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MODULAR ELECTRICAL THERAPY DEVICE

Abstract

A therapeutic electrode component includes a base plate having a first side and a second side having a conductive surface. A repository having an internal volume to releasably retain a conductive fluid is disposed on the first side of the base plate. A rupturable membrane is disposed between the internal volume of the repository and the conductive surface of the base plate. A coupling is disposed on the base plate that is configured to detachably engage a gas charge, whereby the gas charge is detachable from the coupling without causing destruction of the gas charge, to provide a hermetic seal with an outlet of the gas charge, and to provide fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling. A retainer is configured to detachably secure the gas charge to the base plate.

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Background/Summary

BACKGROUND

[0001] The present disclosure is generally directed to systems and methods of delivering electrical therapy to a patient.

[0002] There are a wide variety of electronic and mechanical devices for monitoring and treating patients' medical conditions. In some examples, depending on the underlying medical condition being monitored or treated, medical devices such as cardiac monitors or defibrillators may be surgically implanted or externally connected to the patient. In some examples, physicians may use medical devices alone or in combination with drug therapies to treat conditions such as cardiac arrhythmias.

[0003] One of the deadliest cardiac arrhythmias is ventricular fibrillation, which occurs when normal, regular electrical impulses are replaced by irregular and rapid impulses, causing the heart muscle to stop normal contractions and to begin to quiver. Normal blood flow ceases, and organ damage or death can result in minutes if normal heart contractions are not restored. Because the victim has no perceptible warning of the impending fibrillation, death often occurs before the necessary medical assistance can arrive. Other cardiac arrhythmias can include excessively slow heart rates known as bradycardia or excessively fast heart rates known as tachycardia. Cardiac arrest can occur when a patient in which various arrhythmias of the heart, such as ventricular fibrillation, ventricular tachycardia, pulseless electrical activity (PEA), and asystole (e.g., heart stops all electrical activity) result in the heart providing insufficient levels of blood flow to the brain and other vital organs for the support of life.

[0004] Cardiac arrest and other cardiac health ailments are a major cause of death worldwide. Various resuscitation efforts aim to maintain the body's circulatory and respiratory systems during cardiac arrest in an attempt to save the life of the patient. The sooner these resuscitation efforts begin, the better the patient's chances of survival. Implantable cardioverter/defibrillators (ICDs) or external defibrillators (such as manual defibrillators or automated external defibrillators (AEDs)) have significantly improved the ability to treat these otherwise life-threatening conditions. Such devices operate by applying corrective electrical pulses directly to the patient's heart. Ventricular fibrillation or ventricular tachycardia can be treated by an implanted or external defibrillator, for example, by providing a therapeutic shock to the heart in an attempt to restore normal rhythm. To treat conditions such as bradycardia, an implanted or external pacing device can provide pacing stimuli to the patient's heart until intrinsic cardiac electrical activity returns.

[0005] Example external cardiac monitoring and/or treatment devices include cardiac monitors, the ZOLL Life Vest® wearable cardioverter defibrillator available from ZOLL Medical Corporation, and the AED Plus also available from ZOLL Medical Corporation.

[0006] Some examples of cardiac monitoring and/or treatment devices include therapy electrodes that release conductive gel onto the skin of a subject prior to delivering electrical therapy to the subject to decrease electrical resistance between the therapy electrode and the subject. Such therapy electrodes have in the past been single use devices that would be replaced after each use with the

older devices being discarded.

SUMMARY

[0007] In accordance with one aspect, there is provided a therapeutic electrode component for application of electrical stimulus to a subject and for allowing reuse of non-destroyed portions of a therapeutic electrode in application of electrical stimulus to a subject. The therapeutic electrode component comprises a base plate having a first side and a second side opposing the first side, the second side having a conductive surface. The therapeutic electrode component further comprises a repository having an internal volume configured to releasably retain a conductive fluid. The repository is disposed on the first side of the base plate. A rupturable membrane is disposed between the internal volume of the repository and the conductive surface of the base plate. A coupling is disposed on the base plate. The coupling is configured to detachably engage a gas charge, whereby the gas charge is detachable from the coupling without causing destruction of at least the gas charge, to provide a hermetic seal with an outlet of the gas charge, and to provide fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling. The therapeutic electrode component further comprises a retainer configured to detachably secure the gas charge to the base plate.

[0008] In some embodiments, the gas charge is detachable from the coupling without causing destruction of at least the base plate, the repository, and the rupturable membrane.

[0009] In some embodiments, the coupling comprises a barb including an internal pneumatic conduit configured to provide the fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling.

[0010] In some embodiments, the therapeutic electrode component further comprises a connector formed of a resilient material and including a conduit having a first opening configured to receive and releasably retain the barb and a second opening configured to receive and retain the outlet of the gas charge.

[0011] In some embodiments, the therapeutic electrode component further comprises pneumatic tubing providing fluid communication between the outlet of the gas charge and the barb.

[0012] In some embodiments, the barb extends in a direction parallel to a plane defined by a surface of the first side of the base plate.

[0013] In some embodiments, the barb extends in a direction perpendicular to a plane defined by a surface of the first side of the base plate.

[0014] In some embodiments, the coupling comprises a snap ring coupled to the first side of the base plate. The therapeutic electrode component may further comprise a feed-through including a base that surrounds an end portion of the gas charge and the outlet of the gas charge, and a barb extending from the base that is configured to releasably engage the snap ring. The therapeutic electrode component may further comprise an O-ring disposed between the base and the snap ring when the barb is engaged with the snap ring and that enhances hermeticity of a seal between the feed-through and snap ring.

[0015] In some embodiments, the therapeutic electrode component further comprises a pneumatic header in fluid communication with the outlet of the gas charge, the snap ring being configured to receive and releasably retain the pneumatic header. The therapeutic electrode component may further comprise an O-ring disposed between the snap ring and pneumatic header when the gas charge is engaged with the coupling and that enhances hermeticity of a seal between the snap ring and pneumatic header. The pneumatic header may be retained within a resilient body coupled to the gas charge.

[0016] In some embodiments, the coupling comprises a feed-through disposed on the first side of the base plate including a neck defining an internal volume. The therapeutic electrode component may further comprise a washer formed of a resilient material that surrounds a length of the outlet of the gas charge and is configured to be retained within the internal volume of the neck of the feed-through, an O-ring surrounding the neck of the feed-through, and a snap ring that couples to the

feed through and traps the O-ring between the snap ring and the feed-through.

[0017] In some embodiments, the gas charge is disposed within a module that is detachably engageable with the base plate. The coupling may include a post disposed on the first side of the base plate and including a pneumatic conduit configured to provide the fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling. The post may be configured to engage an aperture in the module. The therapeutic electrode component may further comprise an O-ring disposed between a neck of the pneumatic conduit and the aperture in the module that enhances hermeticity of a seal between the pneumatic conduit and module. The module may be configured to couple to the first side of the base plate by sliding the module in a plane defined by a surface of the first side of the base plate into a cradle coupled to the first side of the base plate. The retainer may include one or more clips disposed on the cradle that engage one or more slots on the module. The retainer may include one or more clips disposed on the module that engage one or more slots on the cradle. The retainer may include one or more conductive fasteners that pass through the base plate and engage one or more respective apertures in the module. The one or more conductive fasteners may electrically engage the conductive surface of the base plate when securing the module to the base plate. The one or more conductive fasteners may be configured to deliver one of a defibrillation pulse or a pacing pulse to the subject through the conductive surface of the base plate. In some examples, the defibrillation pulse may include a biphasic current pulse of between about 0 and 150 A. In some embodiments, the therapeutic electrode component further comprises a circuit board disposed within the module and configured to control activation of the gas charge. The therapeutic electrode component may further comprise signal leads in electrical communication between the circuit board and the gas charge and configured to deliver an activation current to the gas charge. In some examples, the activation current may be at least 0.1 mA.

[0018] In some embodiments, the module is configured to couple to the first side of the base plate by moving the module in a direction perpendicular to a plane defined by a surface of the first side of the base plate onto the first side of the base plate.

[0019] In some embodiments, the therapeutic electrode component further comprises a conduit disposed on the base plate providing fluid communication between the coupling and the internal volume of the repository. The rupturable membrane may be configured to rupture responsive to delivery of gas from the gas charge to the internal volume of the repository through the conduit. The repository may be configured to release the conductive fluid onto the conductive surface of the base plate responsive to delivery of gas from the gas charge to the internal volume of the repository through the conduit. The repository may comprise a plurality of separate chambers each releasably retaining a volume of the conductive fluid and in fluid communication with the conduit.

[0020] In accordance with another aspect, there is provided a wearable therapeutic device for allowing reuse of non-destroyed portions of a therapeutic electrode in application of electrical stimulus to a subject. The device comprises a garment configured to be worn about the subject, at least one therapeutic electrode component configured to be removably retained by the garment, circuitry configured to provide a therapeutic pulse of energy to the at least one therapeutic electrode component, and at least one processor operatively coupled to the circuitry and the at least one therapeutic electrode component. The at least one therapeutic component comprises a base plate having a first side and a second side opposing the first side. The second side has a conductive surface. The at least one therapeutic component further comprises a repository having an internal volume configured to releasably retain the conductive fluid. The repository is disposed on the first side of the base plate. A rupturable membrane is disposed between the internal volume of the repository and the conductive surface of the base plate. A coupling is disposed on the base plate. The coupling is configured to detachably engage a gas charge, whereby the gas charge is detachable from the coupling without causing destruction of at least the gas charge, to provide a hermetic seal with an outlet of the gas charge, and to provide fluid communication between the

internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling. The at least one therapeutic component further comprises a retainer configured to detachably secure the gas charge to the base plate.

[0021] In accordance with another aspect, there is provided a method for delivery of electrical stimulus to a subject and allowing reuse of non-destroyed portions of a therapeutic electrode in application of the electrical stimulus to the subject. The method comprises securing a gas charge to a coupling disposed on a first surface of a base plate of a therapeutic electrode component, the coupling providing fluid communication with an internal volume of a repository disposed on the base plate, the repository configured to dispense a conductive fluid onto a conductive second surface of the base plate through a rupturable membrane disposed between the internal volume of the repository and the conductive surface of the base plate. The method further comprises, responsive to determining that the gas charge should be replaced, removing the gas charge from the coupling without causing destruction to at least the base plate, the repository, and the rupturable membrane, and securing a replacement gas charge to the coupling.

[0022] In accordance with another aspect, there is provided a method for delivery of electrical stimulus to a subject and allowing reuse of non-destroyed portions of a therapeutic electrode in delivery of the electrical stimulus to the subject. The method comprises securing a gas charge to a coupling disposed on a first surface of a base plate of a therapeutic electrode component, the coupling providing fluid communication with an internal volume of a repository disposed on the base plate, the repository configured to dispense a conductive fluid onto a conductive second surface of the base plate through a rupturable membrane disposed between the internal volume of the repository and the conductive surface of the base plate. The method further comprises, responsive to determining that the gas charge should be moved from the therapeutic electrode component to a second therapeutic electrode component, removing the gas charge from the coupling without causing destruction to at least the base plate, the repository, and the rupturable membrane, and securing the gas charge to a second coupling of the second therapeutic electrode component.

[0023] In accordance with another aspect, there is provided a therapeutic electrode component for application of electrical stimulus to a subject and for allowing reuse of non-destroyed portions of a therapeutic electrode in application of electrical stimulus to a subject. The therapeutic electrode component comprises a base plate having a first side and a second side opposing the first side, the second side having a conductive surface. The therapeutic electrode component further comprises a repository having an internal volume configured to releasably retain a conductive fluid. The repository is disposed on the first side of the base plate. A rupturable membrane is disposed between the internal volume of the repository and the conductive surface of the base plate. A coupling is disposed on the base plate. The coupling is configured to detachably engage a gas charge. The gas charge is detachable from the coupling without causing destruction of at least the gas charge and/or the coupling. The coupling provides a hermetic seal with an outlet of the gas charge, and fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling. The therapeutic electrode component further comprises a retainer configured to detachably secure the gas charge to the base plate.

