



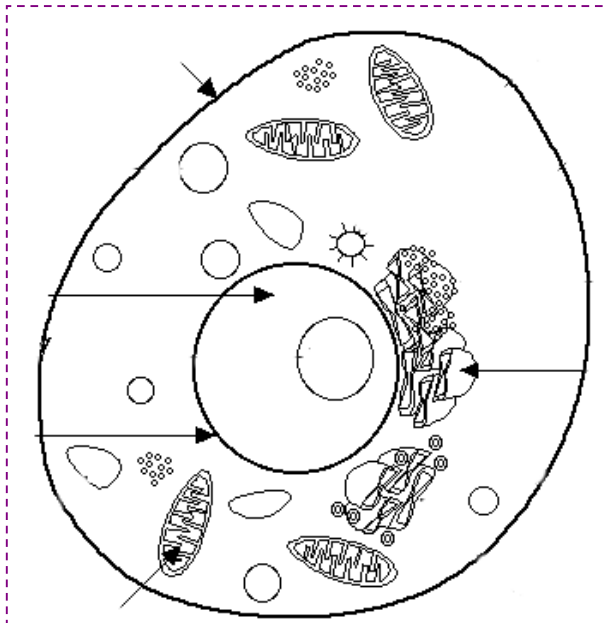
Electrophysiology of Neurons

Zhang Yi, *IEEE Fellow*
Autumn 2018

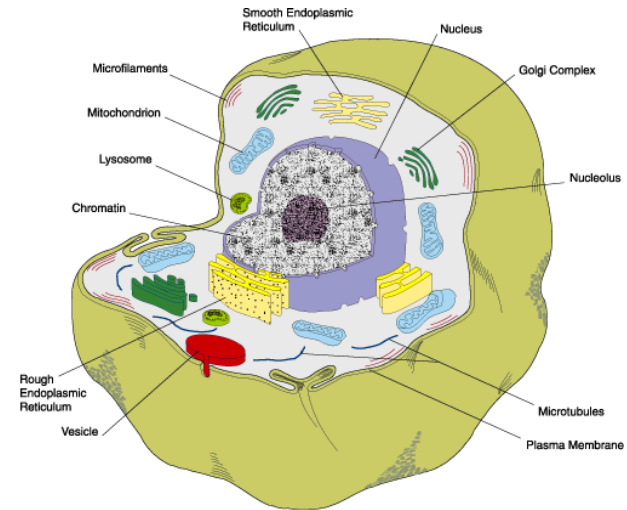
Outline

- Cell Membrane & Ions
- Electrochemical gradients
- Equivalent circuit
- Hodgkin-Huxley gate model
- Hodgkin-Huxley Model

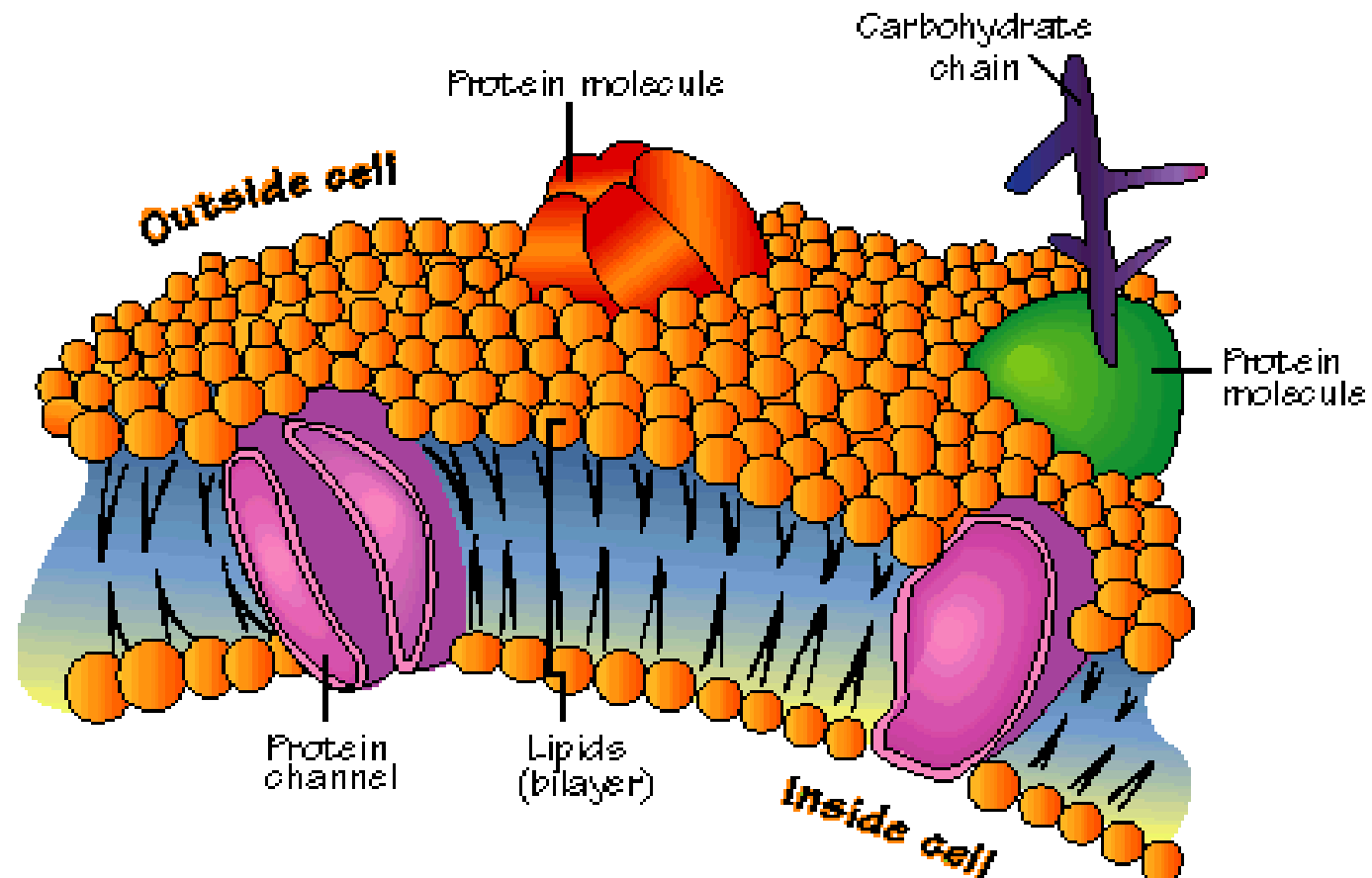
Cell Membrane & Ions



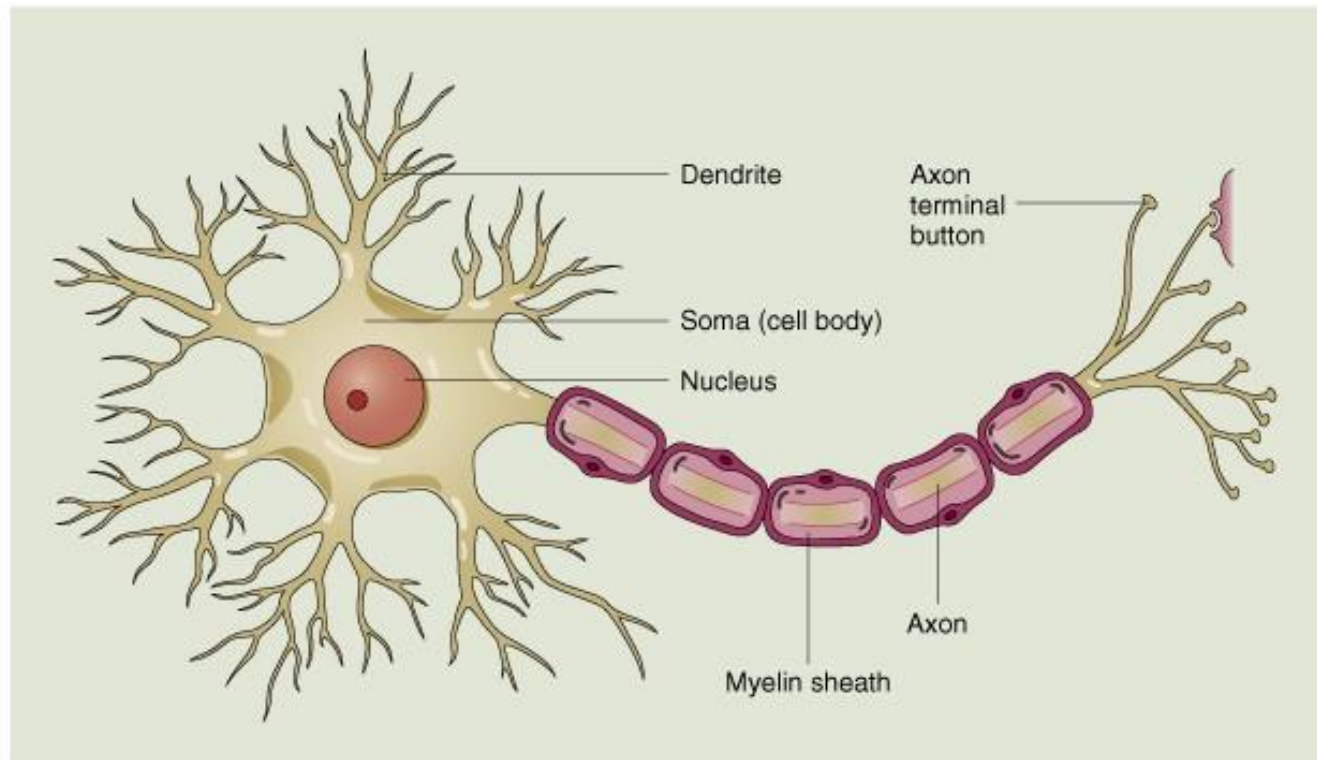
Cell Membrane
Cell Body
Nuclear Membrane
Nucleus
Endoplasmic Reticulum
Mitochondria



Cell Membrane & Ions

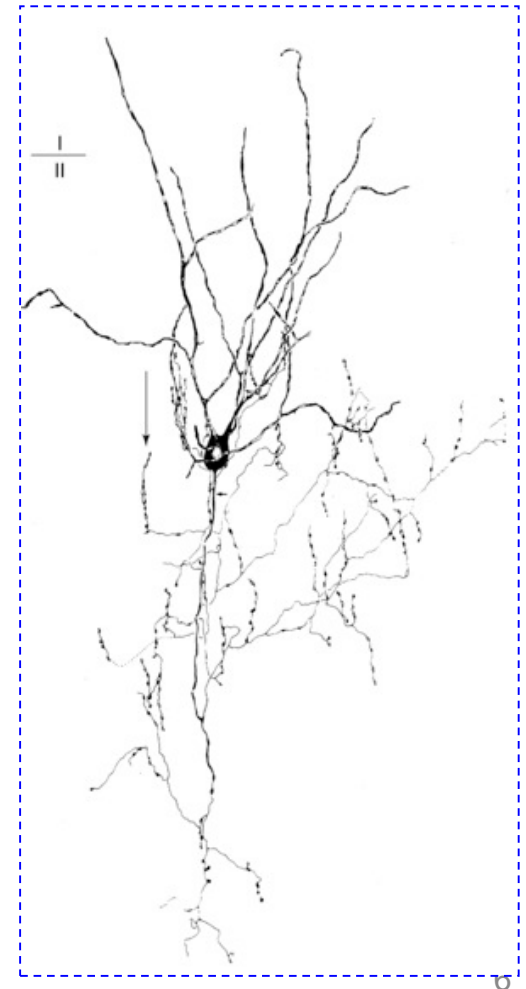
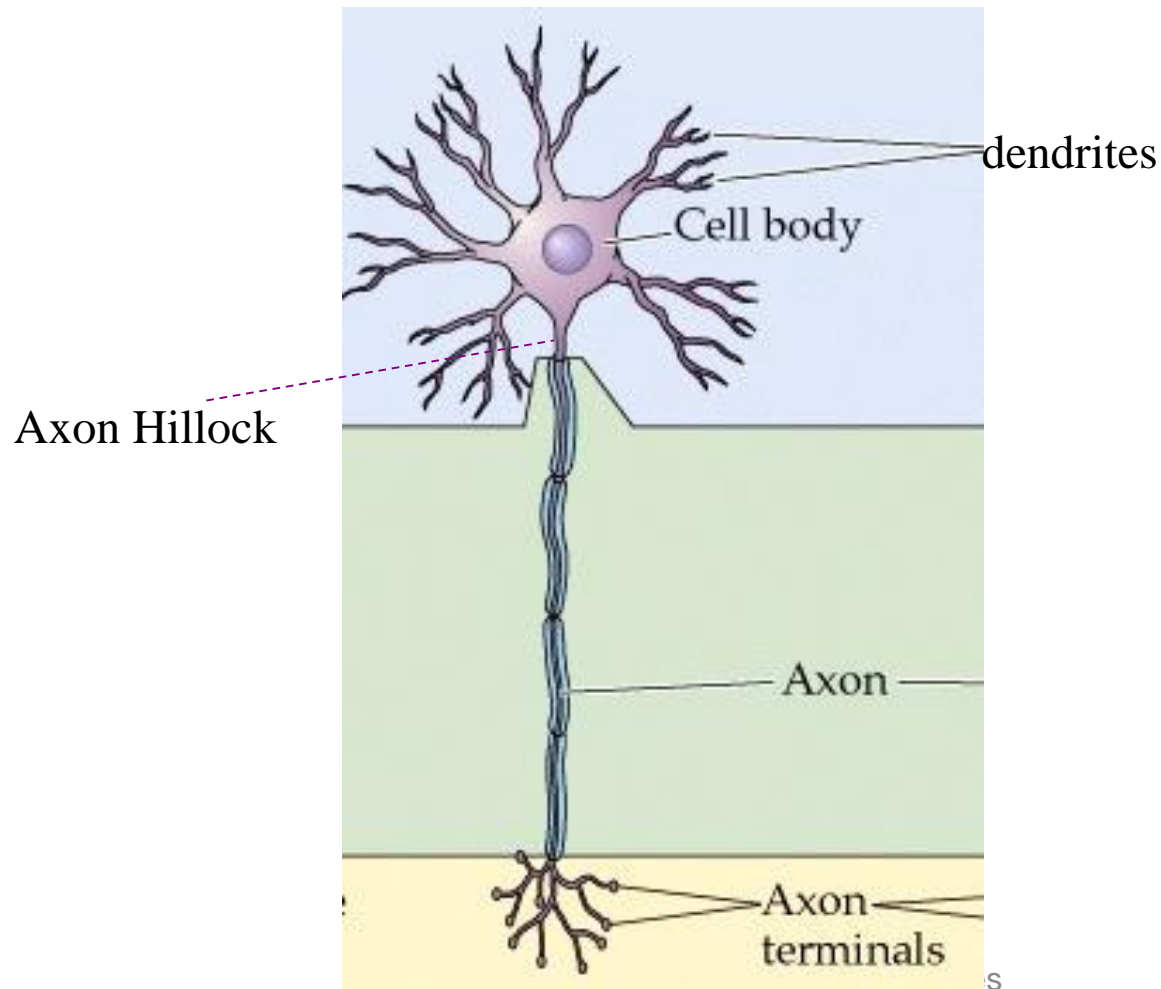


