

BEM-FMM TES Modeling Toolkit (Module) v. 0.3

Description

September 5, 2020

Contents

1. **Quick start sequence for code evaluation (Windows, MATLAB)**
2. Use, System Requirements, and Third-Party Components
3. Toolkit Organization
4. Computational Workflow Overview (main folder)
5. Head Model Import and Processing Overview (subfolder Model)
6. Control and Test of Numerical Accuracy
7. Application Example #1. Two electrodes on the surface of a cube
8. Application Example #2. Two electrodes on the surface of a composite cube
9. Application Example #3. Intracranial fields for Connectome Subject 110411

The toolkit is intended for academic use only. The software platform is MATLAB 2019a or newer (Windows/Linux). While the Windows implementation is stable and fast, the Linux implementation of the method may require extra recompilation of the FMM distributables ([3]) as described in the FMM software manual.

1. Quick start sequence for code evaluation (Windows, MATLAB)

Download the software – folder TES_Package. Open MATLAB. Go to folder Version0.3_example3_110411. From this main folder, switch the working directory to the Model subfolder.

- Run model01_main_script.m to perform necessary model precomputations.

Switch to the main folder, then run all the scripts of the main folder strictly sequentially to analyze all fields in the default example:

- Run bem0_load_model.m
- Run bem1_configure_electrodes.m. Observe and close the figure.
- Run bem2_charge_engine.m. Observe and close the figure.
- Run bem3_surface_field_c.m. Observe and close the figure.
- Run bem3_surface_field_e.m. Observe and close the figure.
- Run bem3_surface_field_p.m. Observe and close the figure.
- Run bem3_surface_field_th.m. Observe and close the figure.
- Run bem4_define_planes.m. Observe and close each figure.
- Run bem5_volume_e_XY/XZ/YZ.m. Observe and close each figure.
- Run bem5_volume_p_XY/XZ/YZ.m. Observe and close each figure.

2. Use, System Requirements, and Third-Party Components

The toolkit is intended for academic use only. The default software platform is MATLAB 2019a/b or newer (Windows/Linux). The toolkit runs “as is” under Windows and does not require any extra compilation. While the Windows implementation is stable and relatively fast (but not yet optimized for maximum speed), the Linux implementation of the method may require extra recompilation of the FMM distributables (Gimbutas et al., 2019) as described in the corresponding software manual (Gimbutas et al., 2019).

The following toolboxes (usually supplied with the MATLAB Academic Package) are required: Image Processing Toolbox (for NIfTI data processing if necessary), Partial Differential Equations or Antenna Toolbox (for model remeshing if necessary), and Statistics and Machine Learning Toolbox (for geometrical search of nearest neighbors used in the volumetric field plots). Those toolboxes are not absolutely necessary, but the toolkit must be modified to operate without them, and its performance will somewhat degrade. The FMM engine (Gimbutas et al., 2019) and example setups with SimNIBS segmentation (Saturnino et al 2019) of Human Connectome Project subjects 101309, 110411, 117122, 120111, 122317, 122620, 124422, 128632, 130013, 131722, 138534, 149337, 149539, 151627, 160123, and 198451 (Van Essen et al 2012-2019), as well as example setups with the SimNIBS Ernie model (Thielscher et al 2015), have been included with permission in the redistributable software package.

3. Toolkit Organization

The toolkit contains a number of short MATLAB or MATLAB-compatible scripts organized within three subfolders – `Model`, `Engine`, and `Electrodes` – and a number of scripts located in the main folder, as shown in Fig. 1. The folders are organized as follows:

1. The main folder contains all major computational scripts which define cortical dipole assembly, perform computations, and output fields and potential both on surfaces and in volume. If NIfTI data are available, surface meshes and fields can be registered against NIfTI slices using the built-in NIfTI viewer.
2. The subfolder `Model` contains the head model that will be used for analysis. It also contains tools for remeshing (coarsening or refining) the head model and for performing necessary precomputations, such as double potential integrals for neighbor facets.
3. The subfolder `Engine` contains computational scripts and functions serving different purposes, including the BEM-FMM engine.
4. The subfolder `Electrodes` contains computational scripts and functions for different electrode assembly.

All scripts can be changed/modified and rearranged to organize parametric loops if necessary. The scripts of the main folder can be executed at any time for the default configuration.

