

Towards kinetic theory for multi-scale muscle models

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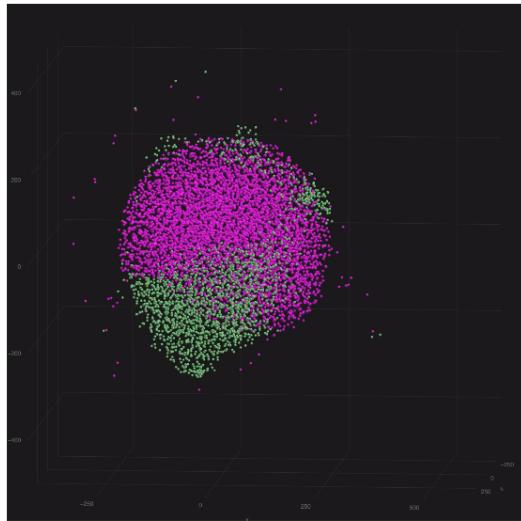
FELIX KLEIN
ZENTRUM FÜR
MATHEMATIK



Short self-introduction

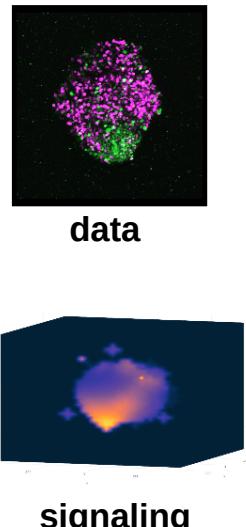
Current research in Kyoto Institute for the Advanced Study of Human Biology (ASHBi)

Limb bud morphogenesis



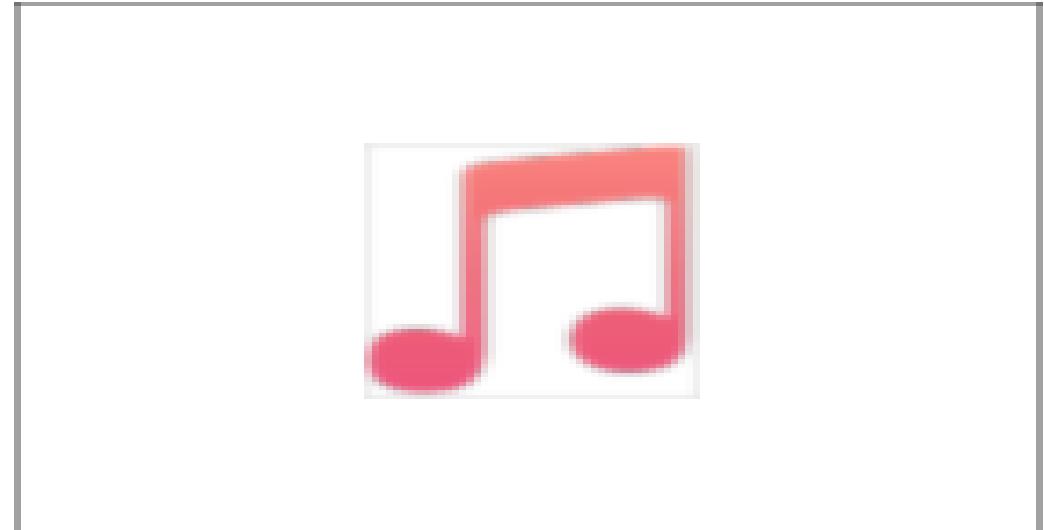
simulation

Epithelial-to-mesenchymal transitions



signaling

Developmental biology



agent-based model for
growing epithelium

Today's talk based on:

- [1] S. Plunder, B. Simeon,
The mean-field limit for particle systems with uniform full-rank constraints.
Kinetic and Related Models. (2023)

- [2] S. Plunder, B. Simeon,
*Coupled Systems of Linear Differential-Algebraic and Kinetic Equations
with Application to the Mathematical Modelling of Muscle Tissue.*
Conference preceding: Progress Differential-Algebraic Equations II. (2020).

Outline

1. Multi-scale (skeletal) muscle models
2. Abstract “**macro-micro**” model for tissue-cross-bridge coupling
3. Convergence in mean-field limit to “**macro-meso**” model
4. Possible extensions
 - *impossible for me*: adding a jump process for cross-bridge cycling
 - *easier (?)*: **global “macro-macro”** model and additive noise,
 - *abstract*: non-full rank constraints



locally
macro-micro
DAE

locally
macro-micro
ODE

locally
macro-meso
mf. char. ODE

locally
macro-meso
mf. PDE

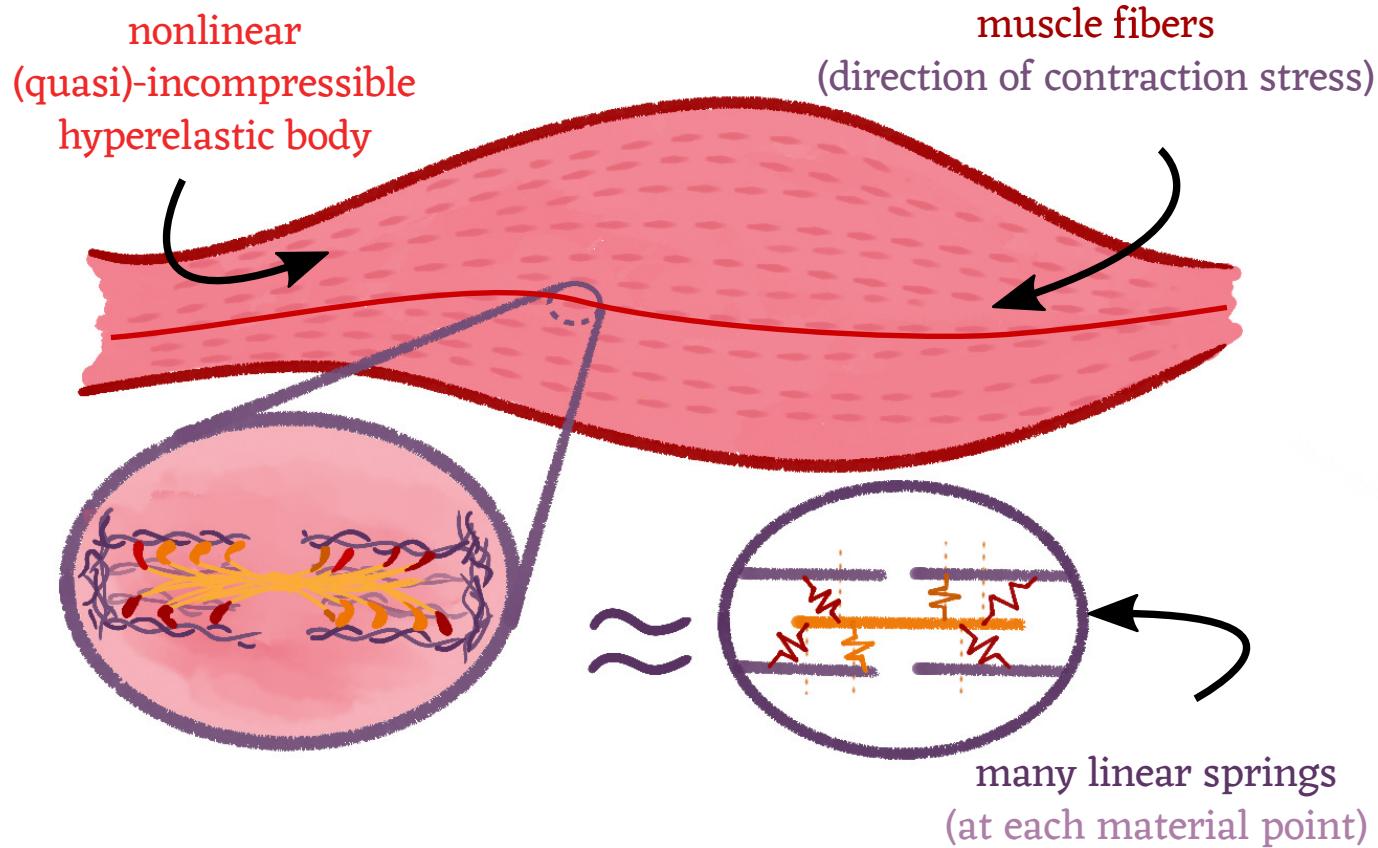
future

locally
macro-macro
mf. PDE

global
macro-macro
mf. PDE

Introduction

Motivation: Multi-scale muscle models



Question: How can we apply kinetic theory to such a system?

