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United States Patent	12383381
Kind Code	B2
Date of Patent	August 12, 2025
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Dental implant, superstructure, and dental prosthesis

Abstract

Dental implant and superstructure each with an interface that allows direct attachment of the superstructure to the dental implant without the use of an abutment. The dental implant comprises an anti-rotation element that is arranged in the opening and is configured to prevent the superstructure from rotating about a longitudinal axis relative to the dental implant. The superstructure comprises an interface corresponding to the anti-rotation element, having a recess with two mutually opposite side flanks which are at a first distance from each other in a first region and, in a second region which is at a greater distance from the longitudinal axis than the first region, are at a second distance from each other, the second distance being smaller than the first distance.

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Appl. No.: 17/874889

Filed: July 27, 2022

Prior Publication Data

Document Identifier	Publication Date
US 20220361989 A1	Nov. 17, 2022

Foreign Application Priority Data

DE	10 2020 102 307.3	Jan. 30, 2020
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Related U.S. Application Data

continuation parent-doc WO PCT/EP2021/052030 20210128 PENDING child-doc US 17874889

Publication Classification

Int. Cl.: A61C8/00 (20060101)

U.S. Cl.:

CPC A61C8/0075 (20130101); A61C8/0022 (20130101);

Field of Classification Search

CPC: A61C (8/0075); A61C (8/0022)

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Background/Summary

CROSS REFERENCE TO RELATED APPLICATIONS (1) This application is a continuation of International Patent Application No. PCT/EP2021/052030, filed on Jan. 28, 2021, which claims priority to German Patent Application No. DE 10 2020 102 307.3, filed on Jan. 30, 2020. The entire disclosures of these applications are incorporated herein by reference.

FIELD

(1) The present disclosure relates to a dental implant and to a superstructure for use in a dental prosthesis. Furthermore, the disclosure relates to a dental prosthesis comprising the dental implant and/or the superstructure.

BACKGROUND

(2) The term “dental implant” is often colloquially used inconsistently and often erroneously for the overall structure of a dental prosthesis. Therefore, it should be clarified at this point that a “dental implant” in the medical and present sense is understood to mean only the implant body, i.e. the artificial tooth root that is implanted in the patient's jaw. Therefore, the term “implant body” is often used instead of the term “dental implant”. In the following, however, the term “dental implant” is uniformly used for the aforesaid part of the dental prosthesis.

(3) The term “superstructure” refers to a denture attached to a dental implant. This can be, for example, an artificial dental crown (also called “implant crown”), a bridge or any other prosthetic or artificial dental structure.

(4) In addition to the dental implant and the superstructure, conventional dental prostheses comprise a so-called abutment, which acts as a connecting part between the dental implant and the superstructure. The abutment forms the sensitive transition through the peri-implant soft tissue to the oral cavity and the superstructure. Such abutments are sometimes referred to as “pillars” or “implant posts”. Commonly, abutments are made of titanium, ceramic or ceramic composites such as aluminum oxide ceramic or zirconium dioxide ceramic.

(5) The superstructure, i.e. the artificial dental crown, is typically made of ceramic or a comparable material. Traditionally, the superstructure is made by a dental technician as follows: First, a wax model is created for the artificial dental crown. Then, the wax model is used to cast the artificial dental crown. The abutment is manually ground to the correct size and shape, and in the final step the cast artificial dental crown is mounted on the abutment. In most cases, the assembly is performed by bonding the superstructure to the abutment. This largely manual process allows highly precise results to be achieved. However, it goes without saying that this is time-consuming and therefore also cost-intensive. Additionally, there is an adhesive gap between the superstructure and the abutment, which gap is susceptible to leaks and can also limit the durability of the dental prosthesis.

(6) Nowadays, there are many efforts to digitize or automate the above-mentioned process as far as possible. The superstructure is now often milled on a milling machine using a 3D model. In this type of fabrication, the connection geometry for the connection with the abutment is directly introduced into the superstructure on its rear side. The shape and size of the abutment must therefore already be known during the fabrication of the artificial dental crown in order to be able to program the milling machine accordingly. This is usually done by means of a CAD model of the abutment, which is read into the control system of the milling machine.

(7) Since the shape and size of the abutment must be known before fabricating the superstructure, many manufacturers choose a short and small abutment that fits any anatomy. However, with elongated, i.e. comparatively long superstructures, a short and small abutment is biomechanically

unsuitable in relation to the superstructure, which may result in loosening or fractures.

(8) Other manufacturers solve this by means of a plurality of different abutments. Depending on the shape and size of the superstructure, abutments of different sizes or shapes are then used. For example, a different abutment has to be used for an artificial incisor than for an artificial molar tooth. If, for example, the rear flank of the abutment is not beveled when used for an artificial incisor, the abutment would be visible on the rear side of the superstructure, which is undesirable from a purely esthetic point of view. However, this problem may not arise when used for an artificial molar tooth.

(9) In automated fabrication with digital CAD models, the manufacturer of the superstructure is usually provided with several CAD data sets that represent the different shapes of the abutments. At the same time, the manufacturer of the superstructure has to keep a large number of abutments of different shapes and sizes in stock. This is often cumbersome and also generates high storage costs.

