

Design methodology of freeze-thaw processes towards industrial manufacturing of induced pluripotent stem cells

iPS細胞の実生産に向けた凍結・解凍プロセスの設計手法

M2

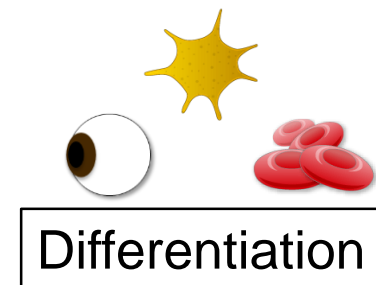
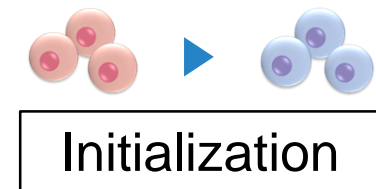
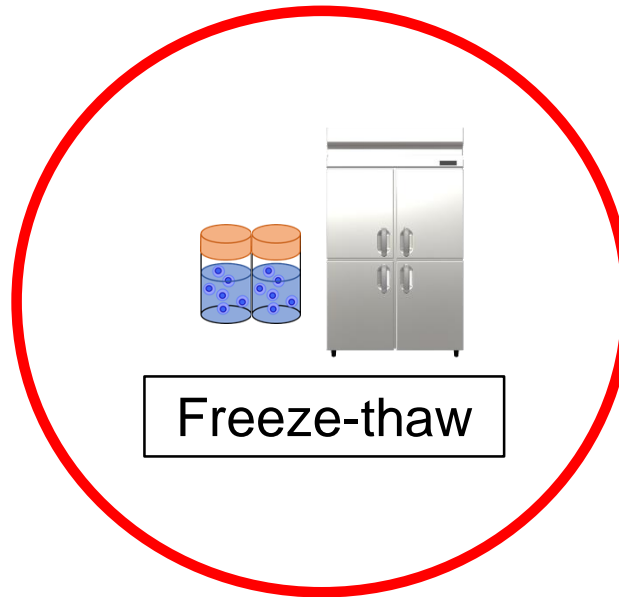
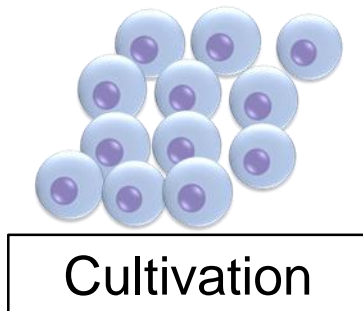
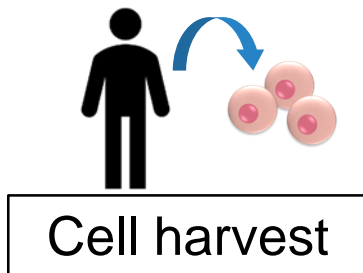
Yusuke Hayashi

Background

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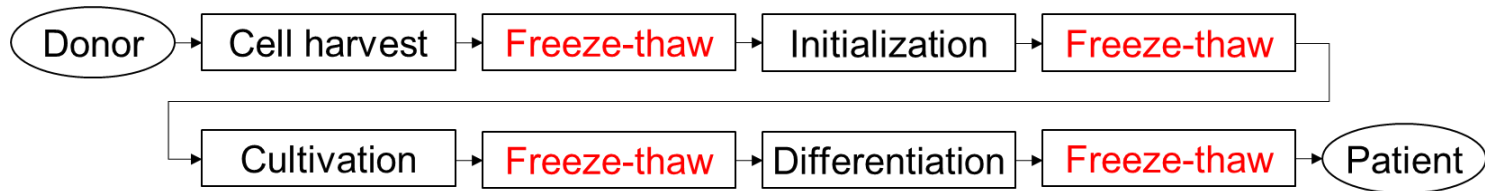
- **Induced pluripotent stem (iPS) cells**

- Potential to be differentiated into all tissue and organs.
- Attract much interest in disease modeling, personalized medicine.
- Standardization of manufacturing process is necessary.



- **Freeze-thaw process**

- It is required to transport and cryopreserve iPS cells.
- There are many freeze-thaw processes in manufacturing.



- iPS cells are known to be vulnerable to freezing and thawing[1].

