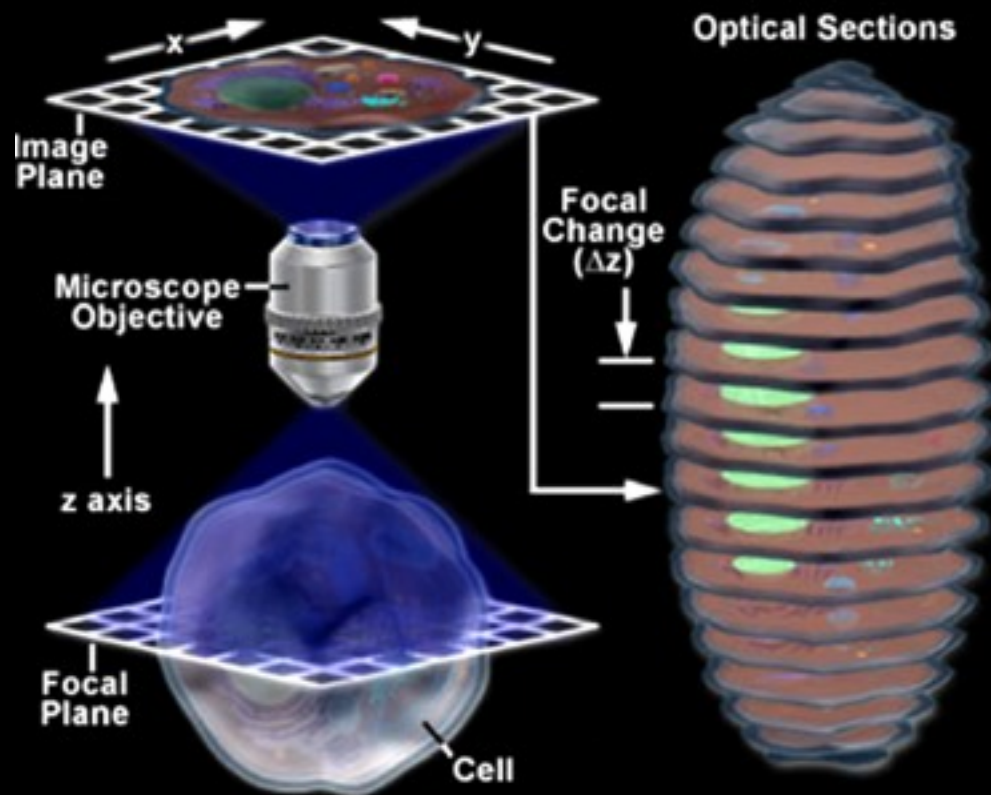


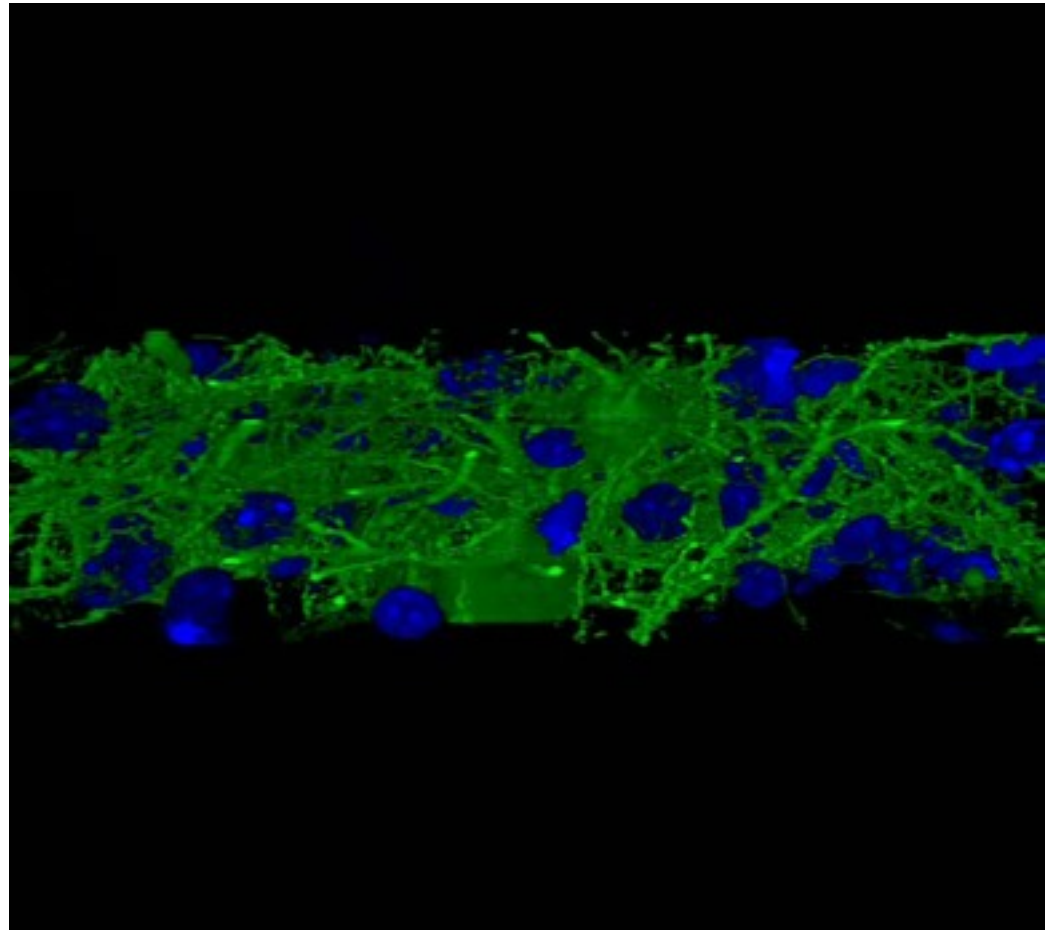
Optical Sectioning



Bo Huang
Pharmaceutical Chemistry

Approaches to 3D imaging

- Physical cutting
 - Technical difficulty
 - Highest resolution
 - Highest sensitivity
- Optical sectioning
 - Simple sample prep.
 - No physical damage
- Tomography



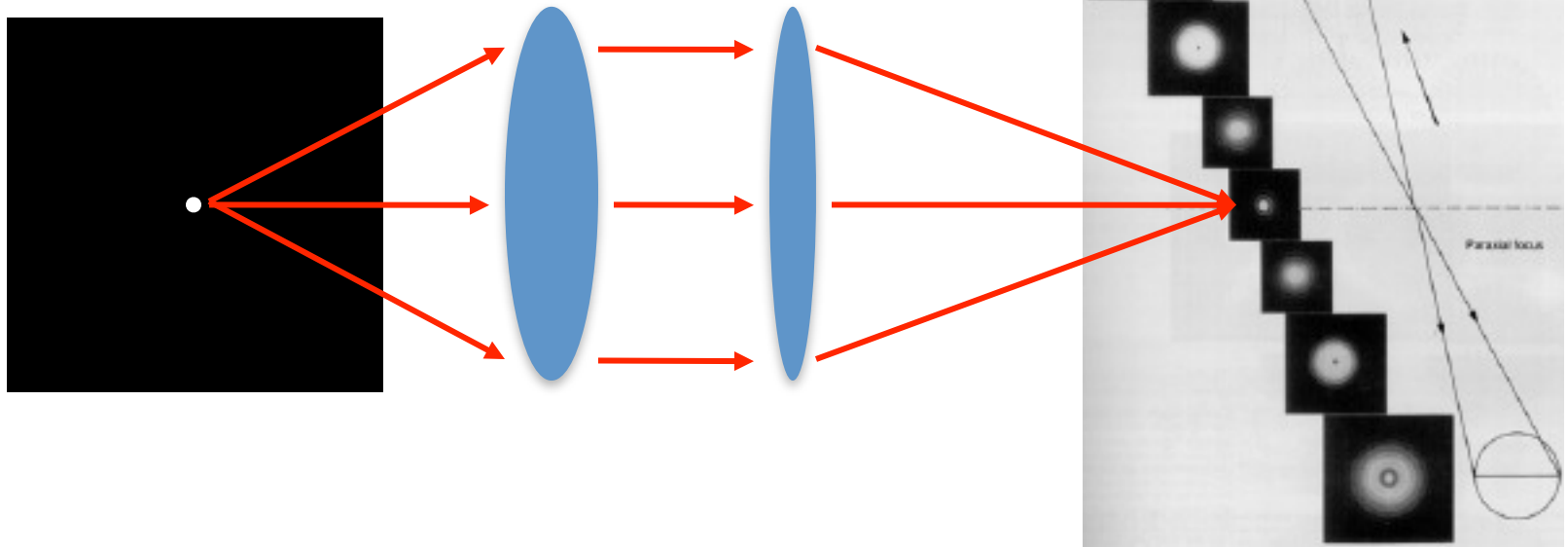
Micheva & Smith, Neuron (2007)

Optical sectioning

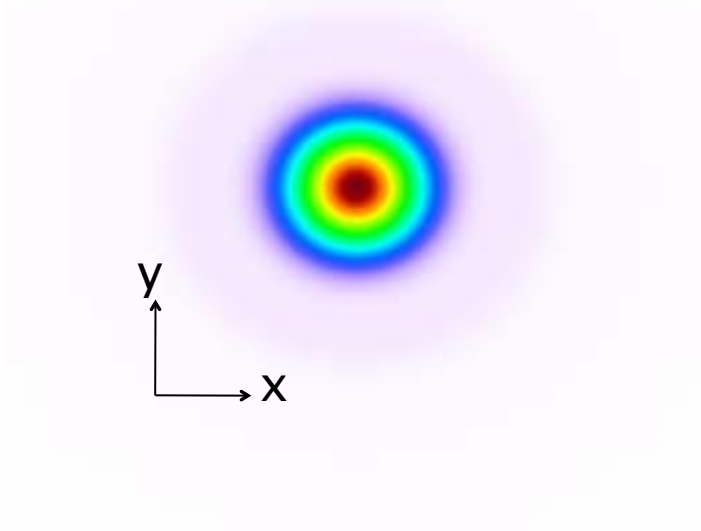
- Confocal microscopy principle
- Point scanning confocal
- Multi-point scanning confocal
 - Spinning disk
- Two-photon microscopy
- Total internal reflection fluorescence (TIRF)
- Other methods

The Point Spread Function (PSF)

- PFS: the three dimensional image of a point object
- (Almost) equivalent: the 3D focus of a laser

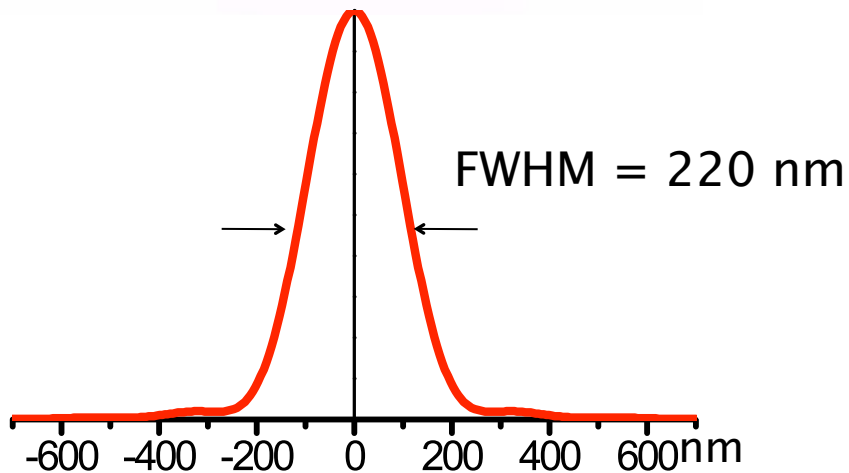


The lateral size of the PSF

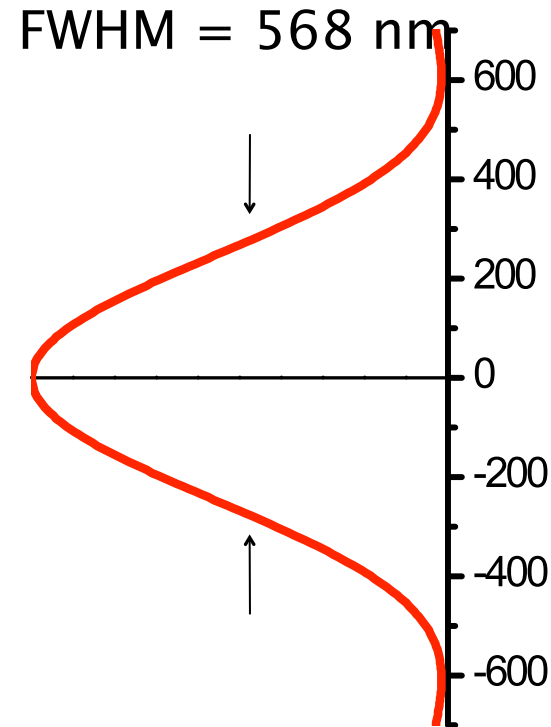
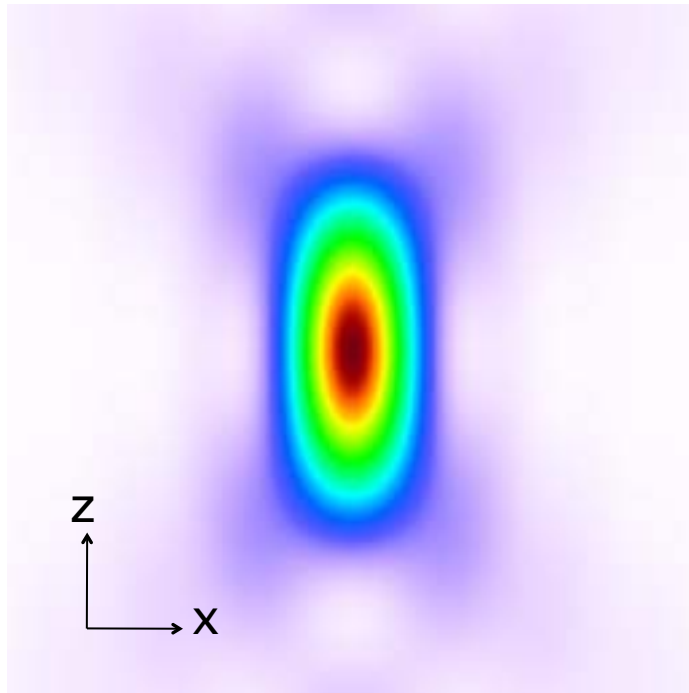