(10) The disadvantages of the previous approaches can thus be summarized as follows: On the one hand, the use of abutments restricts the freedom of shape and design of the superstructure including its transgingival portion. A non-flexible transgingival portion of the superstructure can cause problems, particularly with soft tissue management. However, ideal soft-tissue management is crucial for an esthetic result and a long-term stable bone level. On the other hand, the material and manufacturing costs for such a dental prosthesis according to the prior art are relatively high. In addition, there is an adhesive gap between the superstructure and the abutment, which gap is disadvantageous in many respects.

(11) DE 10 2018 113 237 A1 describes a completely new approach in which a dental prosthesis of the abovementioned type manages even without an abutment, i.e. wherein the superstructure is connected directly to the dental implant. This is achieved in particular by specially configured interfaces on the dental implant and the superstructure, permitting the two components to be fixed directly to each other. The interface on the dental implant and the interface which is complementary thereto on the superstructure permit a geometrically unambiguously defined arrangement of the superstructure directly on the dental implant (without an abutment arranged in between). This guarantees an unambiguously defined relative position between superstructure and dental implant.

(12) In order to avoid an undesirable rotation of the superstructure in relation to the dental implant, an anti-rotation device is required. In the case of the dental implant described in DE 10 2018 113 237 A1, said anti-rotation device is achieved by a non-rotationally symmetrical design of said interface on the dental implant and an interface, correspondingly formed as a counterpart, on the superstructure.

(13) Although the dental implant described in DE 10 2018 113 237 A1 has proven entirely advantageous, the inventors have set themselves the aim of improving the anti-rotation device of the dental implant to an even greater extent.

SUMMARY

(14) It is an object to provide a dental implant and a superstructure that can be connected directly to each other without the use of an abutment, comprising an improved anti-rotation device for preventing rotation of the superstructure in relation to the dental implant.

(15) According to a first aspect, a dental implant is provided, which comprises, on an outer side, an external thread for fixing the dental implant to a jaw bone, and an opening which extends along a central longitudinal axis of the dental implant and in which an internal thread for fixing a superstructure to the dental implant is arranged, wherein the dental implant furthermore comprises an interface for fixing the superstructure to the dental implant, said interface being arranged in a region of an end face of the dental implant and comprising an inner surface which is arranged in the opening and at least partially surrounds the longitudinal axis. The dental implant furthermore comprises an anti-rotation element that is arranged in the opening and is configured to prevent the superstructure from rotating about the longitudinal axis relative to the dental implant. The anti-rotation element is at a smaller distance from the longitudinal axis than the inner surface. A radially

outer side of the anti-rotation element that faces away from the longitudinal axis faces the inner surface and is spaced apart therefrom such that there is an upwardly open cavity between the radially outer side of the anti-rotation element and the inner surface.

(16) According to a second aspect, a superstructure is provided, which comprises an opening extending along a central longitudinal axis of the superstructure and an interface for fixing the superstructure to a dental implant. The interface is configured as an extension that is arranged on a lower side of the superstructure, surrounds the opening and has a lateral surface which forms an outer side of the extension. The lateral surface of the extension is interrupted by a recess which leads into the opening extending along the central longitudinal axis of the superstructure. The recess has two mutually opposite side flanks which, in a cross section oriented orthogonally with respect to the longitudinal axis, are at a first distance from each other in a first region and, in a second region which is at a greater distance from the longitudinal axis than the first region, are at a second distance from each other that is smaller than the first distance.

(17) The anti-rotation element provided on the dental implant produces a type of undercut in which the extension, which is provided on the lower side of the superstructure, at least partially engages. The undercut refers here to the upwardly open cavity which is formed between the radially outer side of the anti-rotation element and the inner surface of the dental implant. The superstructure engages in said cavity with a radially outer end of the extension.

(18) For this purpose, the recess which is introduced into the extension arranged on the lower side of the superstructure tapers somewhat radially outward. In other words, the recess is narrower at its radially outer end than at its radially inner end, which is arranged closer to the central longitudinal axis. This tapering of the recess is apparent in particular in the mentioned cross section which is oriented orthogonally with respect to the central longitudinal axis of the superstructure.

(19) The cavity mentioned which is produced on the dental implant by the anti-rotation element and the tapering mentioned of the recess introduced into the extension of the superstructure lead in particular to the following advantages: firstly, a mechanically highly stable anti-rotation device can thereby be realized. Not only the anti-rotation element arranged on the dental implant, but also the extension formed on the lower side of the superstructure can be formed in a mechanically stable way.

(20) The increase in stability at the extension of the superstructure should essentially be attributed to the fact that the recess which is provided therein can be comparatively small, in particular because of its tapering outward. The tapering of the recess means that the latter can be, for example, smaller than the recess which has purely rectilinear side flanks on the superstructure disclosed in the earlier patent application with the application number 10 2019 111 699.6. Furthermore, the cavity provided on the dental implant and the associated shape of the recess on the extension of the superstructure permit a more compact design of the superstructure and of the dental implant.

(21) According to a refinement of the dental implant, the upwardly open cavity tapers downward, as viewed in a longitudinal section of the dental implant, such that a first distance between the radially outer side of the anti-rotation element and the inner surface, as measured in the longitudinal section in a region of an upwardly open end of the cavity, is greater than a second distance between the radially outer side of the anti-rotation element and the inner surface, as measured in the longitudinal section in a region of a lower end of the cavity.