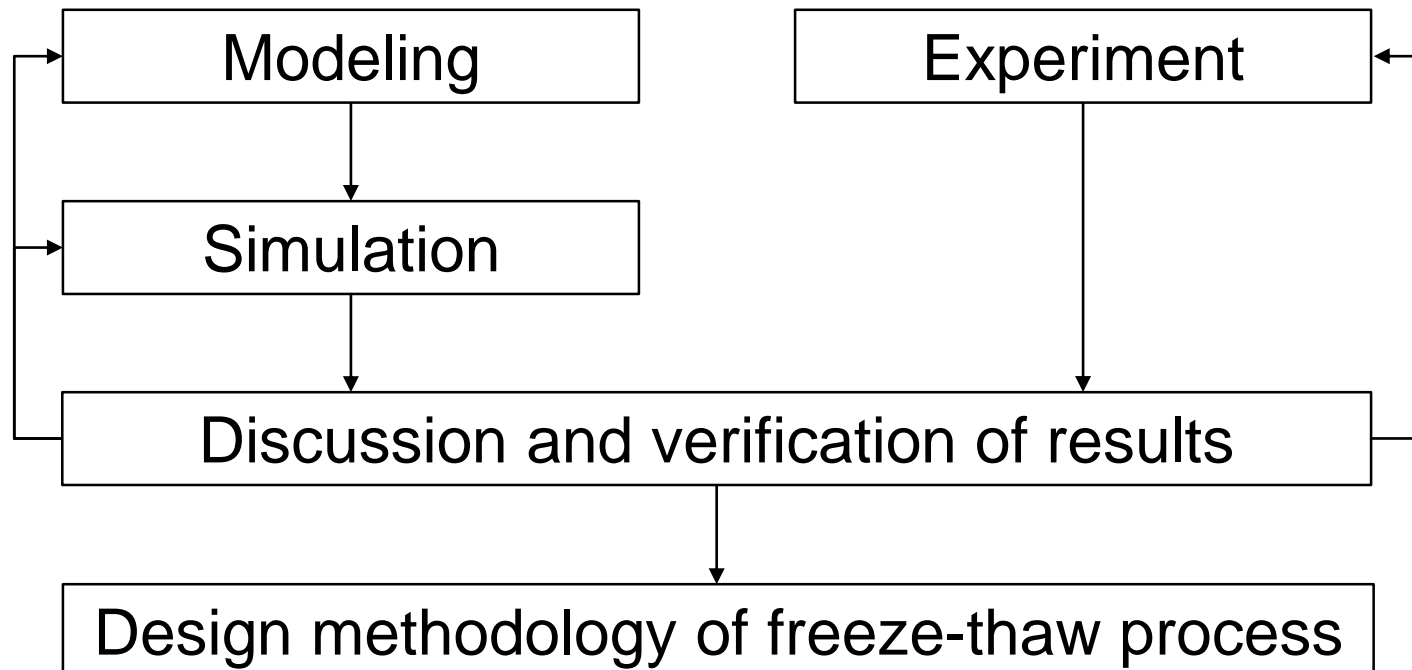
- **Previous study**

- Cryoprotective agent study[2]
- Experimental study[3,4]

In the freeze-thaw process, it is important to evaluate the impact of heat and mass transfer through the cell membrane.

Objective

Development of design methodology of freeze-thaw process for iPS cells considering heat and mass transfer



Experiment (In the future)

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- **Program freezer (Freezing)**

- Cooling rate : 1 K~3 K/min
- Lowest temp. : 193 K



Program freezer



Cryovial[1]

