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POLYMER-LIPID NANOCOMPLEX FOR ENHANCED AQUEOUS SOLUBILISATION AND ABSORPTION OF HYDROPHOBIC ACTIVE COMPOUNDS

Abstract

The current invention relates to a polymer-lipid nanocomplex for enhanced aqueous solubilisation and absorption of hydrophobic active compounds, a process for producing such a nanocomplex, and to methods of use of such a nanocomplex.

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Background/Summary

CROSS-REFERENCE TO RELATED APPLICATIONS [0001] This application is a National Stage of International Application No. PCT/IB2020/054370 filed May 8, 2020, which claims priority to South Africa application No. 201902992, filed May 14, 2019, the disclosures of which are incorporated herein by reference in their entirety.

FIELD OF THE INVENTION

[0002] The current invention relates to a polymer-lipid nanocomplex for enhanced aqueous solubilisation and absorption of hydrophobic active compounds, a process for producing such a nanocomplex, and to methods of use of such a nanocomplex.

BACKGROUND OF THE INVENTION

[0003] It is estimated that more than 40% of new chemical entities (NCEs) approved by the FDA in the pharmaceutical industry and nearly 90% of the lead compounds coming in the developmental pipeline consist of water-poorly soluble active compounds. Poor water solubility or hydrophobicity is a prime compound property among the key physicochemical parameters that are used in the early screening process for best pharmaceutical candidates.

[0004] Drugs suffering from poor water solubility, present subsequently low permeability, rapid metabolism, high protein bound by plasma proteins for elimination from the body, a huge dose-to-solubility ratio, thus low bioavailability. The therapeutic levels are achieved with large quantities of the drug that may result in poor safety and tolerability, thus an emergence of drug resistance and undesirable side effects [1, 2].

[0005] The hydrophobicity of a compound is usually expressed by its ability to partition between an organic solvent (octanol) and water, also known as the partition coefficient (Log P). The positive value of Log P is ranked as hydrophobic compounds and highly hydrophobic as the values reached 10, translating in solubility below 10⁻⁴ as depicted in Table 1 suggested by the FDA [1]. This is a real challenge for the pharmaceutical industry because if the actives transit undissolved in the gastro-intestinal tract (GIT), they will not be able to reach the target site for their intended effects in the body; hence they will remain useless compounds. Furthermore, hydrophobic drugs often require an intake of fat-rich food to facilitate their absorption, leading to erratic absorption with large variability in the inter-and-inpatient dose response.

TABLE-US-00001 TABLE 1 USP solubility description Parts of solvent required Descriptive term
for 1 part of solute Very soluble <1 Freely soluble From 1 to 10 Soluble From 10 to 30 Sparingly
soluble From 30 to 100 Slightly soluble From 100 to 1000 Very slightly soluble From 1000 to
10,000 Practically insoluble or insoluble 10,000 and over

[0006] Another aspect to always consider during drug development is the categorization of drugs as given by the Biopharmaceutical Classification system (BCS) in Table 2 [3]. This system assists in the prediction of the drug behavior using concomitantly the three parameters of drug including the solubility, dissolution and intestinal permeability. These are important parameters that will assist reaching preferred levels of drug in the systemic circulation following an oral administration for desired pharmacological response. The BCS is therefore an effective tool that is extensively used in drug development processes [3].

TABLE-US-00002 TABLE 2 Biopharmaceutical drugs classification system Class Solubility

Permeability I High High II Low High III High Low IV Low Low

[0007] All these types of drugs pose inherent challenges, and Class IV is usually considered to be outside of the so-called “drugable space”, but if proven to be efficacious, it can be formulated to overcome its dual challenges of low solubility and low permeability.

[0008] Several strategies have been used in the pharmaceutical industry to enhance drug solubility. They include: physical modifications (e.g., size reduction), chemical modifications (e.g., polymer-drug conjugation) and miscellaneous methods including supercritical fluid micronisation. Vimalson et al [1] has extensively reviewed the various techniques to achieve these modifications. It is worth mentioning that most of the physical modifications aimed at reducing the size, the crystallinity and altering the morphological habit of drug particles in order to increase the solubility.

[0009] This mechanism of improving drug solubility by physical means is well described by Noyes-Whitney equation [4] expressing the increase of the dissolution rate of the API following the reduction of the active pharmaceutical ingredient (API) particle size to submicron range, thus the shrinking of the effective boundary layer thickness. However, it is directly proportional to the particle surface area. Emulsions-based strategies are equally extensively used in the pharmaceutical industry in order to increase the drug solubility and dissolution rate. In this case, a nanoemulsion or microemulsion is used to encapsulate the hydrophobic drug, subsequently rendering it soluble in aqueous solutions. Depending on the power of solvency of the emulsions, only hydrophobic actives with a narrow range of Log P can be solubilised in these solutions.

