

CSE475: Machine Learning[Fall 2025]

Section : 02

Group Number : 08

Submitted by:

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## Related Work

Ref.	Title	Dataset Description	Methods	Results	Pros	Cons	Future Work
1	<b>Study on the use of standard 12-lead ECG data for rhythm-type ECG classification problems</b> (Park et al.)	Large standard 12-lead ECG dataset (13,241 tests) from <b>Konkuk University Hospital</b> (used for analysis) and <b>Seoul National University Bundang Hospital</b> (used for verification),. Data was categorized into <b>5 rhythm classes</b> (Normal, AF, APC, VPC, and "other"). Data frequency was downsampled from 500 Hz to <b>200 Hz</b>	Proposed a methodology for <b>fusion of various single-lead ECG data as training data</b> for single-lead classification,. Used a <b>152-layer Squeeze-and-Excitation Residual Network (SE-ResNet)</b> as the baseline model. Included transformation of Lead aVR to <b>Lead -aVR</b> . Evaluation used Accuracy and F1 score.	The classification performances achieved by the 152-layer SE-ResNet using Leads -aVR and II were the best overall, associated with F1 scores of 97.5% and 97.4%, respectively . Specifically, the model trained on the fusion of single-lead ECGs achieved a high F1 score using <b>Lead -aVR</b> for the most fundamental	Methodology offers an <b>alternative to improve the ECG classification performance of wearable devices</b> that measure only single-lead ECG. Performance on critical arrhythmias (AF, APC, VPC) was <b>higher than previous studies</b> .	<b>F1 scores for APC were much lower</b> than for other diagnoses, suggesting potential <b>insufficient APC-scored data</b> . The <b>optimal combination of single-lead ECG data was not confirmed</b> .	Focus on <b>increasing the F1 scores for APC</b> . Develop methods to <b>find the best combination of ECG leads</b> , including <b>nonlinear transformation</b> . Implement training data that includes <b>mechanically generated noise</b> (e.g., power line noise, baseline wander).

				rhythm classes: • <b>Normal</b> (98.7%) • <b>AF</b> (98.2%) • <b>APC</b> (95.1%) • <b>VPC</b> (97.4%)			
2	<b>In-Distribution and Out-of-Distribution Self-supervised ECG Representation Learning for Arrhythmia Detection</b> (Soltanieh et al.)	<b>PTB-XL</b> (12-lead, 21,837 records, 100Hz), <b>Chapman</b> (12-lead, 10,646 records, downsampled to 100Hz), and <b>Ribeiro</b> (test set only, 827 samples, downsampled to 100Hz),,. Datasets confirmed suitable for cross-dataset OOD analysis.	Conducted systematic investigation of <b>Self-Supervised Learning (SSL)</b> in <b>In-Distribution (ID)</b> and <b>Out-of-Distribution (OOD)</b> settings. Evaluated three SSL methods: <b>SimCLR</b> , <b>BYOL</b> , and <b>SwAV</b> , using <b>xResNet1d50</b> as the backbone. Used diverse augmentations (Gaussian Noise, Masking, Time Warping, etc.)	<b>SwAV</b> consistently achieved the <b>best overall results</b> across all explored datasets in ID and OOD settings. SSL methods achieved <b>comparable performances for ID and OOD data</b> , indicating learned representations generalize well. The SSL model (SwAV) showed <b>greater robustness against synthetic 60 Hz power line interference</b> than the	SSL methods <b>outperform fully supervised training</b> . SSL effectively enhances model <b>generalization to OOD scenarios</b> . The models, particularly SwAV, are robust against common ECG noise.	Features corresponding to some diseases (HYP and STTC) proved <b>more challenging to learn</b> compared to others.	Investigate <b>finer step sizes and wider parameter ranges</b> for augmentations. Examine <b>more sophisticated augmentations</b> (e.g., in the frequency domain). Expand the number of <b>SSL methods and backbone encoders</b> . Collect a <b>combination of different datasets for pre-training</b> for improved generalizability.

