

Reverse Correlation Uncovers More Complete Tinnitus Spectra

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Abstract—Goal: This study validates a reverse correlation method for characterizing the sounds experienced by tinnitus patients with potential for characterizing a wider range of sounds than currently possible. **Methods:** Ten normal-hearing subjects assessed the subjective similarity of random auditory stimuli and target tinnitus-like sounds (“buzzing” and “roaring”). Reconstructions of the targets were obtained by regressing subject responses on the stimuli, and were compared for accuracy to the frequency spectra of the targets using Pearson’s r . **Results:** Reconstruction accuracy was significantly higher than chance across subjects: **buzzing** ($M = 0.53$, $SD = 0.27$): $t(9) = 5.766$, $p < 0.001$; **roaring** ($M = 0.57$, $SD = 0.30$): $t(9) = 5.76$, $p < 0.001$. **Conclusion:** Reverse correlation can accurately reconstruct non-tonal tinnitus-like sounds in normal-hearing subjects, indicating its potential for characterizing the sounds experienced by patients with non-tonal tinnitus.

Index Terms—reverse correlation, tinnitus, behavioral assay

Impact Statement—Characterization of tinnitus can inform tinnitus treatment by allowing for individualized sound therapies, leading to better outcomes for patients suffering from the cognitive and psychological effects of tinnitus.

I. INTRODUCTION

TINNITUS—the perception of sound in the absence of any corresponding external stimulus—affects up to 50 million people in the U.S. [1], [2], a third of whom experience functional cognitive impairment and substantial reduction in quality of life [3]–[5]. Clinical guidelines for tinnitus management frequently involve targeted exposure to tinnitus-like sounds, either as a form of habituation therapy (termed *sound therapy*), or using Cognitive Behavioral Therapy [6]. Critically, sound therapy is shown to improve with knowledge of the patient’s internal tinnitus experience [7]–[14]. However, existing strategies for characterizing tinnitus sounds, such as Pitch Matching (PM)

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methods, are best suited for patients whose tinnitus resembles pure tones (e.g., ringing), which may represent only 20–50% of patients [15]–[17]. There is a pressing need for more robust characterization methods [18]–[21].

Tinnitus sounds are presumed to be complex and heterogeneous [18], [22], [23], although few specifics have been firmly established. Therefore, we base our approach on *reverse correlation* (RC), an established behavioral method [24]–[26] for probing internal representations of visual and auditory percepts, unconstrained by prior knowledge. RC asks subjects to render subjective judgments over random stimuli, from which unbiased estimates of the percepts can be produced. RC is closely related to Wiener theory [27], which has inspired “white-noise” approaches to system characterization in physiology [28], [29] and engineering [30].

Here, we validate RC as a method for characterizing all component frequencies of non-tonal tinnitus sounds by estimating the full psychoacoustic tinnitus spectrum (PTS). To that end, we asked normal-hearing participants to complete an augmented RC experiment, comparing random stimuli to a target sound. The estimated PTS were subsequently validated against the targets. Our results demonstrate, for the first time, that tinnitus-like sounds with complex spectra can be accurately estimated using RC.

II. MATERIALS AND METHODS

A. Stimuli

Stimuli were composed of $b = 8$ Mel-spaced frequency bins, which divide the frequency spectrum between [100, 13,000] Hz into continuous segments of equal amplitude (i.e., “rectangular” bins). Reconstruction detail increases with b , but $b = 8$ provides a good approximation to the chosen target sounds (see Fig. 3).

For each stimulus, [2, 7] bins were randomly “filled” with power 0 dB. “Unfilled” bins were assigned a power of –100 dB. Assigning random phase, the inverse Fourier transform of the spectrum yields a 500 ms stimulus waveform.¹

B. Target Sounds

Two spectrally complex and complimentary target sounds (“buzzing” and “roaring”) were downloaded from the American Tinnitus Association [31] and truncated to 500 ms in duration.

