
Modeling Biological Neural Networks

Kai Deng

April 6, 2024

CONTENTS

1. Introduction	3
2. Background Context	3
2.1. Anatomy of a Neuron	3
2.2. Physiology of a Neuron	4
2.3. Spike train	6
3. Historical Models	6
3.1. The M-P model	6
3.2. Hebb learning rules	8
3.3. Hodgkin–Huxley model	8
3.4. Mark I perceptron	10
3.5. Delta learning rules	12
3.6. Hopfield neural network model	12
3.7. Boltzmann machine	14
4. Hodgkin-Huxley Model	14
4.1. Introduction	14
4.1.1. Historical Background	14
4.2. Biological Basis of Neuronal Excitability	15
4.2.1. Resting Membrane Potential	15
4.2.2. Generation of Action Potentials	16
4.2.3. Propagation of Action Potentials	16
4.2.4. Repolarization and Hyperpolarization	16

4.3. Formulation of the Hodgkin-Huxley Model	16
4.3.1. Electrical Circuit Representation	16
4.3.2. The Hodgkin-Huxley Equation	17
4.4. Python Simulation	19
4.4.1. Simulation Results	19
5. Applications	25
A. Python Code	28

1. INTRODUCTION

Biological neural networks are the complex systems of neurons and their connections in organisms, crucial for processing and transmitting information, enabling perception, decision-making, and behavior. Modeling these networks through computational frameworks aims to replicate their structure and function, shedding light on how information processing leads to complex cognitive functions and behaviors. In the following we will show you how Modeling Biological Neural Networks works.

2. BACKGROUND CONTEXT

Neurons are cells — small bodies of mostly water, ions, amino acids and proteins with remarkable electrochemical properties. They are the primary functional units of the brain. Our mental experiences — our perceptions, memories, and thoughts — are the result of the ebb and flow of salts across neural bi-lipid membranes and the synaptic transmissions between neurons.

2.1. ANATOMY OF A NEURON

Neurons receive signals from other neurons through synapses located – not exclusively – on their dendritic tree, which is a complex, branching, sprawling structure. If you are wondering what the king of dendritic complexity is, that would be the Purkinje cell, which may receive up to 100,000 other connections. Dendrites are studded with dendritic spines – little bumps where other neurons make contact with the dendrite.

Signals from the dendrites propagate to and converge at the soma – the cell's body where nucleus and other typical cell organelles live.

Coming off the soma is the axon hillock which turns into the axon. The axon meets other neurons at synapses. It allows a neuron to communicate rapidly over long distances without losing signal integrity. To allow signals to travel rapidly, the axon is myelinated – it is covered with interspersed insulators which allows the neuron's signal to jump between insulated sections. To allow the signal to maintain integrity, the neuron signal in the axon is 'all-or-nothing' – it is a rather bit-like impulse, which we will discuss next.

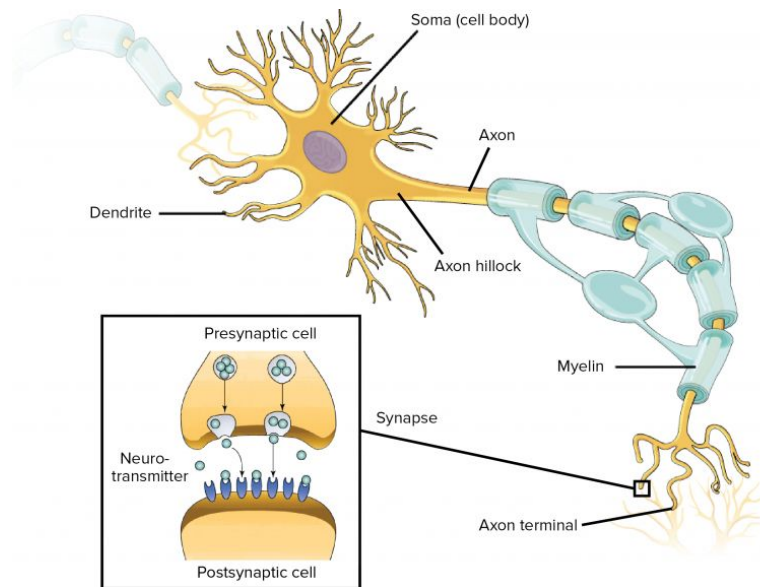


Figure 2.1: Anatomy of the neuron

Source: Source:“Neurons and glial cells” by OpenStax College, Biology CC BY-NC-SA 3.0 License.

2.2. PHYSIOLOGY OF A NEURON

THE second thing to appreciate about neurons is their specialized physiology — that is the cellular functions of neurons. The most striking feature of neural cellular function is the action potential. This is the mechanism which allows neurons to transmit information reliably over long distances without the transmission attenuating.

It is important to remember that neurons bathe in an extracellular solution of mostly water, salts and proteins. The forces caused by the movement of salts into and out of the cell and the different concentrations of these salts is the physical basis of the neuron’s remarkable behavior. There are sodium-potassium pumps which move sodium out of the cell and potassium in, so that the concentration of sodium outside the cell is higher than inside and the concentration of potassium outside the cell is lower then inside.

An action potential is a discrete event in which the membrane potential rapidly rises (depolarizes) and then falls (polarizes). This discrete event is all-or-nothing, meaning that if an action potential occurs at one part of the neurons membrane, it will also occur in the neighboring part, and so on until it reaches the axon terminal. Action potentials do not tend to travel backwards, because, once a section of the membrane has fired an action potential, electrochemical-forces hyper-polarize the region of membrane while the channels which were previously open close and become inactive for some duration of time.

The action potential is the result of different species of ions traveling across the cell membrane through channels and the activation and inactivation of those channels on different

time scales. A stereotypical action potential occurs as follows:

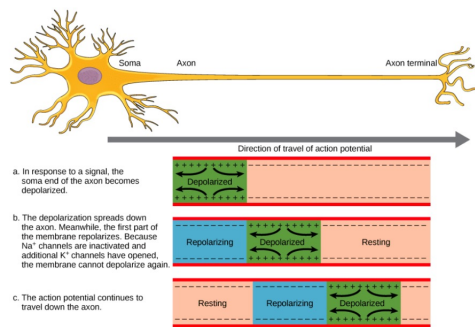


Figure 2.2: Propagation of nerve impluse

Source: [Opentext](#)

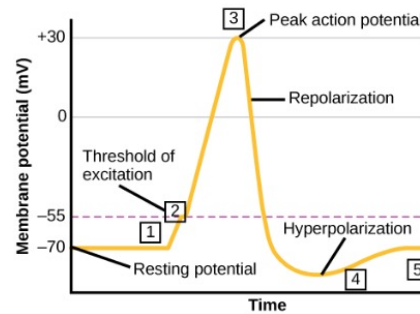


Figure 2.3: Neuronal action potential

Source: [Opentext](#)

- **Equilibrium:** The neuron's equilibrium membrane potential is near -70 mV — roughly the Nernst Equilibrium of $E_{K^+} \approx -75$. At equilibrium, the net current is 0 — inward and outward currents are balanced.
- **Depolarization:** Incoming excitatory signals depolarize the membrane. Quick-to-respond voltage gated Na^+ channels are activated, and Na^+ rushes in, pushing the membrane potential higher. Slower-to-respond K^+ channels open, and K^+ rushes out, pushing the membrane potential lower.
- **Amplification:** If the neuron becomes more stimulated or is stimulated rapidly, many more Na^+ channels are activated than K^+ channels. This causes a feedback loop where the influx of Na^+ causes more Na^+ channels to activate.
- **Repolarization:** Eventually the membrane potential is near the Nernst Equilibrium of Na^+ as the sodium channels are maximally open. The slower K^+ channels catch up to Na^+ , which repolarizes the membrane potential. Meanwhile, the Na^+ channels become inactive.
- **Hyper-polarization:** K^+ channels are open while Na^+ channels are inactive, causing the membrane potential to dip below its typical equilibrium point, near the K^+ Nernst equilibrium.
- **Refractory Period:** The Na^+ channels, take a while to become deinactivated, meaning after an action potential, they remain incapable of opening again for a period of time. The period in which most Na^+ channels are called the absolute refractory period (the neuron cannot spike no matter the strength of the stimulus) while the period in which many Na^+ channels are inactivated is called the relative refractory period (the neuron can spike given a sufficiently strong stimulus).