- **Cryovial**

- Made of polypropylene
- Diameter : 12 mm
- Height : 48 mm

- **Constant temperature water bath (Thawing)**

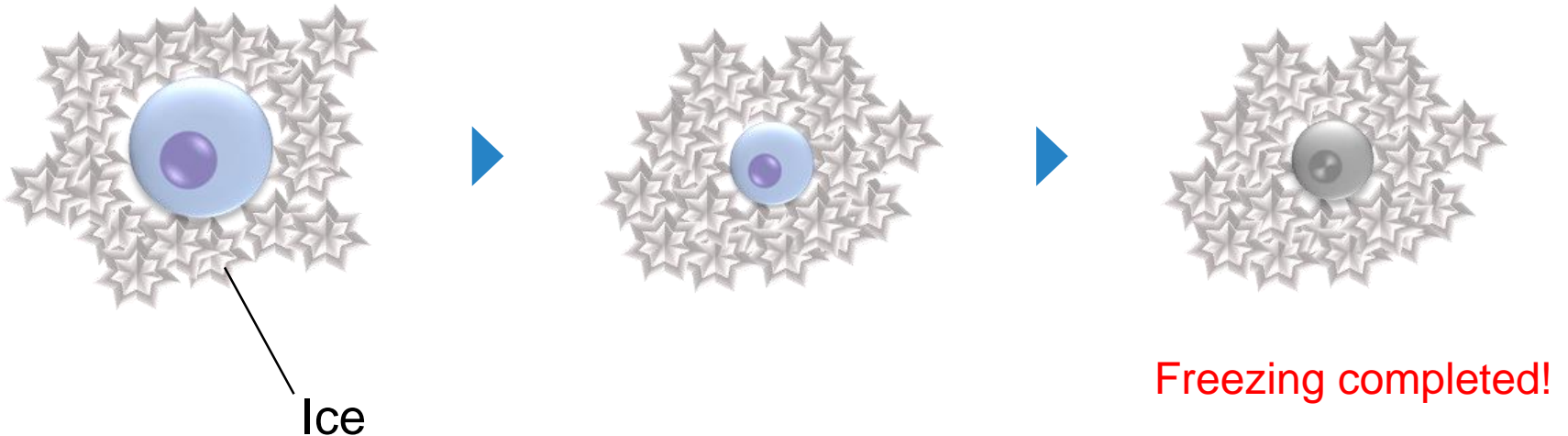
- Temperature : 37°C



Water bath

Mechanism

1. Extracellular water is frozen.
2. Water in a cell is transported by osmotic pressure.
3. Depression of freezing point inside a cell occurs.
4. The solute in a cell is frozen at the eutectic point.

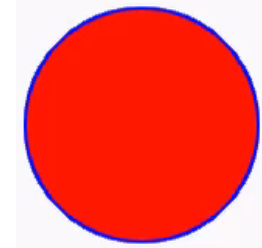
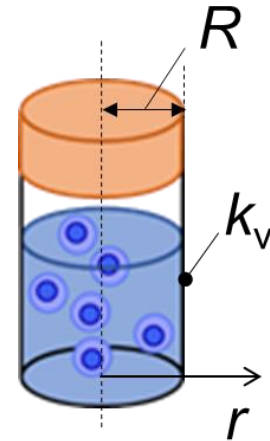


Heat transfer

$$\frac{\partial T(r, t)}{\partial t} = \alpha \left(\frac{\partial^2 T(r, t)}{\partial r^2} + \frac{1}{r} \frac{\partial T(r, t)}{\partial r} \right)$$

$$\frac{d\delta}{dt} = \frac{1}{\rho_s H_f} \left[k_s \left(\frac{\partial T}{\partial r} \right)_{\delta} - k_l \left(\frac{\partial T}{\partial r} \right)_{\delta+d\delta} \right]$$

δ : Thickness of ice [m]
 H_f : Heat of fusion of ice [kJ kg⁻¹]



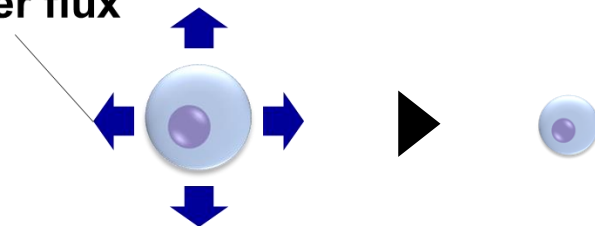
Mass transfer

$$\frac{dV_w}{dt} = A L_p \Delta P$$

$$L_p = L_{p0} \exp \left[-\frac{E}{R} \left(\frac{1}{T} - \frac{1}{T_0} \right) \right]$$

L_p : Membrane permeability [m s⁻¹ Pa⁻¹]
 ΔP : Osmotic pressure difference [Pa]

