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FMRIE
Oxford Centre for Functional M

FSL Pre-Processing Pipeline

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FSL Pre-Processing Pipeline

Standard pre-processing:

- Task fMRI
- Resting-state fMRI

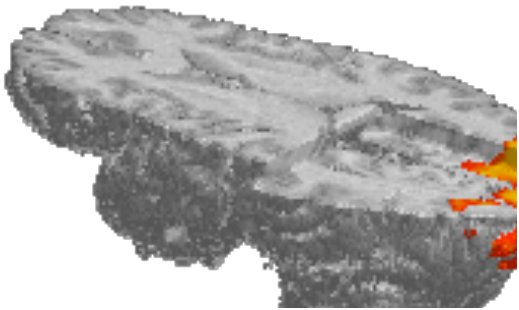
Quality Assessment

Alternatives

- Other pre-processing options
- GLM-based or ICA-based "pre-processing"

Complications

- Spatial and temporal interactions
- HRF variation



HCP Pipeline

FSL Pre-Processing Pipeline

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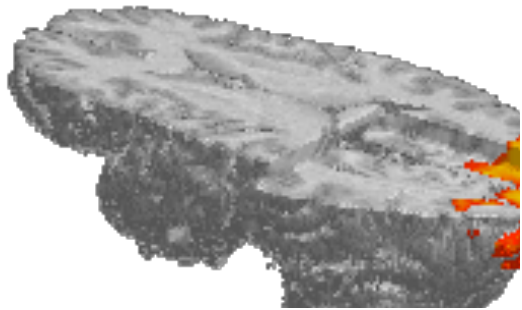
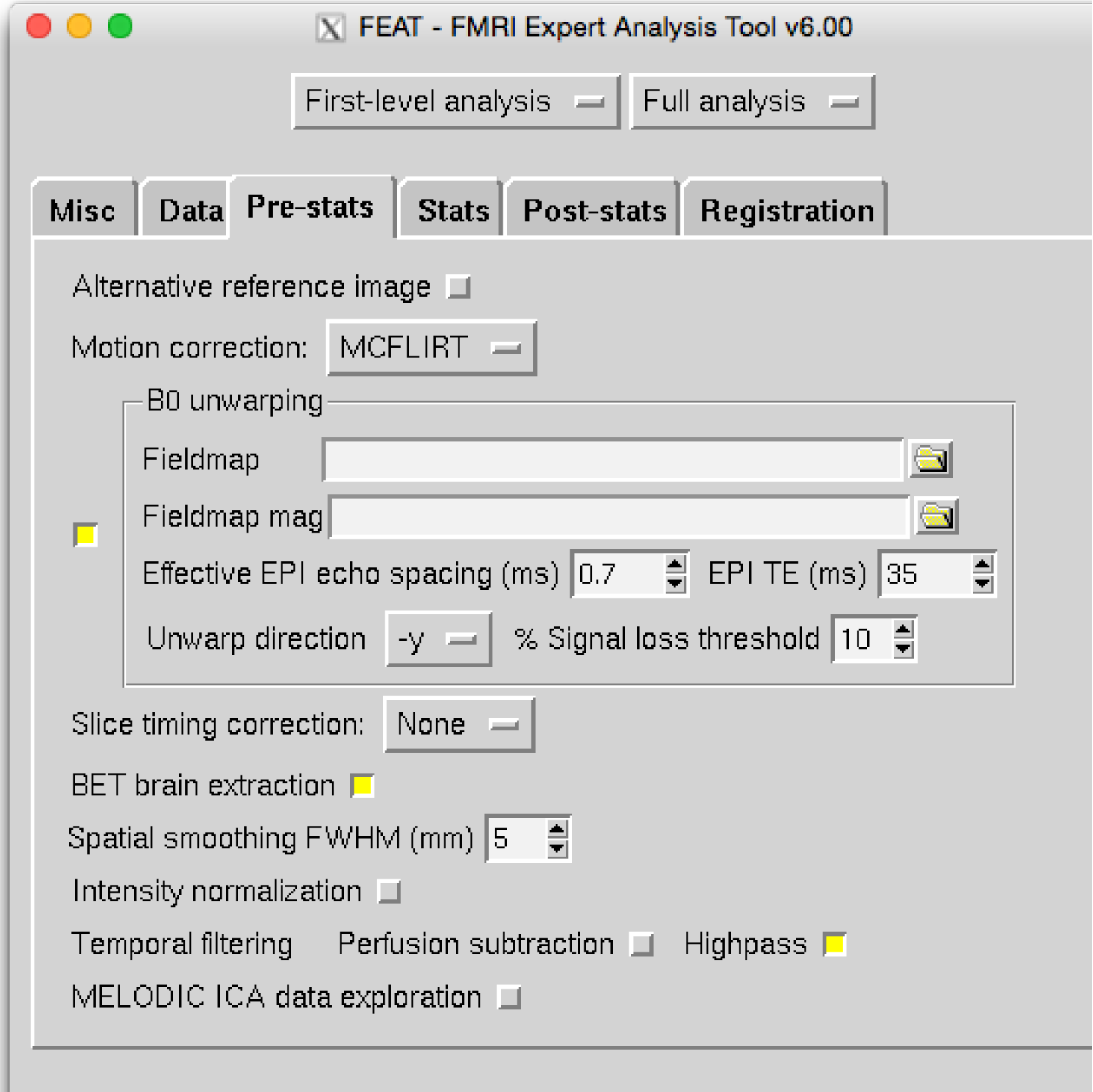


HCP Pipeline

Standard Pre-Processing Pipeline

Task-fMRI
(GLM-based)



Standard Pre-Processing Pipeline

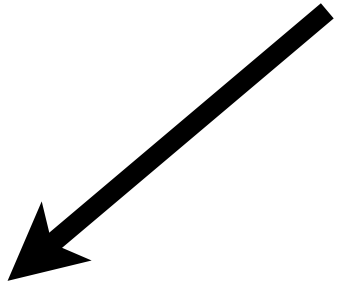
Task-fMRI
(GLM-based)

- Motion Correction
- Distortion Correction
- Spatial Smoothing
- Temporal Filtering
- GLM
- Resampling to

Standard Pre-Processing Pipeline

Task-fMRI *(GLM-based)*

- 6 DOF
- Whole-volume
- Normalised correlation
- First volume is reference (or can select other)



- Motion Correction
- Distortion Correction
- Spatial Smoothing
- Temporal Filtering
- **GLM**
- Resampling to

Standard Pre-Processing Pipeline

Task-fMRI
(GLM-based)

- Requires fieldmaps
- Uses BBR
- Makes a substantial difference to group-level results even in non-distorted areas

Motion Correction

Distortion Correction

Spatial Smoothing

Temporal Filtering

GLM

Resampling to

Standard Pre-Processing Pipeline

Task-fMRI *(GLM-based)*

- De-weights different tissues (esp. CSF)
- SUSAN algorithm
- Very similar to Gaussian within GM & WM
- Recommend small FWHM

Motion Correction

Distortion Correction

Spatial Smoothing

Temporal Filtering

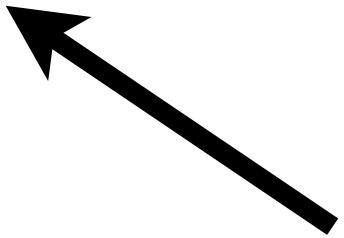
GLM

Resampling to

Standard Pre-Processing Pipeline

Task-fMRI
(GLM-based)

- Highpass only
- Tool for calculating cutoff based on design matrix



Motion Correction

Distortion Correction

Spatial Smoothing

Temporal Filtering

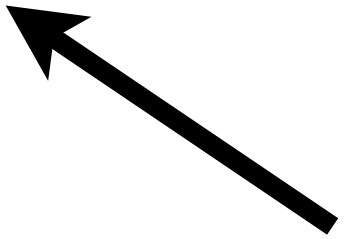
GLM

Resampling to

Standard Pre-Processing Pipeline

Task-fMRI *(GLM-based)*

- Slice-timing effects modelled with temporal derivatives
- Related to basis functions and HRF variability *(see later)*



Motion Correction

Distortion Correction

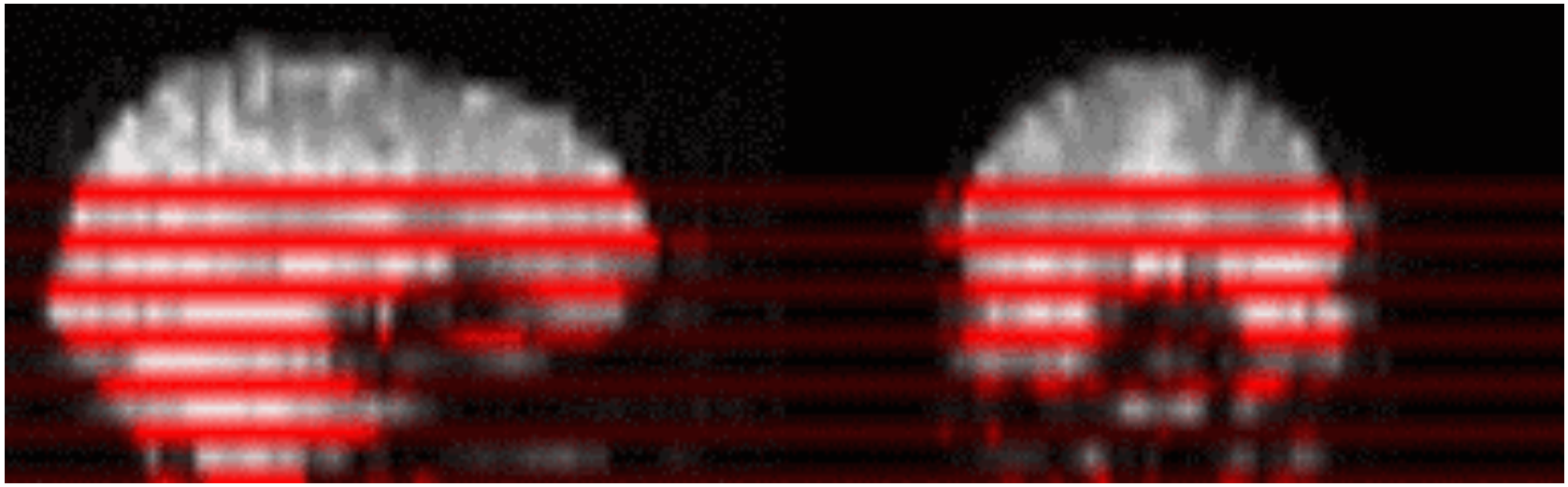
Spatial Smoothing

Temporal Filtering

GLM

Resampling to

Slice Timing



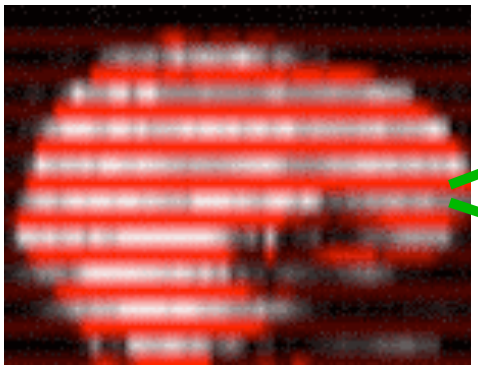
Almost all FMRI scanning takes each slice separately

Each slice is scanned at a slightly different time

Slice order can be interleaved (as shown) or sequential (up or down)

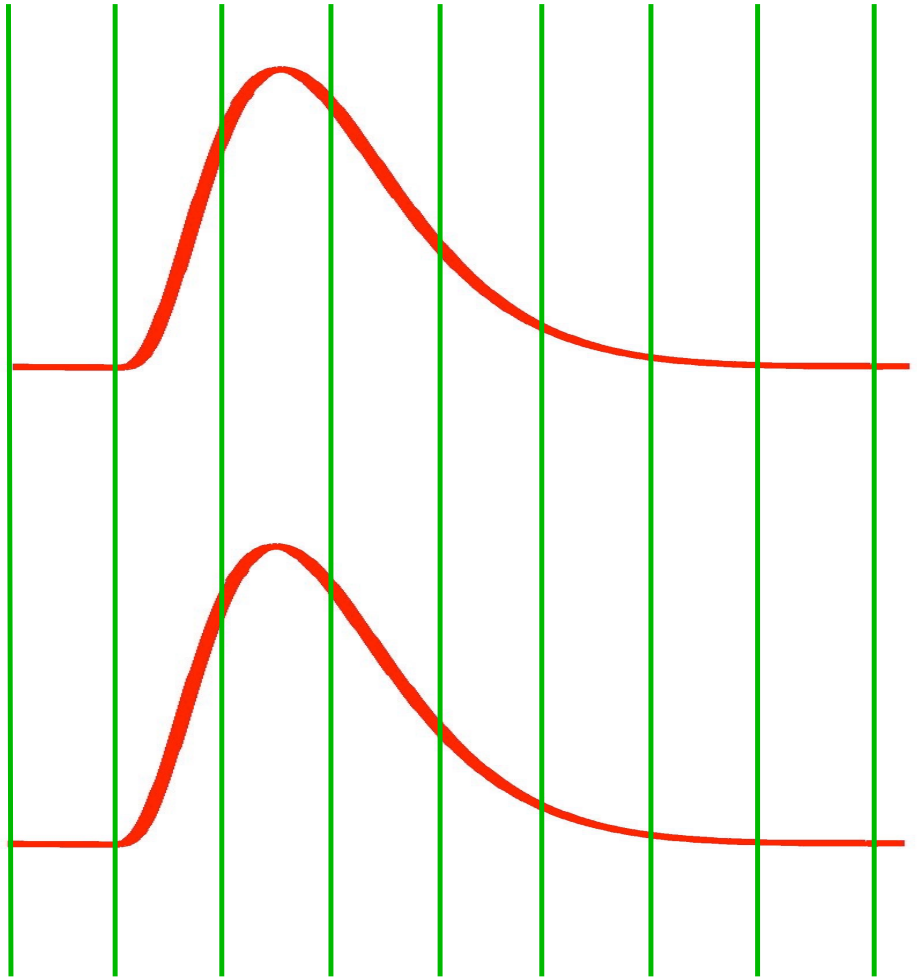
Slice Timing

Without any adjustment, the model timing is always the same



slice 10

slice 9

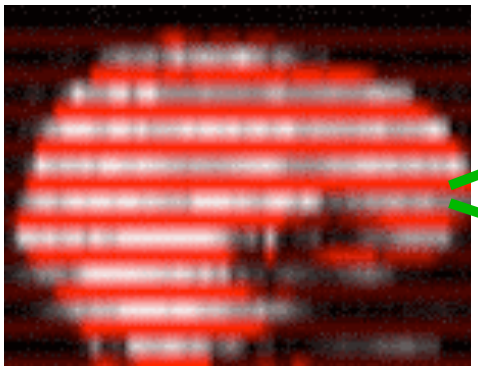


Slice 9 acquired 1.5 secs after slice 10

acquisition timing (TRs)