2.3. SPIKE TRAIN

Spike trains are the language of neurons. People tend to think of spikes as point-events and spike trains as point-processes. We describe these with the neural response function:

$$\rho(t) = \sum_{i=1}^k \delta(t - t_i) \quad (2.1)$$

where an impulse is defined as the dirac delta function (which is convenient for counting things):

$$\delta(t) = \begin{cases} 1 & \text{if } t = 0, \\ 0 & \text{otherwise} \end{cases} \quad (2.2)$$

Often, it is useful for analysis to assume spike trains are generated by random processes. Assuming spikes are independent of each other, we can model this point process as a Poisson process, in which we know the probability n spikes occur in the interval ΔT :

$$P\{n \text{ spikes occur in } \Delta t\} = \frac{(r \Delta t)^n}{n!} \exp(-r \Delta t) \quad (2.3)$$

To generate spikes according to a Poisson point process, generate a random number r in a sufficiently small time interval, such that only 1 spike should occur, and check whether $r < \text{firingRate} \Delta T$. However, make sure that $\text{firingRate} \Delta T < 1$.

3. HISTORICAL MODELS

3.1. THE M-P MODEL

Since the Spanish anatomist Cajal founded the neuron theory at the end of the 19th century, the biological characteristics and related electrical properties of neurons have been discovered one after another. In 1943, the M-P model of neurons (shown in Figure 1.4) was first proposed in the paper "Logical Activities of Thoughts Contained in Neural Activities" [1]. The model was created by psychologists W.S. McCulloch and W.S. McCulloch from the United States. Another mathematician, W.A. Pitts.

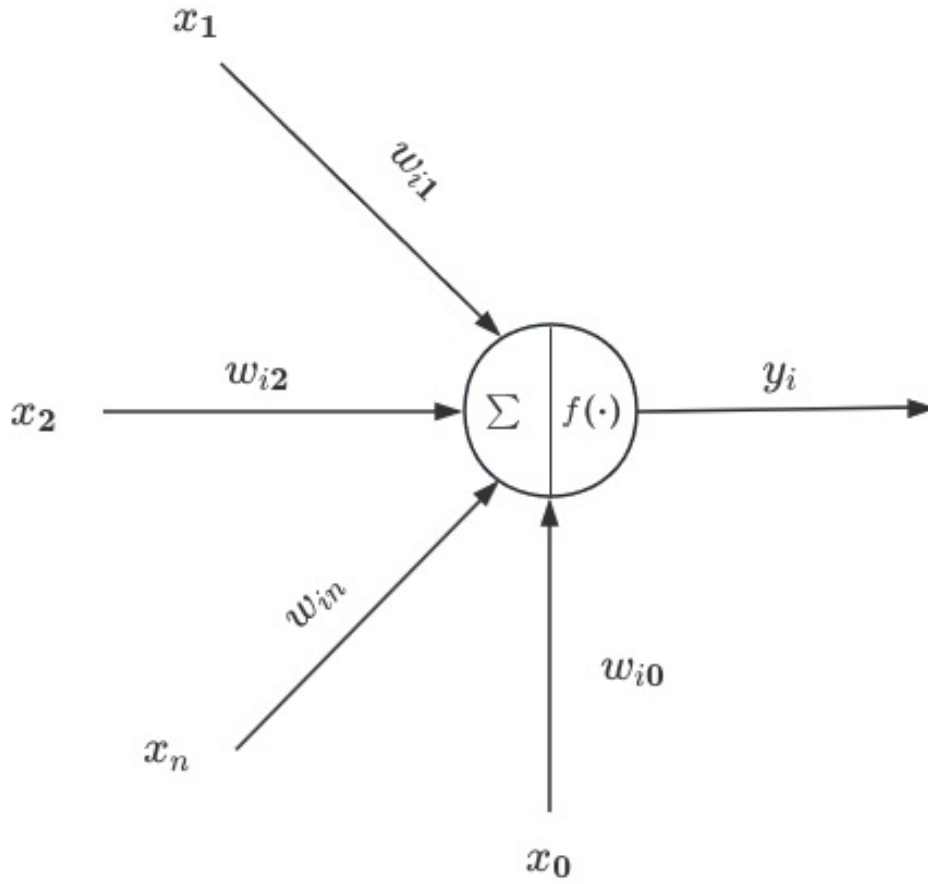


Figure 3.1: Schematic diagram of the M-P model of neurons

In the figure, x_i , 1, 2, ..., represents the input signal transmitted from other neurons connected to the current neuron, w_{ij} represents the connection strength or weight from neuron j to neuron i , θ_i is the neuron The activation threshold or bias of the element, f is called the activation function or transfer function. The output of the neuron y_i can be expressed as follows:

$$y_i = f\left(\sum_{j=1}^n w_{ij}x_j - \theta_i\right) \quad (3.1)$$

This model describes neurons from the perspective of logical functional devices, opening up a path for theoretical research on neural networks. The M-P model is a mathematical simplification of the biological neuron information processing model, and subsequent neural network research work is based on it.

3.2. HEBB LEARNING RULES

In 1949, in the book "The Organization of Behavior", the psychologist Donald O. Hebb analyzed the change rules of the connection strength between neurons, and based on this, he proposed the famous Hebb learning rule [2]. Inspired by Pavlov's conditioned reflex experiments, Hebb believed that if two neurons are fired at the same moment, the connection between them should be strengthened. The Hebb learning rule defined based on this is as follows:

$$w_{ij}(t+1) = w_{ij}(t) + \alpha y_j(t) y_i \quad (3.2)$$

Among them, $w_{ij}(t+1)$ and $w_{ij}(t)$ represent the connection strength between neuron j and neuron i at time t and $t+1$ respectively, while y_i and y_j are the outputs of neurons i and j .

Hebb's rule belongs to the category of unsupervised learning algorithms. Its main idea is to adjust the connection relationship between two neurons according to their excitation state, so as to realize the simulation of simple neural activities. Following the Hebb learning rule, the supervised delta learning rule of neurons was proposed to solve the learning problem of neuron weights when the input and output are known. This algorithm continuously adjusts the connection weights to make the actual output of the neuron consistent with the expected output. Its learning correction formula is as follows

$$w_{ij}(t+1) = w_{ij}(t) + \alpha(d_i - y_i)x_j(t) \quad (3.3)$$

Among them, α is the learning rate of the algorithm, d_i and y_i are the expected output and actual output of neuron i , x_j represents the state (activation or inhibition) of neuron j at time t .

Intuitively speaking, when the actual output of neuron i is greater than the expected output, the connection weight with the activated neuron is reduced, and the connection weight with the inhibited neuron is increased; when the actual output of neuron i is smaller than the expected output, the connection weight with activated neurons will be increased, while the connection weight with inhibited neurons will be reduced. Through such an adjustment process, neurons will store the correct mapping relationship between input and output in the weight, thus possessing the ability to represent data. The Hebb learning rule and the Delta learning rule are both proposed for a single neuron. The learning rules for parameters in a network composed of neurons will be discussed later. The research work done by the above pioneers paved the way for the emergence of neural computing and inspired many scholars to continue exploring and researching this field.

3.3. HODGKIN-HUXLEY MODEL

The Hodgkin-Huxley model, or conductance-based model, is a mathematical model that describes how action potentials in neurons are initiated and propagated [3]. It is a set of nonlinear differential equations that approximates the electrical engineering characteristics of excitable cells such as neurons and muscle cells. It is a continuous-time dynamical system.

The typical Hodgkin–Huxley model treats each component of an excitable cell as an electrical element (as shown in the figure). The lipid bilayer is represented as a capacitance (C_m). Voltage-gated ion channels are represented by electrical conductances (g_n , where n is the specific ion channel) that depend on both voltage and time. Leak channels are represented by linear conductances (g_L). The electrochemical gradients driving the flow of ions are represented by voltage sources (E_n) whose voltages are determined by the ratio of the intra- and extracellular concentrations of the ionic species of interest. Finally, ion pumps are represented by current sources (I_p).