Neuron

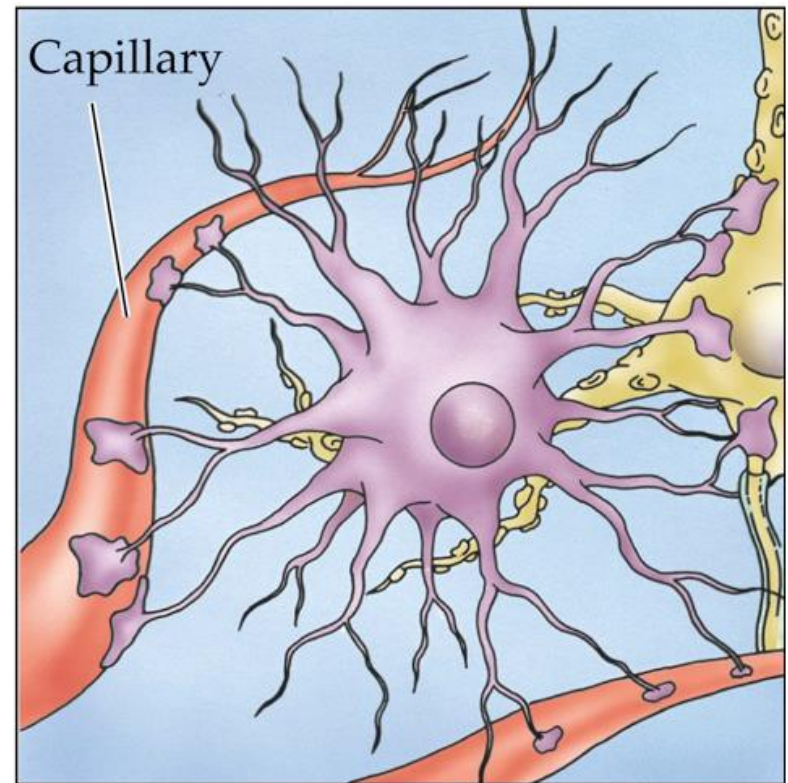
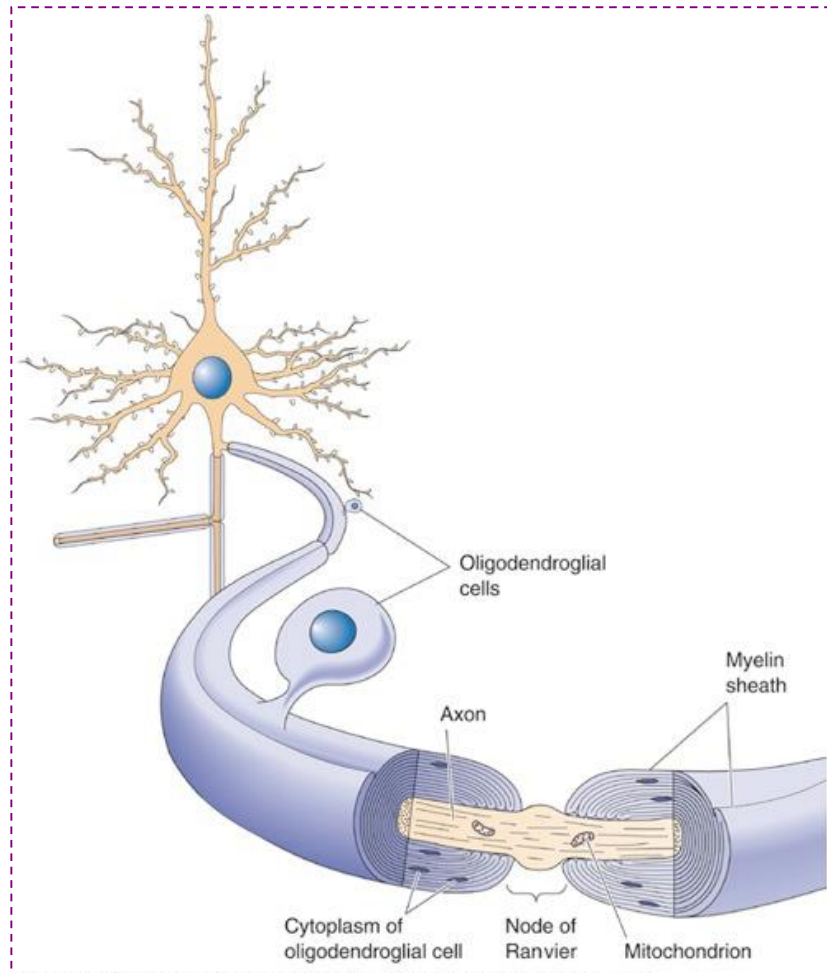


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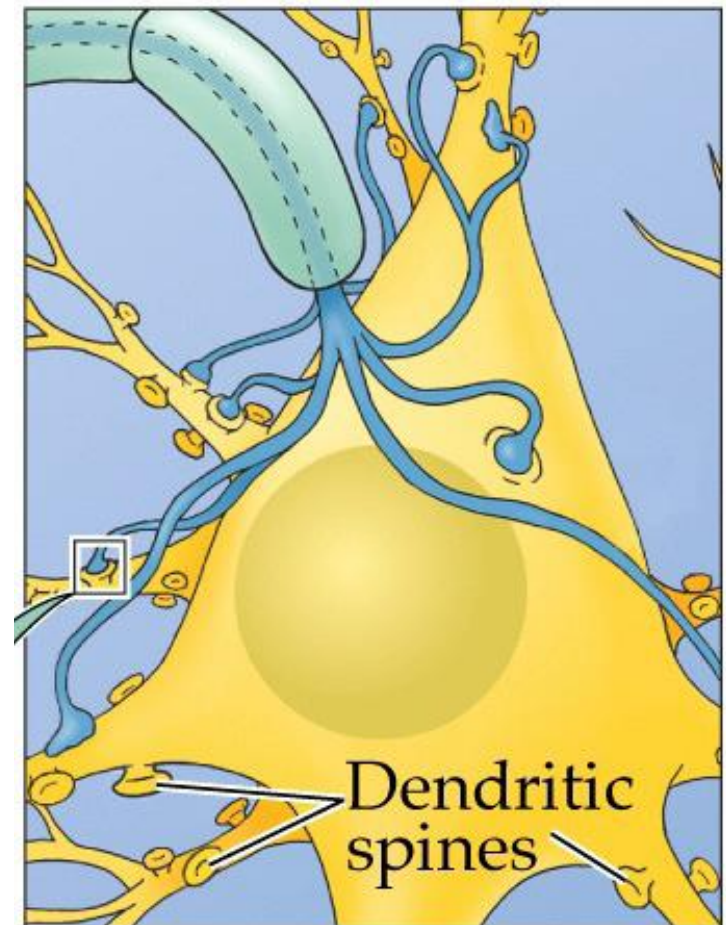
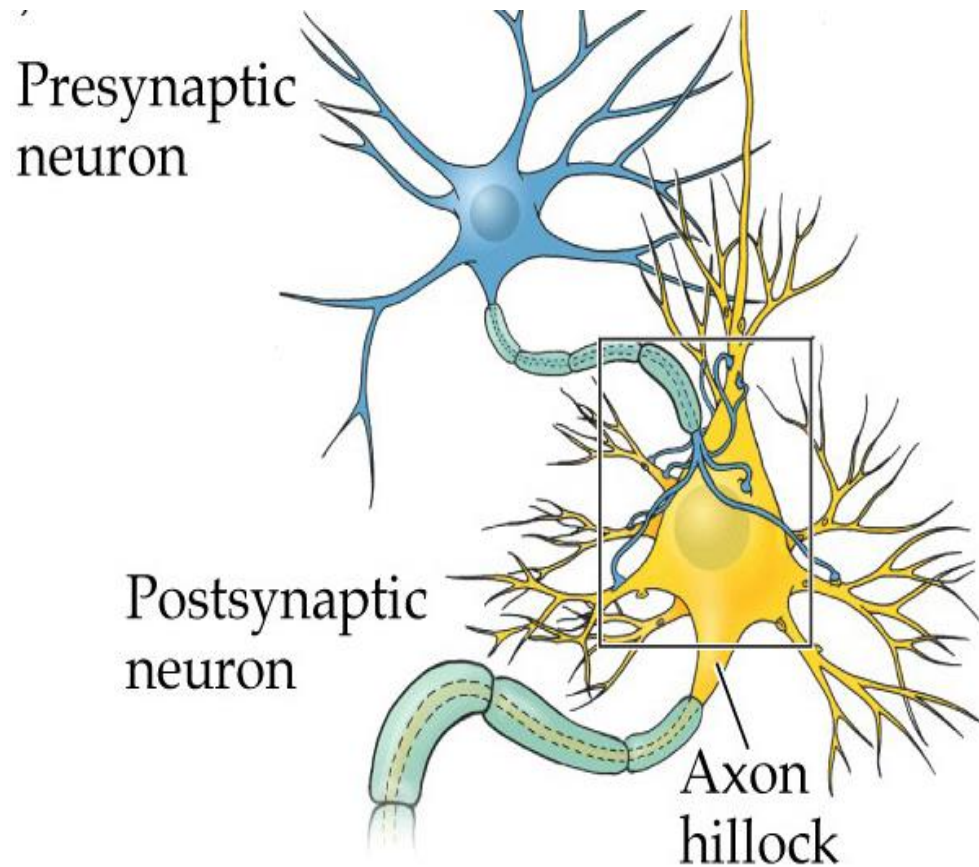
Neuron