¹Software for the experiments and analysis was written in MATLAB and is freely available at <https://github.com/alec-hoyland/tinnitus-reconstruction/>

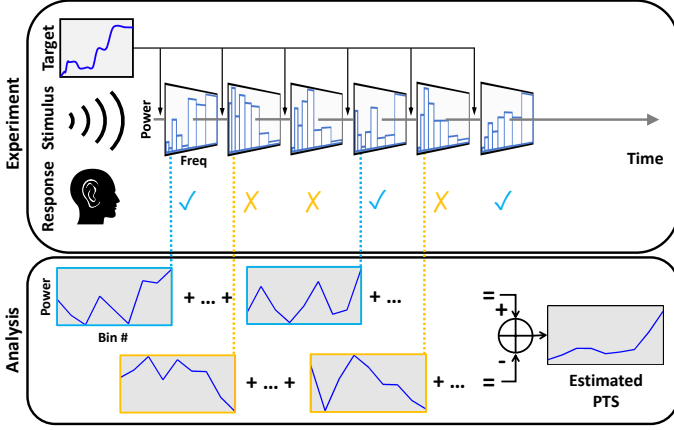


Fig. 1. Diagram of the experimental protocol. Subjects listen to a series of random stimuli, each preceded by a target sound. Subjects compare the stimulus to the target, and respond either “yes” or “no” depending on their perceived similarity. The recorded stimulus-response pairs are used to form an estimate of the target.

C. Experiment

10 normal-hearing subjects listened to the same target sound followed by a random stimulus for each trial (Fig. 1). The task is designed to mimic how a tinnitus patient might compare random stimuli to their tinnitus.

Subjects were instructed to respond “yes” to any stimuli that sounded similar to the target, and “no” otherwise. Subjects completed 200 trials for both target sounds within 10–20 minutes.

D. Reconstruction

A subject performing n RC trials with b frequency bins produces a stimulus matrix $\Psi \in \mathbb{R}^{b \times n}$ and a response vector $y \in \{1, -1\}^n$, where 1 corresponds to a “yes” response and -1 to a “no.” RC classically assumes the subject response model:

$$y = \text{sign}(\Psi^T x), \quad (1)$$

where $x \in \mathbb{R}^b$ is the subject’s internal representation of interest (e.g., their tinnitus percept). This model can be inverted, yielding the following formula:

$$\hat{x} = \frac{1}{n} \Psi y \quad (2)$$

This formula is a restricted form of the Normal equation, under the assumption that the stimulus dimensions are uncorrelated [25]. Intuitively, \hat{x} is the sum of all stimuli eliciting a “yes” response, after subtracting all stimuli eliciting a “no.”

E. Validation

The experimental paradigm allows for direct validation of the reconstructions \hat{x}_{buzzing} and \hat{x}_{roaring} . We represent the spectra of the target sounds as vectors $s_{\text{buzzing}} \in \mathbb{R}^b$ and $s_{\text{roaring}} \in \mathbb{R}^b$ using the same frequency bins as in stimulus generation with power equal to the mean power of frequencies within that bin. Pearson’s r between s_{buzzing} and s_{roaring} and their corresponding reconstructions represents reconstruction accuracy. One-sample

t-tests were performed on the mean Fisher-transformed Pearson’s r values across subjects to assess significant differences from zero.

F. Synthetic Subjects

To establish bounds on human performance, additional experiments were run with two simulated subjects who give either *ideal* or *random* responses. Each experiment ran for $n = 200$ trials and was repeated 1000 times.

The *ideal* subject gives responses following:

$$y_i = \begin{cases} 1 & \text{if } \Psi_i s \geq Q(0.5; \Psi s) \\ -1 & \text{otherwise} \end{cases} \quad (3)$$

for $i \in 1, \dots, n$, where $Q(x, y)$ is the quantile function for $x \in [0, 1]$ of the similarity calculation Ψs , and Ψ_i is the i^{th} column of Ψ . The ideal subject has precise knowledge of every stimulus and responds mirroring Eq. 2.

The *random* subject responds with uniformly random probability.

