

# AIF Induced Limits of Parameter Uncertainty in Pharmacokinetic Models of Pre-Clinical DCE-MRI

Tammo Rukat<sup>1,2</sup>, Simon Walker-Samuel<sup>3</sup>, Stefan A. Reinsberg<sup>1</sup>

<sup>1</sup>University of British Columbia; <sup>2</sup>Humboldt Universität zu Berlin; <sup>3</sup>University College London



## Motivation – How fast an AIF do I need?

- ▶ The **arterial input function** (AIF) of contrast agent (CA) concentration in the blood plasma is crucial for the application of pharmacokinetic (PK) models in dynamic contrast-enhanced magnetic resonance imaging (DCE-MRI).
- ▶ The functional form of the AIF itself is an inherent limitation to **parameter accuracy**.
- ▶ **Slow injection** → **wide AIF** → **low accuracy**

## Questions

1. How does the CA injection rate and subsequent AIF affect the precision of model parameters ( $K^{trans}$ )?
2. How do the simplifications within PK models affect this precision?

## Goal

- ▶ Derive an estimate for the variability of  $K^{trans}$  estimates as a function of injection rate and model imperfections:

$$\text{Variance} [\hat{K}^{trans}(\text{Injection Rate, Model})]$$

## Tracer Distribution Model (TDM)

Connection: **Injection Profile** → **AIF** is established by a phenomenological TDM:

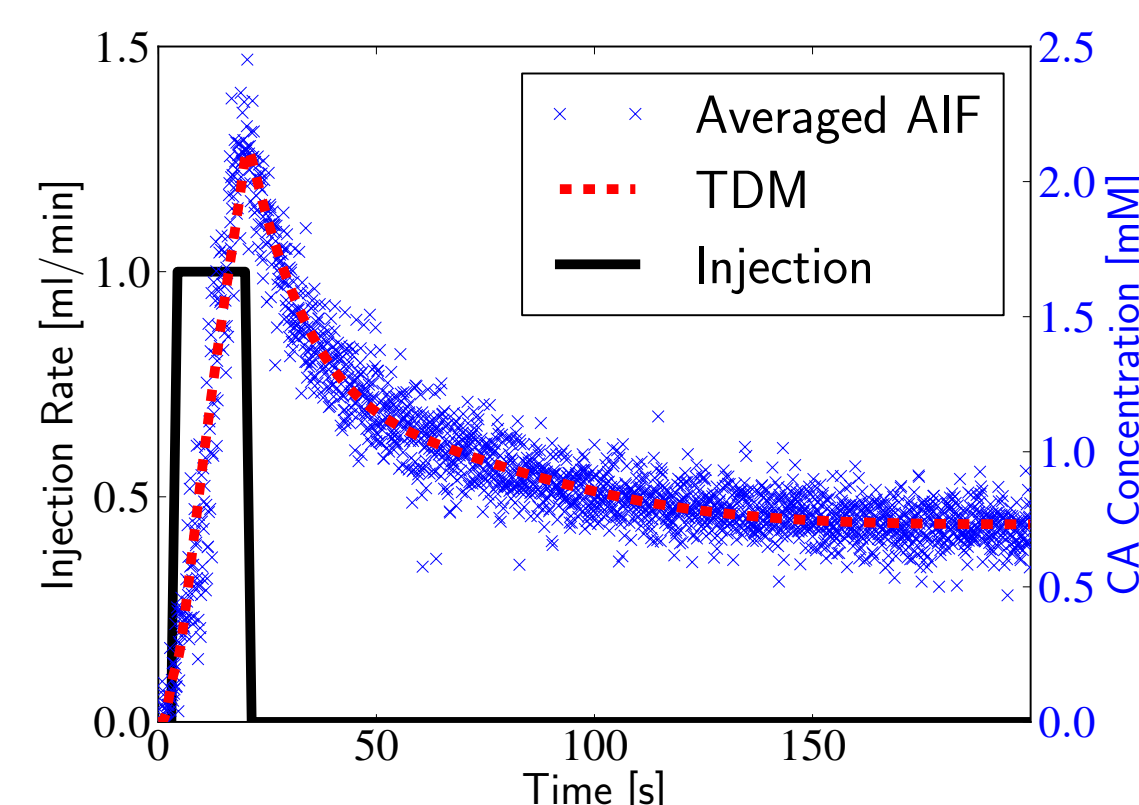
- ▶ Predicts AIFs by convolution of the injection input  $I(t)$  with the transfer function:

$$AIF(t) = H_{TDM}(t) * I(t),$$

- ▶ Third-order linear transfer function in the frequency domain:

$$\tilde{H}_{TDM}(\omega) = \frac{B_3\omega^3 + B_2\omega^2 + B_1\omega + B_0}{\omega^3 + A_2\omega^2 + A_1\omega + A_0}$$