[0010] There is therefore a need for a microemulsion system that is able to facilitate the solubilisation of a broad range of actives from highly refractory hydrophobic actives (i.e., Log P of 9) to lesser hydrophobic compounds (with a Log P below 3).

[0011] Furthermore, it is not sufficient to just increase the dissolution rate in the GIT of orally administered actives in order to increase their bioavailability in the systemic circulation. Strategies aimed at improving their permeability through the epithelial linings of the intestine and ensuring a prolonged residence time in the blood to achieve high levels of drugs are equally needed.

SUMMARY OF THE INVENTION

[0012] According to a first aspect of the invention, there is provided a polymer-lipid nanocomplex comprising: [0013] i. an inner microemulsion matrix comprised of at least one hydrophobic active compound, at least one fatty acid dissolved in a polar aprotic solvent, and a surfactant; and [0014] ii. an outer shell comprising one or more hydrophilic polymers.

[0015] The outer shell may, in particular, comprise an aqueous solution of an aqueous mixture of hydrophilic polymers such as polyvinyl alcohol (PVA) and polyethylene glycol (PEG), for example, PEG 4000.

[0016] The inner microemulsion matrix may further comprise at least one organic carboxylic acid. The at least one organic carboxylic acid may be a weak acid, including those approved for human consumption comprising acetic acid, lactic acid, citric acid, or phosphoric acid, preferably acetic acid.

[0017] Additionally, the inner microemulsion matrix may comprise at least one copolymer, poly(lactic-co-glycolic acid) or PLGA, or alternatively, any biocompatible and biodegradable polymer suitable for use in drug delivery, including polylactic acid, polyglycolic acid, or poly ϵ -caprolactone.

[0018] Preferably the at least one fatty acid comprises or consists of any one or more of stearic acid, palmitic acid and lauric acid, preferably stearic acid.

[0019] The polar aprotic solvent may comprise of either ethanol or acetone, or may be a blend of ethanol and acetone. Preferably the polar aprotic solvent is acetone.

[0020] The surfactant may comprise any surfactant having a Hydrophile-Lipophile Balance (HLB) value of greater than 10. Preferably, the surfactant is polysorbate 80, also known as Tween 80®.

[0021] According to a further aspect of the invention, there is provided a process for producing a polymer-lipid nanocomplex comprising at least one hydrophobic active compound comprising the

steps of: [0022] I. mixing at least one hydrophobic active compound, a fatty acid dissolved in a polar aprotic solvent, and a surfactant to form an organic phase; [0023] II. optionally heating the organic phase; [0024] III. dispensing the organic phase into an aqueous mixture comprising at least one hydrophilic polymer to form a microemulsion; and [0025] IV. stabilising the microemulsion in a phosphate buffer at about 0° C. to form a nanoprecipitate of the polymer-lipid nanocomplex. [0026] The process may further comprise a final step of drying the nanoprecipitate to produce a free flowing polymer-lipid nanocomplex powder either by freeze drying or by spray drying. [0027] The process may further comprise mixing an organic carboxylic acid with the organic phase. [0028] The process may further comprise dissolving at least one biocompatible and biodegradable polymer or copolymer suitable for use in drug delivery, poly(lactic-co-glycolic acid) or PLGA, or polylactic acid, polyglycolic acid, or poly ε-caprolactone, into the polar aprotic solvent with the fatty acid for mixing with the at least one hydrophobic active compound and the surfactant to form the organic phase. [0029] The at least one fatty acid may comprise any one or more of stearic acid, palmitic acid and lauric acid, preferably stearic acid. [0030] The polar aprotic solvent may comprise either ethanol or acetone, or may be a blend of ethanol and acetone. Preferably the polar aprotic solvent is acetone. [0031] The organic carboxylic acid may comprise at least one weak acid. For example, the weak acid may include any one or more of those approved for human consumption comprising acetic acid, lactic acid, citric acid, or phosphoric acid. Preferably the weak acid is acetic acid. [0032] The surfactant may comprise any surfactant having a Hydrophile-Lipophile Balance (HLB) value of greater than 10. Preferably, the surfactant is polysorbate 80, also known as Tween 80®. [0033] In particular, the process may comprise: [0034] a) dissolving at least one fatty acid in a polar aprotic solvent to form a fatty acid solution; [0035] b) dissolving at least one hydrophobic active compound in the fatty acid solution; [0036] c) adding drop-wise, a surfactant to form an organic phase; [0037] d) optionally heating the organic phase; [0038] e) dispensing the organic phase into an aqueous mixture comprising at least one hydrophilic polymer while stirring to form a microemulsion; and [0039] f) nanoprecipitating the microemulsion by adding a phosphate buffer at 0° C. while stirring to form the polymer-lipid nanocomplex. [0040] The process may further comprise an additional step of drying the nanoprecipitate to produce a free flowing polymer-lipid nanocomplex powder either by freeze drying or by spray drying. [0041] The process may further comprise, at step a), dissolving PLGA, or alternatively, any biocompatible and biodegradable polymer suitable for use in drug delivery, including polylactic acid, polyglycolic acid, or poly ε-caprolactone, into the polar aprotic solvent with the fatty acid. [0042] The process may further comprise, at step c), adding drop-wise, an organic carboxylic acid with the surfactant. [0043] The process may further comprise in step e) heating while stirring to form the microemulsion. The heating steps may be performed at from between about 40° C. to 50° C., preferably 40° C. [0044] The phosphate buffer may comprise a pH of from about 7.2 to about 7.6, more preferably, about 7.4 at 0° C. [0045] The nanoprecipitation of the microemulsion may be performed by adding the microemulsion to the phosphate buffer solution at a ratio about 1:1. It is to be appreciated that a variety of factors influence the optimum ratio of microemulsion to buffer, including drug loading, stability of the formulation, including during the drying process, and the like. [0046] The freeze drying may be performed following an initial snap-freezing step in liquid nitrogen. [0047] The spray drying may be performed using a spray dryer such as the Top bench Buchi-B290.

