

A Brief Summary of Three Selected Projects

Tasks

- ✓ Regression (IQA) and Classification (EEG)

IQA Research Novelty

- ✓ [Definition] Non-local Modeling and Local Modeling
- ✓ [Definition] Global Distortions and Local Distortions
- ✓ [Motivation] Human Visual System (HVS) perceives Image Quality:
Adaptive to local content + Long-range Dependency constructed among different regions
- ✓ [Method] Superpixel-based Graph Neural Network to explore Non-local Interactions

EEG Research Novelty

- ✓ [Motivation] Graph Modeling for EEG Electrodes System
- ✓ [Method] Graph Representation Learning of EEG Signals
- ✓ [Motivation] Spatial-Temporal Analysis of EEG Signals
- ✓ [Method] Deep Feature Mining of EEG Signals



No-reference Image Quality Assessment via Non-local Modeling



GCNs-Net: A Graph Convolutional Neural Network Approach for Decoding Time-Resolved EEG Motor Imagery Signals



Deep Feature Mining via Attention-based BiLSTM-GCN for Human Motor Imagery Recognition

Selected Research Projects

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January 10th, 2023

<https://github.com/SuperBruceJia>

No-reference Image Quality Assessment via Non-local Modeling

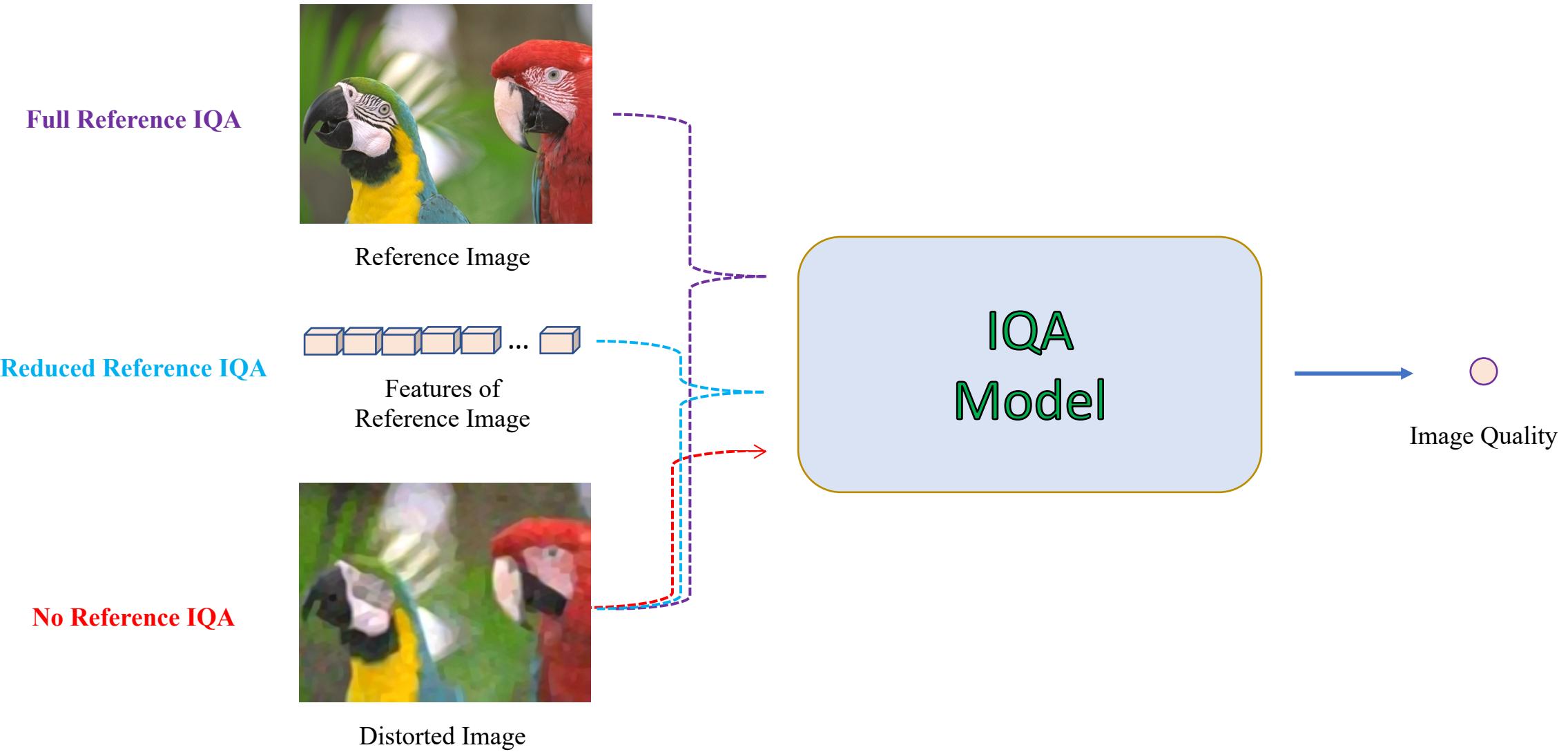
Shuyue Jia¹, Baoliang Chen¹, Dingquan Li², and Shiqi Wang^{1*}

¹ Department of Computer Science, City University of Hong Kong

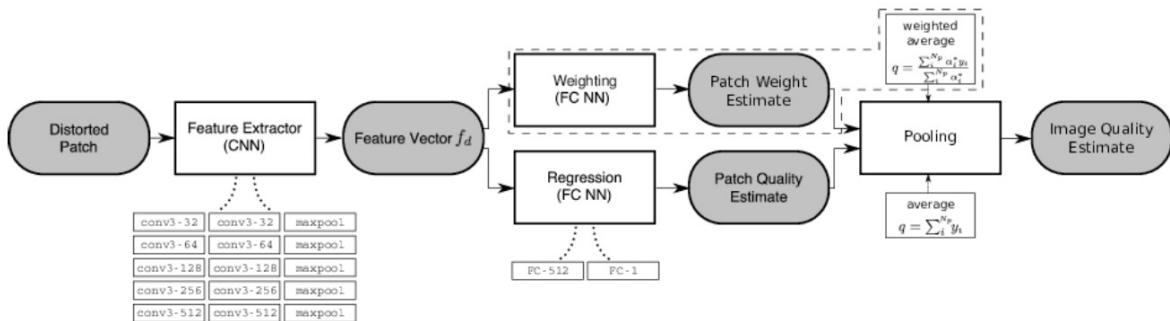
² Peng Cheng Laboratory

Project: <https://github.com/SuperBruceJia/NLNet-IQA>

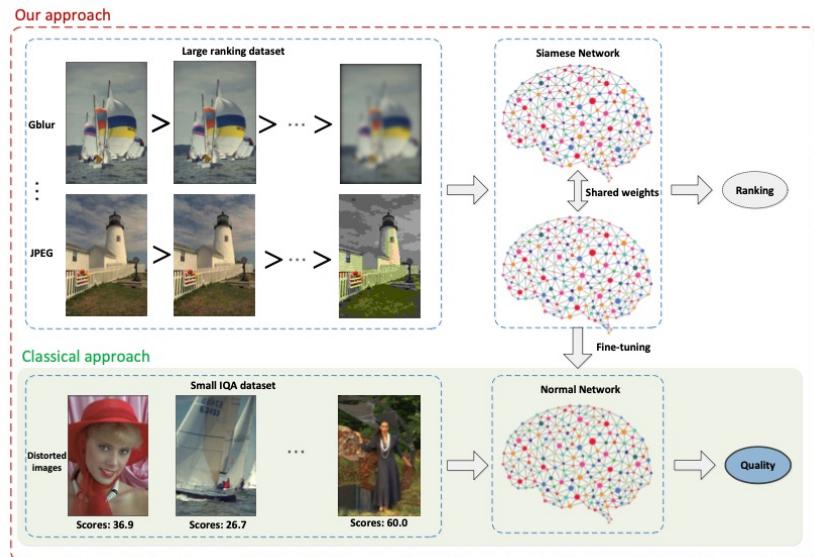
Image Quality Assessment (IQA)



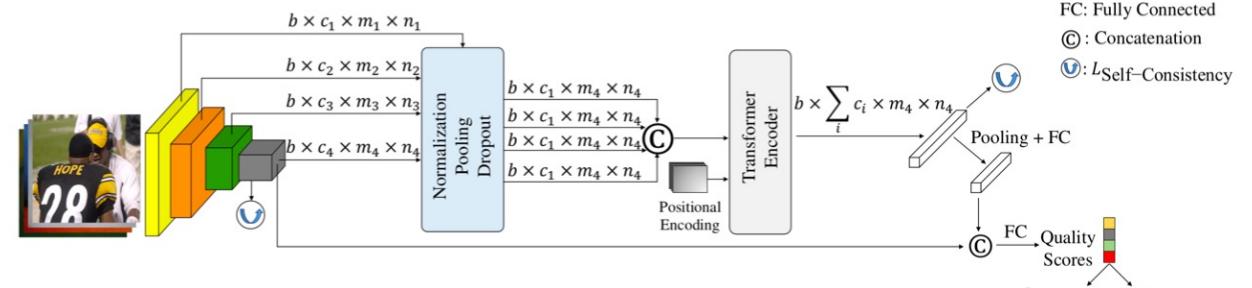
Recent Progress on No-reference IQA



CNN-based Methods [1]



Ranking-based Methods [2]



Transformer-based Methods [3]

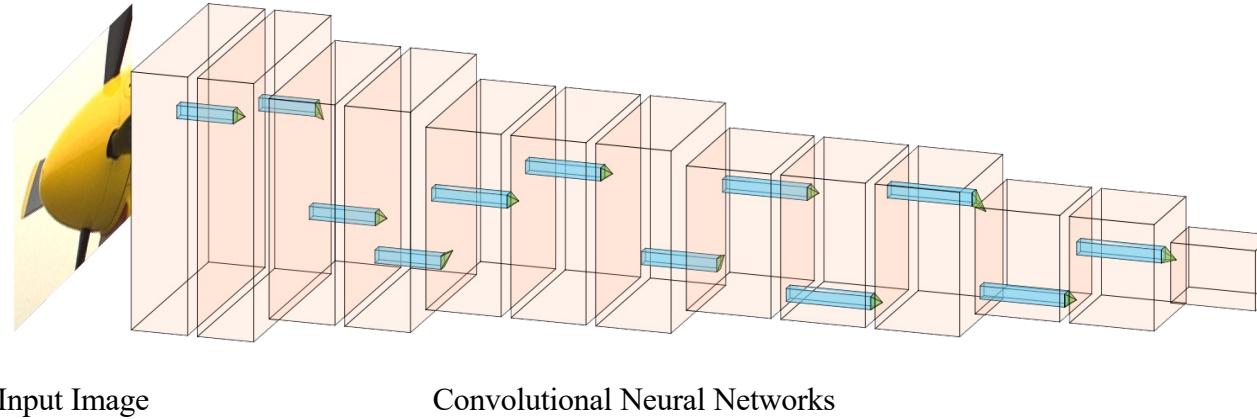
Credit:

[1] Bosse *et al.*, Deep Neural Networks for No-Reference and Full-Reference Image Quality Assessment, In TIP 2018

[2] Liu *et al.*, RankIQA: Learning from Rankings for No-reference Image Quality Assessment, In ICCV 2017

[3] Golestaneh *et al.*, No-Reference Image Quality Assessment via Transformers, Relative Ranking, and Self-Consistency, In WACV 2022

Challenges

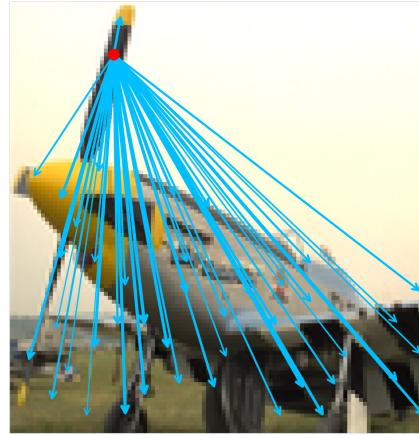


- **Local Modeling** (Convolutional Neural Networks):
 - ✓ Translation Invariance (Pooling)
 - ✓ Translation Equivalence (Convolution)
 - ✓ Sharable Parameters (Weight Sharing)
- **Limitations:**
 - ✓ Small-sized Receptive Field → **Extracted features are too local**
 - ✓ Parameters Fixed across the whole image → **Image content is equally treated**
 - ✓ Lack of Geometric and Relational Modeling → **Missing complex relations and dependencies**

Motivation



Local Feature Extraction



Non-local Dependency

- ✓ HVS is Adaptive to the Local Content

→ ***Local feature extraction*** via a pre-trained CNN

- ✓ HVS perceives image quality with Long-range Dependency Constructed among Different Regions

→ ***Non-local feature extraction*** for long-range dependency and relational modeling

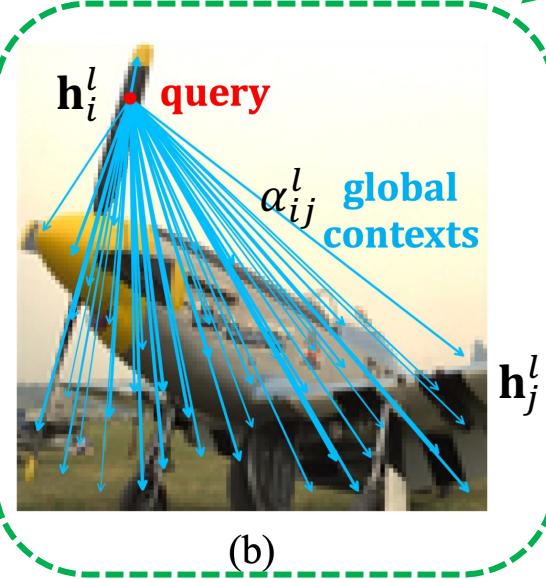
Definition



**Convolution:
Pixel-to-Pixel
Modeling**

Local feature extraction is critical

Figure 2: Local region feature extraction and non-local dependency feature extraction



**Non-Local:
Object-to-Pixel
Modeling** *Beauty is in Simplicity*

Spatial Integration of Information

$$\mathbf{h}_i^l = \text{ELU} \left(\sum_{j \in \mathcal{N}(i)} \alpha_{ij}^l \mathbf{W}^l \mathbf{h}_j^l \right)$$

Spatial Weighting Functions

$$\alpha_{ij}^l = \frac{\exp(a_{ij}^l)}{\sum_{k \in \mathcal{N}(i)} a_{ik}^l}$$

$$a_{ij}^l = \text{LeakyReLU}(\text{FC}([\mathbf{W}^l \mathbf{h}_i^l \parallel \mathbf{W}^l \mathbf{h}_j^l]))$$

- ✓ **Local Modeling:** encodes spatially proximate **Local Neighborhoods**.
- ✓ **Non-local Modeling:** establishes **Spatial Integration of Information** by **Long- and Short-Range Communications** with different **Spatial Weighting Functions**.

Communications with different Spatial Weighting Functions.

Non-local Behavior

Object-to-Pixel Modeling
Region Feature Extraction



**Non-local
Dependency & Relational
Modeling**



Semantics and Content
Understanding

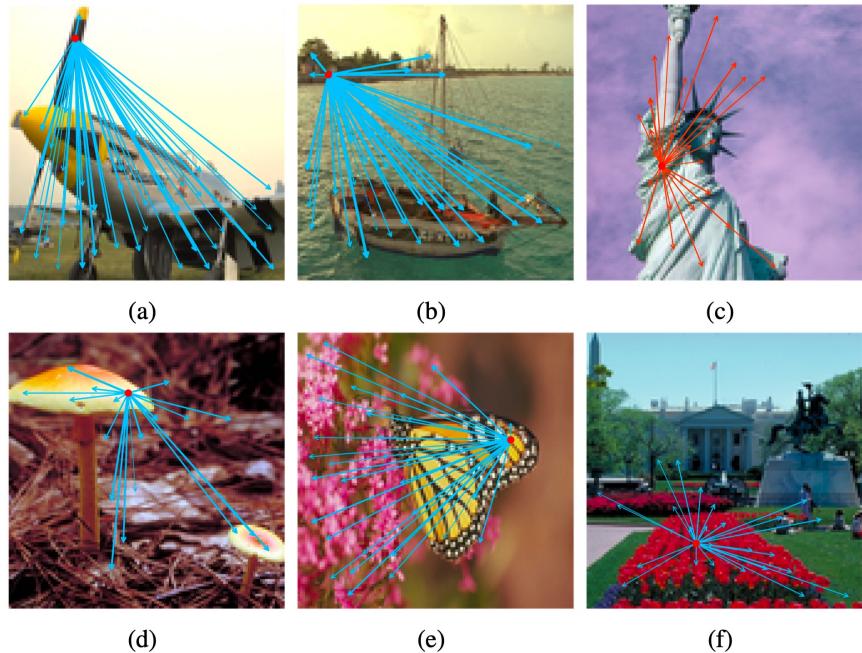


Figure 3.1: The non-local behavior of the long-range dependency and relational modeling. (a) The plane image with a query on wings. (b) The boat image with a query on nearby river bank. (c) The Statue of Liberty image with a query on the lady. (d) The shrooms image with a query on one shroom. (e) The butterfly image with a query on the wing. (f) The Lafayette Square, Washington, D.C. image with a query on flowers.

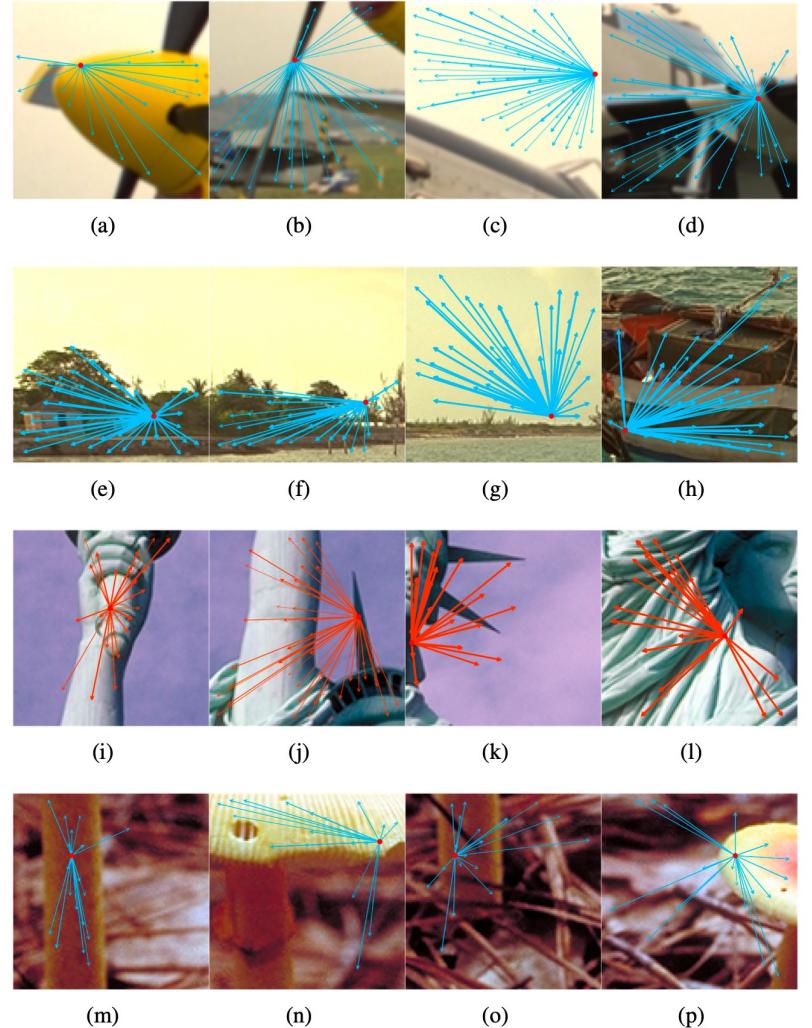


Figure 3.2: Selected demonstrations of the non-local behavior and long-range dependencies with regard to the cropped image patches from the illustrated images.
The details of Figure (a) to (p) are described in the thesis.

