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Intracranial stent for insertion into the cerebral venous sinus system and methods of use

Abstract

A stent for insertion into an intracranial blood vessel of the cerebral venous sinus system includes a proximal end, a distal end, a body between the proximal end and the distal end, the body comprising a plurality of wires in a closed pattern, wherein the stent is configured for insertion into an intracranial blood vessel of the cerebral venous sinus system. The stent is further capable of being repositioned, retrieved/re-sheathed, and removed for more precise delivery.

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Background/Summary

RELATED APPLICATIONS (1) This application claims priority to U.S. application Ser. No. 17/393,120, filed on Aug. 3, 2021, which claims the benefit of U.S. Provisional Application No. 63/060,218, filed on Aug. 3, 2020, the entire contents of which are hereby incorporated by reference in their entirety.

FIELD OF THE DISCLOSURE

(1) The present disclosure relates to stents suitable for treating conditions or diseases in the intracranial/cerebral veins. In particular, the present disclosure relates to expandable, retrievable, and re-sheathable structures configured to reduce restenosis and thrombus formation in the intracranial/cerebral veins.

BACKGROUND

(2) Generally, stents are commonly indicated for a variety of intravascular and non-vascular applications, including restoration and/or maintenance of patency within a patient's vessel. Stents are also used to reduce restenosis of a blood vessel post-dilation, thereby ensuring adequate blood flow through the vessel.

(3) A new procedure has been carried out that involves placing a stent in the cerebral venous sinuses of patients to ameliorate a collapse of and/or a stenosis in the sigmoid and/or transverse sinus and/or superior sagittal sinus and to restore blood flow out of the brain. The cerebral venous sinus system (also known as dural venous sinus system) includes the large veins of the brain, namely the superior sagittal venous sinus, the transverse venous sinus, the sigmoid venous sinus and the straight venous sinus. The transverse and sigmoid venous sinuses are collectively called the “lateral” venous sinus. The cerebral venous sinuses receive blood from tributaries called cortical veins that drain in the side wall of the venous sinuses.

(4) The stent used in the new procedure typically is the same stent used for procedures in other parts of the body, such as the carotid/peripheral arteries or even the biliary system. The cerebral venous sinus structure, for instance, does not resemble any vein or arteries of other parts of the body. Instead, the venous sinus is a void created where the dura joins and forms a cavity (i.e., sinus) primarily along the inside of the skull. In this regard, the dura has no smooth muscle cell lining and is inelastic when compared to veins and arteries. In addition, the cerebral venous sinus system does not have a cylindrical shape, and is instead ovoid or even triangular.

(5) Another limitation of the current stent systems used in the cerebral venous sinuses is that the length of cerebral venous sinus stenosis often exceeds the length of existing stents, often leading to placement of more than one stents adjacent to each other. A stent specifically designed for this anatomic location needs to have longer length in order to treat the entire length of the stenosis.

(6) Current stent designs have struts designed to expand a stiff calcified atherosclerotic plaque. These struts are numerous and thick, leading to increased risk of obstructing flow from a tributary vein into the cerebral venous sinus.

(7) The first stent that was designed for the intracranial veins (River Stent, Serenity Medical, Inc.) is being currently evaluated in clinical trials. The River stent is an open cell, self-expandable, Nitinol stent delivered over 0.014 wire. However, even this stent experiences some shortcomings. Namely, once this stent is positioned in the desired location, it cannot be repositioned, retrieved/re-sheathed, or removed.

(8) There is therefore a need for a stent that is capable of being inserted into the cerebral venous sinus system and that can also be repositioned, retrieved, or removed to allow for more precise delivery. This and other benefits the present disclosure provides.

SUMMARY

(9) There is a need for developing a stent that is capable of being inserted into cerebral venous sinus system. The present disclosure is directed toward further solutions to address this need, in addition to having other desirable characteristics. For example, the stent of the present disclosure can also be repositioned, retrieved, or removed to allow for more precise delivery into the cerebral venous sinus system than previously known stents.