(22) The cavity preferably essentially has a V shape in this longitudinal section. The mentioned longitudinal section of the dental implant is spanned by the longitudinal axis of the dental implant and by a radial direction oriented orthogonally with respect thereto.

(23) The mentioned tapering of the cavity downward has in particular the advantage that the inner surface of the dental implant produces a supporting effect for the superstructure. In addition, the superstructure can be mounted relatively simply on the dental implant and the corresponding part of the superstructure can be introduced from above into the cavity.

- (24) According to a refinement, the anti-rotation element provided on the dental implant comprises two planar drive surfaces extending parallel to each other.
- (25) In the mounted state of the dental prosthesis, said planar drive surfaces preferably lie on planar drive surfaces which are shaped equivalently thereto and are arranged on the two opposite side flanks of the recess provided on the superstructure. The drive surfaces serve for absorbing force in the circumferential direction and prevent rotation or torsion of the superstructure about the longitudinal axis relative to the dental implant.
- (26) Preferably, the drive surfaces provided on the dental implant and the mutually corresponding drive surfaces provided on the superstructure each run parallel to each other and parallel to the respective longitudinal axis of the dental implant or of the superstructure.
- (27) It should be noted at this juncture that, in the mounted state of the dental prosthesis, the longitudinal axis of the dental implant preferably coincides with the longitudinal axis of the superstructure.
- (28) Furthermore, it is preferred that the drive surfaces which are provided on the dental implant and the mutually corresponding drive surfaces which are provided on the superstructure each run parallel to a radial direction which is oriented orthogonally with respect to the respective longitudinal axis.
- (29) Such an orientation permits a large transmission of the forces acting in the circumferential direction between superstructure and dental implant. Owing to the orientation mentioned, the drive surfaces can also be produced very simply by milling.
- (30) In the mounted state of the dental prosthesis, between the anti-rotation element provided on the dental implant and the recess provided on the superstructure there is preferably only contact along said planar drive surfaces. This ensures a mechanically defined contact between superstructure and dental implant, the contact not being mechanically overdetermined.
- (31) According to a further refinement, the anti-rotation element has a convex-concave shape in a cross section which is oriented orthogonally to the longitudinal axis.
- (32) The anti-rotation element is preferably a type of lamella or web which is offset radially further inward in comparison to the described inner surface which, in the region of the interface of the dental implant, forms the inner circumferential surface of the opening introduced centrally therein. Said anti-rotation element preferably runs parallel to the longitudinal axis of the dental implant. By means of its convex-concave cross section, the anti-rotation element is optimally adapted to the shape of the opening (bore) in the dental implant and therefore takes up relatively little space.
- (33) The anti-rotation element preferably has a constant wall thickness. The wall thickness measured in the cross section (orthogonally with respect to the longitudinal axis of the dental implant) is meant here.
- (34) The constant wall thickness has the advantage that the anti-rotation element, which is configured as a lamella or web, has a high degree of rigidity despite its space-saving design. In addition, the screw which is used for connecting the superstructure to the implant can thereby lie stably on the implant. In more precise terms, the anti-rotation element provides a contact surface for the screw.
- (35) A radially inner side of the anti-rotation element, which side lies opposite the radially outer side of the anti-rotation element, preferably runs parallel to the radially outer side of the anti-rotation element and therefore likewise parallel to the longitudinal axis. This therefore preferably results in a convex-concave cross section of the anti-rotation element with mutually opposite sides which run parallel to one another and run transversely with respect to the planar drive surfaces provided on the anti-rotation element.
- (36) The term “transversely” is preferably understood here as meaning any type of orientation which is not parallel. “Transversely” is therefore preferably, but not necessarily, understood as meaning orthogonally. Orientations deviating from vertical orientations are also referred to here as transversely if said orientations are not parallel to one another.

(37) According to a further refinement, the interface provided on the dental implant is mirror-symmetrical with respect to a longitudinal sectional plane in which the longitudinal axis lies and which divides the anti-rotation element into two halves of identical size. Equivalently thereto, it is preferred that the extension which is provided on the lower side of the superstructure is mirror-symmetrical with respect to a longitudinal sectional plane in which the longitudinal axis and which divides the recess into two halves of identical size. The anti-rotation element arranged on the dental implant and the recess which is shaped in a complementary manner with respect thereto and is provided in the extension of the superstructure are preferably likewise mirror-symmetrical with respect to said longitudinal sectional plane.

(38) According to a further refinement, the inner surface comprises a curved surface that is curved convexly in a longitudinal section in which the longitudinal axis lies. This curved surface preferably extends over an angular range of at least 90 degrees) ($^{\circ}$) about the longitudinal axis of the dental implant. Particularly preferably, the curved surface runs (360°) about the longitudinal axis of the dental implant.

(39) A “convex” curvature is understood here as meaning any outwardly curved curvature; a convex curvature forms the counterpart to a concave, inwardly curved trough. Simply for clarification purposes, the convex curvature is additionally also defined here as rounded even though the term “convex” already implies such a rounding. The curvature which is defined here as convex and rounded preferably has a continuous tangent slope (without a “bend”).

(40) Said convexly curved surface which forms part of the inner surface of the dental implant serves for fixing the superstructure to the dental implant. In the mounted state of the dental prosthesis, the latter preferably lies on a concavely curved lateral surface of the superstructure that is shaped in a complementary manner with respect thereto.