- ✓ **Non-local Modeling:** establishes the **Spatial Integration of Information**

by **Long- and Short-Range Communications with different Spatial Weighting Functions.**

Definition

Non-Local Recurrence

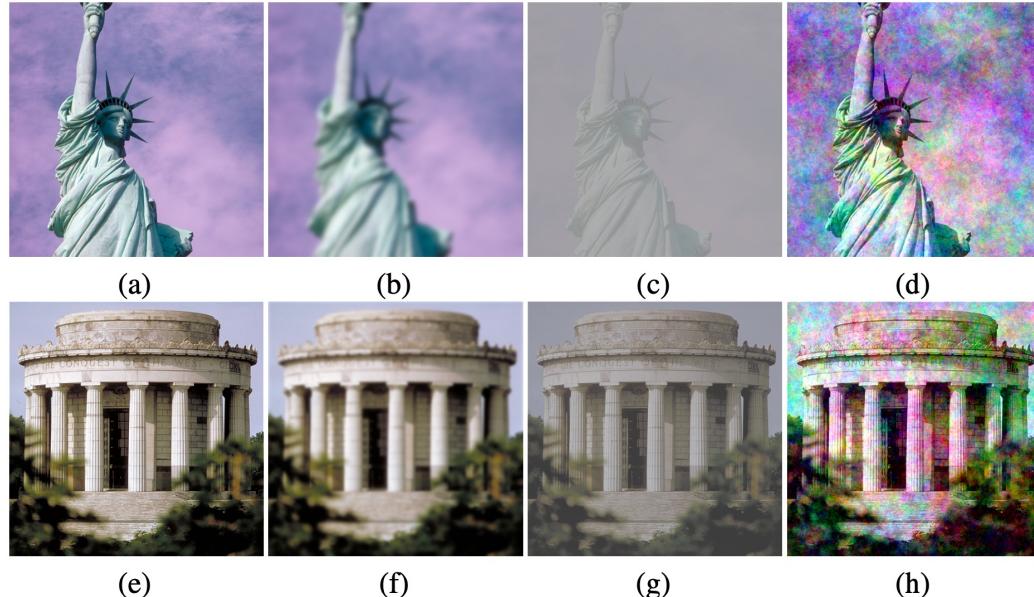


Figure 4.9: Demonstrations of the global distortions (b/f: GB, c/g: CC, d/h: PN) contaminating the Statue of Liberty and George Rogers Clark Memorial images.

Figure (a) and Figure (e) are reference images from the CSIQ database.

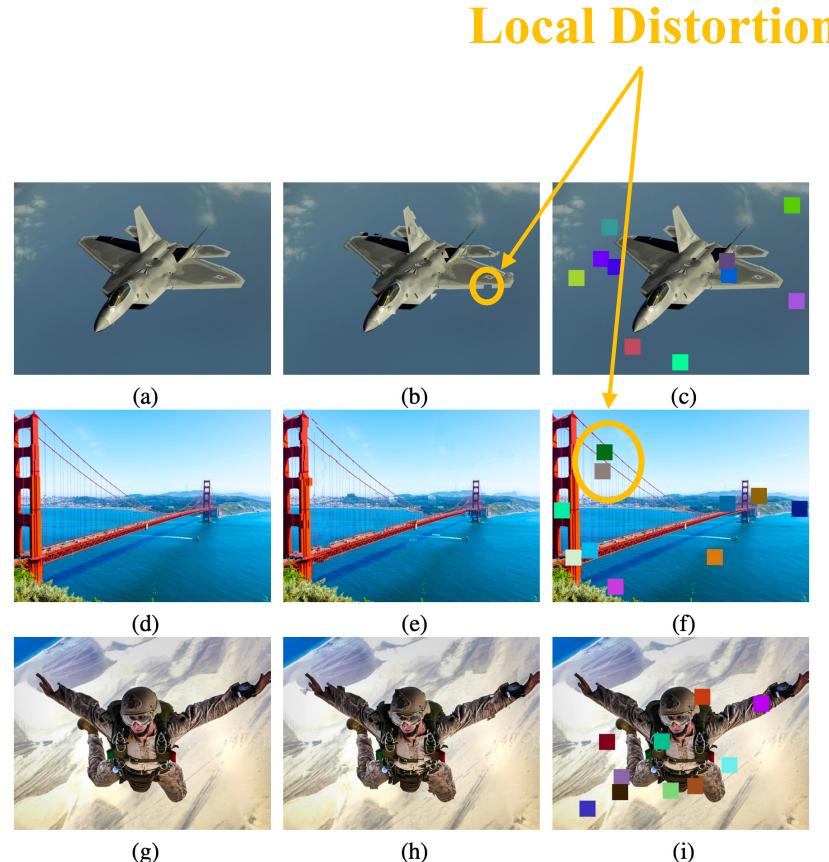


Figure 4.11: Demonstrations of the local distortions (b/e/h: non-eccentricity patch and c/f/i: color block). Figure (a), Figure (d), and Figure (g) are reference images from the KADID-10k database.

- ✓ **Global Distortion: Globally and Uniformly Distributed** distortions with **Non-Local Recurrences** over the image.
- ✓ **Local Distortion: Local Nonuniform-Distributed** distortions **in a Local Region**.

Superpixel Segmentation

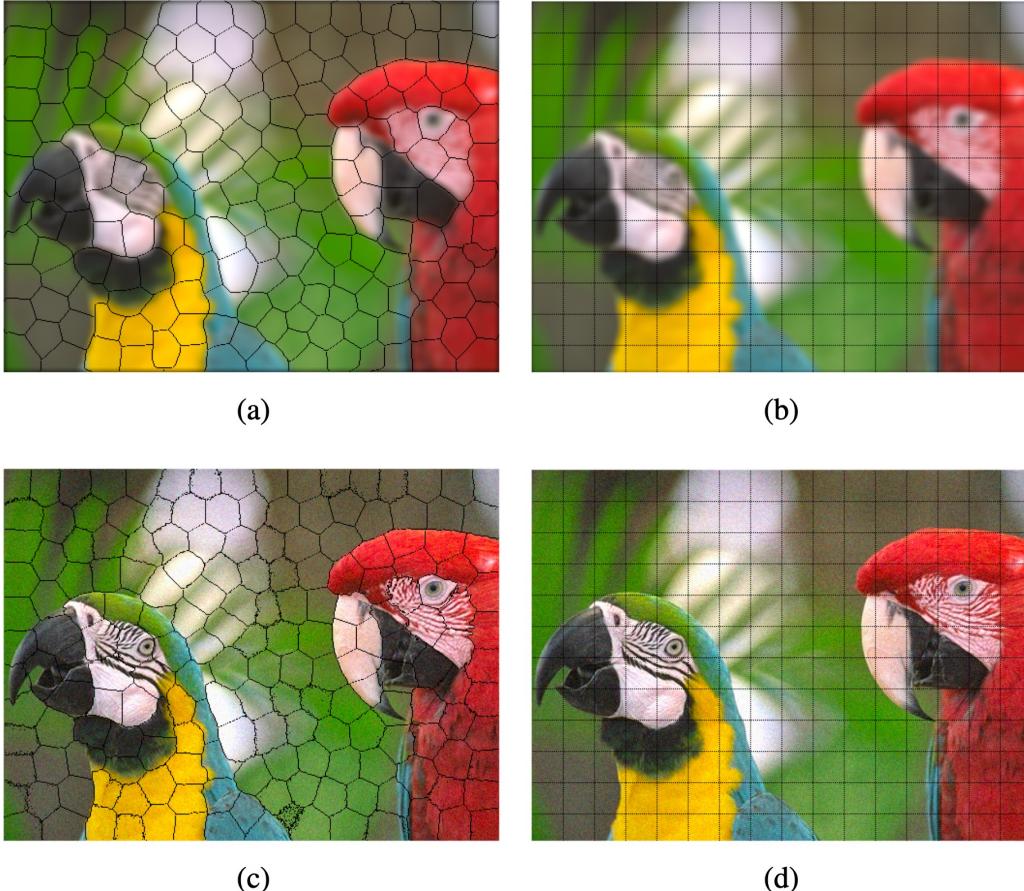


Figure 4.2: The superpixel *vs.* square patch representation (with size of $\approx 32 \times 32$) of the plane image from the TID2013 database.

Superpixel *vs.* Square Patch

- ✓ Adherence to boundaries and **Visually Meaningful**
- ✓ **Accurate Feature Extraction**

Superpixel Segmentation

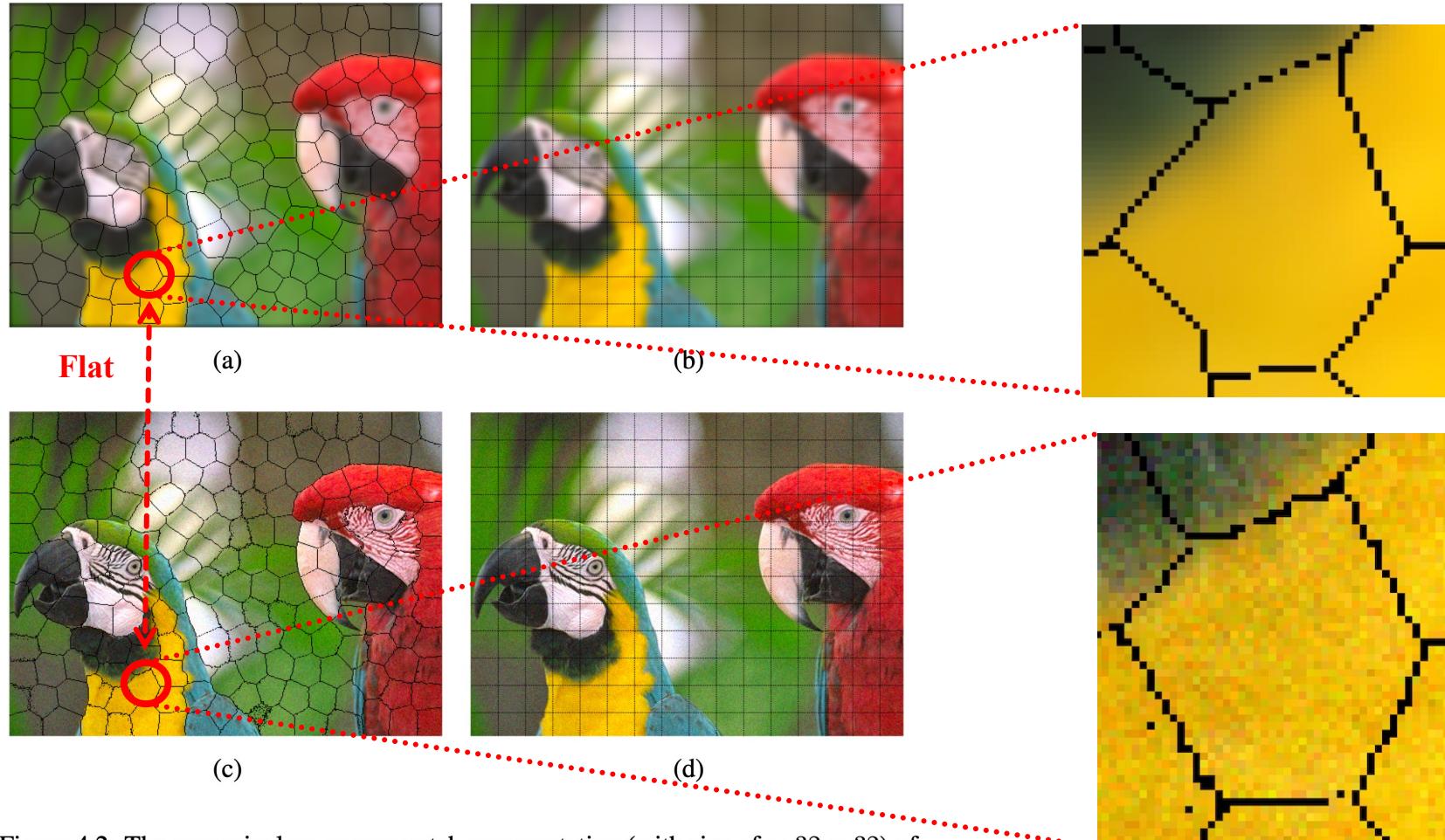


Figure 4.2: The superpixel vs. square patch representation (with size of $\approx 32 \times 32$) of the plane image from the TID2013 database.

Superpixel Segmentation

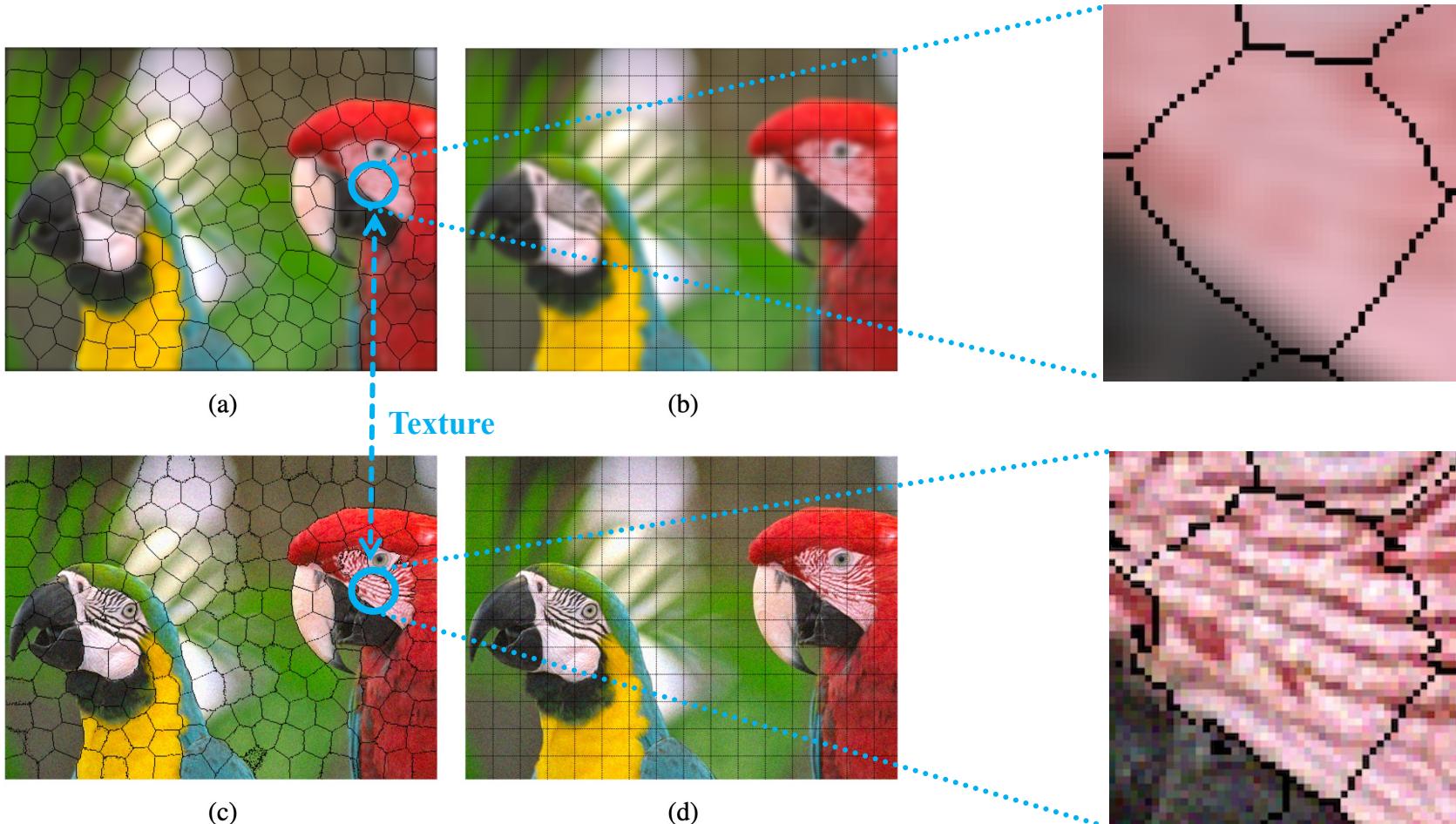
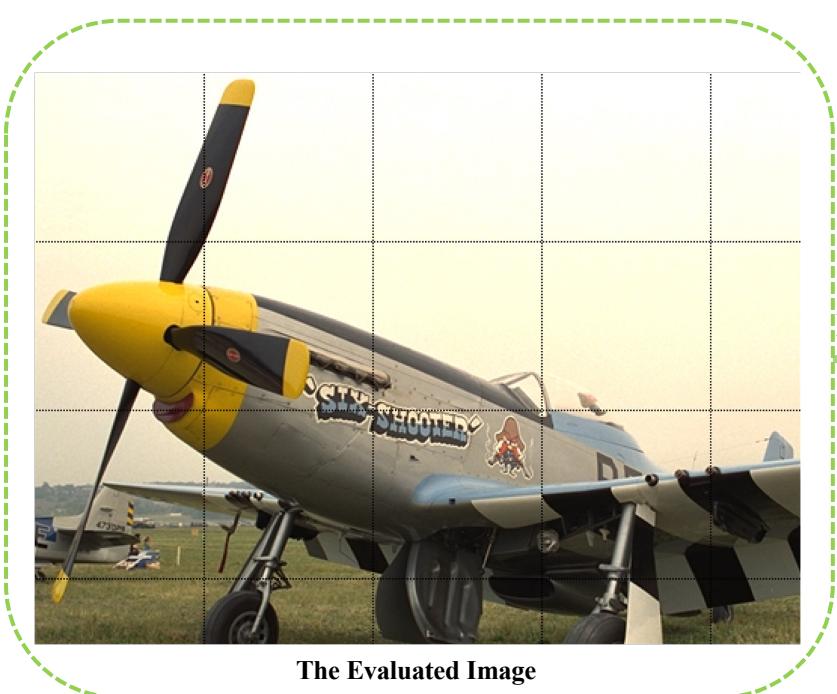