				fully-supervised model			
3	<b>Subject-based Non-contrastive Self-Supervised Learning for ECG Signal Processing (Atienza et al.)</b>	Training Dataset: <b>The Sleep Heart Health Study (SHHS)</b> (2,643 subjects with two records each),. Evaluation Datasets: <b>MIT-BIH Arrhythmia Database (MIT Arr), MIT-BIH Atrial Fibrillation Database (MIT AFib), and MIT-BIH Polysomnographic Database (MIT PSG)</b> (all publicly available on PhysioNet)	Proposed <b>SBnCL</b> (Subject-based Non-contrastive Self-Supervised Learning) method that operates <b>without data augmentation or negative pairs</b> . Compared performance using a <b>Vision Transformer (ViT)-based model</b> against a <b>CNN-based XResNet50</b> ,. Evaluation included gender classification and downstream tasks like age regression and sleep stage classification	The ViT-SBnCL model achieved comparable performance to existing methods in extracting <b>stable, subject-based static features</b> such as gender ( <b>95.7%</b> accuracy),. The <b>ViT model showed a higher learning capability</b> than the CNN-based XResNet50	Demonstrated that <b>neither data augmentations nor negative pairs are necessary</b> for learning useful representations. The proposed method allows for the design of SSL models capable of capturing <b>dissimilarities</b> (instead of just similarities).	The model <b>failed to capture dynamic characteristics</b> such as <b>arrhythmias (AFib) or sleep stages</b> . The training dataset (SHHS) contained a <b>smaller number of subjects</b> (2,643 subjects) compared to other studies (e.g., PCLR study).	Design a <b>new SSL method that captures dissimilarities as well as similarities</b> to improve representation learning for <b>transient states</b> and different rhythm diseases
4	<b>ECG</b>	Multiclass	Proposed the	Overall	Achieved	SqueezeNet	Improve the

	<b>Classification for Detecting ECG Arrhythmia Empowered with Deep Learning Approaches</b> (Rahman et al.)	ECG classification dataset taken from <b>Kaggle</b> (16,879 images), which was <b>augmented and fused with the MIT-BIH dataset</b> ,. The model classified <b>five classes</b> : F, N, Q, S, and V. Images were preprocessed to dimensions of 227×227.	<b>CAA-TL</b> (ECG Classification for Detecting ECG Arrhythmia Empowered with Transfer Learning) model. Compared and used transfer learning on three deep learning models: <b>AlexNet</b> (25 layers), <b>SqueezeNet</b> (68 layers), and <b>ResNet50</b> (177 layers),. The train/validation split was 80:20.	accuracy achieved was: <b>AlexNet 98.38%</b> , SqueezeNet 90.08%, and ResNet50 91%,. <b>AlexNet</b> was found to be the <b>most effective method</b> as it could train and validate <b>all</b> the classes. SqueezeNet and ResNet50 showed outstanding accuracy for classes Q, S, and V but <b>failed to train the N (Normal) class</b> effectively,,.	<b>remarkable accuracy</b> compared to previous machine learning methods. <b>Augmentation</b> and image processing were applied to increase the number of images.	and ResNet50 showed <b>poor performance or failure to detect specific classes</b> (N and F),. The computational complexity is significant.	dataset quality for classes showing less accuracy ( <b>N and F</b> classes),. Improve computational speed using <b>GPU or AWS cloud computing service</b> . Apply the innovative approach of <b>federated deep learning</b> to enhance security and consistency. Utilize <b>K fold Cross-validation</b> .
5	<b>Deep Learning for ECG Analysis: Benchmarks and Insights from PTB-XL</b> (Strodthoff et al.)	Primary Dataset: <b>PTB-XL</b> (21,837 12-lead ECG records from 18,885 patients). Annotations cover three	Proposed and evaluated a new <b>resnet-adaptation (xresnet1d101)</b> along with other CNN (ResNet and	<b>xresnet1d101</b> showed the <b>strongest performance</b> across all tasks (macro AUC up to <b>0.96</b> in <i>rhythm</i> category),.	Established <b>comprehensive benchmarking results</b> for deep learning algorithms on the PTB-XL dataset. Demonstrated	Recurrent architectures were <b>less performant</b> than convolutional counterparts. The performance of	Conduct further studies on <b>co-occurring pathologies</b> to identify hidden stratification. Analyze the correlation of <b>human-provid</b>