(41) The two curved surfaces which are shaped in a complementary manner with respect to each other absorb forces in the radial direction, i.e. orthogonally with respect to the longitudinal axis of the dental implant. In addition, they are used to center the superstructure in relation to the dental implant.

(42) According to a further refinement, the interface of the dental implant comprises a support surface that is arranged radially further outward than the inner surface, wherein the support surface extends around the longitudinal axis and is, all around the longitudinal axis, oriented at a constant angle transversely with respect to the longitudinal axis.

(43) This support surface is preferably a circular-ring-shaped support surface which surrounds the convexly curved surface. The circular-ring-shaped support surface preferably has a constant angle greater than 60° all around with respect to the longitudinal axis of the dental implant. Said angle is particularly preferably a right angle (90°).

(44) In the mounted state of the dental prosthesis, said support surface lies on a support surface which is shaped in a complementary manner with respect thereto and is arranged on the lower side of the superstructure. This serves for absorbing axial forces parallel to the longitudinal direction. Tensile stresses which could lead to fracturing of the superstructure are thereby avoided.

Furthermore, the two support surfaces which are formed in a complementary manner with respect to each other on the dental implant and the superstructure are used as boundary surfaces or sealing surfaces in order to avoid intermediate spaces along the circumference between the superstructure and the dental implant, through which intermediate spaces impurities might enter.

(45) The support surfaces therefore preferably form the radially outermost region of the respective interface on the dental implant and on the superstructure, which surrounds all of the other regions of the respective interface. Said support surface is therefore also preferably arranged radially further outward than the anti-rotation element and is therefore at a greater radial distance from the longitudinal axis than the anti-rotation element.

(46) The support surface which is arranged on the dental implant preferably forms an end surface which is arranged on the upper side of the dental implant and over which the anti-rotation element

does not protrude. The anti-rotation element is therefore arranged below the support surface.

(47) According to a further refinement, the convexly curved surface which forms part of the inner surface of the dental implant is directly adjacent to the support surface. A radially outer edge of the inner surface preferably merges tangentially into the support surface.

(48) Furthermore, it is preferred that the internal thread which is provided in the dental implant is at a greater distance from the end face of the dental implant than the anti-rotation element. In other words, the anti-rotation element is therefore preferably arranged above the internal thread and therefore closer to the end face of the dental implant.

(49) The following refinement possibilities are provided with regard to the superstructure:

(50) According to a refinement, each of the two mutually opposite side flanks of the recess comprises a planar drive surface and an adjacent, concavely curved surface, wherein the planar drive surfaces are each arranged in the first region of the side flanks, and the concavely curved surfaces are each arranged in the second region of the side flanks.

(51) The concavely curved surfaces and the planar drive surfaces of the two side flanks of the recesses each lie opposite one another. The concavely curved surfaces which are at a greater distance from the longitudinal axis, i.e. are arranged radially further outward than the planar drive surfaces, ensure the abovementioned tapering of the recess. In particular, in the mounted state of the dental prosthesis, that part of the concavely curved surfaces which is arranged radially further outward is arranged in the cavity provided behind the anti-rotation element in the dental implant. With the aid of the concavely curved surfaces, the extension which is arranged on the lower side of the superstructure at least partially engages around the anti-rotation element.

(52) The concavely curved surfaces are preferably curved concavely in the cross section which is oriented orthogonally with respect to the longitudinal axis. By contrast, the drive surfaces are configured as flat, planar surfaces.

(53) As already mentioned, the two drive surfaces which are arranged on the side flanks of the recess lie opposite each other and run parallel to each other and preferably parallel to the longitudinal axis of the superstructure. In the mounted state of the dental prosthesis, the anti-rotation element particularly preferably lies only on said drive surfaces and otherwise has no further contact with the superstructure.

(54) According to a further refinement, the recess is arranged in the region of a lower free end of the extension and is open downward toward the free end. The recess is particularly preferably configured as a tunnel-like recess.

(55) This has the advantage that the superstructure can be mounted very simply on the dental implant despite the anti-rotation device. The recess is namely merely placed from above onto the anti-rotation element or is at least partially pulled over the latter. Owing to the complementary design of the recess and of the anti-rotation element relative to each other, an unambiguous positioning of the superstructure relative to the dental implant is guaranteed.

(56) According to a further refinement, the recess in the radial direction runs orthogonally with respect to the longitudinal axis. Preferably, in particular a longitudinal direction along which the recess extends runs in the radial direction. The drive surfaces arranged on the two side flanks preferably run parallel to said longitudinal direction or parallel to the radial direction of the superstructure.

(57) According to a further refinement, the lateral surface which is arranged on the outer side of the extension is curved concavely in a longitudinal section in which the longitudinal axis lies. The lateral surface is preferably curved concavely in each longitudinal section in which the longitudinal axis lies. The lateral surface is preferably configured as a counterpart to the convexly curved inner surface provided on the dental implant. This surface is used to center the superstructure in relation to the dental implant. In addition, forces can be absorbed by it in the radial direction.

(58) As already mentioned at the beginning, the present disclosure relates not only to the dental implant and the superstructure, but also to a dental prosthesis having such a dental implant and/or

such a superstructure. The superstructure is preferably fixed directly to the dental implant with the aid of a fixing element. A screw is particularly preferably used as the fixing element.