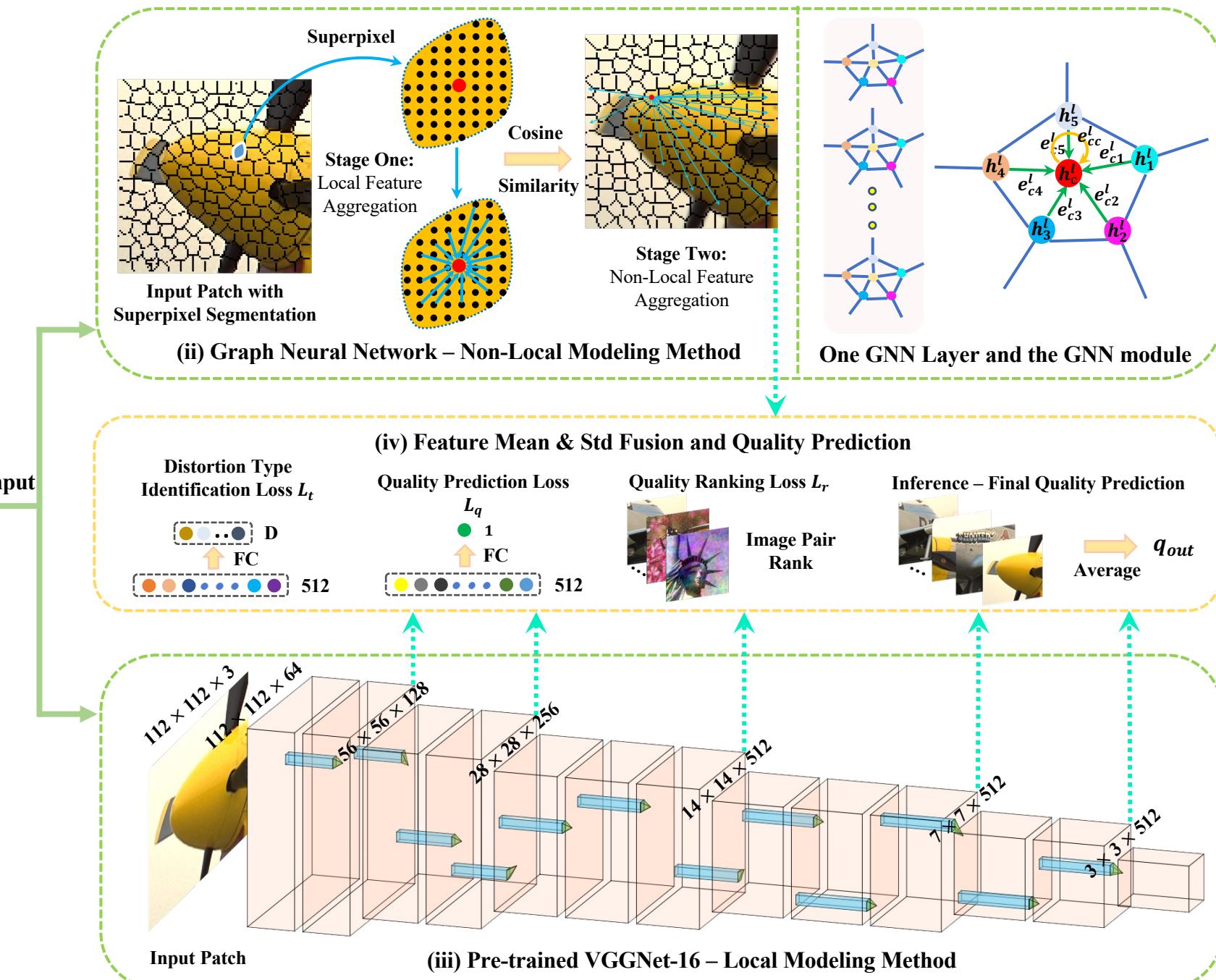
Figure 4.2: The superpixel vs. square patch representation (with size of $\approx 32 \times 32$) of the plane image from the TID2013 database.

NLNet

Architecture



(i) Image Preprocessing



Experimental Setup

- **Databases:**
 - ✓ LIVE, CSIQ, TID2013, and KADID-10k
- **Evaluation Metrics:**
 - ✓ SRCC (Spearman Rank-order Correlation Coefficient)
 - ✓ PLCC (Pearson Linear Correlation Coefficient)
- **Experimental Setting:**
 - ✓ Intra-Database Experiments:
 - 60% training, **20% validation**, and
 - 20% testing, with `random` seeds from 1 to 10
 - The median SRCC and PLCC are reported.
 - ✓ Cross-Database Evaluations:
 - One database as the training set, and the other databases as the testing set
 - Report the last epoch's performance

Screen Content



Figure 1.1: Natural images and a screen content image from the constructed databases.
(a) LIVE Database [13] (b) CSIQ Database [14] (c) TID2013 Database [15] (d)
KADID-10k Database [16].

Table 4.1: Brief summary of the LIVE, CSIQ, TID2013, and KADID-10k databases.

Database	LIVE [13]	CSIQ [14]	TID2013 [15]	KADID-10k [16]
Num. of Reference Images	29	30	25	81
Num. of Distorted Images	779	866	3,000	10,125
Num. of Distortion Types	5	6	24	25
Num. of Distortion Levels	5 ~ 8	3 ~ 5	5	5
Annotation	DMOS	DMOS	MOS	MOS
Range	[0, 100]	[0, 1]	[0, 9]	[1, 5]

Natural Images

Intra-Database Experiments

Table 4.2: Performance comparisons on the LIVE, CSIQ, and TID2013 databases.
Top two results are highlighted in bold.

**SOTA
Transformer**

**Fewer Training Data
↓ 20% Total Data
↑ Highly Competitive Performance**

Method	LIVE		CSIQ		TID2013	
	SRCC	PLCC	SRCC	PLCC	SRCC	PLCC
BRISQUE (2012) [10]	0.939	0.935	0.746	0.829	0.604	0.694
CORNIA (2012) [104]	0.947	0.950	0.678	0.776	0.678	0.768
M3 (2015) [105]	0.951	0.950	0.795	0.839	0.689	0.771
HOSA (2016) [103]	0.946	0.947	0.741	0.823	0.735	0.815
FRIQUEE (2017) [90]	0.940	0.944	0.835	0.874	0.68	0.753
DIQaM-NR (2018) [35]	0.960	0.972	-	-	0.835	0.855
DB-CNN (2020) [64]	0.968	0.971	0.946	0.959	0.816	0.865
HyperIQA (2020) [65]	0.962	0.966	0.923	0.942	0.729	0.775
GraphIQA (2022) [86]	0.968	0.970	0.920	0.938	-	-
TReS (2022) [87]	0.969	0.968	0.922	0.942	0.863	0.883
NLNet	0.962	0.963	0.941	0.958	0.856	0.880

Table 4.3: Performance comparisons on the KADID-10k database.

Top two results are highlighted in bold.

Method	BRISQUE [10]	CORNIA [104]	HOSA [103]	InceptionResNetV2 [16]	DB-CNN [64]	HyperIQA [65]	TReS [87]	NLNet
SRCC	0.519	0.519	0.609	0.731	0.851	0.852	0.859	0.846
PLCC	0.554	0.554	0.653	0.734	0.856	0.845	0.858	0.850

Cross-Database Settings and Evaluations

Table 4.9: Cross-database performance comparisons.

Training	LIVE		CSIQ		TID2013	
Testing	CSIQ	TID2013	LIVE	TID2013	LIVE	CSIQ
BRISQUE (2012) [10]	0.562	0.358	0.847	0.454	0.790	0.590
CORNIA (2012) [104]	0.649	0.360	0.853	0.312	0.846	0.672
M3 (2015) [105]	0.621	0.344	0.797	0.328	0.873	0.605
HOSA (2016) [103]	0.594	0.361	0.773	0.329	0.846	0.612
FRIQUEE (2017) [90]	0.722	0.461	0.879	0.463	0.755	0.635
DIQaM-NR (2018) [35]	0.681	0.392	-	-	-	0.717
DB-CNN (2020) [64]	0.758	0.524	0.877	0.540	0.891	0.807
HyperIQA (2020) [65]	0.697	0.538	0.905	0.554	0.839	0.543
NLNet	0.771	0.497	0.923	0.516	0.895	0.730

Similar
Distortions

TID:
More Distortion Types & Levels

Single Distortion Type Evaluation

Table 4.4: The average SRCC and PLCC results of the individual distortion type on the LIVE database. Top two results are highlighted in bold.

SRCC	Global Distortion				Local Distortion FF
	JPEG	JP2K	WN	GB	
BRISQUE (2012) [10]	0.965	0.929	0.982	0.964	0.828
CORNIA (2012) [104]	0.947	0.924	0.958	0.951	0.921
M3 (2014) [105]	0.966	0.930	0.986	0.935	0.902
HOSA (2016) [103]	0.954	0.935	0.975	0.954	0.954
FRIQUEE (2017) [90]	0.947	0.919	0.983	0.937	0.884
dipIQ (2017) [82]	0.969	0.956	0.975	0.940	-
WaDIQaM (2018) [35]	0.953	0.942	0.982	0.938	0.923
DB-CNN (2020) [64]	0.972	0.955	0.980	0.935	0.930
HyperIQA (2020) [65]	0.961	0.949	0.982	0.926	0.934
NLNet	0.979	0.958	0.990	0.964	0.941
PLCC	Global Distortion				Local Distortion FF
	JPEG	JP2K	WN	GB	
BRISQUE (2012) [10]	0.971	0.940	0.989	0.965	0.894
CORNIA (2012) [104]	0.962	0.944	0.974	0.961	0.943
M3 (2014) [105]	0.977	0.945	0.992	0.947	0.920
HOSA (2016) [103]	0.967	0.949	0.983	0.967	0.967
FRIQUEE (2017) [90]	0.955	0.935	0.991	0.949	0.936
dipIQ (2017) [82]	0.980	0.964	0.983	0.948	-
DB-CNN (2020) [64]	0.986	0.967	0.988	0.956	0.961
NLNet	0.986	0.961	0.993	0.964	0.951

Noisy
and
Compressed
Images

Global
Distortion

Non-local
Recurrence

Local
Distortion

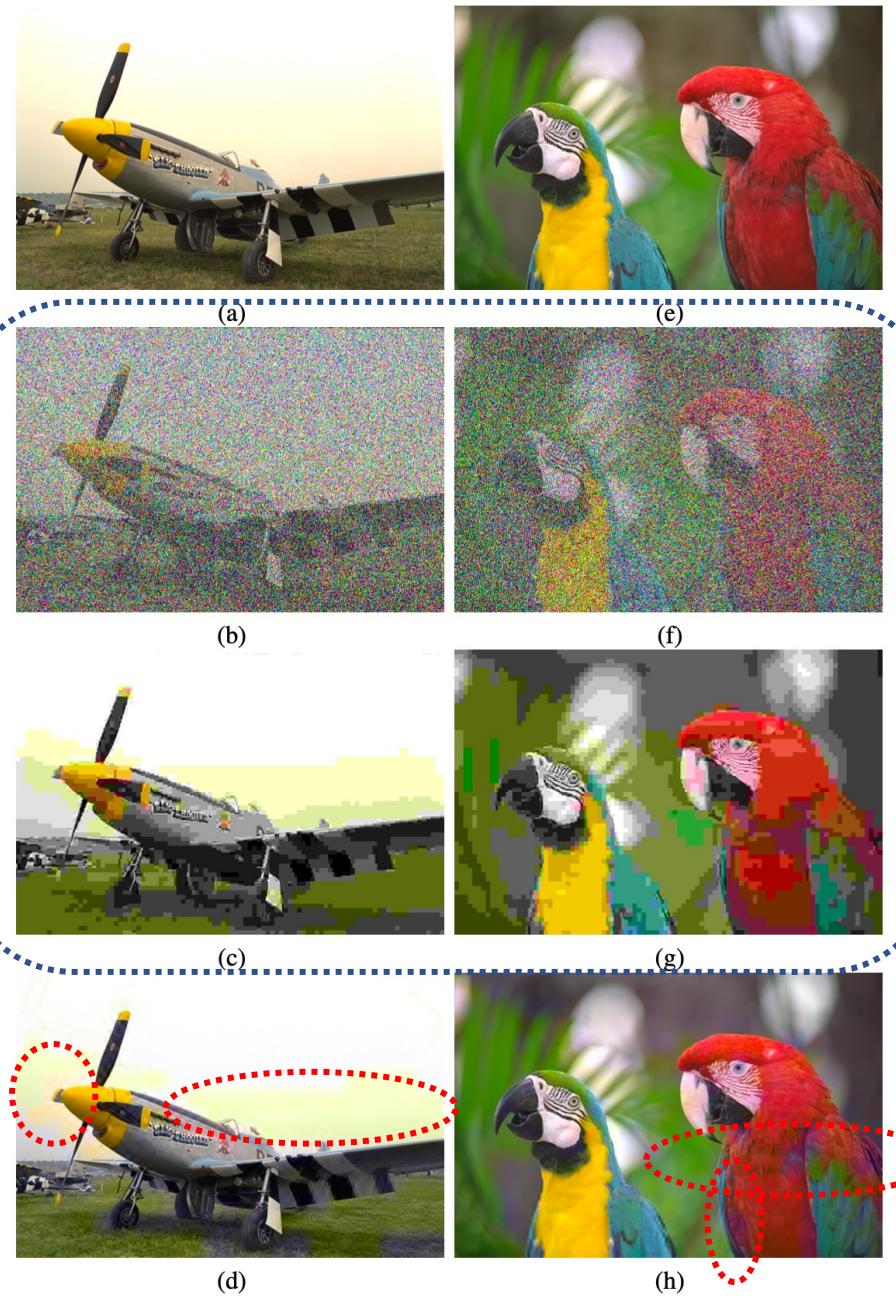


Figure 4.7: Demonstrations of the global distortions (b/f: WN and c/g: JPEG) and local distortions (d/h: FF) contaminating the plane and parrot images. Figure (a) and Figure (e) are reference images from the LIVE database.

Single Distortion Type Evaluation

Noise-Related Distortions

Table 4.5: The average SRCC and PLCC results of the individual distortion type on the CSIQ database. Top two results are highlighted in bold.

SRCC	JPEG	JP2K	WN	GB	PN	CC
BRISQUE (2012) [10]	0.806	0.840	0.723	0.820	0.378	0.804
CORNIA (2012) [104]	0.513	0.831	0.664	0.836	0.493	0.462
M3 (2014) [105]	0.740	0.911	0.741	0.868	0.663	0.770
HOSA (2016) [103]	0.733	0.818	0.604	0.841	0.500	0.716
FRIQUEE (2017) [90]	0.869	0.846	0.748	0.870	0.753	0.838
dipIQ (2017) [82]	0.936	0.944	0.904	0.932	-	-
MEON (2018) [71]	0.948	0.898	0.951	0.918	-	-
WaDIQaM (2018) [35]	0.853	0.947	0.974	0.979	0.882	0.923
DB-CNN (2020) [64]	0.940	0.953	0.948	0.947	0.940	0.870
HyperIQA (2020) [65]	0.934	0.960	0.927	0.915	0.931	0.874
NLNet	0.972	0.963	0.965	0.955	0.969	0.968
PLCC	JPEG	JP2K	WN	GB	PN	CC
BRISQUE (2012) [10]	0.828	0.887	0.742	0.891	0.496	0.835
CORNIA (2012) [104]	0.563	0.883	0.687	0.904	0.632	0.543
M3 (2014) [105]	0.768	0.928	0.728	0.917	0.717	0.787
HOSA (2016) [103]	0.759	0.899	0.656	0.912	0.601	0.744
FRIQUEE (2017) [90]	0.885	0.883	0.778	0.905	0.769	0.864
dipIQ (2017) [82]	0.975	0.959	0.927	0.958	-	-
MEON (2018) [71]	0.979	0.925	0.958	0.946	-	-
DB-CNN (2020) [64]	0.982	0.971	0.956	0.969	0.950	0.895
NLNet	0.991	0.976	0.967	0.9746	0.966	0.969

Global
Distortion



Figure 4.9: Demonstrations of the global distortions (b/f: GB, c/g: CC, d/h: PN) contaminating the Statue of Liberty and George Rogers Clark Memorial images.

Figure (a) and Figure (e) are reference images from the CSIQ database.

Single Distortion Type Evaluation

Table 4.6: The average SRCC results of the individual distortion type on the TID2013 database. Top two results are highlighted in bold.

