ASSIGNMENT – 4 Advanced Programming Lab

Name: Utsav Balar Roll.no. t24cs003

Objective

Assignments on Seizure Detection using the CHB-MIT Scalp EEG Database. Develop a machine learning model to automatically detect seizure events from EEG data.

Dataset link: https://physionet.org/content/chbmit/1.0.0/

*Analysis:

Epilepsy and Seizures

Epilepsy is the most common neurological disorder in which clusters of nerve cells (neurons) in the brain sometimes signal abnormally and cause seizures. Currently it affects 60 million people worldwide. Normal function of neurons is to generate electrical and chemical signals that act on other neurons, which in turn cause secondary actions leading to a desired behavior. During a seizure, many neurons try to send signals at the same time; this abnormal surge of excessive electrical activity causes involuntary movements, and may cause a loss of control, lapse of attention or whole-body convulsion.

The introduction of new anti-epileptic drugs has provided most patients the ability to control their seizures, however, three in ten patients with epilepsy continue to have seizures despite treat-ment. Given the nature of the disease is quite unpredictable, patients often experience high levels of anxiety, mainly due to the impending loss of control and/or awareness during a seizure. Thus, prediction is key to minimizing the anxiety and fear experienced by the patient, and prediction begins with detection. A device able to detect seizures quickly could vastly improve patient care.

A classification problem

Seizure detection is usually done using scalp electroencephalogram (EEG), a non-invasive, multichannel recording of the brain's electrical activity. Classification between normal activity and a seizure is usually done in two steps: noise filtering and classification. We propose here two approaches to noise filtering: use two transforms, Fourier and Discrete wavelets, to filter the data but also extract the useful information and structure behind the signals. We will test classical models of classification using Python's sklearn libraries to run them.

Data

A study was conducted at the Children's Hospital Boston where EEG was recorded on pediatric subjects with intractable (i.e. epileptic) seizures. There were 22 subjects in the study: 5 male, ages 3-22,

and 17 females, ages 1.5-19; subject 21 was evaluated a second time 1.5 years later, thus re- sulting in 23 cases. Each case contains between 9 and 42 continuous .edf fles from a single subject, typically consisting of one hour each. Prior to measuring, subjects were taken of of any anti- seizure medication. The files can be found at https://physionet.org/physiobank/database/chbmit/

EEG Samples

Most of the EEG files have 23 recordings from electrodes placed around the head of the patient. Figures 1 and 2 present two EEG recordings of 40 seconds each. The first one was recorded at 1:43pm, while the patient was awake, and so should represent normal activity of the brain. The second one was recorded 50 minutes later. Within this 40 seconds, the patient experiences one epileptic seizure. As the size of the EEG makes it difficult to assess how much bigger the amplitudes are when the patient is experiencing a seizure, Figure 3 zooms in on one channel for the non-seizure and seizure activity. Here we begin to see a marked difference between the two.

1. Signal Extraction for training data

Each 8 second signals of 18 channels are extracted, sliding forward by 4 seconds. Each set of signals are labeled with the ratio of seizure in the time window. i.e. a set of signals are labeled 1.0 if it is in the middle of seizure.

1. Preprocessing The original signal frequency is 256 Hz, but to simplify the data, it has been resampled to 128 Hz.

Certainly! Let's walk through this code block-by-block to understand its purpose, including the rationale for using specific callbacks, models, and visualizations:

1. Imports and Setup

The code imports essential libraries:

- 1. **Pandas, Matplotlib, NumPy**: Used for data manipulation and visualization.
- 2. **MNE, WFDB**: Specialized libraries for handling EEG data from .edf files and annotations, respectively.
- 3. **Keras & TensorFlow**: For building and training the neural network.

2. Data Setup and Listing Files

- 1. **Channel Labels**: Defined for EEG data processing. There are 18 labels, representing EEG channels, for analyzing the EEG signals.
- 2. **Base Path**: Specifies the data directory.
- 3. **List Files Function**: This function walks through the data directory and lists all file paths, helping in understanding the dataset's structure.