Lateral resolution $\approx \frac{0.61\lambda}{NA}$

Example: 1.4 NA objective at 550 nm
 $\Delta_{xy} \approx 240 \text{ nm}$



The axial size of the PSF

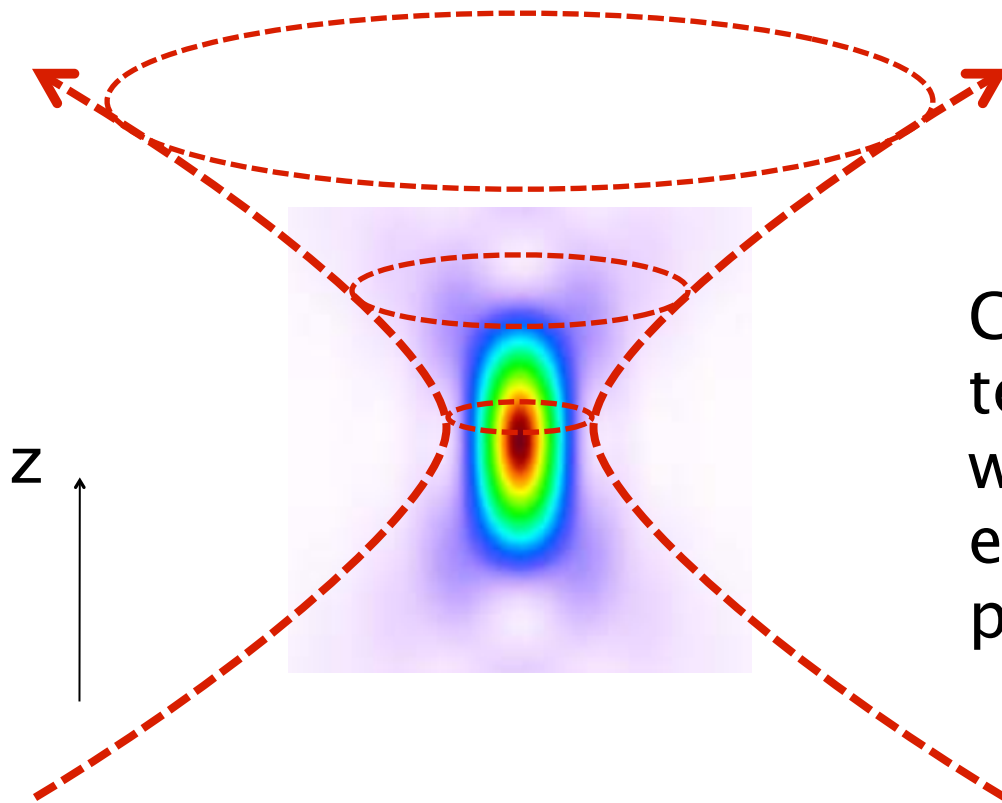


Axial resolution $\approx \frac{2n\lambda}{NA^2}$
(works only for low NA system)

Example: 1.4 NA objective at 550 nm

$\Delta_z \approx 850 \text{ nm}$

z resolution \neq z sectioning



Conservation of energy tells that the detector will collect the signal equally well at any z position

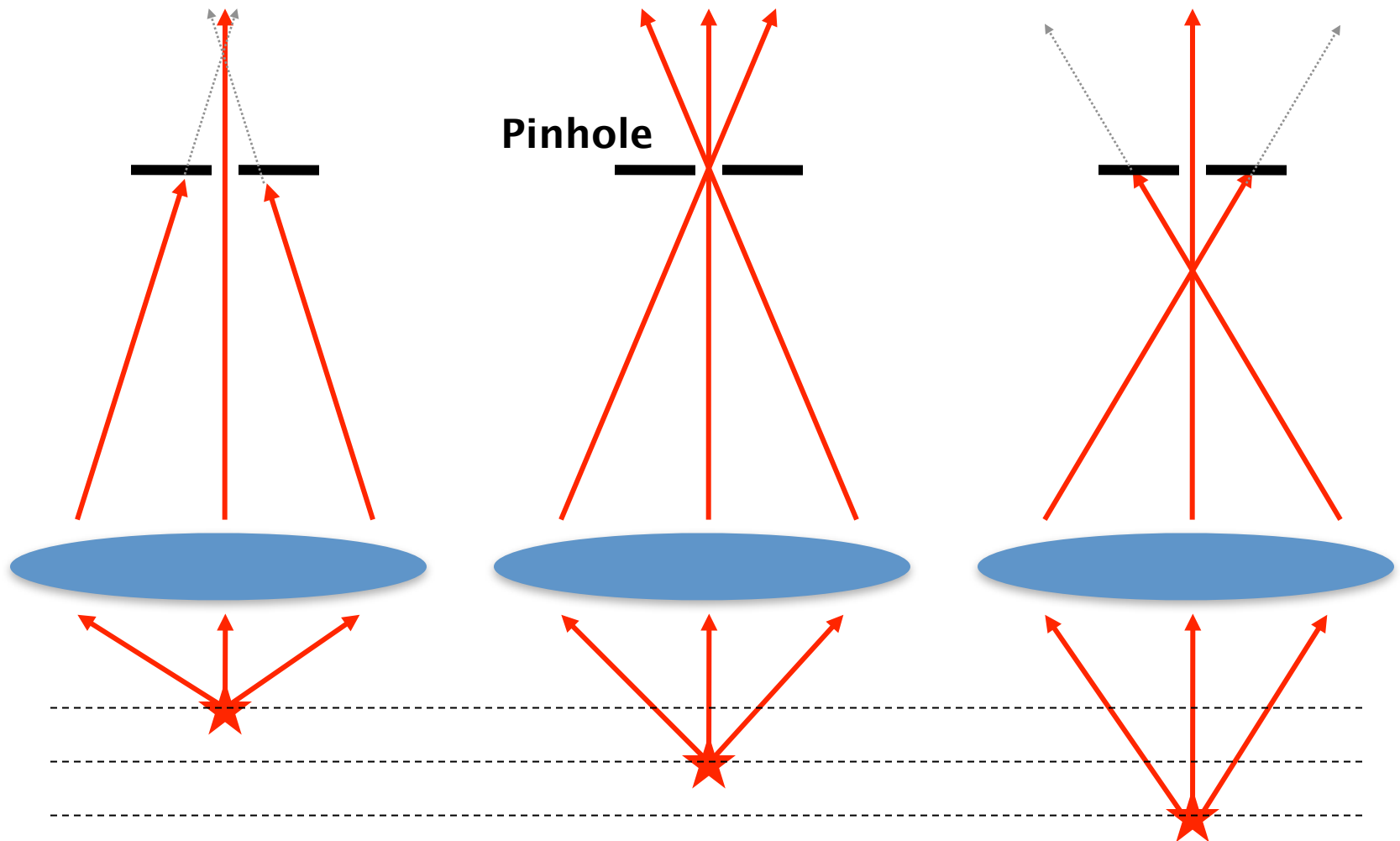
How to achieve optical

- Mathematics
 - Deconvolution microscopy
- Limiting the detection depth
 - Confocal microscopy
- Limiting the excitation depth
 - Two-photon microscopy
 - Total internal reflection fluorescence (TIRF) microscopy
 - Single plane illumination microscopy (SPIM)

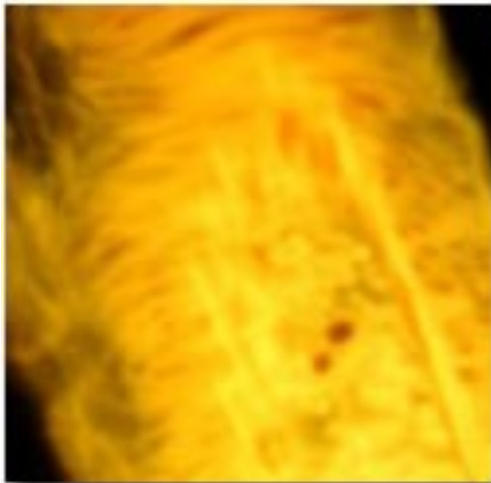
z



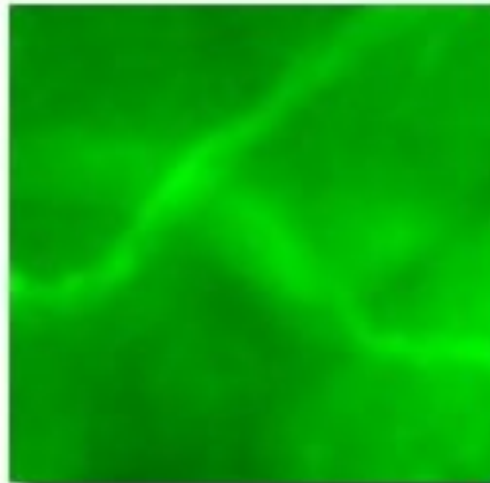
Principle of confocal



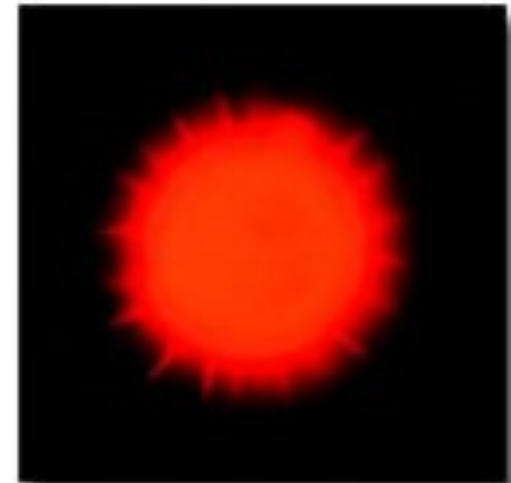
Confocal vs. widefield fluorescence microscopy



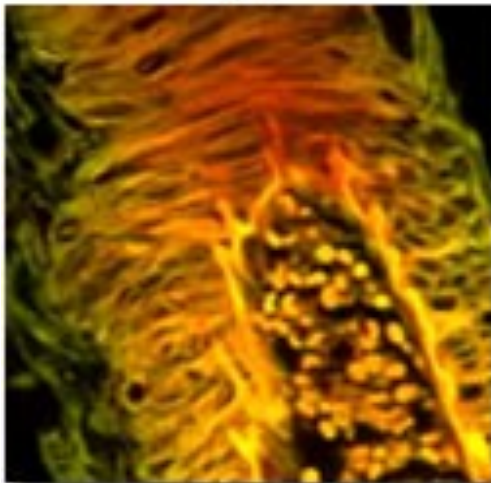
(a)



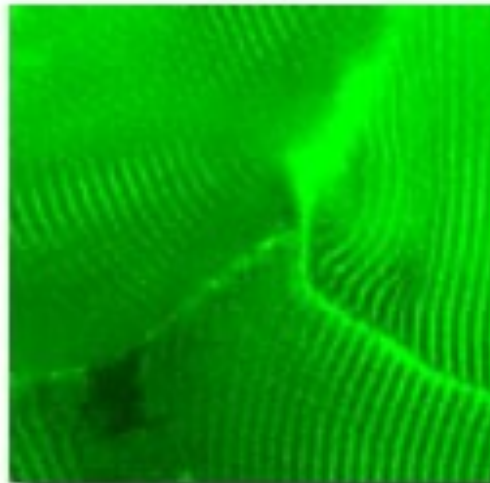
(b)



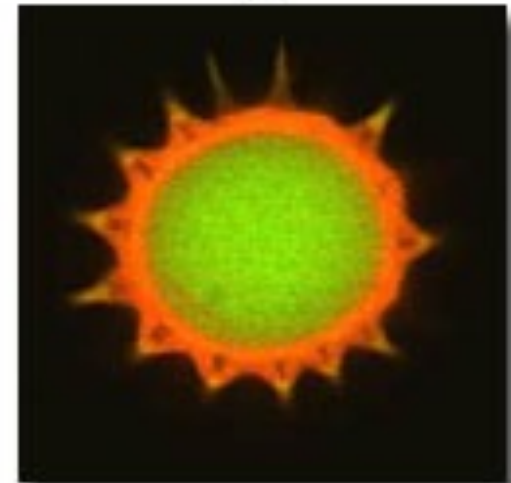
(c)



(d)

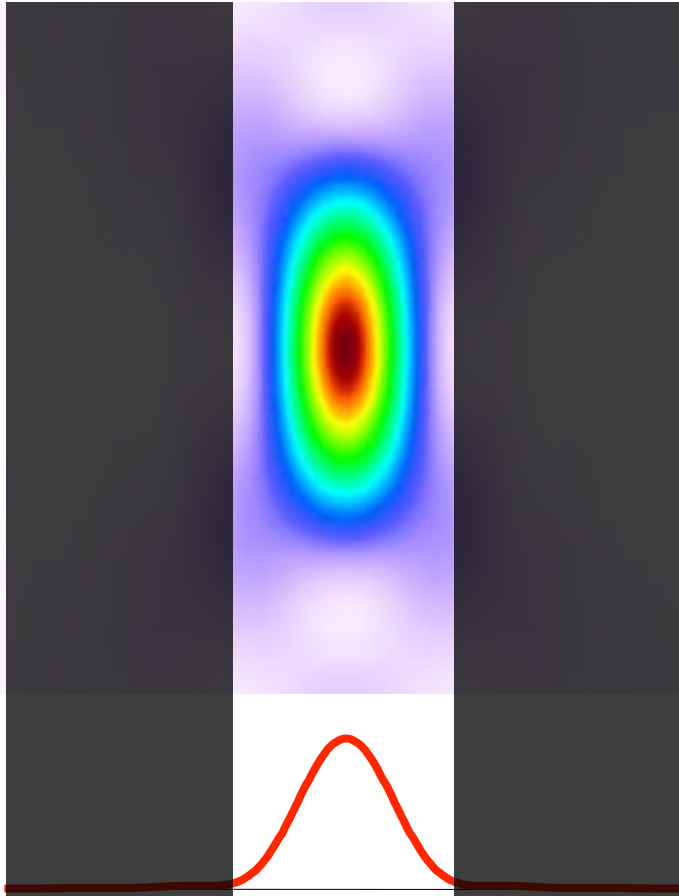


(e)



(f)

The pinhole size in confocal microscopy



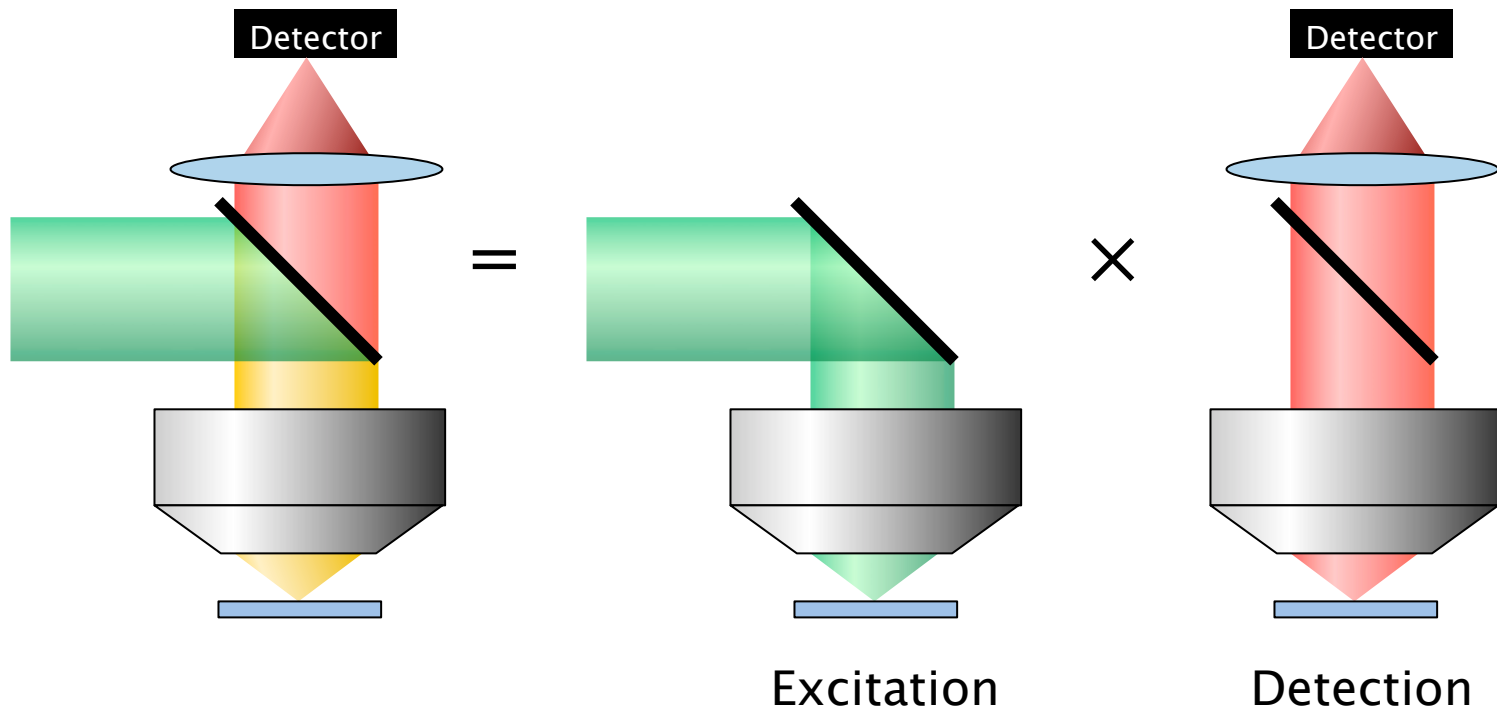
Detection efficiency
(PSF_{det})

$$= \text{PSF} \otimes \text{Pinhole}$$

Pinhole size should be related
to PSF width:

- | | |
|---------------------|--------------|
| – 100x / 1.4 NA | 220 nm x 100 |
| = 22 μm | |
| – 40x / 1.3 NA | 235 nm x 40 |
| = 9.4 μm | |
| – 20x / 0.75 NA | 407 nm x 20 |
| = 8.1 μm | |
| – 10x / 0.45 NA | 678 nm x 10 |
| = 6.8 μm | |

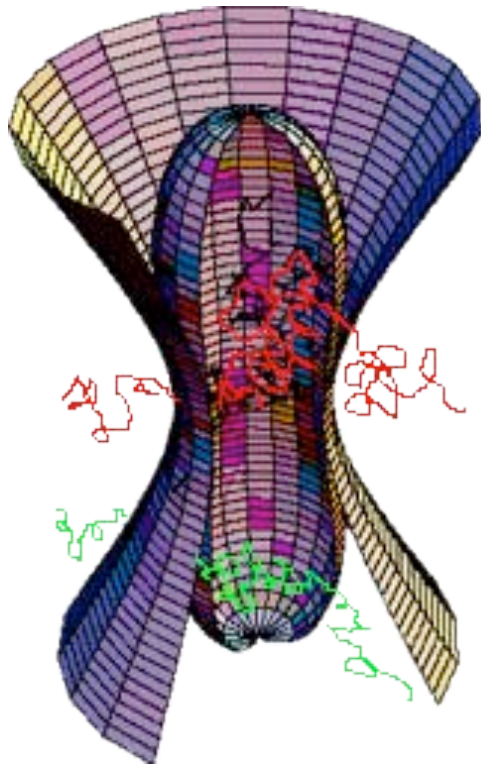
The PSF of confocal microscopy



$$\text{PSF}_{\text{Confocal}} = \text{PSF}_{\text{ex}} \times \text{PSF}_{\text{det}}$$

In the case of infinitely small pinhole: $\text{PSF}_{\text{Confocal}} \approx \text{PSF}_{\text{ex}}^2$

The confocal volume

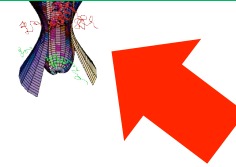
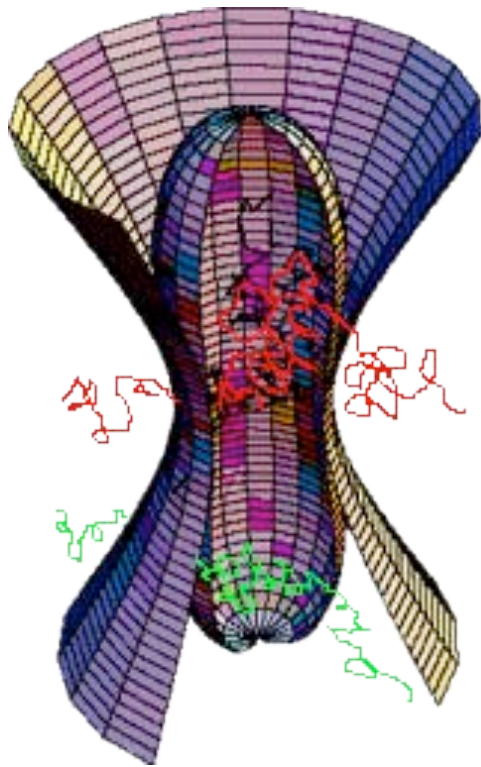


Integrating $\text{PSF}_{\text{confocal}}$ over the entire space now gets a finite value

Diffraction limited volume:

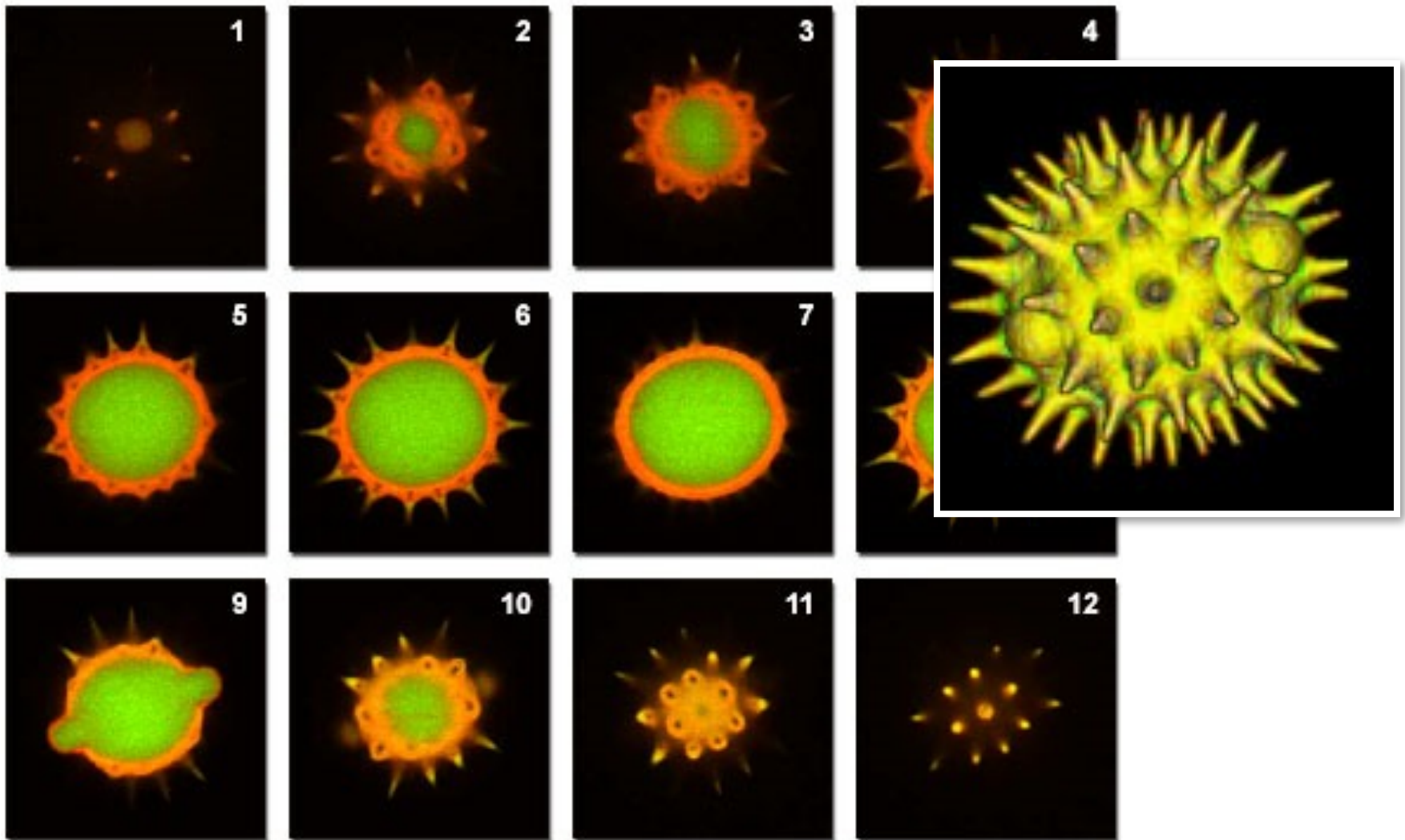
$$\Delta_{xy} \approx 250 \text{ nm}, \Delta_z \approx 600 \text{ nm}$$

The sectioning ability of confocal microscopy

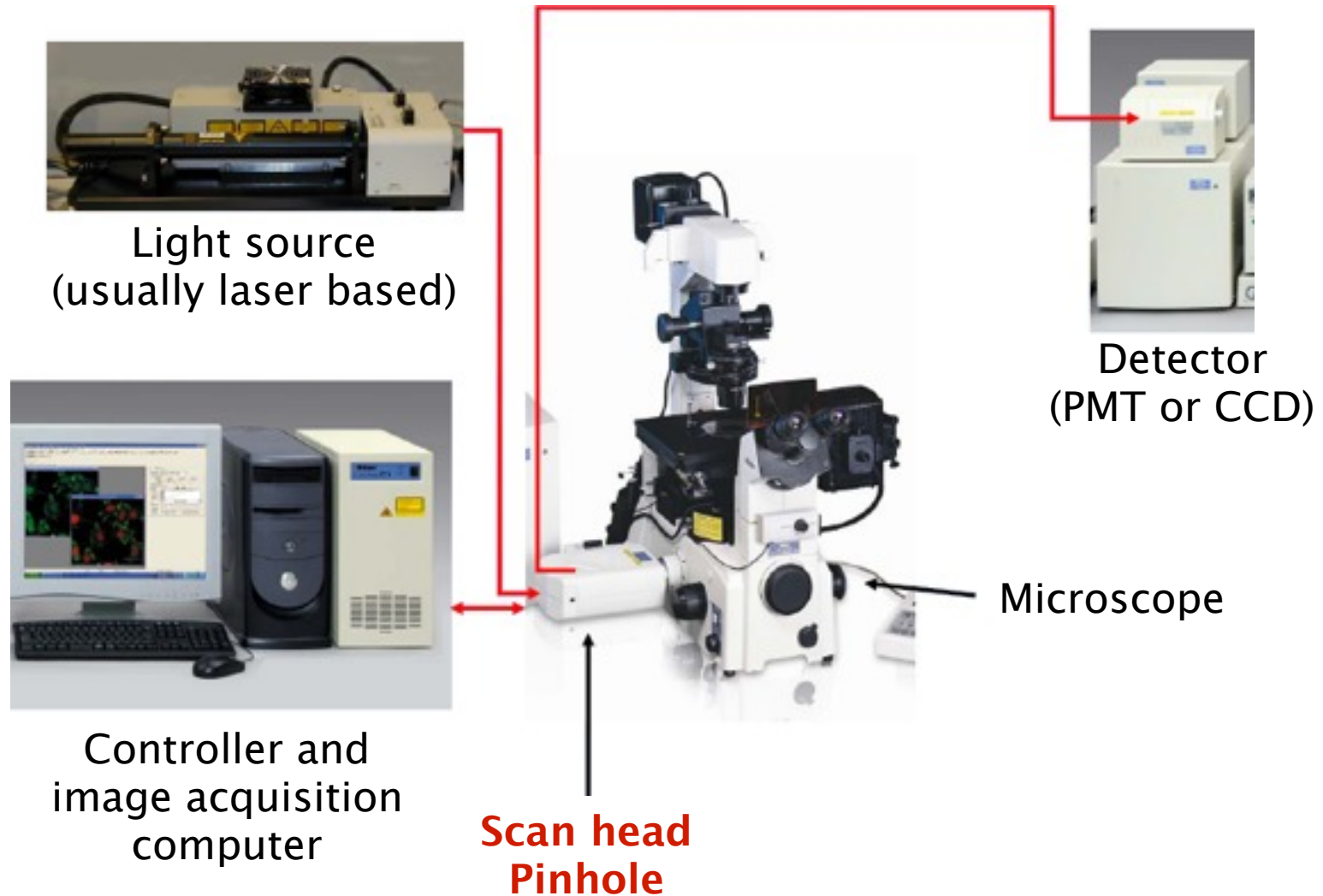


Guess:
When imaging a thick homogenous sample with
the best confocal microscope, what is the
fraction

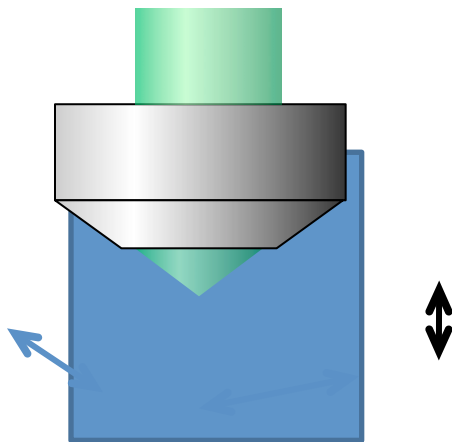
Confocal sectioning and 3D reconstruction