- ▶ Parameters ( $A_i, B_i$ ) are determined by fitting simulated to measured population-averaged AIF. ( $[C]_{CA} = 60\text{mM}$ ,  $\Delta t = 100\text{ms}$ , 4 mice)

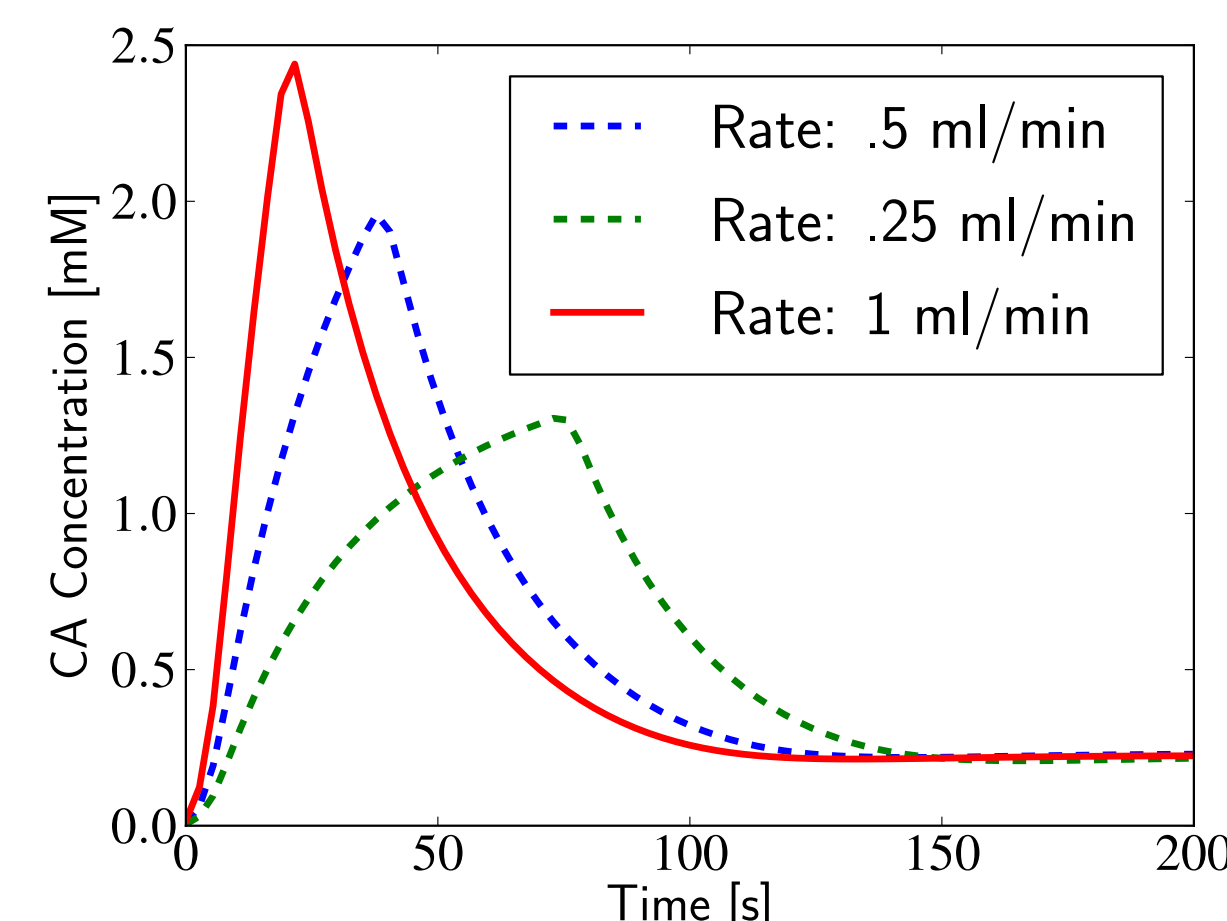


## Procedure – Resampling Bootstrap

1. Generate AIFs for different injection rates (TDM).
2. Generate tissue uptake curves  $C(t)$  for each AIF using MMID4 and ideal PK model predictions with fixed  $K^{trans}$ ,  $v_e$ .
3. Add Gaussian noise to  $C(t)$ .
4. Fit Tofts Model to the AIF and the noisy  $C(t)$ .
5. Iterate steps 3 and 4 for different realizations of Gaussian noise ( $10^5$  iterations) to derive a  $K^{trans}$  distribution.

## Simulating the Arterial Input

- ▶ AIFs are derived for a variety of experimentally relevant injection rates (TDM).
- ▶ Trapezoidal injection profiles are assumed.