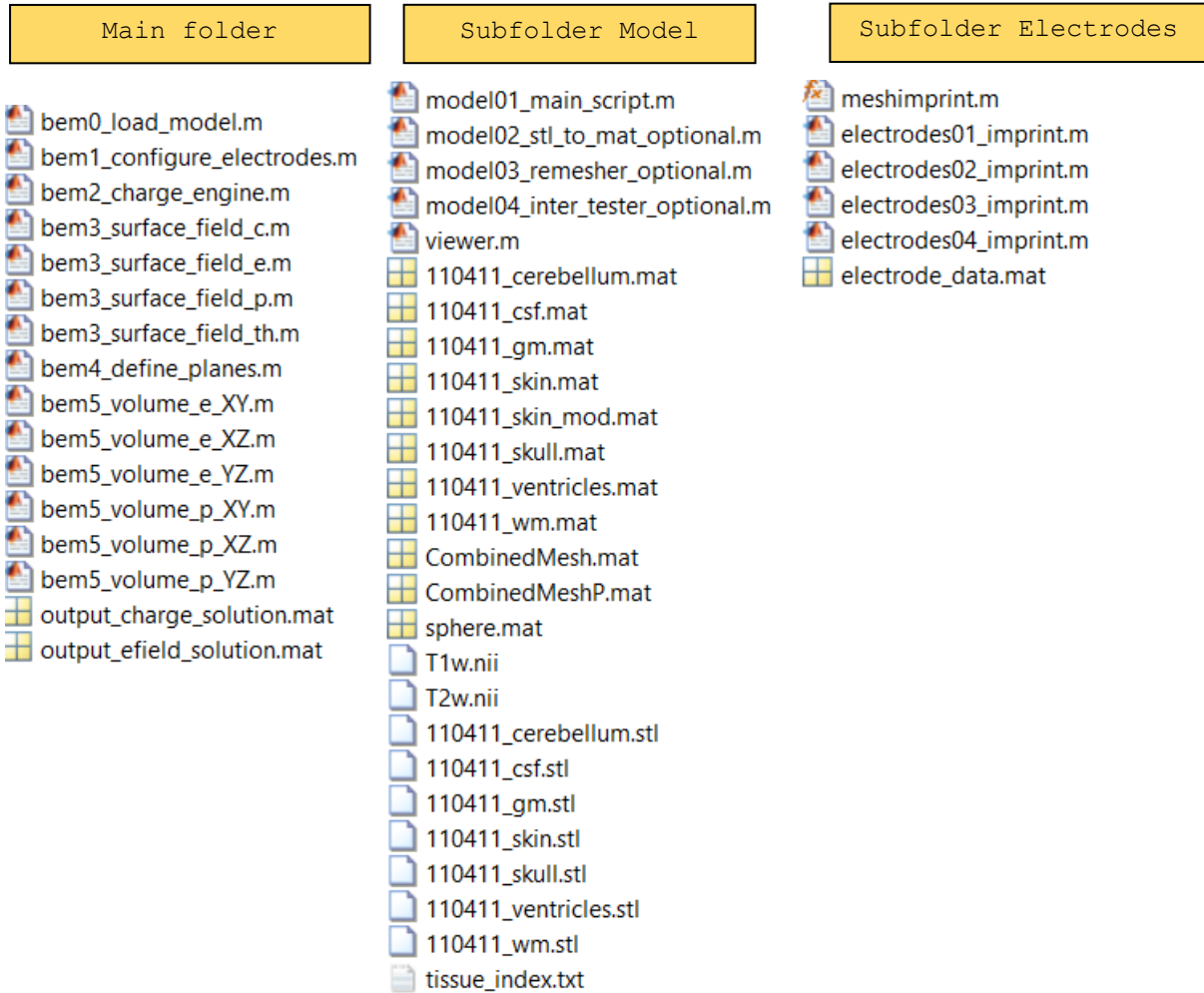


Fig. 1. Low-level organization chart of the toolkit.

4. Computational Workflow Overview (main folder)

The computations are performed in the main folder. The scripts of the main folder should initially be executed sequentially but may subsequently be executed in any order since all the data have already been computed.

The first script, `bem0_load_model.m`, imports head model data into the MATLAB workspace and sets the MATLAB path. It also imports the previously computed solution, if available.

The second script `bem1_configure_electrodes.m` loads pre-existing electrode configuration and initializes electrode voltages. The electrode configuration itself is defined and assembled in subfolder `Electrodes` via a separate MATLAB script and prior to performing any computations. Electrodes are accurately imprinted, and the skin surface mesh is modified accordingly. After every new geometrical electrode assembly, you must rerun the `model01_main_script.m` script in the `Model` folder to update the complete head mesh. Otherwise, incorrect results will be generated.

BEM-FMM engine. The next script to be executed is `bem2_charge_engine.m`. This script

- (i) computes the iterative solution of the BEM integral equation for the induced surface charge density using the FMM, precomputed near-field potential integrals, and MATLAB GMRES (generalized minimum-residual method, Saad 2003);
- (ii) displays the time for every iteration step in the MATLAB command window and plots the entire convergence history when completed;
- (iii) computes the resulting surface electric fields (the principal component) and surface electric potentials via triangle subdivision (optional).

As for the near-field integration accuracy, the double potential integrals for three neighbor triangular patches (default value is given in the script `model01_main_script.m`) are computed precisely using the solid-angle approach. For non-neighbor triangles, the center-point approximation is used for the double potential integrals and FMM. The number of neighbor integrals can be increased at the expense of larger memory usage.

Surface charge averaging (optional). For practical purposes, it might be convenient to introduce weighted surface charge averaging (i.e., to low pass filter the surface charge density). One option is to average over the target facet and its three immediate topological neighbor triangles. After the solution is obtained, we might substitute in the script `bem2_charge_engine.m`

```
c = (c.*Area + sum(c(tneighbor).*Area(tneighbor), 2))./(Area + sum(Area(tneighbor), 2));
```

This rule can be modified if necessary.

When performing mathematical (FMM) operations, the scripts of this folder call original and derived FMM functions from the subfolder `Engine`.

Fields at interfaces. After the computations have been completed, the scripts

`bem3_surface_field_c/e/p/th.m` display the surface charge density distribution, the surface electric field just inside/outside any interface, the continuous electric potential/voltage at the interfaces, and thresholded electric field just inside/outside any interface.

Surface data precomputation and NIfTI data import. The next script is

`bem4_define_planes.m`. This script defines three principal observation planes and prepares mesh cross-sections that will be used in the field output plots.

If NIfTI data are available (e.g. `T1w.nii`), they will be included in subsequent visualizations which will superimpose mesh cross-sections and/or fields onto the corresponding NIfTI slices.

Volumetric fields in principal planes. The scripts `bem5_volume_e/p_XY/XZ/YZ.m` compute and output the electric field (any of its Cartesian components or a magnitude), and the electric potential in the three principal planes. The plane position and its size are specified in the script `bem4_define_planes.m`.