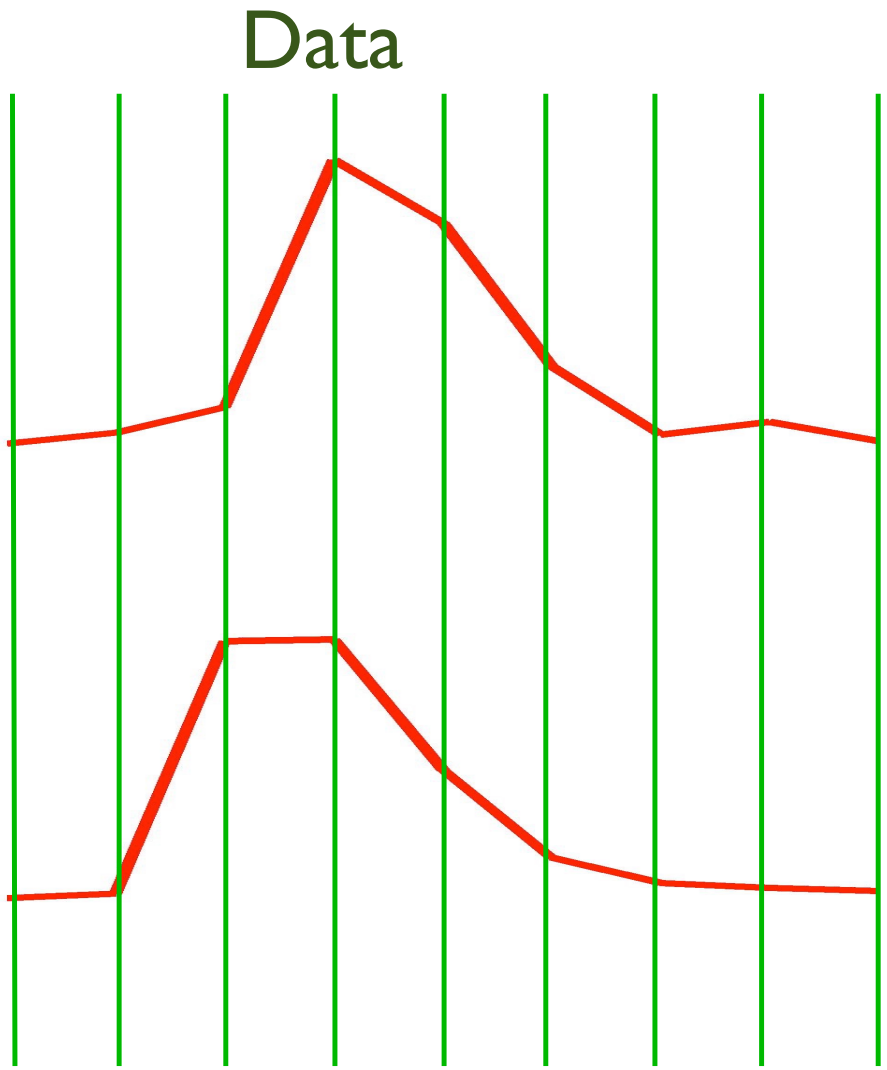
Slice Timing

... but the timing of each slice's data is *different*



slice 10

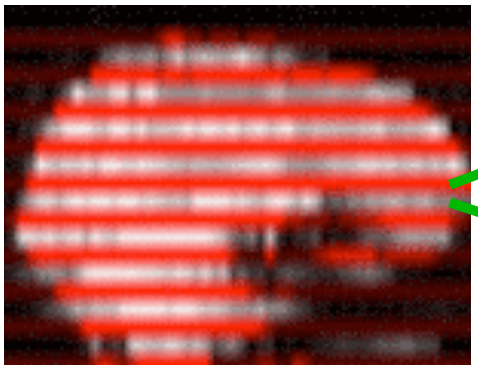
slice 9



Slice 9 acquired 1.5 secs after slice 10

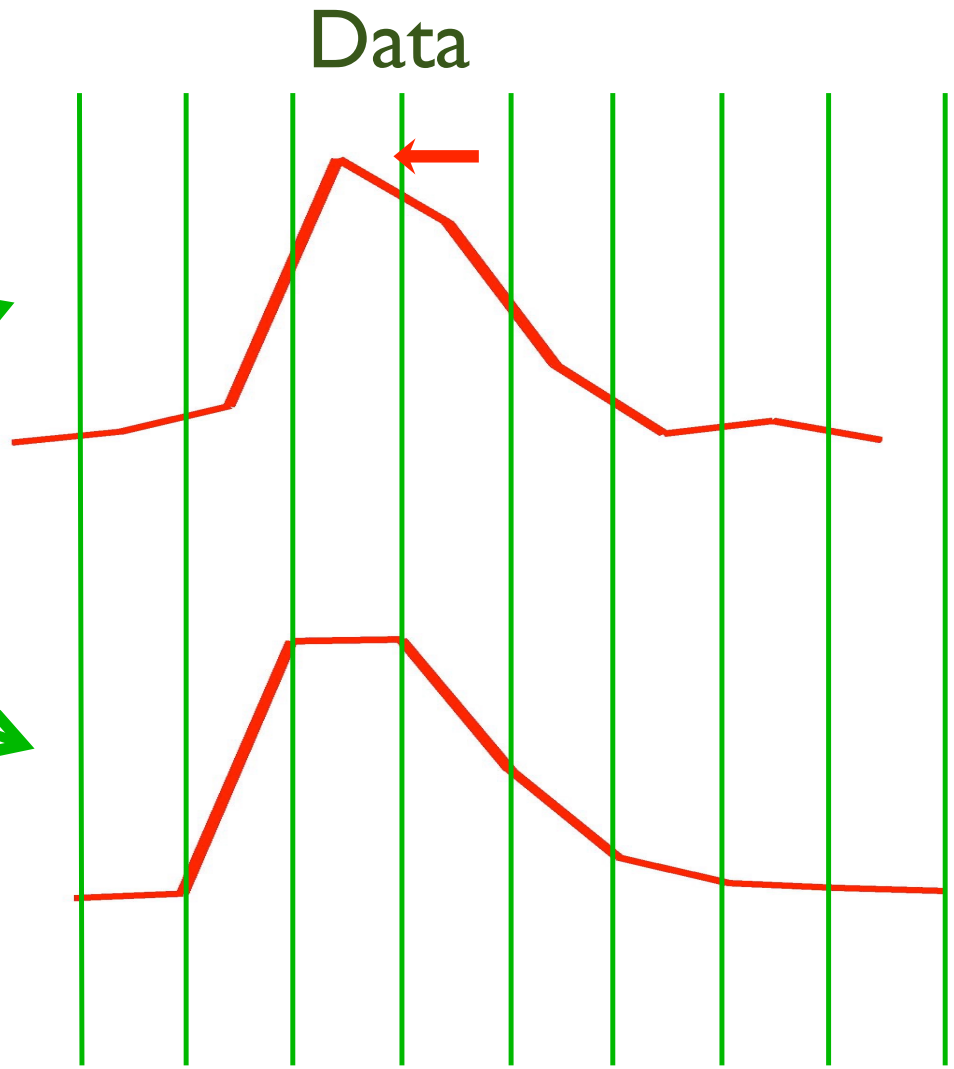
Slice Timing

Can get consistency by shifting the ***data***



slice 10

slice 9

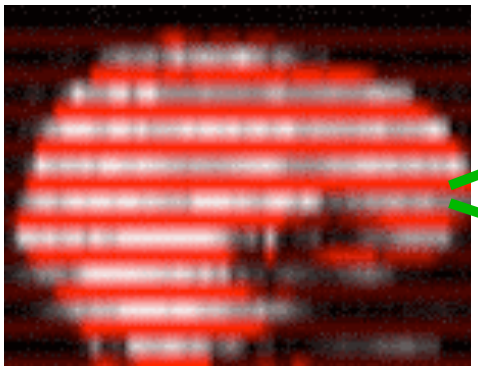


Slice 9 acquired 1.5 secs after slice 10

acquisition timing (TRs)

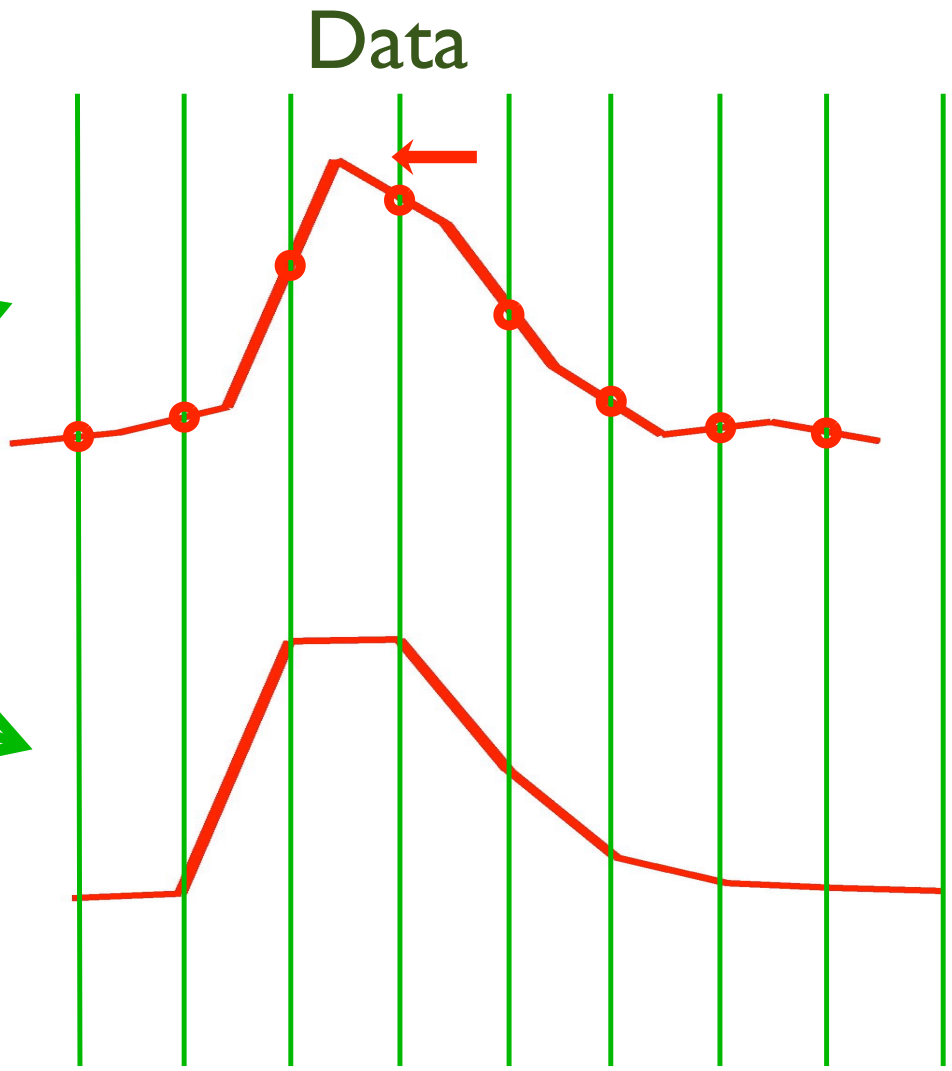
Slice Timing

... and then interpolating the data = *slice timing correction*



slice 10

slice 9



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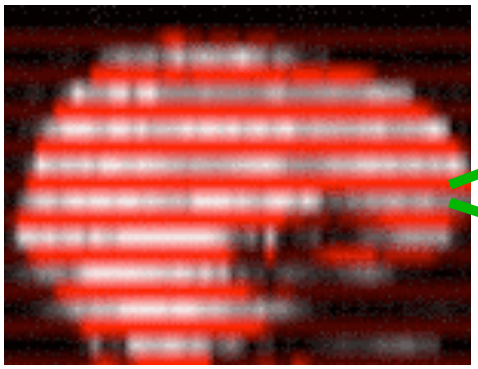
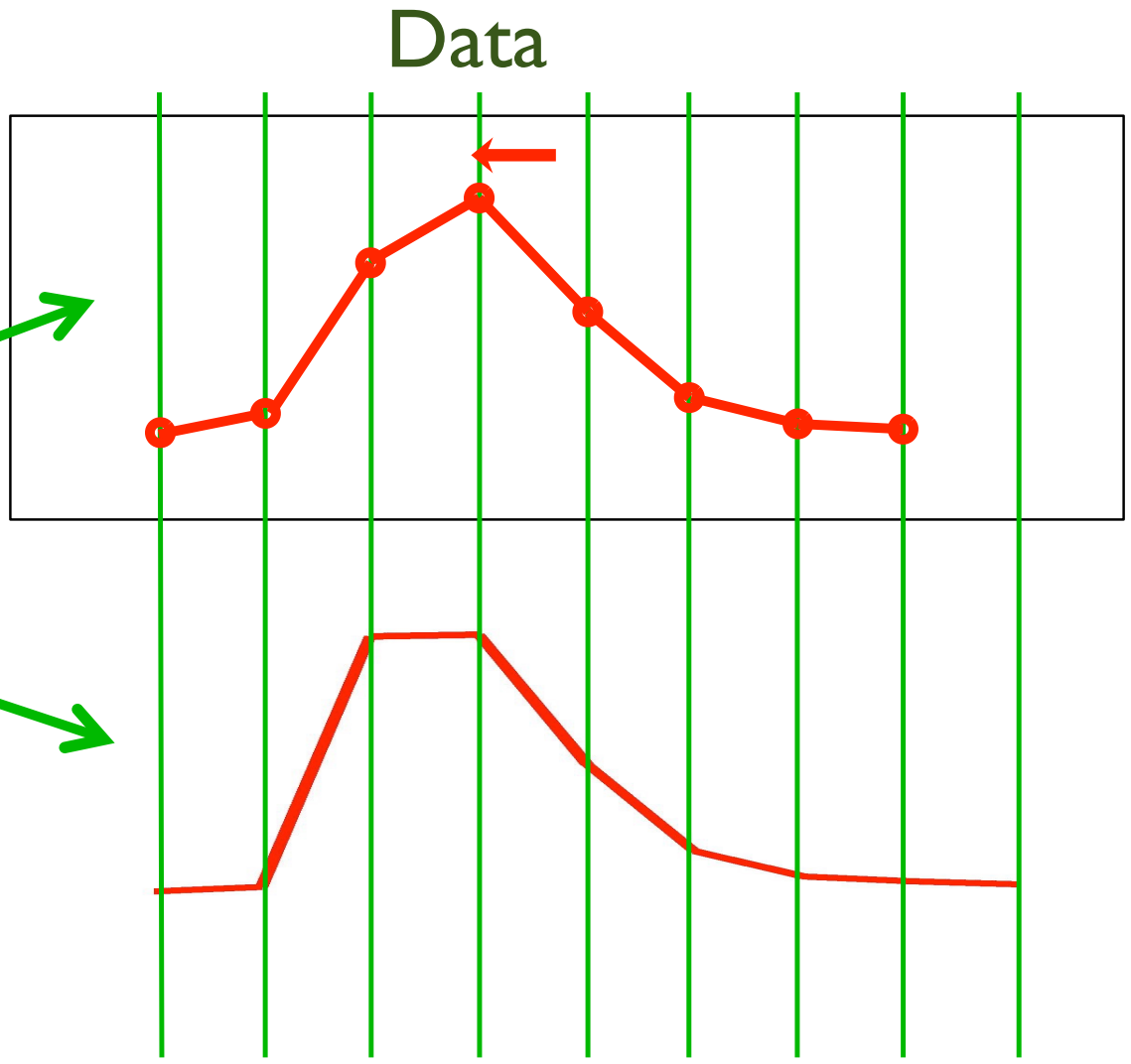
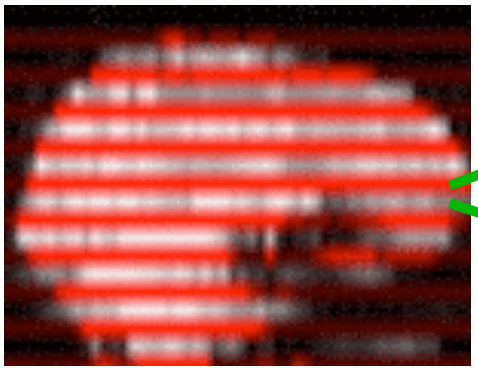




Slice 9 acquired 1.5 secs after slice 10

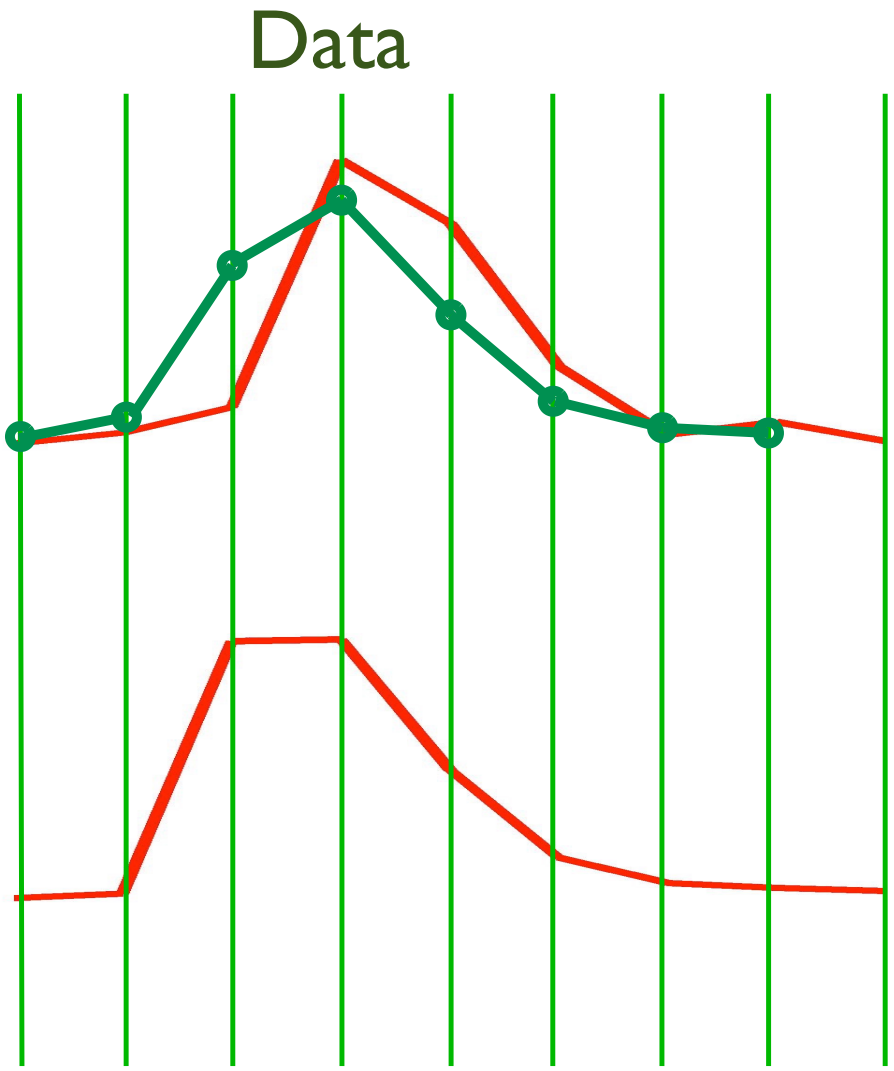
Slice Timing

... and then interpolating the data = *slice timing correction*



slice 10

slice 9

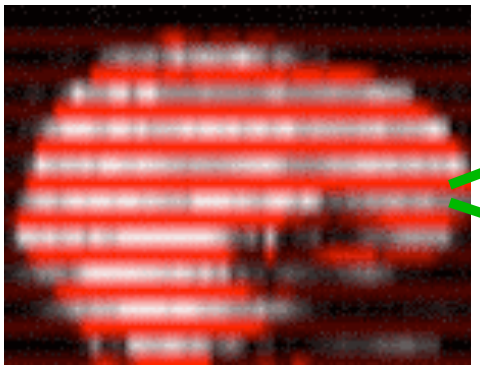


Slice 9 acquired 1.5 secs after slice 10

acquisition timing (TRs)

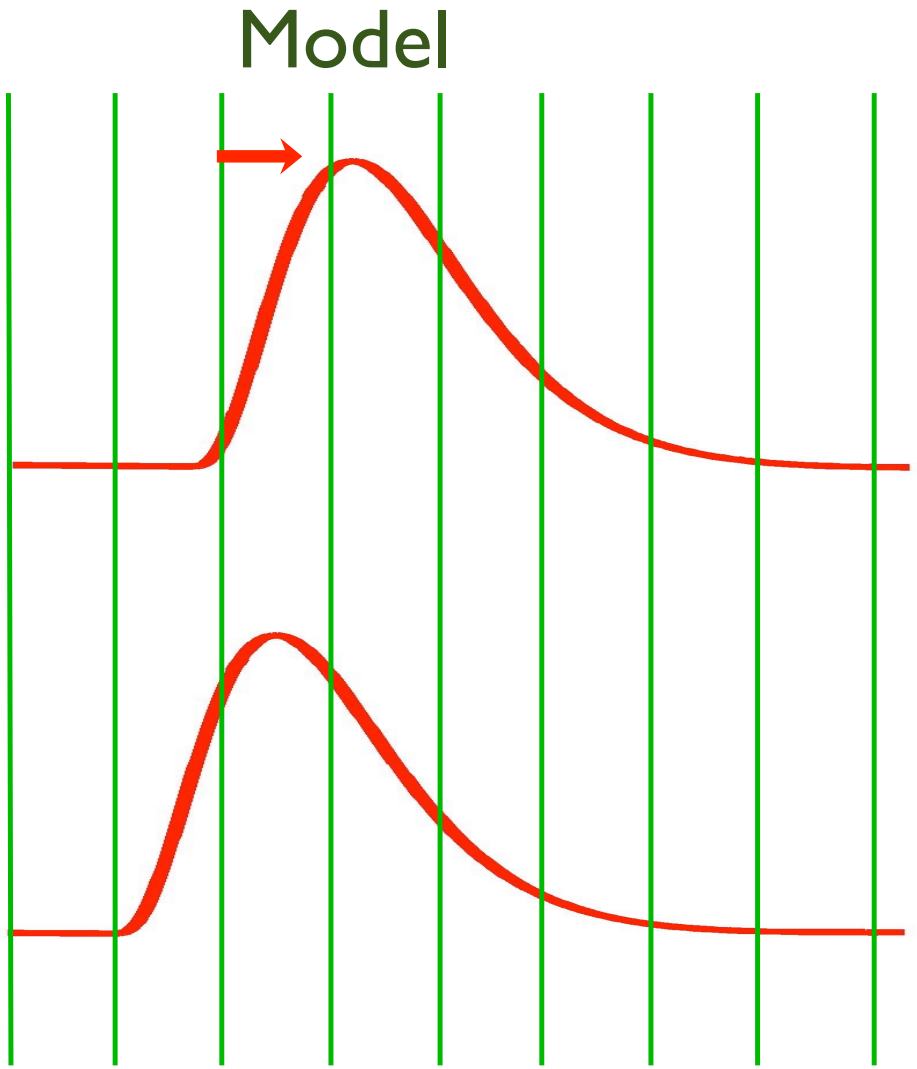
Slice Timing

Alternatively, can get consistency by shifting the *model*



slice 10

slice 9



Slice 9 acquired 1.5 secs after slice 10

acquisition timing (TRs)