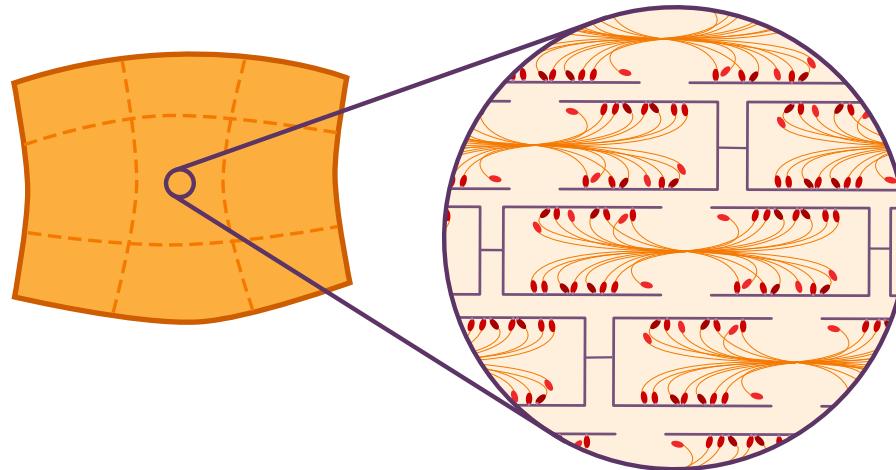
Challenges: From a kinetic theory perspective

Macroscopic component:

Passive muscle tissue

Particles:

Actin-myosin filaments



$$\begin{aligned}\dot{X}_i &= F(X_i, y) \\ \dot{y} &= G(X_1, \dots, X_N, y)\end{aligned}$$

Each attached cross-bridge is coupled to tissue deformation.
Hence, all particles interact with each other through the tissue!

(However, *once formulated properly*, kinetic theory works out rather well.)

Multi-scale muscle models

... and their lack of perfect physical structure

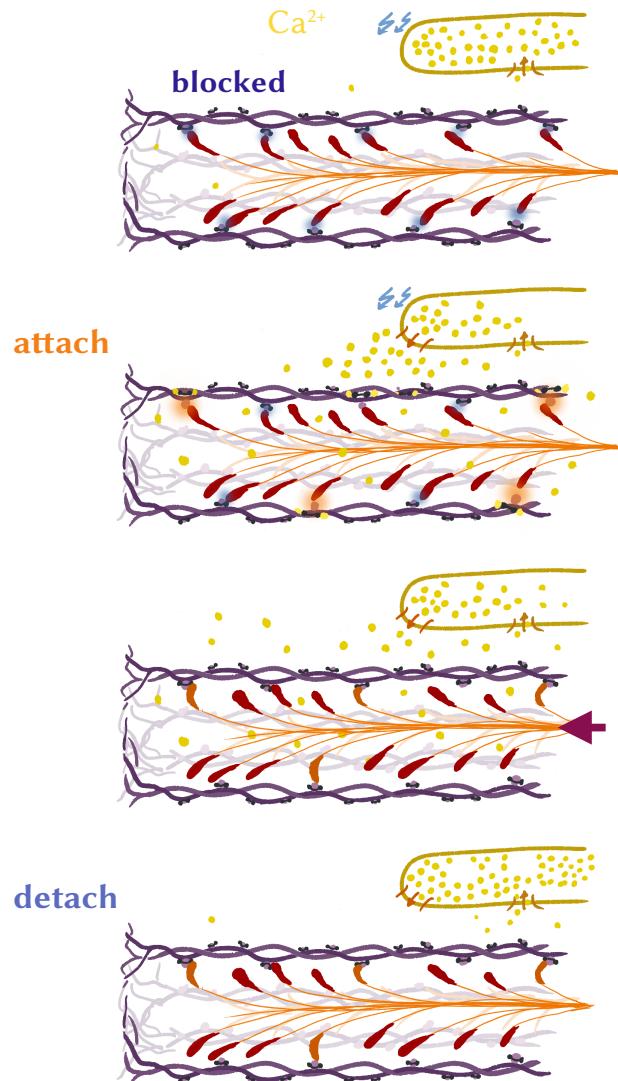
Foundations: Sliding filament theory

Huxley's two-state mode:

1. Cross-bridges have two states:
attached or detached.
2. Cross-bridge extension determines transition probabilities between states.
3. Muscle deformation changes cross-bridge extensions

$$\partial_t \rho(x, t) + \operatorname{div}(\rho(x, t)v(t)) = f(x)(1 - \rho(x, t)) - g(x)\rho(x, t)$$

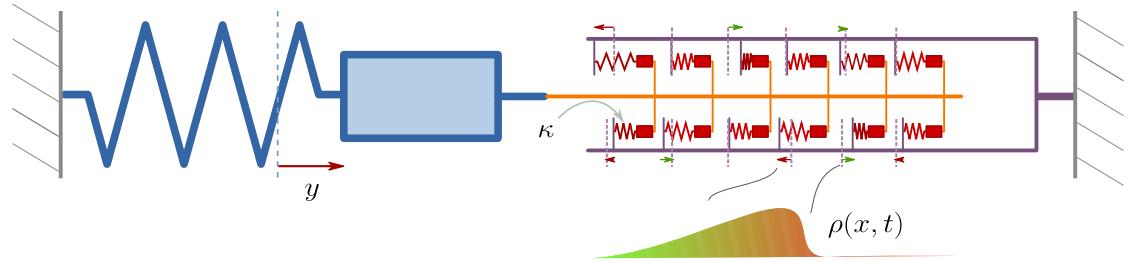
Generated force: $F = -\kappa \int_{\mathbb{R}} x \rho(x, t) dx$



Unilateral tissue-cross-bridge coupling

Simplest model:

$$\left\{ \begin{array}{l} F_{\text{xb}} = -\kappa \int_{\mathbb{R}} x \rho(x, t) dx \\ m \ddot{y} = F_{\text{passive}} + F_{\text{xb}} \\ \partial_t \rho + \text{div}_x(\rho \dot{y}) = 0 \end{array} \right.$$



$$\mathcal{W} = \mathcal{W}_{\text{passive}} + \int_{\mathbb{R}} \frac{\kappa}{2} x^2 d\rho(x, t)$$

$$\mathcal{T} = \frac{m}{2} \|\dot{y}\|^2 + \frac{1}{2} \int_{\mathbb{R}} \|\dot{y}\|^2 d\rho(x, t)$$

Potential issues:

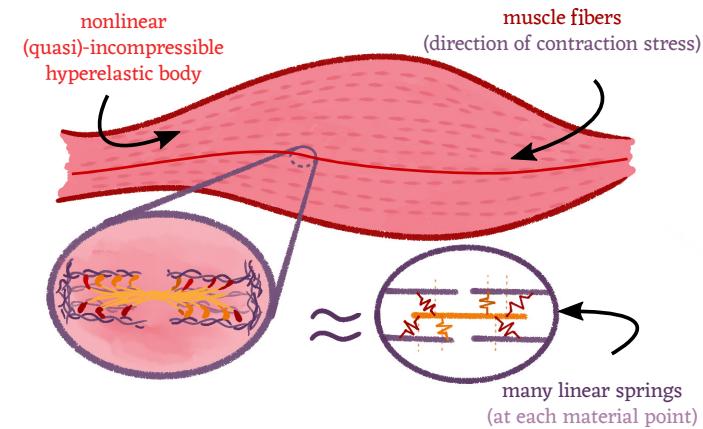
- This type of coupling ignores cross-bridge momentum.
- Ideally, the system should be conservative (no-cross bridge cycling, but it isn't exactly)...
Not clearly a Lagrangian system/Euler-Lagrange equation?