The volumetric field computations require more time since the potential integrals are no longer precomputed and must be calculated at the time of execution, depending on the position of a

given observation point relative to the nearest interface(s). The critical numerical parameter here is the dimensionless (vs. average triangle size) radius, R , of an integration sphere within which integration of the surface charge density is performed. Its default value ranges between 2 and 5; higher numbers (e.g., $R = 10$) may provide better field accuracy but simultaneously slow down the computations.

Comparisons with FEM numerical solutions. A comparison with Ansys Maxwell Electronics Desktop FEM software solutions obtained using adaptive mesh refinement and very large tetrahedral meshes is performed in two separate folders: Version 0.3_example1_single_brick and Version 0.3_example2_composite_brick.

5. Head Model Import and Processing Overview (subfolder **Model1**)

Two acceptable model formats. The head model files should always be located in the dedicated folder **Model** with contents shown in Fig. 1. The primary set are *.stl (stereolithography) files for every individual brain compartment in the form of a faceted shell. The *.stl files use triangular facets with normal vectors facing out of the shell. This is the standard output of the SimNIBS segmentation pipeline and other relevant software packages. The number of shells may be arbitrary. The script `model02_stl_to_mat_optional.m` converts *.stl files, either binary or ASCII, to equivalent MATLAB data files (using MATLAB's built-in function `stlread` or otherwise) containing arrays of vertices P , facets t , and normal vectors \mathbf{n} . Every MATLAB data file can further be inspected and visualized using the function `viewer.m` from the same subfolder (as shown in Fig. 2a below). Repeat this last operation for every brain compartment (or spherical shell) in the folder.

Built in head models. For computational studies that do not involve MRI data collection, the present package is augmented with 16 realistic head models for 16 Connectome Project (Van Essen et al., 2012-2019) subjects with isotropic voxel resolution of 0.7 mm. These are subjects #101309, 110411, 117122, 120111, 122317, 122620, 124422, 128632, 130013, 131722, 138534, 149337, 149539, 151627, 160123, and 198451. The datasets have been converted to surface models with the help of the SimNIBS 2.1 pipeline; every model includes seven brain compartments (skin, skull, CSF or cerebrospinal fluid, GM or gray matter, WM or white matter, ventricles, cerebellum). Every model has been checked and confirmed against the original NIfTI images and with regard to mesh manifoldness (Htet et al., 2019b). The default average cortical surface mesh edge length is 1.4 mm, the cortical nodal density is 0.55 nodes per mm², and the total number of facets is 0.9 M.

In addition to the Connectome Project head models, the package also includes the default example model of the SimNIBS 2.1 pipeline, the Ernie model. This model is comparable in complexity to the Connectome models, with 0.9 M facets and seven tissue meshes.

Any other surface model obtained from the SimNIBS pipeline may be used in *.stl or *.mat (MATLAB) format. In particular, fifty CAD models, known as the Population Head Model

Repository or PHM (Lee et al 2016, Lee et al 2018), have been made available from the website of the IT'IS Foundation, Switzerland (IT'IS Foundation 2016).