		<p>non-mutually exclusive categories: <i>diagnostic</i>, <i>form</i>, and <i>rhythm</i>. Secondary dataset for transfer learning validation: <b>ICBEB2018</b> (6877 12-lead ECGs).</p>	<p>Inception variants), Recurrent (LSTM, GRU), and feature-based (Wavelet+NN) architectures,,. Tasks included ECG statement prediction, age regression, and sex prediction. Used <b>transfer learning</b> by fine-tuning models pretrained on PTB-XL onto ICBEB2018. Primary metric: macro-average d AUC.</p>	<p><b>Transfer learning was highly effective in the small dataset regime.</b> Age regression achieved MAE = <b>6.86 years</b> (on normal subjects). Sex prediction achieved AUC of <b>0.96</b> (on normal patients).</p>	<p>the <b>prospects of transfer learning</b> using PTB-XL as a resource, reducing the amount of target data required. Provided evidence of <b>hidden stratification</b> and successful comparison of <b>model uncertainty with human-provided diagnosis likelihoods</b>,.</p>	<p>the feature-based approach (<b>Wavelet+NN</b>) was significantly lower than the deep learning models.</p>	<p><b>ed diagnosis likelihoods with model uncertainties.</b> Apply <b>interpretability methods</b> (e.g., relevance propagation) for statistical analysis of attribution maps,.</p>
6	<p><b>SELF-SUPERVISED PRE-TRAINING with Joint-Embedding Predictive Architecture Boosts ECG Classification Performance</b> (Weimann &amp; Conrad, 2023)</p>	<p>Unsupervised pre-training dataset combining <b>ten public ECG databases</b> (including MIMIC-IV-ECG, CODE-15, PTB-XL, etc.) totaling <b>over one million</b></p>	<p>Proposed the use of the <b>Joint-Embedding Predictive Architecture (JEPA)</b> for self-supervised pre-training, which predicts latent features,. The model architectures</p>	<p>JEPA achieved <b>state-of-the-art performance</b> on the PTB-XL <i>all statements</i> task with an AUC of <b>0.945</b> (ViT-S, two-stage fine-tuning), surpassing the previous</p>	<p>JEPA overcomes limitations of traditional SSL methods by <b>predicting latent features and not relying on hand-crafted data augmentations</b></p>	<p>Increasing model size (ViT-B) or expanding dataset diversity beyond MIMIC-IV-ECG provided <b>negligible impact</b> on performance,</p>	<p>Study <b>different techniques for unsupervised or self-supervised pretraining</b> that do not rely on expensive human annotations.</p>

		<p><b>ECG records.</b> Evaluation performed on various <b>PTB-XL benchmarks.</b></p>	<p>were <b>Vision Transformers (ViT)</b> in three configurations: <b>ViT-B, ViT-S, and ViT-XS.</b> Implemented a <b>masking strategy</b> to create compatible pairs. Evaluation included linear evaluation, fine-tuning, and two-stage fine-tuning.</p>	<p>benchmark (CPC, 0.942 AUC),,. <b>JEPA consistently learned the highest quality representations</b>, confirmed by linear evaluation (ViT-S: <b>0.940 AUC</b>),. Pre-training was <b>always advantageous</b>, even when using no additional data beyond PTB-XL.</p>	<p>. Achieved <b>state-of-the-art performance</b> across multiple PTB-XL benchmarks,. Demonstrated strong feature quality in <b>linear evaluation.</b></p>	<p>suggesting larger models may require even more data to utilize full capacity.</p>	
7	<p><b>ECG classification using 1-D convolutional deep residual neural network</b> (Khan et al.)</p>	<p><b>PhysioNet MIT-BIH Arrhythmia database</b> (48 two-channel recordings, 360 Hz),. Heartbeats are grouped into <b>five AAMI Standard classes</b>: N, S, V, F, and Q. The dataset is <b>highly</b></p>	<p>Proposed a <b>1-D convolutional deep Residual Neural Network (ResNet)</b> for feature extraction. Employed the <b>Pan-Tompkins algorithm</b> for R-peak detection and heartbeat segmentation,.</p>	<p>Achieved an <b>average accuracy of 98.63%</b> and an average F1-score of <b>92.63%</b> on the test dataset,. The deeper ResNet model performed significantly well with <b>increased network</b></p>	<p>The model performed feature extraction directly from heartbeats, avoiding separate, complex signal processing phases. <b>SMOTE effectively addressed the severe</b></p>		