(59) It goes without saying that the features mentioned above and those which have yet to be explained below are usable not only in the respectively stated combination, but also in different combinations or by themselves without departing from the spirit and scope of the present disclosure.

Description

BRIEF DESCRIPTION OF THE DRAWINGS

- (1) FIG. 1 shows a perspective view of a dental implant according to the principles of the present disclosure;
- (2) FIG. 2 shows a longitudinal sectional view of the dental implant shown in FIG. 1;
- (3) FIG. 3 shows an enlarged view of a portion of the dental implant shown in FIG. 2 within a circle III shown in FIG. 2;
- (4) FIG. 4 shows a top view of the dental implant shown in FIG. 1;
- (5) FIG. 5 shows a perspective view of a superstructure according to the principles of the present disclosure;
- (6) FIG. 6 shows a bottom view of the superstructure shown in FIG. 5;
- (7) FIG. 7 shows an enlarged view of a portion of the superstructure shown in FIG. 5 within a chain-dotted circle shown in FIG. 5;
- (8) FIG. 8 shows a cross section of a portion of the superstructure shown in FIG. 5; and
- (9) FIG. 9 shows a longitudinal sectional view of a dental prosthesis according to the principles of the present disclosure.

DETAILED DESCRIPTION

- (10) FIGS. 1-4 show an embodiment of a dental implant according to the present disclosure in various views. The dental implant is denoted therein in its entirety by the reference numeral **10**.
- (11) The dental implant **10** is typically manufactured from titanium or zirconium oxide. It has, on its outer side, an external thread **12** which can be used to screw the dental implant **10** in a patient's jaw bone. The dental implant **10** extends substantially along a longitudinal axis **14**, which may also be referred to as the center axis. In its interior, the dental implant **10** has an opening **16** which extends along the longitudinal axis **14**. At least part of said opening **16** is preferably configured as a bore, particularly preferably as a blind bore.
- (12) An internal thread **18** is arranged in the opening **16**. Said internal thread **18** is used to fix a superstructure **20** (artificial dental crown) to the dental implant **10**. In order to fix the superstructure **20** to the dental implant **10**, use is preferably made of a screw **22** which engages in the internal thread **18** (see FIG. 9). Instead of a screw **22**, use may basically also be made of a different type of fixing means, for example a bolt, for connecting the superstructure **20** to the dental implant **10**.
- (13) On the upper end face, the dental implant **10** has an interface **24** which is illustrated in the top view shown in FIG. 4. Said interface **24** is used for fixing the superstructure **20** to the dental implant **10**. The interface **24** forms, as it were, the contact region with which the dental implant **10** makes contact with the superstructure **20** in the mounted state of a dental prosthesis **100**.
- (14) A particular characteristic of the interface **24** can be seen in the fact that the latter, because of its shape and design, permits the superstructure **20** to be directly attached to the dental implant **10** (without the use of an abutment arranged in between).
- (15) The interface **24** has an inner surface **26** which is arranged in the opening **16**. Said inner surface **26** is an inner lateral surface which at least partially surrounds the longitudinal axis **14**. The inner lateral surface **26** faces the longitudinal axis **14**. Each normal vector which is oriented perpendicularly to said inner lateral surface **26** preferably intersects the longitudinal axis **14**,

specifically independently of the point at which said normal vector is placed onto the inner lateral surface **26**. In the exemplary embodiment shown here, the inner lateral surface **26** is at least partially convexly curved, as viewed in longitudinal section, as will be explained in more detail further below.

(16) The interface **24** furthermore has an anti-rotation element **28**. In the mounted state of the dental prosthesis **100**, said anti-rotation element **28** prevents the superstructure **20** from rotating in relation to the dental implant **10**. In the embodiment shown here, the anti-rotation element **28** is connected integrally to the dental implant **10**. However, in principle, the anti-rotation element **28** can also be configured as a separate component which is fixed in the dental implant **10**.

(17) The anti-rotation element **28** preferably runs parallel to the longitudinal axis **14**. In comparison to the previously mentioned convexly curved inner surface **26**, the anti-rotation element **28** is arranged radially somewhat further inward, i.e. closer to the longitudinal axis **14**. As can be seen from the top view shown in FIG. 4, the anti-rotation element **28** has a convex-concave shape in a cross section orthogonally with respect to the longitudinal axis **14**. A radially outer side **30** of the anti-rotation element **28** faces away from the longitudinal axis **14**. Said radially outer side **30** faces part of the inner lateral surface **26**. However, the radially outer side **30** of the anti-rotation element **28** is spaced apart from the inner lateral surface **26** such that a cavity **32**, which is a type of undercut, is produced between the radially outer side **30** of the anti-rotation element **28** and the inner lateral surface **26**. Said cavity **32** is open upward.

(18) As is apparent in particular from FIG. 3 which shows a detail of the longitudinal section shown in FIG. 2, the cavity **32** tapers downward. The cavity **32** has approximately the shape of a V, as viewed in this longitudinal section. Expressed in other words, a first distance D1 between the radially outer side **30** of the anti-rotation element **28** and the inner surface **26**, as measured in the longitudinal section in the region of the upper open end of the cavity **32**, is greater than a second distance D2 between the radially outer side **30** of the anti-rotation element **28** and the inner surface **26**, as measured in the longitudinal section in the region of a lower end of the cavity **32**.