SRCC	Distortion Type	BRISQUE [10]	FRIQUEE [90]	HOSA [103]	MEON [71]	M3 [105]	DB-CNN [64]	CORNIA [104]	NLNet
Global Distortion	Additive Gaussian noise	0.711	0.730	0.833 ↑ 8.4%	0.813	0.766	0.790	0.692	0.917
	Lossy compression of noisy images	0.609	0.641	0.838	0.772	0.692	0.860 ↑ 7.5%	0.712	0.935
	Additive noise in color components	0.432	0.573	0.551	0.722 ↑ 12.8%	0.740	0.700	0.137	0.850
	Comfort noise	0.196	0.318	0.622	0.406	0.353	0.752 ↑ 11.8%	0.617	0.870
	Contrast change	-0.001	0.585	0.362	0.252	0.155	0.548	0.254	0.793
	Change of color saturation	0.003	0.589	0.045	0.684	-0.199	0.631	0.169	0.827
	Spatially correlated noise	0.746	0.866	0.842	0.926 ↑ 3.2%	0.82	0.826	0.741	0.958
	High frequency noise	0.842	0.847	0.897	0.911 ↑ 1.0%	0.000	0.879	0.815	0.921
	Impulse noise	0.765	0.730	0.809	0.901 ↑ 1.2%	0.738	0.708	0.616	0.913
	Quantization noise	0.662	0.764	0.815	0.888 ↑ 4.1%	0.832	0.825	0.661	0.929
	Gaussian blur	0.871	0.881	0.883	0.887	0.896	0.859	0.850	0.912
	Image denoising	0.612	0.839	0.854	0.797	0.709	0.865 ↑ 1.7%	0.764	0.882
	JPEG compression	0.764	0.813	0.891	0.850	0.844	0.894 ↑ 1.1%	0.797	0.905
	JPEG 2000 compression	0.745	0.831	0.919 ↑ 1.1%	0.891	0.885	0.916	0.846	0.930
	Multiplicative Gaussian noise	0.717	0.704	0.768	0.849 ↑ 5.5%	0.738	0.711	0.593	0.904
	Image color quantization with dither	0.831	0.768	0.896	0.857	0.908	0.833	0.683	0.911
	Sparse sampling and reconstruction	0.807	0.891	0.909	0.855	0.893	0.902	0.865	0.940
	Chromatic aberrations	0.615	0.737	0.753	0.779	0.570	0.732	0.696	0.773
	Masked noise	0.252	0.345	0.468	0.728	0.577	0.646	0.451	0.700
	Mean shift (intensity shift)	0.219	0.254	0.211	0.177	0.119	-0.009	0.232	0.358
Local Distortion	JPEG transmission errors	0.301	0.498	0.730	0.746	0.375	0.772 ↑ 3.3%	0.694	0.805
	JPEG 2000 transmission errors	0.748	0.660	0.710	0.716	0.718	0.773 ↑ 10.2%	0.686	0.875
	Non eccentricity pattern noise	0.269	0.076	0.242	0.116	0.173	0.270 ↑ 34.6%	0.200	0.616
	Local block-wise distortions with different intensity	0.207	0.032	0.268	0.500	0.379	0.444	0.027	0.493

Noise and Compression-Related Distortions

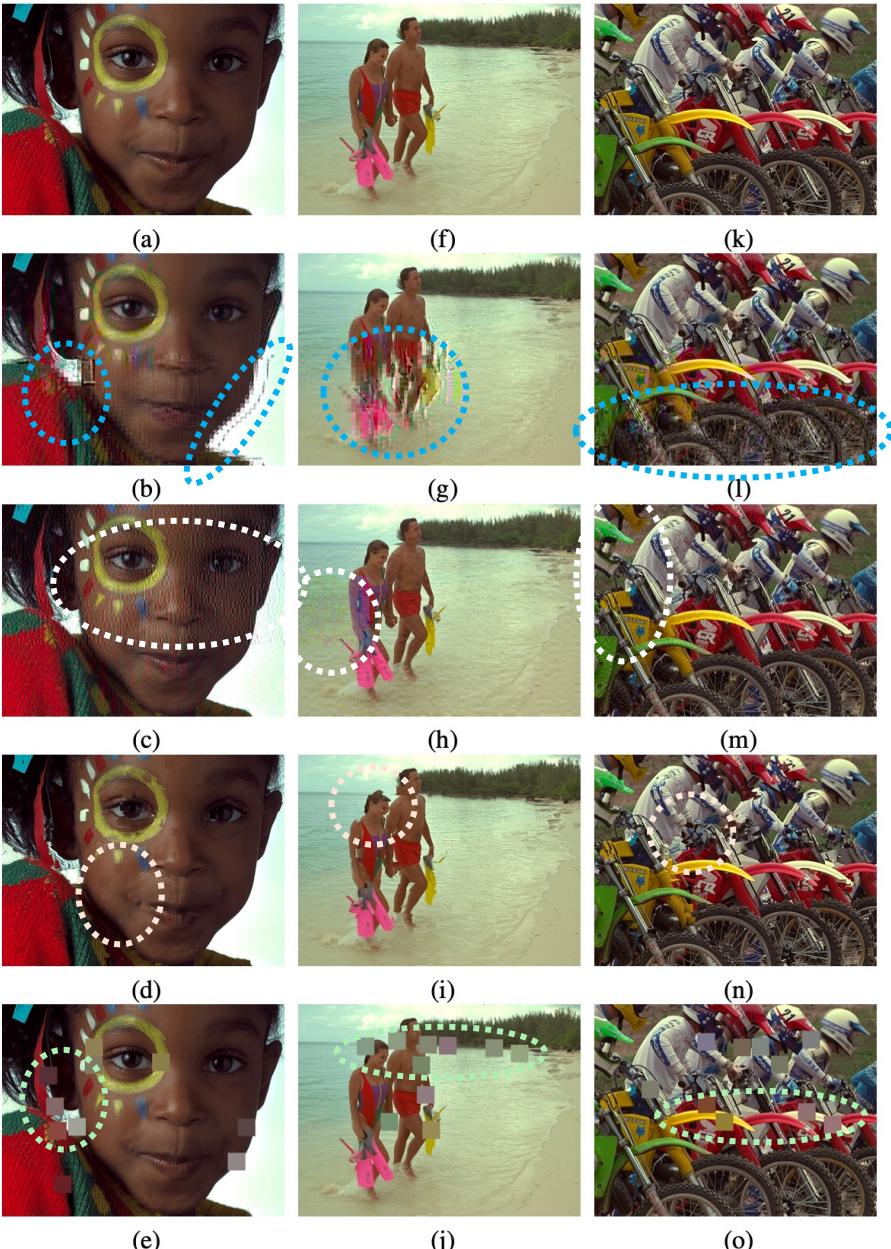


Figure 4.10: Demonstrations of the local distortions (b/g/l: JPEG transmission errors, c/h/m: JPEG2000 transmission errors, d/i/n: non eccentricity pattern noise, e/j/o: local block-wise distortions of different intensities). Figure (a), Figure (f), and Figure (k) are reference images from the TID2013 database.

Single Distortion Type Evaluation

Table 4.7: The average SRCC results of the individual distortion type on the KADID-10k database. The local distortions are highlighted in blue and the top two results are highlighted in bold.

Distortion Type		BLIINDS-II [91]	BRISQUE [10]	ILNIQE [102]	CORNIA [104]	HOSA [103]	WaDIQaM [35]	NLNet
Blurs	Lens blur	0.781	0.674	0.846	0.811	0.715	0.730	0.914
	Gaussian blur	0.880	0.812	0.883	0.866	0.852	0.879	0.914
	Motion blur	0.482	0.423	0.779	0.532	0.652	0.730	0.899
Color distortions	Color diffusion	0.572	0.544	0.678	0.243	0.727	0.833	0.916
	Color saturation 2	0.602	0.375	0.677	0.120	0.841	0.836	0.909
	Color quantization	0.670	0.667	0.676	0.323	0.662	0.806	0.853
	Color shift	-0.139	-0.182	0.090	-0.002	0.050	0.421	0.777
Compression	Color saturation_1	0.091	0.071	0.027	-0.019	0.216	0.148	0.604
	JPEG compression	0.414	0.782	0.804 ↑ 6.2%	0.556	0.582	0.530	0.866
Noise	JPEG 2000 compression	0.655	0.516	0.790 ↑ 6.3%	0.342	0.608	0.539	0.853
	Denoise	0.457	0.221	0.856 ↑ 9.7%	0.229	0.247	0.765	0.953
	White noise in color component	0.757	0.718	0.841	0.418	0.745↑ 1.1%	0.925	0.936
	Multiplicative noise	0.702	0.674	0.682	0.306	0.776↑ 5.0%	0.884	0.934
	Impulse noise	0.547	-0.543	0.808	0.219	0.254↑ 10.2%	0.814	0.916
Brightness change	White Gaussian noise	0.628	0.708	0.776	0.357	0.680↑ 1.7%	0.897	0.914
	Brighten	0.458	0.575	0.301	0.227	0.753	0.685	0.822
	Darken	0.439	0.405	0.436	0.206	0.744	0.272	0.647
Spatial distortions	Mean Shift	0.112	0.144	0.315	0.122	0.591	0.348	0.335
	Jitter	0.629	0.672	0.441	0.719	0.391	0.778	0.899
	Pixelate	0.196	0.648	0.577	0.587	0.702	0.700	0.814
	Quantization	0.781	0.714	0.571	0.259	0.681	0.735	0.791
	Color block	-0.020	0.067	0.003	0.094	0.388	0.160	0.440
Sharpness and contrast	Non-eccentricity patch	0.083	0.191	0.218	0.121	0.461	0.348	0.433
	High sharpen	-0.015	0.361	0.681	0.114	0.230	0.558	0.932
	Contrast change	0.062	0.105	0.072	0.125	0.452	0.421	0.513

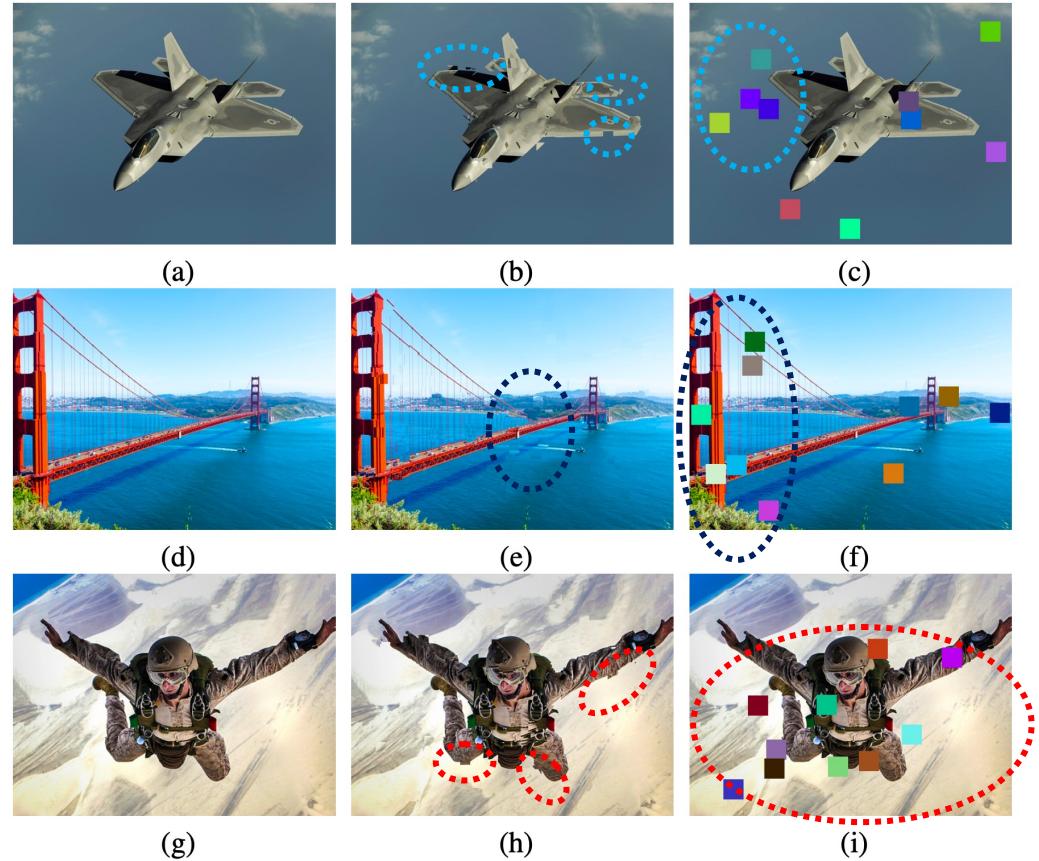


Figure 4.11: Demonstrations of the local distortions (b/e/h: non-eccentricity patch and c/f/i: color block). Figure (a), Figure (d), and Figure (g) are reference images from the KADID-10k database.

Takeaways and Future Work

- ✓ [Non-local & Local Modeling]

- (1) The Non-local Modeling is complementary to traditional local methods.
- (2) CNN's Local Modeling features are effective and robust.

- ✓ [Global & Local Distortions]

- (1) Handle a wide variety of Global Distortions: globally and uniformly distributed with non-local recurrences.
- (2) Maintain sensitivity to Local Distortions: local nonuniform-distributed distortions in a local region.
- (3) Better assess Noisy and Compressed Images quality.

- ✓ [Generalization Capability] Cross-Dataset Setting → High Generalization Capability

- ✓ [Future Work] Non-local Statistics [1, 2]

Credit:

[1] Zontak *et al.*, Internal Statistics of a Single Natural Image, In CVPR 2011

[2] Buades *et al.*, A Non-local Algorithm for Image Denoising, In CVPR 2005



GCNs-Net: A Graph Convolutional Neural Network Approach for Decoding Time-Resolved EEG Motor Imagery Signals

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EEG Deep Learning Library: <https://github.com/SuperBruceJia/EEG-DL>

Background

- ▶ **BCI:** establish connections between the brain and machines
 - (1) Acquire and analyze brain signals while conducting **actual or imagery** tasks
 - (2) Control machines
- ▶ **Significance:** help the disabled and understand the human brain
- ▶ **Types of BCI:**
 - ▶ Electroencephalography (EEG)
 - ▶ Magnetoencephalography (MEG)
 - ▶ Functional Magnetic Resonance Imaging (fMRI)
 - ▶ Invasive BCI Technologies (*e.g.*, Neuralink)
- ▶ **Reasons for using EEG for this project:**
 - ▶ Non-Invasiveness
 - ▶ High Temporal Resolution
 - ▶ Portability
 - ▶ Inexpensive Equipment
- ▶ **Specific Task:** EEG Motor Imagery (*e.g.*, control a wheelchair via imagery-based EEG signals)
- ▶ **Our Research:** develop EEG-based BCI technologies to improve current stroke rehabilitation strategies



Key Points in dealing with EEG time series

► Individual Variability → Lower Classification Accuracy

- Low SNR
- Different brain electrical conductivity ← different anatomical structure of brain
- Electrodes' positional error

Feature Extraction

EEG Electrodes'
Structure Modeling

► Slow Responding → Hard to develop Real-life Applications

- [most literature] Trial-level prediction (e.g., 4 s)
- Window/Slide-level prediction (e.g., 0.4 s)
- Time-resolved prediction (e.g., 6.25 ms) (Our Work)

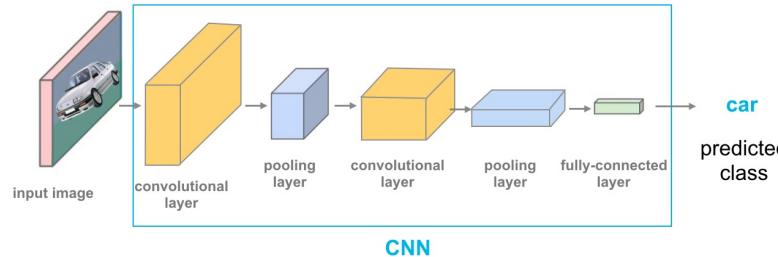
Time-resolved or Window-based
Signal Sampling

► Lower Group-level Accuracy → Hard to develop Applications for a Group of People

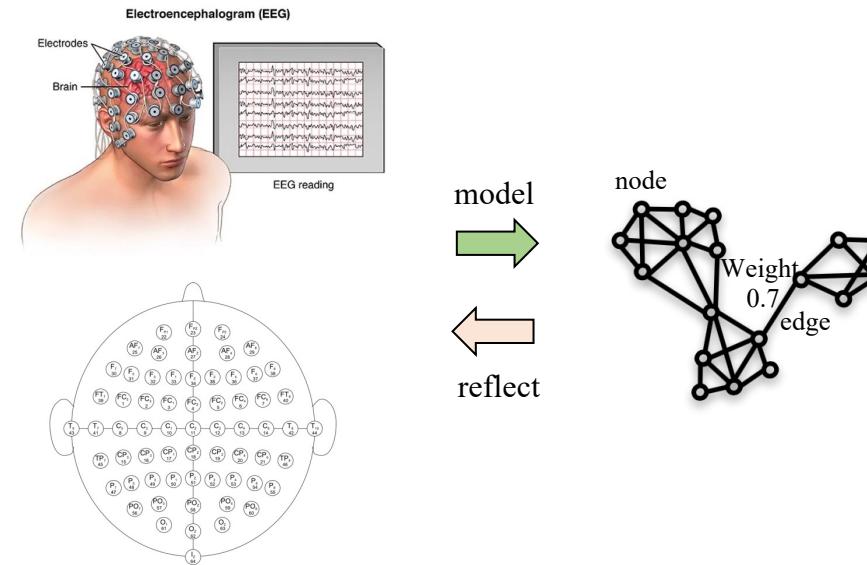
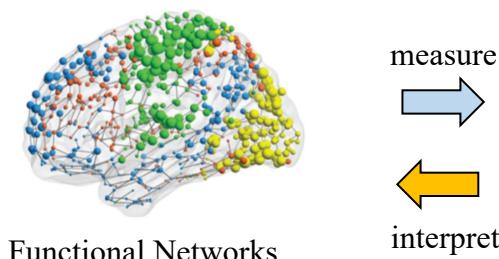
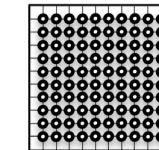
- [most literature] Subject-level prediction (Our Work)
- Group-level prediction (Our Work)

Motivation

Convolutional Neural Networks:



- **Module:** Convolution → Pooling → Fully-connected
- **Modeling:** Euclidean-Structured Data (e.g. Image, Speech, Natural Language)
- Neuroscience research has increasingly emphasized **Brain Network Dynamics**
 - Model **Functional Topological Connectivity** of EEG Electrodes → **Graph** (Non-Euclidean Structure)



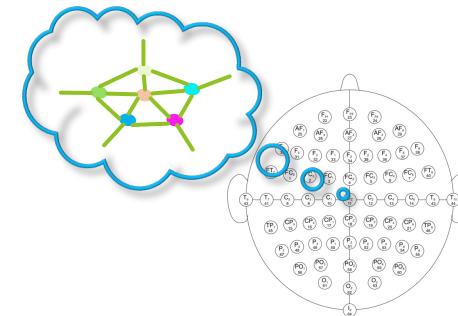
Our Question

How to model the EEG System
as a **Graph**?

How can we process EEG Signals
via **Graph Representation Learning**?

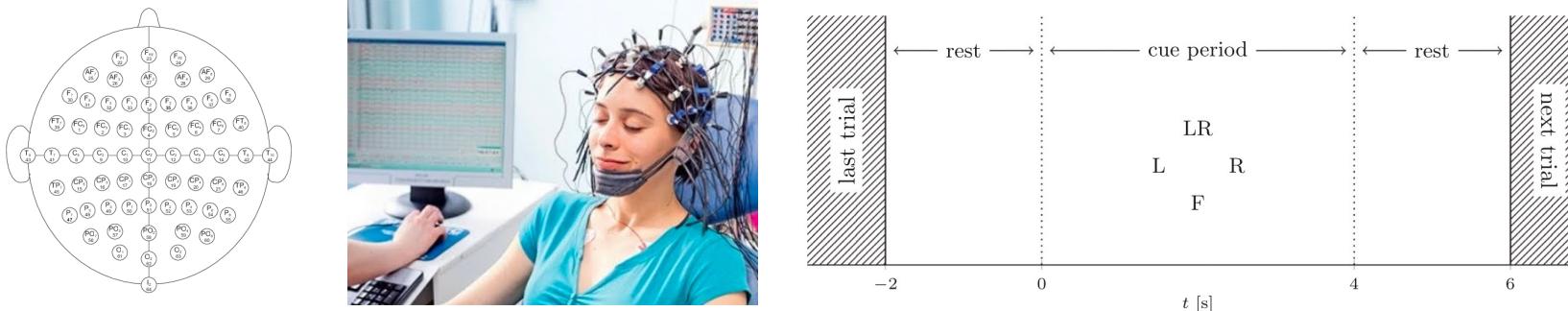
Can we directly apply convolutions on graphs?