Components of a confocal

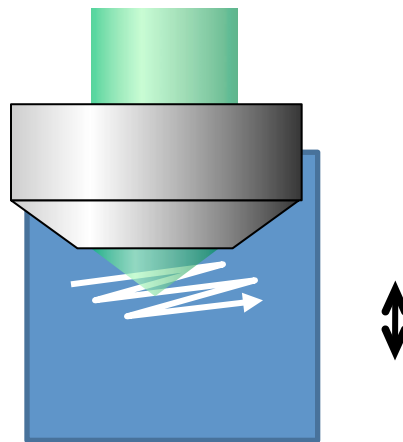


Point scanning confocal

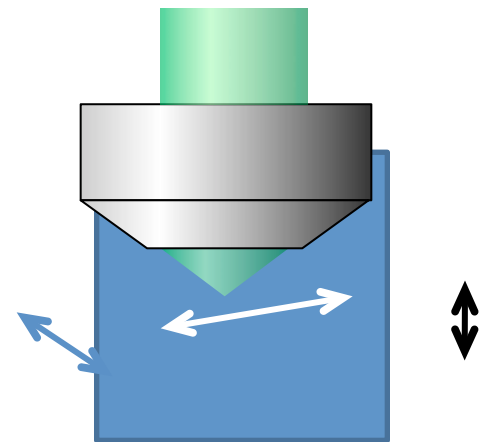


Stage scan

Simple but slow



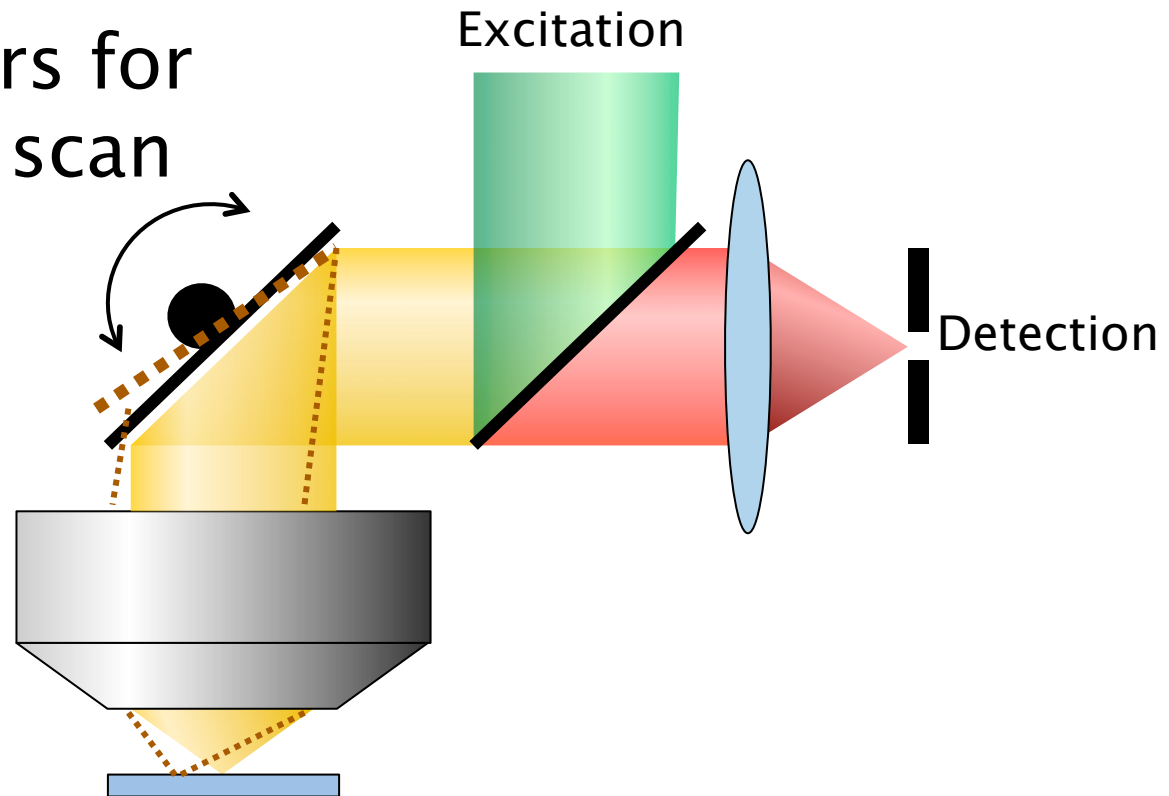
Laser scan



Hybrid

Galvanometer scanning /

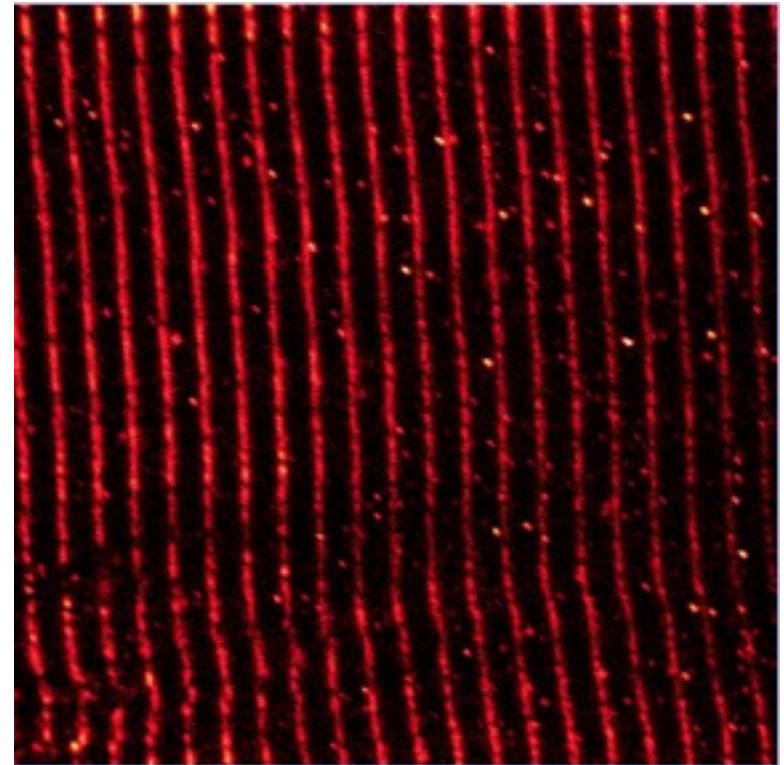
Two mirrors for
x-y raster scan



Averaging multiple scans to enhance S/N



1 frame



8-frame average

How to scan faster?

- Normal galvo mirror: several μ s per pixel
0.5 – 2 sec per image
- Resonance scanner: up to 30 fps
- The answer is:

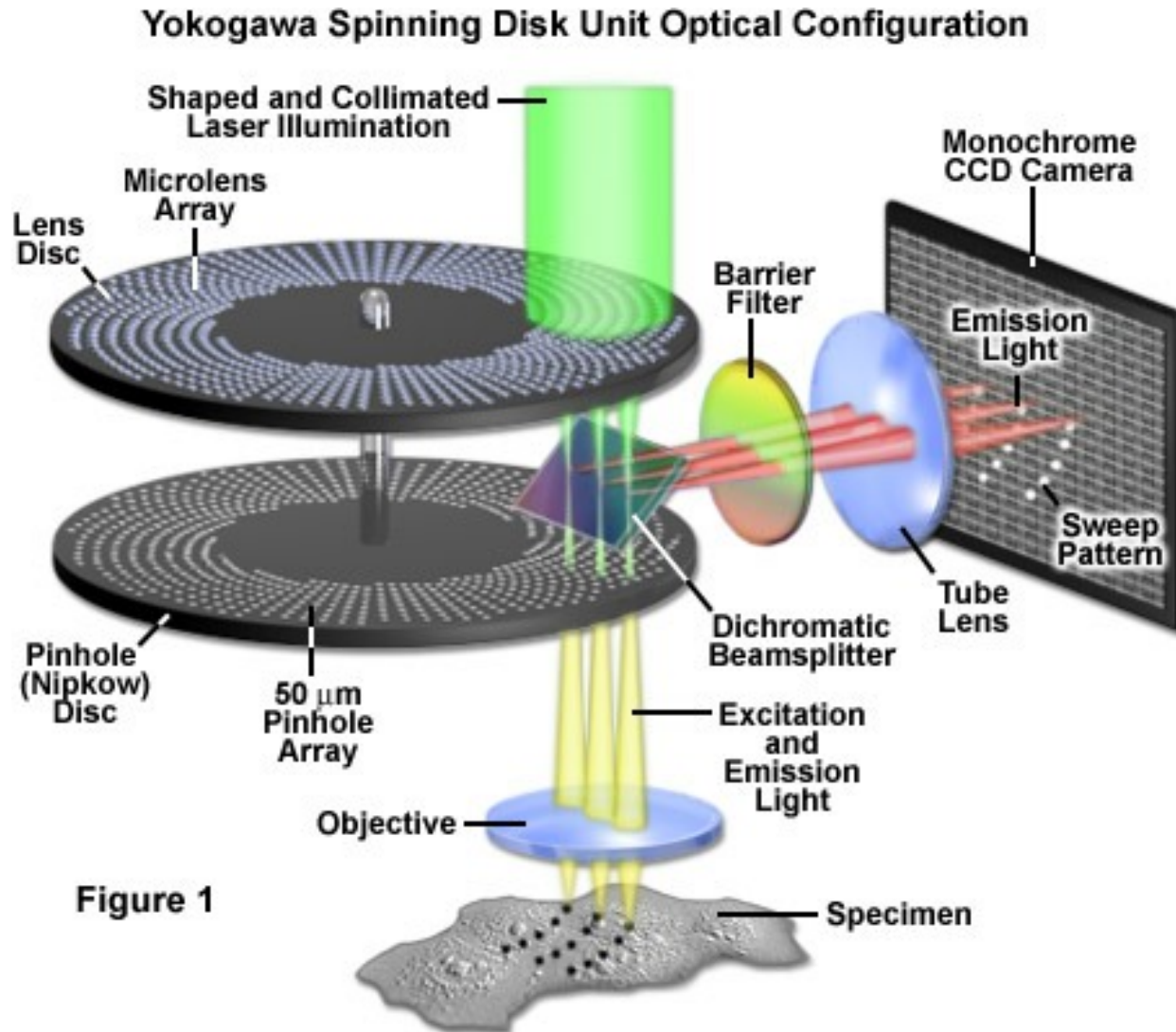


Spinning disk confocal

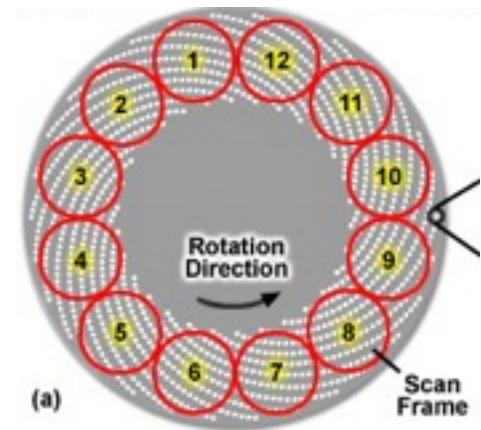
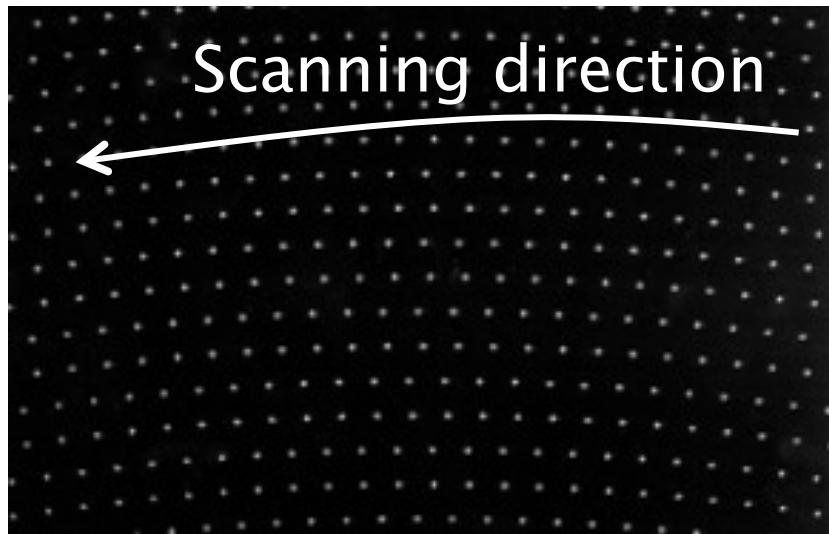
- Scanning with a rotating pinhole array
- CCD camera detection



Spinning disk confocal

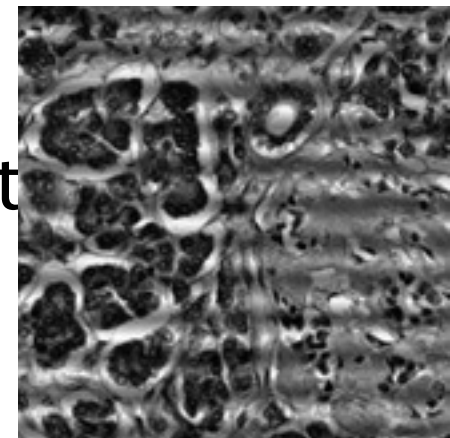


Spinning disk confocal

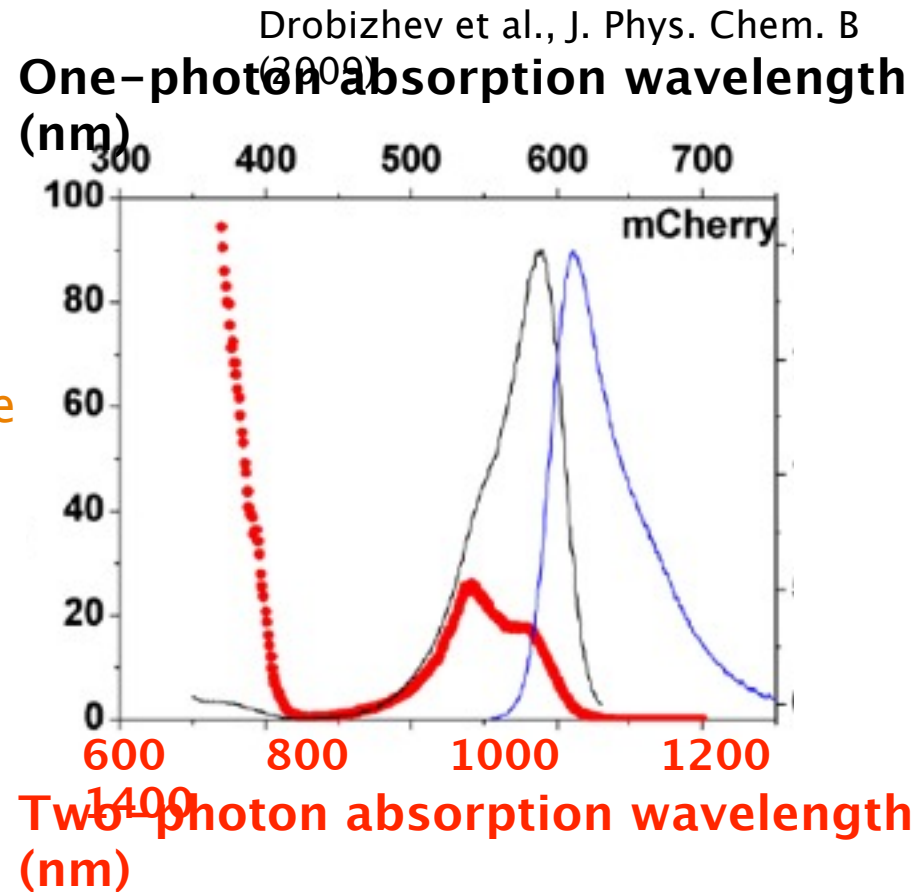
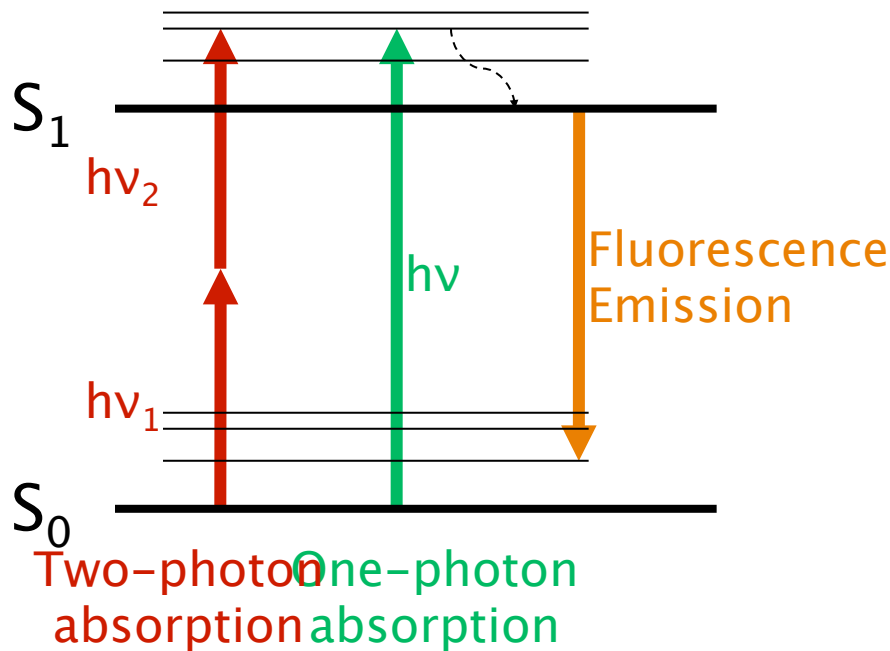