Typical multi-scale models*

Quasi-incompressible hyperelasticity (for muscle tissue)

$$\partial_t \varphi = \operatorname{Div}(P_{\text{passive}} + P_{\text{active}} + pG)$$

$$\det(\partial\varphi) = 1 + \frac{p}{\kappa}$$



Cross-bridge model enters via active stress term:

$$P_{\text{active}} = -\frac{\partial \mathcal{W}_{\text{active}}}{\partial D\varphi} \quad \mathcal{W}_{\text{active}} = \left(\kappa \int x \, d\rho(x, t) \right) \cdot \text{"stress tensor in fiber direction"}$$

some equation to approximate $\partial_t \rho + \operatorname{div}_x(\rho v_{\text{xb}}) = 0$ (e.g. *distributed moment method*).

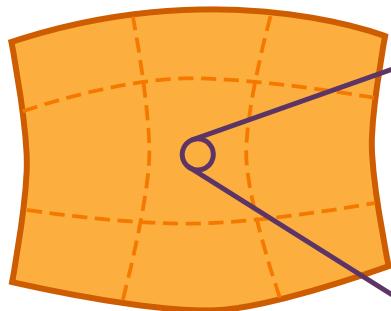
The system doesn't seem to be a direct Euler-Lagrange equation.

* Very non-comprehensive list: [2008] M. Böhl, S. Reese [2016] T. Heidlauf, O. Röhrle [2017] Herzog, W. [2022] M. H. Gfrerer; B. Simeon

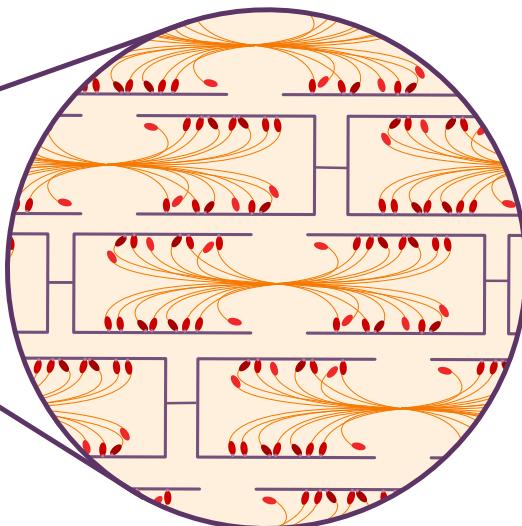
The microscopic dynamics are governed by the macroscopic scale

Macroscopic component:

Passive muscle tissue



Particles:
Actin-myosin filaments



“Unilateral” coupling:

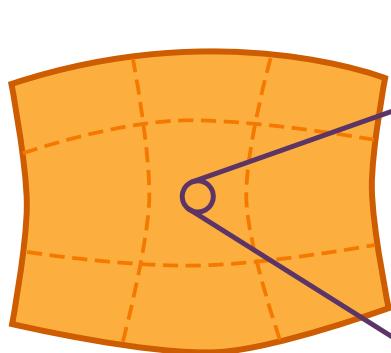
Actin-myosin contractions
accumulate
to macroscopic stress.



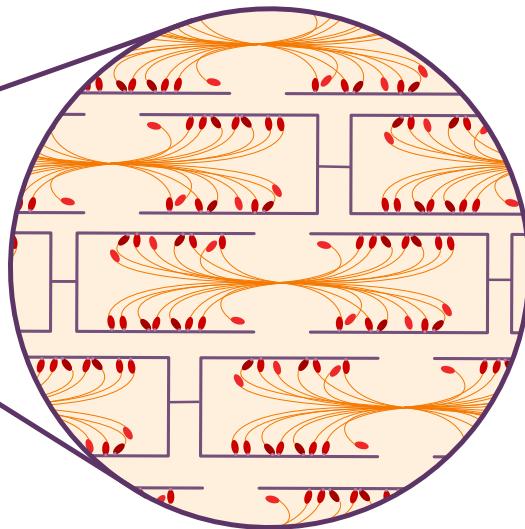
*Tissue deformation
determines cross-bridge dynamics.*

Focus today on bilateral coupling for multi-scale model

Macroscopic component:
Passive muscle tissue



Particles:
Actin-myosin filaments



Both levels impact each other equally:

Actin-myosin contraction
accumulates
to macroscopic force.

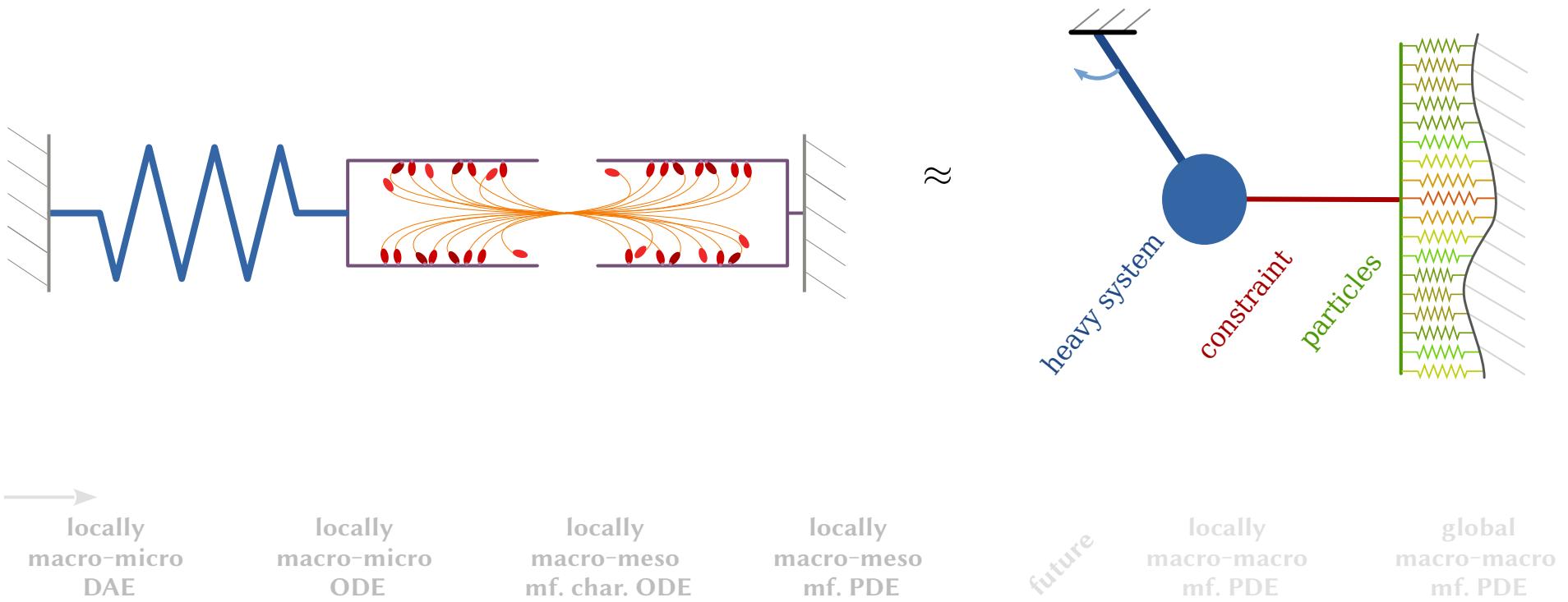


*Tissue deformation
pulls or pushes cross-bridges.*

Disclaimer: *In terms of physical units, the concrete changes we discuss today are often insignificantly small!*

This talk is about the math of these models, with the hope get insights into the structure of the systems.