(19) As is likewise apparent from FIG. 3, the anti-rotation element **28** preferably has a constant wall thickness. The wall thickness of the anti-rotation element **28** is constant at least in cross section (also see FIG. 4).

(20) As will also be explained in detail further below, a part of the superstructure **20** engages in said cavity **32**, thus enabling a special manner of configuring the superstructure **20** and a special manner of connecting the superstructure **20** to the dental implant **10** in the region of the anti-rotation element **28**.

(21) The radially inner side **36** of the anti-rotation element **28**, which side is opposite the radially outer side **30**, faces the opening **16** or the longitudinal axis **14**. While the radially outer side **30** is preferably a convex surface, the radially inner side **36** is preferably a concave surface. Accordingly, the anti-rotation element **28** is adapted to the cross-sectional shape of the opening or bore **16**, and is therefore comparatively space-saving. The internal thread **18** is freely accessible from above for the screw **22**.

(22) The anti-rotation element **28** furthermore has two mutually opposite drive surfaces **34a**, **34b**. Said two drive surfaces **34a**, **34b** are arranged on opposite sides of the anti-rotation element **28**. The drive surfaces **34a**, **34b** run transversely and between the radially outer side **30** and the radially inner side **36** of the anti-rotation element **28**. They are each configured as planar surfaces.

(23) The two drive surfaces **34a**, **34b** preferably run parallel to a radial direction **38** which is oriented orthogonally with respect to the longitudinal axis **14**. Said radial direction **38** is in each case indicated as an arrow in FIGS. 2 and 4. An imaginary longitudinal sectional plane E.sub.1 spanned by said radial direction **38** and the longitudinal axis **14** divides the anti-rotation element **28** into two halves of identical size. The anti-rotation element **28** is preferably mirror-symmetrical with respect to said longitudinal sectional plane E.sub.1.

(24) The drive surfaces **34a**, **34b** are used as contact surfaces for corresponding counter surfaces

which are arranged on the superstructure **20**. The drive surfaces **34a**, **34b** are essentially used to absorb a torque acting about the longitudinal axis **14** between the superstructure **20** and the dental implant **10**. They prevent the superstructure **20** from rotating about the longitudinal axis **14** in relation to the dental implant **10**.

(25) Owing to the described arrangement of the drive surfaces **34a**, **34b**, the latter essentially absorb forces acting in the circumferential direction. In the mounted state of the dental prosthesis **100**, the superstructure **20** preferably makes contact with the anti-rotation element **28** only along said two drive surfaces **34a**, **34b**.

(26) In this embodiment, material incisions **40** are provided on both sides laterally next to the anti-rotation element **28**. Said material incisions **40** are essentially used to simplify the production of the dental implant **10** in terms of manufacturing.

(27) The interface **24** is preferably mirror-symmetrical with respect to the previously mentioned imaginary plane E.sub.1. As already mentioned, the inner surface **26** belonging to the interface **24** has a curved surface **42** which is curved convexly in the longitudinal section shown in FIG. 2. Said convexly curved surface **42** preferably runs around the longitudinal axis **14**. It lies on a concavely curved surface, which is correspondingly shaped as a counterpart, on the superstructure **20**. The convexly curved surface **42** is used essentially for absorbing forces in the radial direction **38**.

(28) The convexly curved surface **42** is surrounded by a support surface **44** which is essentially used for absorbing axial forces, i.e. forces parallel to the longitudinal axis **14**. The support surface **44** is arranged radially further outward than the convexly curved surface **42**. In the embodiment shown here, the convexly curved surface **42** merges, preferably tangentially, at its radially outer edge into the support surface **44**. The support surface **44** extends around the longitudinal axis **14** and is oriented around the latter at a constant angle transversely with respect to the longitudinal axis **14**. In the present case, this angle is an angle less than 90°. The support surface **44** is therefore a conical surface. In principle, however, the support surface **44** may also be oriented orthogonally with respect to the longitudinal axis **14**. Irrespective of the angle of the support surface **44** with respect to the longitudinal axis **14**, it is preferred, as already mentioned, for said support surface to merge tangentially into the convexly curved surface **42**.

(29) In the mounted state of the dental prosthesis **100**, the superstructure **20** is supported both on the convexly curved surface **42** and on the support surface **44**.

(30) As viewed in the longitudinal section of the dental implant **10** (see FIG. 2), the convexly curved surface **42** is preferably configured as a sector of a circle. Accordingly, the convexly curved surface **42** forms part of the surface of a torus. Like also the remaining parts of the interface **24**, it can therefore be produced very simply using a ball cutter. However, it goes without saying that the convexly curved surface **42** does not inevitably have to be circular in the longitudinal section. In the described longitudinal section of the dental implant **10**, it can also be shaped elliptically or configured as a freely shaped surface, but it is preferably “bend-free” in said cross section.

(31) FIGS. 5 and 6 show an embodiment of the superstructure **20** which serves as a counterpart to the dental implant shown in FIGS. 1-4. The superstructure **20** has an artificial denture **46** which is illustrated here as an artificial dental crown. An interface **48** which is used for the connection to the dental implant **10** is arranged on the lower side of said artificial dental crown **46**.