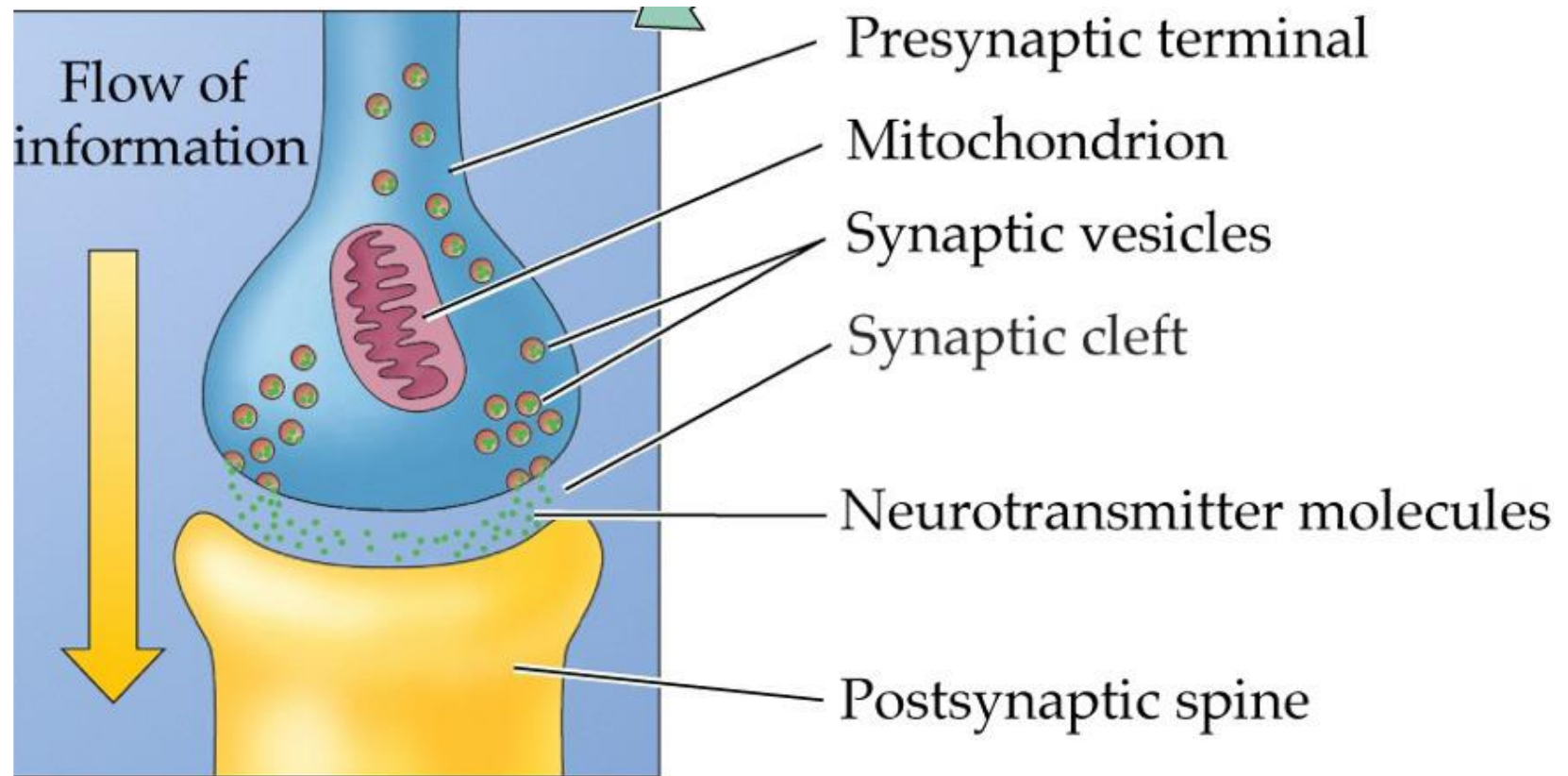
Neuron



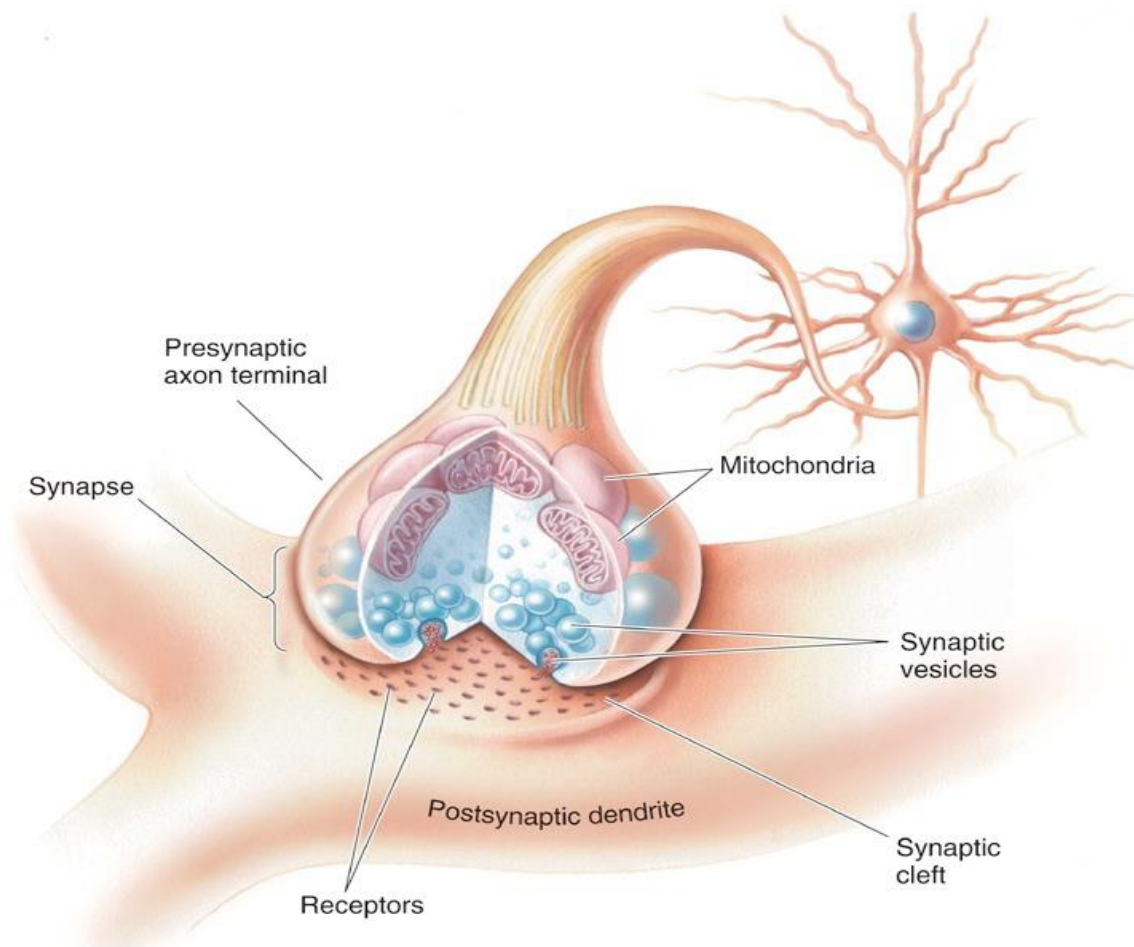
Connection of Neurons



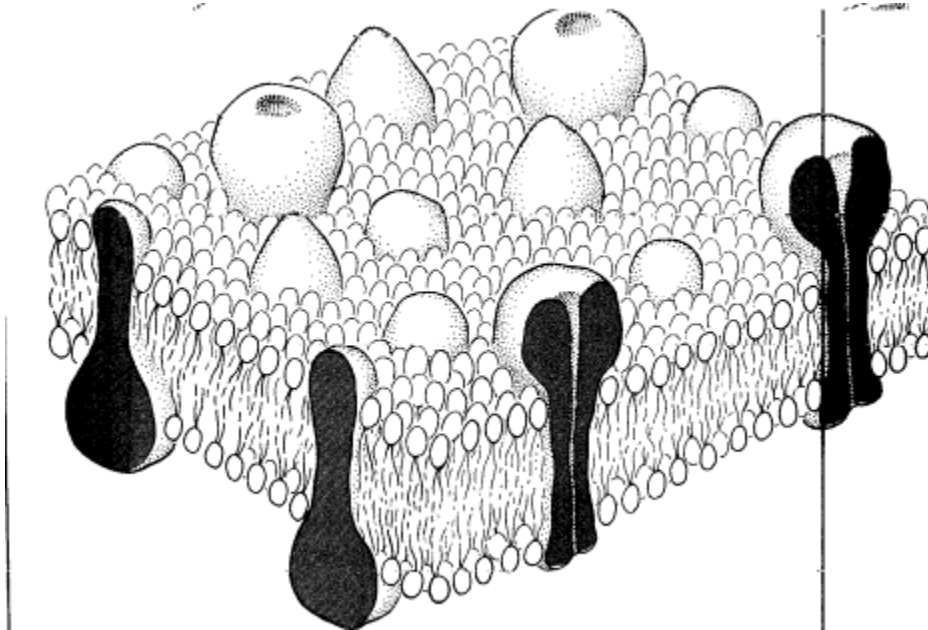
An Individual Synapse



An Individual Synapse

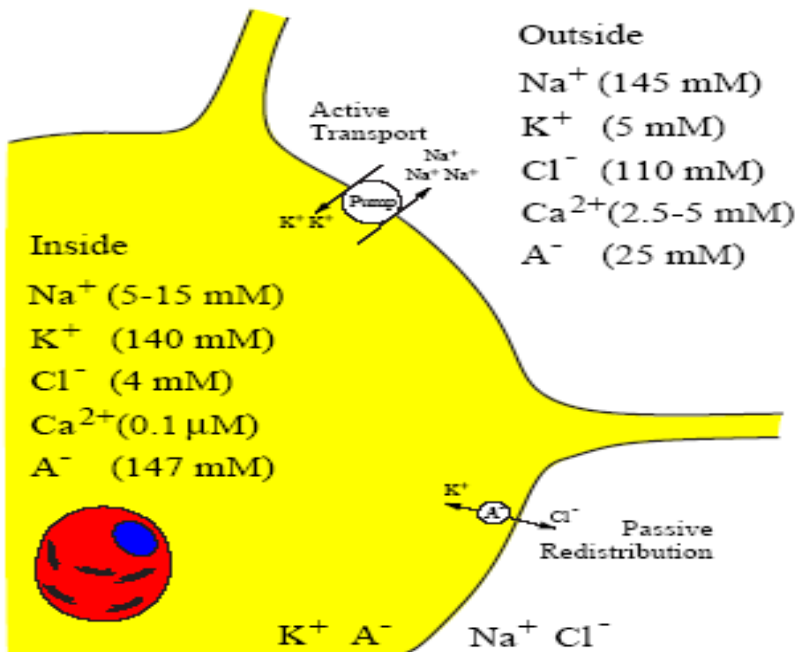


Neuron membrane



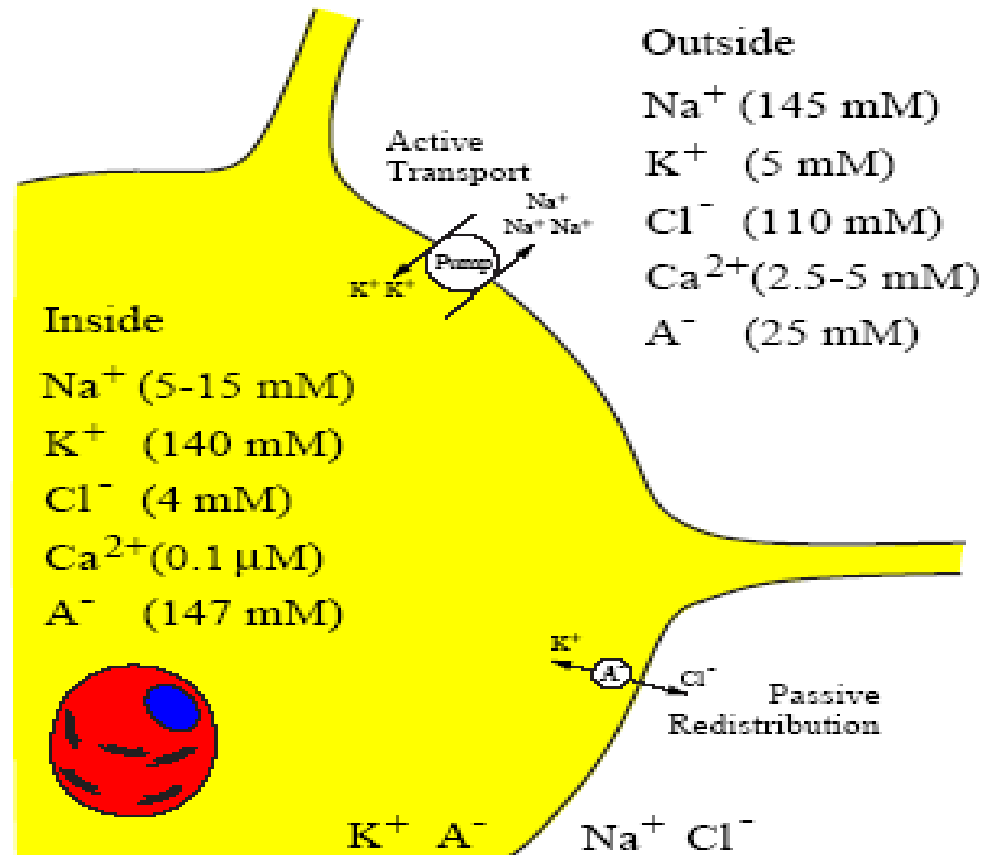
Neurons & Ions

Electrical activity in neurons is sustained and propagated via ionic currents through neuron membranes. Most of these transmembrane currents involve four ionic species: sodium (Na^+), potassium (K^+), calcium (Ca^{2+}), and chloride (Cl^-).

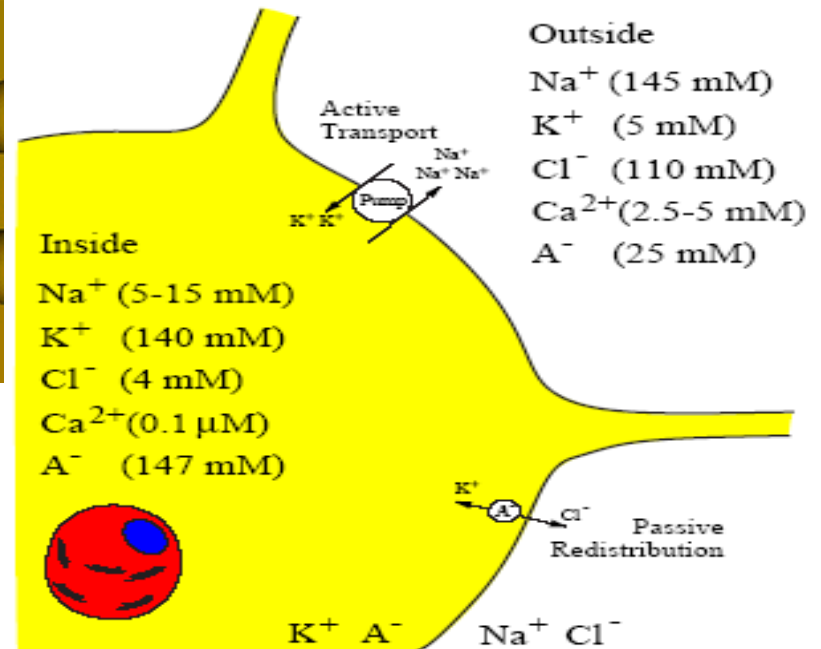
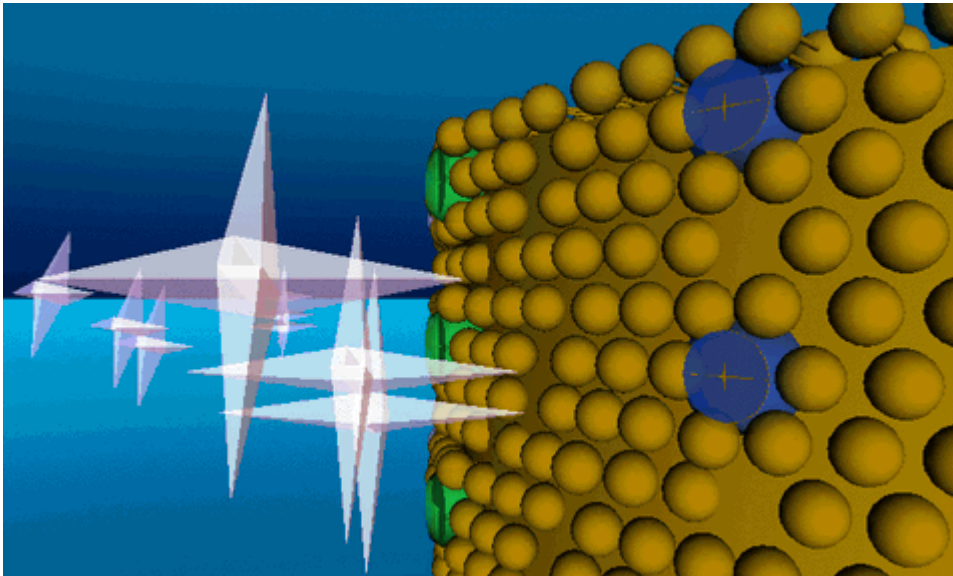


Electrochemical gradients

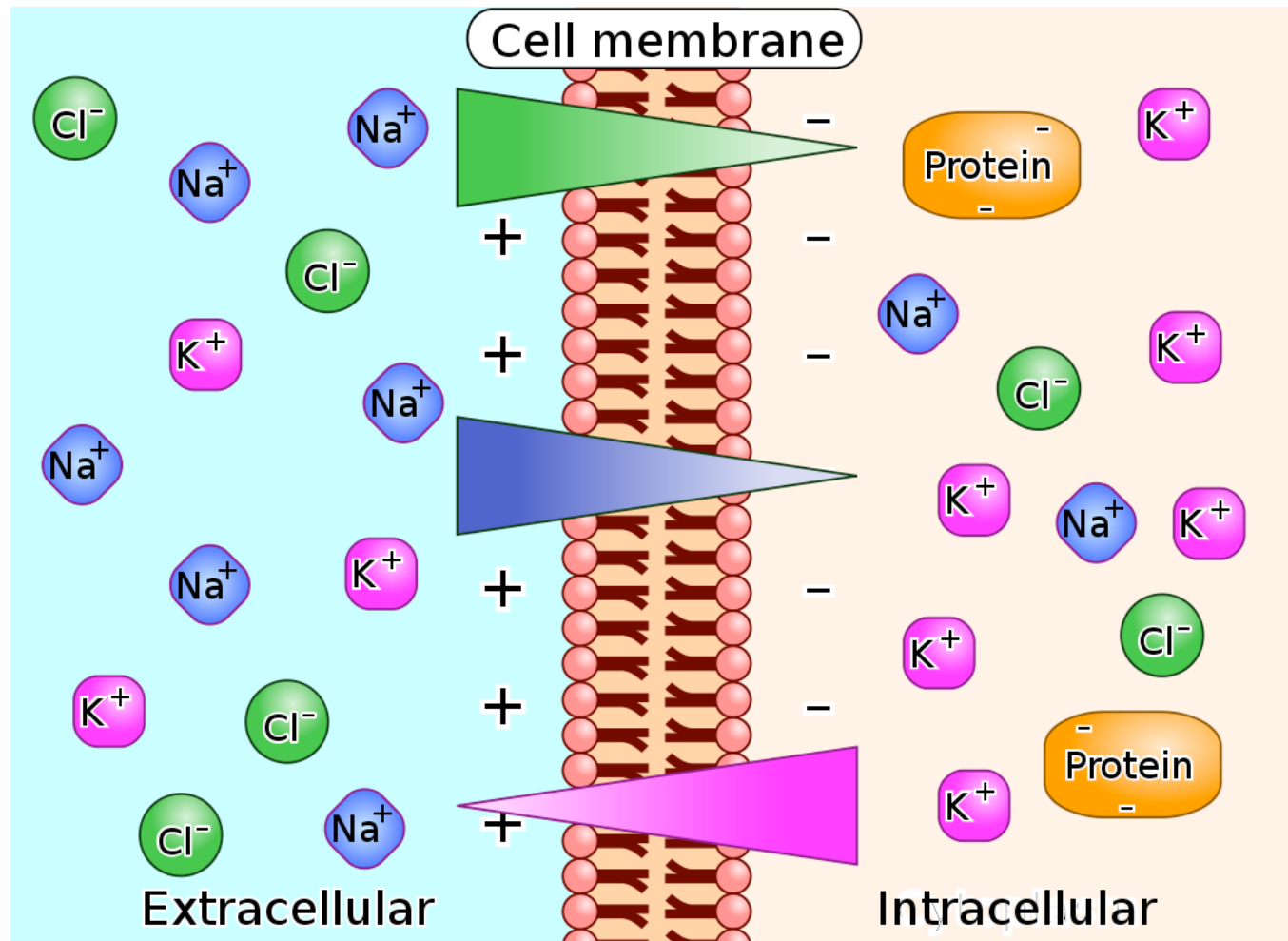
Different concentrations on the two sides --- major driving forces of neural activity.