12 scanning frames per 360° rotation

- Up to 2000 frames / sec
- The disk rotation must match the camera frame rate



Multi-photon microscopy



Two-photon excitation: Fluorescence $\propto I^2$

Optical sectioning without a

$$\text{Fluorescence} \propto I^2$$



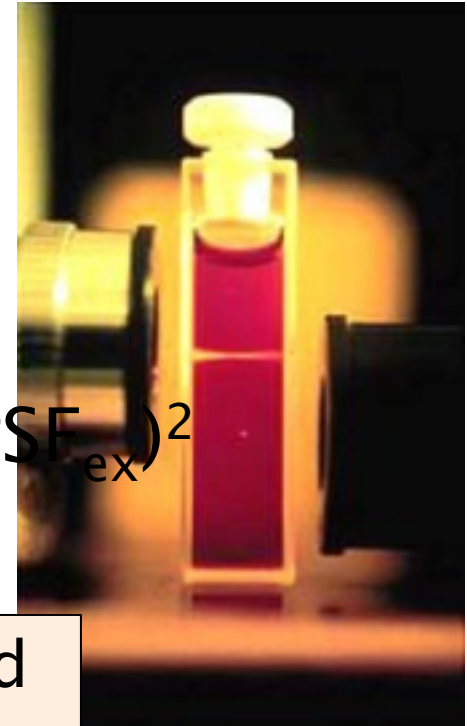
$$\text{PSF}_{2\text{P.ex}} = (\text{PSF}_{1\text{P.ex}})^2$$

Recall:

$$\text{PSF}_{\text{Confocal}} = \text{PSF}_{\text{ex}} \times \text{PSF}_{\text{det}} \approx (\text{PSF}_{\text{ex}})^2$$

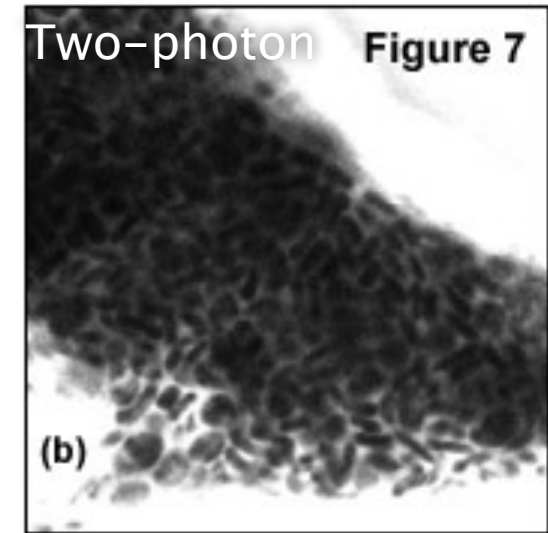
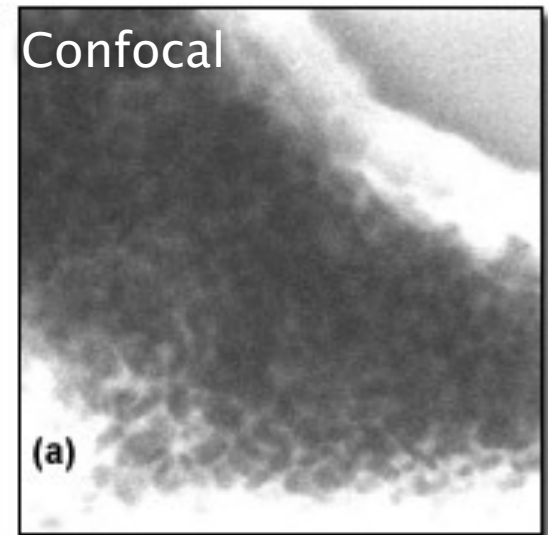
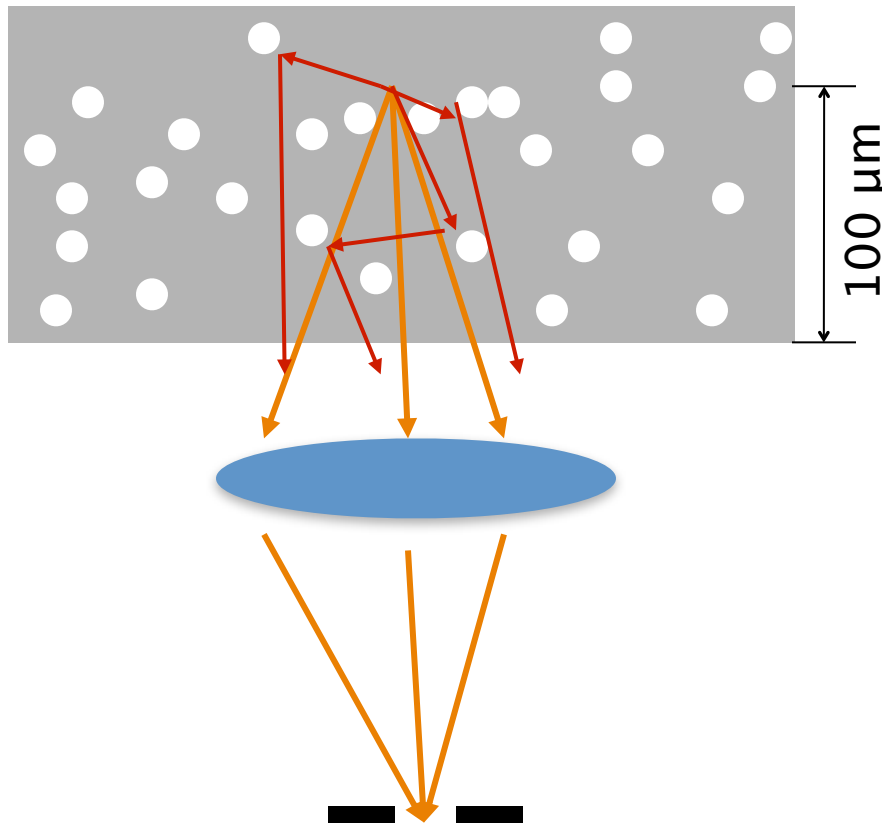


Two-photon excitation is localized to the laser focal point



Deep tissue imaging

Tissue scattering and absorption decrease confocal performance



Ultrafast laser source for 2PE

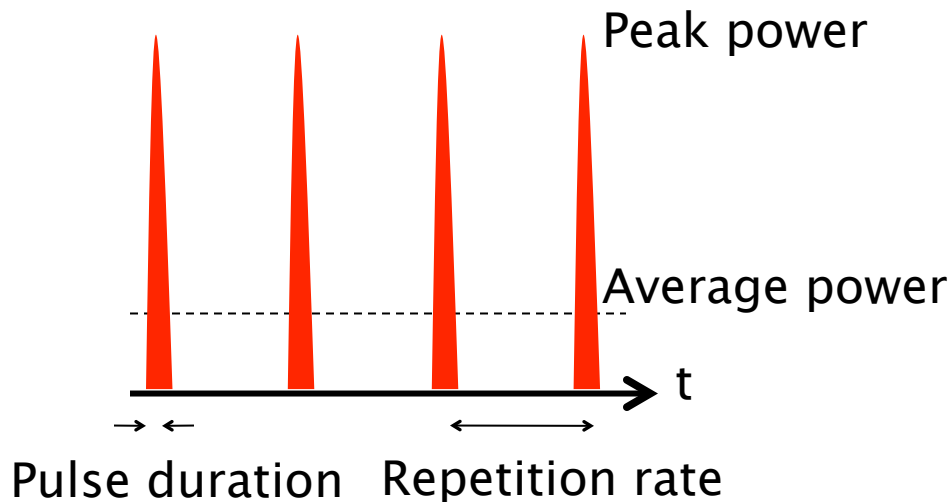
Continuous wave (CW) laser



To see reasonable 2PE with CW laser:
~ 1W power



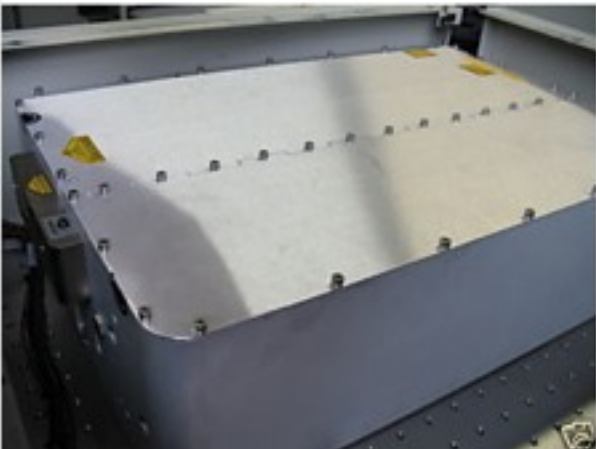
Pulsed laser




Ti:Sapphire laser, 100 fs, 80 MHz
10 mW avg \approx 1.2 kW peak



Ultrafast laser source for 2PE



Enlarge



Spectra Physics Mai Tai femtosecond laser New Diodes

Item condition: **Used**

Price: **US \$65,000.00** [Buy It Now](#)


or


Best Offer: [Make Offer](#)

[Add to Watch list](#)

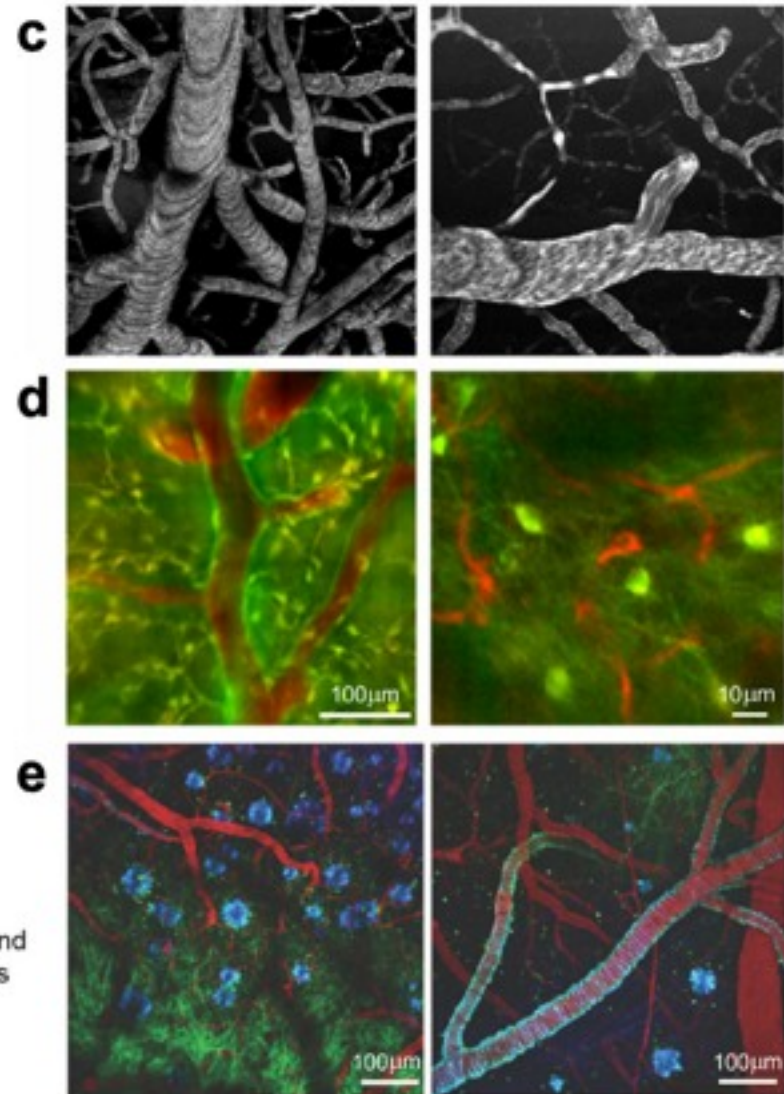
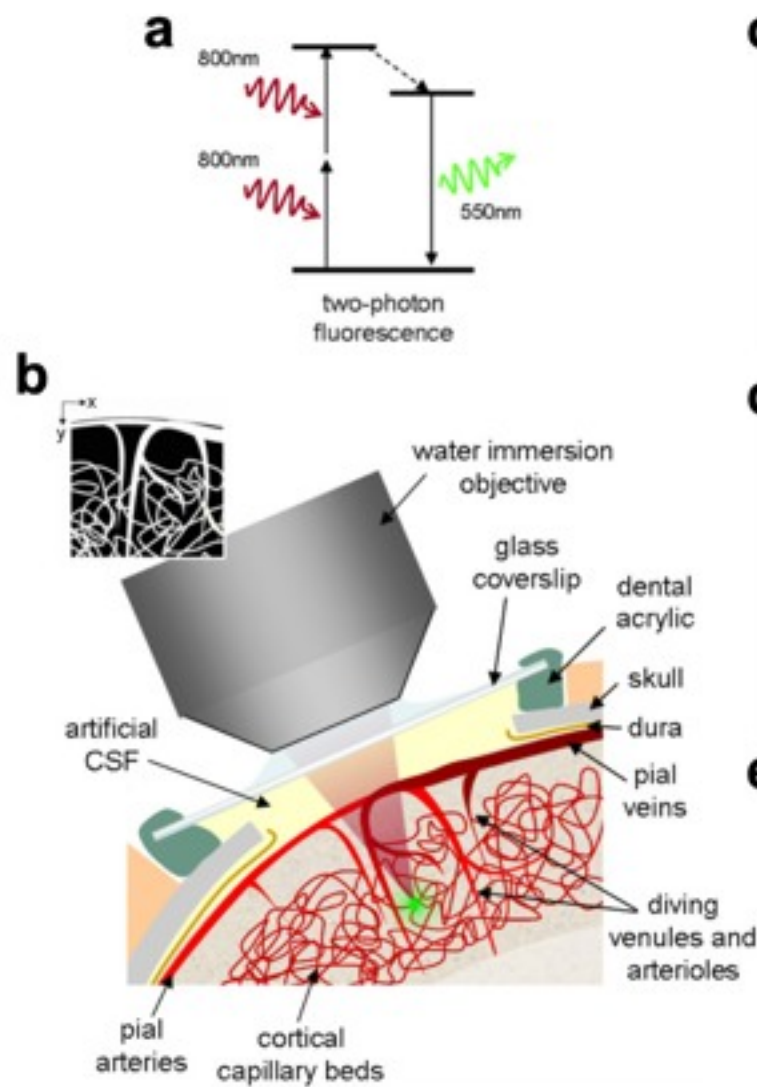
Shipping: Freight - See shipping details
[See all details](#)
Estimated delivery time varies for freight shipping.