- ▶ Traditional CNN **cannot** directly process graph signals
 - ▶ **Graphs are irregular** (*i.e.*, unordered and vary in size)
 - ▶ Convolutions **cannot** keep **Translation Invariance** on non-Euclidean signals
- ▶ **Graph Convolutional Neural Networks** (GCN)
 - ▶ Directly process **non-Euclidean graph-structured signals**
 - ▶ Consider **relationship properties** (*e.g.*, correlations) between nodes
 - Model **Functional Topological Relationships** among EEG electrodes
 - Analyze and interpret **Brain Network Dynamics**



Benchmark Dataset

- ▶ The PhysioNet Dataset (EEG Motor Movement/Imagery Dataset)
- ▶ International 10-10 EEG System, **64 electrodes**
(excluding electrodes Nz, F9, F10, FT9, FT10, A1, A2, TP9, TP10, P9, and P10)

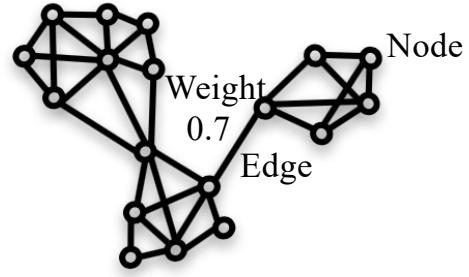


- ▶ **109 subjects** (the largest number of participants in the field of EEG Motor Imagery)
- ▶ Task: **4-class EEG Motor Imagery Classification**
 - ✓ Imagining (Task 1) left fist, (Task 2) right fist, (Task 3) both fists, (Task 4) both feet
- ▶ For each subject, **3 runs, 7 trials, 4 classes** → 84 trials in total
- ▶ For each trial, **4 seconds** experimental duration, **160 Hz** Sampling Rate → **640 Time Points**
- ▶ We apply **Time-resolved Sampling Method**:
 - ✓ Total samples per subject: $3 \text{ runs} \times 7 \text{ trials} \times 4 \text{ classes} \times 4 \text{ seconds} \times 160 \text{ Hz} = 53,760 \text{ samples}$
 - ✓ Experimental Settings: 90% as the training set and the left 10% as the test set

Preliminary: Graph Representation

Definition: An Undirected and Weighted Graph with N nodes: $\mathbf{G} = \{\mathbf{V}, \mathbf{E}, \mathbf{A}\}$

- \mathbf{V} : nodes (vertices), $|\mathbf{V}| = N$
- \mathbf{E} : edges (links) that connect nodes
- \mathbf{A} : weights (correlations) between nodes



Nodes Correlations: Pearson Matrix $\mathbf{P} \in \mathbb{R}^{N \times N}$ (denotes as PCC matrix)

- Measure the linear correlations between node \mathbf{x} and node \mathbf{y}
- μ is the mean, σ is the standard deviation, and $P_{x,y}$ is the Pearson Correlation Coefficient between node \mathbf{x} and node \mathbf{y}

$$P_{x,y} = \frac{E((\mathbf{x} - \mu_x)(\mathbf{y} - \mu_y))}{\sigma_x \sigma_y}$$

- Absolute Pearson Matrix: $|\mathbf{P}| \in \mathbb{R}^{N \times N}$ and $|P_{ij}| \in [0, 1]$ → **Note:** In this work, we only consider scale.

Graph Weights: Adjacency Matrix $\mathbf{A} = |\mathbf{P}| - \mathbf{I} \in \mathbb{R}^{N \times N}$, where \mathbf{I} is an Identity Matrix

Graph Degrees: Degree Matrix $\mathbf{D} \in \mathbb{R}^{N \times N}$

$$D_{ii} = \sum_{j=1}^N A_{ij}$$

Graph Representation: Combinatorial Laplacian $\mathbf{L} \in \mathbb{R}^{N \times N}$

$$\mathbf{L} = \mathbf{D} - \mathbf{A}$$

Normalized:

$$\mathbf{L} = \mathbf{I} - \mathbf{D}^{-\frac{1}{2}} \mathbf{A} \mathbf{D}^{\frac{1}{2}}$$

Preliminary:

Spectral Theorem for Graph Laplacian \mathbf{L}

$$\mathbf{L} = \mathbf{U}\Lambda\mathbf{U}^T$$

$$\mathbf{L}\mathbf{U} = \Lambda\mathbf{U}$$

- \mathbf{U} : Fourier basis → **real** and **orthonormal** eigenvectors of \mathbf{L}
- Λ : Fourier modes → the diagonal is the **ordered** and **real nonnegative** eigenvalues of \mathbf{L}

Graph Fourier Transform of Signal f

can be seen as the $e^{-j\omega t}$
in Fourier Transforms

$$F[f(\lambda)] = \hat{f}(\lambda) = \sum_{i=1}^n f(i) \times U(i)$$

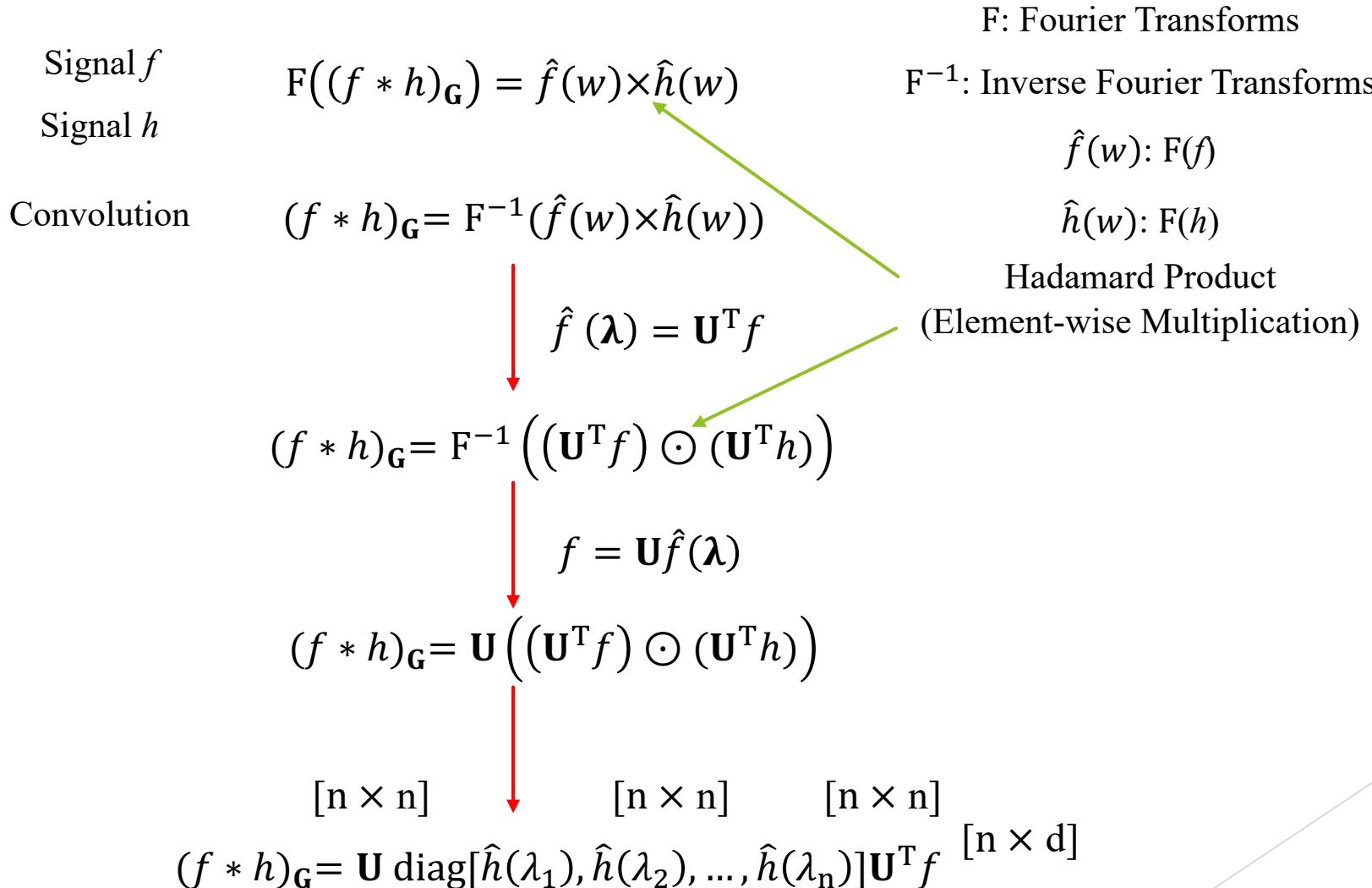
$$\hat{f}(\lambda) = \mathbf{U}^T f \Leftrightarrow f = \mathbf{U}\hat{f}(\lambda)$$

$\hat{f}(\lambda)$ is the projection value of Fourier basis \mathbf{U}

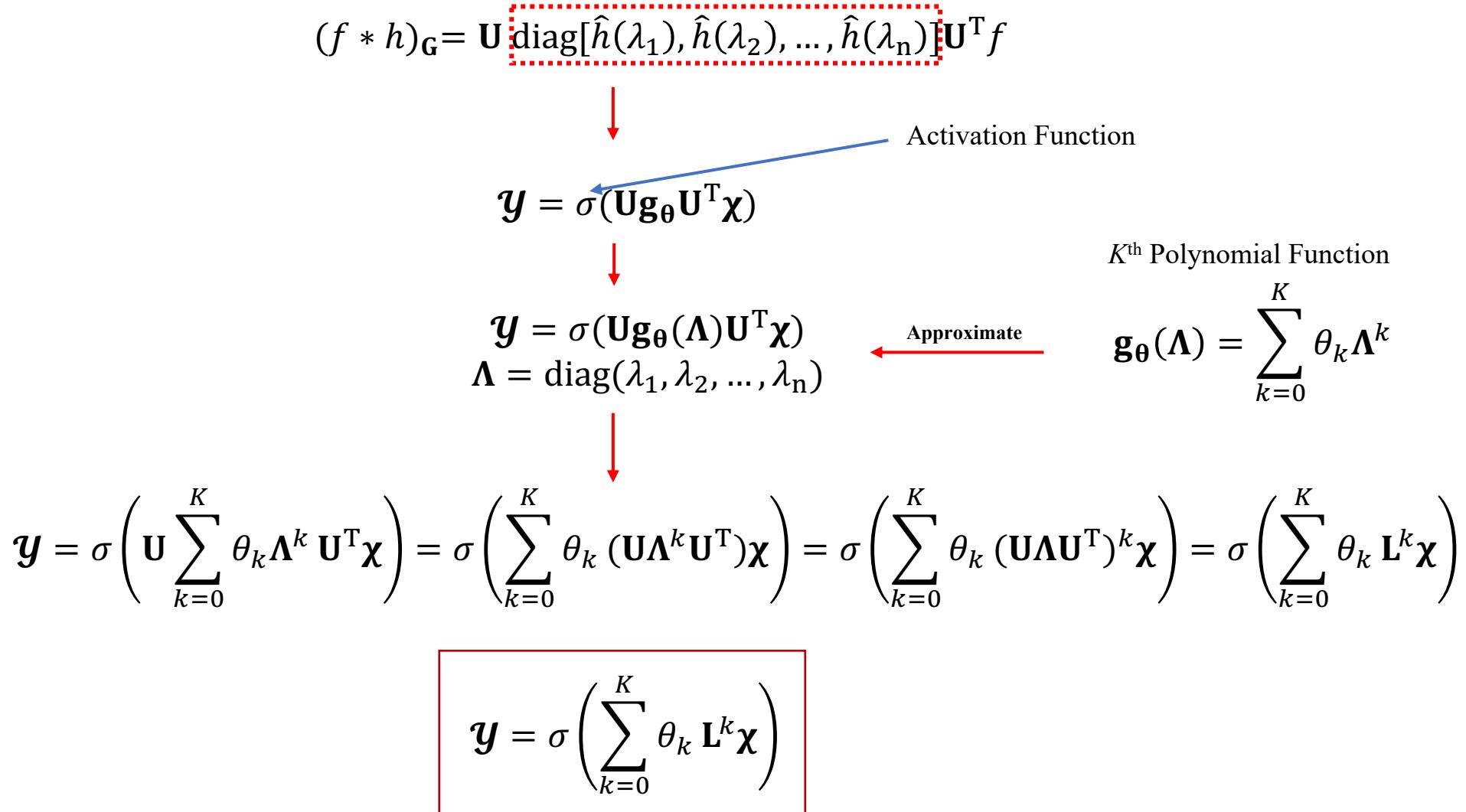
Preliminary: Graph Convolution via Graph Fourier Transform

Convolution in the spatial domain \Leftrightarrow

Inverse Fourier Transforms of *point-wise multiplication of two transformed signals* in the frequency domain



Graph Convolution



Graph Convolution

Node Aggregation
 K is Filter Size

$$y = \sigma \left(\sum_{k=0}^K \theta_k \mathbf{L}^k \mathbf{x} \right)$$

Convolution:
Weighted Sum

Weight Sharing

No need for Fourier Transform

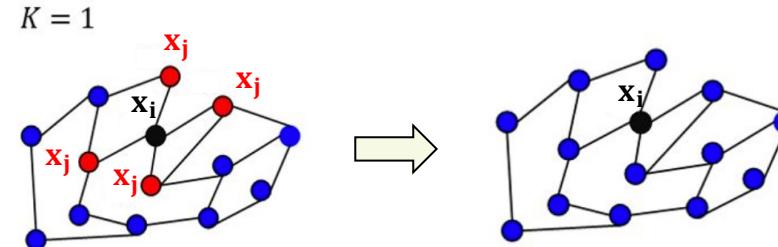
Beauty is in Simplicity

GCN Key Idea: Use "edge information" to aggregate "node information" to generate a new "node representation"

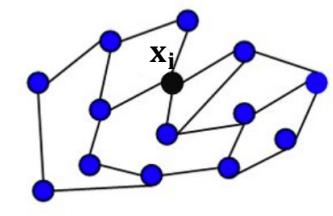
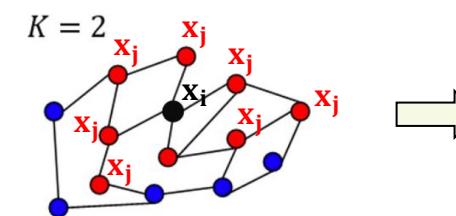
Laplace Operator

Local connectivity

$$\mathbf{x}_{\text{new}} \leftarrow \mathbf{L} \mathbf{x}_i = \sum_j A_{ij} (\mathbf{x}_i - \mathbf{x}_j)$$



Localize in Space



Pros:

1. No need for Spectral Decomposition of \mathbf{L}
2. Less number of parameters (decrease model complexity) $\rightarrow K \ll N$

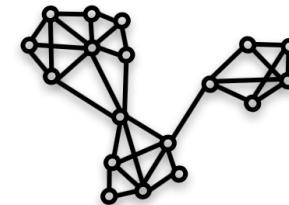
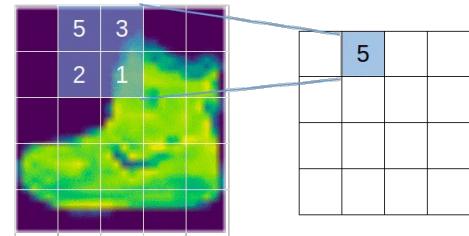
Cons: Need to compute \mathbf{L}^k

Pooling on Graphs (Graph Coarsening)

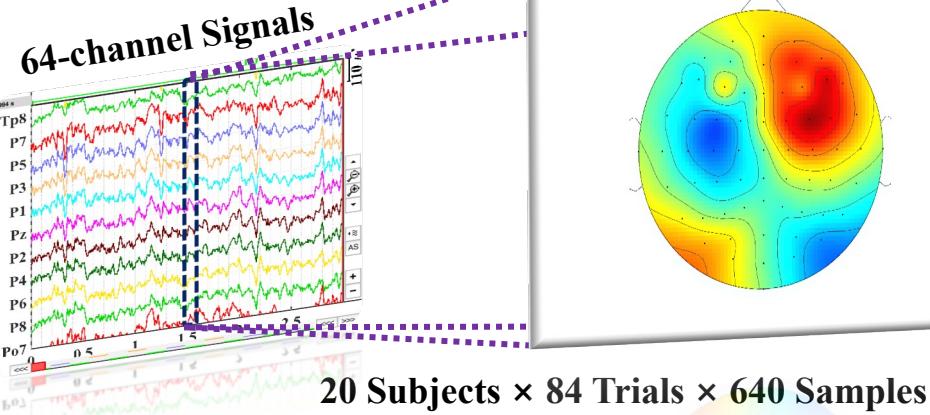
- Traditional CNN doesn't need to consider **neighbors** after convolutions
 - [Euclidean Structure] The output Feature Maps are “**regular**”
 - The neighbor is “**meaningful**”
- GCNs need to consider neighbors after convolutions
 - [Non-Euclidean Structure] The output **graphs' nodes are not arranged in any meaningful way**
 - Use **Graclus Multilevel Clustering Algorithm** to find “meaningful” neighbors
 - Minimize the **Local Normalized Cut** (a cluster grouping method)

$$-W_{ij}\left(\frac{1}{d_i} + \frac{1}{d_j}\right)$$

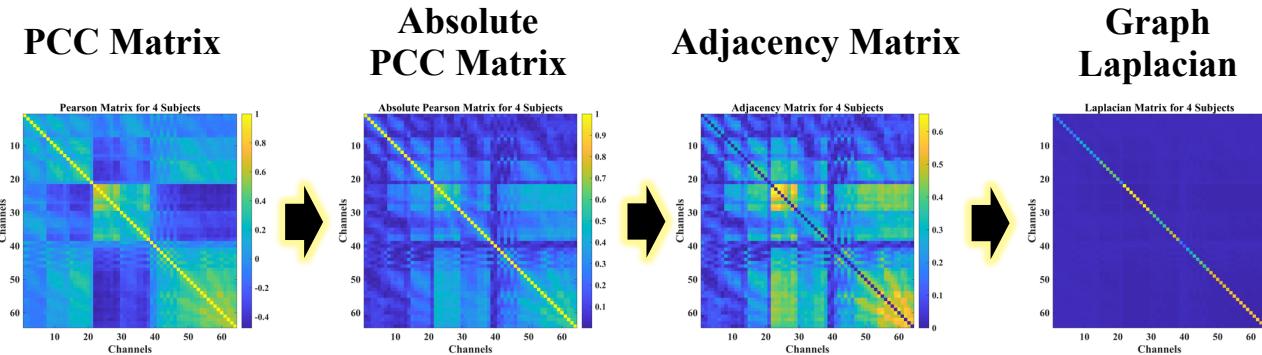
- i and j denote node i and node j
- W_{ij} is the **learned weight** between node i and node j



(i) EEG Data Acquisition

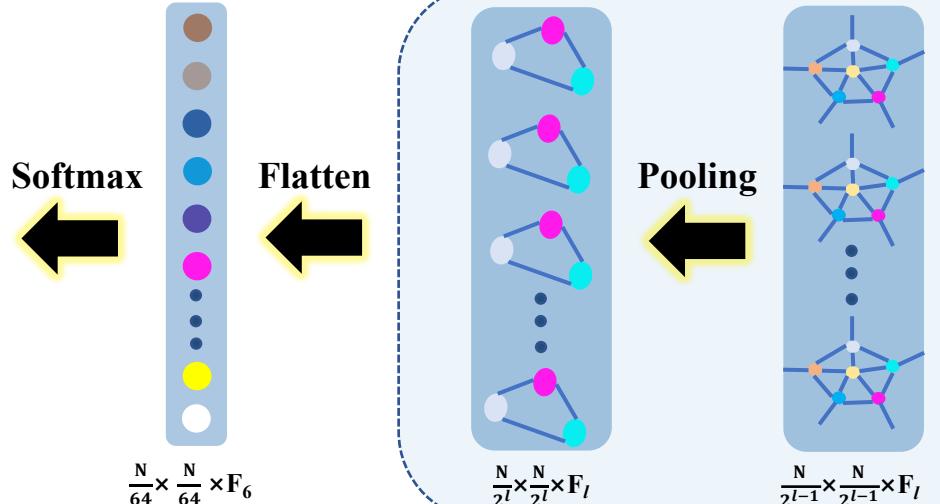


(ii) Correlations between EEG Electrodes

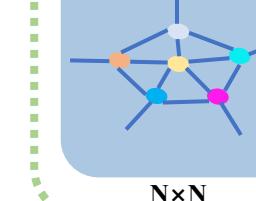
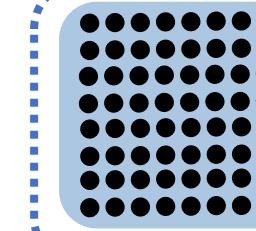