[0024] In accordance with another aspect, there is provided a therapeutic electrode component for application of electrical stimulus to a subject and for allowing reuse of non-destroyed portions of a therapeutic electrode in application of electrical stimulus to a subject. The therapeutic electrode component comprises a base plate having a first side and a second side opposing the first side, the second side having a conductive surface, a repository having an internal volume configured to releasably retain a conductive fluid, the repository disposed on the first side of the base plate, a rupturable membrane disposed between the internal volume of the repository and the conductive surface of the base plate, a coupling disposed on the base plate, the coupling configured to detachably engage a gas charge, the gas charge being detachable from the coupling without causing

destruction of at least the gas charge, the coupling further configured to provide a hermetic seal with an outlet of the gas charge, and to provide fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling, and a retainer configured to detachably secure the gas charge to the base plate.

[0025] In some embodiments, the gas charge is detachable from the coupling without causing destruction of at least the base plate, the repository, and the rupturable membrane.

[0026] In some embodiments, the coupling comprises a barb including an internal pneumatic conduit configured to provide the fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling.

[0027] In some embodiments, the therapeutic electrode component further comprises a connector formed of a resilient material and including a conduit having a first opening configured to receive and releasably retain the barb and a second opening configured to receive and retain the outlet of the gas charge.

[0028] In some embodiments, the coupling comprises a snap ring coupled to the first side of the base plate, and a pneumatic header in fluid communication with the outlet of the gas charge, the snap ring being configured to releasably retain the pneumatic header.

[0029] In some embodiments, the pneumatic header is retained within a resilient body coupled to the gas charge.

[0030] In some embodiments, the coupling comprises a feed-through disposed on the first side of the base plate including a neck defining an internal volume, a washer formed of a resilient material that surrounds a length of the outlet of the gas charge and is configured to be retained within the internal volume of the neck of the feed-through, an O-ring surrounding the neck of the feed-through, and a snap ring that couples to the feed through and traps the O-ring between the snap ring and the feed-through.

[0031] In some embodiments, the gas charge is disposed within a module that is detachably engageable with the base plate, and the coupling includes a post disposed on the first side of the base plate and including a pneumatic conduit configured to provide the fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling, the post configured to engage an aperture in the module.

[0032] In some embodiments, the gas charge is disposed within a module that is detachably engageable with the base plate, and wherein the module is configured to couple to the first side of the base plate by sliding the module in a plane defined by a surface of the first side of the base plate into a cradle coupled to the first side of the base plate.

[0033] In some embodiments, the retainer includes one or more conductive fasteners that pass through the base plate and engage one or more respective apertures in the module.

[0034] In some embodiments, the one or more conductive fasteners electrically engage the conductive surface of the base plate when securing module to the base plate.

[0035] In some embodiments, the therapeutic electrode component further comprises one or more conductive fasteners, the one or more conductive fasteners configured to deliver one of a defibrillation pulse or a pacing pulse to the subject through the conductive surface of the base plate.

[0036] In some embodiments, the defibrillation pulse comprises a biphasic current pulse of between about 0 and 150 Amps and the pacing pulse comprises a current of between about 0 mAmps to about 200 mAmps.

[0037] In some embodiments, the gas charge is disposed within a module that is detachably engageable with the base plate, and the therapeutic electrode component further comprises a circuit board disposed within the module and configured to control activation of the gas charge, and signal leads in electrical communication between the circuit board and the gas charge and configured to deliver an activation current to the gas charge.

[0038] In some embodiments, the gas charge is disposed within a module that is detachably engageable with the base plate, the module being configured to couple to the first side of the base

plate by moving the module in a direction perpendicular to a plane defined by a surface of the first side of the base plate on to the first side of the base plate.

[0039] In some embodiments, the therapeutic electrode component further comprises a conduit disposed on the base plate providing fluid communication between the coupling and the internal volume of the repository.

[0040] In some embodiments, the repository comprises a plurality of separate chambers each releasably retaining a volume of the conductive fluid and in fluid communication with the conduit.

[0041] In some embodiments, the rupturable membrane is configured to rupture responsive to delivery of gas from the gas charge to the internal volume of the repository through the conduit.

[0042] In some embodiments, the repository is configured to release the conductive fluid onto the conductive surface of the base plate responsive to delivery of gas from the gas charge to the internal volume of the repository through the conduit.

[0043] In accordance with another aspect, there is provided a wearable therapeutic device for allowing reuse of non-destroyed portions of a therapeutic electrode in application of electrical stimulus to a subject. The wearable therapeutic device comprises a garment configured to be worn about the subject, at least one therapeutic electrode component configured to be removably retained by the garment, circuitry configured to provide a therapeutic pulse of energy to the at least one therapeutic electrode component, and at least one processor operatively coupled to the circuitry and the at least one therapeutic electrode component. The at least one therapeutic component comprises a base plate having a first side and a second side opposing the first side, the second side having a conductive surface, a repository having an internal volume configured to releasably retain the conductive fluid, the repository disposed on the first side of the base plate, a rupturable membrane disposed between the internal volume of the repository and the conductive surface of the base plate, a coupling disposed on the base plate, the coupling configured to detachably engage a gas charge, the gas charge being detachable from the coupling without causing destruction of at least the gas charge, the coupling further configured to provide a hermetic seal with an outlet of the gas charge, and to provide fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling, an a retainer configured to detachably secure the gas charge to the base plate.

[0044] In some embodiments, the gas charge is detachable from the coupling without causing destruction of at least the base plate, the repository, and the rupturable membrane.

[0045] In some embodiments, the wearable therapeutic device further comprises one or more conductive fasteners, the one or more conductive fasteners configured to deliver one of a defibrillation pulse or a pacing pulse to the subject through the conductive surface of the base plate.

[0046] In some embodiments, the defibrillation pulse comprises a biphasic current pulse of between about 0 and 150 Amps and the pacing pulse comprises a current of between about 0 mAmps to about 200 mAmps.

[0047] In some embodiments, the gas charge is disposed within a module that is detachably engageable with the base plate, and the therapeutic electrode component further comprises a circuit board disposed within the module and configured to control activation of the gas charge, and signal leads in electrical communication between the circuit board and the gas charge and configured to deliver an activation current to the gas charge.

[0048] In some embodiments, the wearable therapeutic device further comprises a conduit disposed on the base plate providing fluid communication between the coupling and the internal volume of the repository.

[0049] In some embodiments, the repository comprises a plurality of separate chambers each releasably retaining a volume of the conductive fluid and in fluid communication with the conduit.

Description

BRIEF DESCRIPTION OF THE DRAWINGS

[0050] Various aspects of at least one example are discussed below with reference to the accompanying figures, which are not intended to be drawn to scale. The figures are included to provide an illustration and a further understanding of the various aspects and examples, and are incorporated in and constitute a part of this specification, but are not intended to limit the scope of the disclosure. The drawings, together with the remainder of the specification, serve to explain principles and operations of the described and claimed aspects and examples. In the figures, each identical or nearly identical component that is illustrated in various figures is represented by a like numeral. For purposes of clarity, not every component may be labeled in every figure.

[0051] FIG. 1 depicts an example of a wearable medical device;

[0052] FIG. 2A depicts a first view of a medical device controller for the wearable medical device of FIG. 1;

[0053] FIG. 2B depicts a second view of a medical device controller for the wearable medical device of FIG. 1;

[0054] FIG. 2C depicts a component-level view of an example of a medical device controller for the wearable medical device of FIG. 1;

[0055] FIG. 3 depicts an example of a therapeutic electrode component;

[0056] FIG. 4 depicts the therapeutic electrode component of FIG. 3 with a module including a gas charge and circuit board detached from a base plate of the therapeutic electrode component;

[0057] FIG. 5A depicts the module of the therapeutic electrode component of FIG. 3 partially disengaged from the base plate;

[0058] FIG. 5B depicts the module of the therapeutic electrode component of FIG. 3 engaged with the base plate;

[0059] FIG. 6 depicts a circuit board and gas charge disposed within the module of the therapeutic electrode component of FIG. 3;

[0060] FIG. 7 illustrates a conductive fastener providing electrical connection between a conductive lower surface and the circuit board disposed within the module of the therapeutic electrode component of FIG. 3;

[0061] FIG. 8A depicts another example of a therapeutic electrode component;

[0062] FIG. 8B depicts the therapeutic electrode component of FIG. 8A with a module including a gas charge detached from a base plate of the therapeutic electrode component;

[0063] FIG. 9 depicts a gas charge disposed within the module of the therapeutic electrode component of FIG. 8A;

[0064] FIG. 10 depicts the module of the therapeutic electrode component of FIG. 8A engaged with a coupling on a base plate of the therapeutic electrode component;

[0065] FIG. 11 depicts an example gel escape hole with a rupturable ring seal;

[0066] FIG. 12A depicts another example of a therapeutic electrode component;

[0067] FIG. 12B depicts the therapeutic electrode component of FIG. 12A with a module including a gas charge and circuit board detached from a base plate of the therapeutic electrode component;

[0068] FIG. 13 depicts the module of the therapeutic electrode component of FIG. 12A engaged with a coupling on a base plate of the therapeutic electrode component;

[0069] FIG. 14A is an enlarged view of the area of engagement of the module of the therapeutic electrode component of FIG. 12A with the coupling on the base plate of the therapeutic electrode component;

[0070] FIG. 14B is an enlarged view of the area of engagement of the module of the therapeutic electrode component of 12A with the coupling on the base plate of the therapeutic electrode component with the module being unengaged with the coupling;

[0071] FIG. 15A depicts another example of a therapeutic electrode component;

[0072] FIG. 15B depicts the therapeutic electrode component of FIG. 15A with a module including

a gas charge and circuit board detached from the base plate of the therapeutic electrode component; [0073] FIG. **16A** depicts the gas charge and circuit board disposed within the module of the therapeutic electrode component of FIG. **15A**; [0074] FIG. **16B** depicts an underside of the module of the therapeutic electrode component of FIG. **15A**; [0075] FIG. **16C** depicts module of the therapeutic electrode component of FIG. **15A** disposed on the base plate and the outlet of the gas charge pneumatically connected to a coupling on the base plate. [0076] FIG. **17A** depicts another connection mechanism for pneumatically coupling a gas charge to a base plate of a therapeutic electrode component in an exploded view; [0077] FIG. **17B** depicts the mechanism of FIG. **17A** in an assembled state; [0078] FIG. **18A** depicts another connection mechanism for pneumatically coupling a gas charge to a base plate of a therapeutic electrode component; [0079] FIG. **18B** depicts the mechanism of FIG. **18A** disposed in an example of a therapeutic electrode component; and [0080] FIG. **18C** depicts the therapeutic electrode component of FIG. **18B** in an assembled state.

DETAILED DESCRIPTION

[0081] This disclosure relates to devices, systems and methods for delivering electrical therapy to a patient.

[0082] Cardiac monitoring and/or treatment devices include therapy electrode components that release conductive fluid or gel onto the skin of a subject prior to delivering electrical therapy. The gel causes a decrease in electrical resistance between the conductive surface of the therapy electrode and the subject's skin. The deployed gel can help avoid causing burns on the patient's skin during therapy. Further, the deployed gel can cause substantially all or most of the current from the therapeutic electrode components to be delivered to the patient. In implementation, the conductive fluid or gel may have a limited shelf life, for example, due to evaporation of liquid from the conductive fluid or gel. For example, such evaporation can occur through the walls of the receptacle(s) in the therapy electrode components that house the conductive fluid or gel prior to dispensing the fluid or gel. Example devices, systems, and methods are described herein to allow for reuse of non-destroyed portions of a therapeutic electrode. For example, during service, the deteriorated conductive fluid or gel can be removed and remaining therapeutic electrode components can be reused.