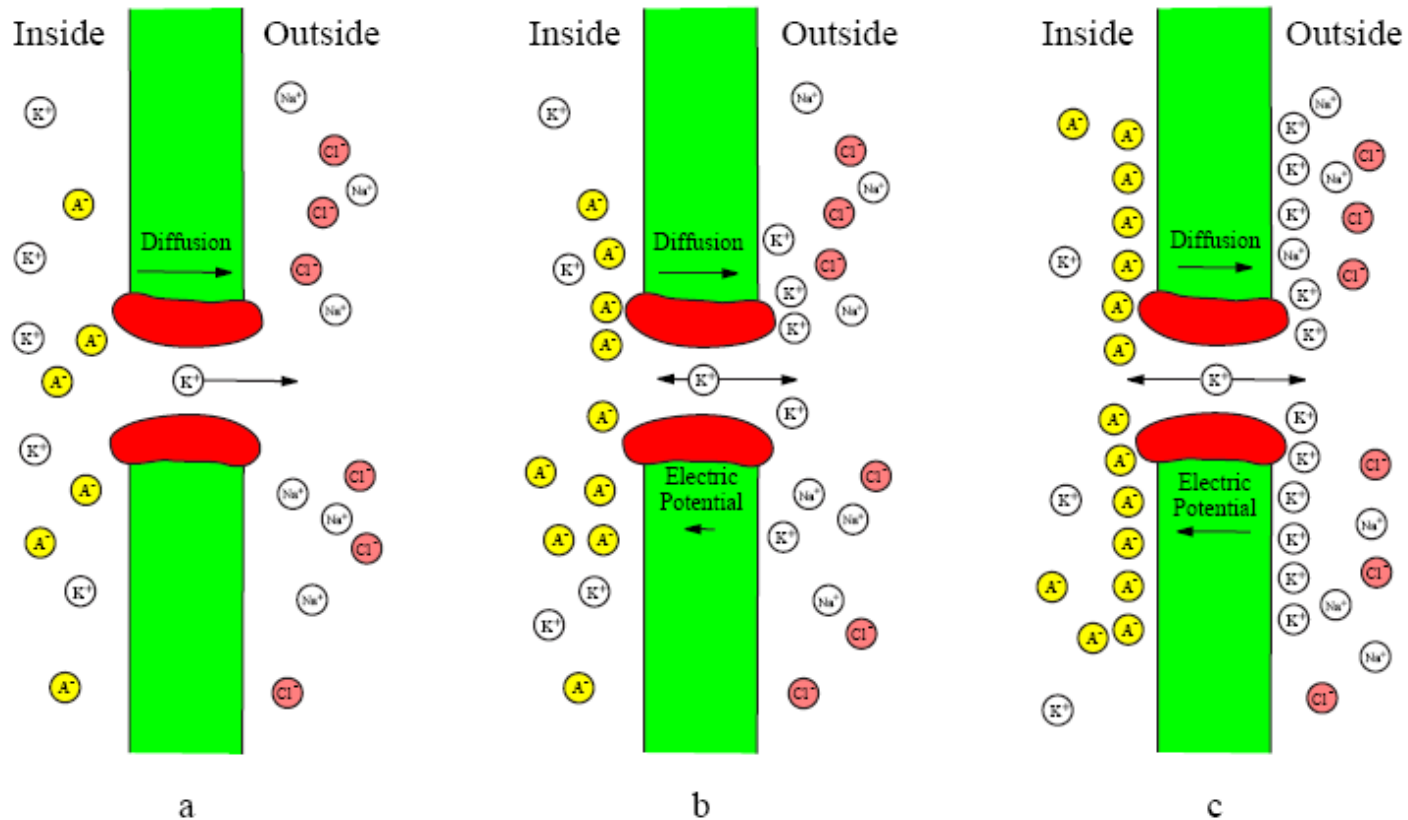
Ions



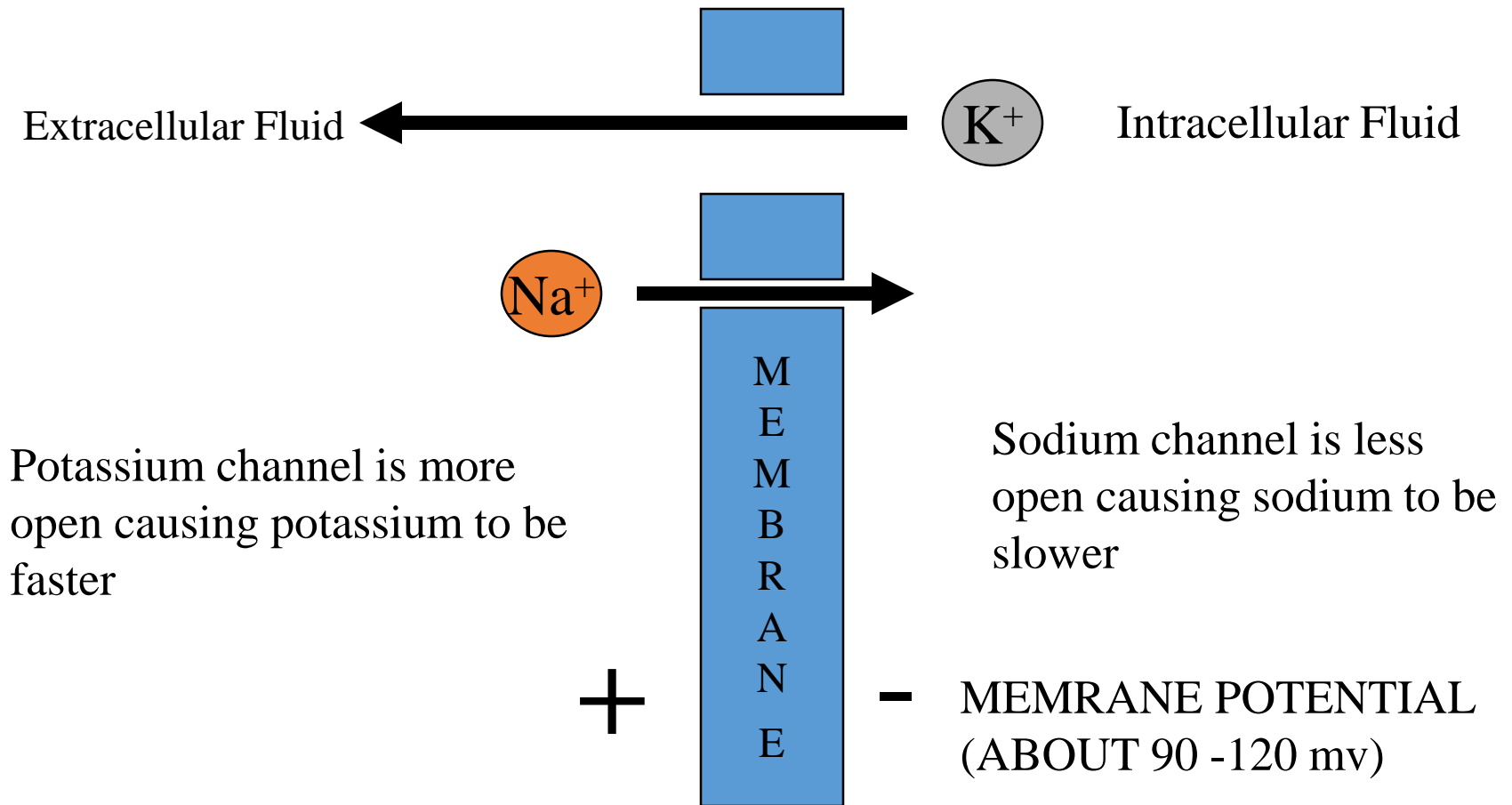
Ionic diffusion



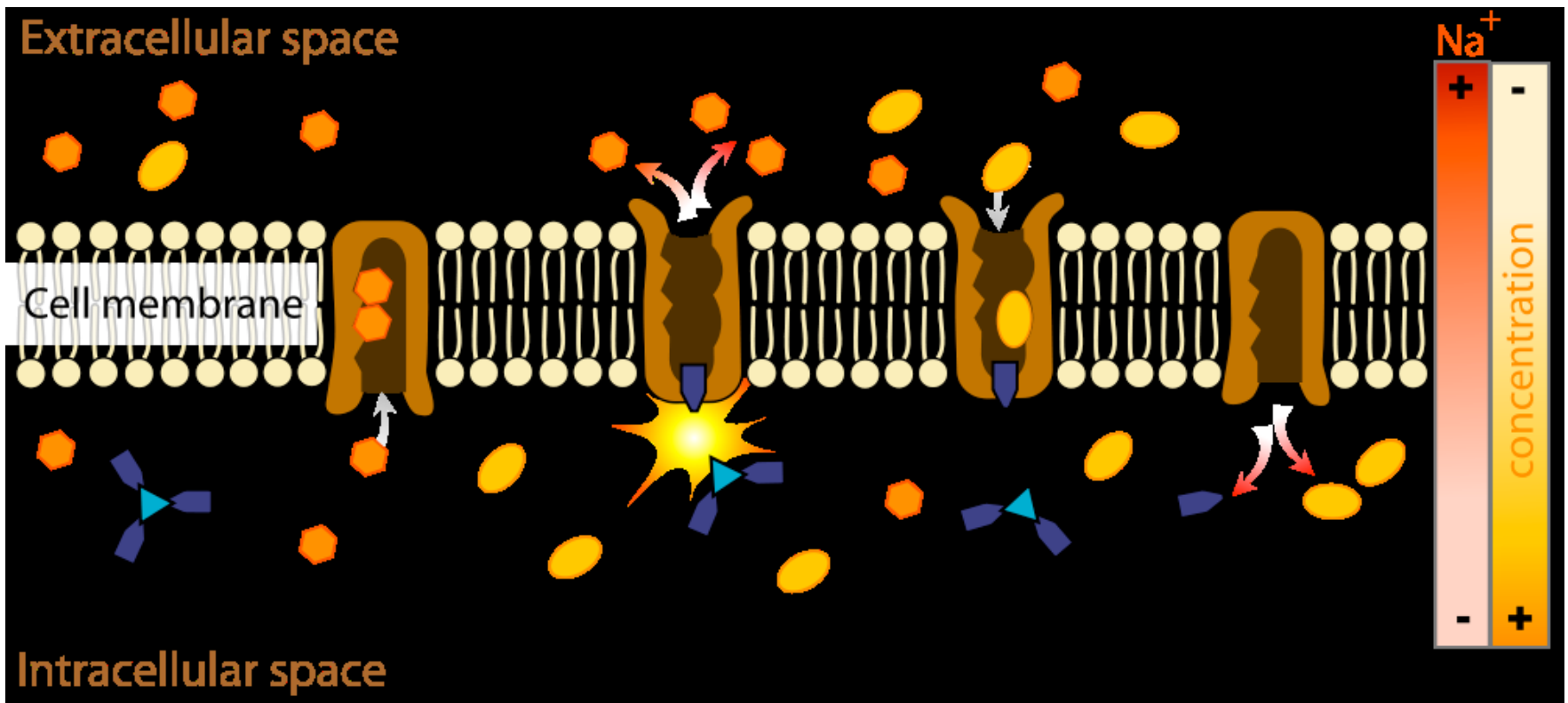
Ionic diffusion



The Membrane Potential



The Membrane Potential



Nernst potential

Nernst equilibrium potential:

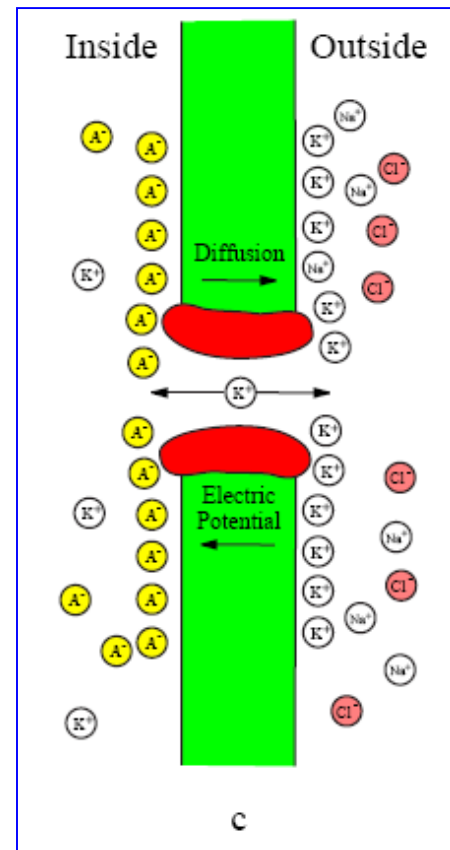
$$E_{ion} = \frac{RT}{zF} \ln \frac{[Ion]_{out}}{[Ion]_{in}}$$