(10) According to some embodiments of the present disclosure, a stent includes a proximal end, a distal end, a body between the proximal end and the distal end, the body comprising a plurality of wires interbraided in a closed cell pattern, wherein the stent is configured for insertion into an intracranial target blood vessel.

(11) The stent is self-expandable or self-expanding, meaning the stent is constrained within a sheath of a delivery catheter until positioned and deployed in a desired location in the target blood vessel.

(12) According to aspects of the present disclosure, the stent can be reconstrained and retrieved within the delivery system and repositioned in the blood vessel even after partial deployment.

(13) According to aspects of the present disclosure, if the stent is partially deployed, it can be retrieved from the blood

vessel after an interval of time.
(14) According to aspects of the present disclosure, the stent can be re-sheathed after it has begun expanding.
(15) According to aspects of the present disclosure, the body has a diameter between about 6 mm and 10 mm.
(16) According to aspects of the present disclosure, the body has a length between about 40 mm and about 80 mm.
(17) According to aspects of the present disclosure, the stent is capable of transitioning between a collapsed configuration and an expanded configuration.
(18) According to some embodiments of the present disclosure, the body is formed of a combination of platinum, cobalt, chromium, stainless steel, nickel and titanium alloy.
(19) According to some aspects of the present disclosure, the target blood vessel for stent deployment can include at least one, or any one of, the cerebral venous sinus, the superior sagittal venous sinus, transverse venous sinus, sigmoid venous sinus and straight venous sinus.
(20) According to aspects of the present disclosure, stent is used to treat any one of a variety of medical conditions including idiopathic intracranial hypertension, pulsatile tinnitus, cerebral venous insufficiency, intracranial venous thrombosis, and intracranial venous stenosis, which venous stenosis includes compression from tumor, compression from brain parenchyma, compression from arachnoid granulation, and compression from blood clot (thrombus).

Description

BRIEF DESCRIPTION OF THE DRAWINGS
(1) These and other characteristics of the present disclosure will be more fully understood by reference to the following detailed description in conjunction with the attached drawings, in which:
(2) FIG. **1** is an exemplary stent in accordance with an embodiment of the present disclosure;
(3) FIG. **2** is an exemplary stent in accordance with an embodiment of the present disclosure;
(4) FIG. **3**A and FIG. **3**B illustrate an exemplary stent delivery system, in accordance with an embodiment of the present disclosure. FIG. **3**A is a schematic view illustrating the stent in a closed position. FIG. **3**B is a schematic view illustrating the stent in a deployed position; and
(5) FIG. **4**A-FIG. **4**C illustrate an exemplary stent delivery system, in accordance with an embodiment of the present disclosure;
(6) FIG. **5**A-FIG. **5**C are schematic isometric views illustrating the basic structure of a stent of the present disclosure in use. FIG. **5**A is a schematic isometric view illustrating the lateral venous sinus in the brain. FIG. **5**B is a schematic isometric view illustrating a close-up of the lateral venous sinus in the brain. FIG. **5**C is a schematic isometric view illustrating an exemplary stent in accordance with an embodiment of the present disclosure secured in the lateral venous sinus in the brain.
DETAILED DESCRIPTION OF EMBODIMENTS
(7) An illustrative embodiment of the present disclosure relates to a stent that is capable of being inserted into the cerebral venous sinuses and that is also capable of being repositioned, retrieved, or removed to allow for more precise delivery.
(8) FIGS. **1** through FIG. **4**A-FIG. **4**C, wherein like parts are designated by like reference numerals throughout, illustrate an example embodiment or embodiments of stent that is capable for being inserted into the cerebral venous sinuses, according to the present disclosure. Although the present disclosure will be described with reference to the example embodiment or embodiments illustrated in the figures, it should be understood that many alternative forms can embody the present disclosure. One of skill in the art will additionally appreciate different ways to alter the parameters of the embodiment(s) disclosed, such as the size, shape, or type of elements or materials, in a manner still in keeping with the spirit and scope of the present disclosure.
(9) As used herein, an element or step recited in the singular and proceeded with the word “a” or “an” should be understood as not excluding plural of said elements or steps, unless such exclusion is explicitly stated. Furthermore, references to “one embodiment” are not intended to be interpreted as excluding the existence of additional embodiments that also incorporate the recited features. Moreover, unless explicitly stated to the contrary, embodiments “comprising” or “having” an element or a plurality of elements having a particular property can include additional elements not having that property. As referred to herein, the terms “proximal” and “distal” are in relation to the delivery handle of the stent delivery system (also referred to as a catheter). For example, the distal end **104** of the stent **100** and the catheter is the end that is inserted first into a body of a patient and the proximal end **106** is opposite the distal end **104**.
(10) FIG. **1** and FIG. **2** illustrate an exemplary stent **100** in accordance with various embodiments of the present disclosure. The stent **100** is shown in an expanded configuration. Stent **100** comprises a tubular flexible body **102** having a distal end **104** and a proximal end **106**. Stent **100** further comprises a web structure **108** that is configured to allow the stent **100** to expand from a contracted delivery configuration to an expanded deployed configuration.
(11) In an embodiment, the web structure **108** can have a braided or closed design. As shown in FIG. **1** and FIG. **2**, the stent **100** is formed by having a plurality of elongate wires **110** formed into the web structure **108**. The elongate wires **110** traverse the length of the stent **100** in a direction traverse to the longitudinal length of the stent **100**. The elongate wires **110** can be formed into the web structure **108** by braiding the wires **110**, winding the wires **110**, knitting the wires **110**, and combinations thereof. In one embodiment, the wires **110** are laser-cut in a closed cell pattern to form the web structure **108**. The diameter of the struts in the web structure **108** will be carefully optimized to modulate the radial outward force across