[0083] As described further below, one of the therapeutic electrode components that is designed herein to be re-used is a gas charge. A gas charge or cartridge is used in some examples of therapy electrode components to generate pressure to push the conductive fluid or gel out of the receptacle(s) in the therapy electrode components and onto the skin of a patient to reduce electrical resistance between the therapy electrode components and the patient. The gas cartridge can be, in some implementations, an expensive component of a therapy electrode. Conventional therapy electrode components including conductive fluid or gel dispensing systems gas cartridges utilizing gas cartridges as a source of pressure to dispense the conductive fluid or gel do not provide for the gas cartridge to be removed or replaced without damaging the gas cartridge or other portions of the therapy electrode component. Thus, in instances in which, for example, the conductive fluid or gel in a therapy electrode component reaches or exceeds its shelf life or if the therapy electrode component or gas cartridge develops a leak or some other defect that would warrant replacement of the gas cartridge, one cannot remove the gas cartridge and replace it or other portions of the therapy electrode component. Rather, the entire therapy electrode component, including the gas cartridge, is discarded. Example devices, systems, and methods are described herein to allow for reuse of non-destroyed portions of a therapeutic electrode. For example, during service, the deteriorated conductive fluid or gel can be removed and remaining therapeutic electrode components can be reused.

[0084] Examples of devices and systems for delivering electrical therapy to a patient disclosed herein include a therapeutic electrode component for application of electrical stimulus to a subject. The therapeutic electrode component allows for reuse of non-destroyed portions of a therapeutic electrode in application of electrical stimulus to a subject. In examples, the therapeutic electrode component includes a base plate having a first side and a second side opposing the first side. The second side of the therapeutic electrode component has a conductive surface that is disposed directly in contact with the skin of a patient, or indirectly such as through clothing, fabric, and/or a conductive mesh. The conductive surface may be disposed against, for example, a portion of the chest or back of the patient. Electrical therapy may be delivered to the patient through the conductive surface. The first side of the base plate includes a repository having an internal volume configured to releasably retain a conductive fluid that is expelled onto the skin of the patient and provides a low impedance electrical path between the conductive surface of the base plate and the skin of the patient to facilitate the delivery of the electrical therapy to the patient. A rupturable membrane is disposed between the internal volume of the repository and the conductive surface of the base plate which ruptures in response to pressure applied to the conductive fluid and allows the conductive fluid to be expelled onto the skin of the patient.

[0085] In implementations herein, a coupling is disposed on the base plate that allows one to detachably engage a gas charge to the base plate. The gas charge is used to provide the pressure to the conductive fluid when it is desired to expel the conductive fluid onto the skin of the subject. The gas charge is detachable from the coupling without causing destruction of at least the gas charge so that the gas charge may be replaced or removed for use with a different therapeutic electrode component. In examples, the coupling provides a hermetic seal with an outlet of the gas charge to prevent leaks of gas from the gas charge and to direct substantially all gas output from the gas charge to a portion of the therapeutic electrode component where it may apply pressure to the conductive fluid. The coupling, for example, provides fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling. The therapeutic electrode component also includes a retainer configured to detachably secure the gas charge to the base plate.

[0086] Examples of systems for delivering electrical therapy to a patient disclosed herein may include a wearable therapeutic device that allows for reuse of non-destroyed portions of a therapeutic electrode component utilized for application of electrical stimulus to a subject. The wearable therapeutic device includes a garment configured to be worn about the subject. The garment is designed to removably retain at least one therapeutic electrode component as described above. The wearable therapeutic device includes circuitry that is used to provide a therapeutic pulse of energy to the at least one therapeutic electrode component. At least one processor is operatively coupled to the circuitry and the at least one therapeutic electrode component to control operation of the wearable therapeutic device and circuitry. The at least one therapeutic electrode component includes a base plate having a first side and a second side opposing the first side. The second side of the therapeutic electrode component has a conductive surface that may be disposed against the skin of a patient directly, or indirectly such as through clothing, fabric, and/or a conductive mesh, for example, on a portion of the chest or back of the patient, and through which electrical therapy may be delivered to the patient. The first side of the base plate includes a repository having an internal volume configured to releasably retain a conductive fluid that is expelled onto the skin of the patient and provides a low impedance electrical path between the conductive surface of the base plate and the skin of the patient to facilitate the delivery of the electrical therapy to the patient. A rupturable membrane is disposed between the internal volume of the repository and the conductive surface of the base plate which ruptures in response to pressure applied to the conductive fluid and allows the conductive fluid to be expelled onto the skin of the patient. A coupling is disposed on the base plate that allows one to detachably engage a gas charge to the base plate. The gas charge is used to provide the pressure to the conductive fluid when it is desired to expel the conductive fluid

onto the skin of the subject. The gas charge is detachable from the coupling without causing destruction of at least the gas charge so that the gas charge may be replaced or removed for use with a different therapeutic electrode component. The coupling provides a hermetic seal with an outlet of the gas charge to prevent leaks of gas from the gas charge and to direct substantially all gas output from the gas charge to a portion of the therapeutic electrode component where it may apply pressure to the conductive fluid. The coupling, for example, provides fluid communication between the internal volume of the repository and the outlet of gas charge when the gas charge is engaged by the coupling. The therapeutic electrode component includes also includes a retainer configured to detachably secure the gas charge to the base plate.

[0087] Examples of methods for delivery of electrical stimulus to a subject disclosed herein provide for reuse of non-destroyed portions of a therapeutic electrode component used to apply the electrical stimulus to the subject. In one example, the method includes securing a gas charge to a coupling disposed on a first surface of a base plate of a therapeutic electrode component. The coupling provides fluid communication with an internal volume of a repository disposed on the base plate. The repository includes conductive fluid which, prior to delivery of the electrical stimulus to the subject, is dispensed onto a conductive second surface of the base plate through a rupturable membrane disposed between the internal volume of the repository and the conductive surface of the base plate. If one determines that the gas charge should be replaced, for example, due to leakage or for use in a different therapeutic electrode component, the gas charge may be removed from the coupling without causing destruction to the gas charge, and in some examples, without causing damage to at least the base plate, the repository, and the rupturable membrane. One may then secure a replacement gas charge to the coupling or secure the gas charge to a coupling on a base plate of another therapeutic electrode component.

[0088] In another example, a method for delivery of electrical stimulus to a subject that allows for reuse of non-destroyed portions of a therapeutic electrode component used for delivery of the electrical stimulus to the subject includes securing a gas charge to a coupling disposed on a first surface of a base plate of a therapeutic electrode component. The coupling provides fluid communication with an internal volume of a repository disposed on the base plate. The repository is configured to dispense a conductive fluid onto a conductive second surface of the base plate through a rupturable membrane disposed between the internal volume of the repository and the conductive surface of the base plate. If one determines that the gas charge should be replaced, for example, to be moved from the therapeutic electrode component to a second therapeutic electrode component, one may remove the gas charge from the coupling without causing destruction to at least the base plate, the repository, and the rupturable membrane. One might desire to move the gas charge from a first therapeutic electrode component to another, for example if one the conductive fluid in the first therapeutic component is approaching or has exceeded its expiration date or if the hermeticity of the first therapeutic electrode component is in question and the gas charge is still expected to be useable. The method further includes securing the gas charge to a second coupling of the second therapeutic electrode component.

[0089] Advantages of various aspects and embodiments disclosed herein provide for the components of a therapy electrode component including a conductive fluid dispensation system to be non-destructively disassembled. In a therapy electrode component in which conductive fluid has expired, portions of the therapy electrode component, for example, the gas cartridge and/or circuit board and/or a module housing same may be removed, and one or more of these components may be installed onto a replacement base portion of the therapy electrode component including fresh conductive fluid. In another example, in a therapy electrode component in which the conductive gel and other associated components, for example, the base plate, conductive fluid repository, and rupturable membrane are all in useable condition, but the gas cartridge or circuit board are in some way defective, the gas cartridge and/or circuit board may be removed and replaced without damaging the base plate, conductive fluid repository, and rupturable membrane. Accordingly,

portions of therapy electrode components may be replaced if desired to provide a functional therapy electrode component rather than disposing and replacing the entirety of the therapy electrode component.

[0090] Aspects and embodiment disclosed herein thus provide advantages with respect to cost and with respect to the number of replacement parts a user or supplier may keep on hand to maintain the therapy electrode components of a therapy electrode system of a patient in usable or optimal condition.

[0091] As described above, the teachings of the present disclosure can be generally applied to external medical monitoring and/or treatment devices (e.g., devices that are not completely implanted within the patient's body). External medical devices can include, for example, ambulatory medical devices that are capable of and designed for moving with the patient as the patient goes about his or her daily routine. An example ambulatory medical device can be a wearable medical device such as a wearable cardioverter defibrillator (WCD), a wearable cardiac monitoring device, an in-hospital device such as an in-hospital wearable defibrillator, a short-term wearable cardiac monitoring and/or therapeutic device, mobile telemetry devices, and other similar wearable medical devices.

[0092] The wearable medical device can be capable of continuous use by the patient. In some implementations, the continuous use can be substantially or nearly continuous in nature. That is, the wearable medical device may be continuously used, except for sporadic periods during which the use temporarily ceases (e.g., while the patient bathes, while the patient is refit with a new and/or a different garment, while the battery is charged/changed, while the garment is laundered, etc.). Such substantially or nearly continuous use as described herein may nonetheless qualify as continuous use. For example, the wearable medical device can be configured to be worn by a patient for as many as 24 hours a day. In some implementations, the patient may remove the wearable medical device for a short portion of the day (e.g., for half an hour to bathe).

[0093] Further, the wearable medical device can be configured as a long term or extended use medical device. Such devices can be configured to be used by the patient for an extended period of several days, weeks, months, or even years. In some examples, the wearable medical device can be used by a patient for an extended period of at least one week. In some examples, the wearable medical device can be used by a patient for an extended period of at least 30 days. In some examples, the wearable medical device can be used by a patient for an extended period of at least one month. In some examples, the wearable medical device can be used by a patient for an extended period of at least two months. In some examples, the wearable medical device can be used by a patient for an extended period of at least three months. In some examples, the wearable medical device can be used by a patient for an extended period of at least six months. In some examples, the wearable medical device can be used by a patient for an extended period of at least one year. In some implementations, the extended use can be uninterrupted until a physician or other caregiver provides specific instruction to the patient to stop use of the wearable medical device.

[0094] Regardless of the extended period of wear, the use of the wearable medical device can include continuous or nearly continuous wear by the patient as described above. For example, the continuous use can include continuous wear or attachment of the wearable medical device to the patient, e.g., through one or more of the therapy electrode components as described herein, during both periods of monitoring and periods when the device may not be monitoring the patient but is otherwise still worn by or otherwise attached to the patient. The wearable medical device can be configured to continuously monitor the patient for cardiac-related information (e.g., electrocardiogram (ECG) information, including arrhythmia information, heart sounds or heart vibrations, etc.) and/or non-cardiac information (e.g., blood oxygen, the patient's temperature, glucose levels, tissue fluid levels, and/or lung sounds or vibrations). The wearable medical device can carry out its monitoring in periodic or aperiodic time intervals or times. For example, the monitoring during intervals or times can be triggered by a user action or another event.

[0095] As noted above, the wearable medical device can be configured to monitor other physiologic parameters of the patient in addition to cardiac related parameters. The wearable medical device can be configured to monitor, for example, lung vibrations (e.g., using microphones and/or accelerometers), breath vibrations, sleep related parameters (e.g., snoring, sleep apnea), tissue fluids (e.g., using radio-frequency transmitters and sensors), among others.

[0096] Other example wearable medical devices include automated cardiac monitors and/or defibrillators for use in certain specialized conditions and/or environments such as in combat zones or within emergency vehicles. Such devices can be configured so that they can be used immediately (or substantially immediately) in a life-saving emergency. In some examples, the wearable medical devices described herein can be pacing-enabled, e.g., capable of providing therapeutic pacing pulses to the patient.

