

US Patent & Trademark Office

Patent Public Search | Text View

United States Patent	12390102
Kind Code	B2
Date of Patent	August 19, 2025
Inventor(s)	Sharma; Utkarsh

Generating and evaluating two- and three-dimensional images of the interior of an eye

Abstract

In certain embodiments, an ophthalmic laser surgical system for imaging and treating a target in an eye includes an optical coherence tomography (OCT) device that: directs an imaging beam towards the eye; generates three-dimensional (3D) image data from the imaging beam reflected from the eye; and generates two-dimensional (2D) enface images from the 3D image data. The 2D enface images include a target enface image imaging the target in the eye and a retinal enface image imaging a shadow cast by the target onto the retina. An xy-scanner directs the imaging beam along an imaging beam path towards the eye, and directs a laser beam from the laser device along a laser beam path aligned with the imaging beam path towards the eye. A computer compares the target of the target enface image and the shadow of the retinal enface image to confirm the presence of the target.

Inventors:	Sharma; Utkarsh (Solon, OH)
Applicant:	Alcon Inc. (Fribourg, CH)
Family ID:	1000008764366
Assignee:	Alcon Inc. (Fribourg, CH)
Appl. No.:	17/938187
Filed:	October 05, 2022

Prior Publication Data

Document Identifier	Publication Date
US 20230157536 A1	May. 25, 2023

Related U.S. Application Data

us-provisional-application US 63281453 20211119

Publication Classification

Int. Cl.: A61B3/10 (20060101); A61B3/00 (20060101); A61F9/008 (20060101); G02B26/10 (20060101); G06T7/13 (20170101); G06T7/60 (20170101); G06T7/73 (20170101)

U.S. Cl.:

CPC A61B3/102 (20130101); A61B3/0058 (20130101); A61F9/008 (20130101); G02B26/101 (20130101); G06T7/13 (20170101); G06T7/60 (20130101); G06T7/73 (20170101); G06T2207/10101 (20130101); G06T2207/20216 (20130101); G06T2207/30041 (20130101)

Field of Classification Search

References Cited

U.S. PATENT DOCUMENTS

Patent No.	Issued Date	Patentee Name	U.S. Cl.	CPC
3780979	12/1972	De Guillebon	N/A	N/A
4357088	12/1981	Pomerantzeff	N/A	N/A
5312396	12/1993	Feld	N/A	N/A
5909270	12/1998	Moser	N/A	N/A
6142630	12/1999	Koester	N/A	N/A
6322556	12/2000	Gwon	N/A	N/A
6789900	12/2003	Van De Velde	N/A	N/A
7374287	12/2007	Van De Velde	N/A	N/A
7510282	12/2008	Ueno	N/A	N/A
7520613	12/2008	Saito et al.	N/A	N/A
7703922	12/2009	Van De Velde	N/A	N/A
8480659	12/2012	Frey et al.	N/A	N/A
8652602	12/2013	Dolla	N/A	N/A
8783868	12/2013	Qiu	N/A	N/A
8876808	12/2013	Feklistov et al.	N/A	N/A
8994753	12/2014	Nakano	N/A	N/A
9033500	12/2014	Utsunomiya	N/A	N/A
9603519	12/2016	Bor et al.	N/A	N/A
9675243	12/2016	Sasak et al.	N/A	N/A
9789002	12/2016	Van De Velde	N/A	N/A
10130511	12/2017	Dantus	N/A	N/A
10478342	12/2018	Dick	N/A	N/A
10555835	12/2019	Schuele et al.	N/A	N/A
2007/0258094	12/2006	Izatt et al.	N/A	N/A
2007/0291277	12/2006	Everett	N/A	N/A
2009/0073384	12/2008	Warden	N/A	N/A
2009/0137989	12/2008	Kataoka	N/A	N/A
2009/0196477	12/2008	Cense et al.	N/A	N/A
2010/0123873	12/2009	Raymond	N/A	N/A
2010/0152847	12/2009	Padrick	N/A	N/A
2011/0077557	12/2010	Wing et al.	N/A	N/A
2012/0281235	12/2011	Murata	N/A	N/A
2013/0131652	12/2012	Dick	N/A	N/A
2013/0173029	12/2012	Caldeira et al.	N/A	N/A
2014/0058367	12/2013	Dantus	N/A	N/A
2014/0216468	12/2013	Goldshleger	N/A	N/A
2014/0257257	12/2013	Grant et al.	N/A	N/A
2014/0268036	12/2013	Ketterling et al.	N/A	N/A
2014/0276674	12/2013	Lee	N/A	N/A
2015/0190278	12/2014	Gooding	N/A	N/A
2015/0342782	12/2014	Mordaunt	N/A	N/A
2016/0058617	12/2015	Luttrull et al.	N/A	N/A
2016/0074214	12/2015	Palanker et al.	N/A	N/A
2016/0074221	12/2015	Tassignon et al.	N/A	N/A
2016/0166431	12/2015	Vogler et al.	N/A	N/A
2016/0227999	12/2015	An et al.	N/A	N/A
2016/0235588	12/2015	Hart et al.	N/A	N/A
2016/0256324	12/2015	Suzuki	N/A	N/A
2016/0278629	12/2015	Schuele	N/A	N/A
2016/0302969	12/2015	Yamamoto	N/A	N/A
2017/0181625	12/2016	Kawakami et al.	N/A	N/A
2017/0252213	12/2016	Furuuchi et al.	N/A	N/A

2017/0326003	12/2016	Schuele et al.	N/A	N/A
2018/0028354	12/2017	Heeren	N/A	N/A
2018/0028355	12/2017	Raksi	N/A	N/A
2018/0140257	12/2017	Govindjee et al.	N/A	N/A
2018/0206719	12/2017	Adler et al.	N/A	N/A
2018/0317767	12/2017	Ryan	N/A	N/A
2018/0353064	12/2017	Soetikno et al.	N/A	N/A
2018/0368915	12/2017	Xia et al.	N/A	N/A
2019/0159933	12/2018	Romano et al.	N/A	N/A
2019/0282403	12/2018	Barrett et al.	N/A	N/A
2019/0290124	12/2018	Laforest et al.	N/A	N/A
2019/0313903	12/2018	Mckinnon	N/A	N/A
2019/0365569	12/2018	Skovgaard et al.	N/A	N/A
2020/0038241	12/2019	Wang et al.	N/A	N/A
2020/0060873	12/2019	Heeren	N/A	N/A
2020/0085292	12/2019	Fukuma et al.	N/A	N/A
2020/0129336	12/2019	Schuele et al.	N/A	N/A
2020/0130103	12/2019	Choi	N/A	N/A
2020/0192080	12/2019	Karam	N/A	N/A
2020/0196853	12/2019	Van Hemert et al.	N/A	N/A
2020/0273218	12/2019	Camino et al.	N/A	N/A
2020/0397289	12/2019	Ralston	N/A	N/A
2020/0400422	12/2019	Ralston	N/A	N/A
2021/0100450	12/2020	Amma	N/A	N/A
2021/0186753	12/2020	Al-Qaisi et al.	N/A	N/A
2021/0275009	12/2020	Yates	N/A	N/A
2021/0378507	12/2020	Wallace	N/A	N/A
2021/0386586	12/2020	Bor	N/A	N/A
2022/0012459	12/2021	Schwiegerling	N/A	N/A
2022/0031511	12/2021	Charles	N/A	N/A
2023/0157889	12/2022	Bor	N/A	N/A