		<b>class-imbalanced</b> (82.8% of beats belong to the N class).	Utilized the <b>Synthetic Minority Oversampling Technique (SMOTE)</b> <b>exclusively on the training dataset</b> to mitigate class imbalance,,. Evaluation used 10-fold cross validation.	<b>depth.</b> Accuracy was significantly higher with SMOTE (98.62%) than without (95%).	<b>class-imbalanced problem.</b>		
8	<b>ECG signal classification based on deep CNN and BiLSTM</b> (Cheng et al.)	Dataset provided by the <b>2017 PhysioNet/CI NC Challenge</b> (8,528 single-lead records),. Data was screened down to 7,561 records with a minimum dimension of 9,000,. Divided into four types: <b>AF, Normal, Other rhythm, and Noise.</b>	Developed a dense heart rhythm network combining a <b>24-layer Deep Convolutional Neural Network (DCNN)</b> and <b>Bidirectional Long Short-Term Memory (BiLSTM)</b> ,. Preprocessing used a <b>combined filter of wavelet</b>	Obtained an overall <b>accuracy rate of 89.3%</b> and an <b>F1 score of 0.891</b> through ten-fold cross validation,. The <b>TMSE loss function effectively suppressed outliers</b> and achieved better accuracy compared to cross-entropy and MSE methods.	The model successfully mined deep-level and <b>time-sensitive features</b> using the combined DCNN and BiLSTM network. The combined filtering method ( <b>WT and MT</b> ) effectively reduced noise and protected signal features.	The filtering effect <b>declined for data collected by ECG acquisition instruments from different manufacturers</b> . The network layers were relatively shallow due to <b>hardware limitations.</b>	Study <b>more robust preprocessing methods</b> to handle different manufacturers' data. Explore using <b>deeper layers</b> for the DCNN and BiLSTM networks. <b>Transplant the classification algorithm to portable terminal devices</b> for dynamic ECG monitoring.



			<b>transform (WT) and median filtering (MT)</b> for noise reduction and baseline drift elimination,,. Proposed a new loss function: <b>Tan Mean Square Error (TMSE)</b> , to control loss fluctuation and suppress outliers.				
9	<b>Transfer learning for ECG classification</b> (Weimann & Conrad, 2021)	Upstream (Pre-training) dataset: <b>Icentia11K</b> (single lead, 250 Hz, 11,000 patients, over 630,000 hours of ECG). Downstream (Finetuning) dataset: <b>PhysioNet/Cin C Challenge 2017 data set</b> (8528 single-lead episodes). Also	Used <b>transfer learning</b> to pretrain CNNs (primarily <b>ResNet-18v2</b> , <b>ResNet-34v2</b> , and <b>ResNet-50v2</b> ) and fine-tune for AF classification. Pretraining tasks included supervised (Beat/Rhythm Classification) and self-supervised	Pretraining improved the macro F1 score on the target task by up to <b>6.57%</b> (Beat Classification pretraining) over random initialization. The pretraining improvement was substantial in the <b>small dataset regime</b> . <b>ResNet-34v2</b> yielded the	Transfer learning <b>improved performance and accelerated training</b> . The approach <b>effectively reduces the number of annotations required</b> to achieve comparable performance. Unsupervised pretraining	Supervised pretraining was generally the <b>better choice</b> if labels were available. The largest model ( <b>ResNet-50v2</b> ) suffered a performance decline, suggesting potential resource or pretraining schedule limitations.	Collect a <b>massive ECG database</b> that reflects data heterogeneity to pretrain large networks. Study <b>different techniques for unsupervised or self-supervised pretraining</b> since they avoid expensive human annotations.

		tested generalization on PTB-XL and ICBEB2018 (12-lead datasets).	( <b>Future Prediction</b> , an adaptation of <b>Contrastive Predictive Coding [CPC]</b> using a <b>Transformer-based attention pooling module</b> ), The primary metric was the macro <b>F1 score</b> .	highest performance improvement (4.51% increase over baseline),.	methods are a <b>viable method</b> for improving performance.		
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Reference:

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