[0097] In implementations, an example therapeutic medical device can include an in-hospital continuous monitoring defibrillator and/or pacing device, for example, an in-hospital wearable defibrillator. In such an example, the electrodes can be adhesively attached to the patient's skin. For example, the electrodes can include disposable adhesive electrodes. For example, the electrodes can include sensing and therapy components disposed on separate sensing and therapy electrode adhesive patches. In some implementations, both sensing and therapy components can be integrated and disposed on a same electrode adhesive patch that is then attached to the patient. In an example implementation, the electrodes can include a front adhesively attachable therapy electrode, a back adhesively attachable therapy electrode, and a plurality of adhesively attachable sensing electrodes. For example, the front adhesively attachable therapy electrode attaches to the front of the patient's torso to deliver pacing or defibrillating therapy. Similarly, the back adhesively attachable therapy electrode attaches to the back of the patient's torso. In an example scenario, at least three ECG adhesively attachable sensing electrodes can be attached to at least above the patient's chest near the right arm, above the patient's chest near the left arm, and towards the bottom of the patient's chest in a manner prescribed by a trained professional.

[0098] A patient being monitored by an in-hospital defibrillator and/or pacing device may be confined to a hospital bed or room for a significant amount of time (e.g., 90% or more of the patient's stay in the hospital). As a result, a user interface can be configured to interact with a user other than the patient, e.g., a nurse, for device-related functions such as initial device baselining, setting and adjusting patient parameters, and changing the device batteries.

[0099] In implementations, an example of a therapeutic medical device can include a short-term continuous monitoring defibrillator and/or pacing device, for example, a short-term outpatient wearable defibrillator. For example, such a short-term outpatient wearable defibrillator can be prescribed by a physician for patients presenting with syncope. A wearable defibrillator can be configured to monitor patients presenting with syncope by, e.g., analyzing the patient's cardiac activity for aberrant patterns that can indicate abnormal physiological function. For example, such aberrant patterns can occur prior to, during, or after the onset of symptoms. In such an example implementation of the short-term wearable defibrillator, the electrode assembly can be adhesively attached to the patient's skin and have a similar configuration as the in-hospital defibrillator described above.

[0100] In examples, the device can output a defibrillation therapy in the form of a biphasic pulse of between about 0 and 150 Amps. For example, the biphasic waveform is a biphasic truncated exponential waveform. The device can be programmed to provide between around 75 joules to around 150 joules ($\pm 5\%$) at 20° C. (68° F.) when discharged into a 50 ohm resistive load. In implementations, settings within that range can be programmable in 25 joule increments. In an implementation, the device can be configured to deliver around 35 Amps for a maximum joule defibrillating shock delivered into a 50 ohm load. In examples, the defibrillation shock sequence can include between around 1 pulse to around 10 pulses. In examples, the sequence can include around 5 pulses. If conversion of the arrhythmia occurs after a shock, the device automatically

precludes delivery of remaining shocks in the sequence. With respect to pacing therapy, in implementations, a maximum current level of current waveform may be set to a value between approximately 0 mAmps to 200 mAmps. In examples, a pulse width may be set to a fixed value between approximately 0.05 ms to 2 ms. In examples, a frequency of the pulses may be set to a fixed value between approximately 30 pulses per minute (PPM) to approximately 200 PPM. In accordance with one implementation, a 40 ms square wave pulse may be used.

[0101] FIG. 1 illustrates an example of a medical device **100** that is external, ambulatory, and wearable by a patient **102**, and configured to implement one or more configurations described herein. For example, the medical device **100** can be a non-invasive medical device configured to be located substantially external to the patient. Such a medical device **100** can be, for example, an ambulatory medical device that is capable of and designed for moving with the patient as the patient goes about his or her daily routine. For example, the medical device **100** as described herein can be bodily-attached to the patient such as the Life Vest® wearable cardioverter defibrillator available from ZOLL® Medical Corporation. In one example scenario, such wearable defibrillators can be worn nearly continuously or substantially continuously for two to three months at a time. During the period of time in which it is worn by the patient, the wearable defibrillator can be configured to continuously or substantially continuously monitor the vital signs of the patient and, upon determination that treatment is required, can be configured to deliver one or more therapeutic electrical pulses to the patient. For example, such therapeutic shocks can be pacing, defibrillation, or transcutaneous electrical nerve stimulation (TENS) pulses.

[0102] The medical device **100** can include one or more of the following: a garment **110**, one or more sensing electrodes **112** (e.g., ECG electrodes), one or more therapy electrodes **114**, a medical device controller **120**, a connection pod **130**, a patient interface pod **140**, a belt, or any combination of these. In some examples, at least some of the components of the medical device **100** can be configured to be affixed to the garment **110** (or in some examples, permanently integrated into the garment **110**), which can be worn about the patient's torso.

[0103] The medical device controller **120** can be operatively coupled to the sensing electrodes **112**, which can be affixed to the garment **110**, e.g., assembled into the garment **110** or removably attached to the garment, e.g., using hook and loop fasteners. In some implementations, the sensing electrodes **112** can be permanently integrated into the garment **110**. The medical device controller **120** can be operatively coupled to the therapy electrodes **114**. For example, the therapy electrodes **114** can also be assembled into the garment **110**, or, in some implementations, the therapy electrodes **114** can be permanently integrated into the garment **110**.

[0104] Component configurations other than those shown in FIG. 1 are possible. For example, the sensing electrodes **112** can be configured to be attached at various positions about the body of the patient **102**. The sensing electrodes **112** can be operatively coupled to the medical device controller **120** through the connection pod **130**. In some implementations, the sensing electrodes **112** can be adhesively attached to the patient **102**. In some implementations, the sensing electrodes **112** and at least one of the therapy electrodes **114** can be included on a single integrated patch and adhesively applied to the patient's body.

[0105] The sensing electrodes **112** can be configured to detect one or more cardiac signals. Examples of such signals include ECG signals and/or other sensed cardiac physiological signals from the patient. In certain implementations, the sensing electrodes **112** can include additional components such as accelerometers, acoustic signal detecting devices, and other measuring devices for recording additional parameters. For example, the sensing electrodes **112** can also be configured to detect other types of patient physiological parameters and acoustic signals, such as tissue fluid levels, heart vibrations, lung vibrations, respiration vibrations, patient movement, etc. Example sensing electrodes **112** include a metal electrode with an oxide coating such as tantalum pentoxide electrodes, as described in, for example, U.S. Pat. No. 6,253,099 titled "Cardiac Monitoring Electrode Apparatus and Method," the content of which is incorporated herein by reference.

[0106] In some examples, the therapy electrodes **114** can also be configured to include sensors configured to detect ECG signals as well as other physiological signals of the patient. The connection pod **130** can, in some examples, include a signal processor configured to amplify, filter, and digitize these cardiac signals prior to transmitting the cardiac signals to the medical device controller **120**. One or more of the therapy electrodes **114** can be configured to deliver one or more therapeutic defibrillating shocks to the body of the patient **102** when the medical device **100** determines that such treatment is warranted based on the signals detected by the sensing electrodes **112** and processed by the medical device controller **120**. Example therapy electrodes **114** can include conductive metal electrodes such as stainless-steel electrodes that include, in certain implementations, one or more conductive gel deployment devices configured to deliver conductive gel to the metal electrode prior to delivery of a therapeutic shock.

[0107] In some implementations, medical devices as described herein can be configured to switch between a therapeutic medical device and a monitoring medical device that is configured to only monitor a patient (e.g., not provide or perform any therapeutic functions). For example, therapeutic components such as the therapy electrodes **114** and associated circuitry can be optionally decoupled from (or coupled to) or switched out of (or switched in to) the medical device. For example, a medical device can have optional therapeutic elements (e.g., defibrillation and/or pacing electrodes, components, and associated circuitry) that are configured to operate in a therapeutic mode. The optional therapeutic elements can be physically decoupled from the medical device to convert the therapeutic medical device into a monitoring medical device for a specific use (e.g., for operating in a monitoring-only mode) or a patient.

[0108] Alternatively, the optional therapeutic elements can be deactivated (e.g., by a physical or a software switch), essentially rendering the therapeutic medical device a monitoring medical device for a specific physiologic purpose or a particular patient. As an example of a software switch, an authorized person can access a protected user interface of the medical device and select a preconfigured option or perform some other user action via the user interface to deactivate the therapeutic elements of the medical device.

[0109] FIGS. 2A-B illustrate an example medical device controller **120**. For example, the controller **120** includes a connector receptacle **201** for connecting the sensing and/or therapy electrode components to the controller **120**. The controller **120** includes a speaker **203** for providing audio prompts to the patient and/or a bystander. The controller **120** includes circuitry as further described below with reference to FIG. 3. The circuitry is housed within a mechanical housing structure **205** to protect the circuitry and other internal components of the controller **120** from physical damage, particle ingress, and/or water ingress. The controller includes one or more response buttons **211a**, **211b**. A patient wearing the wearable medical device can communicate with the controller **120** via the buttons **211a**, **211b**. For example, if the device detects a life-threatening arrhythmia condition in the patient, the controller **120** can direct the patient to press the one or more buttons **211a**, **211b**. In some examples, the controller **120** can include a display screen **221**. For example, the display screen **221** can be a touch-sensitive panel screen responsive to patient input in the form of touch or physical force applied to the screen. For example, the display screen **221** can display controls and/or prompts to the patient, and is responsive to the patient's touch or application of physical force on the displayed controls. The controller **120** can be powered by a removable battery **210** (see FIG. 2C below) that is housed within a battery chamber **223**.

[0110] FIG. 2C illustrates a sample component-level view of the medical device controller **120** of the medical device **100** of FIG. 1. As shown in FIG. 2C, the medical device controller **120** can include a therapy delivery interface circuit **202**, a data storage **204**, a network interface **206**, a user interface **208**, at least one battery **210**, a sensor interface **212**, a user interface/alarm manager **214**, and least one processor **218**.

[0111] The therapy delivery interface circuit **202** can be coupled to one or more electrodes **220** configured to provide therapy to the patient (e.g., therapy electrodes **114** as described above in

connection with FIG. 1). For example, the therapy delivery interface circuit **202** can include, or be operably connected to, circuitry components that are configured to generate and provide the therapeutic shock. The circuitry components can include, for example, resistors, capacitors, relays and/or switches, electrical bridges such as an H-bridge (e.g., including a plurality of insulated gate bipolar transistors or IGBTs), voltage and/or current measuring components, and other similar circuitry components arranged and connected such that the circuitry components work in concert with the therapy delivery circuit and under control of one or more processors (e.g., processor **218**) to provide, for example, one or more pacing or defibrillation therapeutic pulses.

[0112] Pacing pulses can be used to treat cardiac arrhythmias such as bradycardia (e.g., less than 30 beats per minute) and tachycardia (e.g., more than 150 beats per minute) using, for example, fixed rate pacing, demand pacing, anti-tachycardia pacing, and the like. Defibrillation pulses can be used to treat ventricular tachycardia and/or ventricular fibrillation.

[0113] The capacitors can include a parallel-connected capacitor bank consisting of a plurality of capacitors (e.g., two, three, four or more capacitors). These capacitors can be switched into a series connection during discharge for a defibrillation pulse. For example, four capacitors of approximately 650 uF can be used. The capacitors can have between 350 to 500 volt surge rating and can be charged in approximately 15 to 30 seconds from a battery pack.

[0114] For example, each defibrillation pulse can deliver between 60 to 180 joules of energy. In some implementations, the defibrillating pulse can be a biphasic truncated exponential waveform, whereby the signal can switch between a positive and a negative portion (e.g., charge directions). This type of waveform can be effective at defibrillating patients at lower energy levels when compared to other types of defibrillation pulses (e.g., such as monophasic pulses). For example, an amplitude and a width of the two phases of the energy waveform can be automatically adjusted to deliver a precise energy amount (e.g., 150 joules) regardless of the patient's body impedance. The therapy delivery interface circuit **202** can be configured to perform the switching and pulse delivery operations, e.g., under control of the processor **218**. As the energy is delivered to the patient, the amount of energy being delivered can be tracked. For example, the amount of energy can be kept to a predetermined constant value even as the pulse waveform is dynamically controlled based on factors such as the patient's body impedance to which the pulse is being delivered.