FOREIGN PATENT DOCUMENTS

Patent No.	Application Date	Country	CPC
2018274939	12/2019	AU	N/A
210009227	12/2019	CN	N/A
108371542	12/2019	CN	N/A
109196333	12/2019	CN	N/A
111281651	12/2019	CN	N/A
112862782	12/2020	CN	N/A
112587302	12/2020	CN	N/A
112587304	12/2020	CN	N/A
19705044	12/1997	DE	N/A
102019007147	12/2020	DE	N/A
102019007148	12/2020	DE	N/A
0770370	12/1996	EP	N/A
1212022	12/2004	EP	N/A
1563785	12/2004	EP	N/A
1638452	12/2005	EP	N/A
1838212	12/2006	EP	N/A
2144552	12/2009	EP	N/A
1928297	12/2009	EP	N/A
2459138	12/2011	EP	N/A
2525706	12/2011	EP	N/A
2898820	12/2014	EP	N/A
3061429	12/2015	EP	N/A
2890340	12/2016	EP	N/A
3459487	12/2018	EP	N/A
3501463	12/2018	EP	N/A
3636137	12/2019	EP	N/A
3861924	12/2020	EP	N/A

2469249	12/2009	GB	N/A
5767014	12/2014	JP	N/A
2017176558	12/2016	JP	N/A
6410468	12/2017	JP	N/A
2018196821	12/2017	JP	N/A
2018196822	12/2017	JP	N/A
2020022569	12/2019	JP	N/A
6736304	12/2019	JP	N/A
6839902	12/2020	JP	N/A
2661016	12/2017	RU	N/A
2692666	12/2018	RU	N/A
2695629	12/2018	RU	N/A
2710058	12/2018	RU	N/A
2726468	12/2019	RU	N/A
9958047	12/1998	WO	N/A
0137769	12/2000	WO	N/A
0195791	12/2000	WO	N/A
2007059189	12/2006	WO	N/A
2009033110	12/2008	WO	N/A
2009036104	12/2008	WO	N/A
2009039315	12/2008	WO	N/A
2009059400	12/2008	WO	N/A
2010117386	12/2009	WO	N/A
2014053824	12/2013	WO	N/A
2015131135	12/2014	WO	N/A
2015171793	12/2014	WO	N/A
2016033590	12/2015	WO	N/A
2017062673	12/2016	WO	N/A
2017196306	12/2016	WO	N/A
2017205857	12/2016	WO	N/A
2020074532	12/2019	WO	N/A
2020180729	12/2019	WO	N/A
2020215359	12/2019	WO	N/A
2020216763	12/2019	WO	N/A
2020257711	12/2019	WO	N/A
2021023799	12/2020	WO	N/A
2021049243	12/2020	WO	N/A
2021066047	12/2020	WO	N/A
2021092211	12/2020	WO	N/A
2021183637	12/2020	WO	N/A
2022149028	12/2021	WO	N/A
2023089416	12/2022	WO	N/A
2023089459	12/2022	WO	N/A
2023097391	12/2022	WO	N/A

OTHER PUBLICATIONS

Damodaran et al., “Digital micromirror device based ophthalmoscope with concentric circle scanning”, 2017, pp. 2766-2780, vol. 8, No. 5, Biomedical Optics Express. cited by applicant

Fischer et al., “Scanning Laser Ophthalmoscopy (SLO)”, In: Bille JF, editor. High Resolution Imaging in Microscopy and Ophthalmology: New Frontiers in Biomedical Optics [Internet], Aug. 14, 2019, accessed on Jan. 30, 2023 from <https://www.ncbi.nlm.nih.gov/books/NBK554043>, Springer. cited by applicant

Ginner et al., “Wide-Field OCT Angiography at 400 KHz Utilizing Spectral Splitting”, Photonics, Oct. 23, 2014, pp. 369-379, vol. 1, No. 4. cited by applicant

Heidelberg Engineering GMBH, “Spectralis. Hardware Operating Instructions,” Version 001, Aug. 2007. cited by applicant

Heidelberg Engineering, “Spectralis. Multimodal Imaging Platform Optimized for the Posterior Segment”, accessed on Jan. 30, 2023 from <https://business-lounge.heidelbergengineering.com/us/en/products/spectralis/spectralis/>. cited by applicant

Hofer et al., “Dispersion encoded full range frequency domain optical coherence tomography”, Jan. 5, 2009, pp. 7-24, vol. 17, No. 1, Optics Express, US. cited by applicant

Hofer et al., “Fast dispersion encoded full range optical coherence tomography for retinal imaging at 800 nm and 1060 nm”, Mar. 1, 2010, pp. 4898-4919, vol. 18, No. 5, Optics Express. cited by applicant

Leitgeb et al., “Complex ambiguity-free Fourier domain optical coherence tomography through transverse scanning”, 2007, pp. 3453-3455, vol. 32, Optics Letters. cited by applicant

Li et al., “DMD-based three-dimensional chromatic confocal microscopy”, 2020, pp. 4349-4356, vol. 59, No. 14, Applied Optics. cited by applicant

Martial et al., “Programmable Illumination and High-Speed, Multi-Wavelength, Confocal Microscopy Using a Digital Micromirror”, Aug. 2012, e43942, vol. 7, No. 8, PLOS One. cited by applicant

Reznicek Lukas et al., “Wide-Field Megahertz OCT Imaging of Patients with Diabetic Retinopathy”, Journal of Diabetes Research, 2015, 5 pages. cited by applicant

Ruggeri et al., “Imaging and full-length biometry of the eye during accommodation using spectral domain OCT with an optical switch”, Jul. 1, 2012, pp. 1506-1520, vol. 3, No. 7, Biomedical Optics Express. cited by applicant