Abstract “macro-micro” model for tissue-cross-bridge coupling



Very short recall of **differential-algebraic equations** (DAEs)

$$\dot{x} = f(x) \quad \text{such that} \quad g(x) = 0$$

can be implemented with Lagrangian multipliers via

$$\begin{aligned}\dot{x} &= f(x) + \partial_x g(x)^T \lambda, \\ g(x) &= 0.\end{aligned}$$



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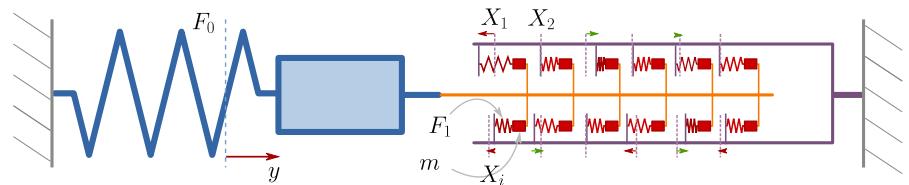
global
macro-macro
mf. PDE

Abstract “macro-micro” system

$$\ddot{y} = F_0(y) + \frac{1}{N} \sum_{j=1}^N \partial_y g(X_j, y)^T \lambda_j,$$

$$mX_i = F_1(X_i) + \partial_{X_i} g(X_i, y)^T \lambda_i + \frac{1}{N} \sum_{j=1}^N K(X_j, X_i),$$

$$g(X_i, y) = g(X_i^{\text{init}}, y^{\text{init}}) \quad \forall 1 \leq i \leq N.$$



$$g : \mathbb{R}^{n_x} \times \mathbb{R}^{n_y} \rightarrow \mathbb{R}^{n_x}$$

Constraints

$$\lambda_1, \dots, \lambda_N \in \mathbb{R}^{n_x}$$

Lagrangian multipliers

$$\left. \begin{array}{l} F_0(y) = -\nabla_y \mathcal{W}_0(y) \\ F_1(X) = -\nabla_X \mathcal{W}_1(X) \end{array} \right\}$$

Forces

$$K(X_j, X_i) = -\nabla_{X_i} \mathcal{V}(X_j - X_i)$$

Interaction forces

→
locally
macro-micro
DAE

locally
macro-micro
ODE

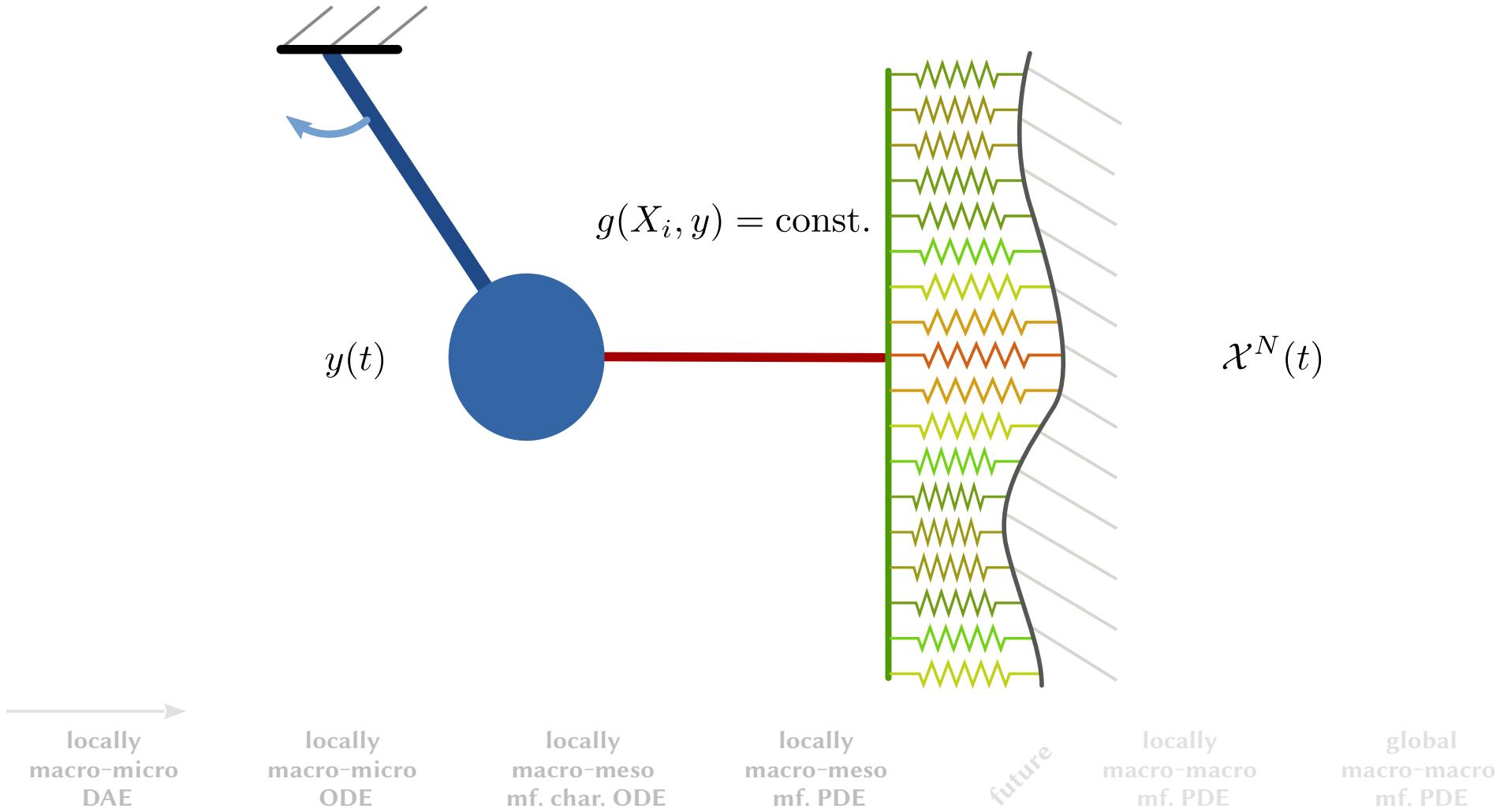
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This is a classical Lagrangian system

$$\begin{aligned}\mathcal{L}(y, \mathcal{X}^N, \Lambda^N) = & \frac{1}{2} \|\dot{y}\|^2 - \mathcal{W}_0(y) + \frac{1}{N} \sum_{i=1}^N \left(\frac{m}{2} \|\dot{X}_i\|^2 - \lambda_i (g(X_i, y) - g(X_i^{\text{init}}, y^{\text{init}})) \right. \\ & \left. - \mathcal{W}_1(X_i) - \frac{1}{2N} \sum_{j=1}^N \mathcal{V}(X_j - X_i) \right)\end{aligned}$$

→ conservation of energy

→ scaling factors picked such that total energy remains of order one in the limit $N \rightarrow \infty$.