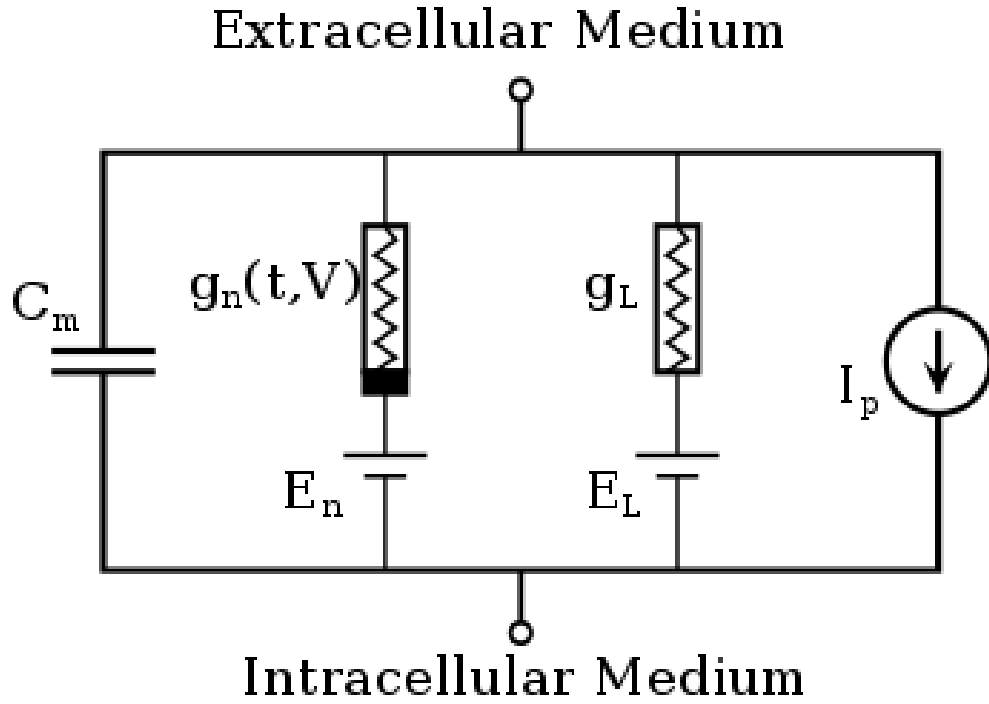


Figure 3.2: Typical Hodgkin–Huxley model

Source: [Wikipedia](#)

Mathematically, the current flowing through the lipid bilayer is written as:

$$I_c = C_m \frac{dV_m}{dt} \quad (3.4)$$

The current through a specific ion channel:

$$I_i = g_i(V_m - V_i) \quad (3.5)$$

For a cell with sodium and potassium channels, the total membrane current per unit area (I) is given by:

$$I = C_m \frac{dV_m}{dt} + g_K(V_m - V_K) + g_{Na}(V_m - V_{Na}) + g_l(V_m - V_l) \quad (3.6)$$

Where:

- I : is the total membrane current per unit area.
- C_m : is the membrane capacitance per unit area.
- g_K and g_{Na} : are the potassium and sodium conductances per unit area, respectively.
- V_K and V_{Na} : are the potassium and sodium reversal potentials, respectively.
- g_l and V_l : are the potassium and sodium reversal potentials, respectively.

The time-dependent elements of this equation are V_m , g_{Na} , and g_K , where the last two conductances depend explicitly on the membrane voltage (V_m) as well.

3.4. MARK I PERCEPTRON

In 1958, F. Rosenblatt invented the perceptron model (Perceptron), which was the first model in history to introduce the concept of neural networks into electronic computer processing, marking a new stage in the development of neural networks [4]. The perceptron is a binary linear classification model that determines the output of a two-class model by weighted summation of the input features followed by an activation function. The activation function is a step function, used to determine whether the input value is positive or negative. The mathematical representation of the perceptron model is as follows, where x represents the input vector, w represents the weight vector, b represents the bias term, and y is the output value, which can be +1 or -1, with the mathematical representation being:

$$y = f(x) = \text{sign}(w \cdot x + b) \quad (3.7)$$

Here, $w \cdot x$ represents the dot product of vectors w and x , and the definition of the sign function is as follows:

$$\text{sign}(x) = \begin{cases} +1, & \text{if } x \geq 0 \\ -1, & \text{if } x < 0 \end{cases} \quad (3.8)$$

The perceptron learning algorithm is based on the principle of reducing the error of classification. When the classification result is incorrect, it adjusts the weights and biases, thus improving the classification ability step by step. The perceptron learning algorithm aims to find the weights and biases that minimize the classification error. Let's define a training set $T = \{(x_1, y_1), (x_2, y_2), \dots, (x_n, y_n)\}$, where x_i is the input vector and y_i is the corresponding output. The goal of the perceptron learning algorithm is to minimize the loss function $L(w, b)$:

$$L(w, b) = - \sum_{x_i \in M} y_i (w \cdot x_i + b) \quad (3.9)$$

where M is the set of misclassified examples. The perceptron updates the weights w and bias b to minimize $L(w, b)$:

$$\min_{w,b} L(w, b) = - \sum_{x_i \in M} y_i (w \cdot x_i + b) \quad (3.10)$$

The gradient descent method is used to update the weights and biases, which aims to adjust the weights and biases in the opposite direction of the gradient of the loss function. The updates for weights w and bias b are as follows:

$$\nabla_w L(w, b) = - \sum_{x_i \in M} x_i \cdot y_i \quad (3.11)$$

$$\nabla_b L(w, b) = - \sum_{x_i \in M} y_i \quad (3.12)$$

Therefore, each time an example (x_i, y_i) is misclassified, the weights w and bias b are updated as follows:

$$w_{\text{new}} = w_{\text{old}} + \eta y_i x_i \quad (3.13)$$

$$b_{\text{new}} = b_{\text{old}} + \eta y_i \quad (3.14)$$

where η is the learning rate, a positive constant determining the size of the update step.

In the algorithm, $0 < \eta \leq 1$ is the learning rate. It determines the size of the adjustment to the weights during the learning process. When the perceptron classifies an example correctly, the weights and bias are not adjusted. When it misclassifies an example, it adjusts the weights and bias towards the direction that could possibly correct the error. This process is not changed until all examples are classified correctly, or the process reaches a preset number of iterations. According to the update rules from equations (10) and (11), the weights w and bias b are adjusted as follows:

$$w = \sum_{i=1}^n a_i y_i x_i \quad (3.15)$$

$$b = \sum_{i=1}^n a_i y_i \quad (3.16)$$

where $a_i = \eta n_i$, and n_i is the number of times the perceptron misclassified the i -th example. The perceptron algorithm is named after the psychologist Frank Rosenblatt, who, along with engineers B. Widrow and M. Hoff, adapted the ADALINE (ADaptive LINear Element) from the model of the same name developed by H. Steinbuch.

3.5. DELTA LEARNING RULES

The basic idea of the delta learning rule is to reduce the difference between the network output and the target output by continuously adjusting the network weights. It determines the adjustment direction and size of the weight by calculating the gradient of the error. At each iteration, the weights are adjusted slightly in the opposite direction of the gradient to gradually reduce the error. A common delta learning rule is a variant of the delta rule, called the delta rule or Widrow-Hoff rule [5]. This rule is based on the perceptron model and updates the weights based on the difference between the actual output and the desired output. The size of the update depends on the size of the input signal as well as the error signal.

The Delta learning rule, also known as the Widrow-Hoff rule, is a simple algorithm used for adjusting the weights of connections in a neural network during training. The formula for updating the weights in the Delta learning rule is as follows:

$$\Delta w_{ij} = \eta \cdot (d_j - y_j) \cdot x_i$$

Where:

- Δw_{ij} : is the change in weight between neuron i and neuron j .
- η : is the learning rate, which controls the step size of the weight update.
- d_j : is the target output for neuron j .
- y_j : is the actual output of neuron j .
- x_i : is the input from neuron i to neuron j .

This formula calculates the change in weight Δw_{ij} based on the error between the target output d_j and the actual output y_j , multiplied by the input x_i and the learning rate η . The weight update is applied to all connections in the network during each training iteration.