Real-time 64-channel Raw EEG Signals

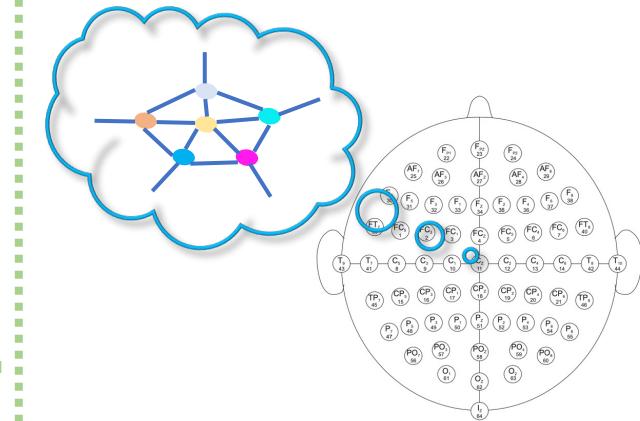
(iv) The GCNs-Net



GCN



(iii) Graph Representation



Correlation among EEG electrodes

Two Subjects: Subject 10 and 5

Problem: Individual Variability

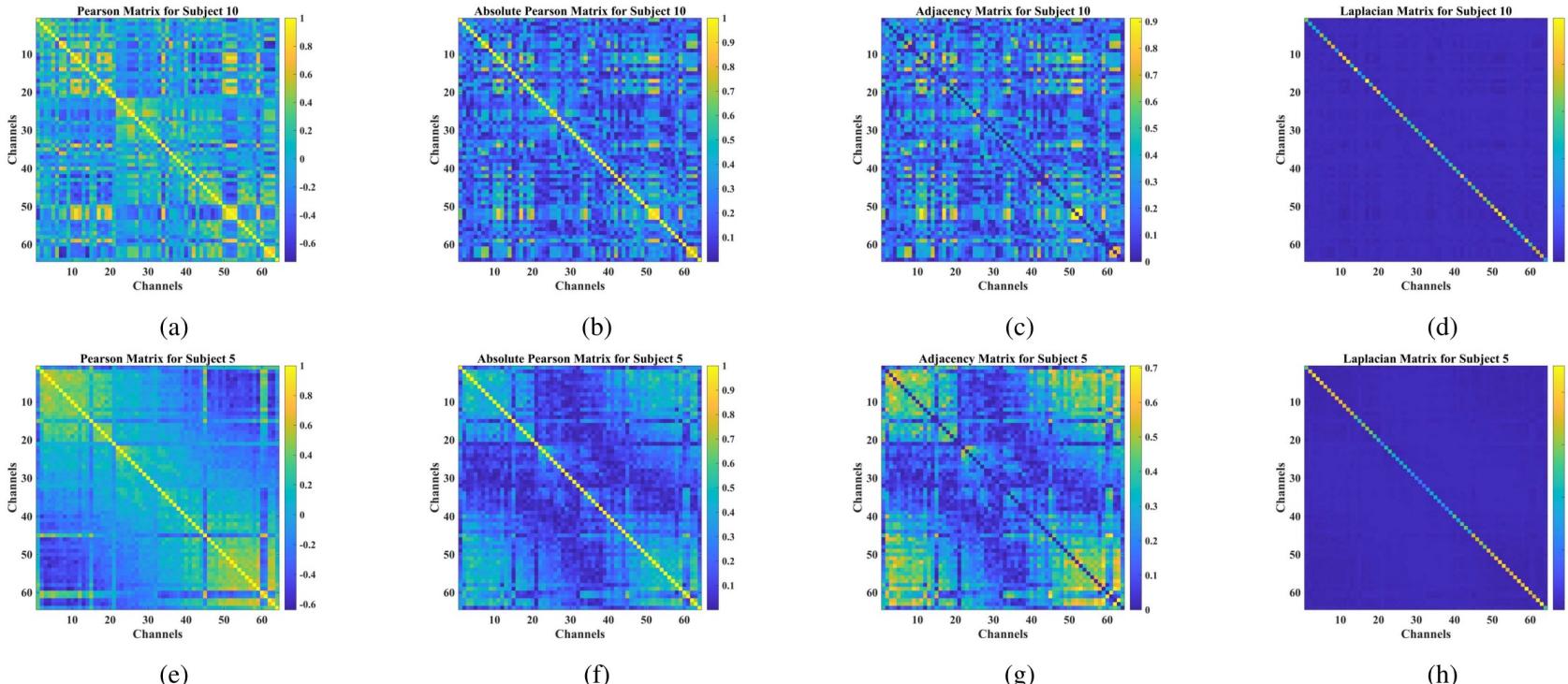


Fig. 6. PCC matrix, absolute PCC matrix, adjacency matrix, and graph Laplacian for Subjects 10 and 5 from the PhysioNet dataset. (a) PCC matrix for Subject 10. (b) Absolute PCC matrix for Subject 10. (c) Adjacency matrix for Subject 10. (d) Graph Laplacian for Subject 10. (e) PCC matrix for Subject 5. (f) Absolute PCC matrix for Subject 5. (g) Adjacency matrix for Subject 5. (h) Graph Laplacian for Subject 5.

Correlation among EEG electrodes

20 Subjects and 100 Subjects

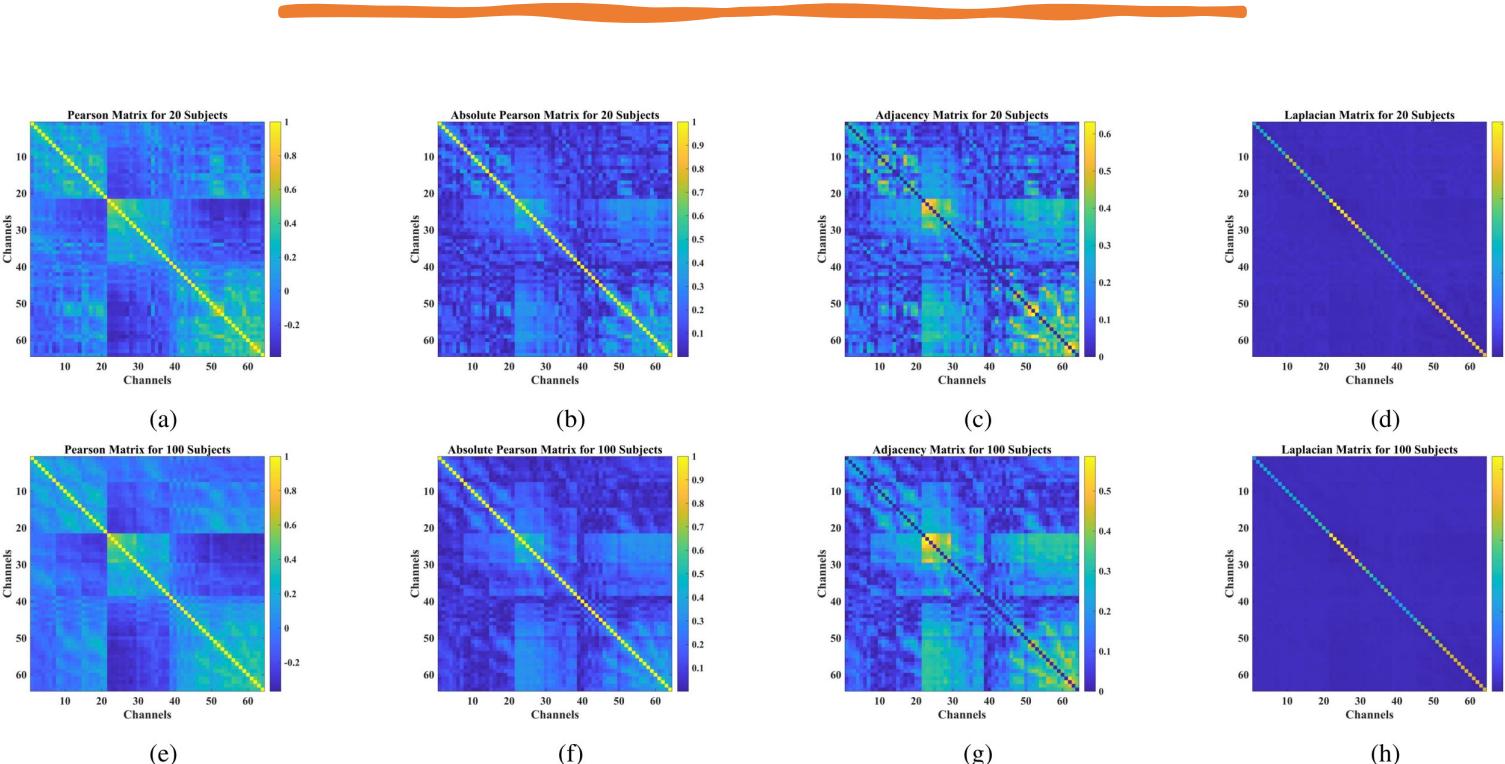


Fig. 2. PCC matrix, absolute PCC matrix, adjacency matrix, and graph Laplacian for 20 and 100 subjects, respectively, from the PhysioNet dataset. (a) PCC matrix for 20 subjects. (b) Absolute PCC matrix for 20 subjects. (c) Adjacency matrix for 20 subjects. (d) Graph Laplacian for 20 subjects. (e) PCC matrix for 100 subjects. (f) Absolute PCC matrix for 100 subjects. (g) Adjacency matrix for 100 subjects. (h) Graph Laplacian for 100 subjects.

Increasing *the number of subjects* alleviates *individual variability*

Model Design for 64-electrode EEG System

TABLE I
IMPLEMENTATION DETAILS OF THE PROPOSED GCNs-NET ON THE PHYSIONET DATASET

Layer	Type	Maps	Size	Edges	Polynomial Order	Pooling Size	Activation	Weights	Bias
Softmax	Fully-connected	—	O	—	—	—	Softmax	$\frac{N}{64} \times \frac{N}{64} \times F_6 \times O$	O
Flatten	Flatten	—	$\frac{N}{64} \times \frac{N}{64} \times F_6$	—	—	—	—	—	—
P6	Max-pooling	F_6	$\frac{N}{32}$	$\sum_{i=1}^{\frac{N}{32}-1} i$	—	2	—	—	—
C6	Convolution	F_6	$\frac{N}{32}$	$\sum_{i=1}^{\frac{N}{32}-1} i$	K	—	Softplus	$F_5 \times F_6 \times K$	$\frac{N}{32} \times F_6$
P5	Max-pooling	F_5	$\frac{N}{16}$	$\sum_{i=1}^{\frac{N}{16}-1} i$	—	2	—	—	—
C5	Convolution	F_5	$\frac{N}{16}$	$\sum_{i=1}^{\frac{N}{16}-1} i$	K	—	Softplus	$F_4 \times F_5 \times K$	$\frac{N}{16} \times F_5$
P4	Max-pooling	F_4	$\frac{N}{8}$	$\sum_{i=1}^{\frac{N}{8}-1} i$	—	2	—	—	—
C4	Convolution	F_4	$\frac{N}{8}$	$\sum_{i=1}^{\frac{N}{8}-1} i$	K	—	Softplus	$F_3 \times F_4 \times K$	$\frac{N}{8} \times F_4$
P3	Max-pooling	F_3	$\frac{N}{4}$	$\sum_{i=1}^{\frac{N}{4}-1} i$	—	2	—	—	—
C3	Convolution	F_3	$\frac{N}{4}$	$\sum_{i=1}^{\frac{N}{4}-1} i$	K	—	Softplus	$F_2 \times F_3 \times K$	$\frac{N}{4} \times F_3$
P2	Max-pooling	F_2	$\frac{N}{2}$	$\sum_{i=1}^{\frac{N}{2}-1} i$	—	2	—	—	—
C2	Convolution	F_2	$\frac{N}{2}$	$\sum_{i=1}^{\frac{N}{2}-1} i$	K	—	Softplus	$F_1 \times F_2 \times K$	$\frac{N}{2} \times F_2$
P1	Max-pooling	F_1	N	$\sum_{i=1}^{N-1} i$	—	2	—	—	—
C1	Convolution	F_1	N	$\sum_{i=1}^{N-1} i$	K	—	Softplus	$1 \times F_1 \times K$	$N \times F_1$
Input	Input	1	N	$\sum_{i=1}^{N-1} i$	—	—	—	—	—

Model Optimization

- **Ablation Study:** Optimal Model Structure (64-electrode EEG System)
 - C6-P6-K2 with [16, 32, 64, 128, 256, 512] filters
- **Gradient Iterative Solver:** Adam Optimizer with Stochastic Gradient Descent (SGD) algorithm
 - Learning Rate: 0.01
 - Batch Size: 1,024
- **Activation Function:** Softplus (Smooth Rectified Linear Unit)

$$F(x) = \log(1 + e^x)$$

- **Model Output:** Softmax: y are labels, \hat{y} are the final output tasks

$$\hat{y}_i = \operatorname{argmax} \left(\frac{e^{y_i}}{\sum_{i=1}^4 e^{y_i}} \right)$$

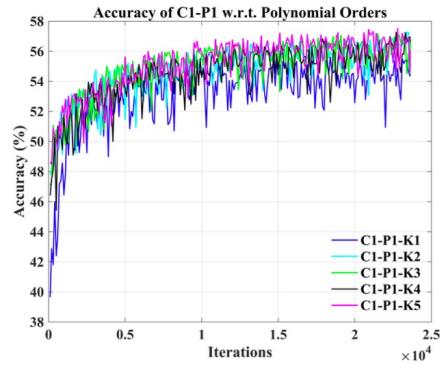
- **Loss Function:** Cross-entropy Loss with L2 regularization

$$\text{Loss} = - \sum_{i=1}^4 y_i \log(\hat{y}_i) + \lambda \left(\sum_{j=1}^n w_j^2 + b_j^2 \right)$$

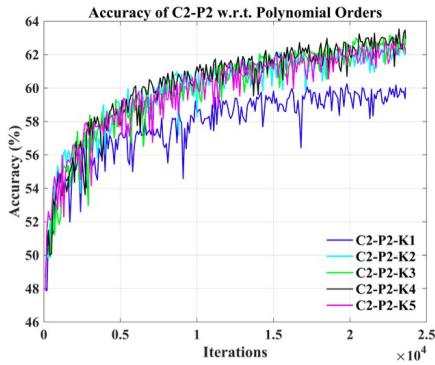
$\lambda = 1 \times 10^{-6}$ is the coefficient of the L2 regularization.

Ablation Study

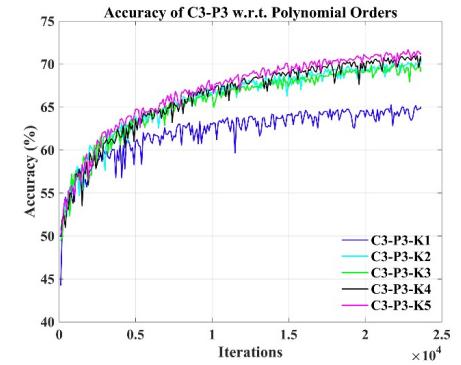
K1
Poor Performance



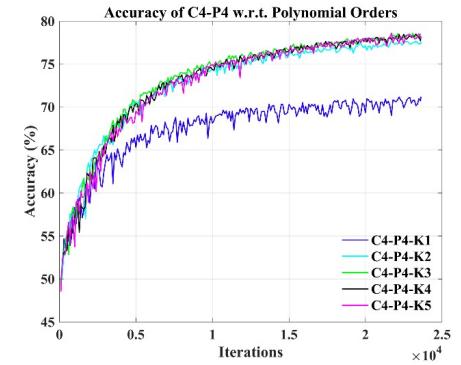
(a)



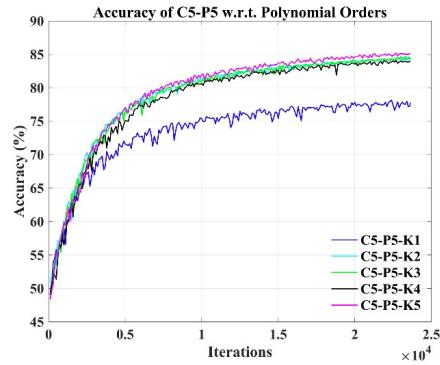
(b)



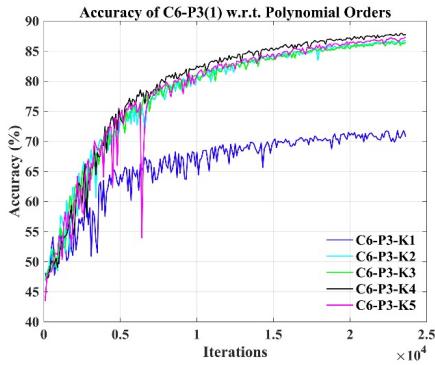
(c)



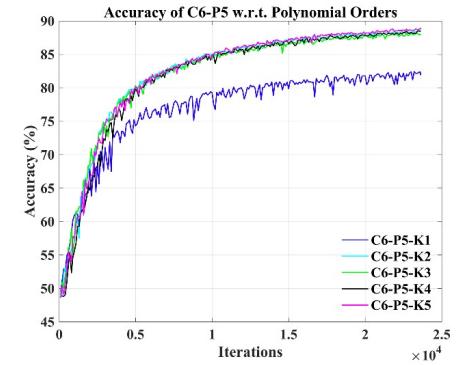
(d)



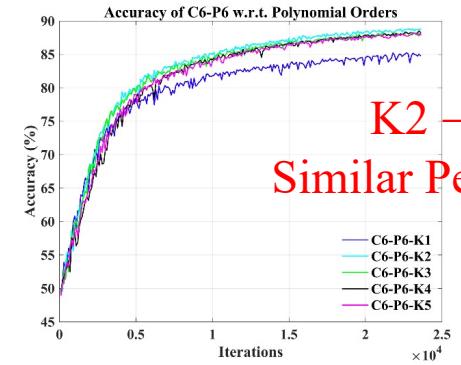
(e)



(f)



(g)



(h)

K2 → K5
Similar Performance

Fig. 3. Accuracy of some selected models regarding different polynomial approximation order. The models are selected from Table II. (a) Accuracy of the model C1-P1 (model 1). (b) Accuracy of the model C2-P2 (model 3). (c) Accuracy of the model C3-P3 (model 6). (d) Accuracy of the model C4-P4 (model 10). (e) Accuracy of the model C5-P5 (model 14). (f) Accuracy of the model C6-P3 (model 16). (g) Accuracy of the model C6-P5 (model 19). (h) Accuracy of the model C6-P6 (model 20).