Slice Timing

One way to shift the model is to use the ***temporal derivative in the GLM***

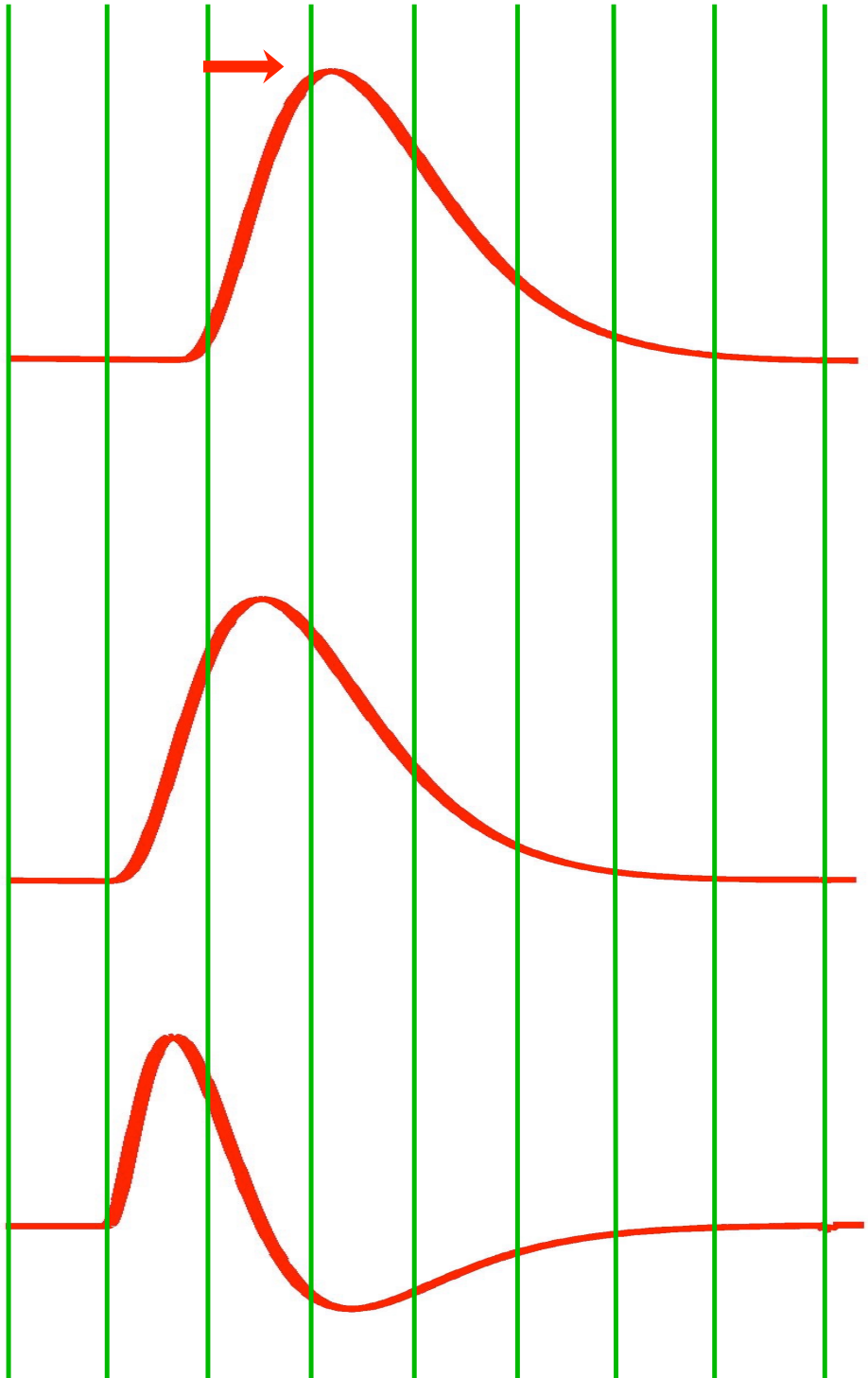
Shifted Model

=

Original Model

-

Temporal Derivative



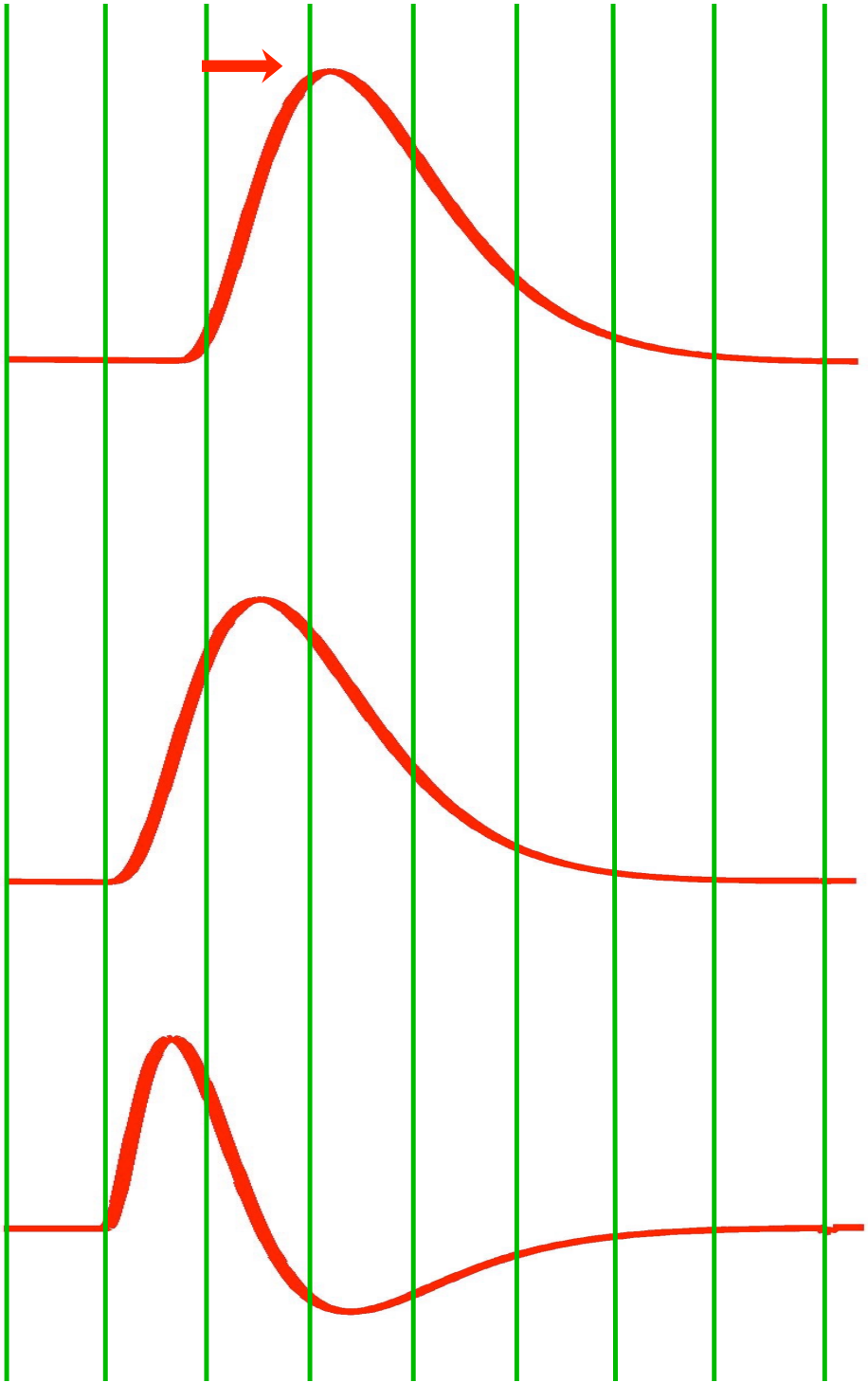
ased on
ylor approx:
$(t+a) = m(t) + a.m'(t)$

Slice Timing

hifting the model can also
ccount for variations in
he HRF delay

- as the HRF is known to vary between subjects, sessions, etc.

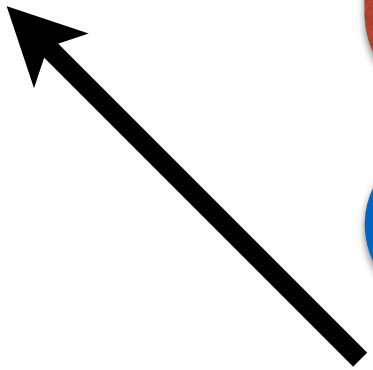
This is an alternative to slice timing correction



Standard Pre-Processing Pipeline

Task-fMRI *(GLM-based)*

- Done just before higher-level analysis
- Non-linear registration to MNI152 by default



Motion Correction

Distortion Correction

Spatial Smoothing

Temporal Filtering

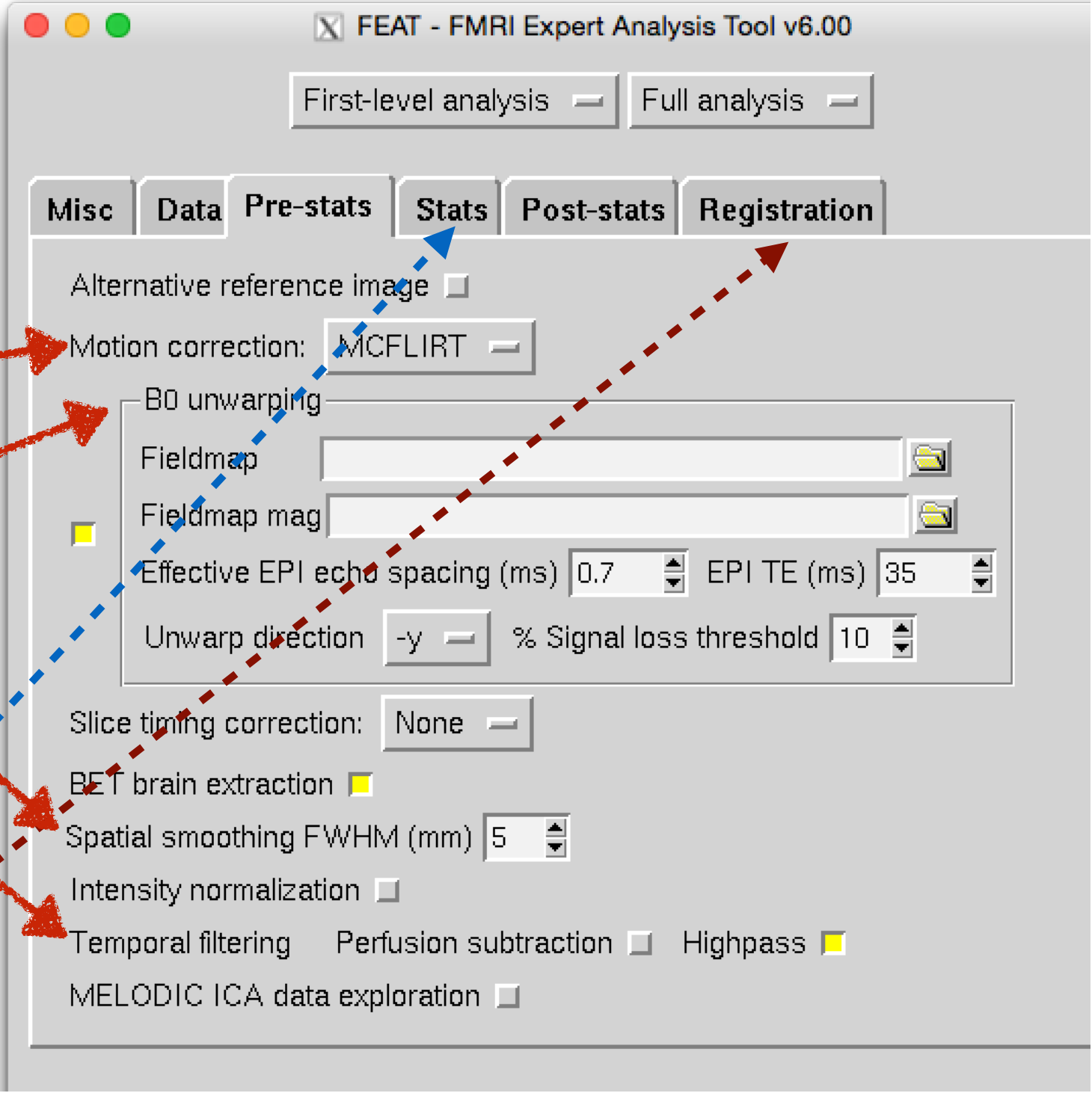
GLM

Resampling to

Standard Pre-Processing Pipeline

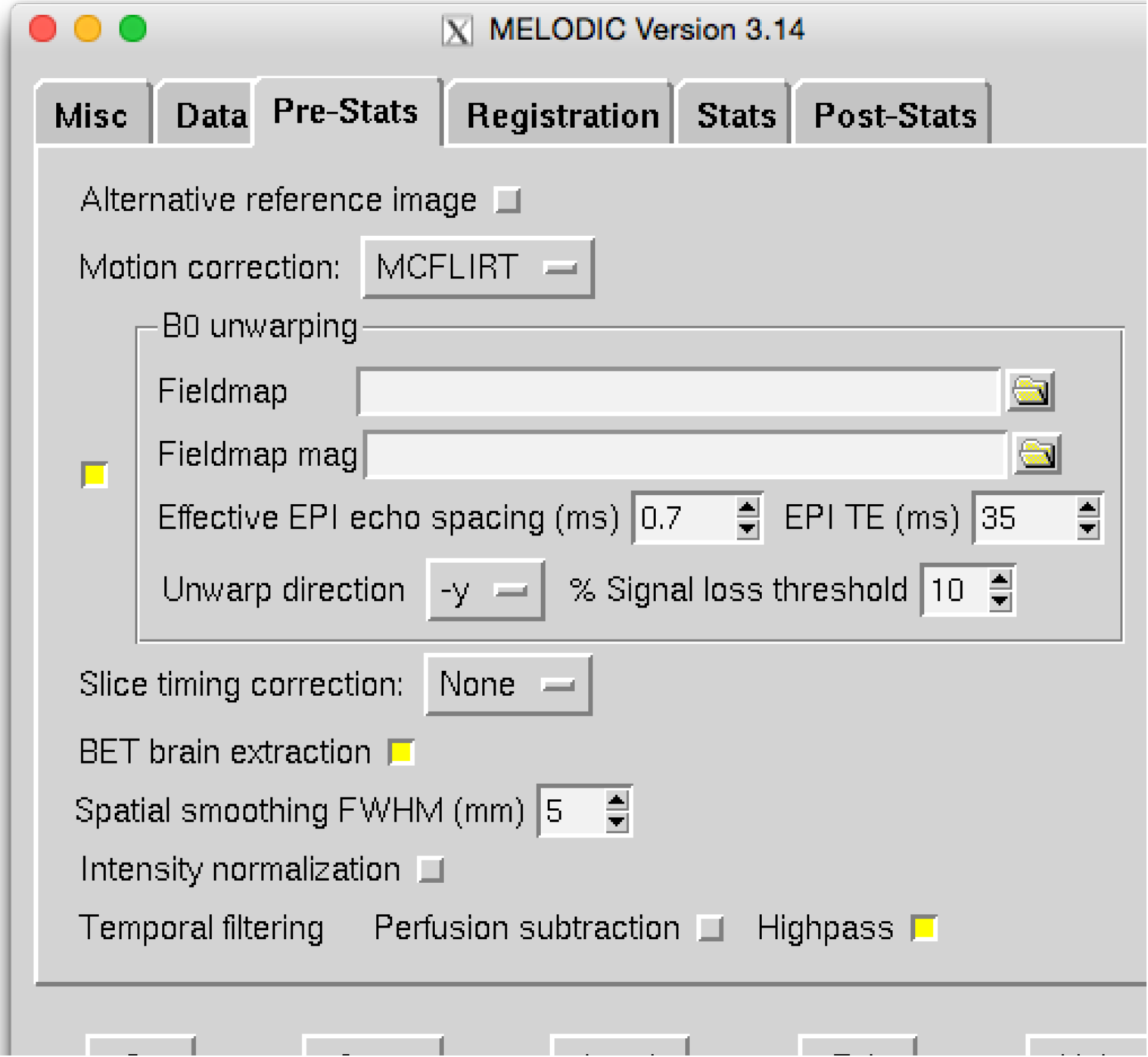
Task-fMRI
(GLM-based)

- Motion Correction
- Distortion Correction
- Spatial Smoothing
- Temporal Filtering
- **GLM**
- Resampling to Standard Space



Standard Pre-Processing Pipeline

Resting-State fMRI *(ICA-based)*



Standard Pre-Processing Pipeline

Resting-State fMRI
(ICA-based)

- Motion Correction
- Distortion Correction
- Temporal Filtering
- Spatial Smoothing
- ICA-Cleanup
- Resampling to Standard Space

Standard Pre-Processing Pipeline

Resting-State fMRI *(ICA-based)*

- Highpass only
- Cutoff around 100-200 sec = 0.005-0.01 Hz
- There is still some useful power in high frequencies, so these are kept

Motion Correction

Distortion Correction

Temporal Filtering

Spatial Smoothing

ICA-Cleanup

Resampling to Standard Space

Standard Pre-Processing Pipeline

Resting-State fMRI *(ICA-based)*

- Motion Correction
- Distortion Correction
- Temporal Filtering
- Spatial Smoothing
- ICA-Cleanup
- Resampling to Standard Space