Examples (linear constraints)

Consider $g(X_i, y) = X_i - Gy = \text{const}$ $G \in \mathbb{R}^{n_x \times n_y}$

Time derivative of constraint:

$$\Rightarrow \boxed{\dot{X}_i = G\dot{y}}$$

$$\Rightarrow F_1(X_i) + \partial_{X_i} g(X_i, y)^T \lambda_i = \boxed{m\ddot{X}_i = mG\ddot{y}}$$

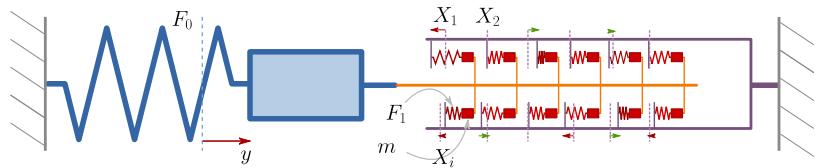
$$\Rightarrow \lambda_i = mG\ddot{y} - F_1(X_i)$$

$$\Rightarrow \ddot{y} = F_0(y) + \frac{1}{N} \sum_{j=1}^N G^T (mG\ddot{y} - F_1(X_j))$$

$$\Rightarrow (1 + mG^T G)\ddot{y} = F_0(y) - \frac{1}{N} \sum_{j=1}^N G^T F_1(X_j)$$

$$\rightsquigarrow \partial_t \rho = -\operatorname{div}_x(\rho G\dot{y})$$

$$\rightsquigarrow m_{\text{eff}} \ddot{y} = F_0(y) - \int_{\mathbb{R}} G^T F_1(x) \rho(x, t) dx = F_{\text{eff}}(y, \rho)$$



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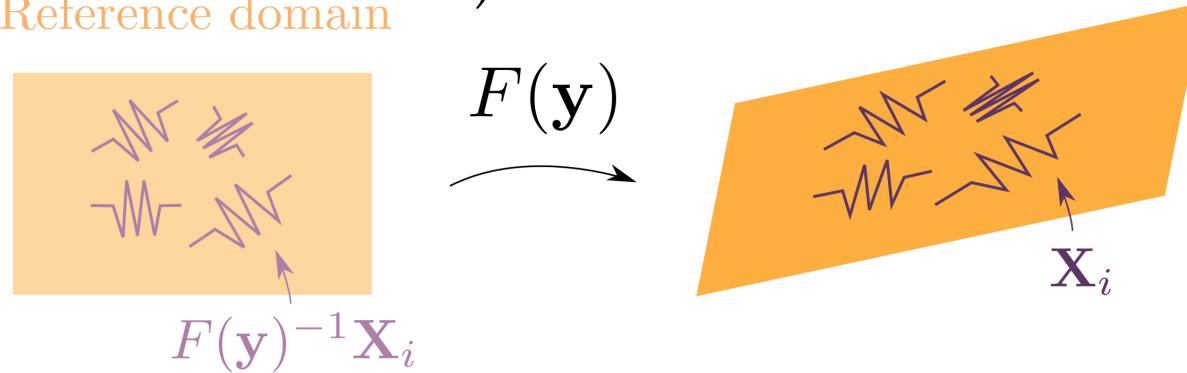
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Examples (nonlinear constraint)

Reference domain



Consider linear deformations of a finite element (e.g. rotation, stretching, **shearing**, ...)

$$g(X_i, y) = F(y(t))^{-1} X_i = \text{const} \quad (= X_i^{\text{in}})$$

Cp. [1996] G. I. Zahalak. *Non-axial Muscle Stress and Stiffness*. Journal of Theoretical Biology

In our framework, we can directly derive resulting active stress component from given constraints.



Strategy towards a mean-field description

DAE model



Mean-field PDAE system

Index reduction
+ multiplier elimination



ODE
model



Mean-field PDE system

Mean-field
limit



On this slide: $g_x := \frac{\partial g}{\partial X}(X_i, y)$ etc.

Index reduction

Index-3 DAE $\mathcal{M} = g^{-1}(\{0\})$

$$g(X_i, y) = 0$$

Assume:

$$\partial_{X_i} g(X_i, y) \in \mathbb{R}^{n_x \times n_x}$$

is always invertible

Index-2 DAE $T_{(X_i, y)} \mathcal{M}$

$$g_X[\dot{X}_i] + g_y[\dot{y}] = 0$$

$$\Rightarrow \quad \dot{X}_i = -g_x^{-1}[g_y[\dot{y}]]$$

$$\dot{X}_i = \Phi(X_i, y)[\dot{y}]$$

Index-1 DAE $T_{(\dot{X}_i, \dot{y}, X_i, y)} T \mathcal{M}$

$$\begin{aligned} & g_x[\ddot{X}_i] + g_{xx}[\dot{X}_i, \dot{X}_i] + 2g_{xy}[\dot{X}_i, \dot{y}] \\ & + g_y[\ddot{y}] + g_{yy}[\dot{y}, \dot{y}] = 0 \end{aligned}$$

$$\ddot{X} = \Phi(X, y)[\ddot{y}] + \Omega(X, y)[\dot{y}, \dot{y}]$$

$$\Omega = -g_x^{-1} (g_{xx}[\Phi \dot{y}, \Phi \dot{y}] + 2g_{xy}[\Phi \dot{y}, \dot{y}] + g_{yy}[\dot{y}, \dot{y}])$$

Elimination of multipliers (uses special structure of system!)

$$m\ddot{X}_i = F_1 + \frac{1}{N} \sum_j K_{ij} + g_x^T \lambda_i = m\Phi[\ddot{y}] + m\Omega[\dot{y}, \dot{y}]$$

$$\Rightarrow \quad \lambda_i = -g_x^{-1} \left(F_1 + \frac{1}{N} \sum_j K_{ij} - m\Phi[\ddot{y}] - m\Omega[\dot{y}, \dot{y}] \right)$$

The equivalent ODE model

$$\ddot{y} = F_0 + \frac{1}{N} \sum_{j=1}^N g_y^T \lambda_j$$

$$\lambda_i = -g_x^{-1} \left(F_1 + \frac{1}{N} \sum K - m\Phi[\ddot{y}] - m\Omega[\dot{y}, \dot{y}] \right)$$

$$\overbrace{\left(1 + \frac{1}{N} \sum_{j=1}^N m\Phi^T \Phi \right) \ddot{y}}^{m_{\text{eff}}(\mathcal{X}^N, y)} = \overbrace{\frac{1}{N} \sum_{j=1}^N \left(F_0 + \Phi^T \left(F_1 - m\Omega[\dot{y}, \dot{y}] + \frac{1}{N} \sum_{k=1}^N K \right) \right)}{F_{\text{eff}}(\mathcal{X}^N, y)}$$

$$\dot{X}_i = \Phi[\dot{y}]$$

Each solution of the DAE model solves the ODE mode, and vice versa.



Dealing with the **non-constant mean-field mass**

ODE model

$$m_{\text{eff}}^N(\mathcal{X}^N, y) \ddot{y} = F_{\text{eff}}^N(\mathcal{X}^N, y, \dot{y}) \quad \dot{X}_i = \Phi(X_i, y)[\dot{y}]$$

“Remember”:

$$\frac{d}{dz} \frac{f(z)}{m(z)} = \frac{f'(z)m(z) - f(z)m'(z)}{m(z)^2}$$

We need that mass is bounded from below...

Lemma: Assume $g : \mathbb{R}^{n_x} \times \mathbb{R}^{n_y} \rightarrow \mathbb{R}^{n_x}$ is twice continuously differentiable and g, Dg, D^2g are all bounded and Lipschitz and the Jacobian is uniformly elliptic, i.e.

$$\inf_{v \in \mathbb{R}^{n_x}} v^T \partial_{X_i} g(X_i, y) v \geq \delta \|v\|^2 \quad \forall X_i \in \mathbb{R}^{n_x}, y \in \mathbb{R}^{n_y},$$

then Φ, Ω and m_{eff}^N are well-defined, bounded and Lipschitz continuous.