In particular, such spray drying may be performed with the following set of parameters; [0048] Inlet temperature: about 90 to 110° C. [0049] Outlet temperature: about 60° C. [0050] Feeding rate: 2% (mL/min).Math. [0051] Atomizing pressure: 6-7 bar [0052] Aspiration vacuum set at 100%. [0053] It is to be appreciated that the inlet temperature should be high enough to evaporate both the polar (water) and nonpolar (organic) solvents without degrading any compounds in the formulation, and that the range provided is one embodiment of the invention and may be modified by those skilled in the art.

[0054] It is further to be appreciated that outlet temperature is affected by the room temperature of the lab in which the apparatus is situated and, apart from requiring that the outlet temperature is above 60° C. in order to obtain a dry, free flowing powder, the specific temperature may vary. The outlet temperature is equally governed by the liquid feeding rate, the inlet temperature and thermal exchange efficiency between droplets and the drying hot air.

[0055] The dried polymer-lipid nanocomplex size may range from between about 150 to 500 nm.

[0056] The liquid polymer-lipid nanocomplex size may range from between about 70 nm to 150 nm.

[0057] The dried polymer-lipid nanocomplex may comprise a polydispersity index (PDI) of 0.3 or less.

[0058] According to a further aspect of the invention, there is provided a method for enhancing aqueous solubilisation and absorption of at least one hydrophobic active compound comprising formulating the at least one hydrophobic active compound using the process of the invention.

[0059] The at least one hydrophobic active compound may comprise any hydrophobic active compound positioned on the Log P positive scale (Log P 2 to Log P 9) of the partition coefficient scale. For example, the at least one hydrophobic active compound may comprise any one or more of antituberculosis drugs, antimalarials, and phytochemicals with antifungal, antiviral, antianxiety, antiobesity, antidepressant and/or analgesic properties.

[0060] In particular, the at least one hydrophobic active compound may comprise an antimalarial agent, and more specifically Lumefantrine.

[0061] Further in particular, the at least one hydrophobic active compound may comprise a phytochemical, and more specifically Cannabidiol (CBD).

[0062] Further in particular, the at least one hydrophobic active compound may comprise an anti-Tuberculosis drug, and more specifically Rifampicin.

[0063] For example, the at least one hydrophobic active compound formulated according to the invention may be for administration through various routes including topical, sub-cutaneous, intravenous, intramuscular, inhalable, nasal, sub-lingual, buccal, rectal, or ophthalmic.

[0064] According to a further embodiment of the invention, there is provided at least one hydrophobic active compound formulated as a polymer-lipid nanocomplex of the invention.

[0065] According to a further embodiment of the invention, there is provided at least one hydrophobic active compound formulated as a polymer-lipid nanocomplex of the invention for use in a method of treatment or prophylaxis of a subject.

[0066] According to a further embodiment of the invention, there is provided a method of treatment or prophylaxis of a subject by administration of at least one hydrophobic active compound formulated as a polymer-lipid nanocomplex of the invention.

[0067] The administration may be through various routes including topical, sub-cutaneous, intravenous, intramuscular, nasal, sub-lingual, inhalable, buccal, rectal or ophthalmic.