(32) The interface **48** has an extension **50** which protrudes downward from the lower side of the artificial dental crown **46**. This extension **50** is configured as a corresponding counterpart to the interface **24** arranged on the dental implant **10**.

(33) In the interior, the superstructure **20** has an opening **52** which is preferably configured as a through bore. Said opening **52** is closed at the upper end face of the artificial dental crown **46** after the dental prosthesis **100** is fitted to the patient. The opening **52** essentially extends along a longitudinal axis **54** of the superstructure **20**. In the mounted state of the dental prosthesis **100**, the longitudinal axis **54** of the superstructure **20** coincides with the longitudinal axis **14** of the dental implant **10** (see FIG. 9).

(34) The interface **48** has a lateral surface **56** which forms an outer side of the extension **50** and surrounds the opening **52** in the circumferential direction. In the exemplary embodiment shown in FIGS. **5** and **6**, the lateral surface **56** is formed concavely as a counterpart to the inner lateral surface **26** arranged on the dental implant **10**. In more precise terms, the outer lateral surface **56** of the extension **50** is curved concavely in a longitudinal section in which the longitudinal axis **54** of the superstructure **20** lies. The outer lateral surface **56** preferably has the shape of a sector of a circle in this longitudinal section. However, like the inner lateral surface **26** on the dental implant **10**, the outer lateral surface **56** can also be shaped elliptically or can have a free shape in the longitudinal section.

(35) In principle, it is also possible to design the outer lateral surface **56** of the extension **50** as a conical or cylindrical surface. In such a case, the inner lateral surface **26** on the dental implant **10** is then also correspondingly configured as a conical or cylindrical surface.

(36) Furthermore, the interface **48** has a recess **58** which is introduced laterally into the extension **50**. The recess **58** is used as a counterpart to the anti-rotation element **28**. In the mounted state of the dental prosthesis **100**, the anti-rotation element **28** engages in said recess **58**.

(37) The recess **58** is open downward. Accordingly, it does not have a closed contour, but rather is open on one side to the lower end face of the interface **48**. Accordingly, the recess **58** can also be described as a tunnel-like or tunnel-shaped recess.

(38) The recess **58** passes through the side wall of the extension **50**. It therefore interrupts the lateral surface **56** and leads into the opening **52** running in the interior of the superstructure **20**.

(39) The recess **58** has two mutually opposite side flanks **60a**, **60b**. One of these two side flanks **60a** is illustrated in detail in FIG. **7**. FIG. **8** shows the cross-sectional shape of the recess **58** in detail. In more precise terms, FIG. **8** is a detailed cutout of a cross section orthogonally with respect to the longitudinal axis **54** of the superstructure **20** through the extension **50**.

(40) As can be seen in particular from FIG. **8**, each of the two side flanks **60a**, **60b** has a first region **62a** or **62b**, in which the side flanks **60a**, **60b** are configured as planar surfaces. By contrast, in a second region **64a**, **64b** arranged radially further outward, the two side flanks **60a**, **60b** are each configured as concavely curved surfaces. This leads to the recess **58** in said cross section tapering radially outward. In the first region **62a**, **62b**, the two side flanks **60a**, **60b** are therefore at a greater distance $d_{sub.1}$ than in the second region **64a**, **64b**. In the second region **64a**, **64b**, the two side flanks **60a**, **60b** of the recess **58** are at a second distance $d_{sub.2}$ from each other which is smaller than the first distance $d_{sub.1}$.

(41) In the radially inner first region **62a**, **62b**, the two side flanks **60a**, **60b** preferably each have a planar drive surface **66a**, **66b**, the drive surfaces serving as counterparts to the drive surfaces **34a**, **34b** which are arranged laterally on the anti-rotation element **28**. The superstructure **20** preferably lies on the anti-rotation element **28** only by said two mutually opposite drive surfaces **66a**, **66b**. In a similar manner to the drive surfaces **34a**, **34b** acting as a counterpart, the planar drive surfaces **66a**, **66b** run parallel to each other and parallel to the longitudinal axis **54** of the superstructure.

(42) Radially further outward, each side flank **60a**, **60b** in each case has a concavely curved surface **68a**, **68b**. The concavely curved surfaces **68a**, **68b** are preferably directly adjacent to the drive surfaces **66a**, **66b** of the respective side flank **60a**, **60b** and merge tangentially into them. In the mounted state of the dental prosthesis **100**, the concavely curved surfaces **68a**, **68b** protrude at least partially into the cavity **32** which is formed behind the anti-rotation element **28** between the radially outer side **30** thereof and the inner lateral surface **26** of the dental implant **10**.

(43) Apart from the recess **58**, the interface **48** provided on the superstructure **20** is (rotationally) symmetrical with respect to the longitudinal axis **54**. The opening **52** accordingly preferably runs centrally through the extension **50** forming the interface **48**. The entire interface **48** is therefore preferably also mirror-symmetrical with respect to a longitudinal sectional plane $E_{sub.2}$ which is spanned by the longitudinal axis **54** and a radial direction **70** running orthogonally with respect thereto and divides the recess **58** into two halves of identical size (see FIG. **6**).