Sarunic et al., “Instantaneous complex conjugate resolved spectral domain and swept-source OCT using 3x3 fiber couplers”, Feb. 2005, pp. 957-967, vol. 13, No. 3, Optics Express. cited by applicant

Shields et al., “Wide-angle Imaging of the Ocular Fundus”, Review of the Ophthalmology, Feb. 15, 2003. cited by applicant

Singh, “Lasers Take Aim at Floaters”, Ophthalmology Management, Jul. 1, 2019, pp. 38, 40-42, 59, vol. 23. cited by applicant

Singh, “Modern vitreolysis—YAG laser treatment now a real solution for the treatment of symptomatic floaters”, Survey of Ophthalmology, Mar. 3, 2020, pp. 581-591, vol. 65, No. 5. cited by applicant

SunLED, NanoPoint-0201 Series LEDs, published Feb. 15, 2016, www.SunLEDusa.com. cited by applicant

Volk Optical, “Volk Idrees Mid-Vitreous Lens”, Dec. 20, 2020, accessed on Dec. 20, 2020 from https://www.volk.com/...s?pr_prod_strat=collection_fallback&pr_rec_pid=4513049018402&pr_ref_pid=4513048952866&pr_seq=uniform cited by applicant

Wang et al., “In vivo full range complex Fourier domain optical coherence tomography”, Jan. 30, 2007, 054103, vol. 90, Applied Physics Letters. cited by applicant

Wojtkowski et al., “Full range complex spectral optical coherence tomography technique in eye imaging”, 2002, pp. 1415-1417, vol. 27, No. 16, Optics Letters. cited by applicant

Yasuno et al., “Simultaneous B—M-mode scanning method for real-time full-range Fourier domain optical coherence tomography”, 2006, pp. 1861-1865, vol. 45, No. 8, Applied Optics. cited by applicant

Zhang et al., Removal of a mirror image and enhancement of the signal-to-noise ratio in Fourier-domain optical coherence tomography using an electro-optic phase modulator, Jan. 15, 2005, vol. 30, No. 2, Optics Letters. cited by applicant

Zhou et al., “Dual channel dual focus optical coherence tomography for imaging accommodation of the eye”, May 25, 2009, pp. 8947-8955, vol. 17, No. 11, Optics Express. cited by applicant

Blake F. Webb, et al.; “Prevalence of vitreous floaters in a community sample of smartphone users”; Internat'l Journal of Ophthalmology; Jun. 18, 2013; pp. 402-405; 6(3); PMC/ US National Library of Medicine National Institutes of Health. cited by applicant

Chirag P. Shah, et al., YAG Laser Vitreolysis vs Sham YAG Vitreolysis for Symptomatic Vitreous Floaters a Randomized Clinical Trial, JAMA Ophthalmology, Sep. 2017, 918-923, 135-9. cited by applicant

Ellex Website, Treatment Guidelines—Laser Floater Removal; 2016, Ellex Medical Pty Ltd. E&OE. VB0002E, downloaded Apr. 20, 2017. cited by applicant

Felix Sauvage et al: “Photoablation of Human Vitreous Opacities by Light—Induced Vapor Nanobubbles”, ACS Nano, vol. 13, No. 7, Jul. 9, 2019, pp. 8401-8416. cited by applicant

Kim Jihwan et al. “Nonmechanical Laser Beam Steering Based on Polymer Polarization Gratings: Design Optimization and Demonstration”, Journal of Lightwave Technology, vol. 33, No. 10, pp. 2068-2077, May 15, 2015. cited by applicant

Michael J. Escuti, et al., “Geometric-Phase Holograms”, Optics & Photonics News, pp. 22-29, Feb. 2016. cited by applicant

Milston Rebecca et al: “Vitreous floaters: Etiology, diagnostics, and management”, Survey of Ophthalmology, vol. 61, No. 2, Mar. 1, 2016, pp. 211-227. cited by applicant

Nicuser Iftimia et al: “Hybrid retinal imager using line-scanning laser ophthalmoscopy and spectral domain optical coherence tomography”, Optics Express, vol. 14, No. 26, Dec. 22, 2006. cited by applicant

Reece Bergstrom, et al., Vitreous Floaters, National Center for Biotechnology Information, May 21, 2020, 4 pages, Bookshelf ID NBK470420, StatPearls Publishing LLC, online. cited by applicant

Wikipedia Encyclopedia, Floater, Wikipedia Encyclopedia, Mar. 29, 2021, online: <https://en.wikipedia.org/wiki/rloater?wprov=sfti.1>. cited by applicant

Zhang Yunbo et al: “Parallel large-range scanning confocal microscope based on a digital micromirror device”, Optik vol. 124, No. 13 (2013), Aug. 4, 2012, pp. 1585-1588. cited by applicant

Adrian G.H. Podoleanu et al., Combined optical coherence tomograph and scanning laser ophthalmoscope mi nije dostupan besplatno., Electronics Letters, 34 (11), 1998. cited by applicant

Chi-Hung Lee, et al., Imaging vitreous floaters and cataracts with optical simulations, Optik, 194, 1-9, 2019. cited by applicant

Christy K. Sheehy et al., High-speed, image-based eye tracking with a scanning laser ophthalmoscope, Biomedical Optics Express, vol. 3, No. 10, 2012. cited by applicant

D. H. Kelly, “Retinal Inhomogeneity. II. Spatial Summation,” J. Opt. Soc. Am., pp. 114-119, vol. 1, No. 1 (Jan. 1984). cited by applicant

D. H. Kelly, “Retinal Inhomogeneity. III. Circular-Retina Theory,” D.H. Kelly, J. Opt. Soc. Am., pp. 810-819, vol. 2, No. 6