the entire length of the stent. The diameter of the struts will vary from about 0.1 mm to about 1 mm. As used herein, the term “about” or “approximately” refers to a variation of 10% from the indicated values (e.g., 0.1 mm, 1 mm, etc.), or in case of a range of values, means a 10% variation from both the lower and upper limits of such ranges. For instance, “about 1 mm” refers to a range of between 0.9 mm and 1.1 mm.

(12) In accordance with an embodiment of the present disclosure, the web structure **108** is configured to allow the stent **100** to self-expand and contract as many times as necessary until the stent **100** reaches the correct location and can be deployed and secured. A stent that is able to contract after it has expanded to a certain point and move back into its delivery system is referred to as a stent that is “retrievable” or “re-sheatheable.” In an embodiment, the stent **100** is capable of being retrieved or re-sheathed even when the stent **100** is between about seventy percent (70%) and eighty-five percent (85%) expanded. In an embodiment, the stent **100** is capable of being retrieved or re-sheathed even when the stent **100** is about eighty-five percent (85%) expanded. In an embodiment, the stent **100** is capable of being retrieved or re-sheathed even when the stent **100** is about eighty percent (80%) expanded. In an embodiment, the stent **100** is capable of being retrieved or re-sheathed even when the stent **100** is about seventy-five percent (75%) expanded. In an embodiment, the stent **100** is capable of being retrieved or re-sheathed even when the stent **100** is about seventy percent (70%) expanded. By being retrievable or re-sheathable, the stent **100** of the present disclosure is capable of being repositioned multiple times before being secured into place. This allows the stent **100** to be positioned, repositioned, and even removed until the desired location is found. In this way, the stent **100** of the present disclosure allows for more precise delivery of the stent **100**.