Full list of mathematical assumptions

$$F_0(y) = -\nabla_y \mathcal{W}_0(y), \quad F_1(X_i) = -\nabla_{X_i} \mathcal{W}_1(X_i), \quad K(X_j, X_i) = -\nabla_{X_i} \mathcal{V}(X_j - X_i)$$

$F_0, F_1, K, g, Dg, D^2g \in BL$ $BL = \text{"bounded and Lipschitz continuous functions"}$

$$\inf_v v^T g(x, y) v \geq \delta \|v\|^2 \quad \forall v, x, y$$

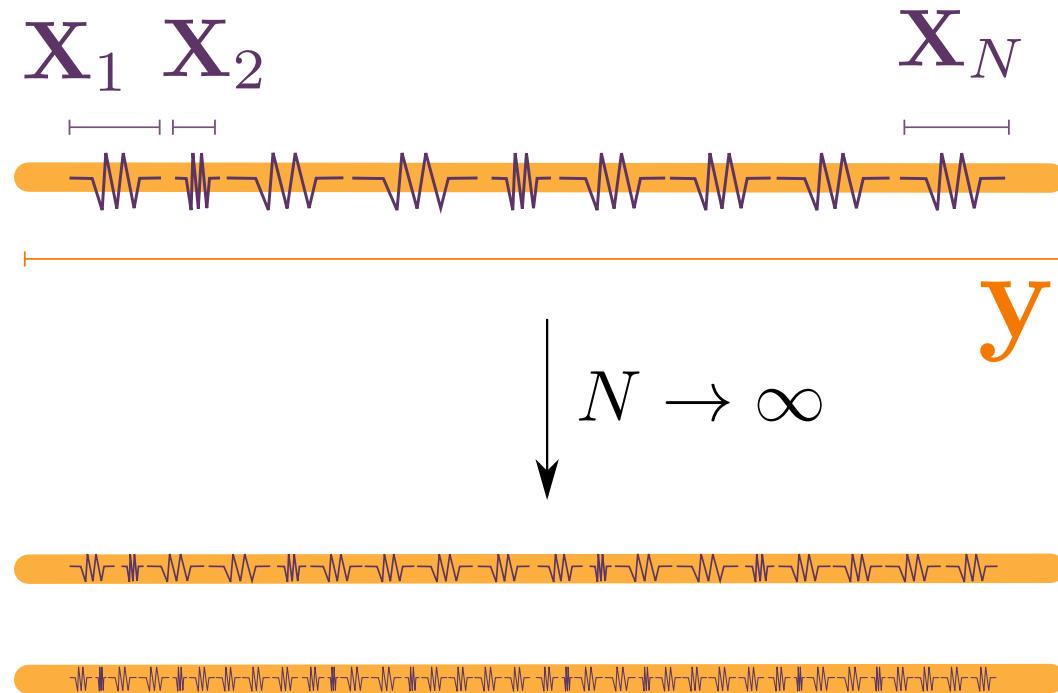
Lemma: The ODE model is well-posed and for any constant $M_v > 0$ the map

$$(y, v, \mathcal{X}^N) \mapsto \left(1 + \frac{1}{N} \sum_{j=1}^N m \Phi^T \Phi \right)^{-1} \left(\frac{1}{N} \sum_{j=1}^N \left(F_0 + \Phi^T \left(F_1 - m \Omega[v, v] + \frac{1}{N} \sum_{k=1}^N K \right) \right) \right)$$

is bounded and Lipschitz on $\mathbb{R}^{n_y} \times B_{M_v}^{\mathbb{R}^{n_y}}(0) \times (\mathbb{R}^{n_x})^N$.



The mean-field limit



Formal transition from **macro-micro** to **macro-meso...**

ODE model

$$m_{\text{eff}}^N(\mathcal{X}^N, y) \ddot{y} = F_{\text{eff}}^N(\mathcal{X}^N, y, \dot{y})$$

$$\dot{X}_i = \Phi(X_i, y)[\dot{y}]$$

Define empirical measure as:

$$\mu_{\mathcal{X}^N}^{\text{emp}} = \frac{1}{N} \sum_{i=1}^N \delta_{X_i}.$$

$$m_{\text{eff}}(\mu^t, y) \ddot{y} = F_{\text{eff}}(\mu^t, y, \dot{y}),$$

Mean-field characteristic flow:

$$\partial_t X^t(x^{\text{in}}) = \Phi(X^t(x^{\text{in}}), y)[\dot{y}] \quad \forall x^{\text{in}} \in \mathbb{R}^{n_x},$$

$$\mu^t(A) := \mu_{\mathcal{X}_N^{\text{in}}}^{\text{emp}}((X^t)^{-1}(A)).$$



Mean-field PDE

For particle densities $\rho(x, t) dx = d\mu^t(x)$ where $X_i \sim \mu^N(x, t) dx$ and $\mu^N \rightarrow \mu$.

The mean-field PDE is

$$m_{\text{eff}}(y, \rho)\ddot{y} = F_{\text{eff}}(y, \dot{y}, \rho)$$

$$\partial_t \rho = -\text{div}(\rho \Phi(x, y)[\dot{y}])$$

with

$$\Phi(x, y) = -(\partial_x g(x, y))^{-1} \partial_y g(x, y)$$

Macro-micro velocity map

$$m_{\text{eff}} = 1 + m \int \Phi(x, y)^T \Phi(x, y) \rho(x, t) dx$$

“Mean-field” mass

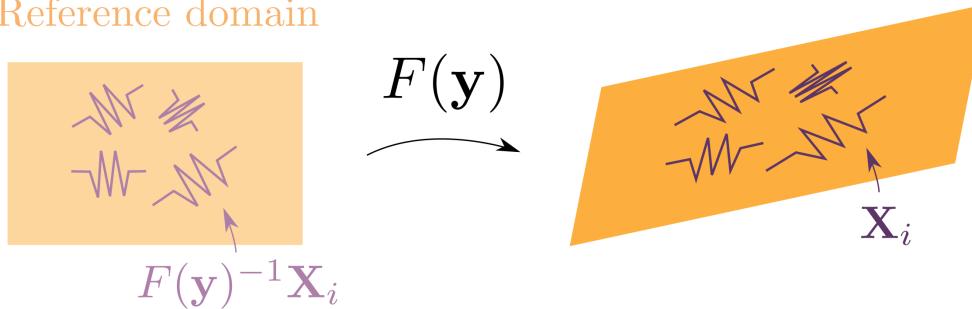
$$F_{\text{eff}} = F_0 - \int \Phi^T \left(F_1(x) + m\Omega(x, y)[\dot{y}] + \int K(x, x') \rho(x', t) dx' \right) \rho(x, t) dx$$

“Mean-field” force



Recall: nonlinear constraint example

Reference domain



Consider linear deformations of a finite element (e.g. rotation, stretching, **shearing**, ...)

$$g(X_i, y) = F(y(t))^{-1}X_i = \text{const} \quad (= X_i^{\text{in}})$$

Resulting **mean-field PDE**

$$\partial_t \rho = -\operatorname{div}_x(\rho F(\dot{y})F(y)^{-1}x) = -\rho \operatorname{tr}(F(\dot{y})F(y)^{-1}) - F(\dot{y})F(y)^{-1}x \cdot (\partial_x \rho)$$



Mathematical setup for **kinetic theory**

$$\mathcal{P}^1(\mathbb{R}^{n_x}) = \{\mu \text{ prob. measure on } \mathbb{R}^{n_x} \mid \int \|x\| d\mu(x) < \infty\}$$

space of probability measures with finite first moment.

$$W_1(\mu, \nu) = \sup_{\phi \in C(\mathbb{R}^{n_x}, \mathbb{R}^{n_x}), \text{Lip}(\phi) < 1} \int \phi(x) d\mu(x) - \int \phi(x) d\nu(x)$$

Wasserstein distance (with exponent 1).

$$\mu_{\mathcal{X}^N}^{\text{emp}} = \frac{1}{N} \sum_{i=1}^N \delta_{X_i}$$

empirical measure

Stability estimate [SP, Simeon] Given two solutions $(y_1, \mu_1), (y_2, \mu_2) : [0, T] \rightarrow \mathbb{R}^{n_y} \times \mathcal{P}^1(\mathbb{R}^{n_x})$

with initial conditions $y_i(0) = y_i^{\text{in}}, \dot{y}_i(0) = v_i^{\text{in}}$ and $\mu_i^0 = \mu_i^{\text{in}}$ then

$$\begin{aligned} \|y_1(t) - y_2(t)\| + \|\dot{y}_1(t) - \dot{y}_2(t)\| + W_1(\mu_1^t, \mu_2^t) \\ \leq C e^{Lt} (\|y_1^{\text{in}} - y_2^{\text{in}}\| + \|v_1^{\text{in}} - v_2^{\text{in}}\| + W_1(\mu_1^{\text{in}}, \mu_2^{\text{in}})) \end{aligned}$$

where the constants C and L only depend on the total energy and

$$C_\mu = \max\left(\int 1 + \|x\| d\mu_1^{\text{in}}(x), \int 1 + \|x\| d\mu_2^{\text{in}}(x)\right).$$

Convergence in mean-field limit For any sequence of microscopic initial conditions $(\mathcal{X}_k^{\text{in}})_k$ such that $W_1(\mu_{\mathcal{X}_k^{\text{in}}}^{\text{emp}}, \mu^{\text{in}}) \rightarrow 0$ as $k \rightarrow \infty$, then $W_1(\mu_{\mathcal{X}_k(t)}^{\text{emp}}, \mu(t)) \rightarrow 0$ for all $0 \leq t \leq T$.