(Jun. 1985). cited by applicant
D.H. Kelly, "Visual Processing of Moving Stimuli," J. Opt. Soc. Am., pp. 216-225, vol. 2, No. 2 (Feb. 1985). cited by applicant
D.H. Kelly, "Motion and Vision. II. Stabilized Spatio-Temporal Threshold Surface," J. Opt. Soc. Am., pp. 1340-1349, vol. 69, No. 10 (Oct. 1979). cited by applicant
D.H. Kelly, "Retinal Inhomogeneity. I. Spatiotemporal Contrast Sensitivity," J. Opt. Soc. Am., pp. 107-113, vol. 1, No. 1 (Jan. 1984). cited by applicant
Mojana F. et al., Observations by spectral-domain optical coherence tomography combined with simultaneous scanning laser ophthalmoscopy: imaging of the vitreous, American Journal of Ophthalmol. Apr. 2010;149(4):641-650. cited by applicant
Nidek, Scanning Laser Ophthalmoscope Mirante SLO/OCT Mirante SLO, https://www.nidek-intl.com/product/ophthaloptom/diagnostic/dia_retina/mirante.htm. cited by applicant
Peter G. J. Barten, "Contrast Sensitivity of the Human Eye and its Effects on Image Quality," Chapter 3, pp. 27-40, Model for the spatial contrast sensitivity of the eye, (1999). cited by applicant
Pointer, J. S., & Hess, R. F. "The contrast sensitivity gradient across the human visual field: With emphasis on the low spatial frequency range," R. F. Vision Research, 29(9), 1133-1151 (1989). cited by applicant
Sebag J et al., Vitreous and Vitreoretinal Interface, Ch. 21, 2015. cited by applicant
Sebag J., Vitreous and Vision Degrading Myodesopsia. Progress in Retinal and Eye Research Nov. 2020;79. cited by applicant
T Ivanova et al., Vitrectomy for primary symptomatic vitreous opacities: an evidence-based review, Eye (Lond) May 2016;30(5):645-55. cited by applicant
Teri T Kleinberg et al., Vitreous substitutes: a comprehensive review, Survey of Ophthalmology, 56 (4), 2011. cited by applicant
Volk Optical, "Volk Singh Mid-Vitreous Lens", Dec. 20, 2020, accessed on Dec. 20, 2020 from https://www.volk.com/products/singh-mid-vitreous-vitreous-slit-lamp-lens?_pos+3&_sid=b50c0674f&_ss=r. cited by applicant

Primary Examiner: Dinh; Jack

Attorney, Agent or Firm: PATTERSON + SHERIDAN, LLP

Background/Summary

TECHNICAL FIELD

(1) The present disclosure relates generally to ophthalmic surgical systems, and more particularly to generating and evaluating two- and three-dimensional images of the interior of an eye.

BACKGROUND

(2) Laser vitreolysis uses laser beams to treat vitreous floaters and other retinal diseases. Precise delivery of a laser beam to the target is important to avoid damaging healthy tissue and ensure ocular safety. Accordingly, imaging systems should provide sufficiently clear images of targets. However, known imaging systems are not satisfactory in certain situations.

BRIEF SUMMARY

(3) In certain embodiments, an ophthalmic laser surgical system for imaging and treating a target in an eye includes an optical coherence tomography (OCT) device, a laser device, an xy-scanner, and a computer. The eye has an eye axis that defines a z-axis, which defines xy-planes within the eye. The OCT device directs an imaging beam along an imaging beam path towards the eye; receives the imaging beam reflected from the eye; generates three-dimensional (3D) image data from the reflected imaging beam; and generates two-dimensional (2D) enface images from the 3D image data. A 2D enface image images an xy-plane within the eye. The 2D enface images include a target enface image imaging the target in the eye and a retinal enface image imaging a retina of the eye. The retinal enface image shows a shadow cast by the target onto the retina. The laser device directs a laser beam along a laser beam path towards the target. The xy-scanner receives the imaging beam from the imaging system and directs the imaging beam along the imaging beam path towards the eye; and receives the laser beam from the laser device and directs the laser beam along the laser beam path aligned with the imaging beam path towards the eye. The computer compares the target of the target enface image and the shadow of the retinal enface image to confirm the presence of the target.

(4) Embodiments may include none, one, some, or all of the following features: The target comprises a vitreous eye floater. The OCT device generates the two-dimensional (2D) enface images from the 3D image data by: taking a slice of the 3D image data; and summing data of the slice to yield a 2D enface image. The OCT device generates the two-dimensional (2D) enface images from the 3D image data by: taking a slice of the 3D image data; and averaging data of the slice to yield a 2D enface image. The OCT device generates the two-dimensional (2D) enface images from the 3D image data by: taking a slice of the 3D image data; and projecting data of the slice to yield a 2D enface image. The computer performs image processing on the target enface image to determine a feature of the target. The computer may perform image processing on the target enface image to identify an outline of the target, and determine a size of the target from the outline of the target. The computer may perform image processing on the target enface image to identify

an outline of the target, and determine a shape of the target from the outline of the target. The computer tracks the target according to the target enface image imaging the target. The computer tracks the target by tracking the shadow cast by the target according to the retinal enface image. The computer overlays an outline of the target onto the target enface image. The computer overlays a no-fire zone onto the target enface image. The OCT device generates three-dimensional (3D) images from the 3D image data.

(5) In certain embodiments, a method images and treats a target in an eye. The eye has an eye axis that defines a z-axis, which defines xy-planes within the eye. The method includes: directing, by an optical coherence tomography (OCT) device, an imaging beam along an imaging beam path towards the eye; receiving the imaging beam reflected from the eye; generating three-dimensional (3D) image data from the reflected imaging beam; and generating two-dimensional (2D) enface images from the 3D image data. A 2D enface image images an xy-plane within the eye. The 2D enface images include a target enface image imaging the target in the eye and a retinal enface image imaging a retina of the eye. The retinal enface image shows a shadow cast by the target onto the retina. The method further includes: directing, by a laser device, a laser beam along a laser beam path towards the target; receiving, by an xy-scanner, the imaging beam from the imaging system and direct the imaging beam along the imaging beam path towards the eye; receiving, by the xy-scanner, the laser beam from the laser device and direct the laser beam along the laser beam path aligned with the imaging beam path towards the eye; and comparing, by a computer, the target of the target enface image and the shadow of the retinal enface image to confirm the presence of the target.

(6) Embodiments may include none, one, some, or all of the following features: The generating the two-dimensional (2D) enface images from the 3D image data includes: taking a slice of the 3D image data; and summing, averaging, or projecting data of the slice to yield a 2D enface image. The method further includes performing, by the computer, image processing on the target enface image to determine a feature of the target. The computer may perform image processing on the target enface image to identify an outline of the target, and determine a size of the target from the outline of the target. The computer may perform image processing on the target enface image to identify an outline of the target, and determine a shape of the target from the outline of the target. The method further includes tracking, by the computer, the target according to the target enface image imaging the target. The method further includes tracking, by the computer, the target by tracking the shadow cast by the target according to the retinal enface image. The method further includes overlaying, by the computer, an outline of the target or a no-fire zone onto the target enface image. The method further includes generating, by the OCT device, a plurality of three-dimensional (3D) images from the 3D image data.