(13) Stents are typically implemented in either a closed cell pattern, an open cell pattern, or a braided cell pattern. A stent with a “closed cell pattern” has each peak and valley of each strut segment connected to a peak or valley of an adjacent strut segment, with the exception of the strut segments on the proximal and distal ends. Stents with an “open cell pattern,” on the other hand, have some peaks and/or valleys that are not connected to peaks and/or valleys of adjacent strut segments. Stents with braided patterns include a one over and one under pattern, but other patterns can suitably be used, knitting wires or wire filaments into a braided loop, the pattern of which loops are formed from a relaxed state, where each row of loops is axially and independently of the rows on either side. In an embodiment, the stent **100** can have a closed cell pattern design, for example, to allow the stent **100** to expand and collapse multiple times before being secured. Moreover, a closed cell pattern stent structure has an enhanced ability to expand and conform to a non-circular cavity wall, such as the sinuses, when compared to an open cell pattern structure. For example, the individual segments of a closed cell pattern stent have more flexibility than the segments of an open cell pattern stent. Such flexibility beneficially increases a clinician's ability to guide the stent to a target site within a patient's vessel. Accordingly, the closed cell pattern segments are better suited for conforming to irregularities of a non-circular cavity.

(14) Furthermore, stents of the present invention preferably exhibit high radial stiffness in the deployed configuration. Implanted stents therefore are capable of withstanding compressive forces applied by a vessel wall, thereby alleviating stenosis and maintaining vessel patency. The web structure **108** of the present disclosure provides the desired combination of flexibility in the delivery configuration to allow for safe navigation and radial stiffness in the deployed configuration to allow for excellent apposition to the vessel wall. In addition, the flexibility of the web structure **108** of the present disclosure allows the stent **100** to conform to the anatomy of the intracranial veins.

(15) The stent **100** of the present disclosure can be sized to cover the anatomy of the intracranial veins. For example, depending on the area of need, the length of the stent **100** can be between about 40 mm to about 80 mm long. In an embodiment, the length of the stent **100** is between about 40 mm to about 45 mm. In an embodiment, the length of the stent **100** is between about 45 mm to about 50 mm. In an embodiment, the length of the stent **100** is between about 50 mm to about 55 mm. In an embodiment, the length of the stent **100** is between about 55 mm to about 60 mm. In an embodiment, the length of the stent **100** is between about 60 mm to about 65 mm. In an embodiment, the length of the stent **100** is between about 65 mm to about 70 mm. In an embodiment, the length of the stent **100** is between about 70 mm to about 75 mm. In an embodiment, the length of the stent **100** is between about 75 mm to about 80 mm. As used herein, the term “about” or “approximately” refers to a variation of 10% from the indicated values (e.g., 40 mm, 45 mm, 50 mm, etc.), or in case of a range of values, means a 10% variation from both the lower and upper limits of such ranges. For instance, “about 40 mm” refers to a range of between 36 mm and 44 mm.

(16) Depending on the area of treatment, the diameter of the stent **100** can be between about 6 mm to about 10 mm. In an embodiment, the diameter of the stent **100** is between about 6 mm and about 7 mm. In an embodiment, the diameter of the stent **100** is between about 7 mm and about 8 mm. In an embodiment, the diameter of the stent **100** is between about 8 mm and about 9 mm. In an embodiment, the diameter of the stent **100** is between about 9 mm and about 10 mm. The diameter can be the same from one end to the other end or the diameter can be tapered. In one embodiment, for example, the stent **100** can be 7 mm at one end and gradually increase to 9 mm at the other end.

(17) The stent **100** of the present disclosure can be made of wires comprising a combination of suitable materials, including platinum, cobalt, chromium, stainless steel, nickel and titanium. Since the stent **100** of the present disclosure is self-expanding and also retrievable/re-sheathable, the web structure **108** in an embodiment is fabricated from an elastic material. In accordance with further embodiments of the present disclosure, stent **100** is fabricated from biocompatible and/or biodegradable materials. Biocompatible material can comprise a biocompatible polymer, for example, a modified thermoplastic Polyurethane, Polyethylene Terephthalate, Polyethylene Tetraphthalate, expanded Polytetrafluoroethylene, Polypropylene, Polyester, Nylon, Polyethylene, Polyurethane, or combinations thereof.

(18) In some embodiment, stent **100** can contain an external coating or attached active groups C configured for localized delivery of radiation, gene therapy, medicaments, thrombin inhibitors, or other therapeutic agents. For example, stent **100**

can be coated with therapeutic agents to help prevent or delay thrombus formation or restenosis within a vessel. Coatings or active groups C can, in an embodiment, be absorbed or adsorbed onto the surface, can be attached physically, chemically, biologically, electrostatically, covalently, or hydrophobically, or can be bonded to the surface through VanderWaal's forces, or combinations thereof, using a variety of techniques that are well-known in the art.