Description

BRIEF DESCRIPTION OF THE DRAWINGS

[0068] FIG. 1 shows a size distribution and the PDI of the LUM microemulsion;

[0069] FIG. 2 shows a DSC Thermal graph for the nanocomplexed LUM as compared to free drug;
[0070] FIG. 3 shows a graph of the direct comparison for delivery of LUM compared to nanocomplexed LUM, dosed orally at an equivalent 20 mpk of LUM in male Balb/c mice;
[0071] FIG. 4 shows a graph of the in vivo efficacy results of nanocomplexed LUM in a malaria-infected NSG mice model; and
[0072] FIG. 5 shows a graph of the in vivo dose-response relationship of LUM-loaded nanocomplexes.
[0073] FIG. 6 shows a size distribution and the PDI of the CBD microemulsion;
[0074] FIG. 7 shows a size distribution and the PDI of the CBD powder;
[0075] FIG. 8 shows a size distribution, PDI, zeta potential, yield and the drug loading of the RIF powder;
[0076] FIG. 9 shows the morphology (SEM) of the RIF powder; and
[0077] FIG. 10 shows a graph of the in vitro releaser profile of RIF-loaded nanocomplexes.

DETAILED DESCRIPTION OF THE INVENTION

[0078] The present invention relates to a polymer-lipid nanocomplex comprising an inner microemulsion matrix including at least one hydrophobic active compound and an outer shell comprising a polymer for enhanced aqueous solubilisation and absorption of the hydrophobic active compound, a process for producing such a nanocomplex, and to methods of use of such a nanocomplex.

[0079] Although the applicant has shown that several hydrophobic active compounds having different Log P values, including antituberculosis drugs, antimalarials, and phytochemicals with antifungal, antiviral, antianxiety, antiobesity, antidepressant and/or analgesic properties are able to be successfully incorporated in this polymer-lipid nanocomplex, the invention will be described in terms of three exemplary examples; an antimalarial drug, Lumefantrine, a phytochemical, Cannabidiol and an anti-Tuberculosis (TB) drug, Rifampicin.

[0080] This is a simple, easy-to-scale up process that would merely require conventional pharmaceutical equipment for production on a commercial scale.

[0081] The exemplary examples below are for illustrative purposes and should in no way be construed as limiting in any way the scope of the invention.

Example One

Lumefantrine (Log P 9)—Antimalarial Drug

1. Background

[0082] Lumefantrine is a water insoluble (Log P of 9) racemic mixture of synthetic fluorene derivatives with the chemical structure as shown in Formula 1.

##STR00001##

[0083] Lumefantrine is used for the treatment of acute uncomplicated malaria caused by a protozoan parasite, *Plasmodium falciparum* (*P. falciparum*). It is administered in combination with an artemisinin methyl ether derivative, artemether, to potentiate efficacy. Lumefantrine is a blood schizonticide active against the erythrocyte stage of uncomplicated *P. falciparum* infections and has a half-life ($T_{1/2}$) of 4-5 days. Although efficacious, it possesses some limitations that hinder maximum efficacy. It has low and slow absorption into the circulatory system which leads to relatively low bioavailability, extensively metabolized in the liver and due to its high lipophilicity; it is highly protein bound (99.7%) upon entry into the blood. These limitations therefore result in a longer period of time (T_{max}) for Lumefantrine to reach peak concentrations; it takes about 6 hours for orally administered Lumefantrine to reach the highest concentration (C_{max}) of 7 $\mu\text{g/mL}$ in the blood.

[0084] As indicated above, Lumefantrine has delayed absorption, which negatively impacts its bioavailability. Its insolubility in polar media (0.002% w/v) results in it being highly metabolised by enzymes of the liver and it is significantly bound by plasma proteins upon crossing the intestinal tract into the blood.

2. Methods and Materials

[0085] 200-300 mg Lumefantrine (LUM) was dissolved in a solution of stearic acid dissolved in a polar aprotic solvent, acetone, to which about 50-100 μL of an organic carboxylic acid, acetic acid, and about 50-100 μL of a surfactant with high Hydrophile-Lipophile Balance (HLB) value, polysorbate 80 or Tween 80®, were added to speed up the dissolution of LUM resulting into the oil phase (internal) of the emulsion.

[0086] The organic phase of LUM was first heated up to 40° C., then rapidly dispensed into an aqueous solution of an aqueous mixture of hydrophilic polymers, polyvinyl alcohol (PVA) and polyethylene glycol (i.e., PEG 4000), while moderately stirring on a magnetic hot plate.

[0087] The microemulsion obtained has a very narrow size distribution as shown in FIG. 1. The emulsion is further stabilized by immediately transferring the emulsion into a high volume (volume ratio 1:1) of an icy phosphate buffer solution (pH 7.4) at 0° C. while stirring. The resulting suspo-emulsion was subsequently dried to produce a free flowing powder either by freeze drying following a snap freezing step in liquid nitrogen or by spray drying using a Top bench Buchi-B290 spray dryer with the following set of parameters: [0088] Inlet temperature: 100° C. [0089] Outlet temperature: 60° C. [0090] Feeding rate: 2% (mL/min).Math. [0091] Atomizing pressure: 6-7 bar [0092] Aspiration vacuum set at 100%.