(7) In certain embodiments, an ophthalmic laser surgical system for imaging and treating a target in an eye includes an optical coherence tomography (OCT) device, a laser device, an xy-scanner, and a computer. The eye has an eye axis that defines a z-axis, which defines xy-planes within the eye. The target is a vitreous eye floater. The OCT device directs an imaging beam along an imaging beam path towards the eye; receives the imaging beam reflected from the eye; generates three-dimensional (3D) image data from the reflected imaging beam; and generates two-dimensional (2D) enface images from the 3D image data. The OCT device generates the 2D enface images from the 3D image data by taking a slice of the 3D image data and summing, averaging, or projecting data of the slice to yield a 2D enface image. A 2D enface image images an xy-plane within the eye. The 2D enface images include a target enface image imaging the target in the eye and a retinal enface image imaging a retina of the eye. The retinal enface image shows a shadow cast by the target onto the retina. The laser device directs a laser beam along a laser beam path towards the target. The xy-scanner receives the imaging beam from the imaging system and directs the imaging beam along the imaging beam path towards the eye; and receives the laser beam from the laser device and directs the laser beam along the laser beam path aligned with the imaging beam path towards the eye. The computer performs the following: compares the target of the target enface image and the shadow of the retinal enface image to confirm the presence of the target; performs image processing on the target enface image to determine a feature of the target by performing image processing on the target enface image to identify an outline of the target and determining a size of the target from the outline of the target, and by performing image processing on the target enface image to identify an outline of the target and determining a shape of the target from the outline of the target; tracks the target according to the target enface image imaging the target; tracks the target by tracking the shadow cast by the target according to the retinal enface image; overlays an outline of the target onto the target enface image; overlays a no-fire zone onto the target enface image; and generates a plurality of three-dimensional (3D) images from the 3D image data.

Description

BRIEF DESCRIPTION OF THE DRAWINGS

- (1) FIG. 1 illustrates an example of an ophthalmic surgical system that can image and treat a target in an eye, according to certain embodiments;
- (2) FIGS. 2A and 2B illustrate examples of two-dimensional (2D) enface images that may be generated by the OCT device of the system of FIG. 1;
- (3) FIG. 3 illustrates an example of a three-dimensional (3D) image that may be generated by the OCT device of the system of FIG. 1; and
- (4) FIG. 4 illustrates an example of a method for imaging and treating a target in the vitreous of an eye, according to

certain embodiments.

DESCRIPTION OF EXAMPLE EMBODIMENTS

(5) Referring now to the description and drawings, example embodiments of the disclosed apparatuses, systems, and methods are shown in detail. The description and drawings are not intended to be exhaustive or otherwise limit the claims to the specific embodiments shown in the drawings and disclosed in the description. Although the drawings represent possible embodiments, the drawings are not necessarily to scale and certain features may be simplified, exaggerated, removed, or partially sectioned to better illustrate the embodiments.

(6) Known surgical systems include imaging systems, such as scanning laser ophthalmoscope (SLO) and optical coherence tomography (OCT) devices, to provide images of targets or their shadows. An SLO device provides two-dimensional (2D) enface images of a target or its shadow on the retina, and an OCT device provides three-dimensional (3D) images of the target. However, these known surgical systems have disadvantages. The two different imaging technologies, SLO and OCT, add expense and complexity to the system. In addition, the known surgical systems make it difficult to determine whether the image shows a target shadow or, e.g., a lens opacity, vignetting, retinal pathology, or imaging artifact.

(7) Accordingly, embodiments of the surgical systems described herein include an OCT device that gathers 3D OCT data and generates both 3D images and 2D enface images from the data. A 2D enface image can be generated from a “slice” of the 3D OCT data between two surfaces, e.g., two xy-planes or layers of the tissue of the eye. A spatial mapping of features between the surfaces yields a 2D enface image.

(8) Certain embodiments may offer several advantages. The surgical systems can use the 2D enface images to determine the presence, size, shape, and/or location of the target. For example, a 2D image of the target can be compared with a 2D image of its shadow to confirm the presence of the target. As another advantage, the surgical systems use only one device (the OCT device) instead of two devices (the OCT and SLO devices) to provide 3D images and 2D enface images, which reduces the cost and complexity of certain embodiments.

(9) As yet another advantage, the surgical systems co-register the OCT and laser devices such that the laser beam can be precisely directed to the target using a 2D enface image. The OCT and laser devices share a beam path through the same optical elements, including an xy-scanner, and through the eye. If the OCT and laser beams are aligned prior to the shared optical elements, the beams are automatically aligned at the target location in the eye, allowing for precise image-guided beam targeting.

(10) FIG. 1 illustrates an example of an ophthalmic surgical system **10** that can image and treat a target in an eye, according to certain embodiments. In the example, the target is a vitreous eye floater in the vitreous of the eye. In the example, an axis of the eye (e.g., visual or optical) defines a z-axis, which in turn defines x- and y-axes orthogonal to the z-axis. X- and y-axes define xy-planes within the eye. X-, y-, and z-directions and locations are relative to the x-, y-, and z-axes, respectively.

(11) In the example, system **10** includes a treatment system (which comprises a laser device **20**), an imaging system (which comprises an optical coherence tomography (OCT) device **22**), an xy-scanner **24**, optical elements **26**, and a computer **38**, coupled as shown. Laser device **20** includes a laser **30** and lenses **32**, **24**, coupled as shown. Optical elements include beamsplitter (e.g., a dichroic mirror (DM)) **28** and lenses **32**, **34**, **40**, **42**, and **46**, coupled as shown. Computer **38** includes logic **52**, memory **54** (which stores a computer program **55**), a user interface (UI) **56**, and a display **58**, coupled as shown.

(12) As an example of operation, OCT device **22** directs an imaging beam along an imaging beam path towards the eye, receives the imaging beam reflected from the eye, generates three-dimensional (3D) image data from the reflected imaging beam, and generates two-dimensional (2D) enface images from the 3D image data. A 2D enface image images an xy-plane within the eye. For example, a target enface image images a target in the eye. Laser device **20** directs a laser beam along a laser beam path towards the target. OCT device **22** and laser device **20** share the same xy-scanner **24**, which allows for precise aiming of the laser beam using the imaging. That is, xy-scanner **24** receives the imaging beam from the imaging system and directs the imaging beam along the imaging beam path towards the target, and receives the laser beam from the laser device and directs the laser beam along the laser beam path aligned with the imaging beam path towards the target. In certain embodiments, OCT device **22** combines 2D enface images to generate a three-dimensional (3D) image, where the 3D image images a volume within the eye.