(19) Referring now to FIG. **3**A and FIG. **3**B, stent **100** is depicted in operation. Using known methods, stent **100** can be delivered over a guide wire **112** via a small incision basilic, femoral, or internal jugular veins and the use of fluoroscopic guidance. To deliver the stent **100** to its desired location, the stent **100**, in a collapsed configuration as shown in FIG. **3**A, is first inserted into a lumen **114**, then guided through the veins with the help of the guide wire **112**. The guide wire **112** can be any known guide wire used in the art that is sufficiently sized to navigate through a venous sinus. In one embodiment, the guide wire **112** may be about 0.014 mm in diameter. Once at the desired location, the lumen **114** can be pulled back to expose the stent **100** as shown in FIG. **3**B. Upon exposure, the stent self-expands and secures itself to the surrounding vessel walls.

(20) To assist in delivering stent **100** to its desired location, stent **100** may have a tip **116** at its distal end **104**. This will allow for atraumatic advancement of the stent through a blood vessel or narrowed venous sinus, especially in cases where there is an abnormality within the lumen of the venous sinus (clot, arachnoid granulation). The tip **116** may be shaped as a cone, a wedge, or other similar shape with a tapered end that allows it to maneuver through the venous sinus. The tip **116** may be approximately 20 mm in length but can also be between approximately 10 mm in length to approximately 25 mm in length. The diameter of tip **116** can be same from one end to the other end or the diameter can be tapered. In one embodiment, for example, the diameter of tip **116** can be 7 mm in one end and gradually increase to 9 mm at the other end.

(21) If necessary, the stent **100** can be retrieved or re-sheathed after it has been deployed. For instance, if the user (e.g., physician) determines that the stent **100** is not in the proper location after the stent **100** has begun to self-expand, the user can still retrieve the stent by causing the stent **100** to collapse back into the lumen **114**. In an embodiment, the stent **100** can still be retrieved or re-sheathed with the lumen **114**, even when the stent **100** is about eighty percent expanded.

(22) FIG. **4**A, FIG. **4**B, and FIG. **4**C illustrate an implant delivery system **120** in accordance with an embodiment of the present disclosure. In an embodiment, the implant delivery system **120** may include stent **100**, a catheter **122** with hub **124** and guide wire **112** extending through catheter **122** and hub **124**. In an embodiment, catheter **122** may have a distal end **130**, a proximal end **132**, and a lumen **134** extending between the distal end **130** and the proximal end **132**. Catheter **122** is relatively flexible, may be comprised of a polymeric material such as nylon or PEBAX, and may range in length from 60 cm to 300 cm. Guide wire **112** diameter may be large enough to allow passage of guidewires ranging in diameter from 0.009 mm to 0.038 mm. Hub **124** is removably attached to the proximal end **132** of catheter **122**, is adapted to reversibly connect to other medical devices, and may be comprised of polycarbonate or any other suitable material. At the distal end **130** of catheter **122** is stent **100**. At distal end **104** of stent **100** is tip **116**.

(23) An exemplary method of using a stent **100** with implant delivery system **120** is now described. A guide wire **112** is advance into a patient's peripheral vein (femoral vein, basilic vein, internal jugular vein) using known techniques, through a patient's vessel and to a treatment site. Stent **100** is loaded onto implant delivery system **120** in a collapsed position and introduced over the guidewire into the patient's vessel. The stent **100** and implant delivery system **120** combination is advanced over the guidewire **112** and through the patient's vessel until stent **100** is located at a treatment site, for example within a stenosis in the cerebral venous sinus system. Stent **100** is deployed by releasing the stent **100** thereby allowing stent **100** to self-expand. If necessary to reposition stent **100**, stent **100** may be retrieved or re-sheathed by collapsing the stent **100** within the catheter **122**. Once the stent **100** is deployed, catheter **122** is then withdrawn through the patient's vessel and out of the patient's body.