3. Patient Data Splitting

1. **Collecting Patient IDs**: Extracts patient identifiers from the folder structure.

2. **Train-Test Split**: Splits the patients into training (80%) and test (20%) sets using a random selection. This is crucial for evaluating model performance on unseen data.

4. Signal Extraction

- 1. Loading or Extracting Signals:
- 2. If preprocessed files exist (signal_samples.npy and is_seizure.npy), they are loaded to save time.
- 3. Otherwise, signals are extracted from .edf files:
- 4. **MNE Library**: Used to read EEG signals and metadata.
- 5. **Sliding Window**: The EEG data is split into 8-second windows, sliding forward by 4 seconds. This temporal segmentation helps in analyzing patterns over time.
- 6. **Labeling**: Windows are labeled based on the presence of seizures using seizure annotations from the WFDB library.
- 7. **Balanced Sampling**: The code balances the data by oversampling seizure events and undersampling non-seizure events.

5. Data Preprocessing

- 1. **Resampling**: EEG signals are downsampled from 256 Hz to 128 Hz to simplify the data.
- 2. **Visualizing Sample Signals**: Plots EEG signals to visualize a sample of the extracted signals:
- 3. The **top plot** shows all 18 channels in one figure, with each channel shifted vertically for clarity.
- 4. The **bottom plot** uses a grayscale colormap to give a heatmap representation of the signals over time.
- 5. **Checking Seizure Distribution**: The number and ratio of windows with seizures are printed, helping to understand class imbalance.

6. Model Definition

- 1. A **Sequential CNN Model** is built for seizure detection:
- 2. **Input Layer**: Specifies the input shape as (18 channels, 1024 time points, 1 channel dimension).
- 3. **Convolutional Layers**: Multiple Conv2D layers with different filters and kernel sizes to capture spatial and temporal features in the EEG data.
- 4. **Pooling Layers**: MaxPooling layers reduce the dimensionality of the data while retaining important features.
- 5. **Global Average Pooling**: Reduces each feature map to a single value, helping to connect the convolutional layers to fully connected layers.
- 6. **Dense Layers**: Fully connected layers with ReLU activation for classification.
- 7. **Dropout Layers**: Used for regularization, preventing overfitting by randomly dropping some neurons during training.
- 8. **Output Layer**: A single neuron with a sigmoid activation function for binary classification (seizure vs. non-seizure).

7. Callbacks for Training

- 1. **Early Stopping**: Monitors the validation loss and stops training if it does not improve for 20 epochs, restoring the best weights. This prevents overfitting.
- 2. **ReduceLROnPlateau**: Reduces the learning rate if the validation loss plateaus, allowing the model to fine-tune its performance.

8. Mixed Precision Training

1. **Mixed Precision**: Uses half-precision (float16) arithmetic to speed up training and reduce memory usage, especially helpful when using modern NVIDIA GPUs.

9. Model Training

- 1. **Model Compilation**: The model is compiled using the Adam optimizer with a learning rate of 0.0001. The loss function is binary cross-entropy, and the metric is accuracy.
- 2. **Model Fitting**: The model is trained for 50 epochs with a batch size of 128, using the defined callbacks for early stopping and learning rate adjustment.
- 3. **Saving the Model**: The trained model is saved in the specified file.

10. Visualizing Training Performance

- 1. **Loss Plot**: Plots the training and validation loss over epochs, with an annotation for the early stopping epoch.
- 2. **Accuracy Plot**: Plots the training and validation accuracy, with an annotation for the early stopping epoch.
- 3. These plots help in understanding how well the model is training and when it starts to overfit.

Purpose of Callbacks and Model Design

- 1. **EarlyStopping**: Avoids overfitting by halting training when performance on the validation set stops improving.
- 2. **ReduceLROnPlateau**: Helps fine-tune the learning process by lowering the learning rate when progress stagnates.
- 3. **CNN Architecture**: The convolutional layers are designed to capture both spatial patterns (across channels) and temporal patterns (over time) in the EEG data, which are crucial for detecting seizure events.
- 4. **Global Average Pooling**: Reduces the model's complexity by summarizing feature maps, making it efficient for classification.