Water flux

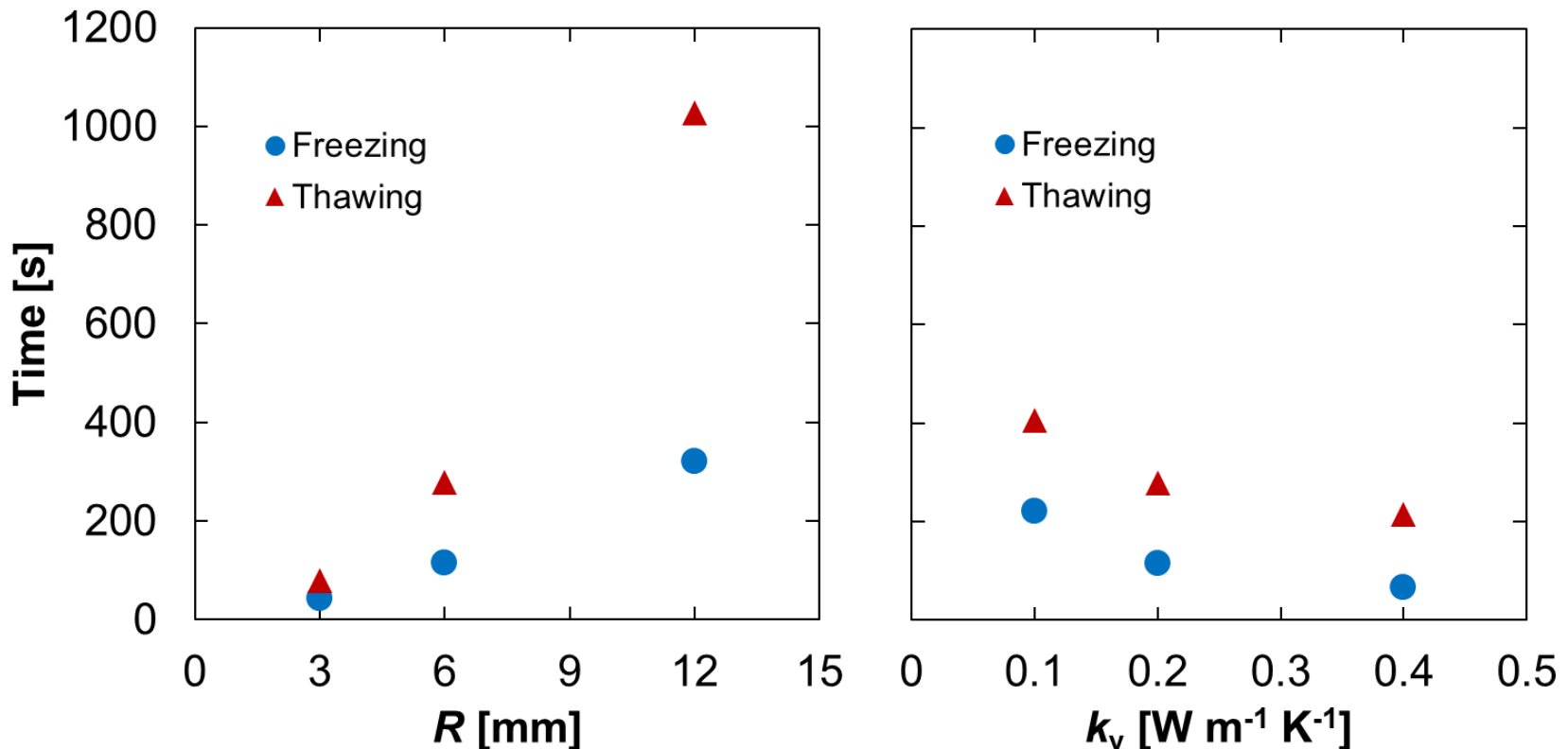
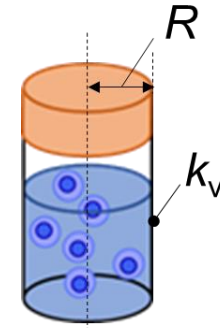


Heat transfer simulation

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- **Assumptions**

- Freezer heat transfer : Natural convection
- Freezer temperature : 193 K (Constant)
- Initial vial temperature : 300 K
- Content of the vial : Water

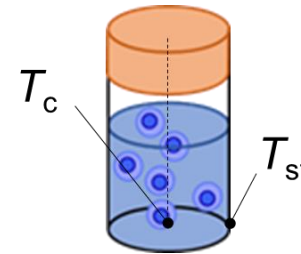


► R and k_v are important design parameters.