(44) In addition to the extension 50, the interface 48 of the superstructure 20 has a support surface 72 which surrounds the extension 50. Said circular-ring-shaped support surface 72 is used as a counterpart to the circular-ring-shaped support surface 44 arranged on the dental implant. In the present exemplary embodiment, it is therefore configured as a conical surface, but, as mentioned previously, may also be oriented orthogonally with respect to the longitudinal axis 54 of the superstructure 20.

Claims

1. A dental implant, comprising: an external thread arranged on an outer side of the dental implant for fixing the dental implant to a jaw bone; an opening extending along a central longitudinal axis of the dental implant and comprising an internal thread for fixing a superstructure to the dental implant; an interface configured for fixing the superstructure to the dental implant, the interface being arranged in a region of an end face of the dental implant and comprising an inner surface that is arranged in the opening and at least partially surrounds the longitudinal axis; and an anti-rotation element arranged in the opening and configured to prevent the superstructure from rotating about the longitudinal axis relative to the dental implant, wherein the anti-rotation element is at a shorter distance from the longitudinal axis than the inner surface, wherein a radially outer side of the anti-rotation element that faces away from the longitudinal axis faces the inner surface and is spaced apart from the inner surface such that there is an open cavity between the radially outer side of the anti-rotation element and the inner surface, wherein the anti-rotation element has a convex-concave shape in a cross section that is oriented orthogonally to the longitudinal axis, wherein a radially inner side of the anti-rotation element facing the opening has concave shape, and the radially outer side of the anti-rotation element opposite the radially inner side has a convex shape, and wherein the anti-rotation element comprises two planar drive surfaces extending parallel to each other, the two planar drive surfaces being arranged on opposite sides of the anti-rotation element and extending transversely and between the radially outer side and the radially inner side of the anti-rotation element.
2. The dental implant as claimed in claim 1, wherein the open cavity tapers downward, as viewed in a longitudinal section of the dental implant, such that a first distance between the radially outer side of the anti-rotation element and the inner surface, as measured in the longitudinal section at an open upper end of the cavity, is greater than a second distance between the radially outer side of the anti-rotation element and the inner surface, as measured in the longitudinal section at a lower end of the cavity.
3. The dental implant as claimed in claim 1, wherein each of the two planar drive surfaces extends parallel to a radial direction that is oriented orthogonally to the longitudinal axis.
4. The dental implant as claimed in claim 1, wherein the anti-rotation element has a constant wall thickness.
5. The dental implant as claimed in claim 1, wherein the anti-rotation element is oriented parallel to the longitudinal axis.
6. The dental implant as claimed in claim 1, wherein the interface is mirror-symmetrical with respect to a longitudinal sectional plane in which the longitudinal axis lies and which divides the anti-rotation element into two halves of identical size.
7. The dental implant as claimed in claim 1, wherein the inner surface comprises a curved surface that is curved convexly in a longitudinal section in which the longitudinal axis lies.
8. The dental implant as claimed in claim 1, wherein the interface comprises a support surface that is arranged radially further outward than the inner surface, wherein the support surface extends around the longitudinal axis and is, all around the longitudinal axis, oriented at a constant angle transversely with respect to the longitudinal axis.
9. The dental implant as claimed in claim 8, wherein a radially outer edge of the inner surface

merges tangentially into the support surface.

10. The dental implant as claimed in claim 1, wherein the internal thread is at a greater distance from the end face than the anti-rotation element.

11. A dental prosthesis, comprising: a dental implant; a superstructure; and a fastening element configured to fasten the superstructure to the dental implant, the dental implant comprising: an external thread arranged on an outer side of the dental implant for fixing the dental implant to a jaw bone; an opening extending along a central longitudinal axis of the dental implant and comprising an internal thread in which the fastening element engages; an interface being arranged in a region of an end face of the dental implant and comprising an inner surface that is arranged in the opening and at least partially surrounds the longitudinal axis; and an anti-rotation element arranged in the opening and configured to prevent the superstructure from rotating about the longitudinal axis relative to the dental implant, wherein the anti-rotation element is at a shorter distance from the longitudinal axis than the inner surface, wherein a radially outer side of the anti-rotation element that faces away from the longitudinal axis faces the inner surface and is spaced apart from the inner surface such that there is an open cavity between the radially outer side of the anti-rotation element and the inner surface, wherein the anti-rotation element has a convex-concave shape in a cross section that is oriented orthogonally to the longitudinal axis, wherein a radially inner side of the anti-rotation element facing the opening has concave shape, and the radially outer side of the anti-rotation element opposite the radially inner side has a convex shape, and wherein the anti-rotation element comprises two planar drive surfaces extending parallel to each other, the two planar drive surfaces being arranged on opposite sides of the anti-rotation element and extending transversely and between the radially outer side and the radially inner side of the anti-rotation element.

12. The dental prosthesis as claimed in claim 11, wherein the open cavity tapers downward, as viewed in a longitudinal section of the dental implant, such that a first distance between the radially outer side of the anti-rotation element and the inner surface, as measured in the longitudinal section at an open upper end of the cavity, is greater than a second distance between the radially outer side of the anti-rotation element and the inner surface, as measured in the longitudinal section at a lower end of the cavity.

13. The dental prosthesis as claimed in claim 11, wherein each of the two planar drive surfaces extends parallel to a radial direction that is oriented orthogonally to the longitudinal axis.

14. The dental prosthesis as claimed in claim 11, wherein the anti-rotation element has a constant wall thickness.