3. Results

[0093] The process resulted in the production of a free flowing powder of encapsulated LUM having a payload efficiency of circa 25% w/w, and 90% of nanoparticle sizes ranging from 200 to 300 nm, with a polydispersity index (PDI) of 0.3 and below.

[0094] The nanocomplexes produced by the process were readily re-dispersed in water at a concentration of 25 mg/mL without any visible sign of precipitation and the nanosuspension was still stable.

[0095] Results showed significantly higher amounts of suspended drug in water as compared to the drug's inherent water solubility of just 0.002% w/v, thus translating in more than 10 000-fold improvement that was achieved.

[0096] Due to its ability to form a clear solution when re-dispersed in aqueous media, the LUM-loaded nanocomplexes can be administered via a number of routes, including orally or intravenously.

[0097] The thermal analysis (differential scanning calorimetry or DSC) of the free-flowing powder showed a disappearance of the melting point peak of LUM that could be interpreted as a conversion from its crystalline morphology to amorphous structure (see FIG. 2). This is beneficial as it indicates a rapid dissolution rate of the drug.

Pharmacokinetic and Pharmacodynamic Evaluation of Nanoformulated LUM (PN35)

[0098] LUM was reformulated into the lipid-polymer nanocomplex for delivery with the aim of improving its bioavailability and enhancing its therapeutic efficacy in vivo.

[0099] This experiment demonstrated pharmacokinetic parameters (i.e., C_{max}) 10-fold greater than the control of un-formulated LUM, with a distinctive prolonged tailing curve above the minimum inhibitory concentration (MIC) for several hours. It shows a fast absorption of LUM following oral administration depicted by a short T_{max}.

[0100] Enhanced absorption was observed in animal studies a few minutes after oral administration of the nanocomplexed LUM resuspended in water. The highest plasma concentrations ever reported of 11.5 mg/mL were obtained in less than 1 hour, thus minimizing the lag-time for LUM absorption. Furthermore, the reported effective dose (ED₉₀) of LUM to clear 90% of parasitaemia in the blood was significantly reduced from 12.01 mg/kg to 5.01 mg/kg (see FIGS. 3, 4 and 5).

Example Two

Cannabidiol (Log P 6)—Phytochemical Analgesic Drug

1. Background

[0101] Cannabidiol (CBD) is a naturally occurring chemical compound or phytochemical that is

found in *cannabis* plants. It is one of the **113** cannabinoid compound extracts from *cannabis* plants, and it is the major phytocannabinoid compound which makes up 40% of the total plant extracts. It belongs to the cannabinoid drug class and can be administered through inhalation with bioavailabilities ranging from 11-45% and orally with only 13-19% bioavailability. The extract (Formula 2) can be administered in a solution form for oral administration or as an additive in food preparation. It has major medicinal benefits to humans including pain and inflammation relief, anxiety management, seizure control and also has antioxidant properties.

##STR00002##

[0102] Although CBD is derived from the *cannabis* plant, which is well known for its psychotropic effects when used recreationally, CBD does not induce psychotropic effects like its co-synthesized *cannabis* extract, Tetrahydrocannabinol (THC) which is the principal psychoactive constituent in the plant. It has also been hypothesized that it may act as antagonist for THC since they bind to the same receptors found in the central and peripheral nervous system of the human body.

[0103] CBD research studies across the world have shown many significant health benefits including pain relief capabilities and reversed inflammatory effects. In addition, combination of CBD with THC in several human studies has shown effective treatment for pain in multiple sclerosis and arthritis. In recent studies with cancer patients, elevated reduction of cancer-related symptoms were also observed. Improvement of heart health through its anti-oxidative properties, antitumor effects, reduction of acne prevalence, antipsychotic effects and has good neuroprotective properties. Treatment with CBD in some studies has suggested the prevention of diabetes and also has high reduction of anxiety and depression. It has also been used to treat patients with substance (drugs etc.) abuse. Although the extract has proven to be beneficial in treating numerous ailments, it also induces a few undesirable immune responses. Side effects include nausea, vomiting, drowsiness, dizziness, and diarrhea, changes in appetite, anxiety, depression and psychosis. The exact mechanism for its beneficial health effects is not clear, but cannabidiol seems to prevent the breakdown of a chemical in the brain that affects pain, mood, and mental function. Preventing the breakdown of this chemical and increasing its levels in the blood seems to reduce psychotic symptoms associated with conditions such as schizophrenia.

[0104] The extract is a water insoluble (0.0126 mg/mL), colourless crystalline powder and it is soluble in a various organic solvents. CBD is known to be non-psychoactive, although, it is highly insoluble in water thus impeding absorption and is also subjected to significant first-pass metabolism. Both these properties have major limitations to treatment outcomes and also contribute to its low bioavailability when orally administrated.