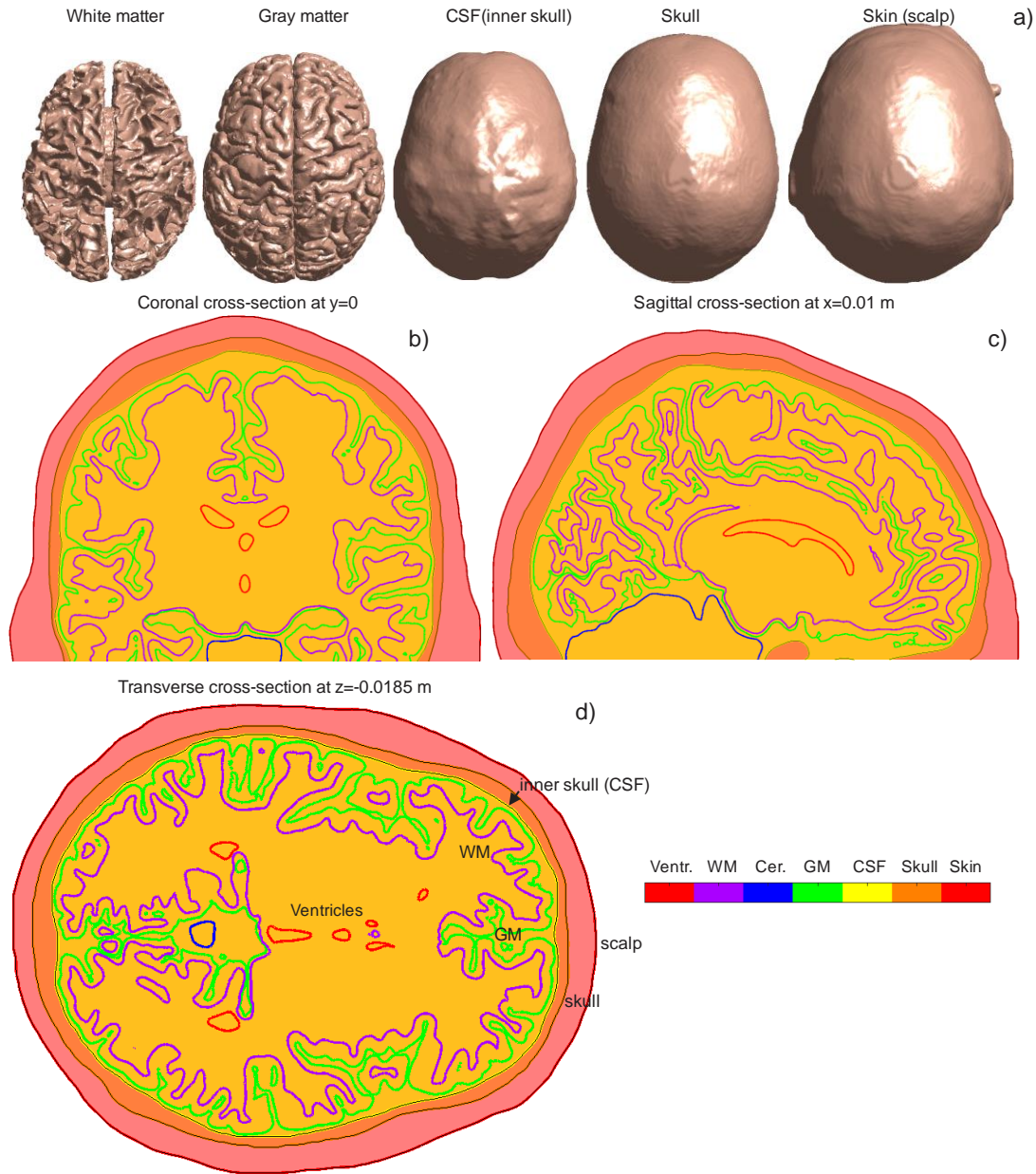


Fig. 2. a): Brain compartments of the default package head model # 110411: white matter (WM), gray matter (GM), cerebrospinal fluid (CSF or inner skull), skull, and skin. Cerebellum and ventricles are not shown. b-d): Head cross-sections in three principal planes.

Alternatively, the models described in detail in (Htet et al., 2019b) may be downloaded independently from the MATLAB Central link (Collection of Sixteen High-Quality Human Head CAD Models, 2019). The default head geometry in the folder `Model` is subject 110411 with the following seven 2-manifold watertight enclosed brain compartments: white matter (WM), gray matter (GM), cerebrospinal fluid (CSF or inner skull), skull, skin, cerebellum, and

ventricles. These brain compartments, with the exception of the cerebellum and ventricles, are shown in Fig. 2.

Processing NIfTI Data. NIfTI data (if available) should be located in the same subfolder `Model` as shown in Fig. 1. For example, the Connectome Project database contains T1 and T2 NIfTI data for every subject, which were made available with permission. The default application example uses subject 110411.

Model remeshing. A CM2 SurfRemesh[®] remeshing program from Computing Objects, France is included in the MATLAB package. This software enables creation of coarser and/or finer surface representations while minimizing the surface deviation error from the master mesh. MATLAB script `model03_remeshmer_optional.m` performs automated remeshing to any required maximum edge length, which should be given at the beginning of the script.

For example, the remeshing program generates a coarser model with the average cortical edge length of 1.9 mm and the average cortical nodal density of 0.32 nodes per mm² when the maximum edge length is chosen as 3 mm; the total number of facets is 0.4 M. On the other hand, the same program generates a finer model with the average cortical edge length of 0.99 mm and average cortical nodal density of 1.2 nodes per mm² when the maximum edge length is chosen as 1 mm; the total number of facets is then 1.8 M. Fig. 3 shows the corresponding surface meshes for the gray matter shell along with the original segmentation. The red circles label sample areas of interest close to the precentral gyrus crown. Note that the remeshing procedure may require significant time. It may also fail in some cases.

Creating combined head mesh. The combined mesh for the entire head is created by appending individual meshes. This operation is performed by running the script `model01_main_script.m`. The combined mesh is stored in the MATLAB data file `CombinedMesh.mat`. An additional data file, `CombinedMeshP.mat`, is generated in the same folder. This file contains precomputed double surface electrostatic integrals over triangles necessary for accurate BEM-FMM simulations. The minimum number of neighbors for accurate EEG/MEG computations is 16. The integrals are computed in parallel, using 20 cores by default. The `numThreads` variable of `model01_main_script.m` may be adjusted depending on the computer configuration. Run the script `model01_main_script.m` to generate the data.

Defining tissue properties. The script `model01_main_script.m` reads from an editable tissue index file (named `tissue_index.txt`) in the `Model` subfolder to determine which `*.mat` tissue files to assemble into the final model and what conductivity values should be assigned to each of those tissues. Each line of a tissue index file provides the following information: tissue name (for reference in subsequent scripts), tissue source file, tissue conductivity, and enclosing tissue. It then assigns initial conductivity information to each facet of each tissue: the facet's interior conductivity (in the opposite direction of the facet's normal vector), the facet's exterior

conductivity (in the direction of the facet's normal vector), and the conductivity contrast across the facet.