(24) Referring to FIG. **5**A, FIG. **5**B, and FIG. **5**C, the stent **100** is shown in use in an intracranial vessel. In operation, the stent is shown secured in the lateral venous sinus which is located within the brain as depicted in FIG. **5**C.

(25) With any embodiment, the stent **100** can be inserted into an intracranial vessel which includes, without limitation, the dural venous sinuses (the superior sagittal sinus, transverse sinus, sigmoid sinus, the straight sinus).

(26) With any embodiment, the stent **100** can be used for a number of purposes including to maintain patency of a cerebral venous sinus. Medical conditions that are suited to be treated using the stent **100** of the present disclosure include, without limitation, idiopathic intracranial hypertension, pulsatile tinnitus, cerebral venous insufficiency, intracranial venous thrombosis, and intracranial venous stenosis, including compression from tumor, compression from brain parenchyma, compression from arachnoid granulation, and thrombus.

(27) The stent **100** of the present disclosure provides several notable advantages over stents currently used. First, the stent **100** is specifically designed for use in cerebral venous sinuses rather than for other parts of the body such as the carotid/peripheral arteries. As such, the stent **100** has enhanced conformability to the anatomy of cerebral venous sinuses as compared to stents that were not designed for use in this region. In addition, the stent **100** of the present disclosure is retrievable and re-sheathable which allow it to be positioned, repositioned, and removed prior to being secured. This enhances the ability of the stent **100** to be precisely delivered to its desired location.

(28) Other notable advantages of the stent **100** of the present disclosure include its flexibility to allow for safe navigation through the intracranial veins, its ability to secure itself to the vessel walls, and its ability to alleviate stenosis and restore patency in the veins. These features of the stent **100** are in part due to the unique combination of materials that provide the stent **100** with the required flexibility, stability, and strength.

(29) To treat different conditions in different vessels, the stent **100** of the present disclosure can be customized. In an embodiment, the stent **100** of the present disclosure can have customized, variable zones of chronic outward force that

mimic the compliance and adapt to the anatomy of the cerebral venous sinuses (e.g., target vessel). This means that the stent **100** may be stiffer or firmer in some areas and not in others. The stiffer sections can help open, and keep open, those areas of the vessel that are more difficult to open. In one embodiment, the stent **100** may be stiffer in the middle.
(30) In another embodiment. the stent can have customized, variable cell size to adapt to the non-cylindrical shape of cerebral venous sinuses (e.g., target vessel) and achieve excellent apposition to the wall of the cerebral venous sinus. This means that certain sections of the stent **100** may have different spacing between the cells to help conform to the shape of the vessel. This allows the stent **100** of the present disclosure to be used to treat various conditions in different vessels.
(31) In another embodiment, the stent can have customized, variable cell size to prevent obstruction of flow from a tributary vein into the cerebral venous sinus.
(32) Numerous modifications and alternative embodiments of the present disclosure will be apparent to those skilled in the art in view of the foregoing description. Accordingly, this description is to be construed as illustrative only and is for the purpose of teaching those skilled in the art the best mode for carrying out the present disclosure. Details of the structure can vary substantially without departing from the spirit of the present disclosure, and exclusive use of all modifications that come within the scope of the appended claims is reserved. Within this specification embodiments have been described in a way which enables a clear and concise specification to be written, but it is intended and will be appreciated that embodiments can be variously combined or separated without parting from the disclosure. It is intended that the present disclosure be limited only to the extent required by the appended claims and the applicable rules of law.
(33) It is also to be understood that the following claims are to cover all generic and specific features of the disclosure described herein, and all statements of the scope of the disclosure which, as a matter of language, might be said to fall therebetween.