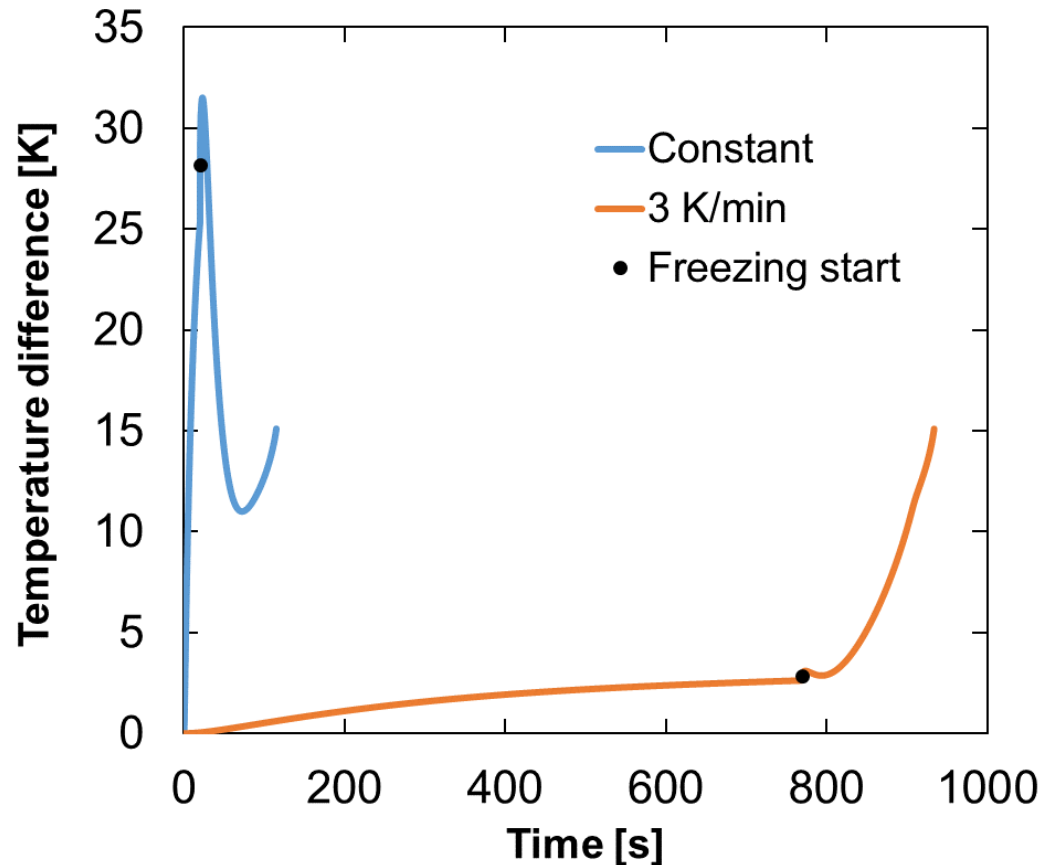
Heat transfer simulation

- **Freezer temperature**

- Constant (193 K)
- -3 K/min (From 300 K)