Experimental Results

Groupwise Prediction and Subject-specific Adaptation

TABLE IV
PERFORMANCE COMPARISONS ON THE PHYSIONET DATASET

Related Work	Max. Accuracy	Avg. Accuracy	<i>p</i> -value	Level	Approach	Num. of Subjects
Dose <i>et al.</i> (2018) [22]	— 80.38%	58.58% 68.51%	— < 0.05	Group Subject	CNNs	105 1
Ma <i>et al.</i> (2018) [60]	82.65%	68.20%	—	Group	RNNs	12
Hou <i>et al.</i> (2020) [20]	94.50% 96.00%	— —	— > 0.05	Group Subject	ESI-CNNs	10 1
Hou <i>et al.</i> (2022) [34]	94.64% 98.81%	— 95.48%	— > 0.05	Group Subject	BiLSTM-GCN	20 1
Jia <i>et al.</i> (2022) [40]	94.16% 98.08%	93.78% 94.18%	— > 0.05	Group Subject	Graph ResNet	20 1
Author	89.39% 88.14% 98.72%	88.57% — 93.06%	— — —	Group Group Subject	GCNs-Net	20 100 1

Note: ***p*-value < 0.05** → Statistically Significant Difference

Takeaways and Future Work

- ✓ [Graph Representation]

Graph Representation Learning to deeply extract **Network Patterns of Brain Dynamics** for EEG classification.

- ✓ [Model Converge]

Converge for both Personalized and Groupwise Predictions, indicating that the GCNs-Net is able to build a generalized representation of EEG time-series **against both Personalized and Groupwise Variations**.

- ✓ [Future Work]

Modeling EEG signals as **Dynamic Graphs** and processing them via **Dynamic Graph Representation Learning**.

Deep Feature Mining via Attention-based BiLSTM-GCN

for Human Motor Imagery Recognition

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¹ School of Automation Engineering, Northeast Electric Power University

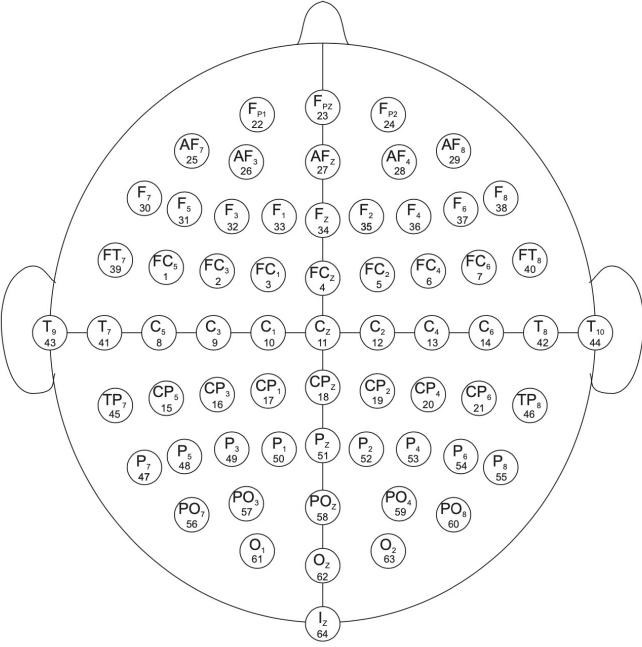
² Department of Computer Science, City University of Hong Kong

³ School of Computer Science, Northwestern Polytechnical University

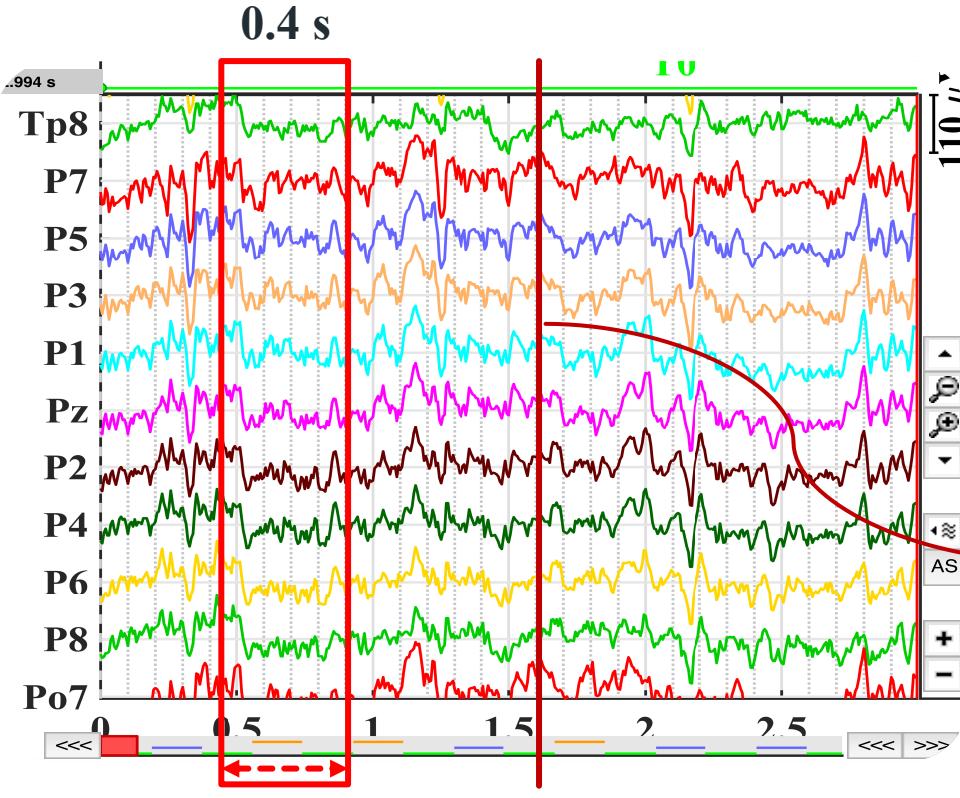
⁴ School of Biomedical Engineering and Brain and Mind Center, The University of Sydney

EEG Deep Learning Library: <https://github.com/SuperBruceJia/EEG-DL>

One Problem of the GCNs-Net



Spatial information



Temporal information

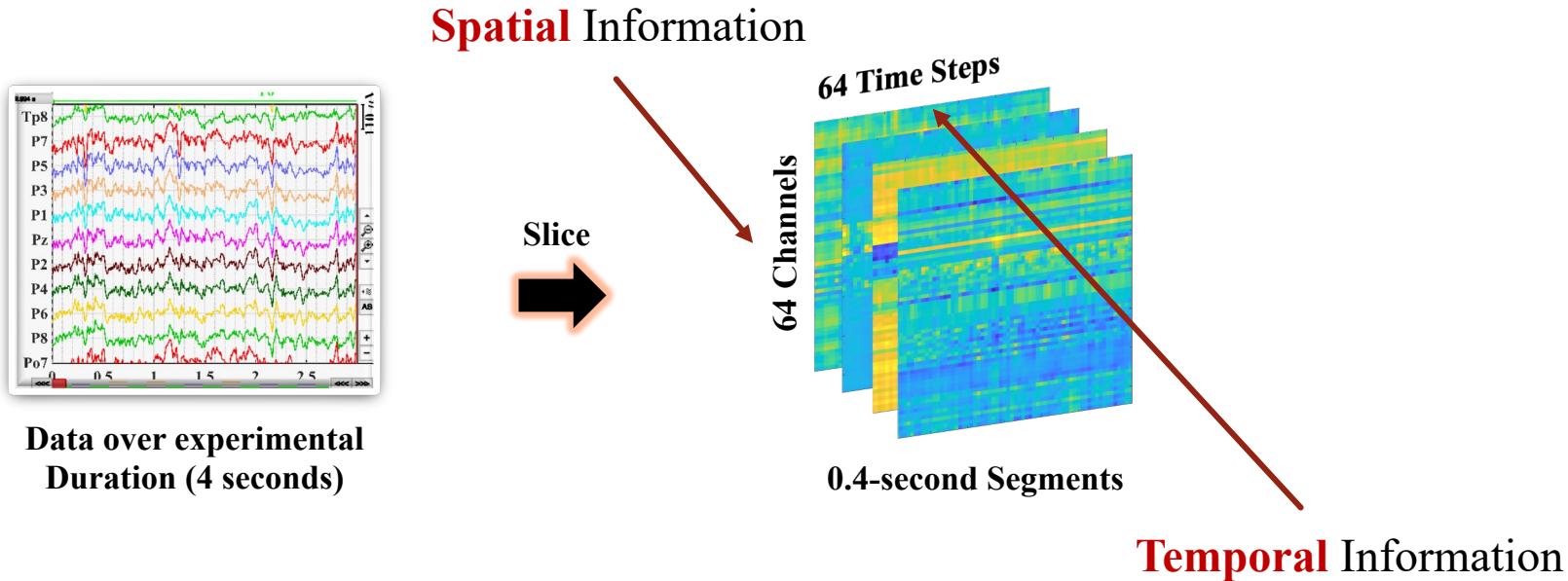
Time-resolved
Signal

- ✓ GCNs-Net is based on **Time-Resolved Signal** → doesn't consider **Temporal Information**

Motivation:

- ✓ [Spatial-Temporal Analysis] Consider **Temporal** and **Spatial Information** from EEG signals
- ✓ [Responsive] Maintain **High Responding Time**

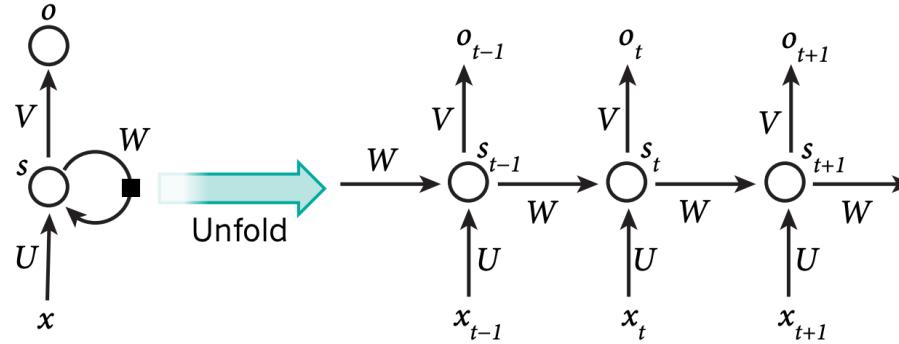
64-channel Raw EEG Signals Acquisition



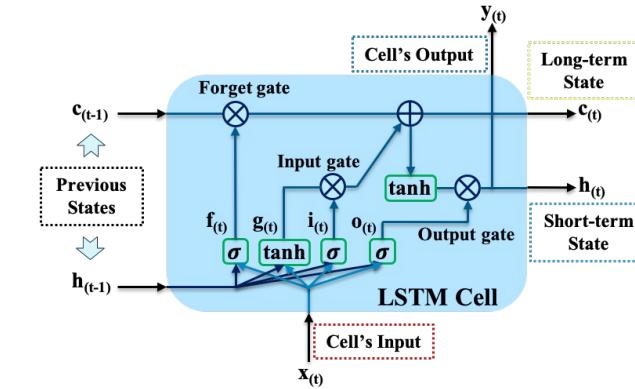
- ✓ 4-s Signals (experimental duration): **0.4-s segments** over time
- ✓ Each Segment: **64 channels \times 64 time steps**
- ✓ Pre-processed Data: **Temporal** Information + **Spatial** Information

Temporal Information Extraction

unrolling the network through time



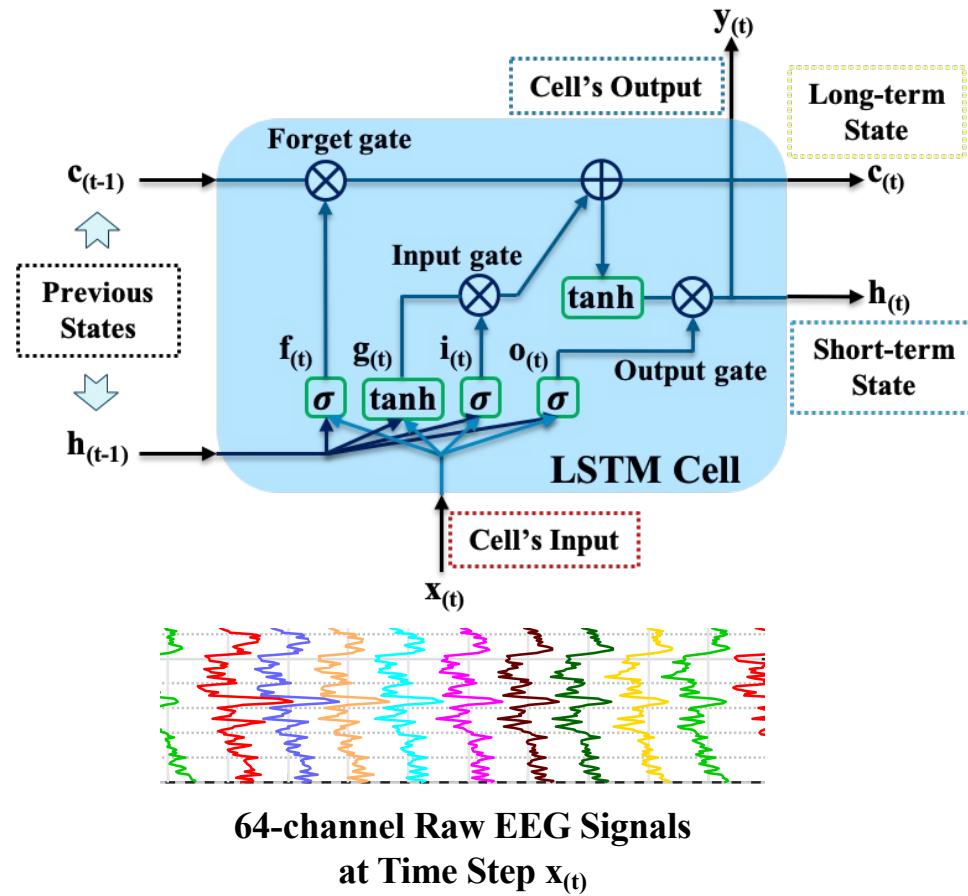
Recurrent Neural Network (RNN)



Long Short-Term Memory (LSTM)

- ✓ Designed for **order-mattered sequential data**, e.g., time series
- ✓ The learned features at *time step t* are affected by \mathbf{x}_t and \mathbf{x}_{t-1} → **continuly learn** from time series
- ✓ **LSTM**: better capture **long-range sequence dependencies**
- ✓ Gated Recurrent Units (**GRU**): **lightweight** architecture with comparable performance

Long Short-term Memory (LSTM)



- ✓ Capture **Long-range Dependencies**
by the long-term state path $c_{t-1} \rightarrow c_t$
- ✓ **Input Gate**: store x_t and control c_t 's input
- ✓ **Forget Gate**: control c_{t-1}
- ✓ **Output Gate**: control c_t 's output
→ short-term state h_t (**Cell's Output**)
- ✓ More parameters to store information
- ✓ Bidirectional:
 - (1) $x_1 \rightarrow x_t$
 - (2) $x_t \rightarrow x_1$



Attention Mechanism

✓ Signals or Outputs

Equally treated/contributed

vs.

Differently treated/contributed with preference/importance

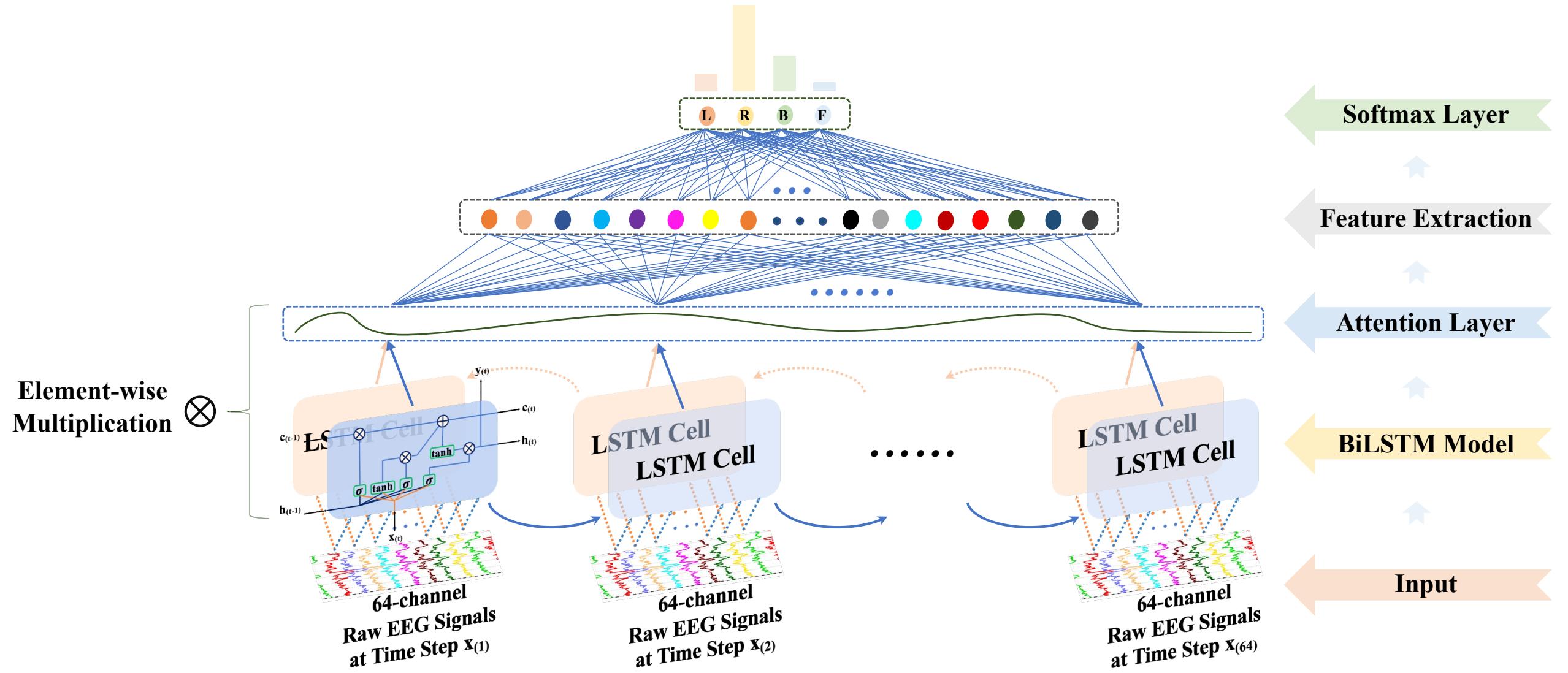
FC Layer $\mathbf{U}_t = \tanh(\mathbf{W}_w \mathbf{y}_t + \mathbf{b}_w)$