R - the universal gas constant

T - temperature

F - Faraday constant

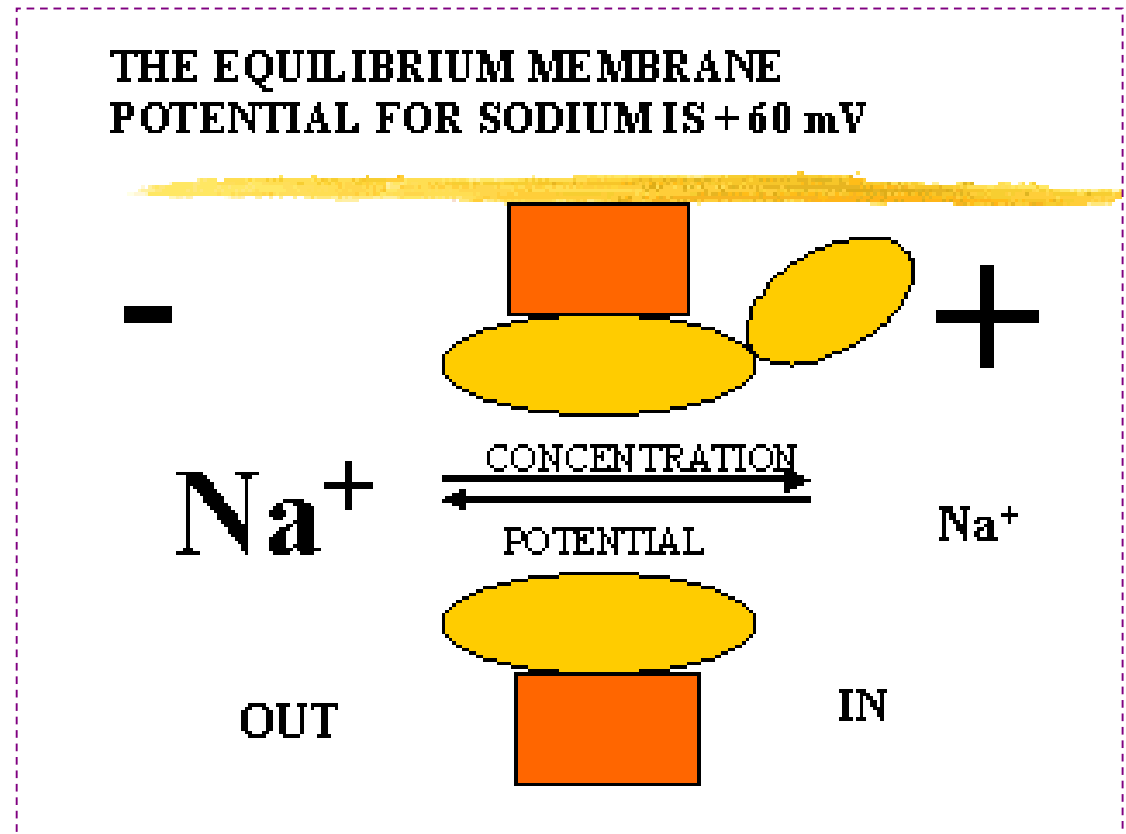
z - the valence of the ion



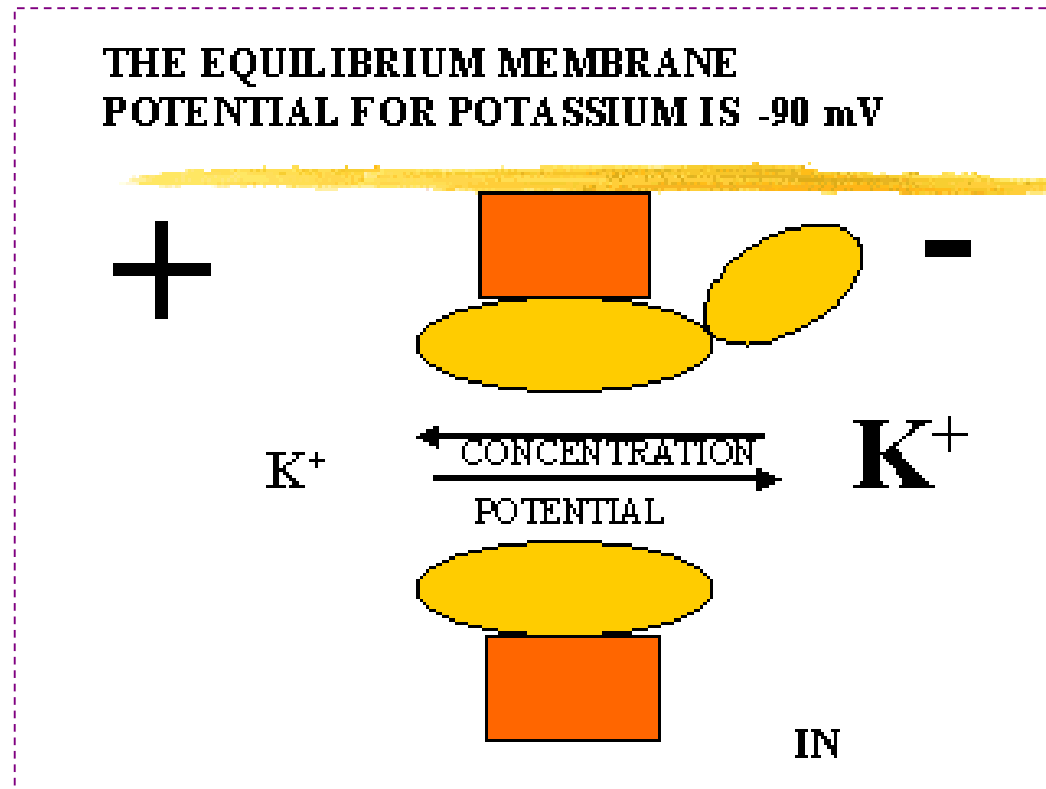
Sodium equilibrium potential

Outside 145mM

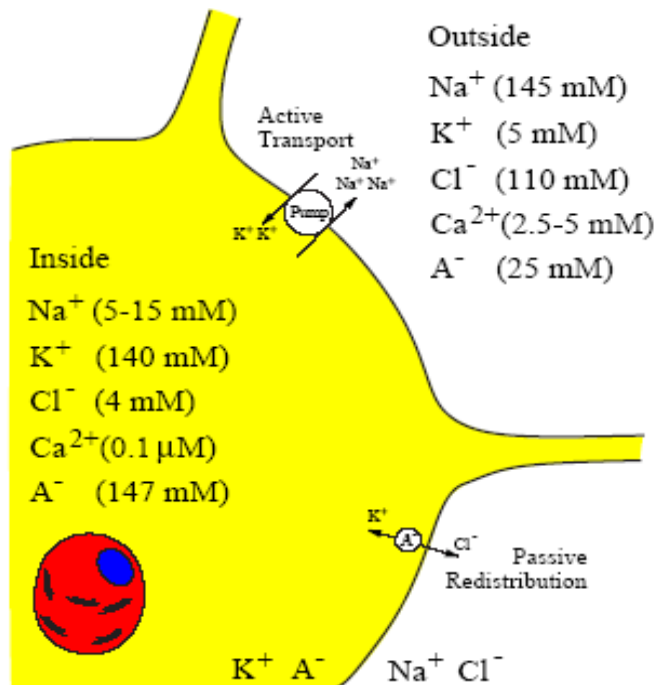
Inside 5-15mM



Equilibrium potential



Equilibrium potentials



Equilibrium Potentials

$$\text{Na}^+ \quad 62 \log \frac{145}{5} = 90 \text{ mV}$$

$$62 \log \frac{145}{15} = 61 \text{ mV}$$

$$\text{K}^+ \quad 62 \log \frac{5}{140} = -90 \text{ mV}$$

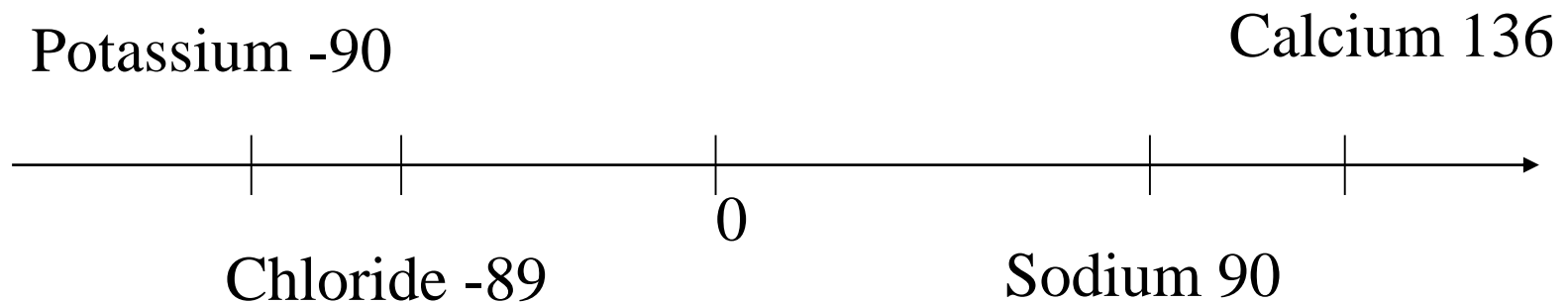
$$\text{Cl}^- \quad -62 \log \frac{110}{4} = -89 \text{ mV}$$

$$\text{Ca}^{2+} \quad 31 \log \frac{2.5}{10^{-4}} = 136 \text{ mV}$$

$$31 \log \frac{5}{10^{-4}} = 146 \text{ mV}$$

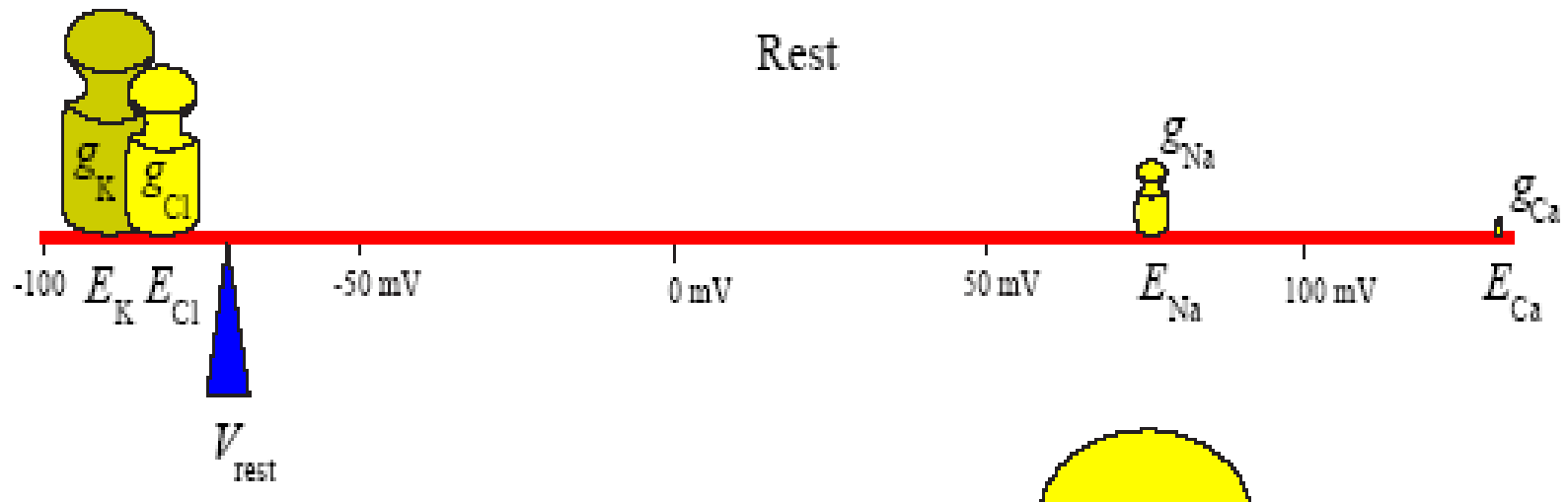
$$T = 37^\circ \text{C}$$

Equilibrium potentials



Resting Potential

$$I=0, dV/dt=0$$



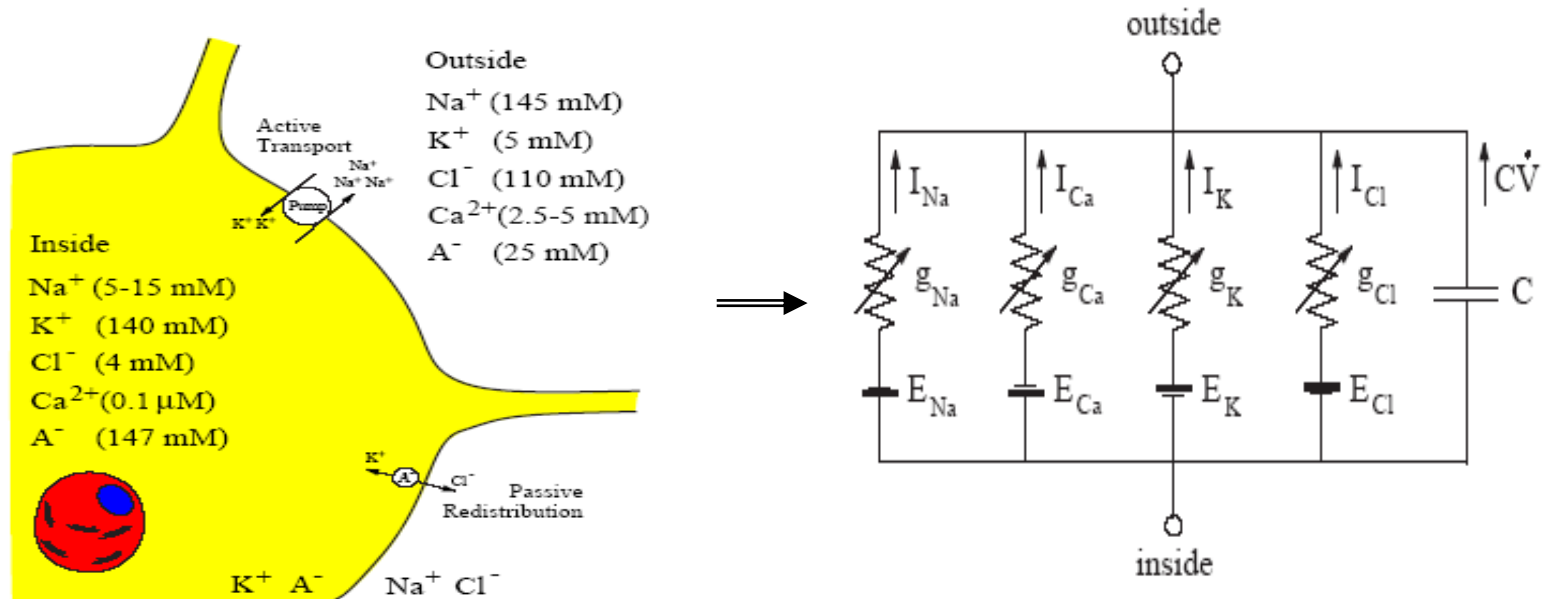
Inward on outward currents

$$E_K < E_{Cl} < V_{(at\ rest)} < E_{Na} < E_{Ca}$$

$$I_{Na}, I_{Ca} < 0 \text{ (inward currents)}$$

$$I_K, I_{Cl} > 0 \text{ (outward currents)}$$

Mapping neural activity to circuits



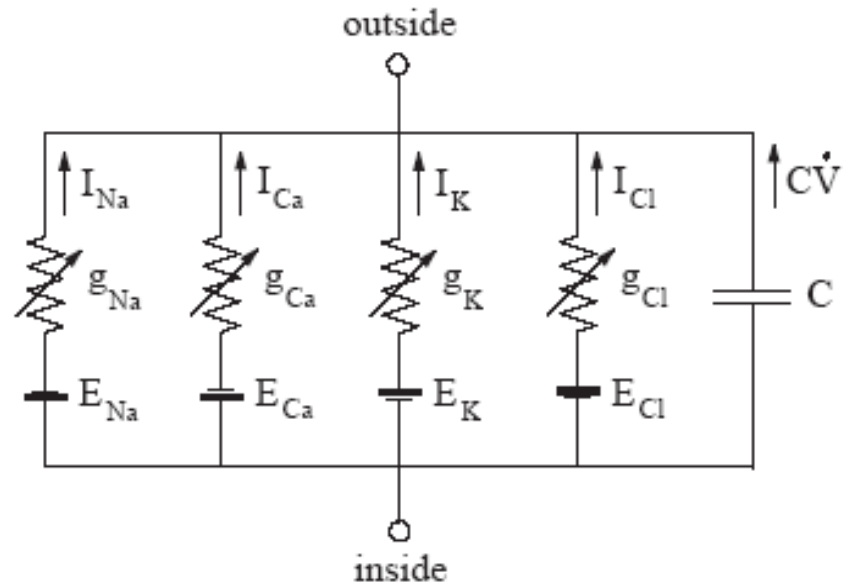
Equivalent circuit

$$I_K = g_K (V - E_K)$$

$$I_{Na} = g_{Na} (V - E_{Na})$$

$$I_{Ca} = g_{Ca} (V - E_{Ca})$$

$$I_{Cl} = g_{Cl} (V - E_{Cl})$$



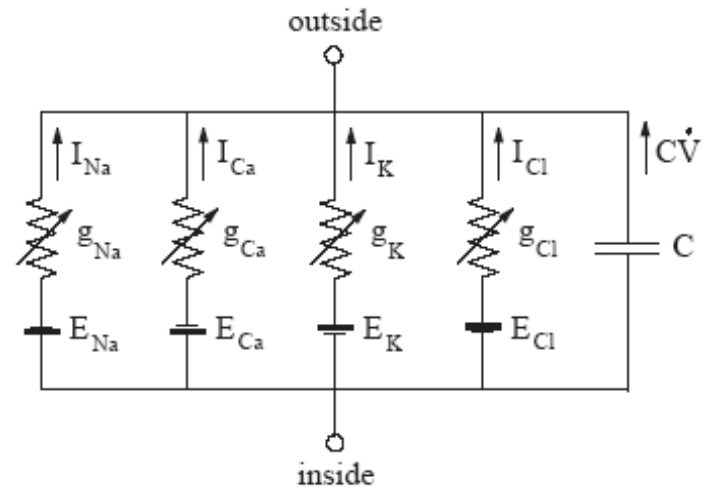
Equivalent circuit

$$I_K = g_K (V - E_K)$$

$$I_{Na} = g_{Na} (V - E_{Na})$$

$$I_{Ca} = g_{Ca} (V - E_{Ca})$$

$$I_{Cl} = g_{Cl} (V - E_{Cl})$$

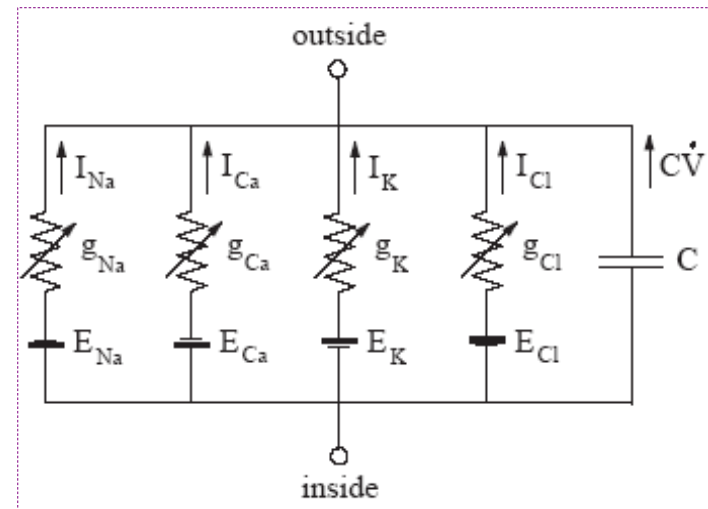
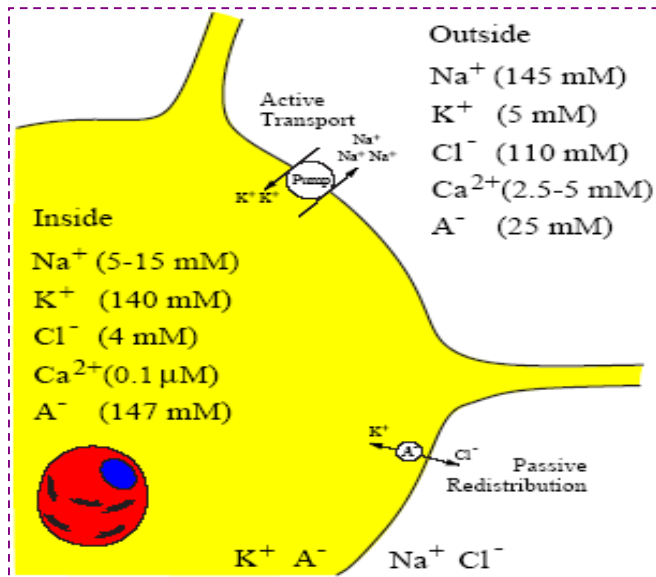


$$I = C\dot{V} + I_{Na} + I_{Ca} + I_K + I_{Cl}$$

$$C\dot{V} = I - I_{Na} - I_{Ca} - I_K - I_{Cl}$$

$$C\dot{V} = I - g_{Na} (V - E_{Na}) - g_{Ca} (V - E_{Ca}) - g_K (V - E_K) - g_{Cl} (V - E_{Cl})$$