[0115] The data storage **204** can include one or more of non-transitory computer readable media, such as flash memory, solid state memory, magnetic memory, optical memory, cache memory, combinations thereof, and others. The data storage **204** can be configured to store executable instructions and data used for operation of the medical device controller **120**. In certain implementations, the data storage can include executable instructions that, when executed, are configured to cause the at least one processor **218** to perform one or more functions.

[0116] In some examples, the network interface **206** can facilitate the communication of information between the medical device controller **120** and one or more other devices or entities over a communications network. For example, where the medical device controller **120** is included in an ambulatory medical device (such as medical device **100**), the network interface **206** can be configured to communicate with a remote computing device such as a remote server or other similar computing device. The network interface **206** can include communications circuitry for transmitting data in accordance with a Bluetooth® wireless standard for exchanging such data over short distances to an intermediary device(s) (e.g., a base station, a “hotspot” device, a smartphone, a tablet, a portable computing device, and/or other devices in proximity of the wearable medical device **100**). The intermediary device(s) may in turn communicate the data to a remote server over a broadband cellular network communications link. The communications link may implement broadband cellular technology (e.g., 2.5G, 2.75G, 3G, 4G, 5G cellular standards) and/or Long-Term Evolution (LTE) technology or GSM/EDGE and UMTS/HSPA technologies for high-speed wireless communication. In some implementations, the intermediary device(s) may communicate with a remote server over a Wi-Fi™ communications link based on the IEEE 802.11 standard.

[0117] In certain implementations, the user interface **208** can include one or more physical interface devices such as input devices, output devices, and combination input/output devices and a software stack configured to drive operation of the devices. These user interface elements may render visual, audio, and/or tactile content. Thus, the user interface **208** may receive input or provide output, thereby enabling a user to interact with the medical device controller **120**.

[0118] The medical device controller **120** can also include at least one battery **210** configured to provide power to one or more components integrated in the medical device controller **120**. The battery **210** can include a rechargeable multi-cell battery pack. In one example implementation, the battery **210** can include three or more 2200 mAh lithium ion cells that provide electrical power to the other device components within the medical device controller **120**. For example, the battery **210** can provide its power output in a range of between 20 mA to 1000 mA (e.g., 40 mA) output and can support 24 hours, 48 hours, 72 hours, or more, of runtime between charges. In certain implementations, the battery capacity, runtime, and type (e.g., lithium ion, nickel-cadmium, or nickel-metal hydride) can be changed to best fit the specific application of the medical device controller **120**.

[0119] The sensor interface **212** can be coupled to one or more sensors configured to monitor one or more physiological parameters of the patient. As shown, the sensors may be coupled to the medical device controller **120** via a wired or wireless connection. The sensors can include one or more electrocardiogram (ECG) electrodes **222** (e.g., similar to sensing electrodes **112** as described above in connection with FIG. 1).

[0120] The ECG electrodes **222** can monitor a patient's ECG information. For example, the ECG electrodes **222** can be galvanic (e.g., conductive) and/or capacitive electrodes configured to measure changes in a patient's electrophysiology to measure the patient's ECG information. The ECG electrodes **222** can transmit information descriptive of the ECG signals to the sensor interface **212** for subsequent analysis.

[0121] The sensor interface **212** can be coupled to any one or combination of sensing electrodes/other sensors to receive other patient data indicative of patient parameters. Once data from the sensors has been received by the sensor interface **212**, the data can be directed by the at least one processor **218** to an appropriate component within the medical device controller **120**. For example, if ECG data is collected by sensing electrode **222** and transmitted to the sensor interface **212**, the sensor interface **212** can transmit the data to the at least one processor **218** which, in turn, relays the data to a cardiac event detector. The cardiac event data can also be stored on the data storage **204**.

[0122] In certain implementations, the user interface/alarm manager **214** can be configured to manage alarm profiles and notify one or more intended recipients of events specified within the alarm profiles as being of interest to the intended recipients. These intended recipients can include external entities such as users (patients, physicians, and monitoring personnel) as well as computer systems (monitoring systems or emergency response systems). The user interface/alarm manager **214** can be implemented using hardware or a combination of hardware and software. For instance, in some examples, the user interface/alarm manager **214** can be implemented as a software component that is stored within the data storage **204** and executed by the at least one processor **218**. In this example, the instructions included in the alarm manager **214** can cause the at least one processor **218** to configure alarm profiles and notify intended recipients using the alarm profiles. In other examples, alarm manager **214** can be an application-specific integrated circuit (ASIC) that is coupled to the at least one processor **218** and configured to manage alarm profiles and notify intended recipients using alarms specified within the alarm profiles. Thus, examples of alarm manager **214** are not limited to a particular hardware or software implementation.

[0123] In some implementations, the at least one processor **218** includes one or more processors (or one or more processor cores) that each are configured to perform a series of instructions that result in manipulated data and/or control the operation of the other components of the medical device

controller **120**. In some implementations, when executing a specific process (e.g., cardiac monitoring), the at least one processor **218** can be configured to make specific logic-based determinations based on input data received, and be further configured to provide one or more outputs that can be used to control or otherwise inform subsequent processing to be carried out by the at least one processor **218** and/or other processors or circuitry with which the at least one processor **218** is communicatively coupled. Thus, the at least one processor **218** reacts to specific input stimulus in a specific way and generates a corresponding output based on that input stimulus. In some examples, the at least one processor **218** can proceed through a sequence of logical transitions in which various internal register states and/or other bit cell states internal or external to the at least one processor **218** may be set to logic high or logic low. As referred to herein, the at least one processor **218** can be configured to execute a function where software is stored in a data store coupled to the at least one processor **218**, the software being configured to cause the at least one processor **218** to proceed through a sequence of various logic decisions that result in the function being executed. The various components that are described herein as being executable by the at least one processor **218** can be implemented in various forms of specialized hardware, software, or a combination thereof. For example, the processor can be a digital signal processor (DSP) such as a 24-bit DSP processor. The at least one processor can be or include a multi-core processor, e.g., having two or more processing cores. The processor can be an Advanced RISC Machine (ARM) processor such as a 32-bit ARM processor. The at least one processor can execute an embedded operating system, and include services provided by the operating system that can be used for file system manipulation, display and audio generation, basic networking, firewalling, data encryption and communications.

[0124] One embodiment of a therapeutic electrode component is illustrated in FIGS. 3-7, indicated generally as **300**. The therapeutic electrode component **300** includes a base plate **305** having a first side **305A** and a second side **305B** opposing the first side. The second side **305B** includes a conductive surface **410** (see FIG. 7). One or more repositories **310**, ten in the embodiment illustrated in FIGS. 3-7, are disposed on the first side **305A** of the base plate **305**. The repositories **310** have an internal volume that releasably retains a conductive fluid **315**.

[0125] Referring briefly to FIG. 11, a rupturable membrane **340**, e.g., in the form of a rupturable ring seal, is disposed between the internal volume of each repository **310** and the conductive surface **410** of the base plate **305**. When the rupturable membrane **340** is ruptured, the fluid **315** flows from the internal volume on to the conductive surface **410** via the fluid or gel escape hole **343**. The respective rupturable membranes **340** associated with each respective repository **310** are configured to rupture responsive to pressure being applied to the internal volumes of the repositories **310** so that the conductive fluid **315** can flow out of the repositories **310** and onto the conductive surface **410** of the second side **305B** of the base plate **305**. Each repository **310** is associated with a fluid or gel escape hole **343** to allow for the fluid or gel to escape on to the conductive surface.

[0126] Referring back to FIGS. 3-7, a conduit **320** is disposed on the base plate **305**. The conduit **320** is in fluid communication between the internal volumes of each repository **310** and a coupling **330** (see FIG. 4). The conduit **320** includes a central portion **320A** and branches **320B** leading to each respective repository **310**. The conduit provides for fluid to flow from the coupling **330** to the internal volumes of the repositories **310** to pressurize the internal volumes of the repositories **310** and cause the rupturable membrane **340** to rupture and the conductive fluid **315** to be pushed out of the repositories **310** through the ruptured rupturable membrane **340** via the fluid or gel escape holes **343**.

[0127] A removable module **325** is detachably engageable with the base plate **305**. As illustrated in FIGS. 5A-7, the module **325** houses a gas charge **365** and a circuit board **385**. The gas charge **365** is a source of pressurized gas that, when the gas charge **365** is activated, causes gas to flow through the coupling **330** and conduit **320** to pressurize the internal volumes of the repositories **310** and

cause the conductive fluid **315** to be dispensed. The circuit board **385** provides communication with an external controller, for example, medical device controller **120** illustrated in FIGS. **1**, **2A**, and **2B**, and controls activation of the gas charge **365** and delivery of electrical therapy to a patient. [0128] The therapeutic electrode component **300** is illustrated in FIG. **4** with the module **325** removed. As illustrated in FIG. **4**, a cradle **335** is coupled to the first side **305A** of the base plate **305**. The cradle **335** is sized and shaped to releasably retain the removable module **325**. The cradle **335** includes a retainer that detachably engages the module **325**. In the embodiment illustrated in FIG. **4** the retainer is in the form of clips **345** that releasably engage slots **350** (see FIG. **5A**) on the module **325**. In other embodiments, the clips **345** may be included on the module **325** and the slots **350** on the cradle.

[0129] Also visible in FIG. **4** is the coupling **330**. The coupling **330** includes a barb **355** having an internal pneumatic conduit **360** (see FIGS. **5A**, **5B**) that provides fluid communication between the internal volumes of the repositories **310** and the outlet of gas charge **365** via the conduit **320** when the gas charge **365** is engaged by the coupling **330**. In the embodiment illustrated in FIG. **4**, the barb **355** extends in a direction parallel to a plane defined by the first side **305A** of the base plate **305**.

[0130] FIGS. **5A** and **5B** illustrate the module **325** disposed on the cradle **335** and without its top cover. In FIG. **5A** the clips **345** of the cradle are not engaged with the slots **350** on the module. If the module **325** is slid to the left in a plane defined by the surface of the first side **305A** of the base plate **305** from the position shown in FIG. **5A** to that shown in FIG. **5B**, the clips **345** engage the slots **350** to retain the module **325** in the cradle **335**. The slots **350** of the module **325** are not visible in FIG. **5B** because they are underneath the clips **345**.

[0131] Disposed within the module **325** is the gas charge **365**. The gas charge **365** may be fixed in place in the module **325** by, for example, an adhesive or one or more fasteners. A connector **370** formed of a resilient material, for example, rubber includes a conduit **375** that has a first opening **375A** that engages the barb **355** of the coupling **330** when the module **325** is in the engaged position illustrated in FIG. **5B**. The conduit **375** of the connector **370** also has a second opening **375B** that receives and retains an outlet **380** of the gas charge **365**. The coupling **330** engages the gas charge **365** via the connector **370**. The gas charge **365** may be detached from the coupling **330** by sliding the module **325** from the position illustrated in FIG. **5B** to the position illustrated in FIG. **5A**. When the gas charge **365** is engaged with the coupling **330** the coupling **330** provides a hermetic seal with the outlet **380** of the gas charge **365** and provides fluid communication between the internal volumes of the repositories **310** and the outlet **380** of gas charge **365**.

[0132] A circuit board **385** is also disposed within the removable module **325**, as illustrated in FIG. **6**. As discussed above, the circuit board **385** provides communication with an external controller, for example, medical device controller **120** illustrated in FIGS. **1**, **2A**, and **2B**, and controls activation of the gas charge **365** and delivery of electrical therapy to a patient through the conductive surface **410** of the base plate **305** of the therapeutic electrode component **300**. An electrical signal lead **390** extends from the circuit board to the gas cartridge **365** for providing an activation current to the gas charge **365**. One or more apertures **395** including or surrounded by an electrical contact is provided in the circuit board **385** for outputting electrical pulses to be delivered to a patient for electrical therapy. In examples, the activation current can be at least 0.1 mA. In some applications, the activation current can be in a range from between around 0.1 mA to around 1 A. In an implementation, the activation current can be between around 0.01 A to around 0.3 A. For example, the activation current comprises a pulse of between around 1 ms and 75 seconds. In examples, the activation current comprises a pulse of around 10 ms to around 30 seconds. An operating range in which the above activation current parameters were tested is between around -25 F and 160 F.