- Minimal amount recommended
- On high quality data can avoid smoothing completely

Standard Pre-Processing Pipeline

Resting-State fMRI *(ICA-based)*

- Individual subject ICA used to split data into noise and signal components
- Automatic and manual classification options *(see later)*
- Aggressive or soft cleanup options

Motion Correction

Distortion Correction

Temporal Filtering

Spatial Smoothing

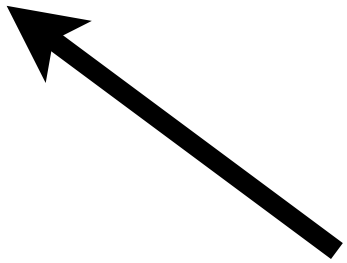
ICA-Cleanup

Resampling to Standard Space

Standard Pre-Processing Pipeline

Resting-State fMRI *(ICA-based)*

- Done before group analysis
- Non-linear registration to MNI152 by default
- Resampled in lower-res (e.g. 4mm)



Motion Correction

Distortion Correction

Temporal Filtering

Spatial Smoothing

ICA-Cleanup

Resampling to Standard Space

Standard Pre-Processing Pipeline

Resting-State fMRI *(ICA-based)*

Note:

- in FSL slice-timing-correction usually skipped as low frequency signals drive correlations

Motion Correction

Distortion Correction

Temporal Filtering

Spatial Smoothing

ICA-Cleanup

Resampling to Standard Space

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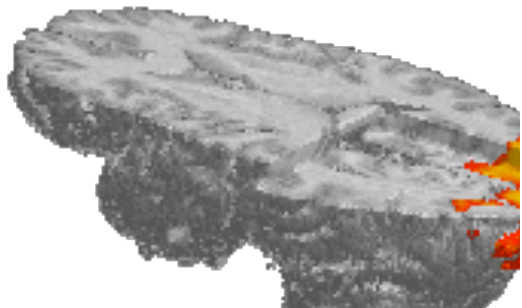


HCP Pipeline

Web Page Output

FEAT Report

/Users/mark/presentations/Graduate/MT08/Analysis/fmri.feat
Finished at Fri 16 Oct 2009 10:14:45 BST

Pre-stats - Stats - Post-stats - Registration - Log

e-stats

ysis methods

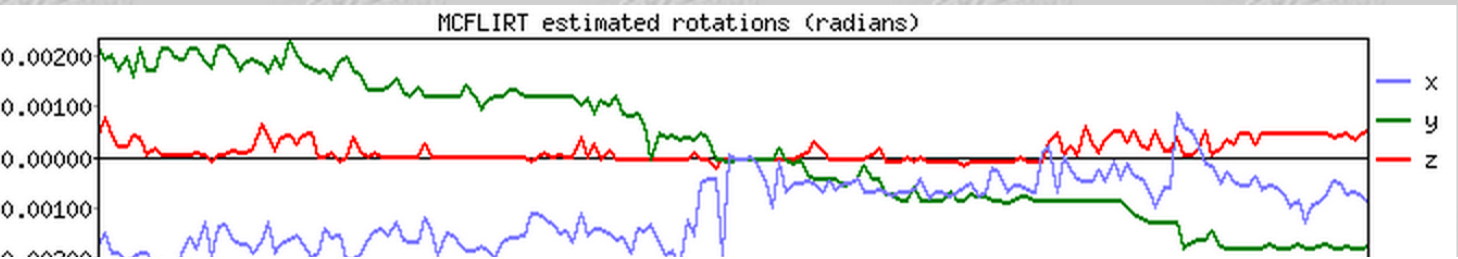
l data processing was carried out using FEAT (FMRI Expert Analysis Tool) Version 5.98, part of FSL (FMRIB's Software Library, .fmrib.ox.ac.uk/fsl). The following pre-statistics processing was applied; motion correction using MCFLIRT [Jenkinson 2002]; non-brain removal usi [Smith 2002]; spatial smoothing using a Gaussian kernel of FWHM 5mm; grand-mean intensity normalisation of the entire 4D dataset by a single plicative factor; highpass temporal filtering (Gaussian-weighted least-squares straight line fitting, with sigma=90.0s).

rences

kinson 2002] M. Jenkinson and P. Bannister and M. Brady and S. Smith. Improved optimisation for the robust and accurate linear registration and on correction of brain images. NeuroImage 17:2(825-841) 2002.
th 2002] S. Smith. Fast Robust Automated Brain Extraction. Human Brain Mapping 17:3(143-155) 2002.

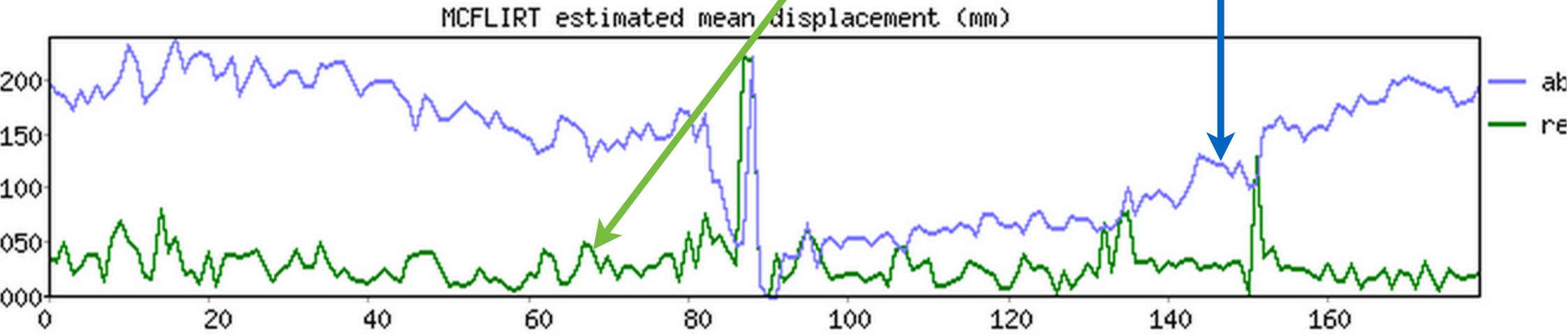
LIRT Motion correction

n displacements: absolute=0.13mm, relative=0.03mm



Web Page Output: Motion

Summary of total motion (relative and absolute)

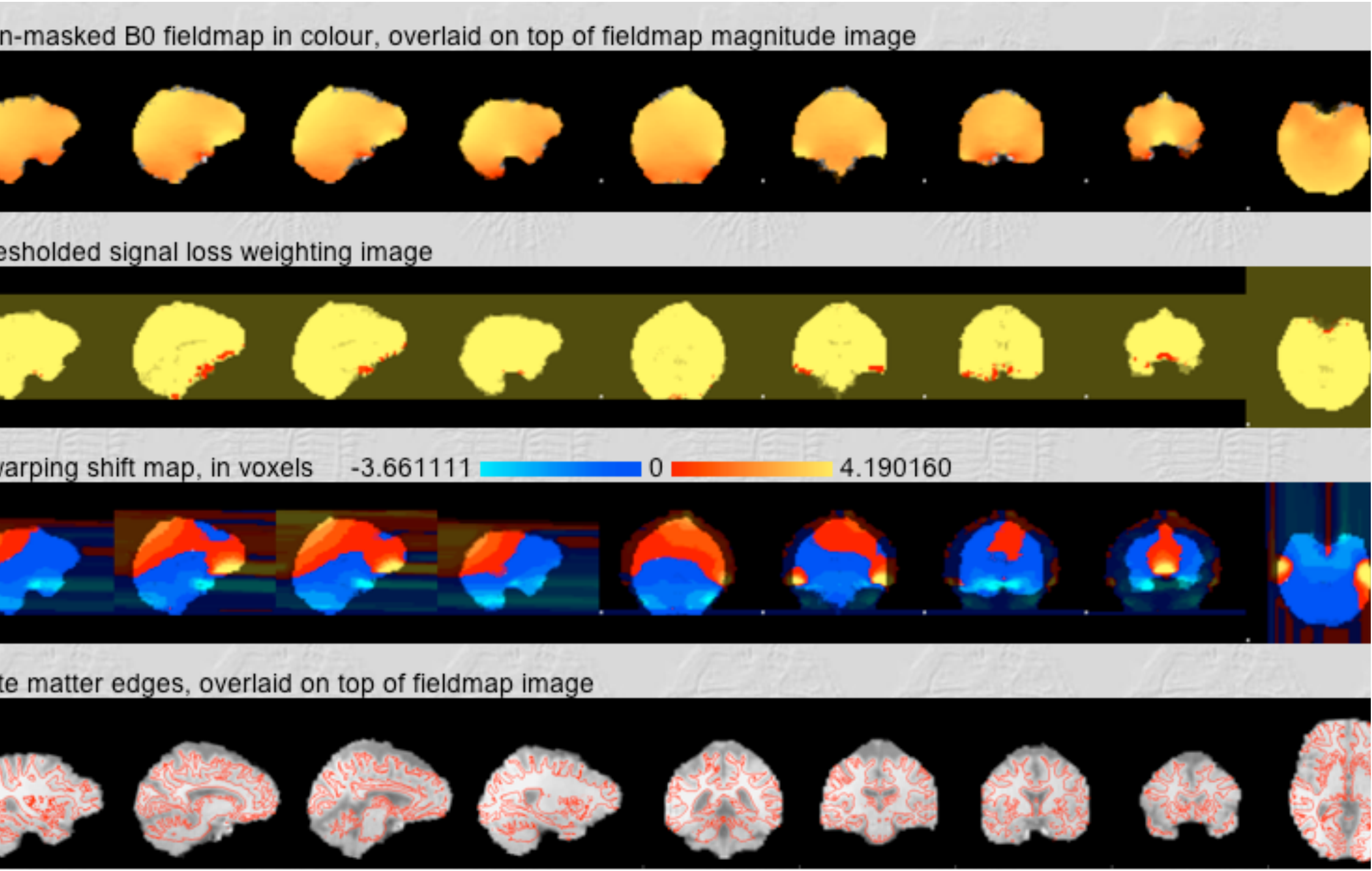


Relative = time point to next time point - shows jumps

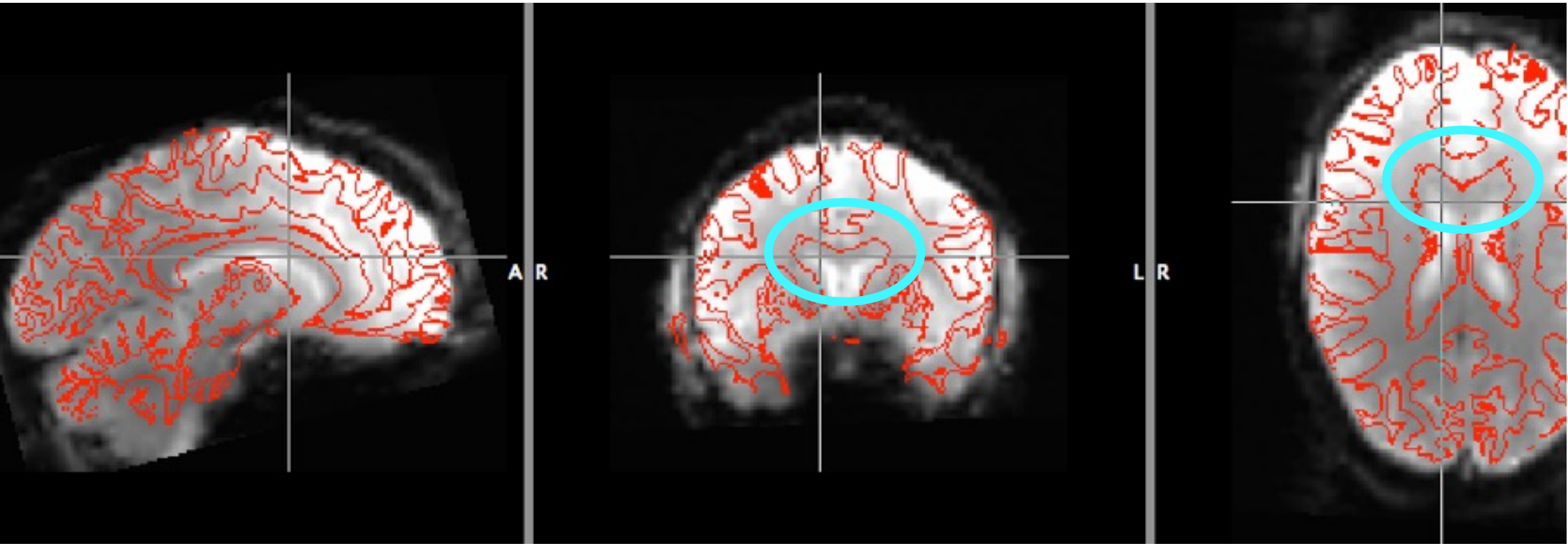
Absolute = time point to reference - shows jumps & drifts

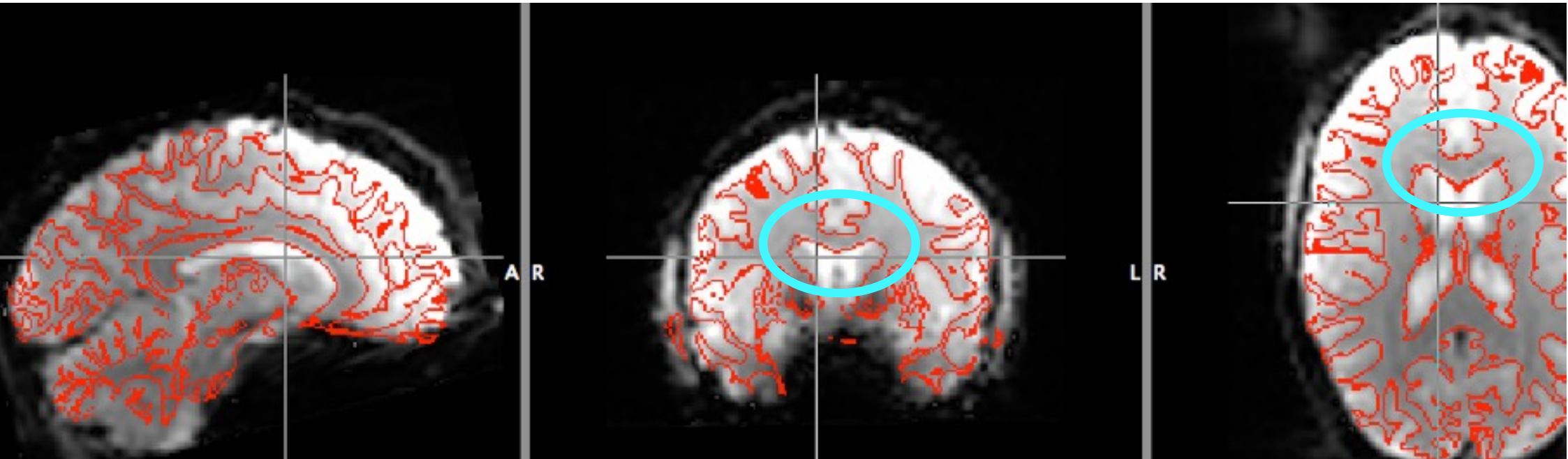
Note that large jumps are more serious than slower drifts,