(13) Turning to the treatment system, laser **30** of laser device **22** generates a laser beam with any suitable wavelength, e.g., in a range from 400 nm to 2000 nm. Laser device **22** delivers laser pulses at any suitable repetition rates ranging from, but not limited to, 1 hertz (Hz) to several hundreds of kilohertz (kHz). A laser pulse may have any suitable pulse duration (e.g., ranging from, but not limited to, a nanosecond (ns) to 20 femtoseconds (fs)), any suitable pulse energy (e.g., 1 microjoule (μJ) to 10 millijoule (mJ)), and a focal point of any suitable size (e.g., ranging from 3 to 20 microns (μm), such as 7 μm). Lenses **32** and **34** are used to adjust the focus position of the laser beam within tissue, such as eye tissue.

(14) Turning to the imaging system, OCT device **22** generates 3D images and 2D enface images of the interior of the eye from the imaging beam reflected from the eye. A 2D enface image may be regarded as a pseudo-SLO image, as OCT device **22** can generate 2D enface images that are very similar to SLO images. OCT device **22** may be any suitable device that utilizes optical coherence tomography to generate images, e.g., a swept-source OCT (SS-OCT), line-field

OCT, full-field OCT, or spectral-domain OCT (SD-OCT) device.

(15) In certain embodiments, OCT device **22** generates the 2D and 3D images from 3D image data determined from the reflected imaging beam. OCT device **22** performs a series of A-scans (i.e., scans in the z-direction), combines the A-scans to form B-scans, and combines the B-scans to yield 3D image data, which can be used to generate a 3D image. To generate a 2D enface image, OCT device **22** takes a slice of the 3D image data that is generally orthogonal to the z-axis. The slice is bounded by two non-intersecting surfaces. The surfaces may represent, e.g., xy-planes or layers of eye tissue. The data in the slice is processed (e.g., averaged, summed, projected) to yield a 2D enface image. For example, for each point (x, y), the values of the image data at point (x, y) are averaged (or summed, projected, or otherwise processed) to yield the value for point (x, y) of the enface image.

(16) In other embodiments, OCT device **22** generates the 2D enface images directly from the A-scans. OCT device **22** generates an A-scan, which a value for an xy-point of an xy-plane. Multiple A-scans yield values for multiple points of an xy-plane, which can be used to generate a 2D enface image at the xy-plane.

(17) Xy-scanner **36** scans treatment and imaging beams transversely in xy-directions. Examples of scanners include a galvo scanner (e.g., a pair of galvanometrically-actuated scanner mirrors that can be tilted about mutually perpendicular axes), an electro-optical scanner (e.g., an electro-optical crystal scanner) that can electro-optically steer the beam, or an acousto-optical scanner (e.g., an acousto-optical crystal scanner) that can acousto-optically steer the beam.

(18) OCT device **22** and laser device **20** share xy-scanner **24**, allowing for co-registration between the OCT imaging and treatment beams. That is, xy-scanner **24** receives the imaging beam from the imaging system and directs the imaging beam along the imaging beam path towards the target, and receives the laser beam from the laser device and directs the laser beam along the laser beam path co-aligned with the imaging beam path towards the target. The OCT imaging and treatment beams share the same path through the optics of the system and the eye, so are affected by the same optical properties and distortions along the beam path. Thus, if the imaging and treatment beams are aligned prior to xy-scanner **24**, they are automatically aligned at the target location. This enables accurate and precise delivery of the laser beam to the target location identified using OCT images.

(19) Optical elements includes beamsplitter (such as a dichroic mirror (DM)) **28** and lenses **32**, **34**, **40**, **42**, and **46**, coupled as shown. In general, an optical element can act on (e.g., transmit, reflect, refract, diffract, collimate, condition, shape, focus, modulate, and/or otherwise act on) a laser beam. Examples of optical elements include a lens, prism, mirror, diffractive optical element (DOE), holographic optical element (HOE), and spatial light modulator (SLM). In the example, lens **40** collimates beams to and from beamsplitter **28**. Beamsplitter **28** directs beams from OCT device **22** and laser device **20** to xy-scanner **24** and directs beam reflected from the eye back to OCT device **22**. Beamsplitter **28** may comprise any suitable beam splitter that can combine beams or separate one beam into multiple beams. For example, a dichroic mirror can combine or split beams of different wavelengths, depending on the configuration. Lenses **32** and **34** collimates the beam from laser **30**. Lens **42** and objective lens **46** collimate and focus beams at the eye.

(20) Computer **38** sends instructions to the OCT device and the laser device. Computer **38** may utilize computer programs **55** to perform operations. Examples of computer programs **55** include target imaging, target tracking, image processing, and target evaluation.

(21) In certain embodiments, computer **26** uses an image processing program **55** to perform image processing on an image, e.g., analyze the digital information of the image to extract information from the image. In certain embodiments, computer **26** performs image processing to analyze an image of a target or a target's shadow (i.e., "target shadow") to obtain information about the target. Localized opacities in the vitreous, such as floaters, can affect vision quality when they are in the path of light and cast a shadow onto the retina. Hence, the target shadow can provide useful information about clinical significance of the floater or other opacity. Moreover, target shadows may yield higher contrast, clearer images than the targets themselves. Accordingly, images of a target shadow may be easier to analyze to evaluate, e.g., the location, size, or density of the target. In addition, it may be easier to track the target shadow to determine the location of the target.

(22) In the embodiments, computer **26** may analyze the target and/or target shadow in any suitable manner. For example, computer **26** may detect a brighter or darker shape in an image (using, e.g., edge detection or pixel analysis) to detect the target or the target shadow. As another example, program **54** may identify an outline of the target, and determine a size and/or shape of the target from the outline. As another example, program **54** may detect the darkness of the target shadow, i.e., how dark the shadow is. In general, a thicker and/or denser target may yield a darker shadow. Similarly, a target closer to the retina may yield a darker shadow. Accordingly, program **54** may analyze the target and/or target shadow to determine clinically relevant information about the target.

(23) In certain embodiments, computer **38** performs image processing to confirm the presence of the target. OCT device **22** generates a target enface image that shows a target candidate and a retinal enface image that shows a shadow. Computer **38** compares the target candidate and the shadow to confirm the presence of the target. For example, computer **38** may align the images to determine that the target casts the shadow. This may rule out shadows caused by, e.g., a lens opacity, vignetting, retinal pathology, or other imaging artifacts. In certain embodiments, computer **38** performs image processing to generate 2D and 3D images, as described above.