Claims

1. A method of treating pulsatile tinnitus (PT) in a subject which comprises: providing a stent that is braided and self-expanding, the stent having a proximal end, a distal end, and a tubular flexible body between the proximal end and the distal end, with the same diameter at the proximal and distal end, the tubular flexible body comprising a wire arrayed in a cellular pattern, wherein the tubular flexible body has a higher degree of stiffness in a first section of the tubular flexible body than in a second section of the tubular flexible body, wherein the tubular flexible body has different zones of outward force, a length of between about 40 mm and about 80 mm, is configured to expand to conform to an ovoid or triangular shape of vessel of a cerebral venous sinus system of the subject, to secure itself to surrounding walls of the vessels, to be retrievable or re-sheathable and to be implanted in a stenosis in a selected vessel of the vessels of the cerebral venous sinus system, inserting a guide wire and a flexible delivery catheter through an incision in the femoral, basilic, or internal jugular vein, the stent being contained within a lumen of the delivery catheter; guiding the stent through one or more of the vessels of the cerebral venous sinus system in a collapsed configuration on the guide wire to the stenosis; and releasing the stent from the guide wire at the stenosis in the selected vessel to allow the stent to self-expand, to alleviate the stenosis by forcing a surrounding narrowed segment of the selected vessel to expand, and to secure itself to the surrounding narrowed segment of the selected vessel to and maintain the patency of the selected vessel to treat the PT.
2. The method of claim 1 wherein the stent is collapsible within the delivery catheter.
3. The method of claim 1 wherein the selected vessel is a member selected from the group consisting of the superior sagittal sinus, the transverse sinus, the sigmoid sinus and the straight sinus.
4. The method of claim 1 wherein the stent comprises cells having different sizes in different sections of the stent.
5. The method of claim 1 further comprising collapsing the stent within the delivery catheter and repositioning the stent within the selected vessel.
6. The method of claim 1 wherein the stent comprises a plurality of wires interbraided in a closed cell pattern.
7. The method of claim 1 wherein the stent is delivered over the guide wire having a tip at the distal end of the guide wire.
8. The method of claim 7 wherein the tip has a tapered end.
9. The method of claim 7 wherein the tip is between 10 and 25 mm in length.
10. The method of claim 1 wherein the stent comprises a web structure that allows the stent to self-expand and contract repeatedly until the stent reaches a correct location and can be deployed and secured.
11. The method of claim 1 wherein the cellular pattern is a closed cell pattern.
12. The method of claim 1 wherein the wire is in a braided configuration.
13. A method of alleviating a stenosis in a cerebral venous sinus of a patient, wherein the stenosis causes pulsatile tinnitus (PT), the method comprising implanting a braided self-expanding stent in a vein of the cerebral venous sinus at a site of the stenosis, the braided self-expanding stent having a proximal end, a distal end, the same diameter of between about 6 mm and about 10 mm at each of the proximal and distal ends, a length of between about 40 mm and about 80 mm and a tubular flexible body between the proximal end and the distal end, the tubular flexible body comprising a plurality of wires arrayed in a closed cell pattern, wherein the tubular flexible body has a higher degree of stiffness in a first section of the stent than in a second section of the stent and is arranged to expand with chronic outward force to secure itself to a surrounding narrowed segment of the cerebral venous sinus such that the tubular flexible body conforms to the anatomy of the cerebral venous sinus to alleviate the stenosis by forcing the narrowed segment of the cerebral venous sinus to expand, and to alleviate the PT.
14. The method of claim 13 wherein the tubular flexible body has a higher degree of stiffness in a first section of the

tubular flexible body than in a second section of the tubular flexible body and expands with chronic outward force to conform to an ovoid or triangular shape of the cerebral venous sinus.

15. The method of claim 13 wherein the wires are laser cut.

16. The method of claim 13 wherein the length of the stent is between 75 mm and 80 mm.

17. The method of claim 13 wherein the stent is delivered over a guidewire having a tip at a distal end.

18. The method of claim 17 wherein the diameter of the tip gradually increases from one end to the other.

19. The method of claim 13 wherein the stent is re-sheathable.

20. The method of claim 13 wherein the braided self-expanding stent comprises different spacings between cells in different sections of the stent to conform the stent to the shape of the cerebral venous sinus.