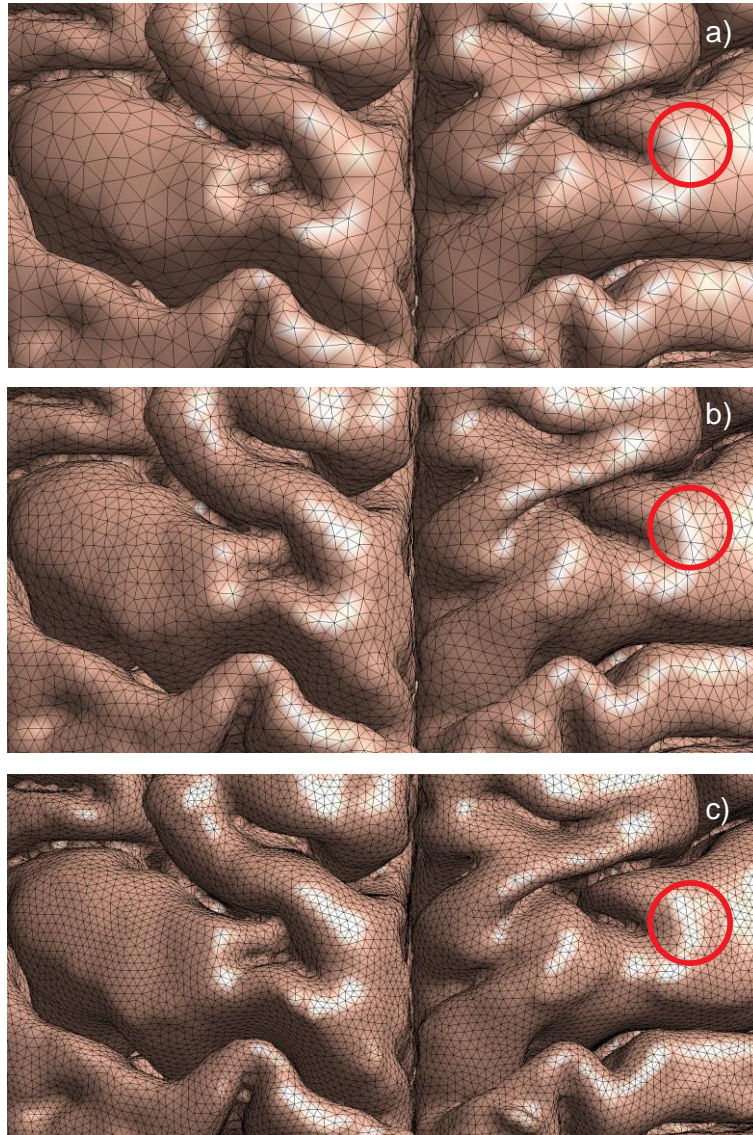


Fig. 3. a) – Coarser model with average cortical edge length of 1.9 mm and average cortical nodal density of 0.32 nodes per mm^2 ; b) – default meshing with average cortical surface mesh edge length of 1.5 mm and average cortical nodal density of 0.55 nodes per mm^2 ; c) – finer model with average cortical edge length of 0.99 mm and average cortical nodal density of 1.2 nodes per mm^2 . The red circle labels an area of interest close to the precentral gyrus crown.

Treating duplicated facets. This script also checks the combined mesh for duplicate facets and for facets whose centroids are too close to be treated with the BEM-FMM algorithm. For the Connectome models, there should be none of these complications, because tissues of these models surround and enclose each other without touching – they are hollow shells, where each shell segments a boundary between exactly two tissue types. Other models, however, do not

follow this meshing scheme. For example, the interior and exterior boundaries of every tissue of the MIDA model (Iacono et al 2015) are explicitly segmented. This means that the MIDA model's white matter and gray matter, for example, both independently segment their mutual boundary, producing a large number of duplicate facets. These duplicate facets would produce singularities that invalidate simulation results, so they are resolved as follows.

For each pair of duplicate facets, one is designated the facet to be deleted, and the other is designated the facet to be kept. The outer conductivity of the facet to be kept is set equal to the inner conductivity of the facet to be deleted, and associated conductivity contrast information is updated for the facet to be kept. The facet to be deleted, and all associated information, is then removed from the model. Fig. 4 below illustrates the results of this operation.

Tissue intersection marker points. The script `model04_inter_tester.m` finds intersection points between selected tissue meshes and an arbitrary ray. These data may be useful for further processing. Run the script and observe the generated results. Change the line definition if desired.

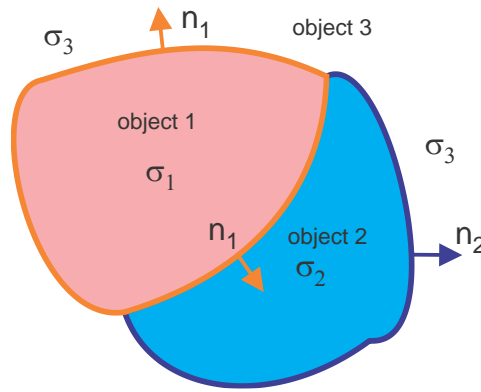


Fig. 4. Object 3 (with interior conductivity σ_3) surrounds and encloses both Object 1 (with interior conductivity σ_1) and Object 2 (with interior conductivity σ_2), so Object 1 and Object 2 initially list σ_3 as the exterior conductivity for all facets in their respective meshes. Because Object 1 and Object 2 have each explicitly segmented their mutual interface, that interface initially contains coincident facets contributed by both objects. In this example, Object 2's copies of the interface facets have been removed, and Object 1's copies of the facets remain. Object 1's facets at the interface still list σ_1 as their interior conductivity, but have changed their exterior conductivity from σ_3 to σ_2 .

6. Control and Test of Numerical Accuracy

For a given surface mesh resolution, the numerical accuracy of the method is controlled by the following parameters:

1. `RnumberE/RnumberP`, found in `Model\model01_main_script.m`: Number of neighbor potential electrostatic double surface integrals (separately for electric field and electric potential) to be computed precisely. The default number varies between 4 and 16. The maximum number is

unlimited, but is subject to memory constraints. Numbers above 16 do not affect the overall solution accuracy significantly.

2. `prec`, found in `Engine\bemf4_surface_field_electric.m` and in all other FFM implementations: Intrinsic FMM precision (Gimbutas et al., 2019). The default value is 0.01 (1%) which may be adequate for surface-based charge distributions. Values smaller than 0.001 do not affect the overall solution accuracy significantly.

3. `iter`, found in `bem2_charge_engine.m` in the main folder: Number of GMRES iterations used. The default value is 25. The maximum number is unlimited but is subject to speed constraints. Numbers above 50 do not affect the overall solution accuracy significantly.

4. `tneighbor`, found in `Model\model01_main_script.m`: Number of neighbor facets for optional averaging of the computed surface charge density after the solution had been obtained. The default number is 3 for manifold meshes.