Equivalent circuit



$$C\dot{V} = I - g_{\text{Na}}(V - E_{\text{Na}}) - g_{\text{Ca}}(V - E_{\text{Ca}}) - g_{\text{K}}(V - E_{\text{K}}) - g_{\text{Cl}}(V - E_{\text{Cl}})$$

Equivalent circuit

$$C\dot{V} = I - g_{Na}(V - E_{Na}) - g_{Ca}(V - E_{Ca}) - g_K(V - E_K) - g_{Cl}(V - E_{Cl})$$

by setting $\dot{V} = 0$ and $I = 0$

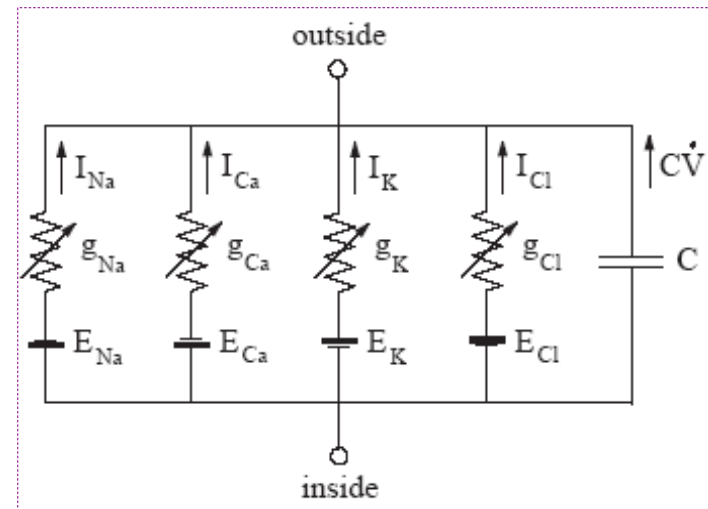
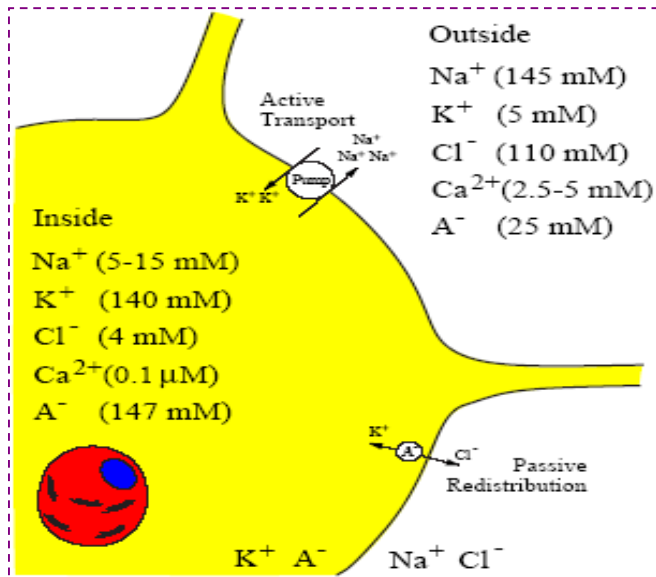
$$V_{rest} = \frac{g_{Na}E_{Na} + g_{Ca}E_{Ca} + g_K E_K + g_{Cl}E_{Cl}}{g_{Na} + g_{Ca} + g_K + g_{Cl}}$$

$$C\dot{V} = I - g_{inp}(V - V_{rest})$$

where

$$g_{inp} = g_{Na} + g_{Ca} + g_K + g_{Cl} \text{ --- input conductance.}$$

Equivalent circuit

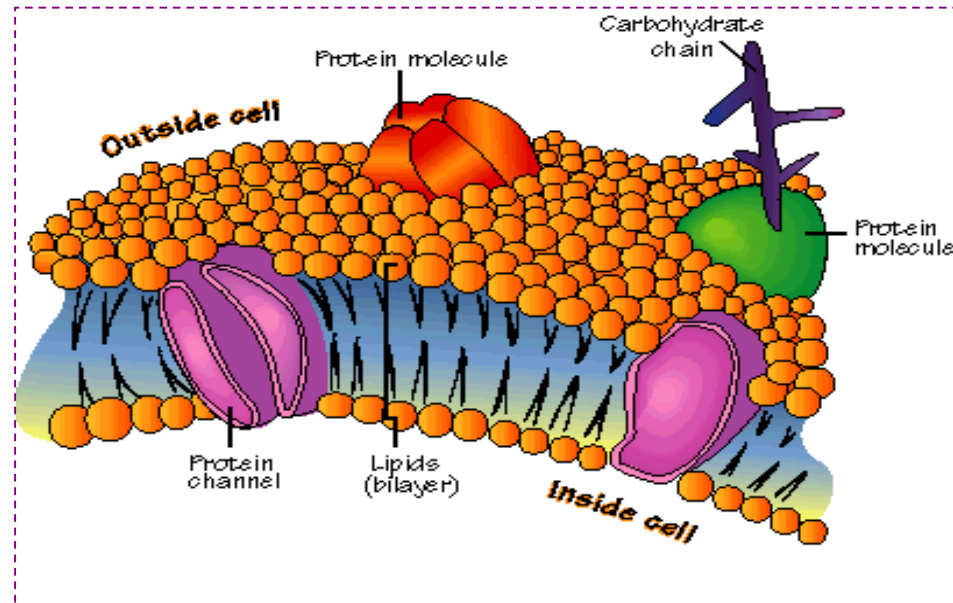
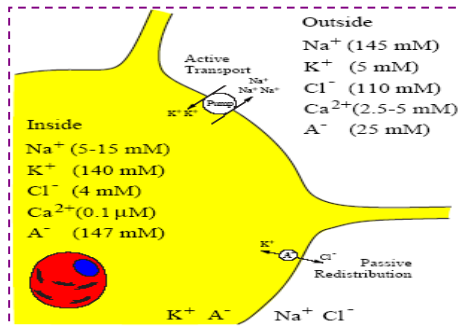


$$C\dot{V} = I - g_{\text{inp}} (V - V_{\text{rest}})$$



total 48 pages

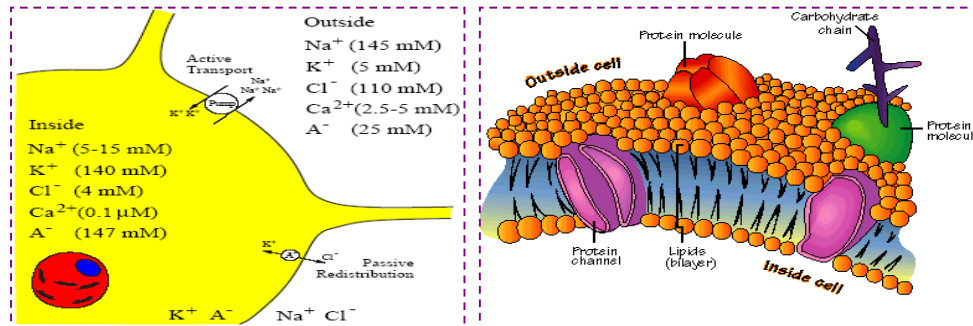
Ionic channels



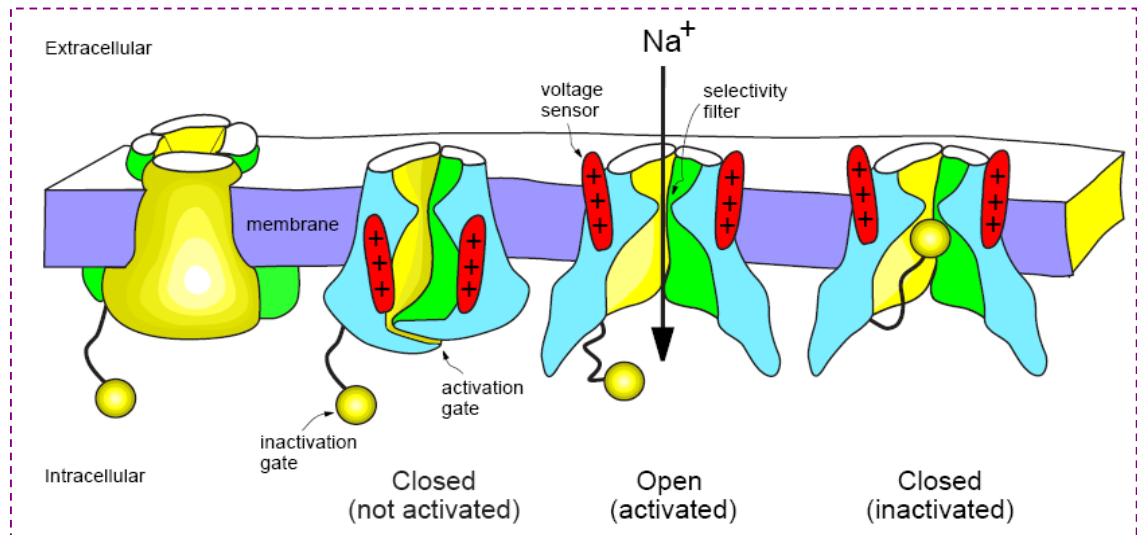
Electrical conductance of individual channels can be controlled by gating particles.

Ionic channels are large transmembrane proteins having aqueous pores through which ions can flow down their electrochemical gradients.

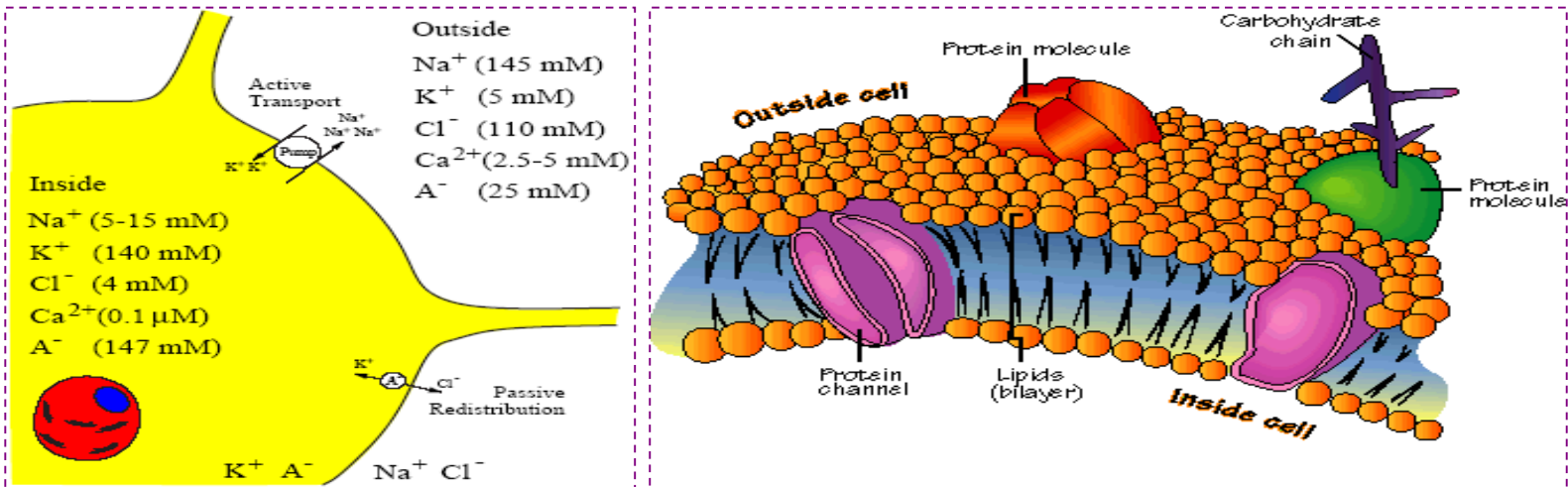
Ionic channels



Electrical conductance of individual channels can be controlled by gating particles.



Hodgkin-Huxley gate model



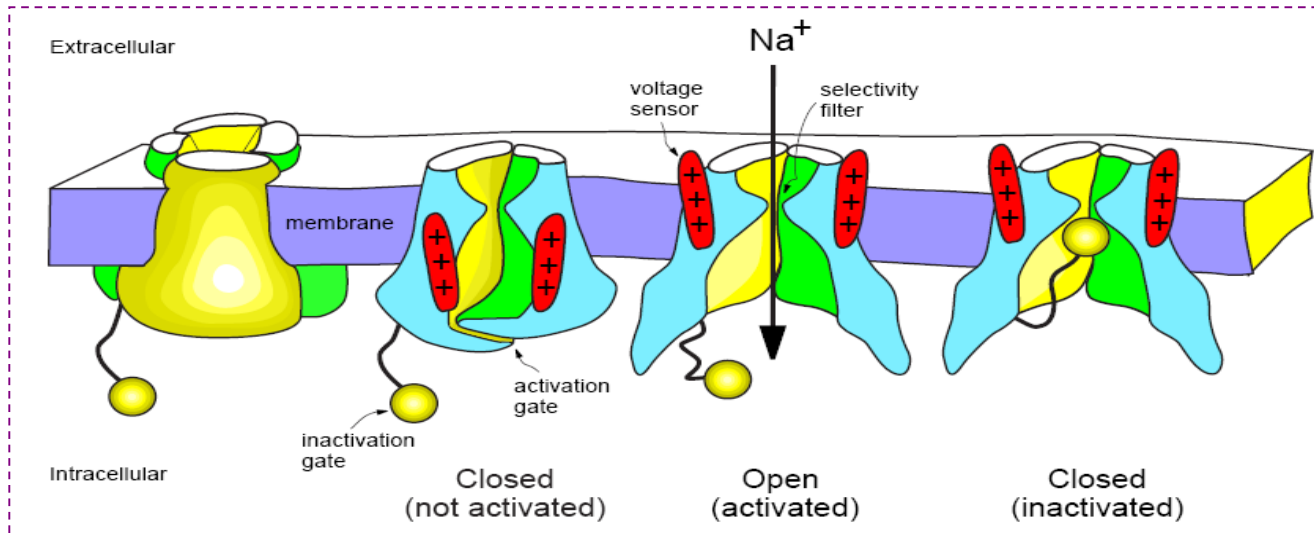
Electrical conductance of individual channels can be controlled by gating particles.