Delta learning rules are widely used in neural network training, especially in supervised learning tasks such as classification and regression. It provides an effective method for neural networks to automatically adjust weights to gradually improve the performance and accuracy of the network.

3.6. HOPFIELD NEURAL NETWORK MODEL

The next significant advancement in the field of neural networks occurred in 1969 when M. Minsky and S. Papert pointed out the limitations of the perceptron in their book "Perceptrons," demonstrating that it was incapable of processing the XOR problem. However, this criticism also motivated further research into neural networks with additional layers, leading to the development of multilayer networks. The key breakthrough was the introduction of the "backpropagation" algorithm that enabled the training of multilayer networks.

A single-layer perceptron can only solve problems linearly separable because it is essentially a linear classifier. It was realized that to overcome the limitations of the perceptron and solve non-linearly separable problems, one must utilize multilayer networks and non-linear

activation functions. The first step in this direction was taken by introducing the concept of a neural network capable of associative memory, which led to the invention of the Hopfield network by J.J. Hopfield in 1982.

The Hopfield network, an energy-based model, is particularly known for solving the Travelling Salesman Problem (TSP). It opened new avenues for using neural networks in optimization problems beyond the domain of traditional computation.

Hopfield's work not only advanced the theoretical foundations of neural networks but also laid the groundwork for the development of modern neural networks, which are capable of learning complex patterns and solving diverse problems. This laid the foundation for significant strides in the field of neural networks, inspiring subsequent developments.

The Hopfield network is characterized by its feedback loops as shown in the figure. In the network, the output of each neuron is fed back into itself and other neurons through a set of resistors. Each neuron has a resistance R_i and a capacitance C_i , and is connected to other neurons via resistors R_{ij} (where $i, j = 1, 2, \dots, n; i \neq j$). Each neuron's voltage U_i changes according to the charge Q_i and its voltage is fed back to itself through a resistor R_i , and to other neurons through resistors R_{ij} , ($i, j = 1, 2, \dots, n$) with different resistances. The network follows Kirchhoff's Current Law (KCL), and the voltage change at each neuron is described by the following equation:

$$\sum_{j=1}^n \frac{V_j(t)}{R_j} + I_i = C_i \frac{dU_i(t)}{dt} + \frac{U_i(t)}{R_i}, \quad i = 1, 2, \dots, n \quad (3.17)$$

However, in a Hopfield network, each neuron's voltage is modified by an activation function f to produce an output V_i :

$$V_i(t) = f_i(U_i(t)), \quad i = 1, 2, \dots \quad (3.18)$$

Then, the state energy of a Hopfield network is defined as:

$$W = R_{i,j}^{-1}(i, j = 1, 2, \dots, n) \quad (3.19)$$

where R'_i are the weights of the network. The energy function of the Hopfield network is given by:

$$E(t) = -\frac{1}{2} \sum_{i=1}^n \sum_{j=1}^n \frac{V_i(t)V_j(t)}{R_{ij}} - \sum_{i=1}^n V_i(t)I_i + \sum_{i=1}^n \frac{1}{R_i} \int_0^{V_i(t)} f^{-1}(V) dV \quad (3.20)$$

Finally, a Hopfield network adjusts its state iteratively to minimize the energy function $E(U)$, which leads to stable states—these are the solutions to the problem that the network is trying to solve. The dynamics of a Hopfield network's voltage adjustment towards stable states is analogous to the process of a physical system reaching its lowest energy state.

The Hopfield network is a recurrent neural network, which is to say, it possesses feedback loops. This feature allows it to have dynamic memory. Dynamic memory is different from the static memory seen in the perceptron, which only allows for the storage of a fixed set of patterns. The Hopfield network can store a variety of patterns and retrieve them based on the input, making it a form of associative memory.

Hopfield's paper not only triggered the renaissance of interest in neural networks but also led to the exploration of new types of neural networks. One significant development in this area was the Boltzmann machine, introduced by G.E. Hinton, T.J. Sejnowski, and D.H. Ackley in 1983. This machine was an extension of the Hopfield network and could solve problems that Hopfield networks could not.

3.7. BOLTZMANN MACHINE

A Boltzmann machine is similar to a Hopfield network in that it is a network of units with a global energy function [7]. However, unlike the Hopfield network, a Boltzmann machine has stochastic units and operates based on probabilistic rather than deterministic rules. This means that a Boltzmann machine can escape from local minima, a feature that is particularly beneficial when dealing with optimization problems.

A special case of the Boltzmann machine is the Restricted Boltzmann Machine (RBM), which constrains the connections between units to form a bipartite graph. This constraint simplifies the learning algorithm and makes it more efficient. RBMs have found a wide range of applications, particularly in the development of deep learning algorithms. For instance, they can be used to pre-train the layers of a deep neural network, improving the efficiency and effectiveness of the training process.

The collaborative work of Hinton and his colleagues on Boltzmann machines and the development of efficient training algorithms have played a vital role in the evolution of neural networks. Their work has paved the way for the deep learning revolution, which is now at the forefront of artificial intelligence research and applications.

4. HODGKIN-HUXLEY MODEL

4.1. INTRODUCTION

The Hodgkin-Huxley model, proposed by Sir Alan Hodgkin and Sir Andrew Huxley in 1952, revolutionized the field of neuroscience by providing a quantitative understanding of the generation and propagation of action potentials in neurons. This mathematical framework emerged from a decade-long collaboration between Hodgkin and Huxley, culminating in the publication of their landmark papers in the *Journal of Physiology*.

4.1.1. HISTORICAL BACKGROUND

The Hodgkin-Huxley theory emerged as a result of a remarkable collaboration between Hodgkin and Huxley from the late 1930s to the early 1950s. Their work was informed by several key experimental findings. Cole and Curtis demonstrated that the action potential is associated with a significant increase in membrane conductance, laying the groundwork for understanding neuronal excitability[1]. Subsequently, Hodgkin and Huxley performed the first intracellular recording of an action potential, revealing that the membrane potential during an action potential exceeds zero mV, thereby challenging existing hypotheses[2]. This experimental breakthrough was complemented by the theoretical insights of Hodgkin

and Katz, who explained the overshooting action potential by elucidating the role of sodium permeability[3]. Additionally, Hodgkin, Huxley, and Katz developed a voltage-clamp circuit, following the pioneering work of Cole and Marmont, enabling precise measurement of ionic currents in squid axons[5].

4.2. BIOLOGICAL BASIS OF NEURONAL EXCITABILITY

Neuronal excitability, the ability of neurons to generate and transmit electrical signals, is fundamental to their function in the nervous system. This excitability arises from the intricate interplay of ion channels and the dynamic changes in membrane potential they produce.

4.2.1. RESTING MEMBRANE POTENTIAL

The resting membrane potential of a neuron, typically ranging from -60 mV to -70 mV, is maintained by the selective permeability of the cell membrane to different ions. This selective permeability is primarily mediated by resting ion channels, particularly those permeable to potassium ions. At rest, these channels allow a small efflux of K^+ ions, establishing the negative charge within the cell compared to the extracellular space.

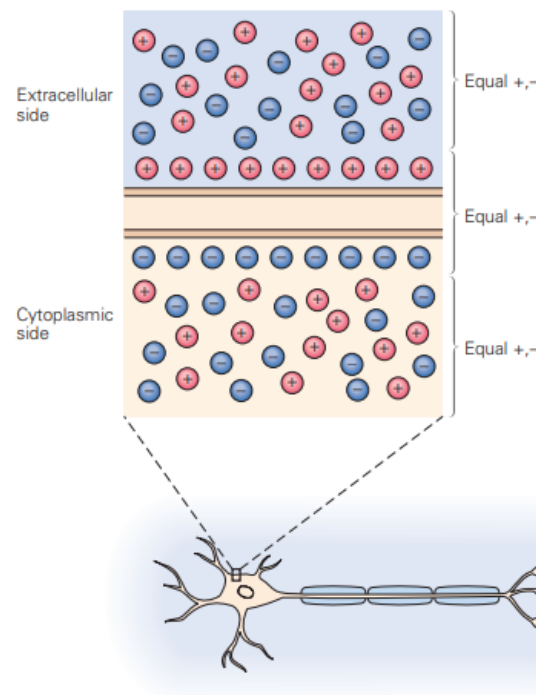


Figure 4.1: Resting membrane potential (Source: Principles of Neural Science[6])

4.2.2. GENERATION OF ACTION POTENTIALS

Action potentials, the transient electrical signals responsible for rapid communication within the nervous system, are generated when the membrane potential depolarizes beyond a certain threshold. This depolarization is initiated by the opening of voltage-gated sodium channels in response to a stimulus. As Na^+ ions rush into the cell, the membrane potential becomes more positive, reaching around +40 mV.