III. RESULTS

Figure 2 shows the distribution of Pearson’s r for human, ideal, and random subject responses. Human accuracies were generally higher than random, with some approaching ideal. Mean random accuracy was 0 in all conditions, while mean human accuracy was significantly different from 0 in all conditions: buzzing: $t(9) = 5.766$, $p < 0.001$; roaring: $t(9) = 5.76$, $p < 0.001$; combined: $t(19) = 7.542$, $p < 0.001$. Greater variability in buzzing results may stem from the target spectrum containing significant high-frequency content, increasing the difficulty for subjects with minor high-frequency hearing loss. Figure 3 plots the most accurate human reconstructions over the target sound spectra.

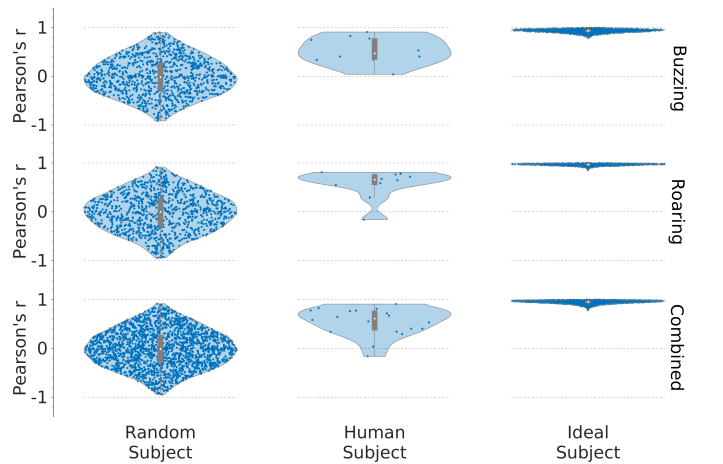


Fig. 2. Human reconstruction accuracy is significantly above baseline, but is not optimal. Random, human, and ideal reconstruction accuracies are shown as violin plots with box plots overlaid. The median is a white dot, the ordinate of the blue points are the Pearson’s r values.

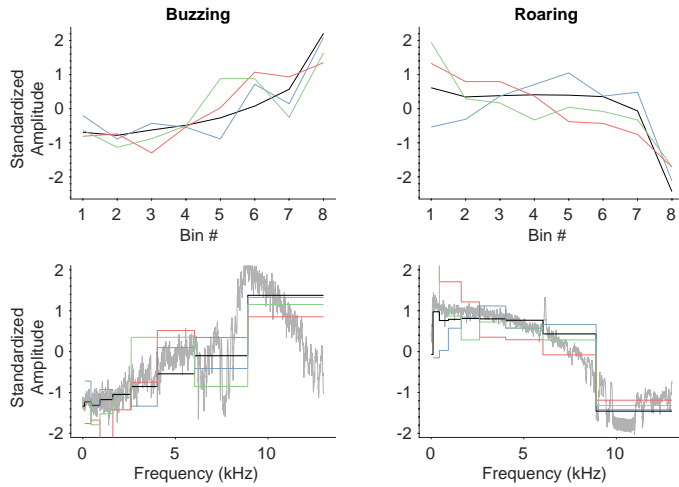


Fig. 3. Reconstructions of the PTS capture many salient features of tinnitus spectra. The black trace indicates the target, while colored traces plot exemplar human reconstructions. The top row shows standardized power levels within each frequency bin. The bottom row maps the 8-dimensional bin domain to a 11025-dimensional frequency domain with the unbinmed power spectral density of the targets shown in gray.

IV. CONCLUSION

Reconstruction accuracies observed here are well below the simulated ideal, which may be attributed to noisy responses universally observed in applications of RC. This may be mitigated by optimizing the experimental protocol, stimulus generation, and reconstruction method. For example, recent approaches to improving RC reconstruction methods can boost efficiency, noise robustness and overall accuracy [32], [33].

Nevertheless, our results show that RC can accurately reconstruct the frequency spectrum of complex, non-tonal tinnitus-like sounds. This indicates that RC may also be useful for developing a clinical assay to characterize a wider variety of tinnitus percepts than currently possible. Additionally, subjects completed the required number of trials within 20 minutes, indicating that this procedure could be conducted in a single clinical visit. Future work will focus on validating this approach in patients suffering from tinnitus.

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