[0133] The therapeutic electrode component **300** further includes one or more conductive fasteners **405**, as illustrated in FIG. **7**, that engage or pass through the one or more apertures **395** in the

circuit board **385**, through one or more aperture **397A** in the module **325**, and through one or more aperture **397B** in the base plate **305**. One or more of the apertures **395**, **397A**, **397B** may be threaded to facilitate retention of the conductive fastener or fasteners **405**. The conductive fastener or fasteners **405** makes an electrical connection with the electrical contact of the aperture **395** of the circuit board **385** on a first end and makes an electrical connection with the conductive surface **410** of the base plate **305** of the therapeutic electrode component **300** on a second end. The conductive fastener or fasteners **405** thus provide electrical communication between the circuit board **385** and the conductive surface **410** of the base plate **305** of the therapeutic electrode component **300**. The conductive fastener or fasteners **405** is configured to deliver one of a defibrillation pulse or a pacing pulse to a subject through the conductive surface **410** of the base plate **305**. The conductive fastener or fasteners **405** also secure the module **325** in place in the cradle **335** on the base plate **305**. The one or more conductive fasteners **405** electrically engage the conductive surface **410** of the base plate **305** when securing module **325** to the base plate **305**.

[0134] Another embodiment of a therapeutic electrode component is illustrated in FIGS. **8A-10**, indicated generally at **900**. The therapeutic electrode component **900** includes many of the same features as the therapeutic electrode component **300**. Features of the therapeutic electrode component **900** that are similar to those of the therapeutic electrode component **300** are indicated with similar reference numbers as used for the therapeutic electrode component **300** but with the reference numbers beginning with a “9” instead of a “3.” The therapeutic electrode component **900** includes, for example, a base plate **905** having a first side **905A** and a second side **905B** opposing the first side that corresponds with the base plate **305** of the therapeutic electrode component **300**. The second side **905B** includes a conductive surface **1010** (see FIG. **10**) corresponding to the conductive surface **410** of the therapeutic electrode component **300**. The therapeutic electrode component **900** includes repositories **910** corresponding to the repositories **310** of the therapeutic electrode component **300** disposed on the first side **905A** of the base plate **905**. The repositories **910** have an internal volume that releasably retains a conductive fluid **915**, corresponding to the conductive fluid **315** of the therapeutic electrode component **300**. The conductive fluid **915** is releasably retained within the internal volumes of the repositories by rupturable membranes corresponding to the rupturable membranes **340** of the therapeutic electrode component **300**. The therapeutic electrode component **900** further includes a conduit **920** disposed on the base plate **905** that corresponds to the conduit **320** and has a central portion **920A** and branches **920B**, corresponding to the central portion **320A** and branches **320B** of the therapeutic electrode component **300**.

[0135] The module of the therapeutic electrode component **900** includes a first portion **925A** that is fixed to the base plate **905** and that includes a circuit board corresponding to the circuit board **385** of the therapeutic electrode component **300**. The circuit board of the therapeutic electrode component **900** is electrically coupled to the conductive surface **1010** of the second side **905B** of the base plate **905** of the therapeutic electrode component **900**, for example, with one or more conductive fasteners corresponding to the one or more conductive fasteners **405** of the therapeutic electrode component **300**.

[0136] A second portion **925B** of the module of the therapeutic electrode component **900** includes a gas charge **965** corresponding to the gas charge **365** of the therapeutic electrode component **300**. The second portion **925B** of the module is detachably engageable with the base plate **905** and with a coupling **930** that provides fluid communication between the internal volumes of the repositories **910** and the outlet of gas charge **965** via the conduit **920** when the gas charge **965** is engaged by the coupling **930**. The second portion **925B** of the module includes one or more tabs or clips **945** that releasably engage one or more apertures or slots **950** in walls **952** coupled to the base plate **905**, and optionally formed integral with the first portion **925A**, that define a cradle for the second portion and that removably retain the second portion **925B** on the base plate **905**.

[0137] As illustrated in FIG. **9**, the second portion **925B** of the module retains a gas cartridge **965**

that includes an electrical signal lead **990** that electrically connects the circuit board (e.g., similar to circuit board **385** of FIG. **6**) within the first portion **925A** of the module to the gas cartridge **965** for providing an activation current to the gas charge **965**. The signal lead **990** can be connected to the circuit board via solder pads. For example, an electrical connection between the signal lead **990** and circuit board components can be made through a two-position connector. For example, a two-position connector can include a wire-to-wire connector with leads on one side going connected to the gas cartridge **965**, and leads on the other side of the connector coupled to solder pads on the circuit board. An end of the gas cartridge **965** including the output of the gas cartridge **965** is engaged by a resilient body **970** formed of a resilient material, for example, rubber. The resilient body **970** includes a recess **972**, for example, a cylindrically shaped recess in fluid communication with the outlet of the gas cartridge **965**.

[0138] As shown in further detail in FIG. **10**, the coupling **930** includes a pneumatic header **934** that is in fluid communication with the outlet of the gas charge **965** via the connector **970**. The pneumatic header **934** is received within the resilient body **970** coupled to the gas charge **965**. The pneumatic header **934** is fixed to and inseparable from the base plate **905**. In such an implementation, the resilient body **970** slides down over the pneumatic header making a radial seal when the gas charge **965** is installed.

[0139] The pneumatic header **934** includes an external side wall or walls **932** that are sealed to an internal wall or walls **974** of the recess **972** of the resilient body **970**. In some implementations, an adhesive is dispersed within the internal wall or walls **974** of the recess **972** and the external side wall or walls **932** of the pneumatic header **934**.

[0140] The pneumatic header **934** includes an internal fluid conduit **960** for flowing gas released from the gas charge **965** into the conduit **920**. The coupling **930** also includes a snap ring **936** that is coupled to the first side **905A** of the base plate **905**. The snap ring **936** may be disposed and retained in place below a layer of plastic material **908** that covers the first side **905A** of the base plate **905** and the repositories **910**. In an implementation, the snap ring **936** is fixed to and inseparable from the base plate **905**. In an implementation, the snap ring **936** is sized and shaped to receive and releasably retain the pneumatic header **934**. An O-ring **938** is disposed between the snap ring **936** and pneumatic header **934** when the gas charge **965** is engaged with the coupling **930** and enhances hermeticity of a seal between the snap ring **936** and pneumatic header **934**. In an example, the snap ring **936** stays with the base plate when the second portion **925B** is removed. In some examples, both the snap ring **936** and the O-ring **938** stay with the base plate when the second portion **925B** is removed.

[0141] Another embodiment of a therapeutic electrode component is illustrated in FIGS. **12A-14B**, indicated generally at **1200**. The therapeutic electrode component **1200** includes many of the same features as the therapeutic electrode component **300**. Features of the therapeutic electrode component **1200** that are similar to those of the therapeutic electrode component **300** are indicated with similar reference numbers as used for the therapeutic electrode component **300** but with the reference numbers beginning with a “12” instead of a “3.” The therapeutic electrode component **1200** includes, for example, a base plate **1205** having a first side **1205A** and a second side **1205B** opposing the first side that corresponds with the base plate **305** of the therapeutic electrode component **300**. The second side **1205B** includes a conductive surface **1310** corresponding to the conductive surface **410** of the therapeutic electrode component **300**. The therapeutic electrode component **1200** includes repositories **1210** corresponding to the repositories **310** of the therapeutic electrode component **300** disposed on the first side **1205A** of the base plate **1205**. The repositories **1210** have internal volumes that releasably retain a conductive fluid **1215**, corresponding to the conductive fluid **315** of the therapeutic electrode component **300**. The conductive fluid **1215** is releasably retained within the internal volumes of the repositories by rupturable membranes corresponding to the rupturable membranes **340** of the therapeutic electrode component **300**. The therapeutic electrode component **1200** further includes a conduit **1220** disposed on the base plate

1205 that corresponds to the conduit **320** and has a central portion **1220A** and branches **1220B**, corresponding to the central portion **320A** and branches **320B** of the therapeutic electrode component **300**.

[0142] A removable module **1225** is detachably engageable with the base plate **1205**. The module **1225** houses a gas charge **1265** and a circuit board **1285**, corresponding to the gas charge **365** and circuit board **385**, respectively, of the therapeutic electrode component **300**. The gas cartridge **1265** that includes an electrical signal lead **1290** that electrically connects the circuit board **1285** within the module **1225** to the gas cartridge **1265** for providing an activation current to the gas charge **1265**. The module **1225** is illustrated without a cover to show the gas charge **1265** and circuit board **1285** contained within, but in use, would include a cover. When the module **1225** is removably secured to the base plate **1205**, the circuit board **1285** of the therapeutic electrode component **1200** may be electrically coupled to the conductive surface **1310** of the second side **1205B** of the base plate **1205** of the therapeutic electrode component **1200**, for example, with one or more conductive fasteners corresponding to the one or more conductive fasteners **405** of the therapeutic electrode component **300**.

[0143] The module **1225** is detachably engageable with the base plate **1205** and from a coupling **1230** that provides fluid communication between the internal volumes of the repositories **1210** and the outlet of gas charge **1265** via the conduit **1220** when the gas charge **1265** is engaged by the coupling **1230**. The therapeutic electrode component **1200** is illustrated in FIG. 12B with the module **1225** removed and the coupling **1230** visible. The module **1225** is removed and placed onto the base plate **1205** by pulling or pushing the module **1225** in a direction normal to a plane defined by the first side **1205A** or second side **1205B** of the base plate **1205**. Installing or removing the module **1225** from the base plate **1205** causes an aperture **1275** in a lower surface **1225B** of the module **1225** to engage or disengage the coupling **1230**.

[0144] As illustrated in further detail in FIGS. 13, 14A, and 14B, the coupling **1230** includes a post **1234** disposed on the first side **1205A** of the base plate **1205** and including a pneumatic conduit **1260** configured to provide the fluid communication between the internal volume of the repositories **1210** and the outlet of gas charge **1265** when the gas charge **1265** is engaged by the coupling **1230**. The post **1234** is sized and shaped to engage the aperture **1275** in the module **1225**. The post **1234** may include a flange portion that is disposed below and retained in place by a layer of plastic material **1208** that covers the first side **1205A** of the base plate **1205** and the repositories **1210**. An O-ring **1238** is disposed between a neck of the pneumatic conduit **1260** defined in the post **1234** and the aperture **1275** in the module **1225**. The O-ring **1238** enhances hermeticity of a seal between the pneumatic conduit **126** defined in the post **1234** and module **1225**.

[0145] The module **1225** can be secured to the base plate **1205** with one or more screws. For example, the one or more screws can include threaded inserts or self-tapping screws. In examples, the module **1225** can be secured to the base plate **1205** with screws that are inserted from the conductive side of the base plate **1205** and pass through the layers of the base plate **1205** and tighten into corresponding screw bosses in the module **1225**.