Outline of the proof (mostly whiteboard)

Ingredients

Mean-field characteristic flow

$$m_{\text{eff}}(\mu^t, y) \ddot{y} = F_{\text{eff}}(\mu^t, y, \dot{y})$$

$$\partial_t X^t(x^{\text{in}}) = \Phi(X^t(x^{\text{in}}), y)[\dot{y}] \quad \forall x^{\text{in}} \in \mathbb{R}^{n_x},$$

$$\mu^t(A) := \mu^{\text{in}}((X^t)^{-1}(A)) \quad \forall A \in \mathfrak{B}(\mathbb{R}^{n_x})$$

$$\Leftrightarrow \dot{z} = b(z, \mu^{\text{in}})$$

$$z = (y, \dot{y}, \varphi) \in \mathbb{R}^{n_y} \oplus B_{M_v}^{\mathbb{R}^{n_y}} \oplus Y =: Z_{M_v} \subset Z$$

$$Y = \{\varphi \in C(\mathbb{R}^{n_x}, \mathbb{R}^{n_x}) \mid \sup_{x \in \mathbb{R}^{n_x}} \frac{\|\varphi(x)\|}{1 + \|x\|} < \infty\}$$

$z \mapsto b(z, \mu^{\text{in}})$ is Lipschitz

(for limited velocities \dot{y}):

$$\|b(z_1, \mu^{\text{in}}) - b(z_2, \mu^{\text{in}})\| \leq L_z \|z_1 - z_2\|_Z$$

$\mu \mapsto b(z, \mu)$ is Lipschitz:

$$\|b(z, \mu_1) - b(z, \mu_2)\| \leq L_\mu W_1(\mu_1, \mu_2)$$

Fundamental lemma:

$$\dot{z}_i = b(z_i, \mu_i^{\text{in}}), \quad z_i(0) = z_i^{\text{in}} \quad \text{for } i = 1, 2.$$

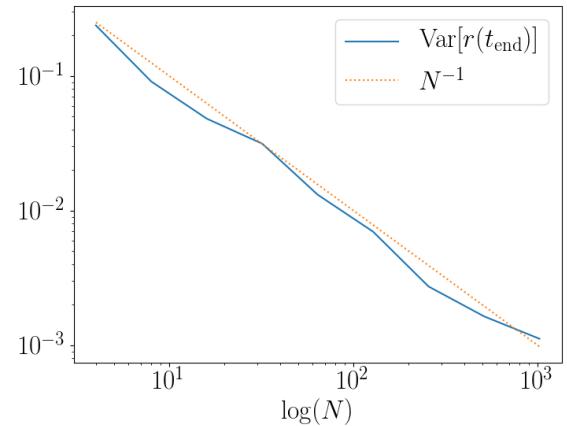
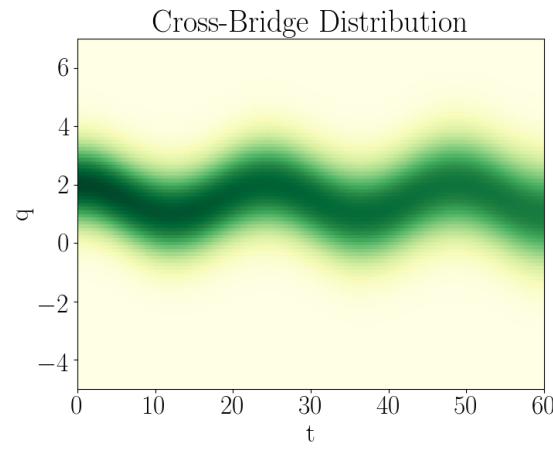
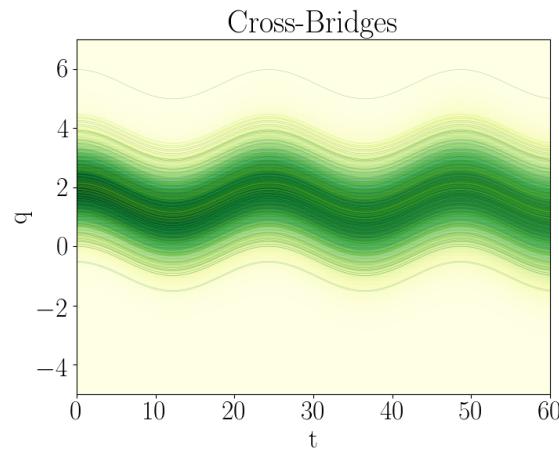
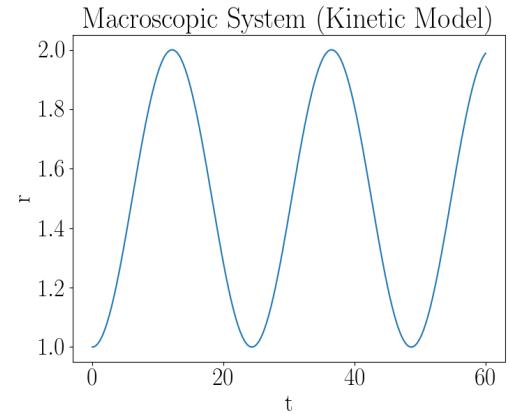
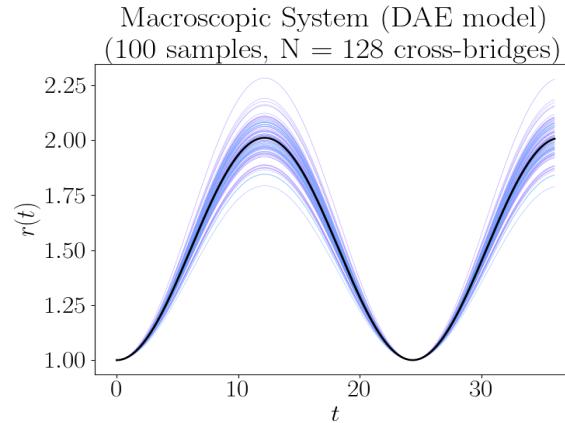
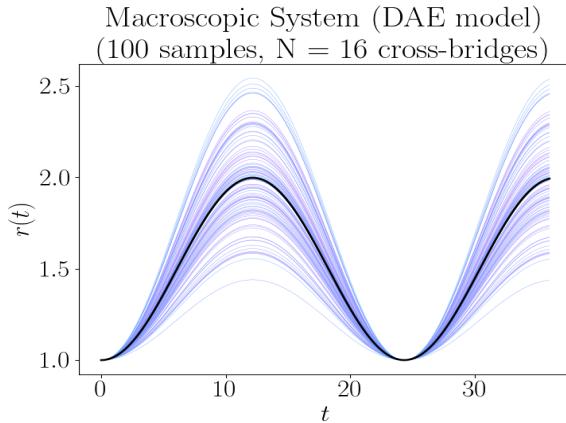
If $\|z_1^{\text{in}} - z_2^{\text{in}}\|_Z \leq \varrho$,

$$\|b(z, \mu_1^{\text{in}}) - b(z, \mu_2^{\text{in}})\| \leq \varepsilon \quad \forall z \in Z_{M_v}$$

$$\|b(z, \mu_1^{\text{in}}) - b(z', \mu_2^{\text{in}})\| \leq L \|z - z'\| \quad \forall z, z' \in Z_{M_v}$$

Then $\|z_1(t) - z_2(t)\| \leq \varrho e^{Lt} + \frac{\varepsilon}{L} (e^{Lt} - 1).$

Small numerical validation (linear case)



locally
macro-micro
DAE

locally
macro-micro
ODE

locally
macro-meso
mf. char. ODE

locally
macro-meso
mf. PDE

future

locally
macro-macro
mf. PDE

global
macro-macro
mf. PDE

Outlooks

Is there general “Macro-macro” system?