2. Methods and Materials

Liquid Formulation

[0105] The CBD (10 to 20 mg) was dissolved in stearic acid and a co-solution of acetone/ethanol, and then 10 to 20 ul of a surfactant with a high HLB value above 10 (Tween 80®) was added to assist in the formation of the oil phase droplets. It is also possible to optionally dissolve PLGA, or alternatively, any biocompatible and biodegradable polymer suitable for use in drug delivery, including polylactic acid, polyglycolic acid, or poly ϵ -caprolactone, in the stearic acid and acetone/ethanol co-solution to further improve stability of the hydrophobic active in the inner matrix of the microemulsion.

[0106] To form the liquid microemulsion, the organic phase was rapidly dispensed into an aqueous solution of an aqueous mixture of hydrophilic polymers, polyvinyl alcohol (PVA) and polyethylene glycol (i.e., PEG 4000). The organic phase may optionally first be heated to about 40° C., then, when dispensed into the aqueous mixture of hydrophilic polymers, may be moderately stirred using a magnetic hot plate at about 40° C., resulting in a stable microemulsion with reproducible droplet size and size distribution.

Powder Formulation

[0107] 200-300 mg of CBD was dissolved in a solution of stearic acid dissolved in a polar aprotic

solvent, acetone, to which 50-100 μL of an organic carboxylic acid, acetic acid, and 10-20 μL of a surfactant with Hydrophile-Lipophile Balance (HLB) value greater than 10, polysorbate 80 or Tween 80®, were added, resulting into the oil phase (internal) of the emulsion.

[0108] The dissolved CBD oil phase was then rapidly dispensed into an aqueous solution of an aqueous mixture of hydrophilic polymers, polyvinyl alcohol (PVA) and polyethylene glycol (i.e., PEG 4000), while moderately stirring. The dissolved CBD oil phase may optionally be heated to about 40° C. before adding the aqueous mixture of hydrophilic polymers, and the moderate stirring may be performed at about 40° C. on a magnetic hot plate.

[0109] The CBD emulsion was further stabilized through incorporation of a high volume (volume ratio 1:1) of an icy phosphate buffer solution (PBS) pH 7.4 at 0° C. while stirring.

[0110] The stabilized emulsion was subsequently dried to produce a free flowing powder either by freeze drying following a snap freezing step in liquid nitrogen or by spray drying using a Top bench Buchi-B290 spray dryer under the following conditions: [0111] Inlet temperature: 100° C. [0112] Outlet temperature: 60° C. [0113] Feeding rate: with the pump knob set at 2 [0114] Atomizing pressure: 6-7 bar [0115] Aspiration vacuum set at 100%.

3. Results

Liquid Formulation

[0116] A water based microemulsion system (>95% water) incorporating CBD was successfully developed using an oil-in-water single emulsion nanoprecipitation technique. The emulsion incorporated 2 mg of CBD in every 1 mL of water (more than 50× improvement) with homogeneous size distributions and oil droplet sizes ranging from 70 nm to 150 nm (FIG. 6) depending on the CBD concentrations and solvent to water ratios. All the formulations incorporating CBD from low to high concentrations have been stable for over 6 months and all retain their initial sizes and size distributions with less than 2% (± 3 nm) of size variations.

Powder Formulation

[0117] The CBD powder is water soluble with size distributions ranging from 200 nm to 460 nm (FIG. 7). The stability of the CBD powder was investigated at room temperature and during refrigeration at between about 4-8° C. and was found to be stable over six months.

Example Three

Rifampicin (Log P 3.85)—Anti-Tuberculosis Drug

1. Background

[0118] Today, almost one-third of the world population is infected with latent Tuberculosis (TB), resulting in the death of two million people every year. TB is caused by a *bacillus* bacterium, *Mycobacterium tuberculosis* (M.TB) and it usually attacks the lungs, but other body systems can also get affected including the central nervous system, the lymphatic system, bones and skin. TB is an airborne disease that usually spread through the air from infected people by cough, sneeze or spit. Infection occurs upon inhalation of the bacterium which is engulfed by alveolar macrophages and throughout the disease progression, the bacterium remains primarily within the macrophages. Here, the bacterium is able to remain in a latent state or multiply and disseminate to other sites and/or be transmitted to other individuals. Current treatment is strenuous, requiring patients to take high drug doses of a combination therapy (Isoniazid, Rifampicin, Pyrazinamide and Ethambutol) per day over a long period of time extending up to at least 18 months often with severe drug related side effect manifestations. As a result, patient compliance to the treatment regimen is low and this has significantly contributed to the emergence of drug resistant M.TB strains. Multidrug resistant-TB (MDR-TB) strains are defined as strains resistant to the frontline drugs, Isoniazid and Rifampicin.