(24) In certain embodiments, computer **38** uses a tracking program to track and/or predict the movement of a target. In some situations, the enface image of the target itself may be clearer than the image of the shadow of the target, so

computer **38** may track the target using the target enface image rather than the retinal enface image with the target shadow. In other situations, the retinal enface image with the target shadow may be more appropriate, so computer **38** may track the target using the target shadow. The tracking program may predict the movement of the target and send to laser device **20** the location of where the target is predicted to be when the laser beam reaches the target. The images of the target may be used to acquire the target (e.g., determine the fingerprint of a floater) and fire the laser beam at the target.

(25) In certain embodiments, computer **38** generates image overlays to superimpose over images of the eye. Examples of image overlays include an outline of the target, a no-fire zone indicating where the laser should not be fired (such as the foveal region), information describing the target (e.g., target size, shape, and/or density) or the eye, or other suitable overlay that enhances the image. Examples of eye images over which an image overlay may be superimposed include a retinal enface image, target enface image, real time video of the eye, or other suitable image of the eye. For example, computer **38** may superimpose an outline of the target onto a retinal enface image, a no-fire zone onto a target enface image, or the target size, shape, and/or density onto a real time video of the eye.

(26) FIGS. **2A** and **2B** illustrate examples of two-dimensional (2D) enface images **60** that may be generated by OCT device **22** of system **10** of FIG. **1**. FIG. **2A** shows examples of enface images **60** (**60a** to **60e**). In the examples, each image is located at an xy-plane within the eye, and each xy-plane is located at a different z-location. Enface images **60** include, e.g., a target enface image that images a target in the eye and a retinal enface image that images the retina of the eye. The retinal enface image may also show the shadow cast by the target onto the retina. FIG. **2B** shows an example of an enface image **60** generated at the retina of the eye.

(27) FIG. **3** illustrates an example of a three-dimensional (3D) image **62** that may be generated by OCT device **22** of system **10** of FIG. **1** from 3D OCT image data. In the example, 3D image **62** images a volume within the eye. The volume image may show the target and/or retina.

(28) FIG. **4** illustrates an example of a method for imaging and treating a target in the vitreous of an eye, according to certain embodiments. The method starts at step **110**, where the OCT device directs an OCT imaging beam towards the eye via an xy-scanner. The OCT device detects the reflected OCT imaging beam at step **112**. The OCT device generates 3D image data from the reflected beam at step **114**. The image data is generated from multiple A-scans and B-scans.

(29) The OCT device generates 2D enface images of the target from the 3D image data at step **116**. Enface images include, e.g., a target enface image that images a target in the eye and a retinal enface image that images the retina of the eye. The retinal enface image may also show the shadow cast by the target onto the retina. The OCT device generates 3D images of the target at step **118**. The 3D image **62** images a volume within the eye. A computer tracks the target using the 2D images at step **120**. In the embodiments, the computer may use the enface image of the target or the target shadow to track the target.

(30) The computer performs image processing of the images to determine features of the target at step **122**. For example, the OCT device generates a target enface image that shows a target candidate and a retinal enface image that shows a shadow, and compares the target candidate and the shadow to confirm the presence of the target. As another example, a computer program may identify an outline of the target from the target enface image, and determine the size and/or shape of the target from the outline. As another example, a computer program may detect the darkness of the target shadow from the retinal enface image, and determine the density or thickness of the target from the darkness of the shadow.

(31) The computer generates image overlays at step **124** to superimpose over images of the eye. For example, the computer may superimpose an outline of the target onto a retinal enface image, a no-fire zone onto a target enface image, or the target size, shape, and/or density onto a real time video of the eye. The computer displays the images at step **126**. The laser device directs a laser beam towards the target via the same xy-scanner at step **130**. OCT device **22** and laser device **20** share xy-scanner **24**, allowing for co-registration between the imaging and treatment beams for more precise aiming of the laser beam. The method then ends.

(32) A component (such as the control computer) of the systems and apparatuses disclosed herein may include an interface, logic, and/or memory, any of which may include computer hardware and/or software. An interface can receive input to the component and/or send output from the component, and is typically used to exchange information between, e.g., software, hardware, peripheral devices, users, and combinations of these. A user interface is a type of interface that a user can utilize to communicate with (e.g., send input to and/or receive output from) a computer. Examples of user interfaces include a display, Graphical User Interface (GUI), touchscreen, keyboard, mouse, gesture sensor, microphone, and speakers.

(33) Logic can perform operations of the component. Logic may include one or more electronic devices that process data, e.g., execute instructions to generate output from input. Examples of such an electronic device include a computer, processor, microprocessor (e.g., a Central Processing Unit (CPU)), and computer chip. Logic may include computer software that encodes instructions capable of being executed by an electronic device to perform operations. Examples of computer software include a computer program, application, and operating system.

(34) A memory can store information and may comprise tangible, computer-readable, and/or computer-executable storage medium. Examples of memory include computer memory (e.g., Random Access Memory (RAM) or Read Only Memory (ROM)), mass storage media (e.g., a hard disk), removable storage media (e.g., a Compact Disk (CD) or

Digital Video or Versatile Disk (DVD)), database, network storage (e.g., a server), and/or other computer-readable media. Particular embodiments may be directed to memory encoded with computer software.

(35) Although this disclosure has been described in terms of certain embodiments, modifications (such as changes, substitutions, additions, omissions, and/or other modifications) of the embodiments will be apparent to those skilled in the art. Accordingly, modifications may be made to the embodiments without departing from the scope of the invention. For example, modifications may be made to the systems and apparatuses disclosed herein. The components of the systems and apparatuses may be integrated or separated, or the operations of the systems and apparatuses may be performed by more, fewer, or other components, as apparent to those skilled in the art. As another example, modifications may be made to the methods disclosed herein. The methods may include more, fewer, or other steps, and the steps may be performed in any suitable order, as apparent to those skilled in the art.

(36) To aid the Patent Office and readers in interpreting the claims, Applicants note that they do not intend any of the claims or claim elements to invoke 35 U.S.C. § 112(f), unless the words “means for” or “step for” are explicitly used in the particular claim. Use of any other term (e.g., “mechanism,” “module,” “device,” “unit,” “component,” “element,” “member,” “apparatus,” “machine,” “system,” “processor,” or “controller”) within a claim is understood by the applicants to refer to structures known to those skilled in the relevant art and is not intended to invoke 35 U.S.C. § 112(f).