4.2.3. PROPAGATION OF ACTION POTENTIALS

Once initiated, the action potential propagates along the axon of the neuron. This propagation occurs through a self-regenerating process where the depolarization of one region of the membrane triggers the opening of voltage-gated sodium channels in the adjacent region, leading to further depolarization. This continues along the length of the axon, allowing the action potential to travel rapidly towards the synapse.

4.2.4. REPOLARIZATION AND HYPERPOLARIZATION

Following depolarization, the membrane potential undergoes repolarization, returning to its resting state. This repolarization is driven by the opening of voltage-gated potassium channels, allowing K^+ ions to exit the cell, while voltage-gated sodium channels undergo inactivation. In some cases, repolarization may overshoot, leading to hyperpolarization, before eventually returning to the resting membrane potential[6].

4.3. FORMULATION OF THE HODGKIN-HUXLEY MODEL

The Hodgkin-Huxley model provides a quantitative description of membrane currents and their role in nerve conduction and excitation. Central to this model is the representation of the neuronal membrane as an electrical circuit, which captures the dynamics of ion flow across the membrane during the generation and propagation of action potentials.

4.3.1. ELECTRICAL CIRCUIT REPRESENTATION

In the Hodgkin-Huxley model, the neuronal membrane is represented as an electrical circuit composed of several components.

Membrane Capacitance (C): The lipid bilayer of the neuronal membrane acts as a capacitor, storing charge and contributing to the membrane's ability to maintain a voltage gradient.

Ion Channels: Voltage-gated ion channels, including sodium (Na^+), potassium (K^+), and leak channels, are represented as resistors in the circuit. These channels control the flow of ions across the membrane in response to changes in membrane potential.

Battery (E_m): The battery in the circuit represents the resting membrane potential, which is typically around -60 to -70 mV in neurons. It serves as the reference voltage against which changes in membrane potential are measured.

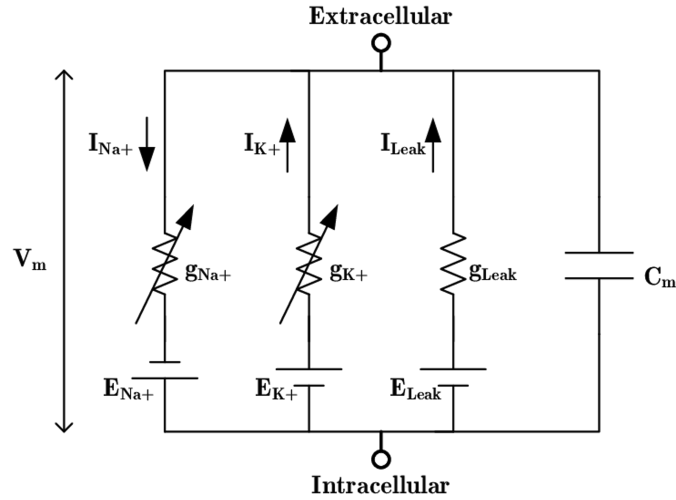


Figure 4.2: Electrical circuit representing membrane. (Source: A quantitative description of membrane current and its application to conduction and excitation in nerve[4])

4.3.2. THE HODGKIN-HUXLEY EQUATION

The Hodgkin-Huxley model provides a quantitative description of membrane current and its application to conduction and excitation in nerve cells. It represents the dynamic interplay of ion channels and membrane capacitance in generating and propagating action potentials.

The model is formulated based on the principles of electrical circuits. The total current in the neuron can be expressed as the sum of the individual ion currents and the capacitive current:

$$I_{\text{Total}} = I_{\text{Na}} + I_{\text{K}} + I_{\text{leak}} + I_{\text{C}}$$

Using the relationship between charge (Q), capacitance (C), and potential difference (V):

$$C = \frac{Q}{V}$$

We can express the capacitive current (I_{C}) as the rate of change of charge with respect to time:

$$C \frac{dV}{dt} = I_{\text{Total}} - I_{\text{Na}} - I_{\text{K}} - I_{\text{leak}}$$

Applying Ohm's law ($I = \frac{V}{R}$), where R is the resistance, to each ion current:

$$I = \frac{1}{R} \times V$$

We can modify this to incorporate the reversal potential (E):

$$I = \frac{1}{R} \times (V - E)$$

Substituting these into the equation for the capacitive current:

$$C \frac{dV}{dt} = I_{\text{Total}} - \frac{1}{R_{\text{Na}}} \times (V_m - E_{\text{Na}}) - \frac{1}{R_{\text{K}}} \times (V_m - E_{\text{K}}) - \frac{1}{R_{\text{leak}}} \times (V_m - E_{\text{leak}})$$

Where V_m represents the membrane potential, and E_{Na} , E_{K} , and E_{leak} represent the equilibrium potentials for sodium, potassium, and leak currents respectively.

Expanding the equation using the Hodgkin-Huxley model for the conductance of each ion (g) and the gating variables (m , h , n):

$$C \frac{dV}{dt} = I_{\text{Total}} - g_{\text{Na}} m^3 h (V_m - E_{\text{Na}}) - g_{\text{K}} n^4 (V_m - E_{\text{K}}) - g_{\text{leak}} (V_m - E_{\text{leak}})$$

Where

$$\frac{dm}{dt} = -\frac{(m - m_{\infty}(V))}{\tau_m(V)}, \quad \frac{dh}{dt} = -\frac{(h - h_{\infty}(V))}{\tau_h(V)}, \quad \frac{dn}{dt} = -\frac{(n - n_{\infty}(V))}{\tau_n(V)}$$

represent the gating variable dynamics.

- The equation $\frac{dm}{dt} = -\frac{(m - m_{\infty}(V))}{\tau_m(V)}$ represents the dynamics of the gating variable m .
 - m represents the activation gating variable for sodium channels.
 - $m_{\infty}(V)$ is the steady-state value of m at membrane potential V , which describes the fraction of sodium channels that are open.
 - $\tau_m(V)$ is the time constant associated with the activation gating variable m , which determines how quickly m changes with respect to time.
- Similarly, the equation $\frac{dh}{dt} = -\frac{(h - h_{\infty}(V))}{\tau_h(V)}$ represents the dynamics of the gating variable h .
 - h represents the inactivation gating variable for sodium channels.
 - $h_{\infty}(V)$ is the steady-state value of h at membrane potential V , which describes the fraction of sodium channels that are inactivated.
 - $\tau_h(V)$ is the time constant associated with the inactivation gating variable h , determining how quickly h changes over time.
- Finally, the equation $\frac{dn}{dt} = -\frac{(n - n_{\infty}(V))}{\tau_n(V)}$ represents the dynamics of the gating variable n .
 - n represents the activation gating variable for potassium channels.
 - $n_{\infty}(V)$ is the steady-state value of n at membrane potential V , indicating the fraction of potassium channels that are open.
 - $\tau_n(V)$ is the time constant associated with the activation gating variable n , governing how quickly n changes with time.

These equations describe how the gating variables m , h , and n change over time in response to changes in membrane potential V . They play a crucial role in determining the conductance of sodium and potassium channels, which, in turn, influences the generation and propagation of action potentials in neurons[4].

4.4. PYTHON SIMULATION

This section presents the results of the simulation using the Hodgkin-Huxley model for different applied external currents. The simulation was conducted to understand the behavior of the neuron in response to varying input stimuli and to validate the model against known physiological phenomena.