Web Page Output: Distortion

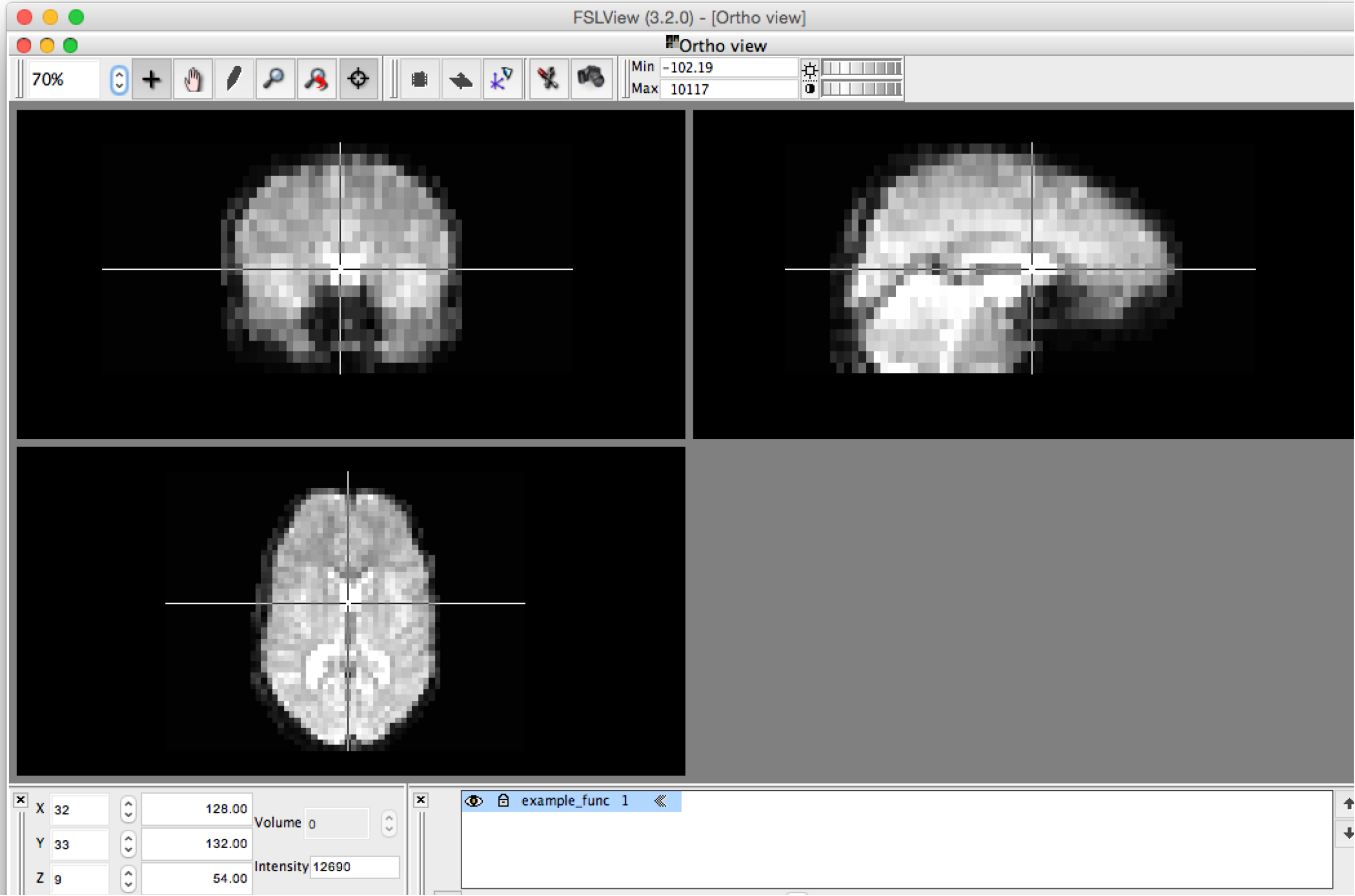


Web Page Output: Distortion

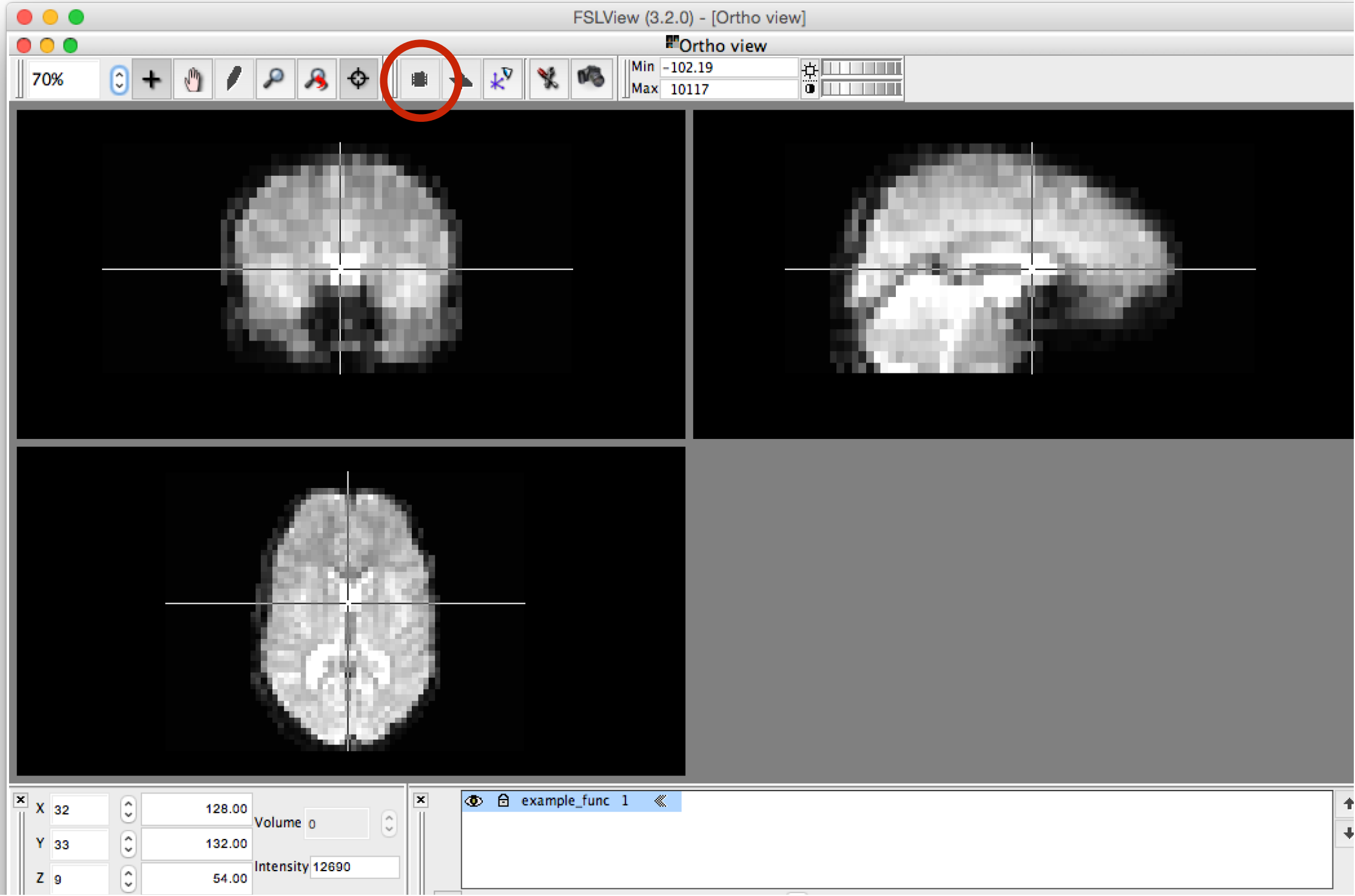




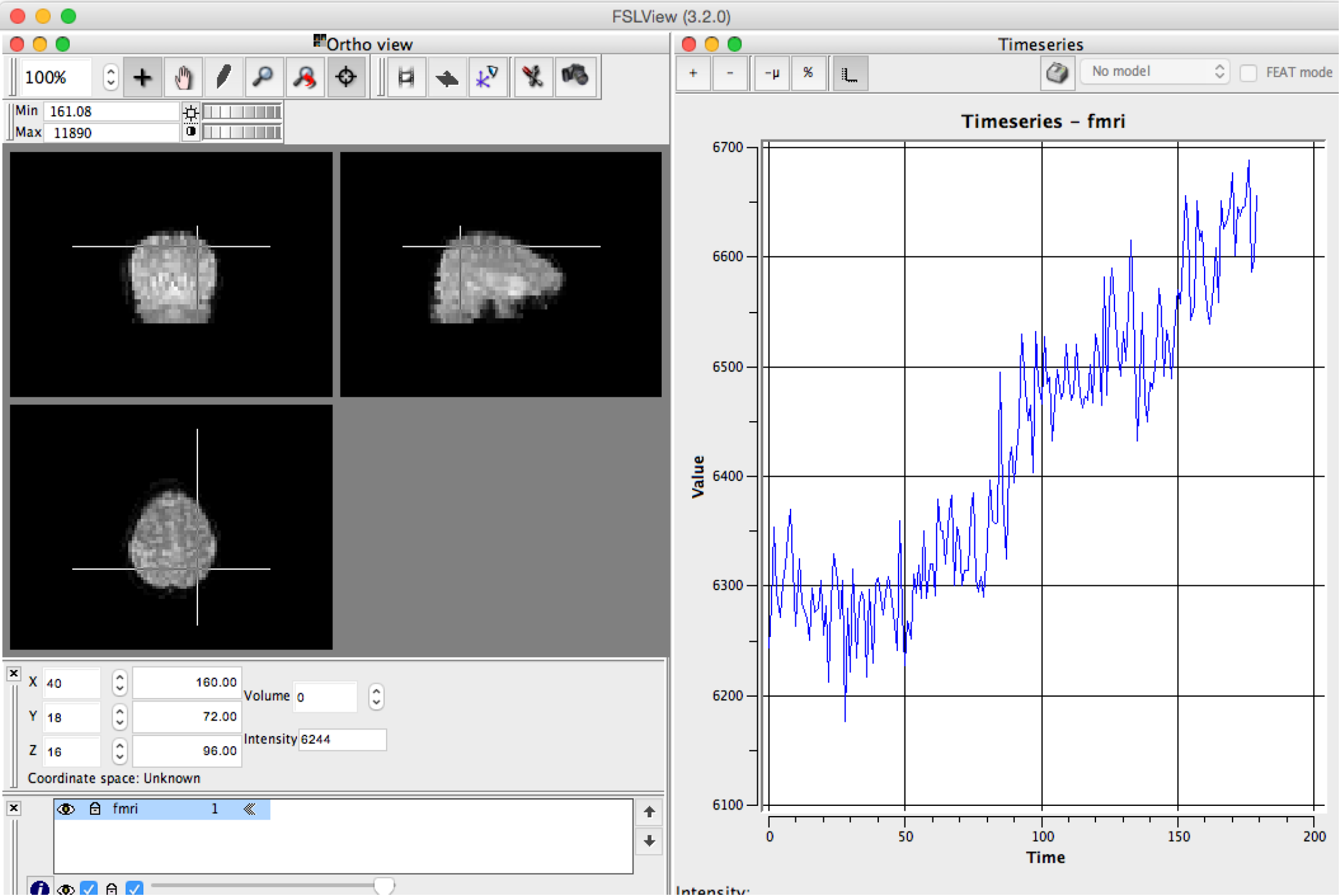
FSLView


FSLView (3.2.0) - [Ortho view]
Ortho view
70%
Min -102.19
Max 10117
X 32
128.00
Volume 0
Y 33
132.00
Intensity 12690
Z 9
54.00
example_func 1

FSLView: Movie Mode



FSLView: Timeseries



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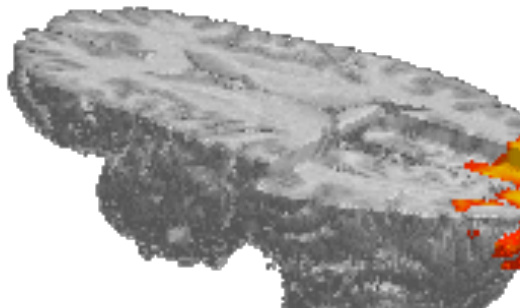


HCP Pipeline

Options in Pre-Processing

The "standard" pre-processing is not the only option available in FSL

It is not always the best approach

Other options are better with different data and subjects

Alternatives include:

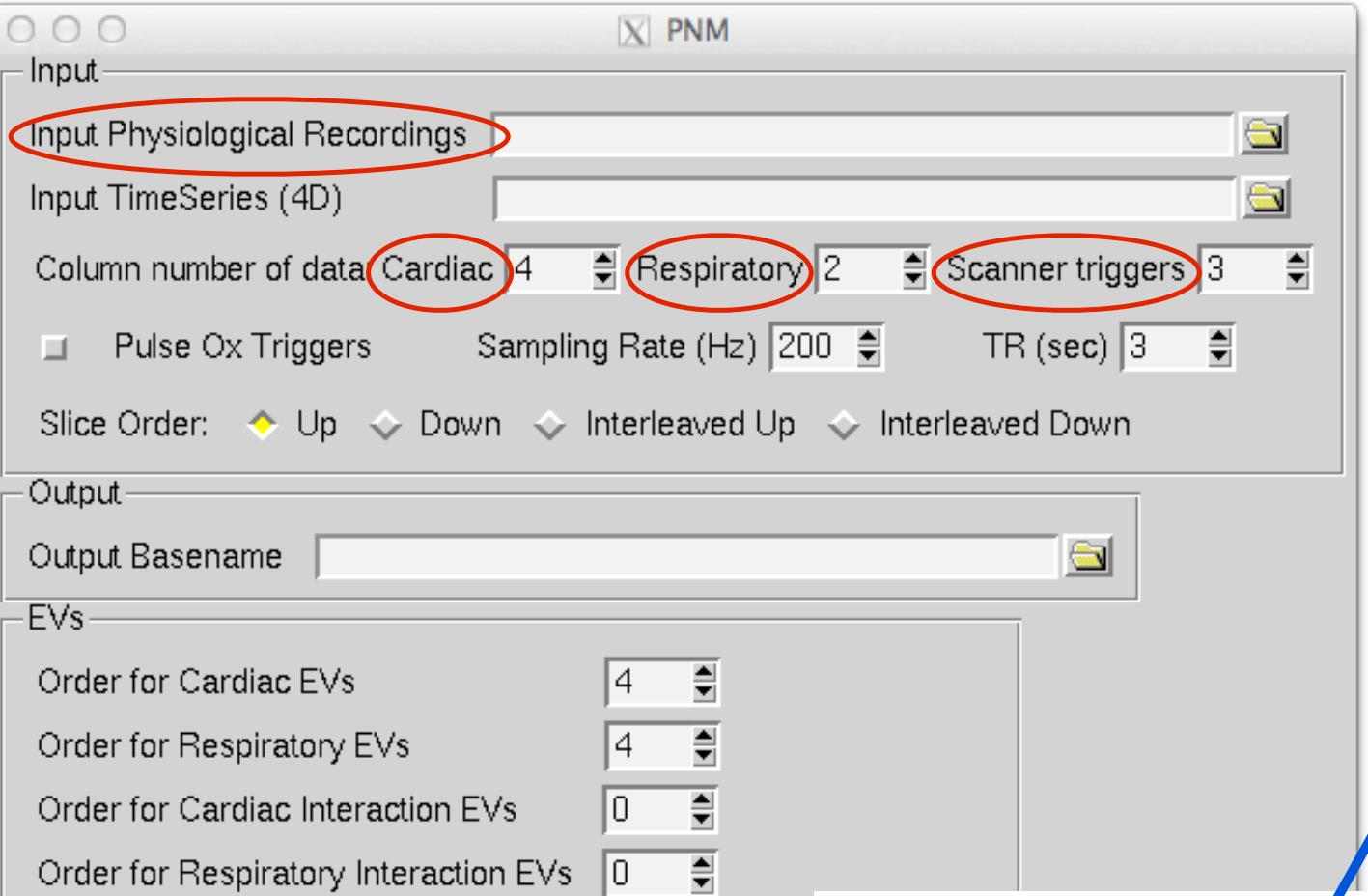
- slice-timing-correction
- lowpass filtering (outside of GUI)
- other reference image for motion/distortion correction (multi-band often needs this)

Also have other cleanup options (using GLM or ICA):

- physiological noise modelling
- confound regressors (e.g. motion parameters)
- motion-outlier detection (fsl_motion_outliers)

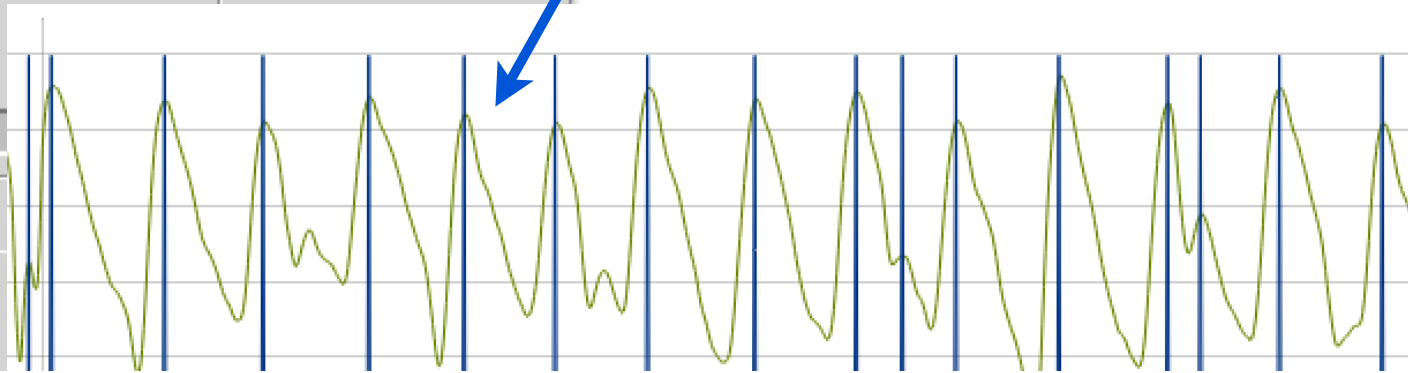
Physiological Noise Model

PNM (GUI)



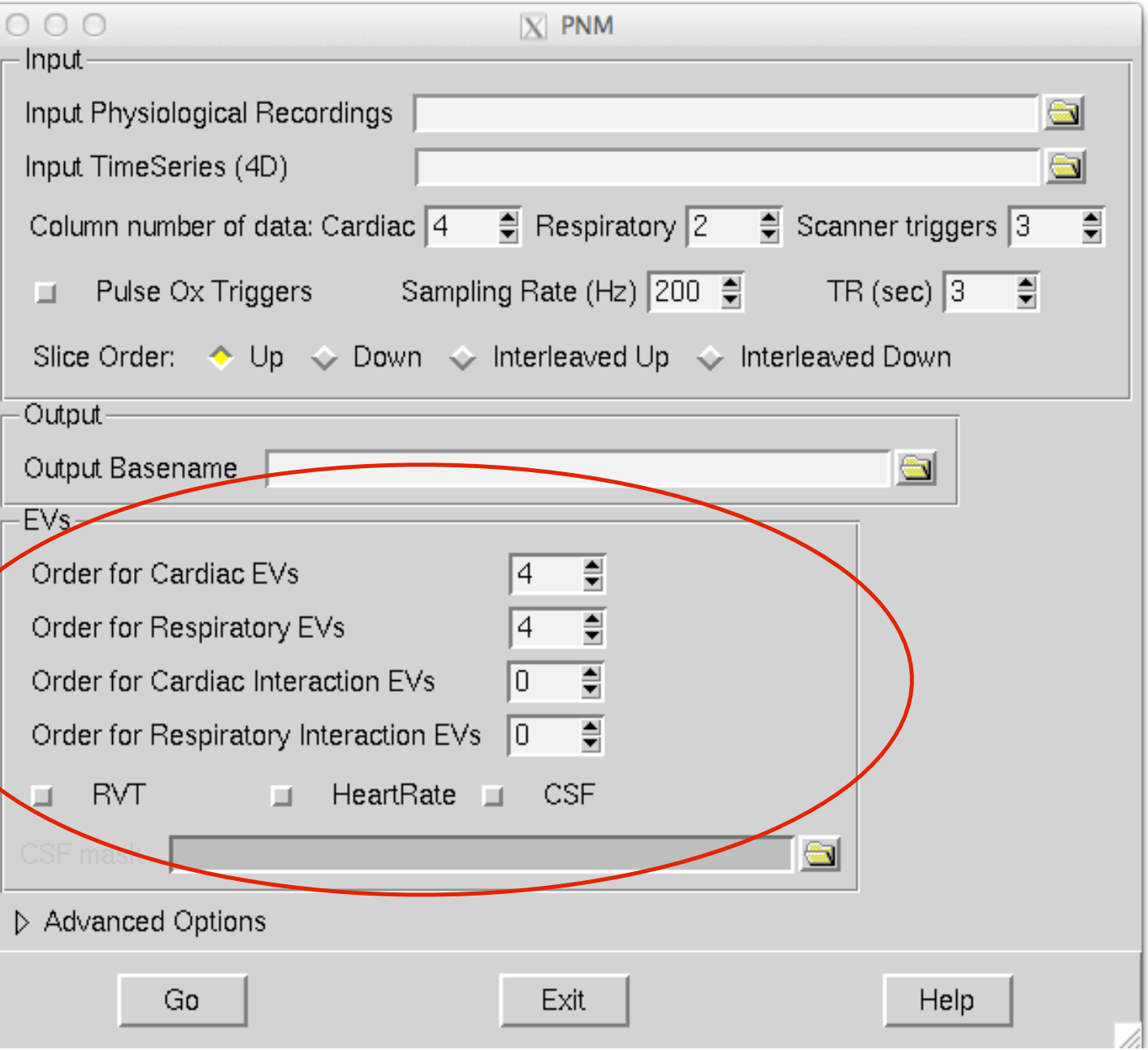
Requires **text file with physiological recordin** (cardiac, respiratory, triggers)