[0146] Another embodiment of a therapeutic electrode component is illustrated in FIGS. 15A-16C, indicated generally at **1500**. The therapeutic electrode component **1500** includes many of the same features as the therapeutic electrode component **300**. Features of the therapeutic electrode component **1500** that are similar to those of the therapeutic electrode component **300** are indicated with similar reference numbers as used for the therapeutic electrode component **300** but with the reference numbers beginning with a “15” instead of a “3.” The therapeutic electrode component **1500** includes, for example, a base plate **1505** having a first side **1505A** and a second side **1505B** opposing the first side that corresponds with the base plate **305** of the therapeutic electrode component **300**. The second side **1505B** includes a conductive surface **1610** corresponding to the conductive surface **410** of the therapeutic electrode component **300**. The therapeutic electrode component **1500** includes repositories **1510** corresponding to the repositories **310** of the therapeutic

electrode component **300** disposed on the first side **1505A** of the base plate **1505**. The repositories **1510** have internal volumes that releasably retain a conductive fluid **1515**, corresponding to the conductive fluid **315** of the therapeutic electrode component **300**. The conductive fluid **1515** is releasably retained within the internal volumes of the repositories by rupturable membranes corresponding to the rupturable membranes **340** of the therapeutic electrode component **300**. The therapeutic electrode component **1500** further includes a conduit **1520** disposed on the base plate **1505** that corresponds to the conduit **320** and has a central portion **1520A** and branches **1520B**, corresponding to the central portion **320A** and branches **320B** of the therapeutic electrode component **300**.

[0147] The therapeutic electrode component **1500** includes a module **1525** detachably engaged with the base plate **1505**. The module **1525** includes a first body **1525A** and a second body **1525B**. As illustrated in FIGS. **16A** and **16C**, the first body **1525A** houses a gas charge **1565** and a circuit board **1585** which correspond to the gas charge **365** and circuit board **385** of the therapeutic electrode component **300**.

[0148] The therapeutic electrode component **1500** is illustrated in FIG. **15B** with the module **1525** removed. As illustrated in FIG. **15B**, a cradle **1535** is coupled to the first side **1505A** of the base plate **1505**. The cradle **1535** is sized and shaped to releasably retain the removable module **1525**. The cradle **1535** includes a retainer that detachably engages the module **1525**. In the embodiment illustrated in FIG. **15B** the retainer is in the form of clips **1545** that releasably engage recesses **1550** (see FIGS. **16A**, **16B**) on the module **1525**. To engage the module **1525** with the cradle **1535** and base plate **1505**, the module **1525** is pushed downward in a direction normal to a plane defined by the base plate **1505** into the cradle **1535** until the clips **1545** of the cradle **1535** engage the recesses **1550** of the module **1525**. The module **1525** may be removed from the cradle **1535** and base plate **1505** by pulling upward on the module **1525** with sufficient force to cause the clips **1545** of the cradle **1535** to disengage the recesses **1550** of the module **1525** and release the module **1525** from the cradle **1535**. In other embodiments, the clips **1545** may be included on the module **1525** and the recesses **1550** on the cradle clips. A portion of the conduit **1520** may be formed by a channel defined in the cradle **1535**.

[0149] Also visible in FIGS. **15B** and **16C** is a coupling **1530**. The coupling **1530** includes a barb **1555** that provides fluid communication between the internal volumes of the repositories **1510** and the outlet of gas charge **1565** via the conduit **1520** when the gas charge **1565** is engaged by the coupling **1530**. In the embodiment illustrated in FIGS. **15B** and **16C**, the barb **355** extends in a direction parallel to a plane defined by the first side **305A** of the base plate **305**. The module **1525** may be removed and replaced from the cradle **1535** and base plate **1505** without damaging the coupling **1530**.

[0150] As illustrated in FIGS. **16B** and **16C**, an outlet **1580** of the gas charge **1565** extends through a wall **1525D** separating an internal volume of the first body **1525A** of the module **1525** from a chamber **1525C** defined in the second body **1525B** of the module **1525**. A short length of pneumatic tubing **1570** engages the barb **1555** of the coupling **1530** and the outlet **1580** of the gas charge **1565** and provides fluid communication between the internal volumes of the repositories **1510** and the outlet **1580** of gas charge **1565** via the coupling **1530** and conduit **1520**.

[0151] The circuit board **1585** includes one or more apertures **1595**, corresponding to the one or more apertures **395** of the therapeutic electrode component **300**, that include or are surrounded by an electrical contact for outputting electrical pulses to be delivered to a patient for electrical therapy. One or more conductive fasteners, corresponding to the one or more conductive fasteners **405** of the therapeutic electrode component **300**, may engage or pass through the one or more apertures **1595** in the circuit board **1585**, through one or more aperture **1597** in the cradle **1535**, one or more apertures (not shown) in the module **1525**, and through one or more apertures (not shown) in the base plate **1505**. One or more of the apertures in the circuit board **1585**, base plate **1505**, and/or module **1525** may be threaded to facilitate retention of the conductive fastener or fasteners.

The conductive fastener or fasteners makes an electrical connection with the electrical contact of the aperture **1595** of the circuit board **1585** on a first end and makes an electrical connection with the conductive surface **1610** of the base plate **1505** of the therapeutic electrode component **1500** on a second end. The conductive fastener or fasteners thus provide electrical communication between the circuit board **1585** and the conductive surface **1610** of the base plate **1505** of the therapeutic electrode component **300**. The conductive fastener or fasteners is configured to deliver one of a defibrillation pulse or a pacing pulse to a subject through the conductive surface **1610** of the base plate **1505**. The conductive fastener or fasteners may also help secure the module **1525** in place in the cradle **1535** on the base plate **1505**. The one or more conductive fasteners electrically engage the conductive surface **1610** of the base plate **1505** when securing module **1525** to the base plate **1505**.

[0152] Another example of a coupling for pneumatically connecting a gas charge to a conduit in fluid communication with internal volumes of one or more repositories in a therapeutic electrode component as disclosed herein is illustrated in FIGS. **17A** and **17B**, indicated generally at **1700**. The coupling **1700** is illustrated along with a gas charge **1775** having an outlet **1780** in the form of a tube, for example, a stainless steel tube, in an exploded view in FIG. **17A**, and in an assembled view in FIG. **17B**. The coupling includes a feed-through **1705** that has a neck **1710** defining an interior volume **1715**. The feed-through **1705** also includes an aperture **1720** to provide fluid communication between the gas charge **1775** and one or more conductive fluid repositories via a conduit of a therapeutic electrode component as disclosed herein. An O-ring **1725** fits around and surrounds the neck **1710** of the feed-through **1705**. The coupling **1700** further includes a washer **1730** formed of a resilient material that surrounds a length of the outlet **1780** of the gas charge **1775** and is configured to be retained within the internal volume **1715** of the neck **1710** of the feed-through **1705**. A snap ring **1735** couples to the feed through **1705** and traps the O-ring **1725** between the snap ring **1735** and the feed-through **1705**. The internal wall of the neck **1710** of the feed-through **1705** may compress the washer **1730** to facilitate forming a hermetic seal between the outlet **1780** of the gas charge **1775** and the aperture **1720** of the feed-through **1705**. The snap ring **1735** may compress the neck **1710** of the feed-through **1705** to help compress the washer **1730**. In some embodiments, the coupling **1700** may be secured to a base plate **1805** of a therapeutic electrode component as disclosed herein by a plastic film **1810** that covers the O-ring **1725** and flange portion **1740** of the feed-through **1705**.

[0153] Another example of a coupling for pneumatically connecting a gas charge to a conduit in fluid communication with internal volumes of one or more repositories in a therapeutic electrode component as disclosed herein is illustrated in FIG. **18A**, indicated generally at **1900**. The coupling **1900** includes a snap ring **1905** coupled to the first side of the base plate **2005** of a therapeutic electrode component as disclosed herein. The snap ring **1905** may be secured to the base plate **2005** by a layer of plastic material **2010** that covers the surface of the base plate **2005**. The coupling **1900** also includes a feed-through **1910** including a base **1910A** that surrounds an end portion of the gas charge **2065** and the outlet **2080** of the gas charge **2065**, and a barb **1910B** extending from the base **1910A** that is configured to releasably engage the snap ring **1905**. An O-ring **1915** is disposed between the base **1910A** and the snap ring **1905** when the barb **1910B** is engaged with the snap ring **1905**. The O-ring **1915** enhances hermeticity of a seal between the feed-through **1910** and snap ring **1905**. A second O-ring **1915** may be disposed on an inner wall or in a recessed region of the base **1910A** to facilitate forming a hermetic seal between the gas charge **2065** and the feed-through **1910**.

[0154] When sealing with O-rings in the manner described herein, a hermetic seal is achieved. An O-ring is a doughnut-shaped object or torus. In application, the opposite sides of an O-ring are squeezed between the walls of the space into which the O-ring is installed. The resulting zero clearance within the space provides an effective seal, blocking the flow of liquids or gases through the space's internal passage. An O-ring is typically defined by its dimensions (e.g., based on inside

hole diameter, ID, and cross section), durometer (Shore A hardness), and material composition. For example, the O-ring can be from any of the following materials. In implementations herein, the O-ring installation incorporates initial O-ring compression. At atmospheric pressure, the inherent resiliency of the compressed O-ring provides the seal. As system pressure activates the seal, the O-ring is forced to the low pressure side of the space. Designed to deform, the O-ring thus fill the diametrical clearance and blocks leakage to form the hermetic seal. For example, the O-ring can be Buna-N/Nitrile rubber, a copolymer of butadiene and acrylonitrile. Nitrile combines resistance to petroleum-based oils and fuels, silicone greases, hydraulic fluids, water and alcohols. It has a low compression set, high tensile strength and high abrasion resistance. The O-ring can be made from a compound in the ethylene-propylene (EPM/EPDM) family. Such materials feature good resistance to such polar solvents as ketones (e.g., acetone). EPM/EPDM is resistant to steam (e.g., up to 400° F.), hot water, silicone oils and greases, dilute acids and alkalis, alcohols and automotive brake fluids. Ethylene propylene can provide extended temperature range of around -76° F. to around +350° F. The O-ring can be made from a compound in the silicone family. Silicone material is resistant to high, dry heat. Silicones are fungus resistant, odorless, tasteless, non-toxic elastomers and possess high-resistance to the aging effects of both sunlight and ozone. The O-ring can be made from a compound in the neoprene family. Neoprene features moderate resistance to petroleum oils, good resistance to ozone, sunlight and oxygen aging, relatively low compression set, good resilience, reasonable cost, and high resistance to ammonia. The O-ring can be made from a compound in the fluorocarbon family. Such materials can combine high-temperature resistance with wide chemical agent compatibility. Fluorocarbon compounds feature good resistance to petroleum products and solvents and good high-temperature compression set characteristics. The O-ring can be made from a compound in the fluoro-silicone family. Such materials combine the good high and low temperature stability of silicones with the fuel, oil and solvent resistance of fluorocarbons. These compounds feature good compression set and resilience properties. The compounds are suitable for exposure to air, sunlight, ozone, chlorinated and aromatic hydrocarbons. For example, the O-rings are standard AS-568 sizes (Aerospace Size Standard for O-rings from the Society of Automotive Engineers).

[0155] In examples, the hermetic seal as described herein can be tested in a following manner. For example, the test as described herein can be carried out as an engineering or validation testing of therapy electrode components containing a detachable gas generator. For example, failure analysis testing on units returned from the field can be tested by inserting a hypodermic needle through the laminate into the air channel and sealing around the entrance point with a cyanoacrylate adhesive. The hypodermic needle can then be attached to a regulated air source. The therapy electrode can be placed into a container filled with water. Using the regulator, the air pressure can be increased until a leak is detected.

[0156] In examples, a Pass/Fail test can be used for production. For example, a burst test for the pressurized receptacles can be set to determine that the receptacles can withstand pressures of at least between 40 psi and 60 psi. For example, a burst test for the pressurized receptacles can be set to a maximum of at least 60 psi. For example, a burst test for the pressurized receptacles can be set to a maximum of at least 50 psi. For example, a burst test for the pressurized receptacles can be set to a maximum of at least 50 psi.

[0157] In examples, a potential production/service test for therapy electrode components containing a detachable gas generator can be as follows. A sealable port or, in some examples, the same port that the detachable gas generator interfaces with the receptacles can serve as the test port. A ring-seal test can be performed where the base plate laminate can be pressurized to at least 12 psi for a prescribed period of time, 3 seconds, before releasing the pressure. This test can help eliminate weak ring seals that could potentially leak in the field. In implementations, the 12 psi pressure supply can be introduced for 3 seconds and then the supply can be cut off to monitor for a period of time, between 15-30 seconds, for a pressure drop. A pressure drop can indicate a leak. After this

period has ended, the pressure can be released.