4.4.1. SIMULATION RESULTS

The Hodgkin-Huxley model explains how the dynamics of ion channels (Na^+ , K^+ etc) contribute to the generation of an Action Potential in a neuron. An Action Potential is a sharp voltage spike elicited by stimulating a neuron with a current that exceeds a certain threshold value. The current amplitude is increased gradually, at a threshold amplitude, the voltage response does not increase proportionally. It shows a sharp, disproportionate increase. Once the membrane voltage reaches a threshold value, it increases further rapidly to maximum value and drops again rapidly to a value that is less than resting value, before returning to the baseline value after a delay.

- For input currents ranging from $0\mu\text{A}$ to $0.02235\mu\text{A}$, no action potentials were observed.
- A sudden onset of action potentials occurred when the input current was increased from $0.02235\mu\text{A}$ to $0.02236\mu\text{A}$. However, these action potentials were not periodic.
- Periodic action potentials were observed when the input current was further increased from $0.0622\mu\text{A}$ to $0.06223\mu\text{A}$.
- For input currents ranging from $0.06223\mu\text{A}$ to $0.450\mu\text{A}$, periodic action potentials were observed.
- Action potentials ceased when the input current was increased beyond $0.450\mu\text{A}$.

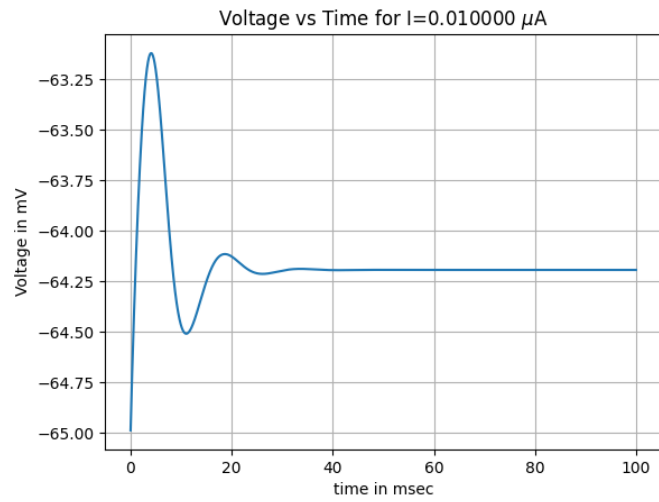


Figure 4.3: Plot of Voltage vs Time for I=0.01 μ A

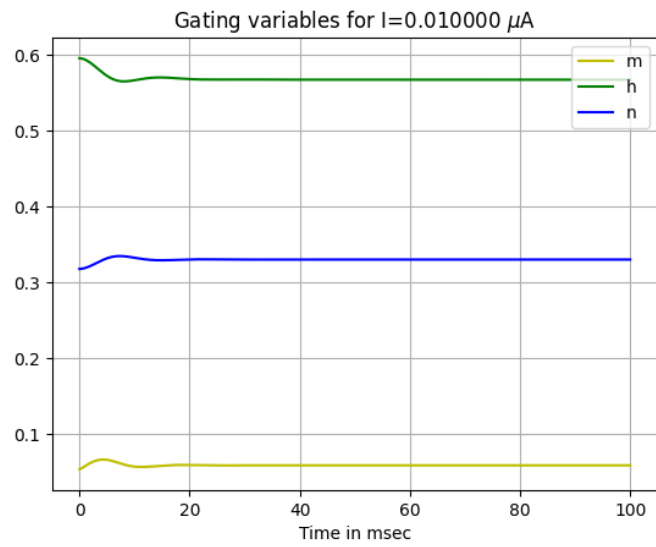