Returns: No Returns Accepted

**eBay Buyer Protection**
eBay will cover your purchase price plus original shipping.
[Learn more](#)

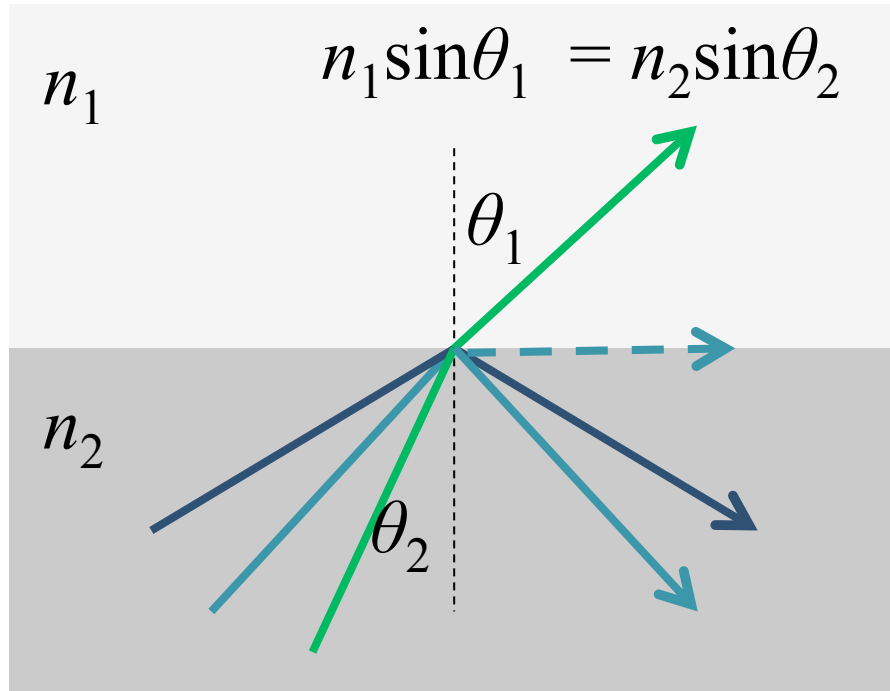


Two-photon microscopy of in vivo brain function



Kherlopian, et al., BMC Systems Biology (

Total internal reflection fluorescence microscopy



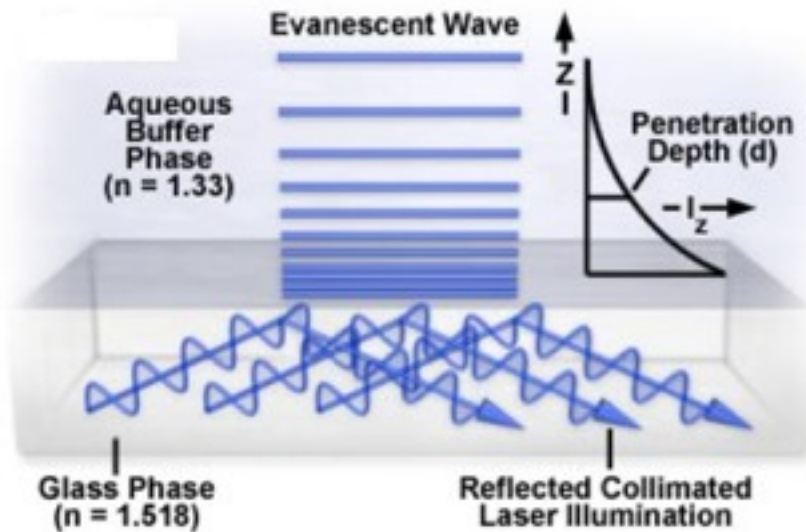
Total internal reflection:

$$\theta_1 = 90^\circ \rightarrow \sin \theta_2 \equiv \sin \theta_c = n_1 / n_2$$

$$n_1 = 1.33 \text{ (water)}, n_2 = 1.52 \text{ (glass)}, \theta_c = 61^\circ$$

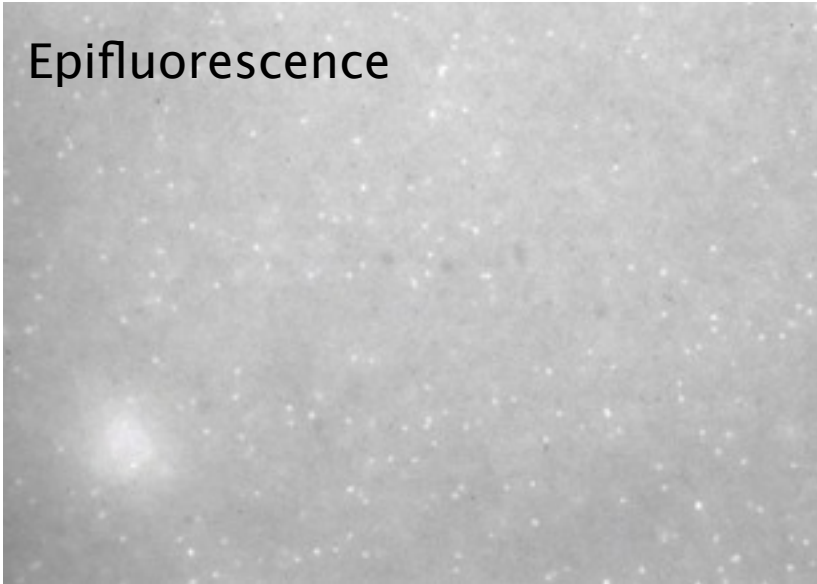
The evanescent wave in TIR

- The energy of the evanescent wave is localized near the interface.
- The strength of the evanescent wave field decreases exponentially.
- The penetration depth is a function of the wavelength and the incident angle.

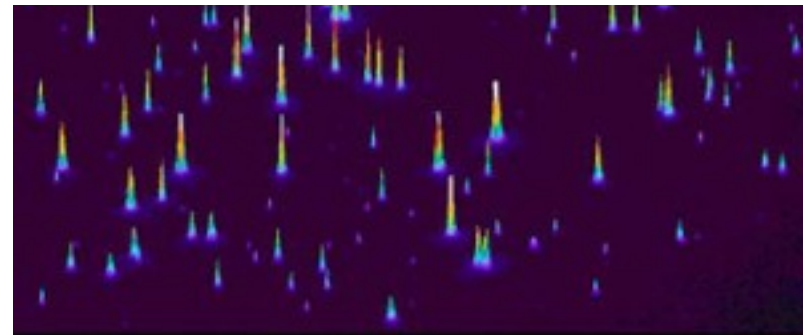
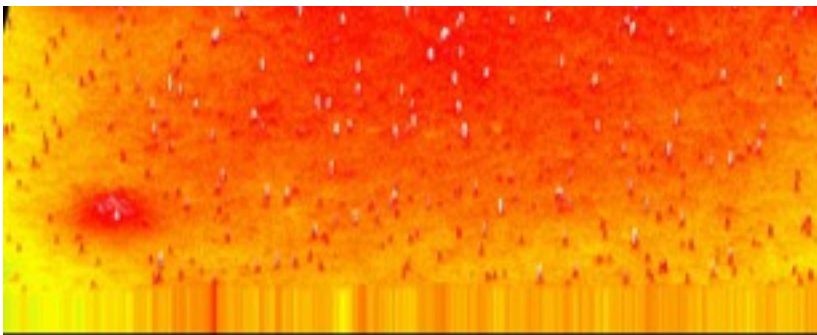
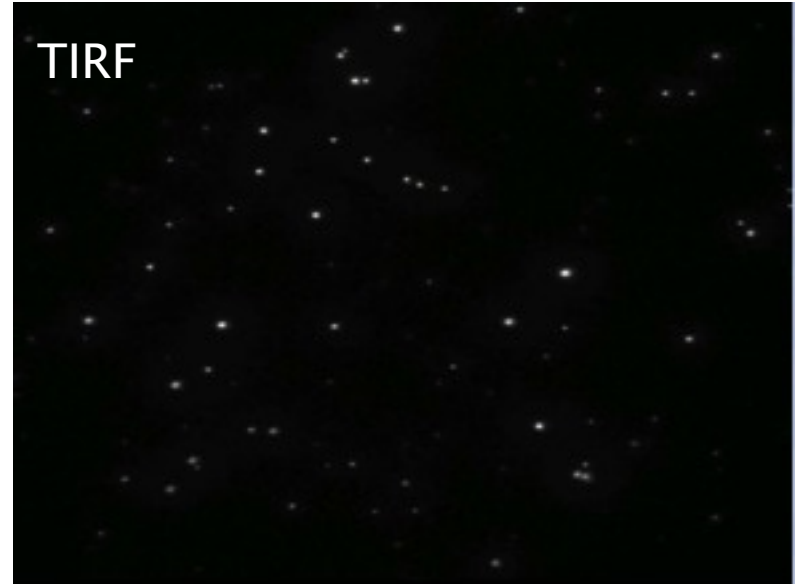


TIRM improves S/N for surface

Epifluorescence



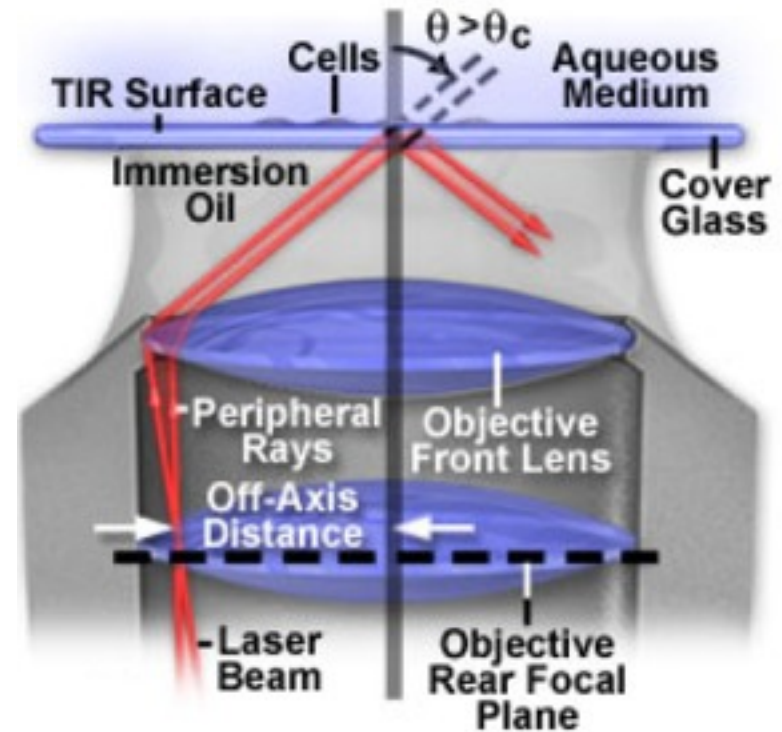
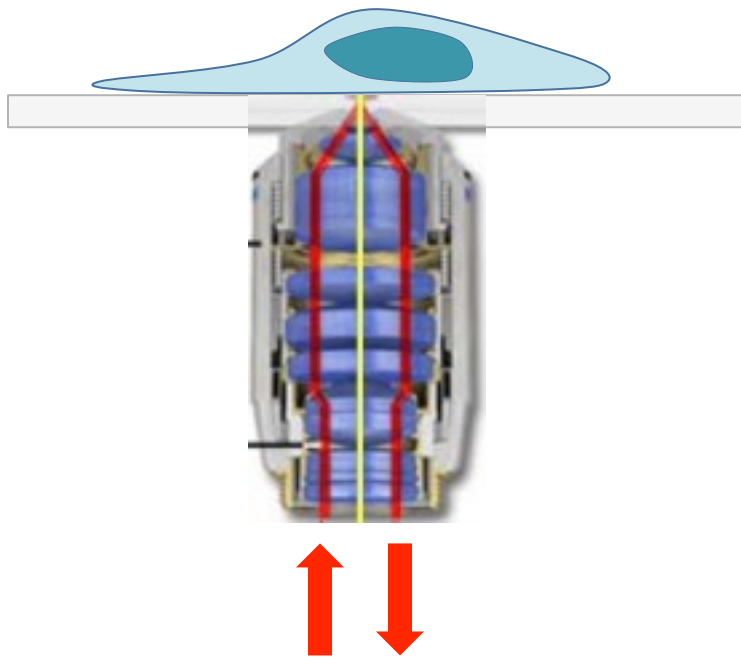
TIRF



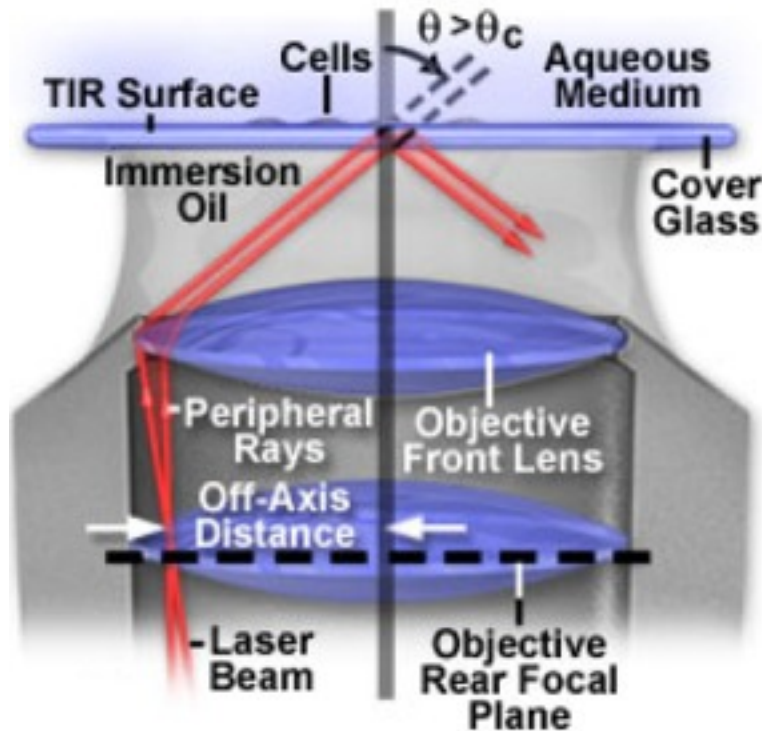
What are the applications of

- Organization of plasma membrane proteins
- Dynamics of plasma membrane lipids
- Endocytosis and exocytosis
- Focal adhesion
- Growth cone migration
- Imaging in supported lipid bilayers
- In vitro reconstituted cytoskeleton filaments
- Single molecule imaging

Through-the-objective TIRF



Requirement for TIRF



$$NA = n_{\text{glass}} \sin \theta_{\text{max}}$$

$$n_{\text{water}} = n_{\text{glass}} \sin \theta_c$$

$$\theta_{\text{max}} \geq \theta_c$$



$$NA \geq n_{\text{water}} \approx 1.33$$

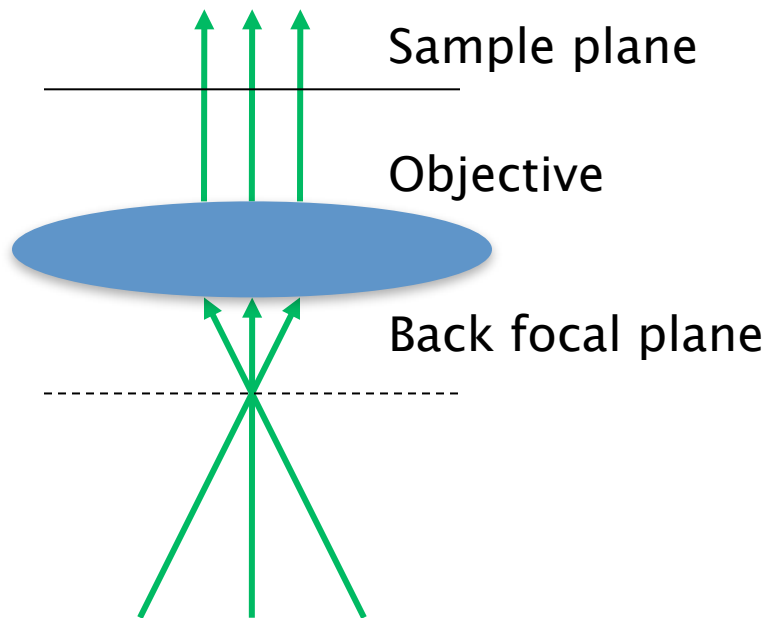
TIRF compatible objectives

- 1.40 NA
 - “Barely enough” for laser TIRF
- 1.45 / 1.49 NA “TIRF” objective
 - More homogenous illumination field
 - Higher efficiency for lamp TIRF
 - Compromised image quality
- 1.65 NA
 - Sapphire coverglass
 - Toxic oil...