##STR00003##

[0119] In 2008-2009, the highest ever number of MDR-TB cases were reported to WHO, about half a million new MDR-TB cases emerging annually. Drug-resistant TB has a higher mortality rate, and is significantly more difficult and costly to treat than drug-susceptible TB. In South

Africa, the recommended MDR-TB treatment regimen consists of a 6-month intensive phase (requiring hospitalization for the entire intensive phase), with daily administration of one injectable drug, i.e., kanamycin, together with at least four pills (Ethionamide, Ofloxacin, Terizidone or Cycloserine), followed by an 18-month continuation phase of daily intake of the four pills. These drugs exhibit significant toxicity, e.g., kanamycin is associated with severe dose dependent auditory and renal damage. Most patients complete treatment with permanent hearing loss. Moreover, failure to adhere to the treatment may lead to a development of a more multi-drug resistant strain, extremely-drug resistant (XDR-TB). This strain is even more difficult to treat with the currently available antibiotics. XDR-TB treatment consists of Capreomycin injection and orally administered Ethionamide, Para-amino Salicylic acid, Moxifloxacin, Terizidone, Pyrazinamide and Clofazimine. The length of the intensive phase is guided by culture conversion but is recommended to be at least 6 months, and the continuation phase recommended being at least 18 months. Again these drugs exhibit severe side effects and combined with the nature of the treatment regimen make patient compliance difficult. Patients also face the prospect of development of further resistance beyond XDR-TB, dubbed Totally Drug Resistant-TB (TDR-TB) which is currently considered incurable. [0120] The project focuses on encapsulation of Rifampicin in biodegradable/biocompatible polymers and lipids. This will improve absorption, protect the drug from the first pass metabolism and subsequently improve the drug bioavailability with an extended plasma half-life.

2. Methods and Materials

[0121] 200-300 mg Rifampicin (RIF) was dissolved in a solution of stearic acid dissolved in a polar aprotic solvent, acetone. Optionally, PLGA, or alternatively, any biocompatible and biodegradable polymer suitable for use in drug delivery, including polylactic acid, polyglycolic acid, or poly ϵ -caprolactone, may further be dissolved in the polar aprotic solvent to improve the stability of the hydrophobic RIF in the inner matrix of the microemulsion. About 10-20 μ L droplets of a surfactant with a Hydrophile-Lipophile Balance (HLB) value of greater than 10, Tween 80®, were added to speed up the dissolution of RIF resulting into the oil phase (internal) of the emulsion. The dissolved RIF was then added to a pool of excipients composed of PVA and PEG to form the emulsion. The resulting emulsion was immediately transferred into a cold PBS (pH 7.4) buffer solution at 0° C. at a 1:1 ratio to further stabilise the emulsion. The latter was subsequently dried to produce a free flowing powder either by freeze drying following a snap freezing step in liquid nitrogen or by spray drying using a Top bench Buchi-B290 spray dryer with the following set of parameters: [0122] Inlet temperature: 100° C. [0123] Outlet temperature: 60° C. [0124] Feeding rate: with the pump knob set at 2 [0125] Atomizing pressure: 6-7 bar [0126] Aspiration vacuum set at 100%.

3. Results

[0127] The hydrodynamic size averaged about 246 nm with good distribution below 0.3 (FIG. 8). The morphology was observed through a scanning electron microscope (SEM) and resulted in spherical particles (FIG. 9).

[0128] The encapsulation efficiency was above 75% w/w with a solid recovery yield of over 90%. The drug loading of RIF was between 7 and 10%. The latter relatively low drug loading of a hydrophobic drug such as RIF might result from the tendency of RIF to precipitate outside of the polymeric shell.

[0129] The in vitro release studies were carried out for 25 days in a shaking water bath set at 37° C. and 100 rpm. A solution of 1 mg/mL, 40 mg of PLGA-RIF NP suspended in 40 mL of PBS pH 7.4 was prepared, all samples were in triplicates.

[0130] Controlled release of RIF was observed for the whole period of 25 days. An initial burst release in just a few minutes was observed, reaching the highest concentrations over 20 μ g/mL, followed by low but sustained levels of release for the entire study (FIG. 10).