Attentional
Weights
$$\alpha_t = \frac{\exp(\mathbf{U}_t^T \mathbf{W}_U)}{\sum_t \exp(\mathbf{U}_t^T \mathbf{W}_U)}$$

Weighted
Sum

$$\hat{\mathbf{U}}_t = \sum_t \alpha_t \mathbf{y}_t$$

Attention-based Bidirectional Long Short-term Memory (Bi-LSTM)



Model Design Ablation Study

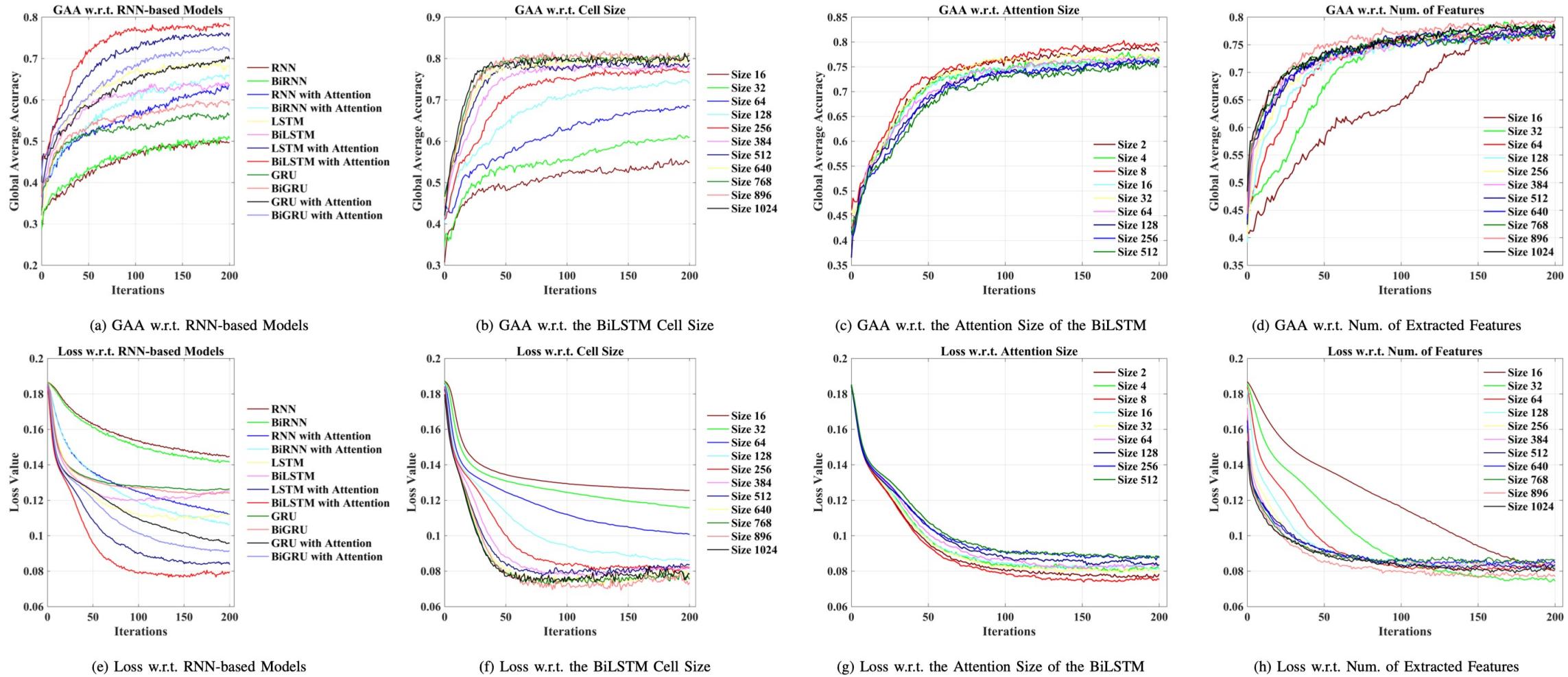
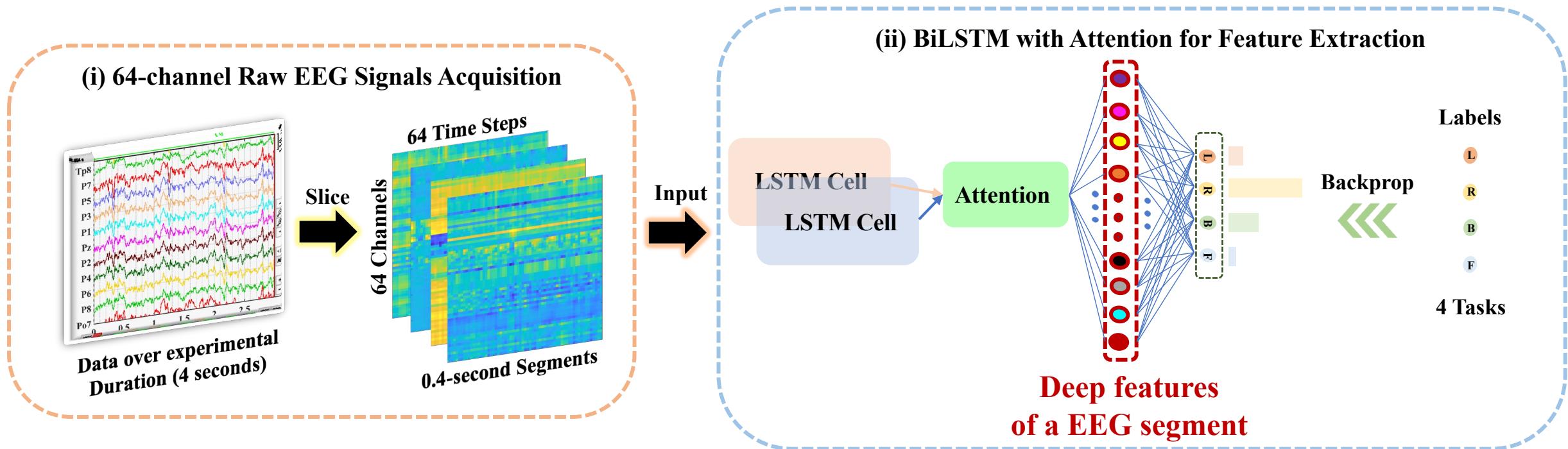


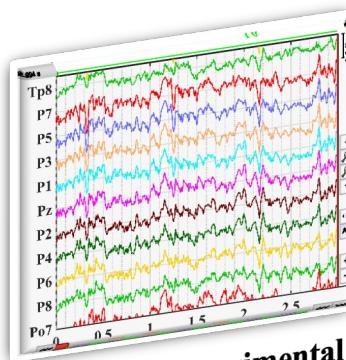
Fig. 3: Models and Hyperparameters Comparison w.r.t. the RNN-based Methods for Feature Extraction

Topological Structure of Features

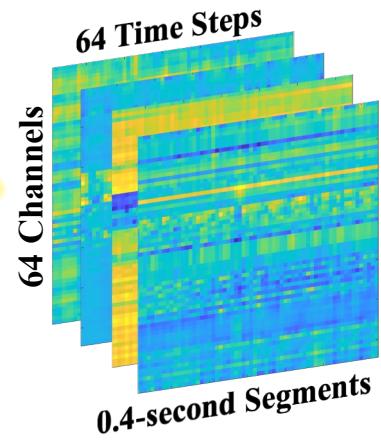


✓ Deep Feature Mining → Intra-feature Relationship → Intra-feature Modeling

(i) 64-channel Raw EEG Signals Acquisition



Slice



Data over experimental Duration (4 seconds)

(ii) BiLSTM with Attention for Feature Extraction

LSTM Cell
LSTM Cell

Attention

Labels

L

R

B

F

Backprop



4 Tasks

Intra-feature Modeling

(iii) Graph Convolutional Neural Network

Labels

L

R

B

F

Backprop

Softmax

Flatten

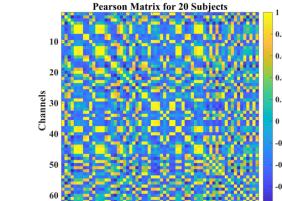
Max Pooling

GCN

Features

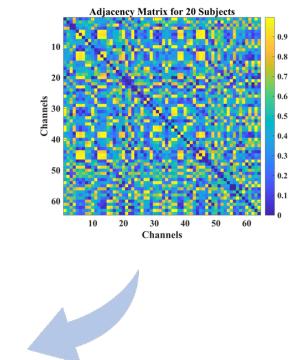


Pearson Matrix

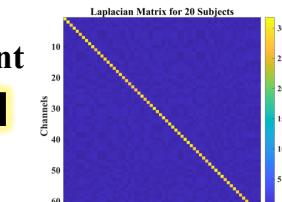


Intra-feature
Relationship

Adjacency Matrix

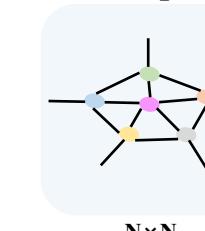


Laplacian Matrix



Present

Graph



Topological Structure of Features

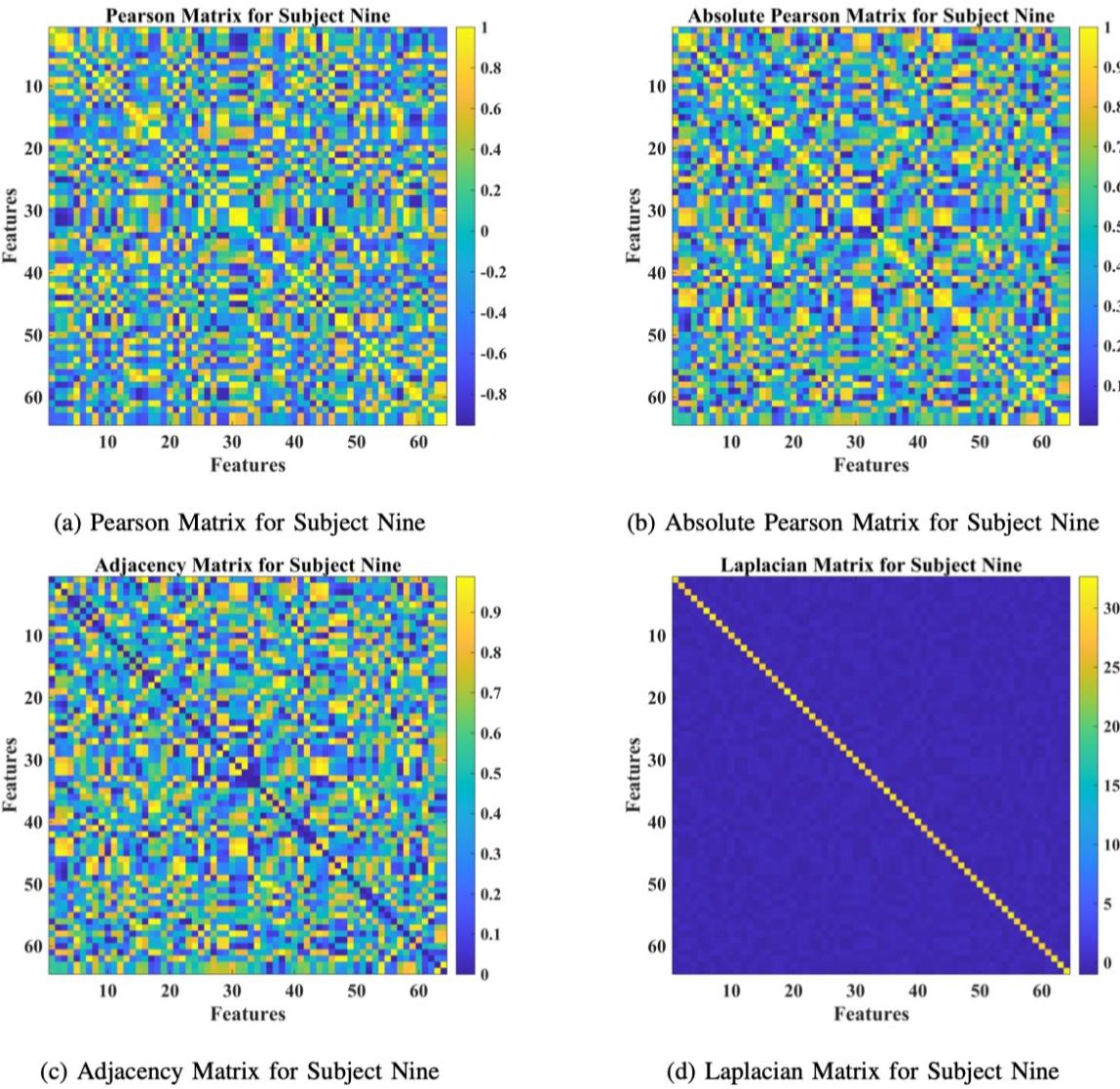
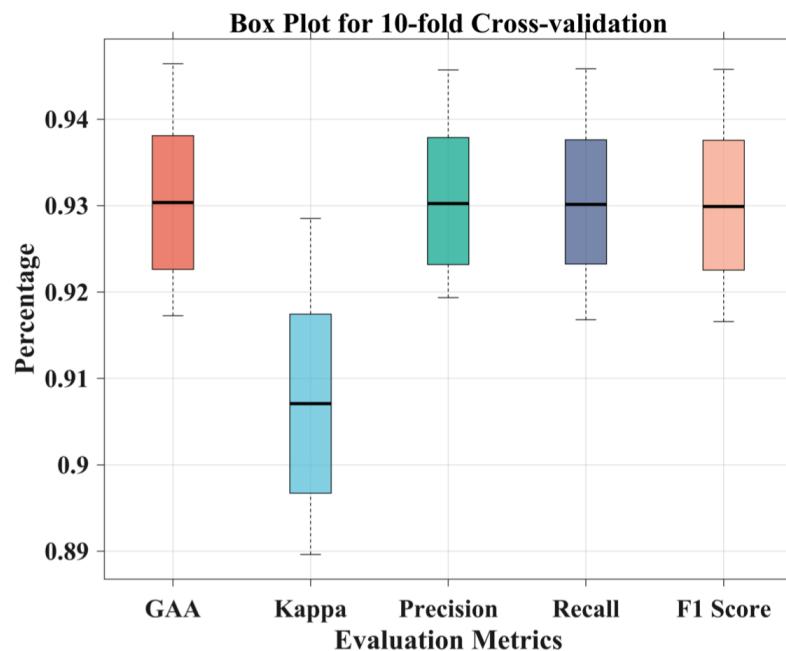
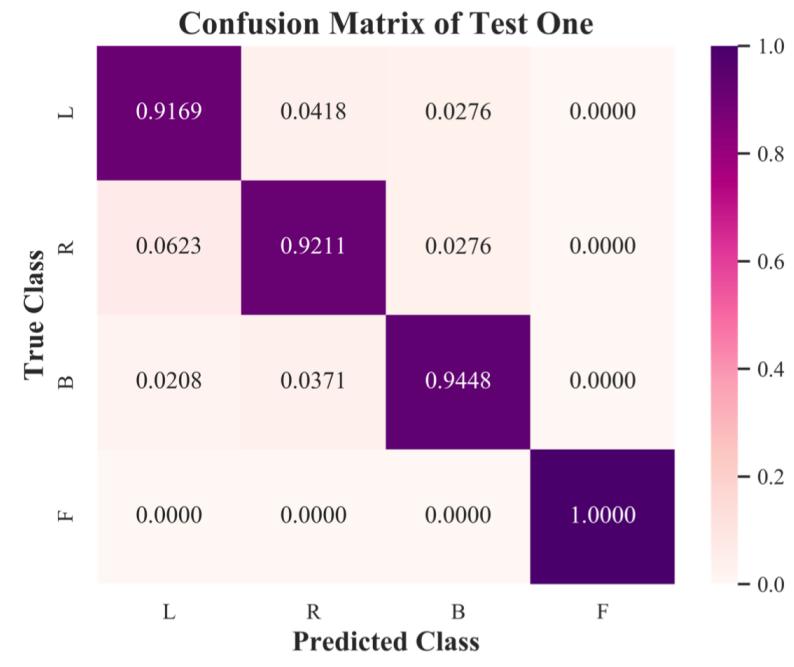


Fig. 4: The Pearson, Absolute Pearson, Adjacency, and Laplacian Matrices for Subject Nine.

Experimental Results - Groupwise Prediction



(a) Box Plot for 10-fold cross validation



(b) Confusion Matrix of Test One

Fig. 5: Box plot and confusion matrix for 10-fold cross validation.

Note:

- (1) Box Plot (Maximum Score, Upper Quartile, Median, Lower Quartile, and Minimum Score)
- (2) Confusion Matrix: TP, TN, FP, and FN

Experimental Results - Subject-Specific Adaptation

TABLE II: Subject-level Evaluation

No. of Subject	GAA	Kappa	Precision	Recall	F1 Score
1	94.05%	92.06%	94.20%	94.32%	94.16%
2	96.43%	95.19%	96.06%	96.06%	96.06%
3	97.62%	96.79%	97.33%	97.08%	97.18%
4	90.48%	87.34%	91.30%	91.11%	90.42%
5	95.24%	93.61%	95.96%	95.06%	95.38%
6	94.05%	92.02%	93.40%	94.96%	93.66%
7	98.81%	98.40%	98.81%	99.07%	98.92%
8	95.24%	93.60%	95.39%	95.04%	95.19%
9	98.81%	98.39%	99.11%	98.68%	98.87%
10	94.05%	91.98%	93.39%	94.70%	93.61%
Average	95.48%	93.94%	95.50%	95.61%	95.35%

TABLE III: Current studies comparison on subject-level prediction

Related Work	Max. GAA	Approach	Database
Ortiz-Echeverri <i>et al.</i> (2019)	94.66%	Sorted-fast ICA-CWT + CNNs	
Sadiq <i>et al.</i> (2019)	95.20%	EWT + LS-SVM	BCI Competition IV-a Dataset
Taran <i>et al.</i> (2018)	96.89%	TQWT + LS-SVM	
Zhang <i>et al.</i> (2019)	83.00%	CNNs-LSTM	
Ji <i>et al.</i> (2019)	95.10%	SVM	BCI Competition IV-2a Dataset
Amin <i>et al.</i> (2019)	95.40%	MCNNs	
Dose <i>et al.</i> (2018)	68.51%	CNNs	
Hou <i>et al.</i> (2019)	96.00%	ESI + CNNs	Physionet Database
This work	98.81%	Attention-based BiLSTM-GCN	

Takeaways and Future Work

✓ [Spatial-Temporal Analysis]

- (1) Converge to both Subject-level and Groupwise Predictions and handle Individual Variability.
- (2) The 0.4-s sample size Time-Resolved Solution toward fast response.

✓ [Deep Feature Mining]

- (1) ↑ Highest Accuracy
- (2) Advance Clinical Translation of EEG MI-based BCI technology to meet diverse demands, such as those of paralyzed patients.

✓ [Future Work]

Long-range Dependencies among intra-subject or inter-subject EEG signals can be modeled via **Non-local Modeling**, **Self-attention Mechanism**, **Transformer**, and **AI foundation Models**.

Thank you!

Any question?