Assuming $x^2\rho(x, t)\Phi(x, y) \rightarrow 0$, as $|x| \rightarrow \infty$:

Mean-field PDE

$$\begin{aligned} m_{\text{eff}}(y, \rho)\ddot{y} &= F_{\text{eff}}(y, \dot{y}, \rho) \\ \partial_t \rho &= -\text{div}(\rho \Phi(x, y)[\dot{y}]) \end{aligned}$$



$$m(t) = \int \rho(x, t) dx$$

$$\nu(t) = \int x\rho(x, t) dx$$

$$\sigma(t) = \int x^2\rho(x, t) dx$$

$$\dot{m}(t) = 0 \quad \text{conservation of mass}$$

$$\dot{\nu}(t) = \dot{y} \int \rho(x, t)\Phi(x, y) dx$$

$$\dot{\sigma}(t) \approx 2\dot{y} \int x\rho(x, t)\Phi(x, y) dx$$

To close the system, one might need to use the concrete constraints...

locally
macro-micro
DAE

locally
macro-micro
ODE

locally
macro-meso
mf. char. ODE

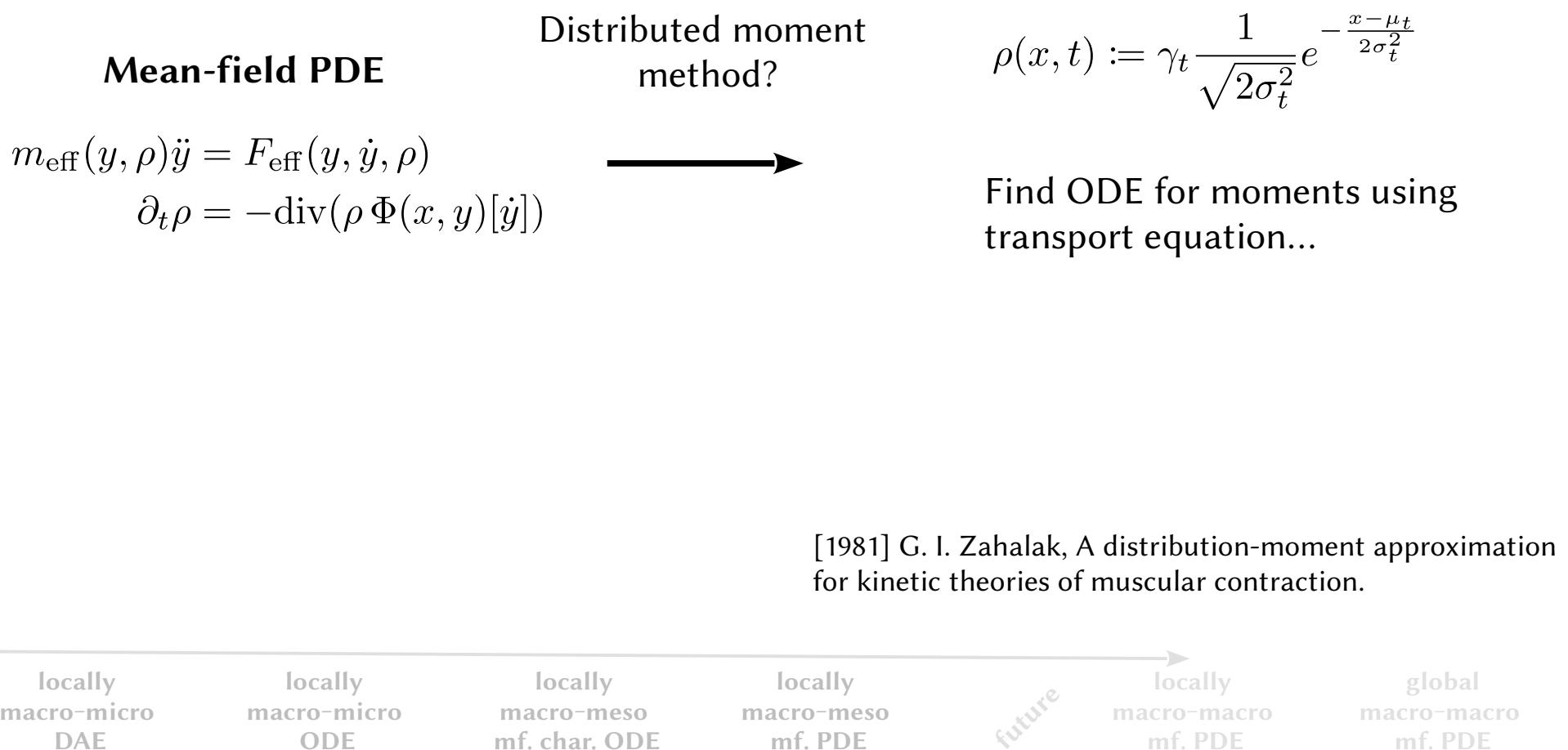
locally
macro-meso
mf. PDE

future

locally
macro-macro
mf. PDE

global
macro-macro
mf. PDE

Or approximate “Macro-macro” systems?



Adding spacial macroscopic model

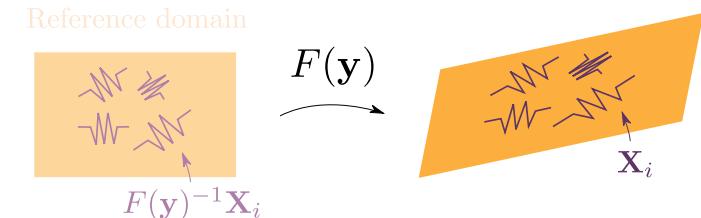
Theory might well generalize for cases where the macroscopic system is a PDE:

$$y(t) \in H^1(\Omega_{\text{ref}}, \mathbb{R}^2)$$

Formally, the current framework always supports this:

$$Z_i = (X_i, p) \in \mathbb{R}^{n_x} \times \Omega_{\text{ref}}$$

$$\dot{Z}_i = \begin{pmatrix} F_1(X_i) + \partial_X g(Z_i, y)\lambda_i \\ \partial_p g(Z_i, y) \end{pmatrix} \quad g(Z_i, y) = \begin{pmatrix} F(y(t, p_i))^{-1} X_i \\ p_i \end{pmatrix} = \text{const.}$$



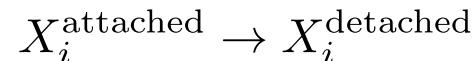
However, it is probably overly complicated...



Further directions

1. Most obvious current flaw: **Cross-bridge cycling is missing!**

Requires either two population with creation/annihilation:



Or one could modulate the constraints (but the analysis breaks):

$$Z_i = (X_i, s), \quad g(Z_i, y) = s \cdot (Z_i - y)$$

(I am sure the audience knows better how to integrate cross-bridge cycling.)

2. Relaxing the full rank condition: $\text{rnk}(\partial_X g(X_i, y)) < n_x$?

Thanks