet	Benign	427	5
	Malignant	43	392

Table 4 Performance analysis matrices for the proposed CapsNet and LCD-CapsNet

Quantifying Metrics	Model	
	CapsNet	LCD-CapsNet
Parameters	295,488	293,440
Precision (%)	93.5	95.0
F1-Score (%)	92.5	94.5
Recall(Sensitivity) (%)	92.5	94.5
Specificity (%)	98.5	99.1
Accuracy (%)	93.0	94.0

The performance of the proposed system is further visualized by the ROC curve and AUC value as shown in Fig. 9. The ROC curve is sketched with the sensitivity on the true positive rate on the y-axis and the 1- specificity (False Positive Rate) on the x-axis. While CapsNet has an AUC of 0.985, LCD-CapsNet has an AUC of 0.989 which is evident from Fig. 9. From these discussions it is understood that LCD-CapsNet outperforms CapsNet on LIDC datasets for lung cancer classification.

The baseline CapsNet model even outperformed the rest of the models in terms of accuracy, AUC, sensitivity, and specificity. Sensitivity and specificity are two important metrics used to gauge a test's accuracy and reliability. In this case, sensitivity is defined as the ability to detect cancer. It is critical to avoid providing a false negative.

A patient's clinical picture will be altered if a false negative is detected. Also, specificity refers to a test's ability to avoid false positives. False-positive results are undesirable for a cancer test because they may give the patient the false impression that they have been exposed to cancer in the past. LCD-CapsNet has better sensitivity, accuracy, and specificity than the state-of-the-art models, which is known from Fig. 10. In Fig. 10, x-axis represents the percentage value of accuracy, sensitivity and specificity and y-axis represents the methods used.

Table 6 presents a comparison between the recently suggested LCD-CapsNet model and the already deployed machine learning lung cancer detection methods. In terms of accuracy, sensitivity, and specificity, LCD-CapsNet performed significantly better than other methods, as shown in Table 6.

Table 5 Comparison of LCD-CapsNet with classical CNN methods

Literature	Accuracy(%)	AUC	Sensitivity(%)	Specificity(%)
Sori et al. [52]	87.80	-	87.40	89.10
Shen et al. [49]	87.14	0.930	77.00	90.03
Song et al. [51]	84.15	-	83.96	84.34
Causey et al. [17]	87.90	0.938	87.90	87.90
Afshar et al. [5]	90.70	0.956	89.50	93.40
Baseline	93.00	0.985	92.50	98.50
Proposed Work	94.00	0.989	94.50	99.07

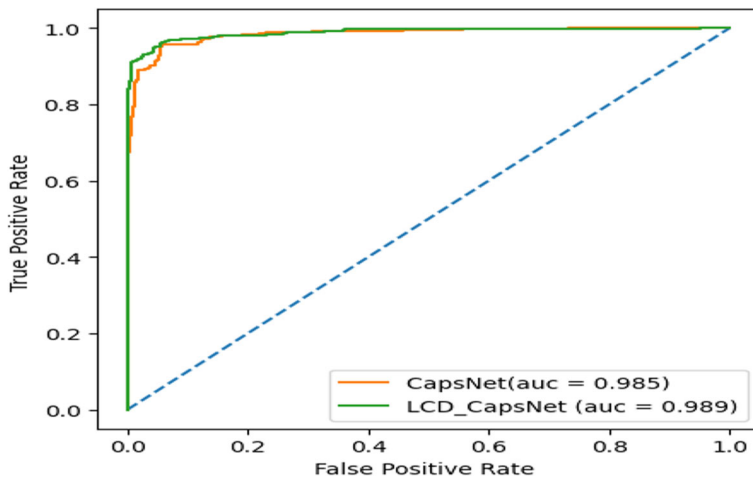


Fig. 9 Comparison of ROC of the Proposed LCD-Capsnet with CapsNet

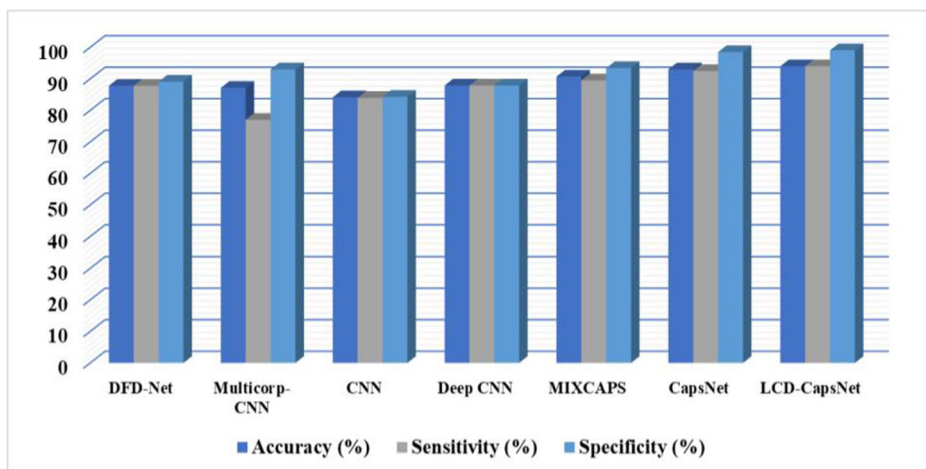


Fig. 10 Comparison of the proposed LCD-CapsNet method with the existing methods in terms of specificity, sensitivity, and accuracy