Figure 4.4: Plot of gating variables for I=0.01 μ A

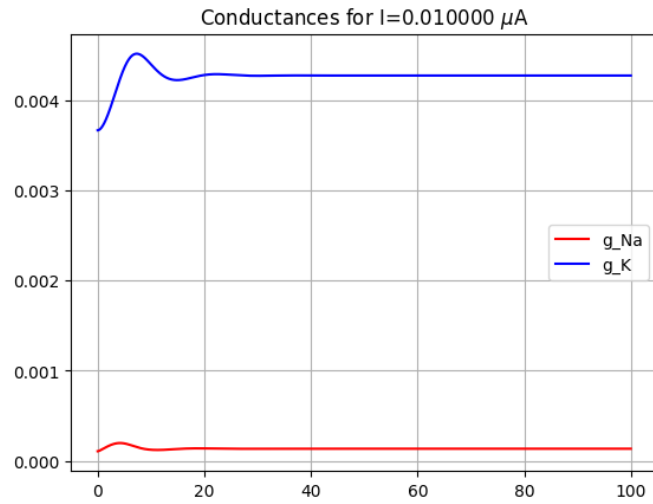


Figure 4.5: Plot of conductances for $I=0.01\mu\text{A}$

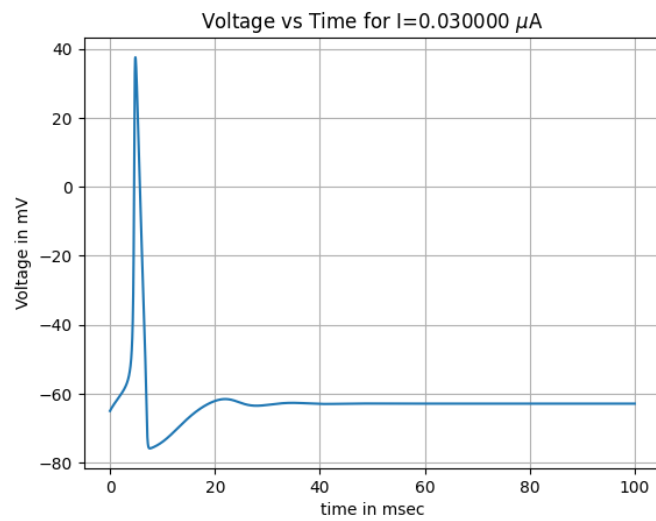


Figure 4.6: Plot of Voltage vs Time for $I=0.03\mu\text{A}$

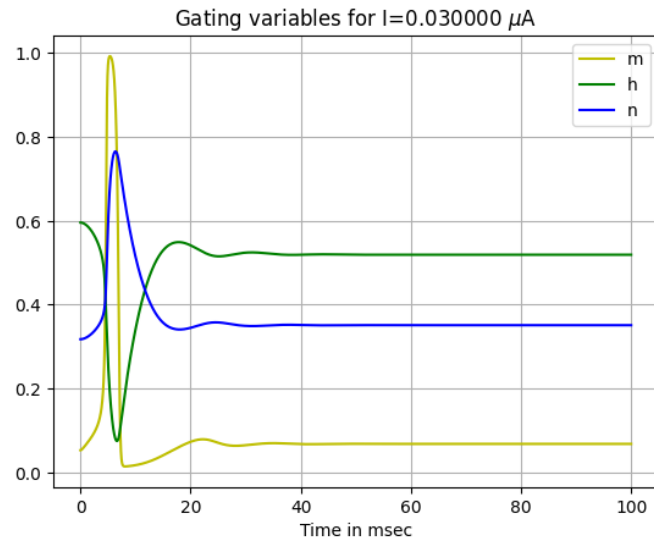


Figure 4.7: Plot of gating variables for $I=0.03\mu\text{A}$

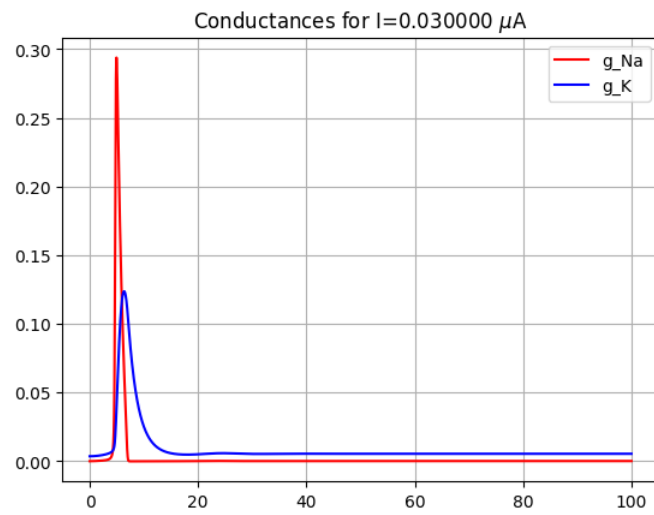


Figure 4.8: Plot of conductances for $I=0.03\mu\text{A}$

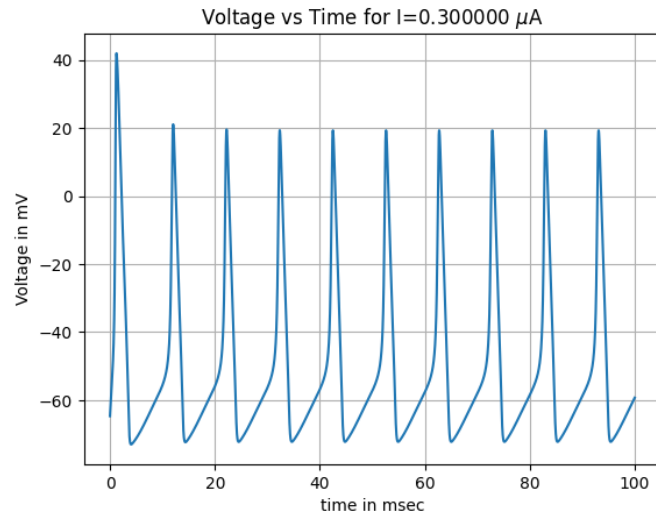


Figure 4.9: Plot of Voltage vs Time for $I=0.3\mu$ A

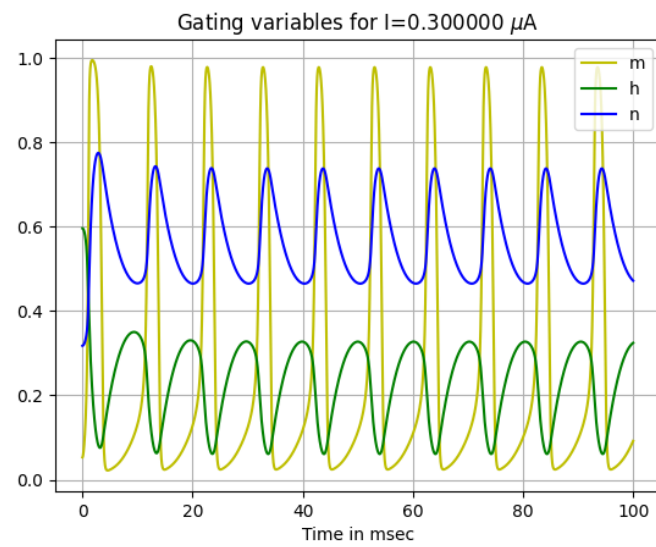


Figure 4.10: Plot of gating variables for $I=0.3\mu$ A

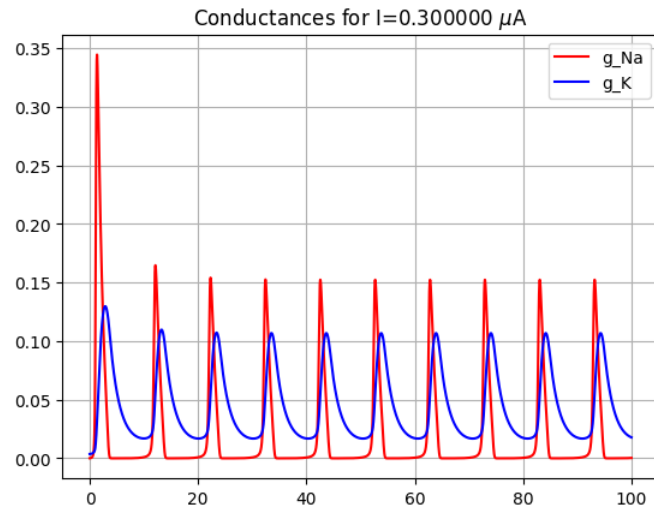


Figure 4.11: Plot of conductances for $I=0.3\mu\text{A}$

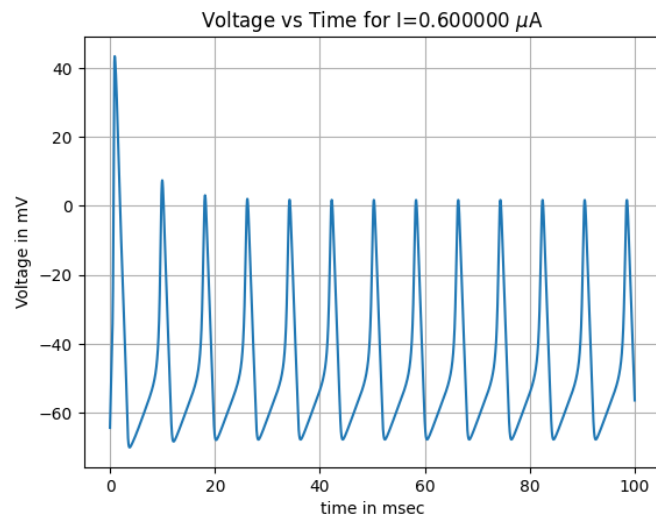


Figure 4.12: Plot of Voltage vs Time for $I=0.6\mu\text{A}$

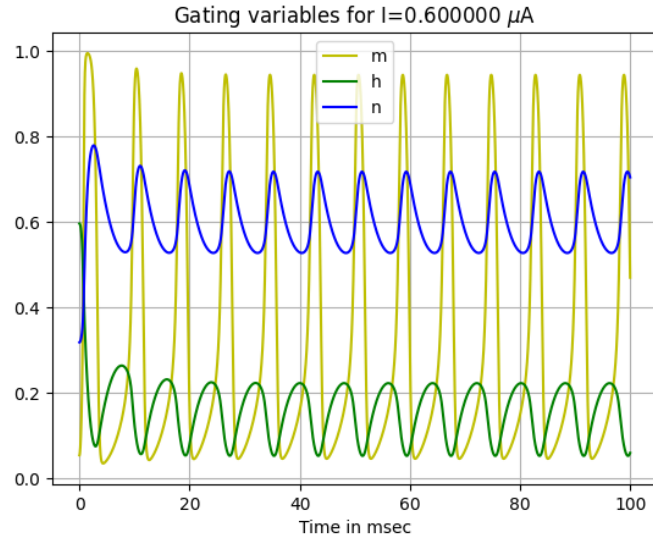


Figure 4.13: Plot of gating variables for $I=0.6\mu$ A

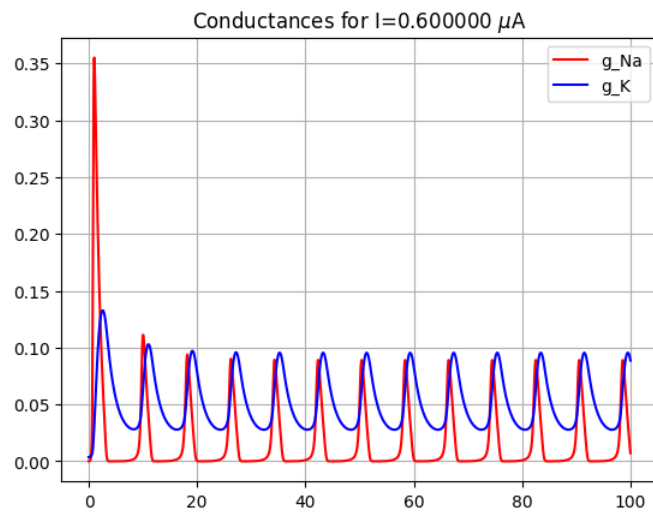


Figure 4.14: Plot of conductances for $I=0.6\mu$ A

5. APPLICATIONS

Biological neural network modeling is pushing the technological frontier in every field by simulating biological neural networks, solving real-world challenges, and improving the quality of human life. These applications demonstrate the power of interdisciplinary collab-

oration, bringing together biology, computer science, engineering and medicine to advance the future of medical technology and technology.