Peak detection in physiological trace needs manual checking via webpag



Physiological Noise Model

PNM (GUI)



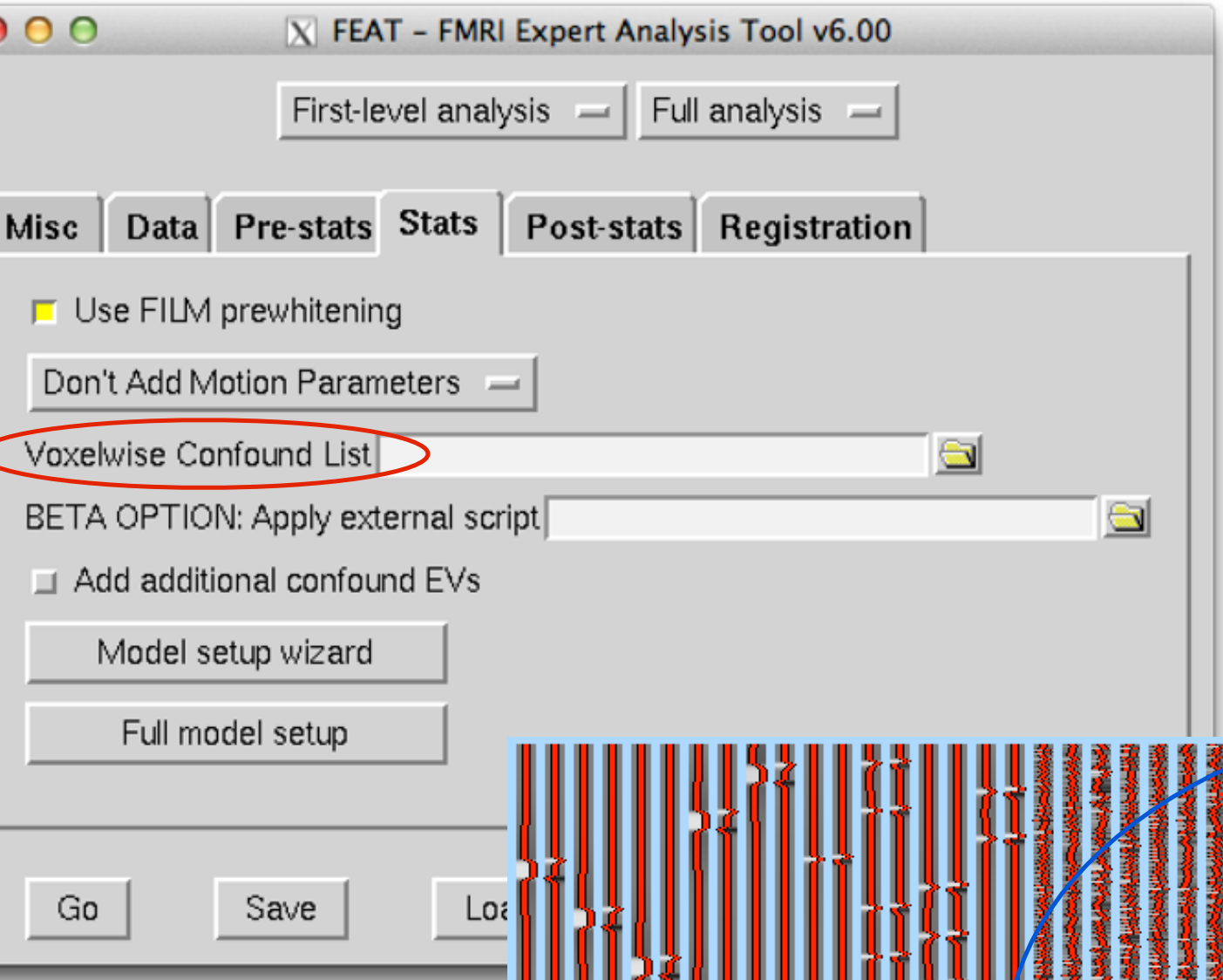
Need to specify what ty
of corrections:

- Fourier series
  (harmonics / shape)
- Interactions
  (resp x cardiac)

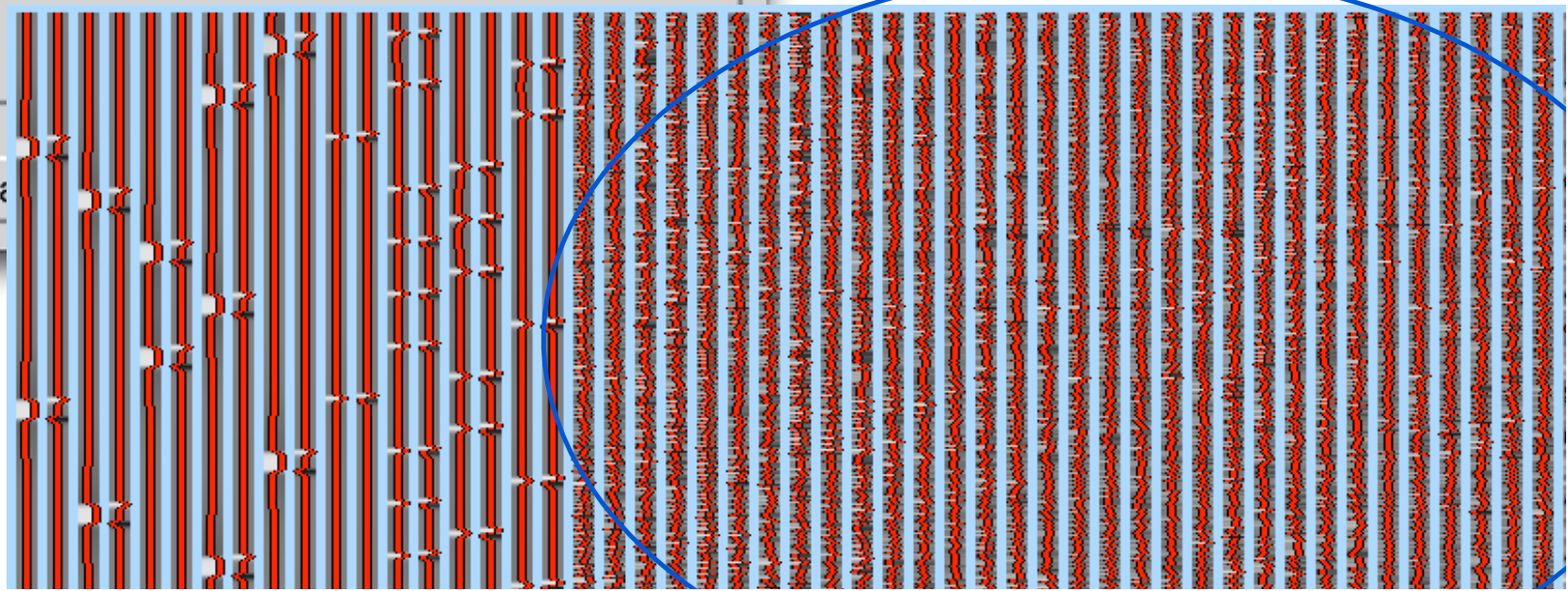
*NB: higher orders = bette
to shape, but many more
EVs and so less DOF*

- RVT
  (resp volume per tim
- HeartRate
- CSF

Physiological Noise Model: GLM

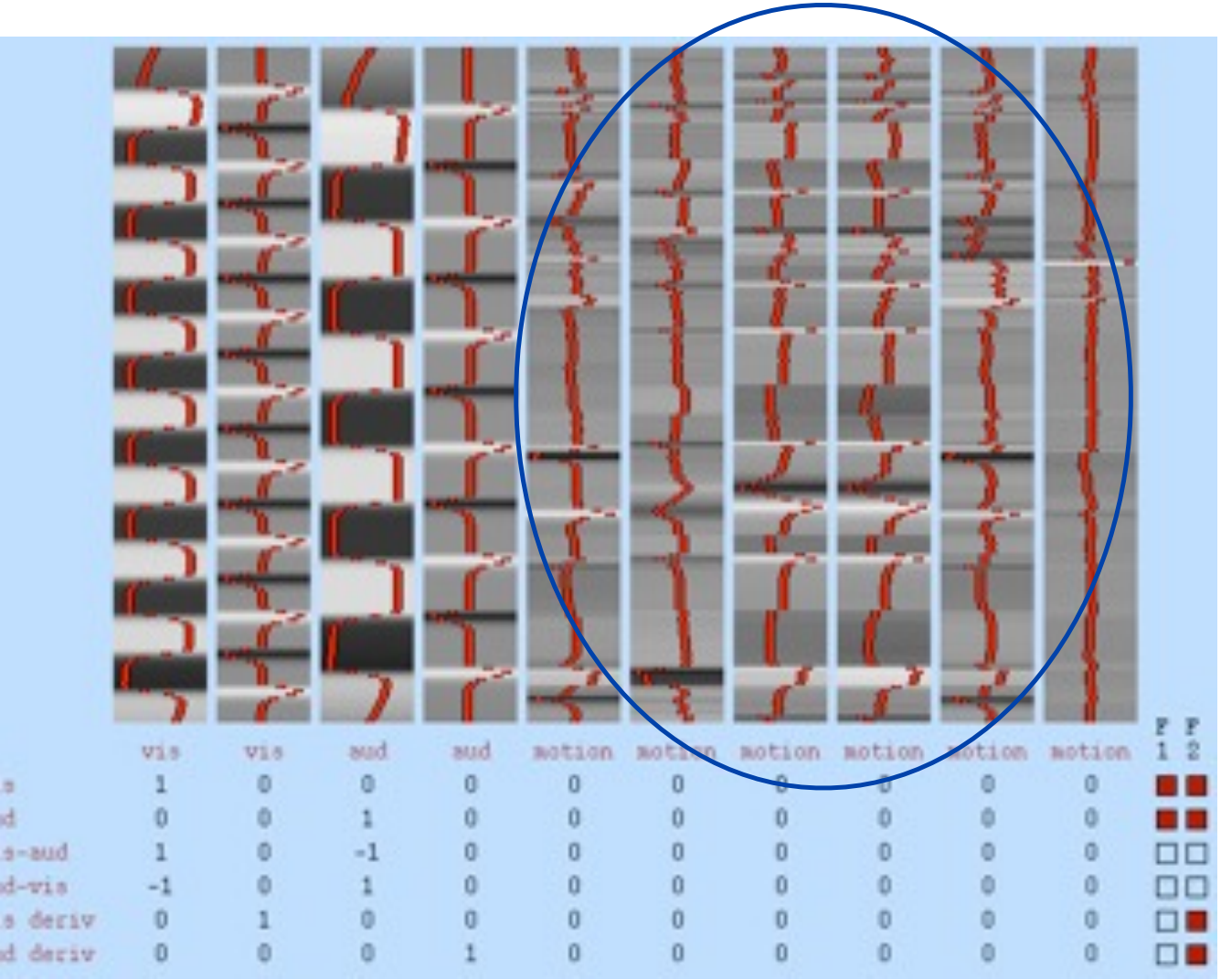


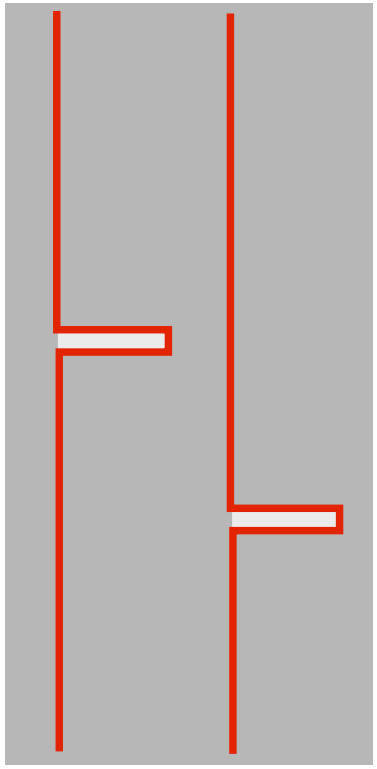
PNM GUI creates files for ***Voxelwise Confoun*** in the GLM



Motion Regressors

wo options (can be combined) both of which work within GLM





Example
2 outlie
timepoi
to remo

Motion Parameters

- use button in GUI

Motion Outliers

- uses fsl_motion_out

ICA-Based Cleanup

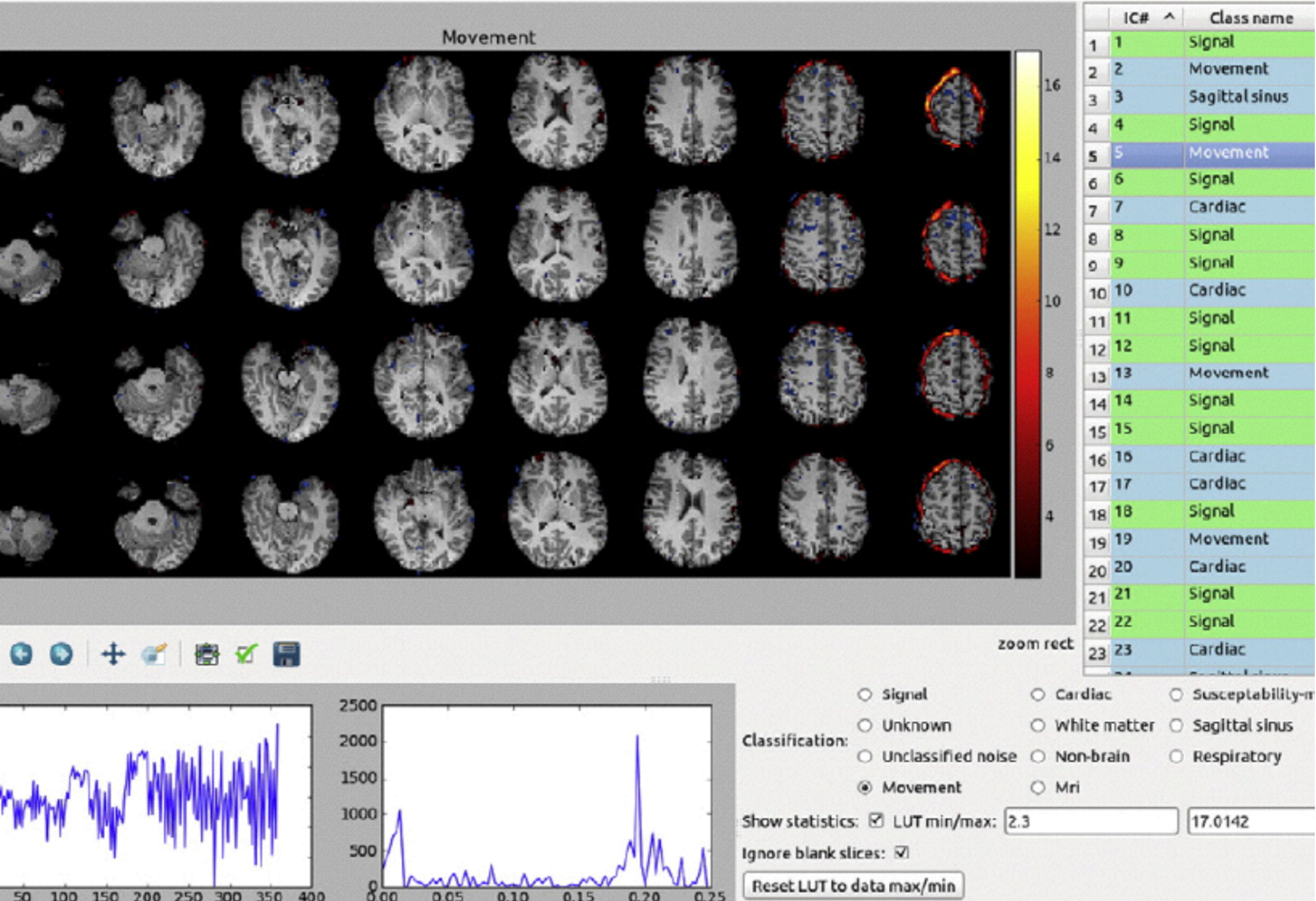
Principle is simple:

- use ICA to find components then remove ones that are considered "noise"

Can classify noisy ones in three ways:

- by hand
- FIX (fully automated and requires ***good training data***)
- AROMA (fully automated, does not need training data, bu often more conservative - *i.e.* leaves more noise)

Often the most powerful way of removing things such as motion effects and scanner artefacts