$$g_{inp} = \bar{g} p$$

p - average proportion of channels in the open state

\bar{g} - maximal conductance of the population

Hodgkin-Huxley gate model



$$g_{inp} = \bar{g} p \Rightarrow p = m^a h^b \Rightarrow g_{inp} = \bar{g} m^a h^b$$

m - probability of the activation gate to be in open state

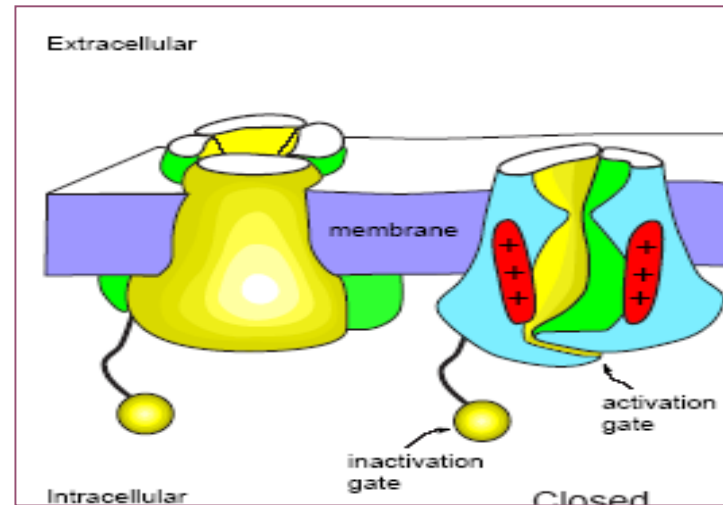
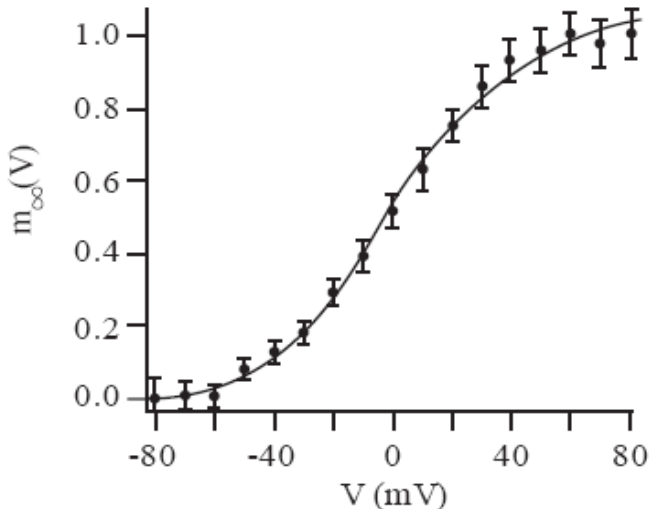
h - probability of the inactivation gate to be in open state

a - number of activation gates

b - number of inactivation gates

Activation gate

$$\tau(V) \dot{m} = (m_{\infty}(V) - m)$$

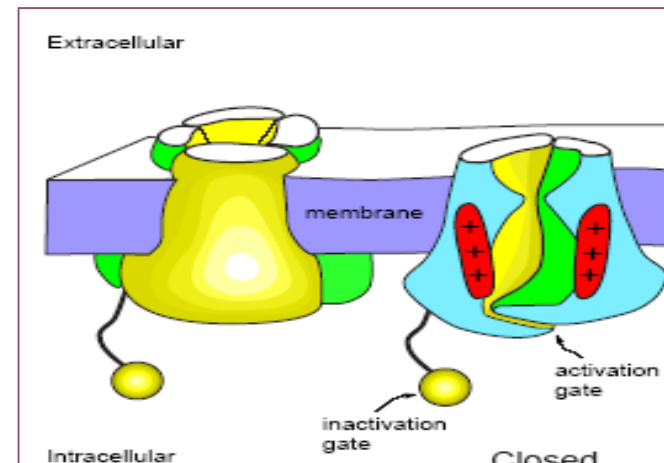
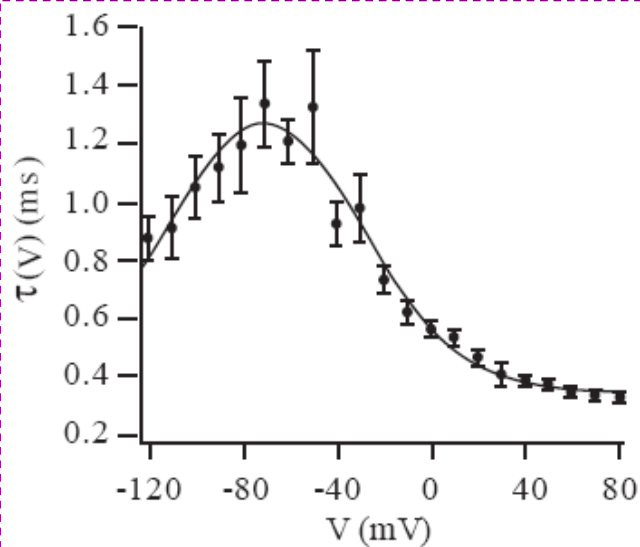


Activation function:

$$m_{\infty}(V) = \frac{1}{1 + \exp\{(V_{1/2} - V)/k\}}$$

Time constant

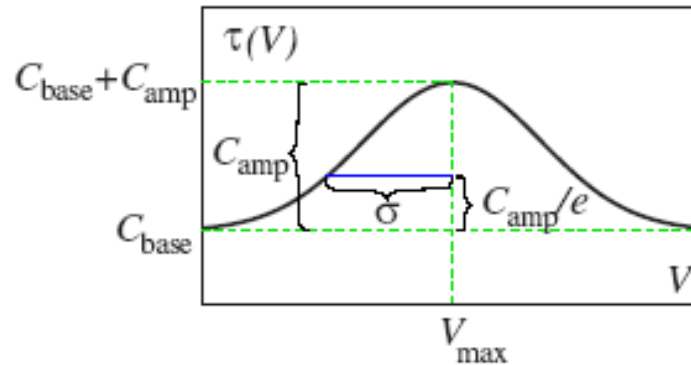
$$\tau(V) \dot{m} = (m_{\infty}(V) - m)$$



Time constant:

$$\tau(V) = C_{base} + C_{amp} \exp \frac{-(V_{max} - V)^2}{\sigma^2}$$

Time constant

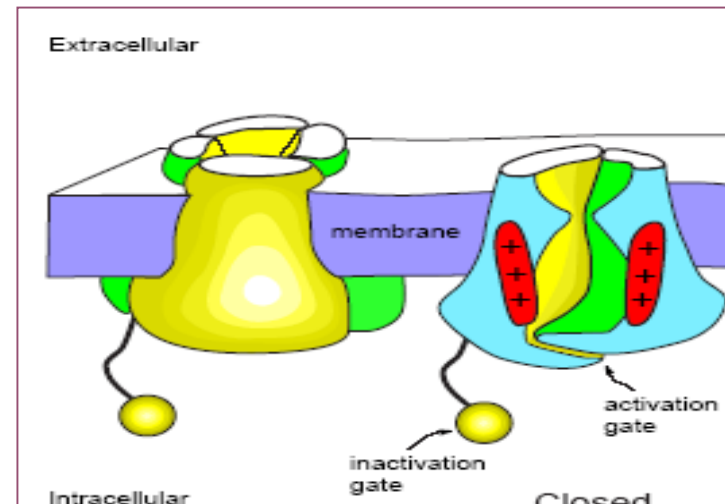
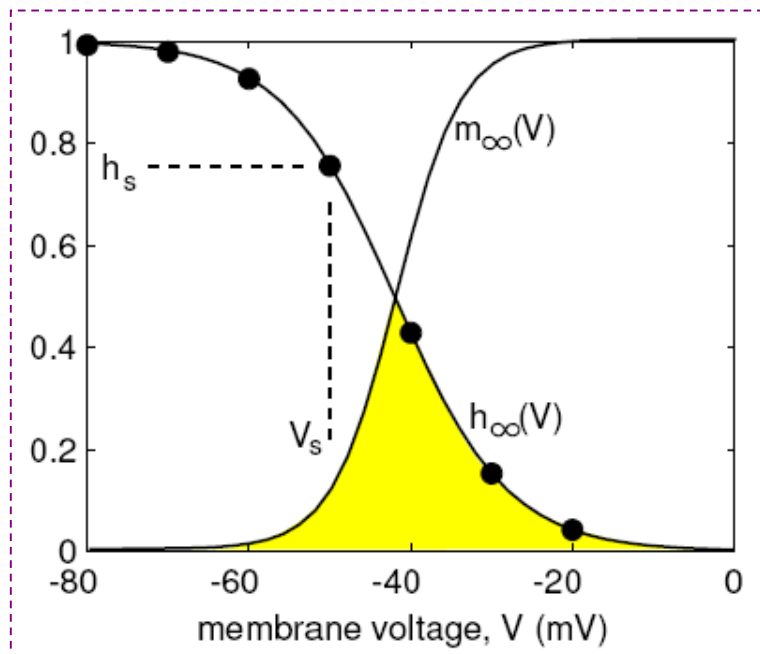


Time constant:

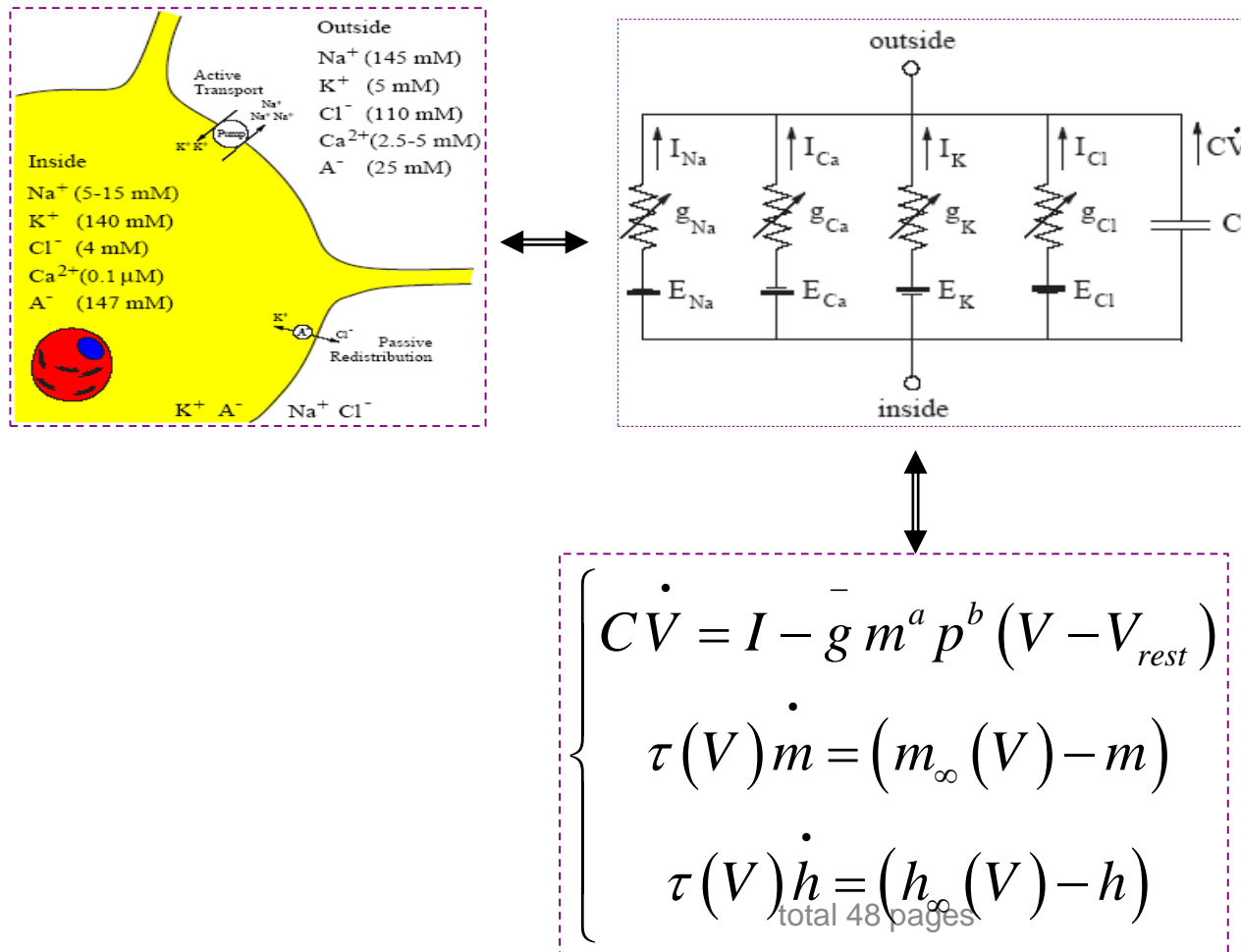
$$\tau(V) = C_{\text{base}} + C_{\text{amp}} \exp \frac{-(V_{\max} - V)^2}{\sigma^2}$$

Inactivation gate

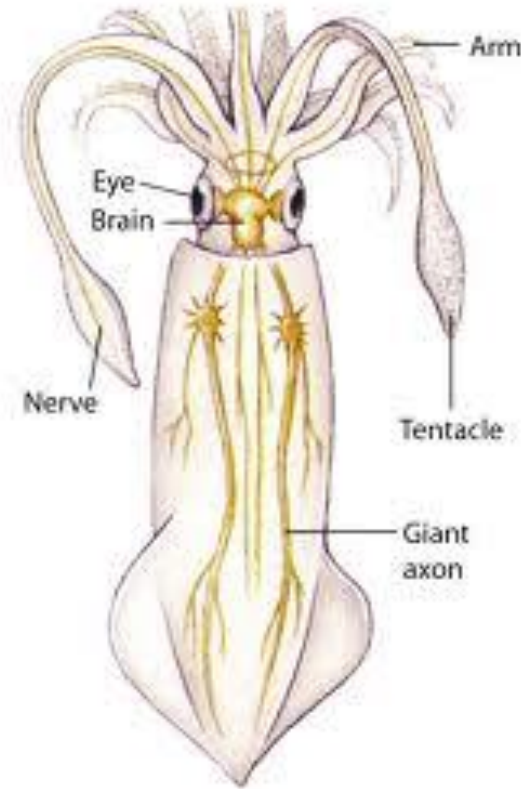
$$\tau(V) \dot{h} = (h_{\infty}(V) - h)$$