Table 6 Comparison of LCD-CapsNet with Machine Learning Methods

Literature	Model	Accuracy(%)	Sensitivity(%)	Specificity(%)
Parveen et al.[40]	SVM	-	91.38	89.56
Lennartz et al.[28]	KNN	87.00	94.00	67.00
Askary et al.[19]	Random Forest	90.73	90.67	90.8
Manju et al. [30]	SVM	87.00	88.00	-
Proposed	LCD-CapsNet	94.00	94.50	99.07

The Area Under the ROC Curve (AUC) is a numerical representation of the diagnostic test's overall performance. Fig. 11 depicts the AUC comparison of the proposed LCD-CapsNet model with other methods, demonstrating that the presented model is superior to the others.

Although the proposed LCD-Capsnet has achieved the highest accuracy, it does have some drawbacks. The most significant of which are that its algorithm is sluggish, primarily as a result of the inner loop of the dynamic routing algorithm, and that its implementation is more difficult than that of CNNs.

5 Conclusion and recommendation

This paper proposes two deep learning frameworks for Lung Cancer prediction based on LCD-CapsNet and CapsNet to enhance the performance in diagnosing Lung Cancer using CT images. The proposed LCD-CapsNet Architecture was developed using algorithms that would classify and analyze images from LIDC IDRI datasets to diagnose whether a patient even had lung tumor or was at possibility of acquiring it. A convolutional neural network was deployed to extract high-level features, and a capsule neural network was utilized to classify them. Lung nodule malignancy and benignness prediction in LIDC-IDRI datasets are compared.

The cross-validation results are quite promising, showing that Capsule Networks are better than CNN models at gathering pose information and spatial correlations, as well as distinguishing between malignant and benign images. Eventhough the amount of trainable parameters in LCD-CapsNet are fewer than in CapsNet, the results showed that LCD-CapsNet has excellent performance with limited set. The findings show that LCD-CapsNet is superior to CapsNet, with an average Accuracy of 94 % , Precision of 95 % , Recall of 94.5 % , F1-Score of 94.5 % , Specificity of 99.07 % , and AUC of 0.989 for both benign and malignant data. The objective of the study is fulfilled by achieving better results of performance matrices while using a smaller sample size of image datasets.

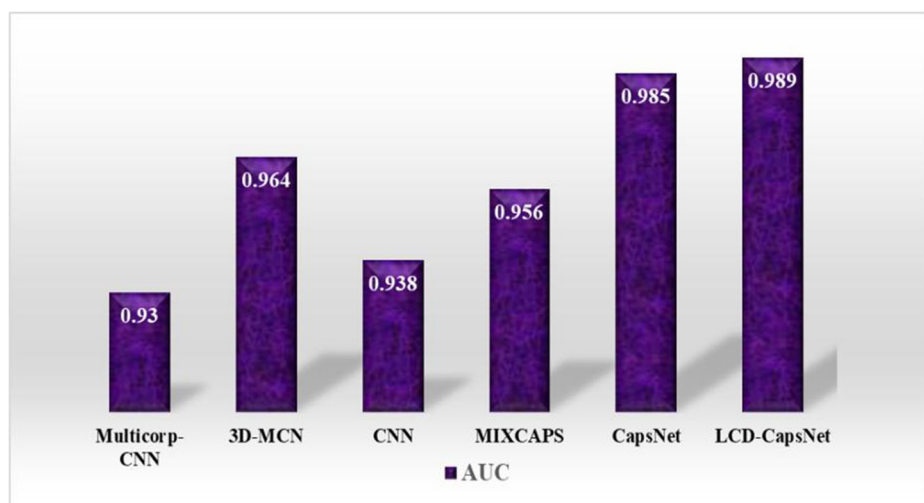


Fig. 11 AUC Comparison of the proposed LCD-CapsNet model with the existing methods

In the future research, VGG can be utilized as an alternative to CNN in the LCD-CapsNet input, to analyze an extension of CapsNet by increasing the number of capsule layers to alleviate the constraints of CapsNet.

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Data Availability LIDC-IDRI data are publicly available

Declarations

Conflict of Interests The authors declare that they have no conflict of interest.

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