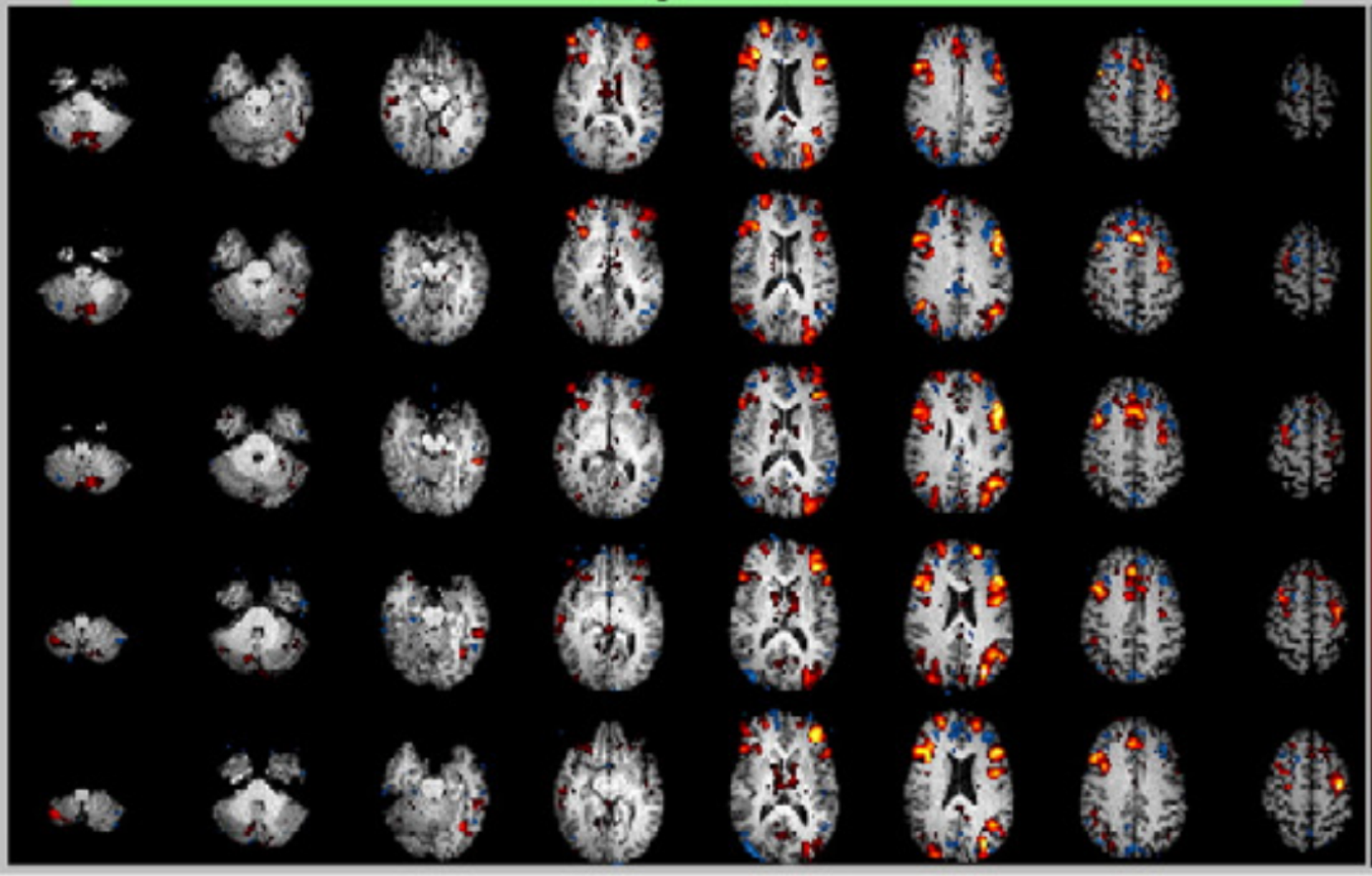
	IC#	Class name
1	1	Signal
2	2	Movement
3	3	Sagittal sinus
4	4	Signal
5	5	Movement
6	6	Signal
7	7	Cardiac
8	8	Signal
9	9	Signal
10	10	Cardiac
11	11	Signal
12	12	Signal
13	13	Movement
14	14	Signal
15	15	Signal
16	16	Cardiac
17	17	Cardiac
18	18	Signal
19	19	Movement
20	20	Cardiac
21	21	Signal
22	22	Signal
23	23	Cardiac

Classification:
- ○ Signal
- ○ Cardiac
- ○ Susceptability-r
- ○ Unknown
- ○ White matter
- ○ Sagittal sinus
- ○ Unclassified noise
- ○ Non-brain
- ○ Respiratory
- ◉ Movement
- ○ Mri

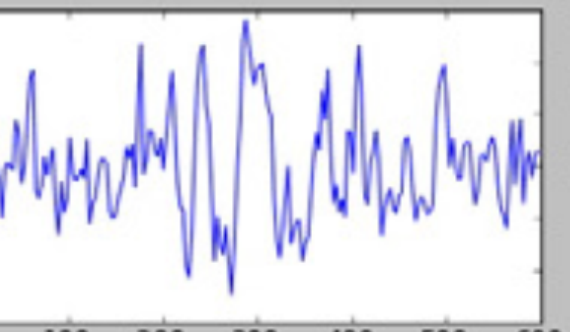
Show statistics: ☑ LUT min/max: 2.3 17.0142

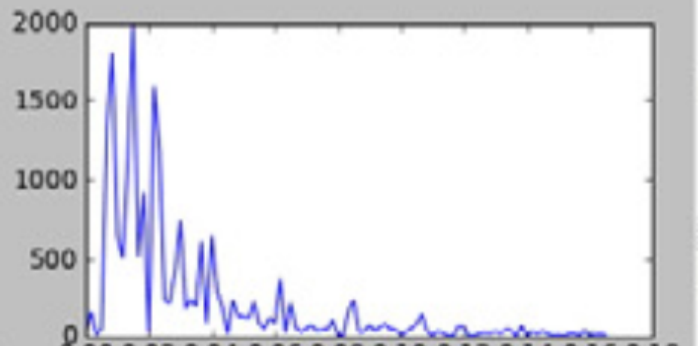
Ignore blank slices: ☑

Reset LUT to data max/min



	IC#	Class nam
1	1	Movement
2	2	Movement
3	3	Cardiac
4	4	Movement
5	5	Movement
6	6	Movement
7	7	Movement
8	8	Movement
9	9	Signal
10	10	Cardiac
11	11	Signal
12	12	Movement
13	13	Signal
14	14	Movement
15	15	Signal
16	16	Cardiac
17	17	Signal
18	18	Susceptability-
19	19	Movement
20	20	Signal
21	21	Signal
22	22	Unknown
23	23	Cardiac





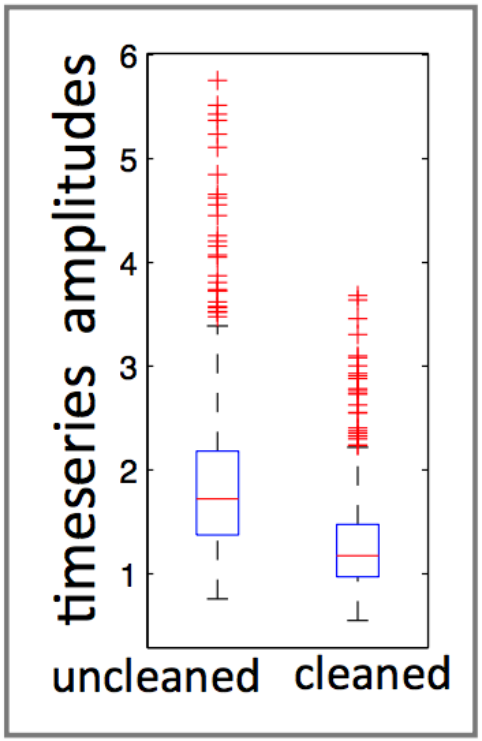
Classification: ◉ Signal ○ Cardiac ○ Susceptability ○ Unknown ○ White matter ○ Sagittal sinus ○ Unclassified noise ○ Non-brain ○ Respiratory ○ Movement ○ Mri

Show statistics: ☑ LUT min/max: 2.3 14.8154

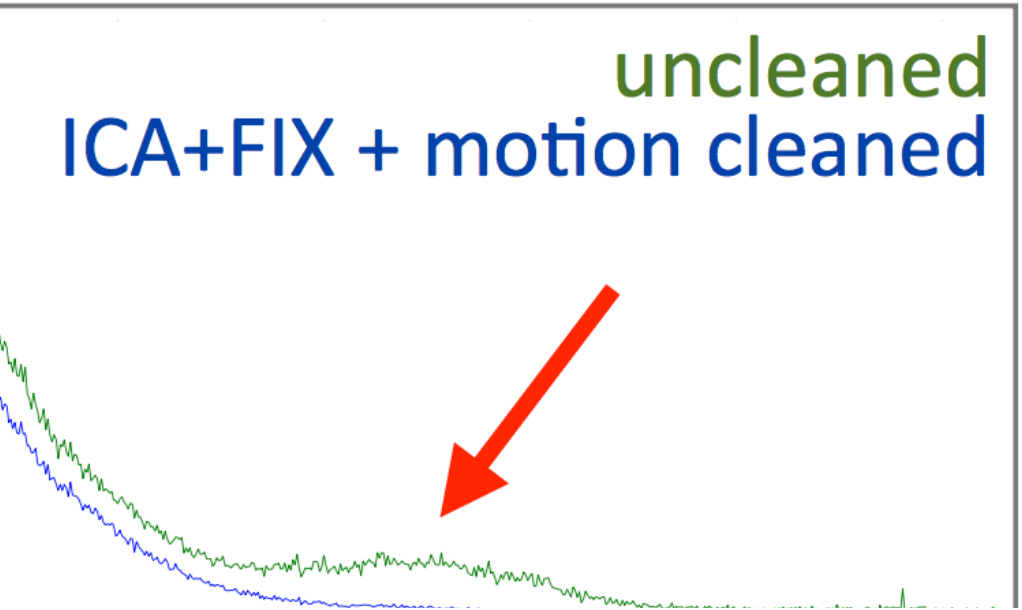
Ignore blank slices: ☑

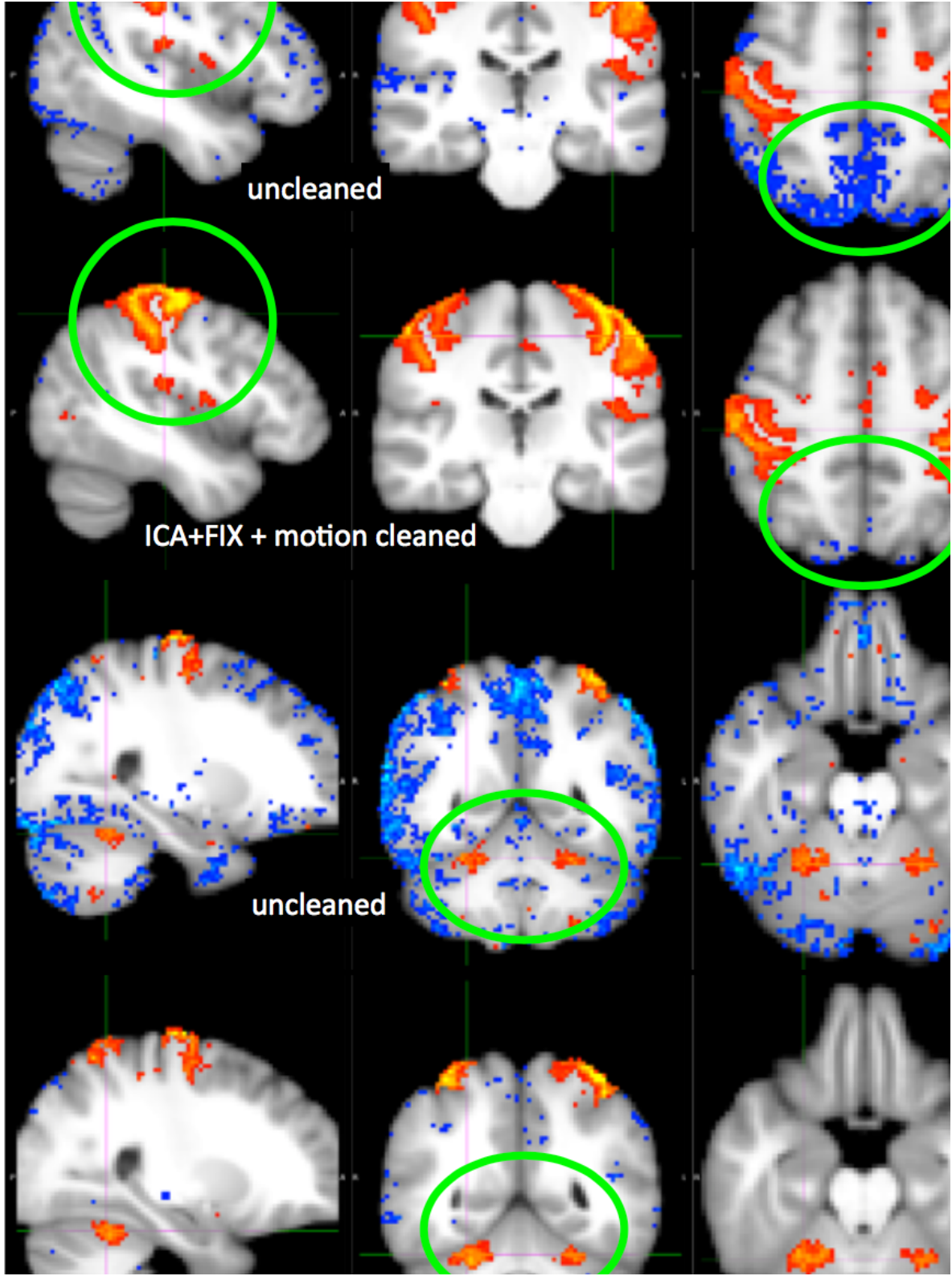
Reset LUT to data max/min

PROJECT



temporal power spectra





FSL Pre-Processing Pipeline

Standard pre-processing:

- Task fMRI
- Resting-state fMRI

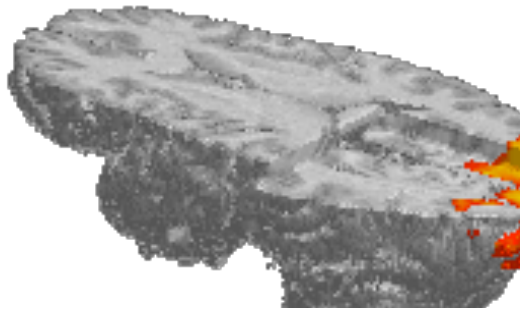
Quality Assessment

Alternatives

- Other pre-processing options
- GLM-based or ICA-based "pre-processing"

Complications

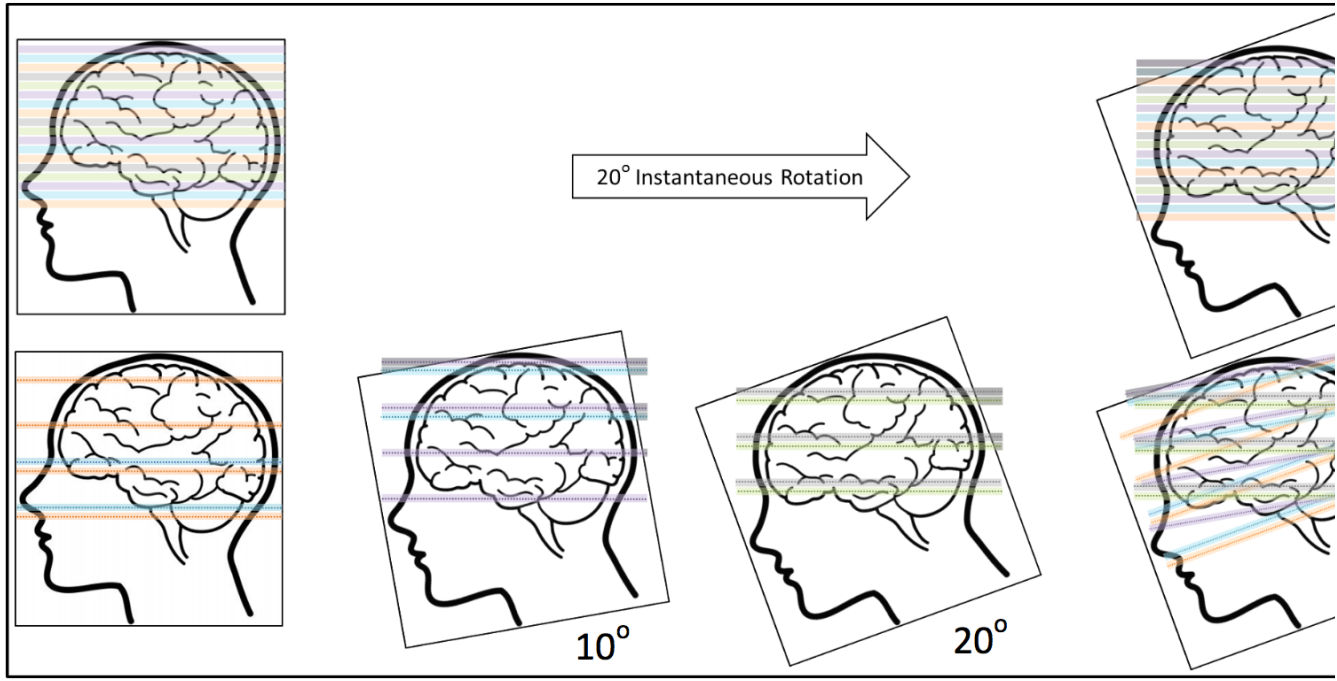
- Spatial and temporal interactions
- HRF variation



HCP Pipeline

Spatial and Temporal Interactions

quiring a slice at a time
ds to complicated
eractions between
otion and slice-timing.