## Tracer Uptake Models

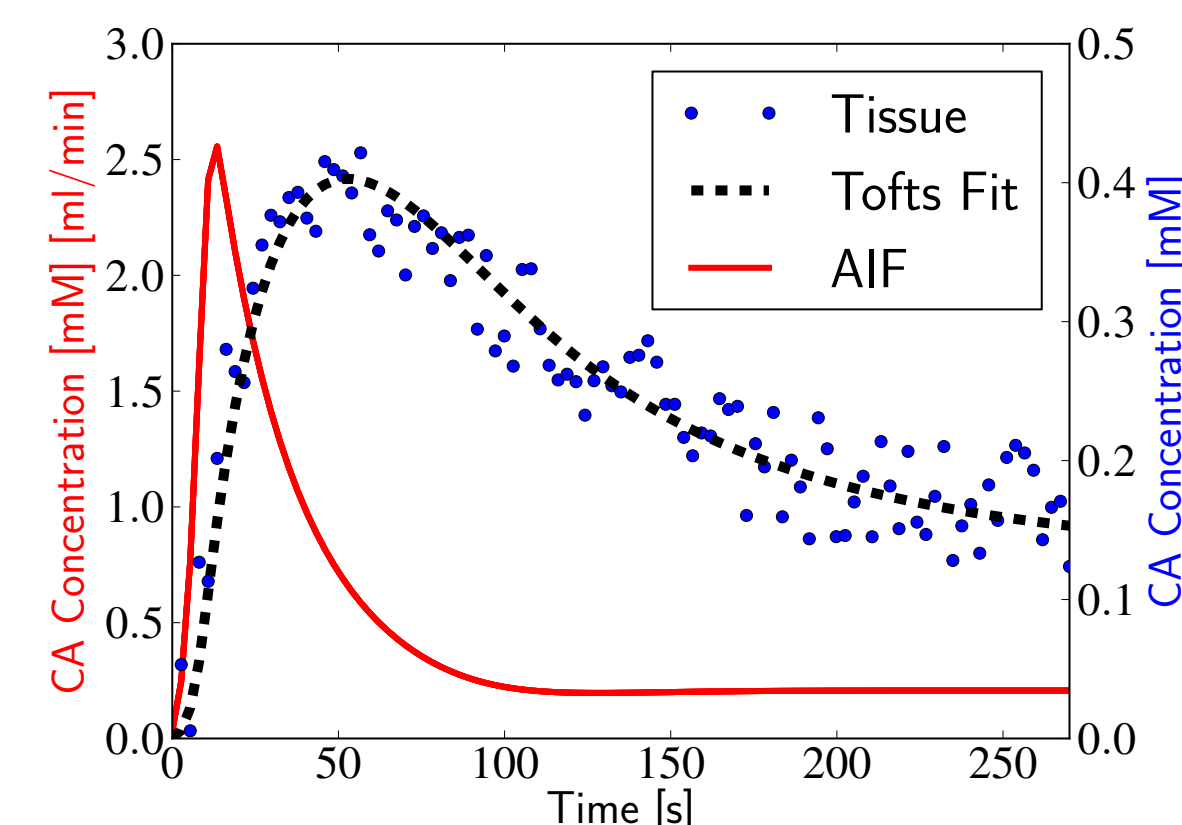
### MMID4

- ▶ Tissue exchange model with 20 flow paths
- ▶ Accounts for heterogeneity and flow dispersion