5. `R`, found in `bem5_volume_b/e/p_XY/XZ/YZ.m` (in the main folder): Dimensionless (vs. average triangular face size) radius R of an integration sphere within which precise integration is performed. In `bem5_volume_b/e/p_XY/XZ/YZ.m`, it is the integration of the induced surface charge density on nearby triangles given an observation point in close proximity to them. The default value ranges between 2 and 5. The maximum number is unlimited but is subject to speed constraints.

7. Application Example #1. Two electrodes on the surface of a cube

In this example (folder `Version 0.3_example1_single_brick`), two voltage electrodes have been imprinted on one side of a conducting cube with a side length of 1 m. The major goal of this (somewhat simplified) example is to become familiar with code functionality and execution flow, and compare the results with another numerical solver – Ansys Electronics Desktop Maxwell. The main computational script `bem2_charge_engine.m` should execute in approximately 5 seconds (using a 2.4 GHz multicore server).

Assigning cube conductivity. There is only one “tissue” mesh in this folder (subfolder `Model`): a brick named `brick01.mat`. It has a size of 1000 mm and approximately 35,000 facets. The average triangle quality (twice the ratio of the inradius to the circumradius) is 0.81, and the average edge length (mesh resolution) is 20.6 mm. Run `viewer.m` and inspect the cube mesh and its properties.

The assigned cube conductivity value is 0.1 S/m. This value is given in the editable tissue index file (named `tissue_index.txt`) in the same subfolder `Model`.

Defining and imprinting electrodes. Go to subfolder `Electrodes` and run the script `electrodes01_imprint.m`. This script imprints two surface electrodes with the radius of 100 mm each separated by 500 mm on one (top) side of the brick.

Assembling model and computing potential integrals. Now, go to subfolder `Model` and run the script `model01_main_script.m`. Reduce the number of cores for parallel computations (the `numThreads` variable) if necessary. This script has to be executed only *once*.

Running simulations. After that, go to the main folder of the example. Run the first script, `bem0_load_model.m`. Next, open and run the second script `bem1_configure_electrodes.m`, which defines electrode voltages and a set of other parameters:

```
% Voltage (V) applied to each electrode
electrodeVoltages = [+1, -1]; % For electrode configuration 1
```

The next script to be executed is `bem2_charge_engine.m`. This script

- (i) computes the iterative solution of the BEM integral equation for the induced surface charge density using the FMM, precomputed near-field potential integrals, and MATLAB GMRES (generalized minimum-residual method);
- (ii) displays the time for every iteration step in the MATLAB command window and plots the entire convergence history when completed;
- (iii) computes resulting surface electric potentials.

Visualizing surface fields. The next scripts to execute are `bem3_surface_field_c/p.m`. These scripts display the surface charge distribution and the continuous surface electric potential.

Comparing two numerical solutions. The next script to execute is

`bem6_volume_comparison_XYZ.m`. This script computes the vector electric field within the cube for 0.125 M points uniformly distributed in space. The minimum offset from the boundary is 50 mm. Next, it compares the field with another numerical solution obtained using Ansys Electronics Desktop 2019 Maxwell FEM software with 5 adaptive mesh refinement passes and with the final mesh of 2 M tetrahedra. The Ansys solution executes in 44 min on the same server.

For the present example, the script generates two metrics of error for the vector electric field: the relative 2-norm (maximum singular value)

$$Error2norm(\mathbf{E}_{BEM}, \mathbf{E}_{FEM}) = \|\mathbf{E}_{BEM} - \mathbf{E}_{FEM}\| / \|\mathbf{E}_{FEM}\| \quad (1)$$

and the vector field norm given by (symbol $\|\cdot\|$ now denotes the Euclidean vector norm)

$$ErrorV(\mathbf{E}_{BEM}, \mathbf{E}_{FEM}) = \frac{\sqrt{\sum_{k=1}^K \|\mathbf{E}_{k,BEM} - \mathbf{E}_{k,FEM}\|^2}}{\sqrt{\sum_{k=1}^K \|\mathbf{E}_{k,BEM}\| \|\mathbf{E}_{k,FEM}\|}} \quad (2)$$

Both electric-field errors appear to be **0.57%**.

Visualizing volumetric fields. Run the script `bem4_define_planes.m` next to define the observation planes. The following scripts `bem5_volume_e/p_XY/XZ/YZ.m` will finally plot the volumetric electric fields and potential distributions in the observation planes.

8. Application Example #2. Two electrodes on the surface of a cube

This example (folder `Version 0.3_example1_composite_brick`) is identical to the previous one, but a composite brick with approximately 71,000 facets is considered shown in Fig. 5.

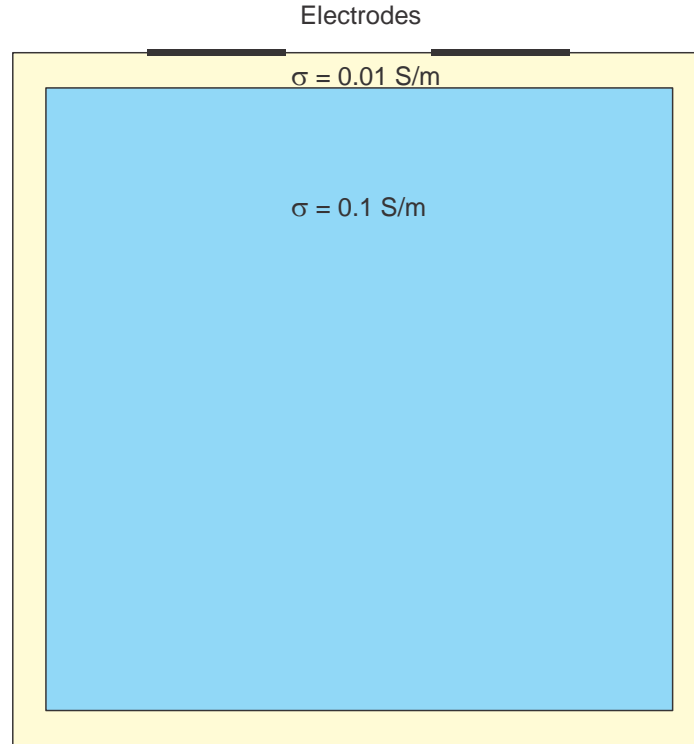


Fig. 5. Problem geometry and electrode position.