- **Brain-Computer Interface (BMI):** Brain-computer interface technology allows the human brain to interact directly with external devices, which has significant potential in providing assistive tools and restoring limb movement to paraplegic patients. Through the application of biological neural network models, researchers can better understand how brain signals map to body movements and how these signals can be interpreted to control external devices. These models also help improve algorithms to decode and translate brain activity into mechanical movements or electrical signals, enhancing the accuracy and responsiveness of brain-computer interfaces.
- **AI:** Biological neural networks provide artificial intelligence with a framework that mimics complex brain processing functions, particularly in the areas of vision and language processing. Deep learning, a biologically inspired algorithm, has led to breakthroughs in image recognition, speech-to-text conversion, and machine translation. Advances in these technologies, due in part to the understanding and simulation of how biological neural networks work, are changing the way we interact with technology and are finding applications in areas such as medicine, self-driving vehicles and smart homes.
- **Cognitive and Behavioral Research:** Biological neural network modeling helps scientists understand how cognitive processes are encoded in the brain. Such models can simulate memory formation, attention control, and decision-making processes, providing insights into studying behavior in humans and other animals. Additionally, they play an important role in explaining cognitive patterns in mental health conditions such as anxiety, depression, and other psychological disorders.
- **Precision medicine and disease diagnosis:** In the field of precision medicine, modeling of biological neural networks can predict how individuals will respond to specific treatments, thereby enabling personalized medicine. By analyzing a patient's gene expression data, protein levels and other biomarkers, the model is able to predict the course of the disease and the patient's response to drug treatment. Such models can also reveal new disease mechanisms, guide the development of future treatment strategies, and help physicians design customized treatment regimens to maximize efficacy and reduce side effects.

REFERENCES

- [1] Warren S Mcculloch and Walter Pitts. A LOGICAL CALCULUS OF THE IDEAS IMMANENT IN NERVOUS ACTIVITY. September 1854.
- [2] D. O. Hebb. *The Organization of Behavior: A Neuropsychological Theory*. L. Erlbaum Associates, Mahwah, N.J, 2002.
- [3] A. L. Hodgkin and Pitts A. F. Huxley. A quantitative description of membrane current and its application to conduction and excitation in nerve. August 1952.
- [4] F. Rosenblatt. The perceptron: A probabilistic model for information storage and organization in the brain. *Psychological Review*, 65(6):386–408, 1958.
- [5] Bernard Widrow and Marcian E. Hoff Jr. Adaptive Switching Circuits. 1960.
- [6] J J Hopfield. Neural networks and physical systems with emergent collective computational abilities. April 1982.
- [7] G. E. Hinton and T. J. Sejnowski. Learning andf Relearning in Boltzmann Machines. 1:282–317, 1986.

REFERENCES

- [1] Cole, K. S., Curtis, H. J. Electric impedance of the squid giant axon during activity. *Journal of General Physiology*, 22(5), 649–670 (1939). <https://doi.org/10.1085/jgp.22.5.649>
- [2] HODGKIN, A., HUXLEY, A. Action Potentials Recorded from Inside a Nerve Fibre. *Nature* 144, 710–711 (1939). <https://doi.org/10.1038/144710a0>
- [3] Hodgkin, A. L., Katz, B. (1949). The effect of sodium ions on the electrical activity of the giant axon of the squid. *The Journal of Physiology*, 108. <https://doi.org/10.1113/jphysiol.1949.sp004310>
- [4] Hodgkin, A. L., Huxley, A. F. (1952), A quantitative description of membrane current and its application to conduction and excitation in nerve. *The Journal of Physiology*, 117 <https://doi:10.1113/jphysiol.1952.sp004764>
- [5] Häusser, M. The Hodgkin-Huxley theory of the action potential. *Nat Neurosci* 3 (Suppl 11), 1165 (2000). <https://doi.org/10.1038/81426>
- [6] Kandel, E. R., Schwartz, J. H., Jessell, T. M., Siegelbaum, S. A., Hudspeth, A. J. (2014). *Principles of Neural Science* (5th ed.). McGraw-Hill Education. ISBN: 978-0-07-181001-2.

A. PYTHON CODE

This code demonstrates the Hodgkin-Huxley model in current clamp experiments and shows action potential propagation.

Listing 1: Python code for Hodgkin-Huxley simulation

#THIS PROGRAM DEMONSTRATES HODGKIN HUXLEY MODEL IN CURRENT CLAMP EXPERIMENTS AND SHOWS A
#Time is in secs, voltage in mvs, conductances in m mho/mm^2, capacitance in uF/mm^2

threshold value of current is 0.0223

```
import numpy as np
import matplotlib.pyplot as plt
from tqdm import tqdm
import sys
from numpy import NaN, Inf, arange, isscalar, asarray, array
ImpCur=0.6 #change input current here
g_K_max=.36 # max conductance of K channel
V_K=-77 #voltage of K channel
g_Na_max=1.20 #max conductance of Na channel
V_Na=50 #voltage of Na channel
g_l=0.003 #conductance of combined gates
V_l=-54.387 #voltage of combined channel
cm=.01

dt=0.01 #0.01 ms
niter=10000
t=np.array([i for i in range(niter)])
I_app=ImpCur*np.ones(niter)
V=-64.9964 #base voltage
m=0.0530
h=0.5960
n=0.3177

#### to store the values
g_Na_hist=np.zeros(niter)
g_K_hist=np.zeros(niter)
V_hist=np.zeros(niter)
m_hist=np.zeros(niter)
h_hist=np.zeros(niter)
n_hist=np.zeros(niter)
```

```

for i in range(niter):
    g_Na = g_Na_max*(m**3)*h
    g_K = g_K_max*(n**4)
    g_total = g_Na+g_K+g_l
    V_inf = ((g_Na*V_Na+g_K*V_K+g_l*V_l)+I_app[i])/g_total
    tau_v = cm/g_total
    V = V_inf+(V- V_inf)*np.exp(-dt/tau_v)
    alpha_m = 0.1*(V+40)/(1-np.exp(-(V+40)/10))
    beta_m = 4*np.exp(-0.0556*(V+65))
    alpha_n = 0.01*(V+55)/(1-np.exp(-(V+55)/10))
    beta_n = 0.125*np.exp(-(V+65)/80)
    alpha_h = 0.07*np.exp(-0.05*(V+65))
    beta_h = 1/(1+np.exp(-0.1*(V+35)))
    tau_m = 1/(alpha_m+beta_m)
    tau_h = 1/(alpha_h+beta_h)
    tau_n = 1/(alpha_n+beta_n)
    m_inf = alpha_m*tau_m
    h_inf = alpha_h*tau_h
    n_inf = alpha_n*tau_n
    m=m_inf+(m-m_inf)*np.exp(-dt/tau_m)
    h=h_inf+(h-h_inf)*np.exp(-dt/tau_h)
    n=n_inf+(n-n_inf)*np.exp(-dt/tau_n)
    V_hist[i]=V
    m_hist[i]=m
    h_hist[i]=h
    n_hist[i]=n

def plot_V_vs_t(V_hist, I_ext):
    plt.plot(t*dt, V_hist)
    plt.grid()
    plt.title('Voltage_vs_Time_for_I=%f_$_\mu$A'%I_ext)
    plt.xlabel('time_in_msec')
    plt.ylabel('Voltage_in_mV')
    plt.show()

def plot_gating_variables(m_hist, h_hist, n_hist, I_ext):
    plt.plot(t*dt, m_hist, 'y', label='m')
    plt.plot(t*dt, h_hist, 'g', label='h')
    plt.plot(t*dt, n_hist, 'b', label='n')
    plt.xlabel('Time_in_msec')
    plt.title('Gating_variables_for_I=%f_$_\mu$A'%I_ext)
    plt.grid()
    plt.legend()
    plt.show()

```

```

def plot_conductances(m_hist, h_hist, n_hist, I_ext):
    g_Na=g_Na_max*(m_hist**3)*h_hist
    g_K=g_K_max*n_hist**4
    plt.plot(t*dt,g_Na, 'r', label='g_Na')
    plt.plot(t*dt,g_K, 'b', label='g_K')
    plt.title('Conductances_for_I=%f_\\mu$A'%I_ext)
    plt.legend()
    plt.grid()
    plt.show()
plot_V_vs_t(V_hist, ImpCur)
plot_gating_variables(m_hist, h_hist, n_hist, ImpCur)
plot_conductances(m_hist, h_hist, n_hist, ImpCur)

```