Ray R

Motion correction moves signals between slices (6 DOF)
Slice-timing-correction assumes spatial alignment of voxels
Spatial smoothing mixes slices (problem for derivative modelling)
HRF delays typically vary (problem for slice-timing-correction)

- These aspects are all inter-related

Interleaved sequences (incl. multi-band) are harder to correct
"Best" answer doesn't yet exist (i.e. integrating all together)
Choice between current options depends on data and subjects

FSL Pre-Processing Pipeline

Standard pre-processing:

- Task fMRI
- Resting-state fMRI

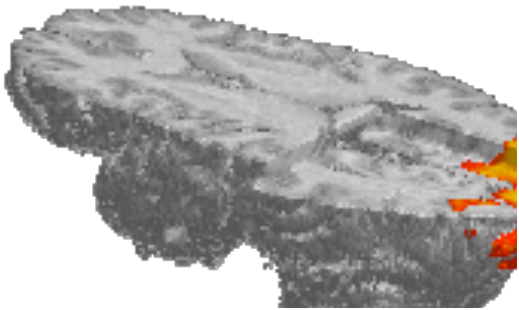
Quality Assessment

Alternatives

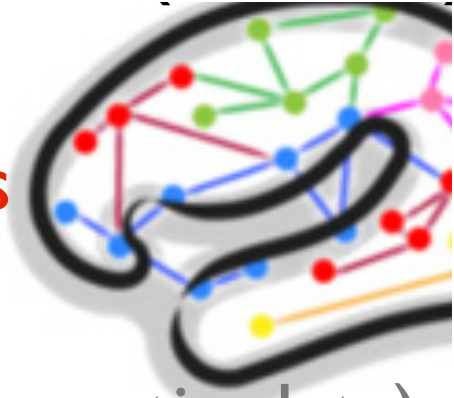
- Other pre-processing options
- GLM-based or ICA-based "pre-processing"

Complications

- Spatial and temporal interactions
- HRF variation



HCP Pipeline



0 million, 5-year project

- Characterize connectivity of healthy adult humans
- 1200 subjects:
  - 22-35 yrs in sibling/twin groups (+ behavioural/genetic data)
- Includes Structural-MRI, Task-FMRI & Resting-FMRI
- Data + network models made freely available
- Provide user-friendly informatics platform

High quality data:

- 1 hour of task-FMRI and 1 hour of Resting-FMRI
- Structural data: 0.7mm isotropic T1-w and T2-w
- FMRI data: 2mm isotropic / TR=0.72s / Multiband 8

8 institution collaboration (>70 investigators) from:

- Washington U (Van Essen) / U Minnesota (Ugurbil)
- FMRIB, Oxford / Donder Institute, Nijmegen

HCP Pipeline Overview

Pre FreeSurfer

FreeSurfer

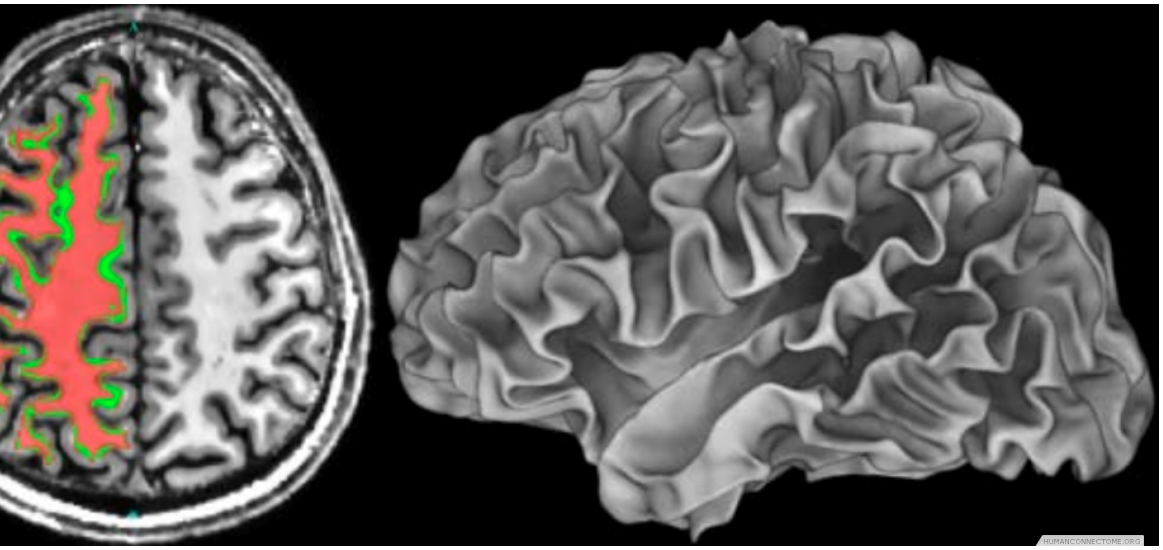
Post FreeSurfer

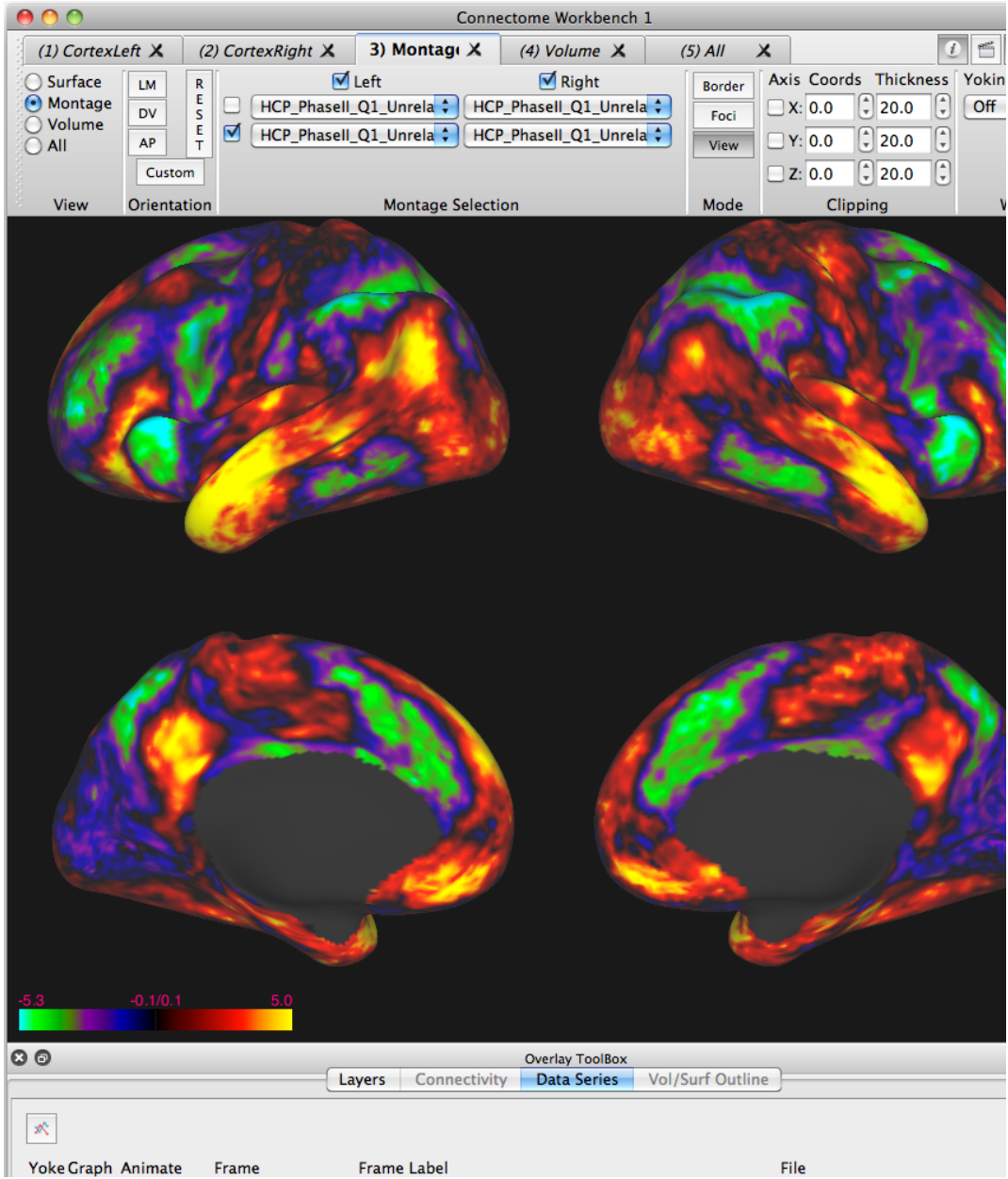
fMRIVol

fMRISurf

* see Glasser et al. NeuroIm

HCP Pipeline Overview





Surface-based analysis

HCP Pipeline Overview

Pre FreeSurfer

FreeSurfer

Post FreeSurfer

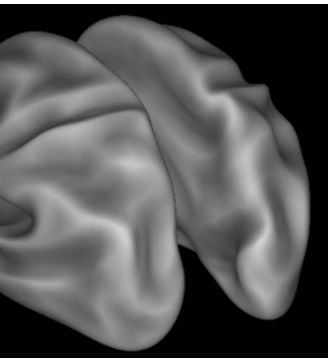
fMRIVol

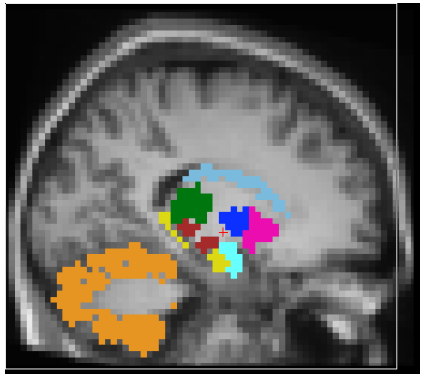
fMRISurf

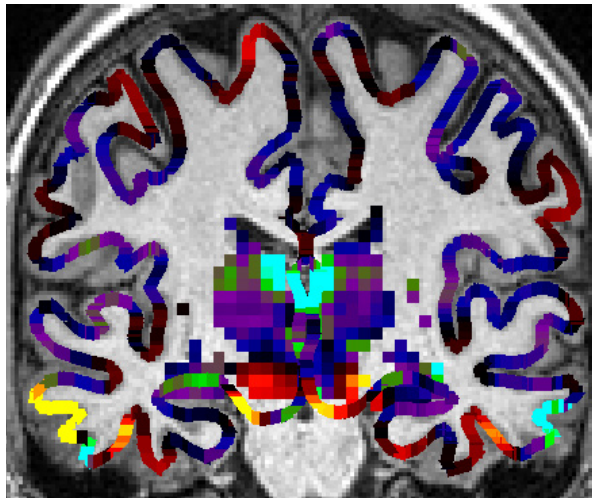
Both volume and surface streams

* Glasser et al. NeuroImage

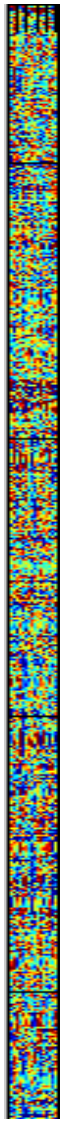
CIFTI Data Format



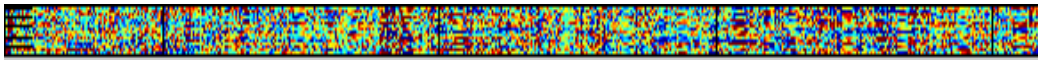


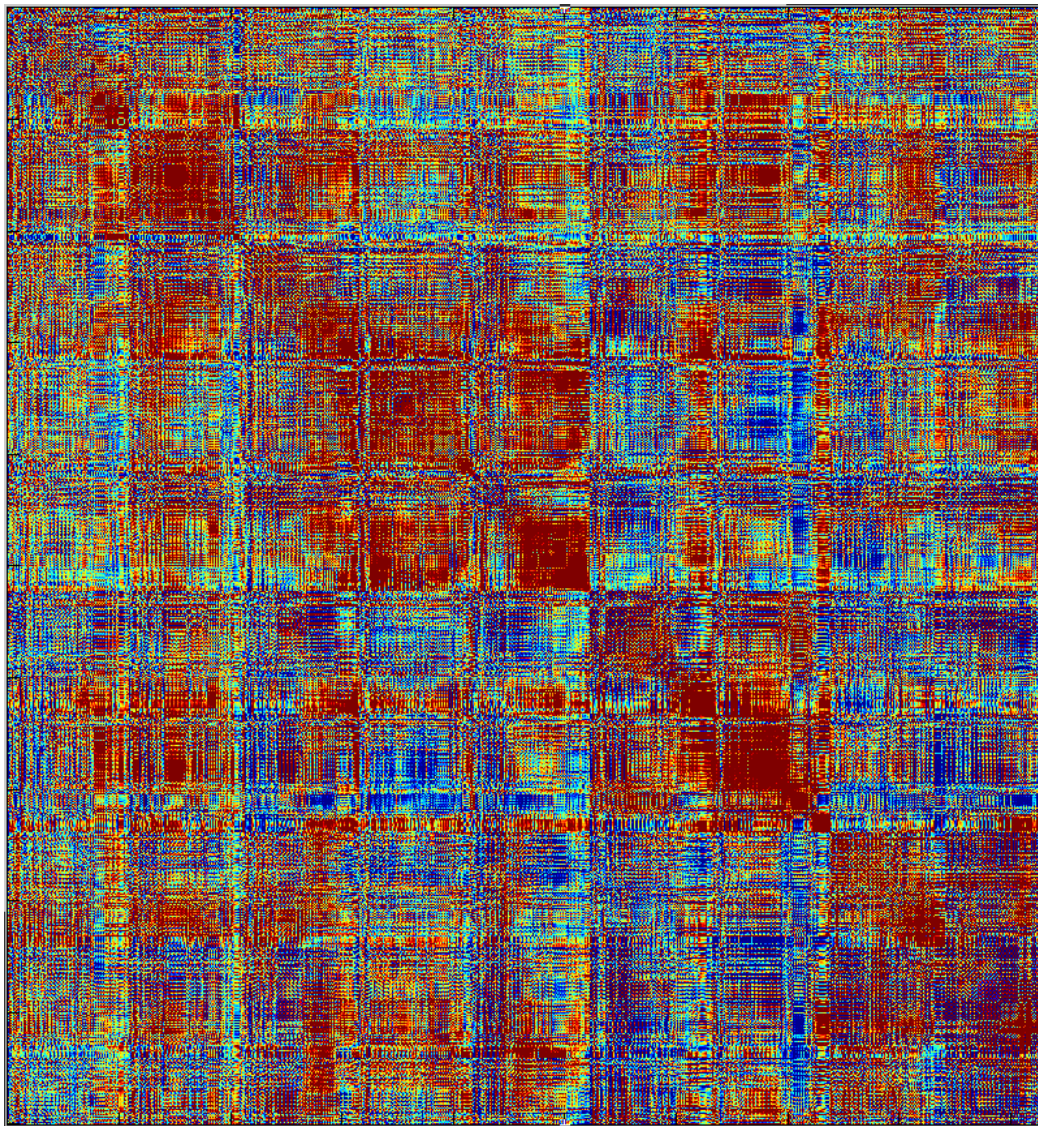


Grayordinates



Time points





functional connectivity matr

HCP Pipeline Overview

Pre FreeSurfer

FreeSurfer

Post FreeSurfer

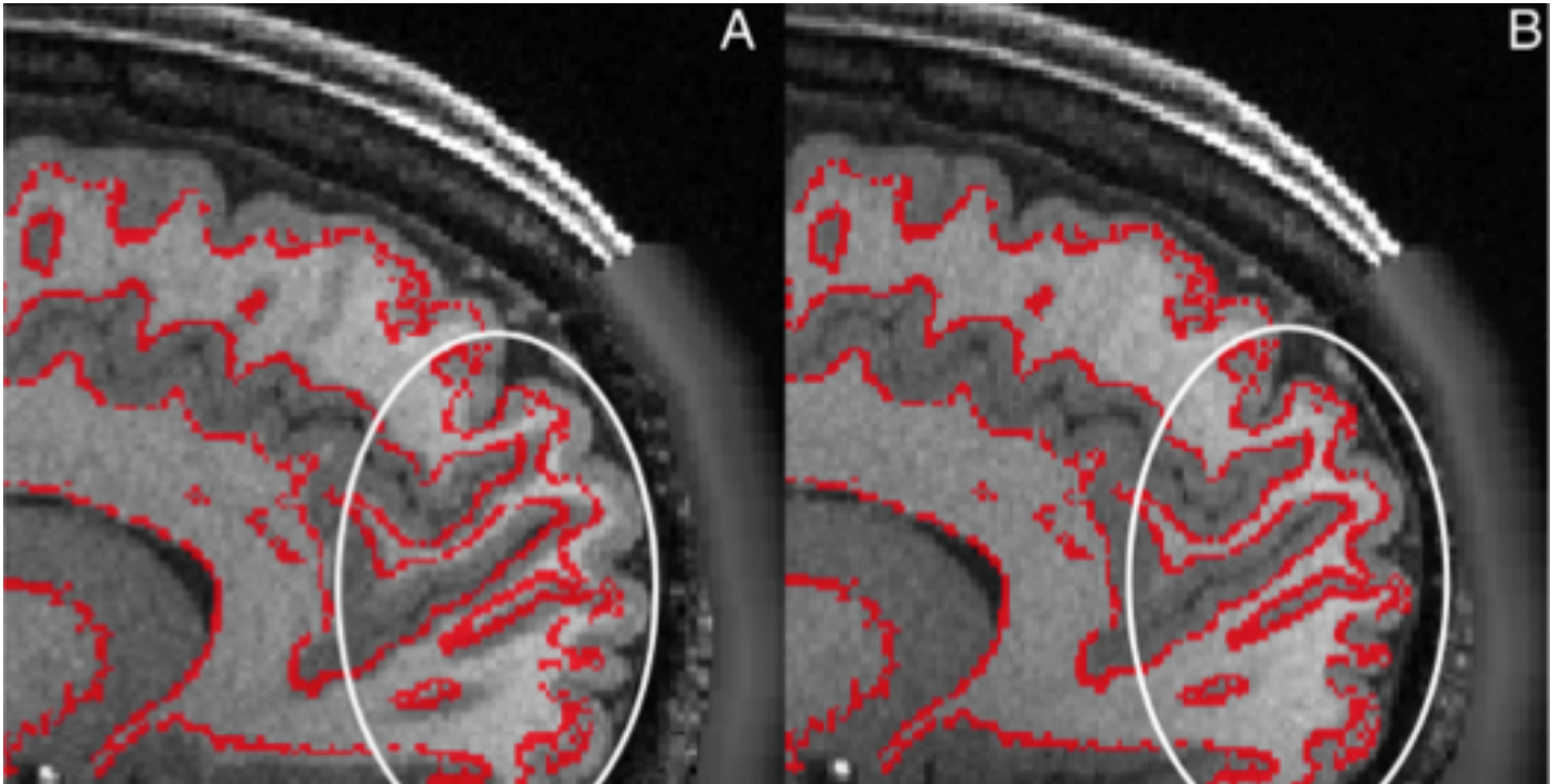
fMRIVol

fMRISurf

* Glasser et al. NeuroImage

Gradient Non-Linearity Distortion

- Correction method (based on MGH code and Siemens coil coefficients) works well



HCP Pipeline Overview

Pre FreeSurfer

FreeSurfer

Post FreeSurfer

fMRIVol

fMRISurf

* Glasser et al. NeuroImage

Pipeline Overview

- Conversion of DICOM to NIfTI
- Anonymise images
- Reorienting to "standard" orientation (MNI) - swapping axes

Pre FreeSurfer

- Gradient Non-Linearity Correction
- Averaging of separate T1w (and T2w) scans
  - using BBR (topup is an alternative)
- ACPC alignment (via MNI registration)
- Brain Extraction (via non-linear registration)
- T2w to T1w registration (BBR)
- Bias correction (B1 inhomog.) - via sqrt(T1w*T2w)
- Atlas (MNI) Registration

Combine all warps together to avoid repeated interpolation

Pipeline Overview

FreeSurfer - creates surfaces

- Create 1mm version
- Run initial FreeSurfer stages (autorecon 1 & 2)
- Fine tune WM intensity normalisation and registration to T2w
- Run intermediate FreeSurfer stages (inflation, etc.)
- Adjustments to Pial surface (using T2w)
- Run final FreeSurfer stages

Post FreeSurfer

- Non-linear registration to fsLR
- Create ribbon
- Complete myelin mapping

HCP Pipeline Overview*

Pre FreeSurfer

FreeSurfer

Post FreeSurfer

fMRIVol

fMRISurf

* Glasser et al. NeuroImage

Pipeline Overview

fMRIVol

- Gradient Non-Linearity Correction
- Motion Correction
- Registration of EPI to T1w
  - with B0 distortion correction (fieldmap)
- Bias field (B1) correction (taken from structural)

fMRISurface

- Extract ribbon from fMRI with voxel outlier exclusion
- Surfaced-based smoothing (2mm FWHM)
- SubCortical processing
  - smooth in volume (same FWHM as on surface)
- Create dense time series (CIFTI)

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n Brooks (Bristol, UK)

oug Greve (MGH, Harvard)