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Claims

1. A polymer-lipid nanocomplex comprising: i. an inner microemulsion matrix comprised of at least one hydrophobic active compound, at least one fatty acid dissolved in a polar aprotic solvent, and a surfactant; and ii. an outer shell comprising one or more hydrophilic polymers.
2. The polymer-lipid nanocomplex according to claim 1, wherein the outer shell comprises an aqueous solution of an aqueous mixture of hydrophilic polymers comprising polyvinyl alcohol (PVA) and polyethylene glycol (PEG).
3. The polymer-lipid nanocomplex according to claim 1, wherein the inner microemulsion matrix further comprises at least one organic carboxylic acid, comprising a weak acid selected from the group comprising acetic acid, lactic acid, citric acid, or phosphoric acid.
4. The polymer-lipid nanocomplex according to claim 1, wherein the inner microemulsion matrix further comprises at least one biodegradable and biocompatible polymer or copolymer suitable for use in drug delivery, including poly(lactic-co-glycolic acid) or PLGA, or polylactic acid, polyglycolic acid, or poly ϵ -caprolactone.
5. The polymer-lipid nanocomplex according to claim 1, wherein the at least one fatty acid comprises any one or more of stearic acid, palmitic acid and lauric acid.
6. The polymer-lipid nanocomplex according to claim 1, wherein the polar aprotic solvent comprises either ethanol or acetone, or a blend of ethanol and acetone.
7. The polymer-lipid nanocomplex according to claim 1, wherein the surfactant comprises any surfactant having a Hydrophile-Lipophile Balance (HLB) value of greater than 10, including polysorbate 80.
8. A process for producing a polymer-lipid nanocomplex comprising at least one hydrophobic active compound according to claim 1, comprising the steps of: I. mixing at least one hydrophobic active compound, a fatty acid comprising any one or more of stearic acid, palmitic acid and lauric acid dissolved in a polar aprotic solvent comprising any one or more of ethanol or acetone, or a blend of ethanol and acetone, and a surfactant having a Hydrophile-Lipophile Balance (HLB) value of greater than 10 comprising polysorbate 80, to form an organic phase; II. optionally heating the organic phase; III. dispensing the organic phase into an aqueous mixture comprising at least one hydrophilic polymer comprising polyvinyl alcohol (PVA) and polyethylene glycol (PEG) to form a microemulsion; and IV. stabilising the microemulsion in a phosphate buffer at about 0° C. to form a nanoprecipitate of the polymer-lipid nanocomplex.
9. The process according to claim 8, which further comprises a final step of drying the nanoprecipitate to produce a free-flowing polymer-lipid nanocomplex powder either by freeze drying or by spray drying.
10. The process according to claim 8, which further comprises mixing an organic carboxylic acid comprising acetic acid, lactic acid, citric acid, or phosphoric acid with the organic phase.
11. The process according to claim 8, wherein the process further comprises dissolving at least one biodegradable and biocompatible polymer or copolymer, poly(lactic-co-glycolic acid) or PLGA, or polylactic acid, polyglycolic acid, or poly ϵ -caprolactone, into the polar aprotic solvent with the fatty acid for mixing with the at least one hydrophobic active compound and the surfactant to form

the organic phase.

12. The process according to claim 8, wherein in step IV, the nanoprecipitation of the microemulsion is performed by adding the microemulsion to the phosphate buffer solution at a ratio about 1:1.

13. A method for enhancing aqueous solubilisation and absorption of at least one hydrophobic active compound, comprising formulating the at least one hydrophobic active compound according to the process according to claim 8.

14. The polymer-lipid nanocomplex according to claim 1, wherein the at least one hydrophobic active compound comprises a hydrophobic active compound positioned on the Log P positive scale (Log P2 to Log P9) of the partition coefficient scale and includes any one or more of antituberculosis drugs, antimalarials, and phytochemicals with antifungal, antiviral, antianxiety, antiobesity, antidepressant and/or analgesic properties.

15. The polymer-lipid nanocomplex of claim 14, wherein the at least one hydrophobic active compound is the antimalarial agent Lumefantrine.

16. The polymer-lipid nanocomplex of claim 14, wherein the at least one hydrophobic active compound is the phytochemical from Cannabinoids and more specifically Cannabidiol (CBD).

17. The polymer-lipid nanocomplex of claim 14, wherein the at least one hydrophobic active compound is the anti-Tuberculosis drug Rifampicin.

18. The method according to claim 13, wherein the at least one hydrophobic active compound is formulated for administration through topical, sub-cutaneous, intravenous, intramuscular, nasal, sub-lingual, buccal, or ophthalmic routes.

19. At least one hydrophobic active compound formulated as a polymer-lipid nanocomplex according to claim 1 for use in a method of treatment or prophylaxis of a subject, wherein the hydrophobic active compound comprises one or more compounds for the treatment or prophylaxis of Tuberculosis, malaria, fungal infections, viral infections, anxiety, obesity, depression and/or pain.

20. A method of treatment or prophylaxis of a subject by administration of a hydrophobic active compound formulated as a polymer-lipid nanocomplex according to claim 1, wherein the hydrophobic active compound comprises one or more compounds for the treatment or prophylaxis of Tuberculosis, malaria, fungal infections, viral infections, anxiety, obesity, depression and/or pain.