Claims

1. An ophthalmic laser surgical system for imaging and treating a target in an eye, comprising: an optical coherence tomography (OCT) device configured to: direct an imaging beam along an imaging beam path towards the eye, the eye having an eye axis, the eye axis defining a z-axis, the z-axis defining a plurality of xy-planes within the eye; receive the imaging beam reflected from the eye; generate three-dimensional (3D) image data from the reflected imaging beam; and generate a plurality of two-dimensional (2D) enface images from the 3D image data, a 2D enface image imaging an xy-plane within the eye, the plurality of 2D enface images comprising at least one target enface image imaging the target in the eye and a retinal enface image imaging a retina of the eye, the retinal enface image showing a shadow cast by the target onto the retina; a laser device configured to direct a laser beam along a laser beam path towards the target; an xy-scanner configured to: receive the imaging beam from the OCT device and direct the imaging beam along the imaging beam path towards the eye; and receive the laser beam from the laser device and direct the laser beam along the laser beam path aligned with the imaging beam path towards the eye; and a computer configured to: compare the target of the target enface image and the shadow of the retinal enface image to confirm the presence of the target.
2. The ophthalmic laser surgical system of claim 1, the target comprising a vitreous eye floater.
3. The ophthalmic laser surgical system of claim 1, the OCT device configured to generate the two-dimensional (2D) enface images from the 3D image data by: taking a slice of the 3D image data; and summing data of the slice to yield a 2D enface image.
4. The ophthalmic laser surgical system of claim 1, the OCT device configured to generate the two-dimensional (2D) enface images from the 3D image data by: taking a slice of the 3D image data; and averaging data of the slice to yield a 2D enface image.
5. The ophthalmic laser surgical system of claim 1, the OCT device configured to generate the two-dimensional (2D) enface images from the 3D image data by: taking a slice of the 3D image data; and projecting data of the slice to yield a 2D enface image.
6. The ophthalmic laser surgical system of claim 1, the computer configured to: perform image processing on the target enface image to determine a feature of the target.
7. The ophthalmic laser surgical system of claim 6, the computer configured to: perform image processing on the target enface image to identify an outline of the target; and determine a size of the target from the outline of the target.
8. The ophthalmic laser surgical system of claim 6, the computer configured to: perform image processing on the target enface image to identify an outline of the target; and determine a shape of the target from the outline of the target.
9. The ophthalmic laser surgical system of claim 1, the computer configured to: track the target according to the target enface image imaging the target.
10. The ophthalmic laser surgical system of claim 1, the computer configured to: track the target by tracking the shadow cast by the target according to the retinal enface image.
11. The ophthalmic laser surgical system of claim 1, the computer configured to: overlay an outline of the target onto the target enface image.
12. The ophthalmic laser surgical system of claim 1, the computer configured to: overlay a no-fire zone onto the target enface image.
13. The ophthalmic laser surgical system of claim 1, the OCT device configured to: generate a plurality of three-dimensional (3D) images from the 3D image data.
14. A method for imaging and treating a target in an eye, comprising: directing, by an optical coherence tomography (OCT) device, an imaging beam along an imaging beam path towards the eye, the eye having an eye axis, the eye axis defining a z-axis, the z-axis defining a plurality of xy-planes within the eye; receiving the imaging beam reflected from

the eye; generating three-dimensional (3D) image data from the reflected imaging beam; generating a plurality of two-dimensional (2D) enface images from the 3D image data, a 2D enface image imaging an xy-plane within the eye, the plurality of 2D enface images comprising at least one target enface image imaging the target in the eye and a retinal enface image imaging a retina of the eye, the retinal enface image showing a shadow cast by the target onto the retina; directing, by a laser device, a laser beam along a laser beam path towards the target; receiving, by an xy-scanner, the imaging beam from the OCT device and direct the imaging beam along the imaging beam path towards the eye; receiving, by the xy-scanner, the laser beam from the laser device and direct the laser beam along the laser beam path aligned with the imaging beam path towards the eye; and comparing, by a computer, the target of the target enface image and the shadow of the retinal enface image to confirm the presence of the target.

15. The method of claim 14, the generating the two-dimensional (2D) enface images from the 3D image data comprising: taking a slice of the 3D image data; and summing, averaging, or projecting data of the slice to yield a 2D enface image.

16. The method of claim 14, further comprising: performing, by the computer, image processing on the target enface image to determine a feature of the target.

17. The method of claim 16, the performing, by the computer, image processing on the target enface image to determine a feature of the target comprising: performing image processing on the target enface image to identify an outline of the target; and determining a size of the target from the outline of the target.

18. The method of claim 16, the performing, by the computer, image processing on the target enface image to determine a feature of the target comprising: performing image processing on the target enface image to identify an outline of the target; and determining a shape of the target from the outline of the target.

19. The method of claim 14, further comprising: tracking, by the computer, the target according to the target enface image imaging the target.

20. The method of claim 14, further comprising: tracking, by the computer, the target by tracking the shadow cast by the target according to the retinal enface image.

21. The method of claim 14, further comprising: overlaying, by the computer, an outline of the target or a no-fire zone onto the target enface image.

22. The method of claim 14, further comprising: generating, by the OCT device, a plurality of three-dimensional (3D) images from the 3D image data.

23. An ophthalmic laser surgical system for imaging and treating a target in an eye, comprising: an optical coherence tomography (OCT) device configured to: direct an imaging beam along an imaging beam path towards the eye, the eye having an eye axis, the eye axis defining a z-axis, the z-axis defining a plurality of xy-planes within the eye, the target comprising a vitreous eye floater; receive the imaging beam reflected from the eye; generate three-dimensional (3D) image data from the reflected imaging beam; and generate a plurality of two-dimensional (2D) enface images from the 3D image data by taking a slice of the 3D image data and summing, averaging, or projecting data of the slice to yield a 2D enface image, a 2D enface image imaging an xy-plane within the eye, the plurality of 2D enface images comprising at least one target enface image imaging the target in the eye and a retinal enface image imaging a retina of the eye, the retinal enface image showing a shadow cast by the target onto the retina; a laser device configured to direct a laser beam along a laser beam path towards the target; an xy-scanner configured to: receive the imaging beam from the OCT device and direct the imaging beam along the imaging beam path towards the eye; and receive the laser beam from the laser device and direct the laser beam along the laser beam path aligned with the imaging beam path towards the eye; and a computer configured to: compare the target of the target enface image and the shadow of the retinal enface image to confirm the presence of the target; perform image processing on the target enface image to determine a feature of the target by: performing image processing on the target enface image to identify an outline of the target and determining a size of the target from the outline of the target; and performing image processing on the target enface image to identify an outline of the target and determining a shape of the target from the outline of the target; track the target according to the target enface image imaging the target; track the target by tracking the shadow cast by the target according to the retinal enface image; overlay an outline of the target onto the target enface image; overlay a no-fire zone onto the target enface image; and generate a plurality of three-dimensional (3D) images from the 3D image data.