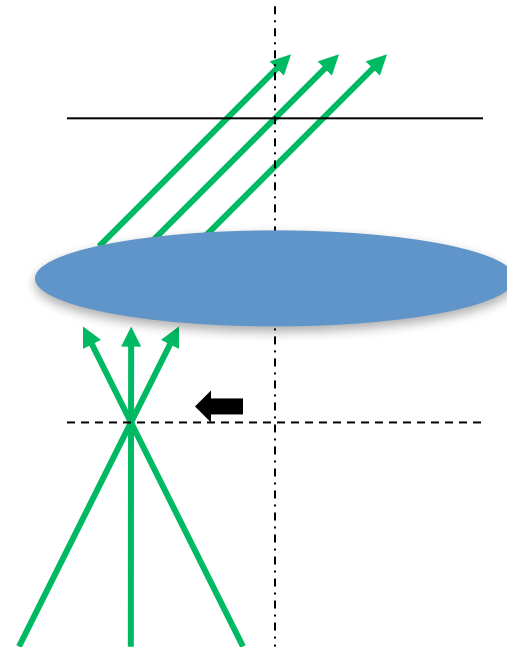


TIRF illuminator

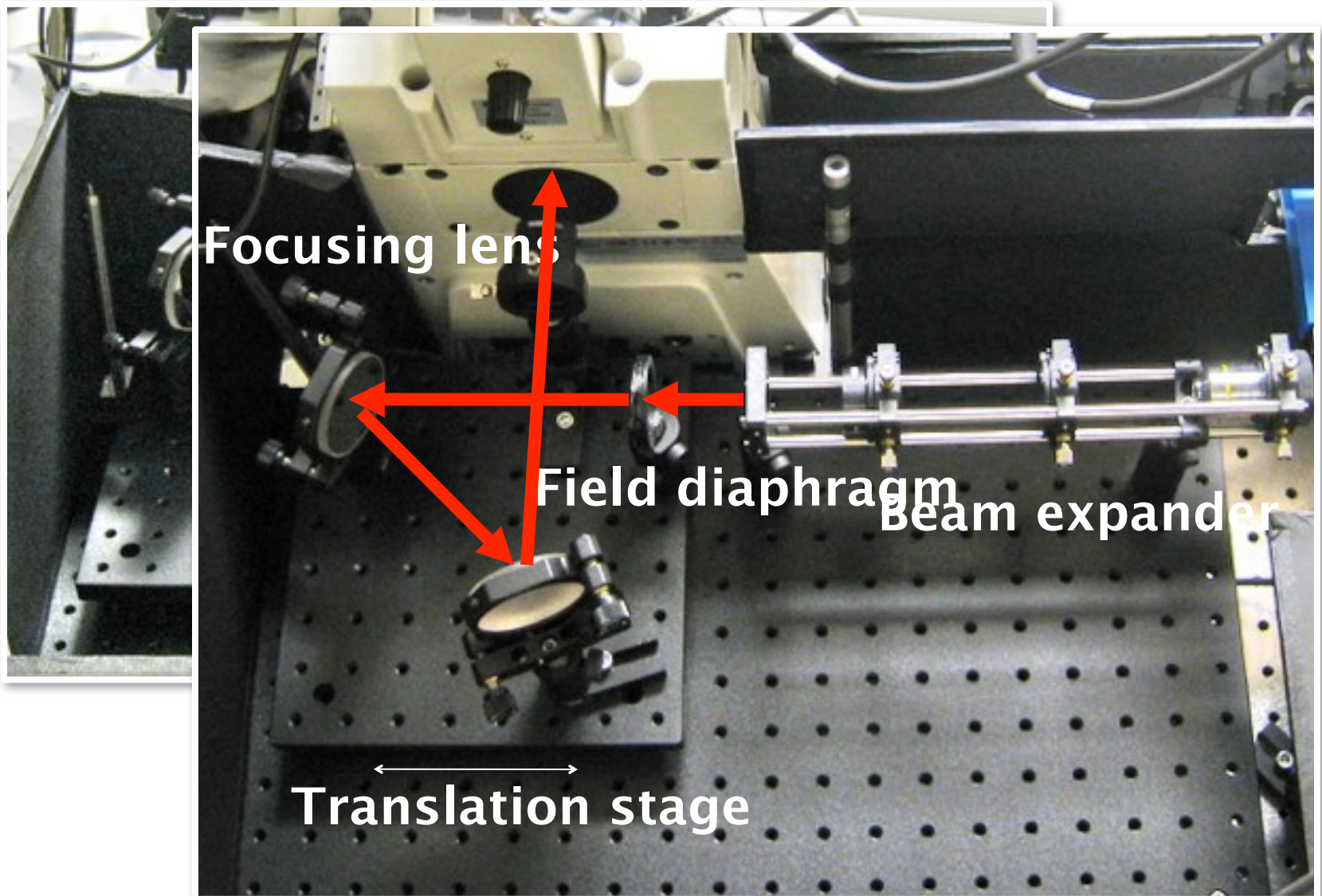
Focusing the light to the back-focal-plane of the objective



Translate the light to the edge of the objective back-aperture



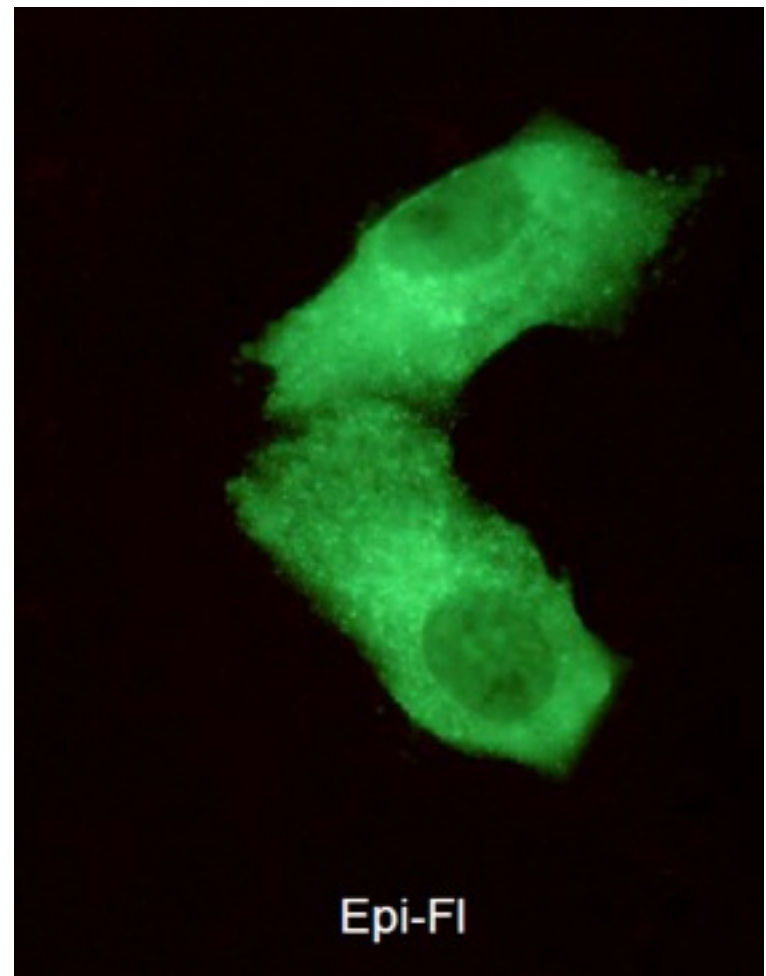
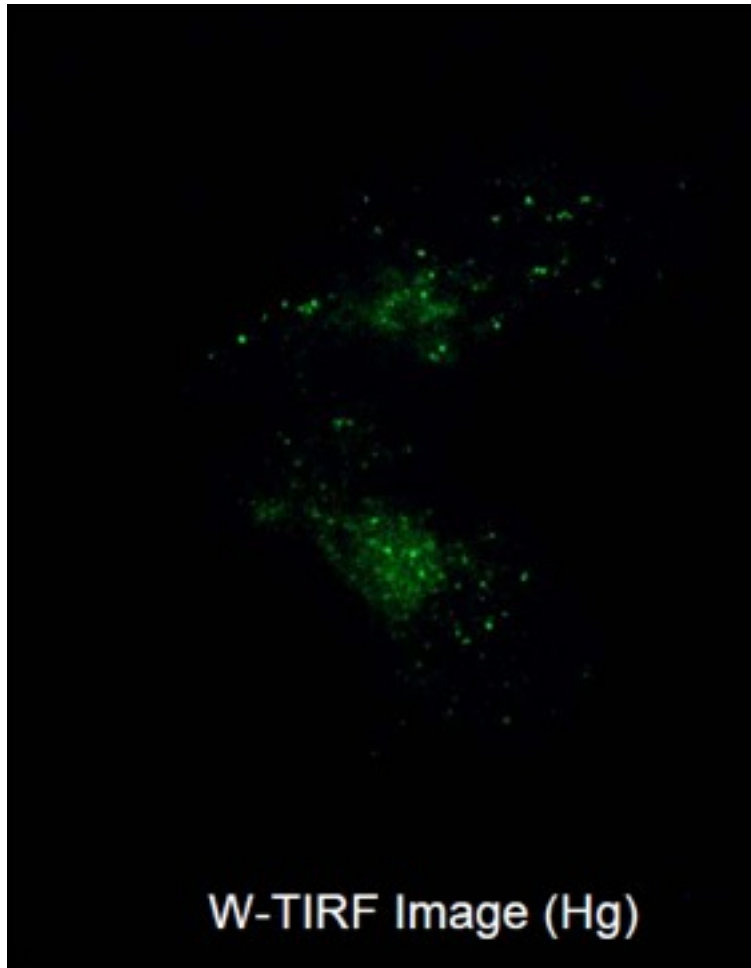
A home-built TIRF illuminator



A commercial TIRF

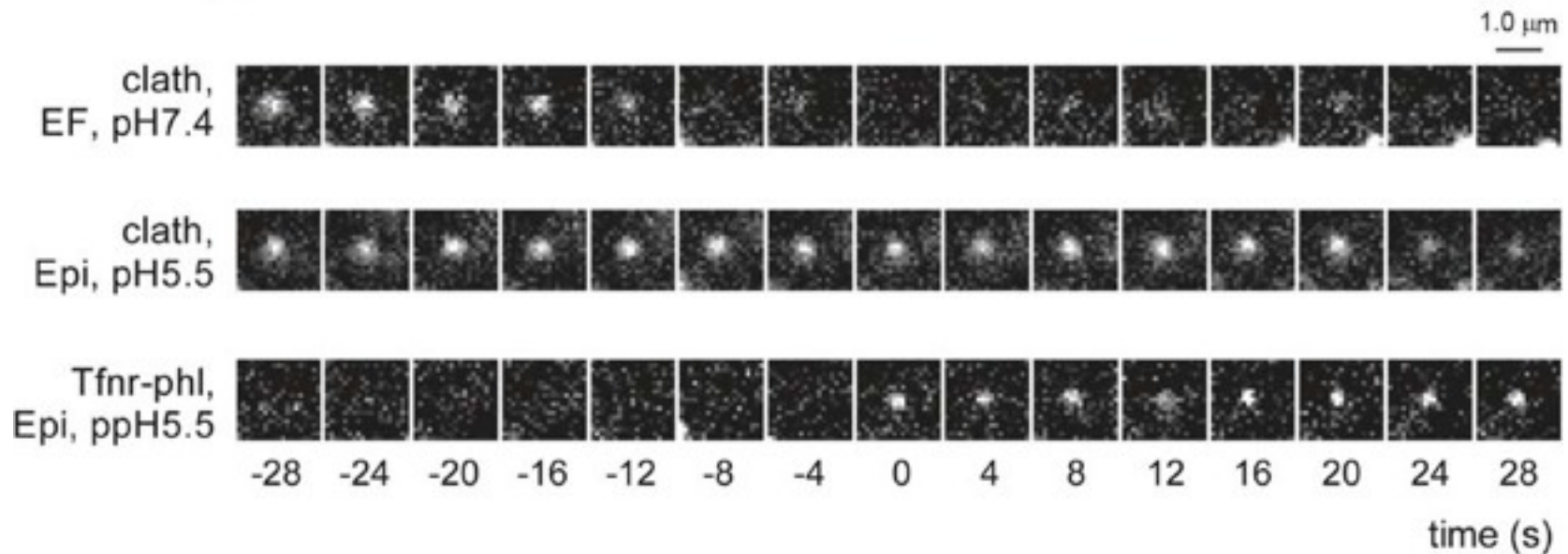
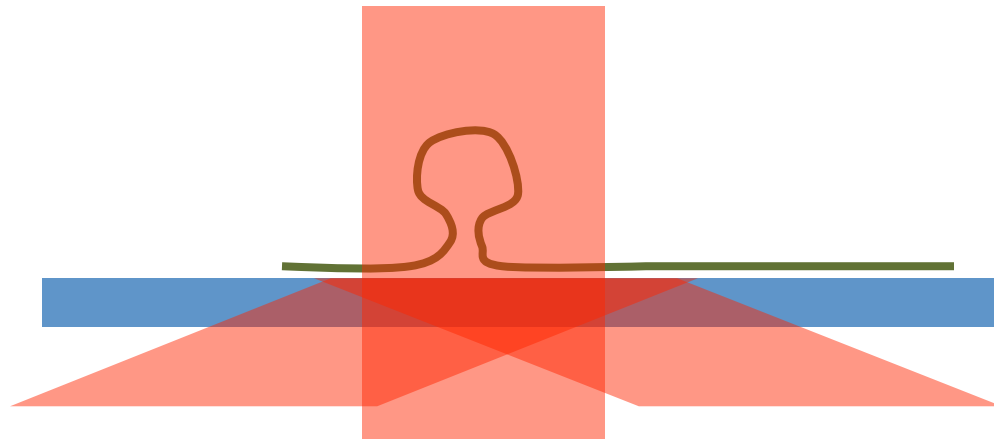