Running simulations. The code sequence of the previous example is executed in approximately 11 seconds (using a 2.4 GHz multicore server). The script `bem6_volume_comparison_XYZ.m` computes the vector electric field within the cube for 0.125 M points uniformly distributed in space. The minimum offset from the inner boundary in Fig. 5 is again 50 mm. Next, it compares the field with another numerical solution obtained using Ansys Electronics Desktop 2019 Maxwell FEM software with 9 adaptive mesh refinement passes and with the final mesh of 2 M tetrahedra. Ansys solution executes in 1 h 42 min on the same server. The script generates both electric-field errors of **0.40%**.

9. Application Example #3. Fronto-Medial Electrode Configuration for Connectome Subject 110411

In this example, we consider a realistic head model – Connectome subject 110411 – with seven head compartments (Htet et al., 2019b). The default average cortical surface mesh edge length is approximately 1.4 mm, the cortical nodal density is 0.55 nodes per mm^2 , and the total number of facets is 0.9 M. The main computational script `bem2_charge_engine.m` should execute in less

than 1-2 min (using a 2.4 GHz multicore server). However, the execution time is typically larger than for EEG/MEG or TMS modeling with the BEM-FMM.

Defining electrodes. The corresponding example folder is `Version 0.3_example3_subject110411`. The electrode configuration itself is defined and assembled in subfolder `Electrodes` via a separate MATLAB script (`electrodes01_imprint.m`) and prior to performing any computations. Electrodes are accurately imprinted, and the skin surface mesh is modified accordingly. After every new geometrical electrode assembly, you must rerun the `model01_main_script.m` script in the `Model` folder to update the complete head mesh. Otherwise, incorrect results will be generated.

Assigning conductivities of spherical compartments, assembling combined geometry, and computing potential integrals. There are seven tissue meshes (skin, skull, CSF, GM, WM, cerebellum, ventricles) in this folder (subfolder `Model`); six of them are shown in Fig. 2. The meshes are inspected with the function `viewer.m` from the same subfolder.

The assigned conductivity values are the standard values used in the SimNIBS package (Saturnino et al 2019). These values are again given in the editable tissue index file (`tissue_index.txt`) in the same subfolder `Model`.

Now, run the script `model01_main_script.m`, which combines all partial meshes (including the skin mesh with embedded electrodes) together and computes necessary potential integrals. Reduce the number of cores for parallel computations (the `numThreads` variable) if necessary. This script has to be executed only *once*.

Next, go to the main folder of the example. Run the first script, `bem0_load_model.m`. After that, open and run the second script `bem1_configure_electrodes.m` to define electrode voltages and other parameters.

Running simulations. The next script to be executed is `bem2_charge_engine.m`. This script

- (i) computes the iterative solution of the BEM integral equation for the induced surface charge density using the FMM, precomputed near-field potential integrals, and MATLAB GMRES (generalized minimum-residual method, Saad 2003);
- (ii) displays the time for every iteration step in the MATLAB command window and plots the entire convergence history when completed;
- (iii) computes resulting surface electric fields (the principal component) and surface electric potentials via triangle subdivision (optional).

Visualizing surface fields. After the computations have been completed, the scripts `bem3_surface_field_c/e/p/th.m` display the surface charge density distribution, the surface electric field just inside/outside any interface, the continuous electric potential/voltage at the interfaces, and thresholded electric field just inside/outside any interface or compartment. The compartment identifier is variable `tissue_to_plot`.

Plotting volumetric fields. Run the script `bem4_define_planes.m` next to define the observation planes. The following scripts `bem5_volume_e/p_XY/XZ/YZ.m` will finally plot the volumetric electric fields and potential distributions in the observation planes. The plot resolution is controlled by variable `Ms`; the field threshold (for graphics) is controlled by variable(s) `th`; the number of plot levels is controlled by variable `levels`.