[0158] FIG. 18B illustrates an example of a therapeutic electrode component **2000** including a gas charge **2065** coupled to the therapeutic electrode component **2000** with a coupling **1900** as illustrated in FIG. 18A. In FIG. 18B, a feed-through **1910** of the coupling **1900** is visible. The gas charge **2065** and a circuit board **2085** are disposed in a cavity **2025** defined in an end of the therapeutic electrode component **2000**. A lid **2015** is used to cover the cavity **2025** in the therapeutic electrode component **2000**. The lid **2020** includes a retainer **2020**, which functions to keep the gas charge from becoming mechanically disengaged (e.g., prevent the gas charge from “popping out”) when activated. For example, the retainer **2020** can mechanically engage with the gas charge **2065** when the lid **2015** is secured. In an implementation, the retainer **2020** can be positioned over the gas charge **2065** to reduce movement of the gas charge **2065** within the cavity **2025** and further keep it from becoming mechanically disengaged when activated. FIG. 18C illustrates the therapeutic electrode component **2000** with the lid **2015** attached.

[0159] In a first example use case, a user wears a wearable therapeutic device including a garment as illustrated in FIG. 1 and multiple therapeutic electrode components **300** as illustrated in FIGS. 3-7 removably disposed within the garment. The user receives a notification, either from the controller of the wearable therapeutic device or from a provider of the wearable therapeutic device, that the conductive fluid in one or more of the therapeutic electrode components **300** has reached its expiration date. The user acquires one or more new base plates including receptacles filled with fresh conductive fluid and including the conduit, cradle, and coupling as illustrated in FIG. 4. The user removes the conductive fastener or fasteners from the one or more therapeutic electrode components that have expired conductive fluid and slides the respective modules including the respective gas charges and circuit boards out of the respective cradles. The user then slides the respective modules including the respective gas charges and circuit boards into the cradles of the replacement base plate and secures the modules in the cradles with the one or more conductive fasteners. The user then replaces the one or more therapeutic electrode components including the replacement base plates back into their respective locations in the garment. The old base plates with the expired conductive fluid may be discarded or returned to the provider.

[0160] A similar use case to the first example use case described above would apply to a user who wears a wearable therapeutic device including a garment as illustrated in FIG. 1 and multiple therapeutic electrode components **1200** as illustrated in FIGS. 12A-14B or multiple therapeutic electrode components **1500** as illustrated in FIGS. 15A-16C removably disposed within the garment. A difference would be that the user removes and replaces the module by lifting the module off of the base plate and replaces the module on the base plate via movement of the module in a direction normal to a plane defined by the first or second surfaces of the base plate. If the user wears a wearable therapeutic device including therapeutic electrode components **1500** the user would disconnect the pneumatic tubing **1570** prior to removing the module from the old base plate and would disengage the clips **1545** from the module to allow it to be removed. The user would press the module into the cradle of the replacement base plate until the clips of the cradle of the replacement base plate engage the module. The user would reconnect the pneumatic tubing between the coupling of the replacement base plate and the outlet of the gas cartridge in the module prior to placing the therapeutic electrode component with the replacement base plate back into the garment.

[0161] In a second example use case, a user again wears a wearable therapeutic device including a garment as illustrated in FIG. 1 and multiple therapeutic electrode components **300** as illustrated in FIGS. 3-7 removably disposed within the garment. The user receives a notification, for example, from the provider of the wearable therapeutic device that one or more of the gas charges in one or more of the therapeutic electrode components disposed in the garment have been discovered to belong to a batch that has been experiencing failures, for example, failures to release gas after receiving an activation current. The provider sends the user one or more replacement modules

including circuit boards and gas charges from a different batch. The user removes the conductive fastener or fasteners from the one or more therapeutic electrode components that have the suspected bad gas charges and slides the respective old modules out of the respective cradles. The user then slides the new modules including the replacement gas charges and circuit boards into the respective cradles of the base plates of the respective therapeutic electrode components and secures the modules in the cradles with the one or more conductive fasteners. The user then replaces the one or more therapeutic electrode components including the replacement modules back into their respective locations in the garment. The old modules with the suspected bad gas charges may be discarded or returned to the provider.

[0162] A similar use case to the second example use case described above would apply to a user who wears a wearable therapeutic device including a garment as illustrated in FIG. 1 and multiple therapeutic electrode components **1200** as illustrated in FIGS. **12A-14B** or multiple therapeutic electrode components **1500** as illustrated in FIGS. **15A-16C** removably disposed within the garment. A difference would be that the user removes and replaces the module by lifting the module off of the base plate and replaces the module on the base plate via movement of the module in a direction normal to a plane defined by the first or second surfaces of the base plate. If the user wears a wearable therapeutic device including therapeutic electrode components **1500** the user would disconnect the pneumatic tubing **1570** prior to removing the old module from the old base plate and would disengage the clips **1545** from the old module to allow it to be removed. The user would press the new module into the cradle until the clips engage the new module. The user would reconnect the pneumatic tubing between the coupling and the outlet of the gas cartridge in the new module prior to placing the therapeutic electrode component with the new module back into the garment.

[0163] In a third example use case, the user may wear a wearable therapeutic device including a garment as illustrated in FIG. 1 and multiple therapeutic electrode components **900** as illustrated in FIGS. **8A-10** removably disposed within the garment. In the therapeutic electrode components **900** the removable module includes a gas charge, but not a circuit board. In a situation similar to that described in the first example use case above, the user would receive a replacement base plate (or more than one) including receptacles filled with fresh conductive fluid and including the conduit, cradle, module first portion **925A** including a new circuit board, and coupling as illustrated in FIG. **8B**. The user removes the therapeutic electrode component including the expired conductive fluid from the garment, lifts the module second portion **925B** including the gas charge out of cradle of the old therapeutic electrode component, and presses the module second portion **925B** into the cradle of the replacement base plate until the one or more tabs or clips **945** on the module engage the one or more apertures or slots **950** in the walls **952** coupled to the base plate **905**. The user then replaces the therapeutic electrode component including the replacement base plate and old module second portion **925B** into the garment.

[0164] In a fourth example use case, the user may wear a wearable therapeutic device including a garment as illustrated in FIG. 1 and multiple therapeutic electrode components **900** as illustrated in FIGS. **8A-10** removably disposed within the garment. In the therapeutic electrode components **900** the removable module includes a gas charge, but not a circuit board. In a situation similar to that described in the second example use case above, the user would receive a replacement module (or more than one) including a circuit board and gas charge from a different batch. The user removes the therapeutic electrode component including the suspect gas charge from the garment, lifts the module second portion **925B** including the suspect gas charge out of cradle of the old therapeutic electrode component, and presses the replacement module second portion **925B** into the cradle of the base plate until the one or more tabs or clips **945** on the module engage the one or more apertures or slots **950** in the walls **952** coupled to the base plate **905**. The user then replaces the therapeutic electrode component including the replacement gas charge and old base plate into the garment.

[0165] It should be appreciated that in any of the example use cases described above, the user of the medical device may be capable of performing the replacement of the portions of the therapy electrode component(s). In other examples, these operations may be performed by a provider of the medical device, for example, by the user sending a wearable medical device including one or more of the therapy electrode components to a provider for service or refurbishment.

[0166] Although the subject matter contained herein has been described in detail for the purpose of illustration, it is to be understood that such detail is solely for that purpose and that the present disclosure is not limited to the disclosed embodiments, but, on the contrary, is intended to cover modifications and equivalent arrangements that are within the spirit and scope of the appended claims. For example, it is to be understood that the present disclosure contemplates that, to the extent possible, one or more features of any embodiment can be combined with one or more features of any other embodiment.

[0167] Other examples are within the scope and spirit of the description and claims. Additionally, certain functions described above can be implemented using software, hardware, firmware, hardwiring, or combinations of any of these. Features implementing functions can also be physically located at various positions, including being distributed such that portions of functions are implemented at different physical locations.

Claims

1-37. (canceled)

38. A therapeutic electrode component comprising: a base plate; a repository disposed on a first side of the base plate and having an internal volume configured to releasably retain a conductive fluid to be expelled onto skin of a patient, wherein the repository is configured to expel the conductive fluid to provide a low impedance electrical path between the therapeutic electrode component and the skin of the patient to facilitate delivery of electrical therapy to the patient; a gas charge; a circuit board in electrical communication with the gas charge; and a removable module detachably engageable with the base plate, wherein the removable module is configured to house the gas charge and the circuit board, wherein the circuit board is configured to control activation of the gas charge, and wherein the gas charge is configured to, when activated via the circuit board, pressurize the internal volume of the repository to cause the conductive fluid to be expelled.

39. The therapeutic electrode component of claim 38, wherein the circuit board is further configured to control delivery of the electrical therapy to the patient.

40. The therapeutic electrode component of claim 38, further comprising a cradle coupled to the base plate, the cradle shaped to releasably retain the removable module.

41. The therapeutic electrode component of claim 40, wherein the cradle comprises a retainer, the retainer configured to detachably engage the removable module.

42. The therapeutic electrode component of claim 38, wherein a second side of the base plate comprises a conductive surface, the conductive surface configured to contact the skin of the patient.

43. The therapeutic electrode component of claim 42, further comprising one or more conductive fasteners configured to releasably secure the removable module to the base plate.

44. The therapeutic electrode component of claim 43, wherein the one or more conductive fasteners are configured to provide electrical communication between the circuit board and the conductive surface of the base plate.

45. The therapeutic electrode component of claim 43, wherein the one or more conductive fasteners releasably engage one or more apertures in the circuit board.

46. The therapeutic electrode component of claim 43, wherein the therapeutic electrode component is configured to deliver electrical current for the electrical therapy to the patient through the one or more conductive fasteners.

47. The therapeutic electrode component of claim 38, further comprising a conduit configured to

provide fluid communication between the internal volume of the repository and an outlet of the gas charge.

48. The therapeutic electrode component of claim 38, wherein the removable module comprises a first body and a second body, wherein the first body is configured to house the gas charge and the circuit board, and wherein the second body comprises a chamber, wherein an outlet of the gas charge is configured to extend through a wall separating the first body from the second body.

49. A wearable therapeutic device comprising: a garment configured to be worn by a patient; and at least one therapeutic electrode component configured to be removably disposed within the garment, wherein the at least one therapeutic electrode component comprises: a base plate; a repository disposed on a first side of the base plate and having an internal volume configured to releasably retain a conductive fluid to be expelled onto skin of a patient, wherein the repository is configured to expel the conductive fluid to provide a low impedance electrical path between the therapeutic electrode component and the skin of the patient to facilitate delivery of electrical therapy to the patient; a gas charge; a circuit board in electrical communication with the gas charge; and a removable module detachably engageable with the base plate, wherein the removable module is configured to house the gas charge and the circuit board, wherein the circuit board is configured to control activation of the gas charge, and wherein the gas charge is configured to, when activated via the circuit board, pressurize the internal volume of the repository to cause the conductive fluid to be expelled.

50. The wearable therapeutic device of claim 49, wherein the therapeutic electrode component further comprises a conductive fastener that passes through the removable module and provides electrical communication between the circuit board and a conductive surface on a second side of the base plate.

51. The wearable therapeutic device of claim 50, wherein the conductive fastener secures the removable module in place in a cradle disposed on the base plate.

52. The wearable therapeutic device of claim 49, wherein the therapeutic electrode component further comprises a conduit configured to provide fluid communication between the internal volume of the repository and an outlet of the gas charge.

53. The wearable therapeutic device of claim 49, wherein the base plate provides for detachment of the removable module and replacement of the removable module with a second removable module housing a second gas charge and a second circuit board.

54. The wearable therapeutic device of claim 49, wherein the removable module is configured to be removable from the base plate and installable on a replacement base plate of the therapeutic electrode component.