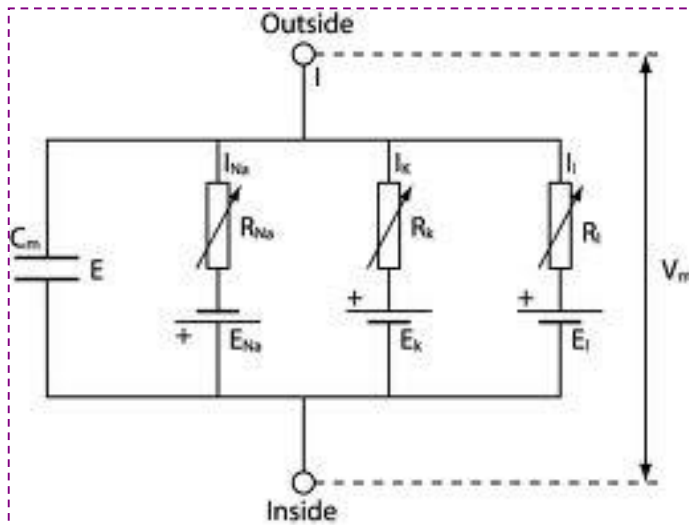
Hodgkin-Huxley Model



Hodgkin-Huxley model of the squid giant axon

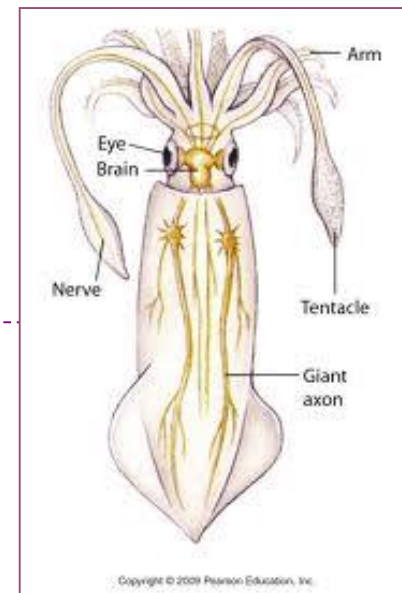


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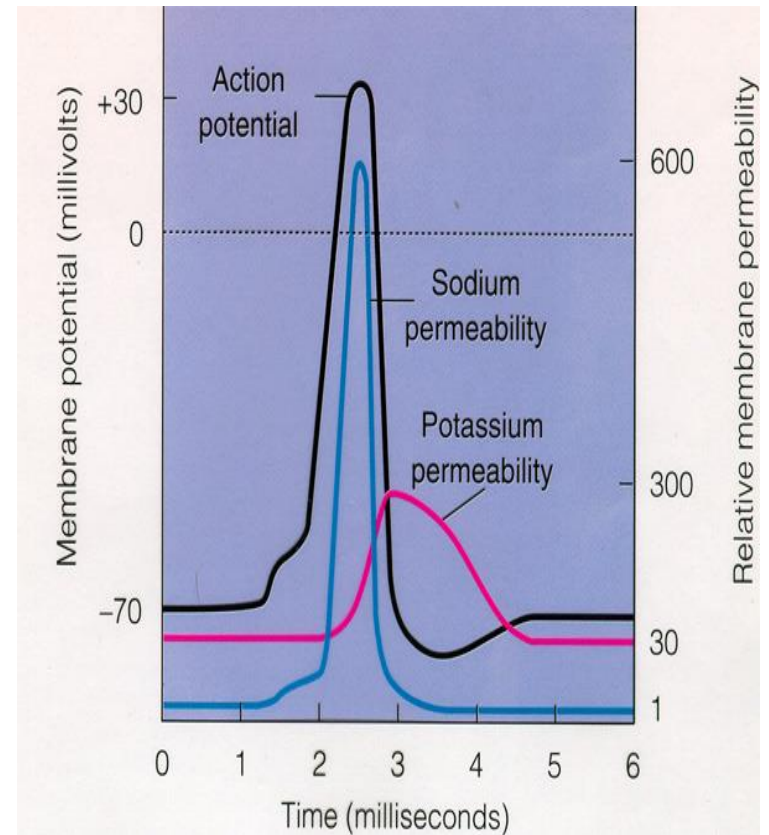
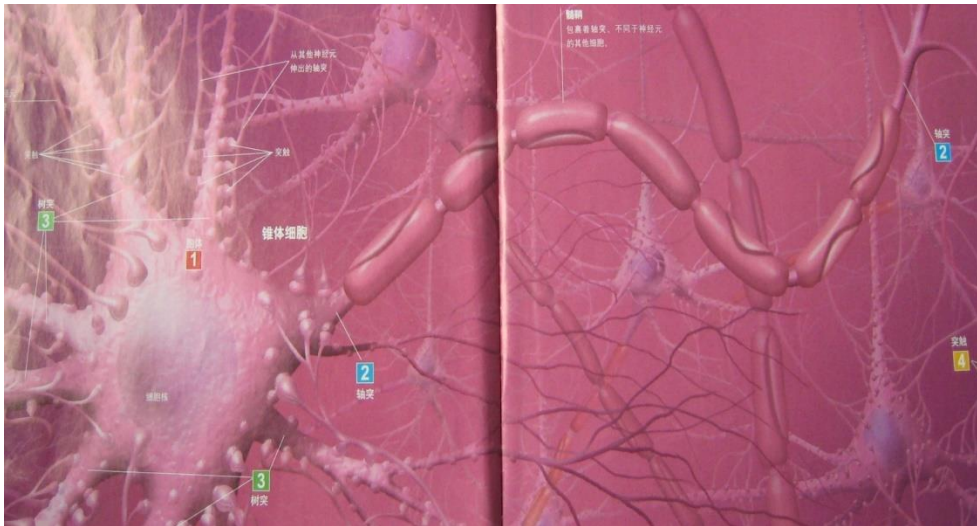
Hodgkin-Huxley model of the squid giant axon

$$\left\{ \begin{array}{l} C\dot{V} = I - \overbrace{g_K n^4 (V - E_K)}^{I_K} - \overbrace{g_{Na} m^3 h (V - E_{Na})}^{I_{Na}} - \overbrace{g_L (V - E_L)}^{I_L} \\ \dot{n} = \alpha_n(V)(1-n) - \beta_n(V)n \\ \dot{m} = \alpha_m(V)(1-m) - \beta_m(V)m \\ \dot{h} = \alpha_h(V)(1-h) - \beta_h(V)h \end{array} \right.$$

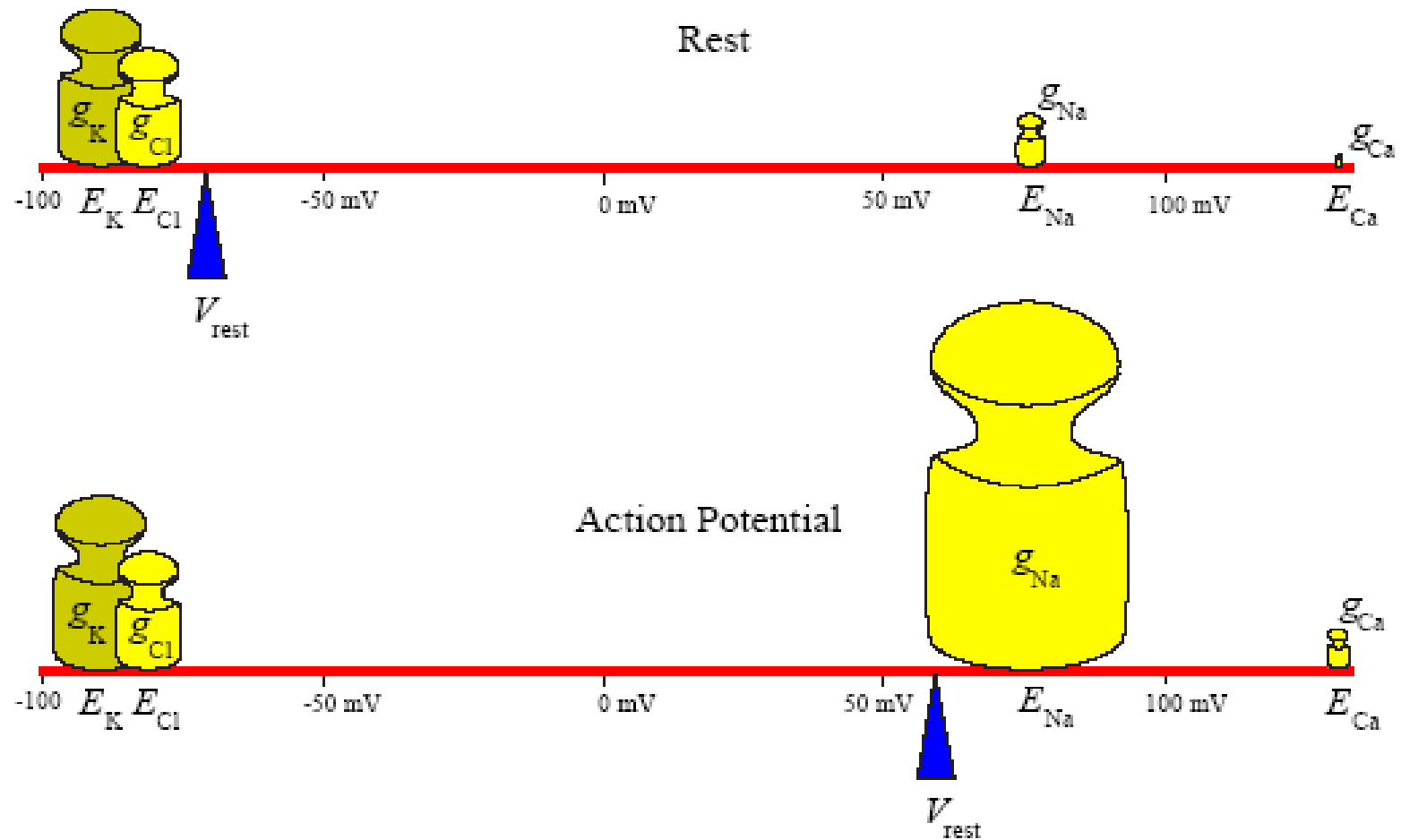


1963 Nobel prize in physiology or medicine

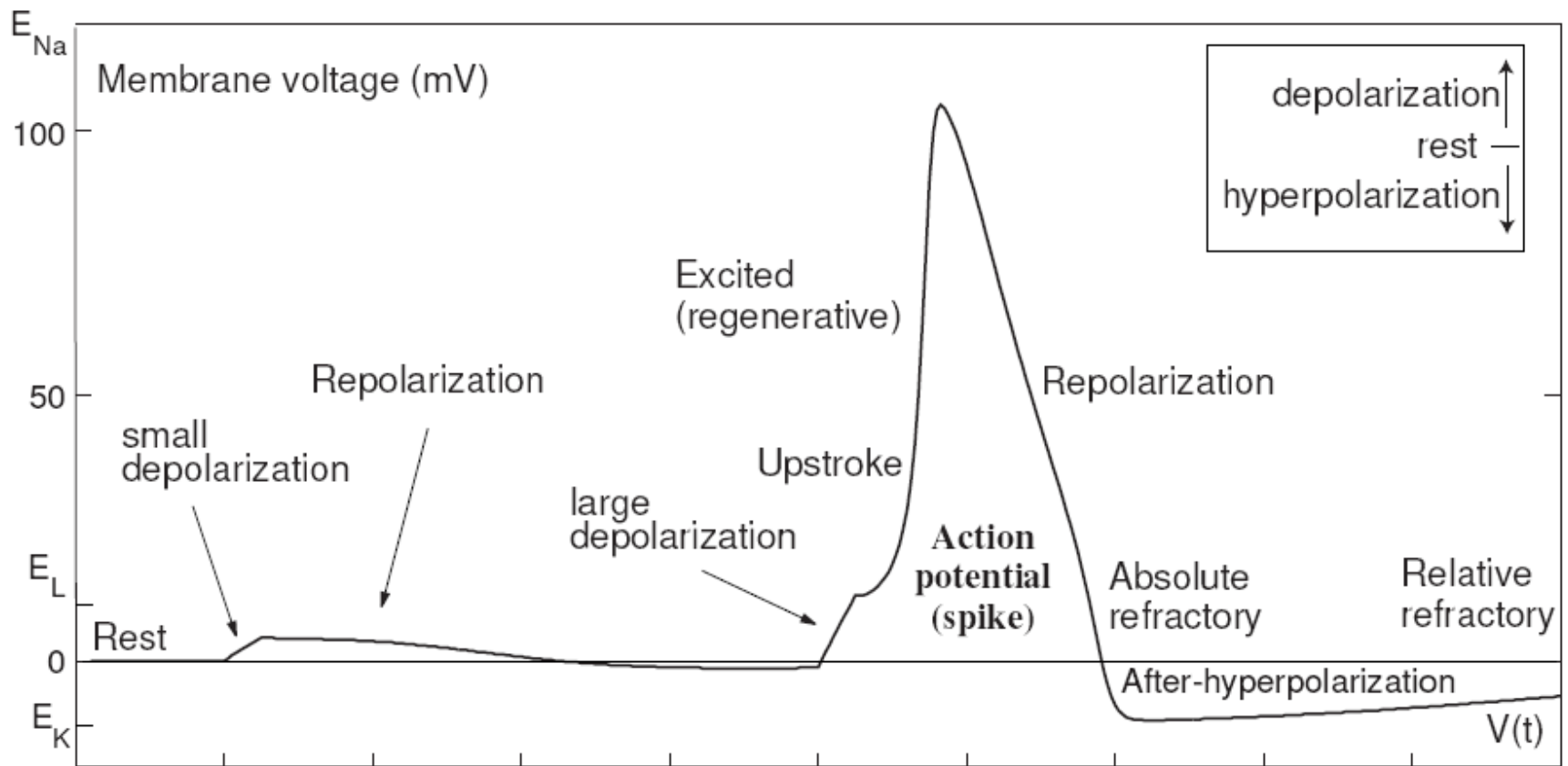
Action potential



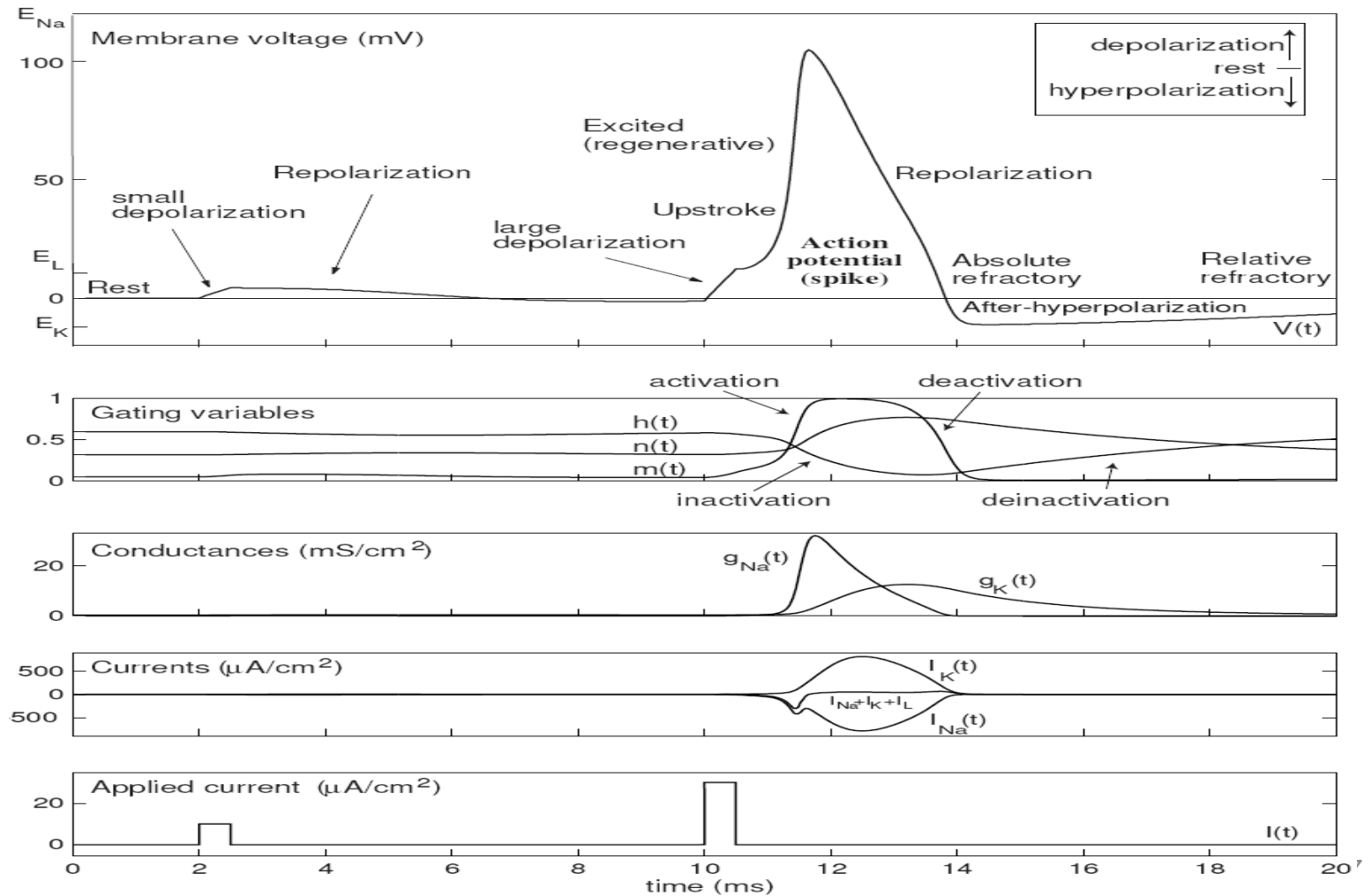
Action potential



Action potential



Action potential





The End