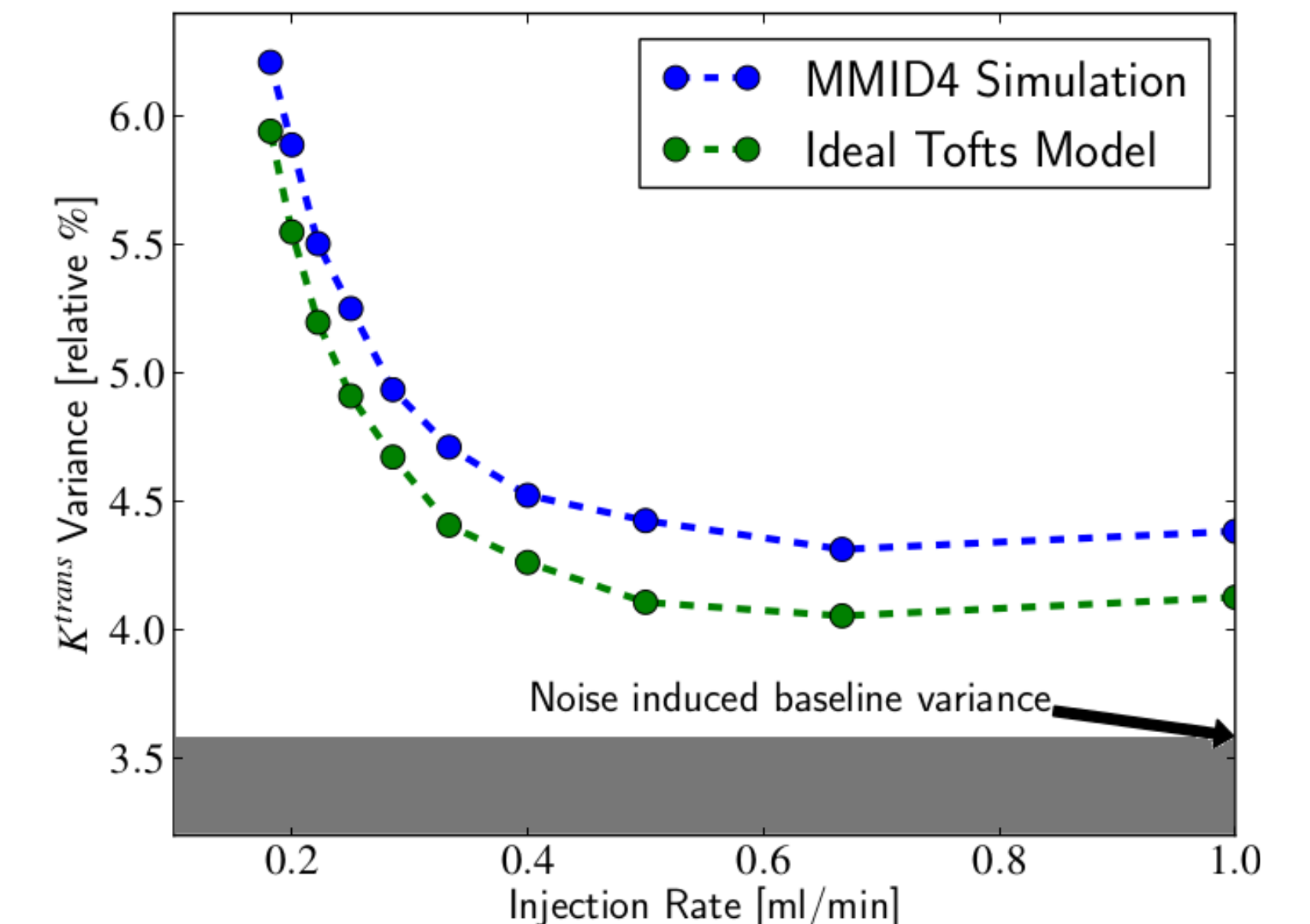
### Tofts Model

- ▶ Based on a rate equation for tracer diffusion

$$C_t(t) = K^{trans} \int_0^t dt' C_p(t') e^{-K^{trans} \cdot (t-t')/v_e}$$



## Results – Variance of Bootstrap $K^{trans}$ distributions



### 1. Effect CA Injection Rate

- ▶ Increase in  $K^{trans}$  variance induced by finite AIF widths for a typical noise level:  
15% (0.6 ml/min rate) up to 70% (0.2 ml/min rate)
- ▶ Injection faster than 0.6 ml/min do not improve precision.
- ▶ Slower injections do not bias observed  $K^{trans}$  distributions (data not shown).

### 2. Effect of Model Simplifications

- ▶ Imperfections of the Tofts Model induce a  $K^{trans}$  variance of less than 10%.

## Conclusion – Speed matters! - But within Limits

- ▶ Slow injections (wide AIFs) induce  $K^{trans}$  variances up to the same order of magnitude as typical measurement noise.
- ▶ The optimal  $K^{trans}$  precision is achieved for rates from 0.6 ml/min onwards.

## References

1. H. J. W. L. Aerts, N. a. W. van Riel, and W. H. Backes. System identification theory in pharmacokinetic modeling of dynamic contrast-enhanced MRI: influence of contrast injection. *Magnetic resonance in medicine : official journal of the Society of Magnetic Resonance in Medicine / Society of Magnetic Resonance in Medicine*, 59(5):1111–9, May 2008.
2. K. Kroll, N. Wilke, M. Jerosch-Herold, Y. Wang, Y. Zhang, R. Bache, and B. JB. Modeling regional myocardial flows from residue functions of an intravascular indicator. *American J Physiol*, 271:H1634–H1655, 1996.
3. P. S. Tofts and a. G. Kermode. Measurement of the blood-brain barrier permeability and leakage space using dynamic MR imaging. 1. Fundamental concepts. *Magnetic resonance in medicine : official journal of the Society of Magnetic Resonance in Medicine / Society of Magnetic Resonance in Medicine*, 17(2):357–67, Feb. 1991.