References

- [1] Collection of Sixteen High-Quality Human Head CAD Models. 2019. MATLAB Central Onl: <https://www.mathworks.com/matlabcentral/fileexchange/69517-collection-of-sixteen-high-quality-human-head-cad-models>
- [2] Engwer C, Vorwerk J, Ludewig J, Wolters CH. A Discontinuous Galerkin Method to Solve the EEG Forward Problem Using the Subtraction Approach. *SIAM J. Sci. Comput.* 2017;39(1): B138–B164. doi. 10.1137/15M1048392.
- [3] Gimbutas Z, Greengard L, Magland J, Rachh M, Rokhlin V. fmm3D Documentation. Release 0.1.0. 2019. Online: <https://github.com/flatironinstitute/FMM3D>
- [4] Gomez L, Dannhauer M, Koponen L, & Peterchev A.V. Conditions for numerically accurate TMS electric field simulation. *bioRxiv 505412* 2018b. doi: <https://doi.org/10.1101/505412>.
- [5] Gomez LJ, Dannhauer M, Koponen LM, Peterchev AV. Conditions for numerically accurate TMS electric field simulation. *Brain Stimul.* 2019 Oct 3. pii: S1935-861X(19)30378-X. doi: 10.1016/j.brs.2019.09.015.
- [6] Greengard L, Rokhlin V. A fast algorithm for particle simulations. *J. Comput. Phys.* 1987;73(2):325-348. doi: 10.1016/0021-9991(87)90140-9.
- [7] Hasgall PA, Di Gennaro F, Baumgartner C, Neufeld E, Lloyd B, Gosselin MC, Payne D, Klingensböck A, Kuster N. *IT'IS Database for thermal and electromagnetic parameters of biological tissues*. Version 4.0, May 15, 2018. doi: 10.13099/VIP21000-04-0. Onl: www.itis.ethz.ch/database.
- [8] Htet AT, Saturnino GB, Burnham EH, Noetscher G, Nummenmaa A, Makarov SN. Comparative performance of the finite element method and the boundary element fast multipole method for problems mimicking transcranial magnetic stimulation (TMS). *J Neural Eng.* 2019a;16:1-13. doi: <https://dx.doi.org/10.1088/1741-2552/aafbb9>.
- [9] Htet AT, Burnham EH, Noetscher GM, Pham DN, Nummenmaa A, Makarov SN. Collection of CAD human head models for electromagnetic simulations and their applications. *Biomedical Physics & Engineering Express.* 2019b; 6(5):1-13. doi: <https://doi.org/10.1088/2057-1976/ab4c76>.
- [10] Human Connectome Project. *S1200 Reference Manual*. April 10 2018. Onl: https://www.humanconnectome.org/storage/app/media/documentation/s1200/HCP_S1200_Release_Reference_Manual.pdf

- [11] Iacono MI, Neufeld E, Akinnagbe E, Bower K, Wolf J, Oikonomidis I, Sharma D, Lloyd B, Wilm B, Wyss M, Pruessman K, Jakab A, Makris N, Cohen E, Kuster N, Kainz W, and Angelone LM. MIDA: A Multimodal Imaging-Based Detailed Anatomical Model of the Human Head and Neck. *PLoS One* 2015; 10(4). doi: 10.1371/journal.pone.0124126
- [12] Lee E, Duffy W, Hadimani R, Waris M, Siddiqui W, Islam F, Rajamani M, Nathan R, Jiles D. Investigational Effect of Brain-Scalp Distance on the Efficacy of Transcranial Magnetic Stimulation Treatment in Depression. *IEEE Trans. Magn.*, 2016;52(7):1-4. doi: 10.1109/TMAG.2015.2514158.
- [13] Lee EG, Rastogi P, Hadimani RL, Jiles DC, Camprodon JA. Impact of non-brain anatomy and coil orientation on inter- and intra-subject variability in TMS at midline. *Clin Neurophysiol.* 2018 Sep;129(9):1873-1883. doi: 10.1016/j.clinph.2018.04.749. Appendix A. Supplementary data.
- [14] Makarov SN, Noetscher GM, Raij T, Nummenmaa A. A Quasi-Static Boundary Element Approach with Fast Multipole Acceleration for High-Resolution Bioelectromagnetic Models. *IEEE Trans. Biomed. Eng.* 2018;65(12):2675-2683. doi: 10.1109/TBME.2018.2813261.
- [15] Piastra MC, Nüßing A, Vorwerk J, Bornfleth H, Oostenveld R, Engwer C, Wolters CH. The Discontinuous Galerkin Finite Element Method for Solving the MEG and the Combined MEG/EEG Forward Problem. *Frontiers in Neuroscience.* 2018;12(Article 30):1-18. doi: 10.3389/fnins.2018.00030
- [16] Rokhlin V. Rapid Solution of Integral Equations of Classical Potential Theory. *J. Computational Physics*, 1985;60(2):187–207. doi: 10.1016/0021-9991(85)90002-6.
- [17] Saad Y. *Iterative Methods for Sparse Linear Systems*. 2nd Ed., Society for Industrial and Applied Mathematics. 2003. ISBN 978-0-89871-534-7.
- [18] Sarvas J. Basic mathematical and electromagnetic concepts of the biomagnetic inverse problem. *Phys. Med. Biol.* 1987; 32(1):11-22. PMID: 3823129.
- [19] Saturnino GB, Puonti O, Nielsen JD, Antonenko D, Madsen KH, Thielscher A. SimNIBS 2.1: A Comprehensive Pipeline for Individualized Electric Field Modelling for Transcranial Brain Stimulation. In: Makarov S, Noetscher G, Horner M. Eds. *Brain and Human Body Modeling*. Springer Nature. NY 2019. ISBN 9783030212926.
- [20] The Population Head Model Repository. 2016. IT'IS Foundation website. doi: 10.13099/ViP-PHM-V1.0. Online: <https://www.itis.ethz.ch/virtual-population/regional-human-models/phm-repository/>
- [21] Thielscher A, Antunes A, and Saturnino GB. Field modeling for transcranial magnetic stimulation: a useful tool to understand the physiological effects of TMS? *IEEE EMBS 2015*, Milano, Italy.
- [22] Van Essen DC, Ugurbil K., Auerbach E, Barch D, Behrens TE, Bucholz R, Chang A, Chen L, Corbetta M, Curtiss SW, Della Penna S, Feinberg D, Glasser MF, Harel N, Heath AC, Larson-Prior L, Marcus D, Michalareas G, Moeller S, Oostenveld R, Petersen SE,

Prior F, Schlaggar BL, Smith SM, Snyder AZ, Xu J, Yacoub E. The Human Connectome Project: A data acquisition perspective. *NeuroImage*, 2012;62(4):2222–2231. doi: 10.1016/j.neuroimage.2012.02.018. PMID: 22366334. Online: <http://www.humanconnectomeproject.org/>.