$$\Delta T = |T_c - T_{sf}|$$

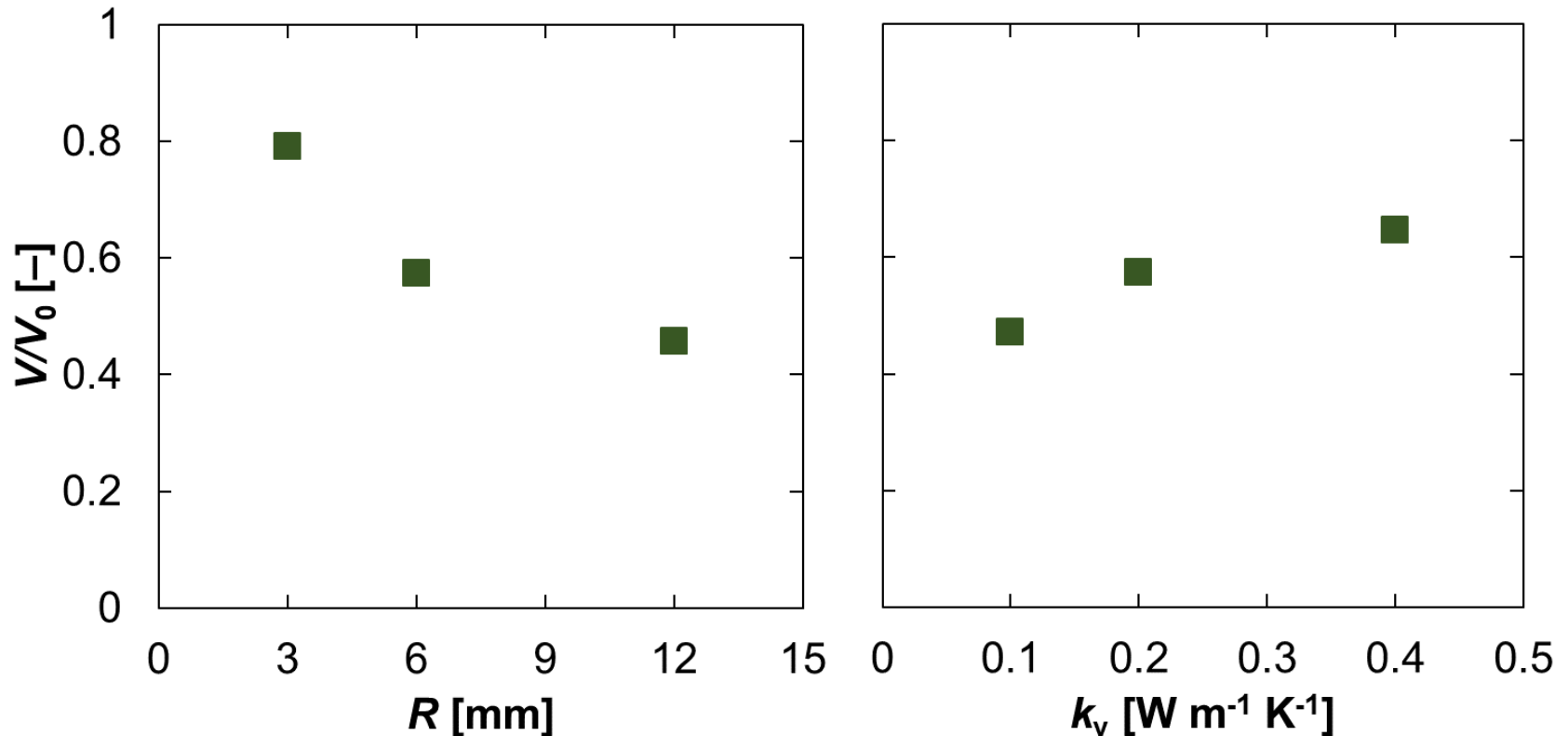
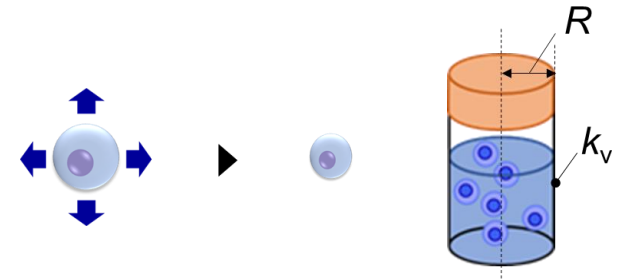


► Freezing procedure is also an important factor.

Mass transfer simulation

Assumptions

- Cryoprotective agent : 10%DMSO
- Initial cell volume V_0 : $2.50 \times 10^{-15} \text{ [m}^3\text{]}$
- Cell surface area A : $8.87 \times 10^{-10} \text{ [m}^2\text{]}$
- Permeable substance : Water



► R and k_v are important design parameters.

- **Experiment**
 - Survival rate after thawing
 - Cell membrane permeability
 - Effect of cryoprotective agent
- **Modeling & simulation**
 - Cell damage by osmotic pressure
 - Intracellular ice formation
- **Evaluation**
 - Survival rate
 - Manufacturing cost