COS cells expressing GFP

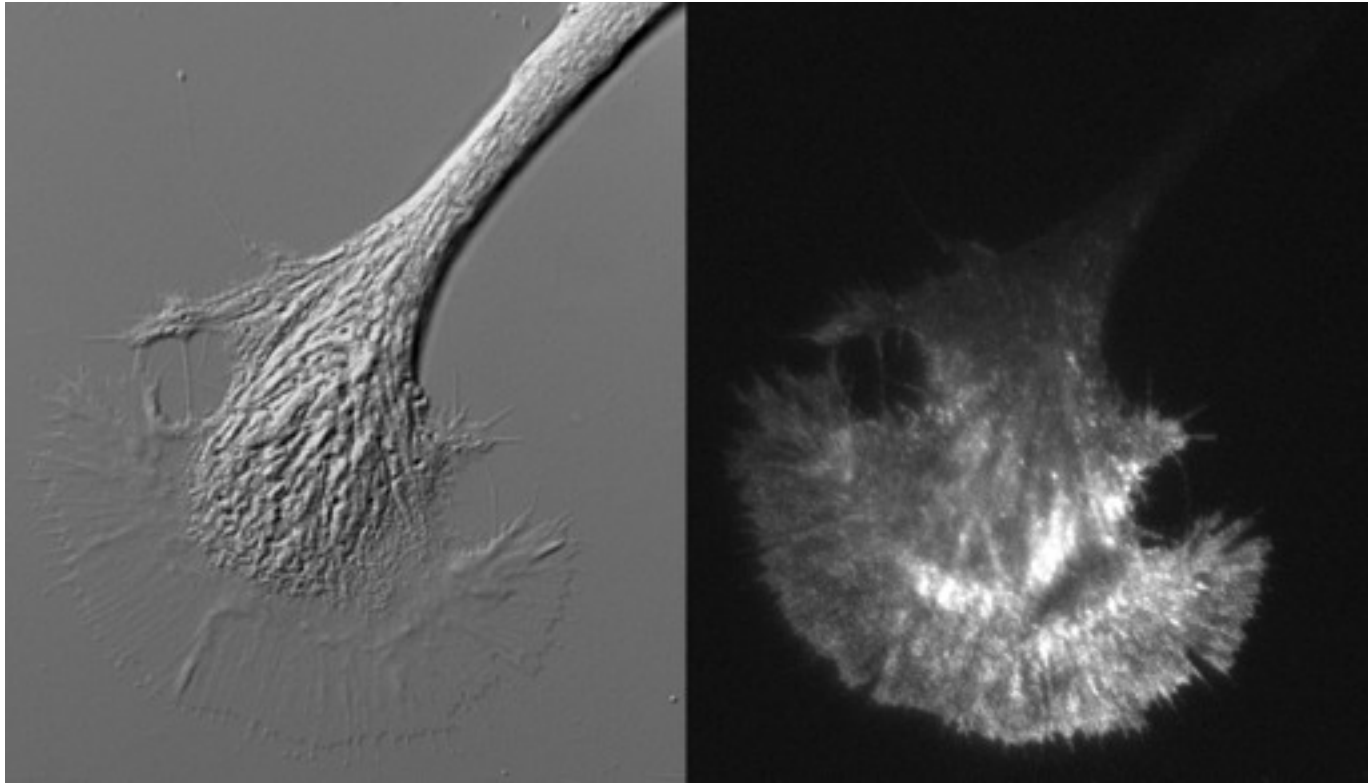


Dan Axelrod, Univ of
Michigan

Alternating Epi/TIRF

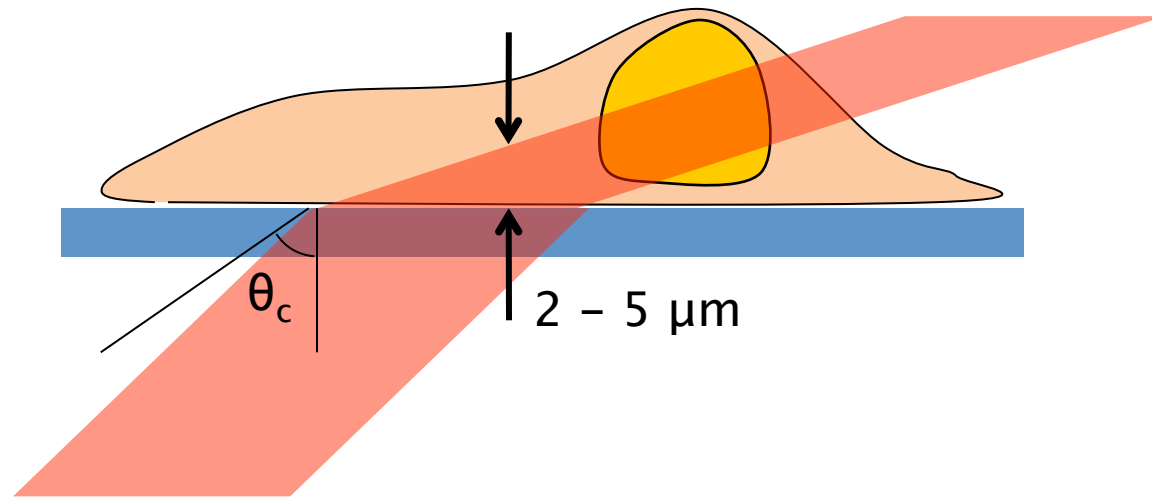


Aplysia growth cone



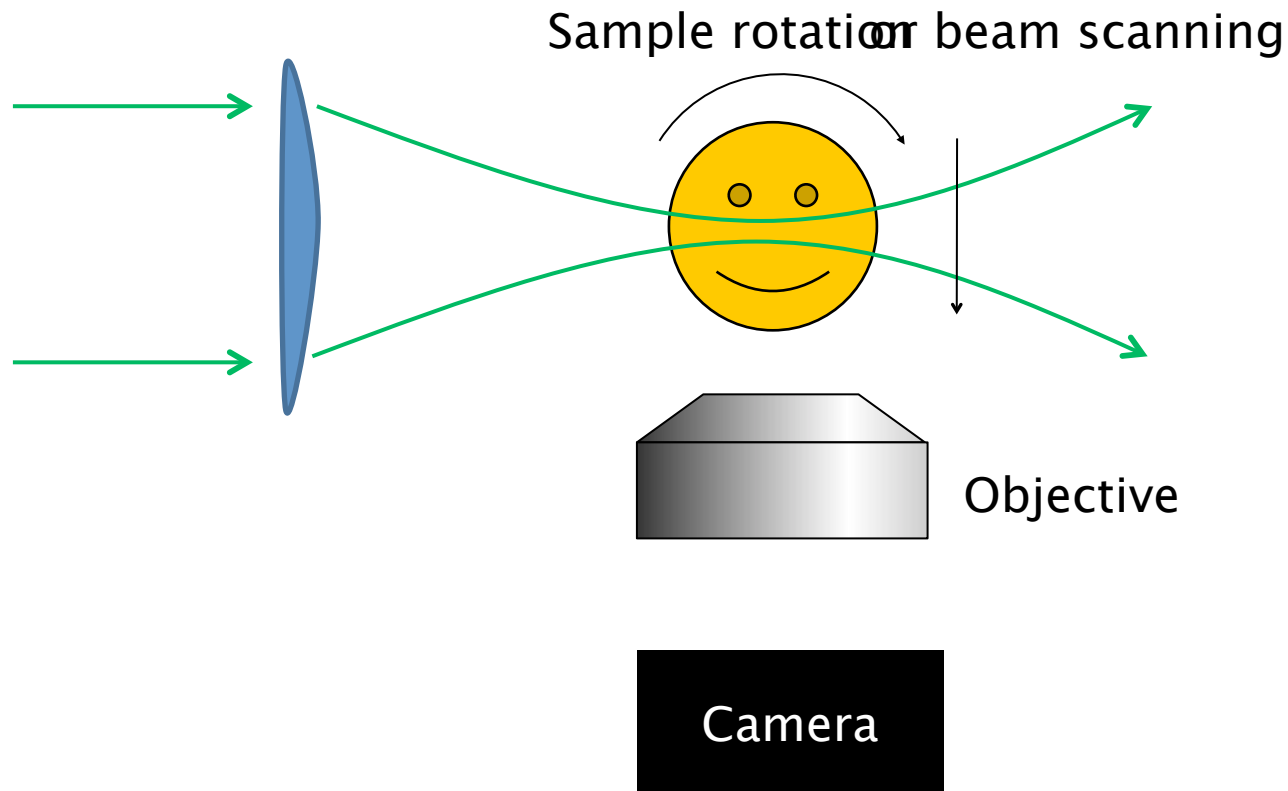
Andy Schaefer, Paul Forscher, Yale Univ.

Oblique angle illumination: the “gray zone”



An incident angle close but smaller than the critical angle can improve the signal from near-surface objects.

Single-plane illumination microscopy (SPIM)

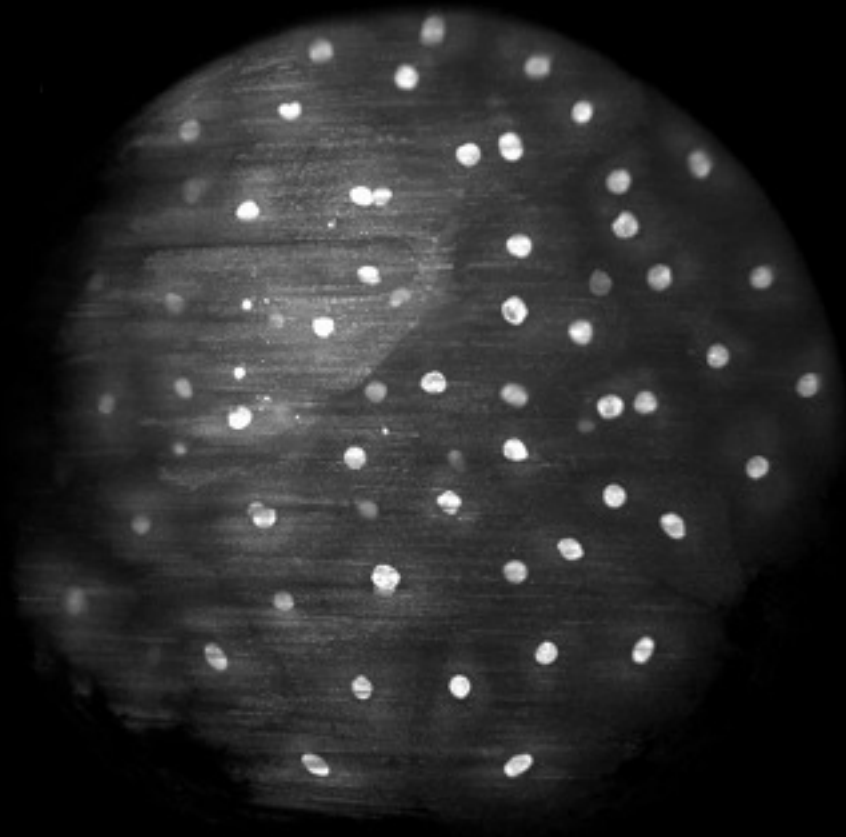


Zebra fish embryo development imaged by SPIM

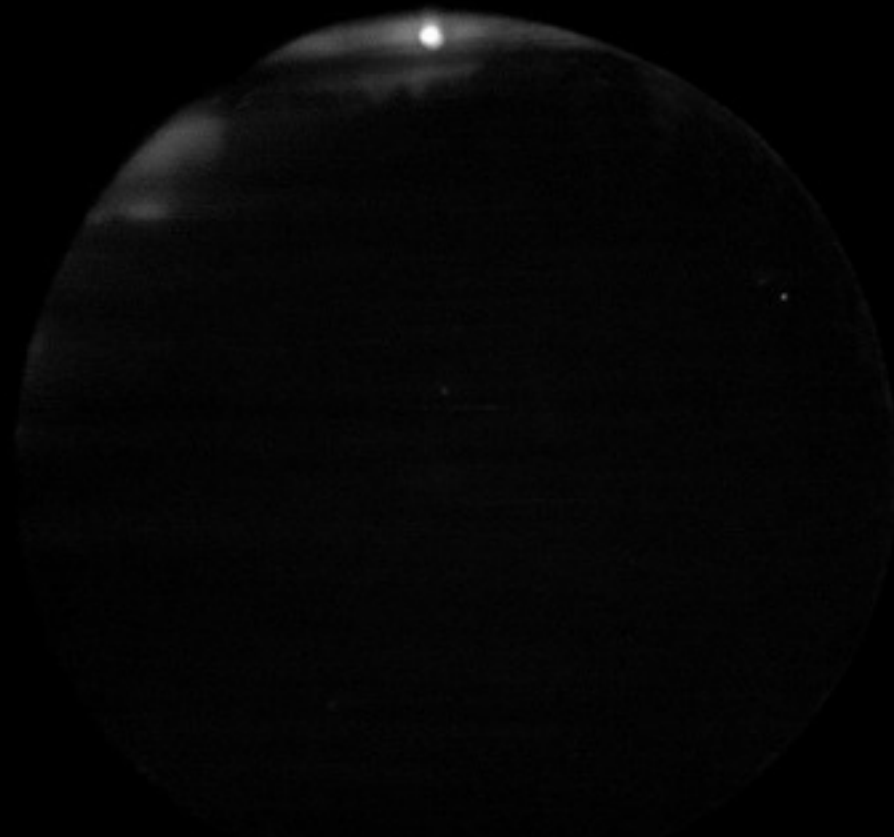
100 min

future dorsal side

future dorsal side



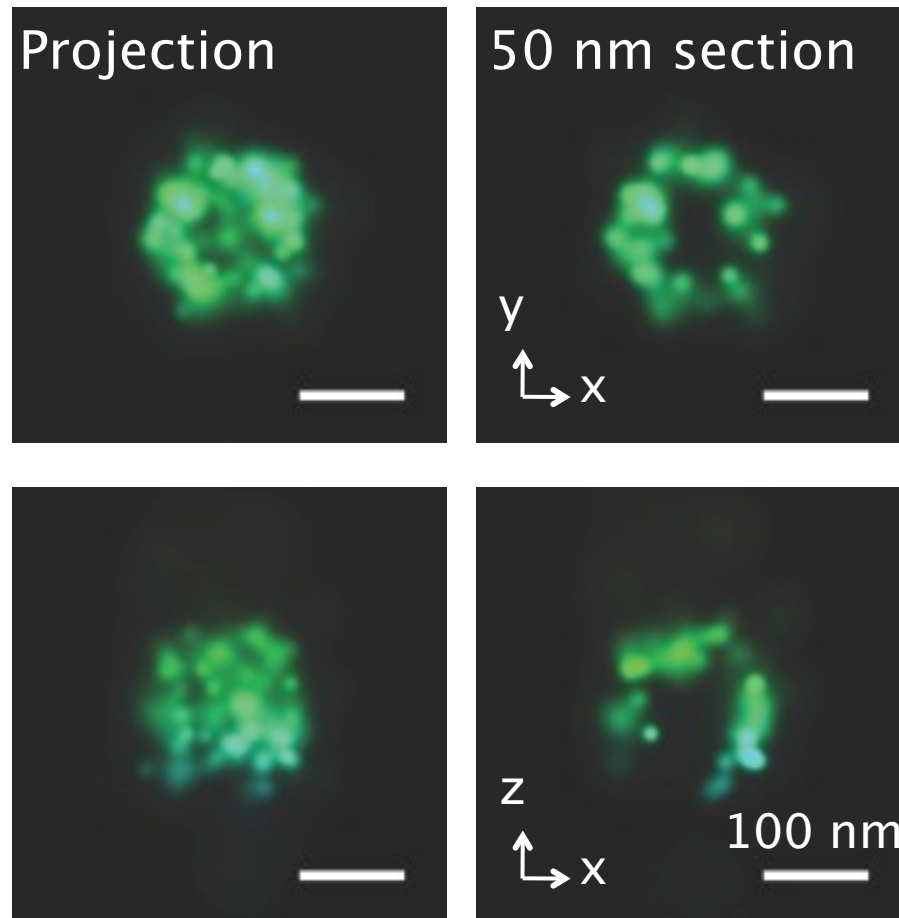
animal view



vegetal view

Keller et al., Science (2006)

Super-resolution microscopy



3D STORM image of a clathrin-coated pit

Now the tools are in your
hands!