Code for training:

```
# import pandas as pd
from keras import layers
from keras.utils import plot model
from sklearn import model selection
from tensorflow import keras
from tensorflow.keras import layers
from tensorflow.keras import mixed precision
from tensorflow.keras.callbacks import ReduceLROnPlateau,
EarlyStopping
from typing import List
import gc
import glob
import keras
import logging
import matplotlib.pyplot as plt
import mne
import numpy as np
import os
import random
import re
import tensorflow as tf
import tqdm
import wfdb
# Define channel labels
ch_labels: List[str] = [
    "FP1-F7",
    "F7-T7",
    "T7-P7",
    "P7-01",
    "FP1-F3",
    "F3-C3",
    "C3-P3",
    "P3-01",
    "FP2-F4",
    "F4-C4",
    "C4-P4",
    "P4-02",
    "FP2-F8",
    "F8-T8",
    "T8-P8",
    "P8-02".
```

```
"FZ-CZ",
    "CZ-PZ",
1
# Define base path to data
base path: str =
"/home/utsav/work/academic/NITM-T24CS003/Programming Lab/chbmit/"
# Walk through the directory and print all filenames
def list_files_in_directory(path: str) → None:
    for dirname, _, filenames in os.walk(path):
        for filename in filenames:
            print(os.path.join(dirname, filename))
list files in directory(base path)
# Gather folders and extract patient numbers
folders: List[str] = sorted(glob.glob(f"{base_path}/*/"))
n patient: List[str] = [folder.rstrip("/").split("/")[-1][-2:] for
folder in foldersl
print("Patients:", *n patient)
# Set seed for reproducibility
random.seed(2024)
# Split patients into train and test sets
# Patients are assigned to training and test groups through a
random selection process.
ratio_train: float = 0.8
train patient str: List[str] = sorted(
    random.sample(n patient, round(ratio train * len(n patient)))
test patient str: List[str] = sorted(
    [patient for patient in n_patient if patient not in
train patient str]
print("Train PT:", *train_patient_str)
print("Test PT:", *test_patient_str)
# Collect file paths for train and test sets
```

```
def collect files(patient str list: List[str], path: str) →
List[str]:
    return [
        edf_file
        for patient in patient str list
        for edf_file in glob.glob(f"{path}/chb{patient}/*.edf")
    ]
files train: List[str] = collect files(train patient str,
base path)
files test: List[str] = collect files(test patient str, base path)
print("Number of training files:", len(files_train))
print("Number of test files:", len(files test))
mne.set log level(verbose="ERROR")
logger = logging.getLogger( name )
fh = logging.FileHandler("read_files.log")
logger.addHandler(fh)
# Sliding window (The EEG data is split into 8-second windows,
sliding forward by 4 seconds)
time window: int = 8
time step: int = 4
if os.path.exists(base path + "signal samples.npy") &
os.path.exists(
    base path + "is seizure.npy"
):
   print("————— File exists———")
    array_signals: np.ndarray = np.load(base path +
"signal samples.npy")
    array is seizure: np.ndarray = np.load(base path +
"is seizure.npv")
else:
    p: float = 0.01
    counter: int = 0
    for temp_f in files_train:
        temp edf = mne.io.read raw edf(temp f)
        temp labels: List[str] = temp edf.ch names
        if sum(
            Γ
```

```
any([0 \text{ if re.match}(c, l) = None else 1 for l in ]
temp edf.ch names])
                for c in ch_labels
        ) = len(ch labels):
            frequency: int = int(1 / (temp edf.times[1] -
temp edf.times[0]))
            step window: int = time window * frequency
            step: int = time step * frequency
            temp_is_seizure: np.ndarray =
np.zeros((temp edf.n times,))
            if os.path.exists(temp_f + ".seizures"):
                temp_annotation: wfdb.Annotation =
wfdb.rdann(temp f, "seizures")
                for i in range(int(temp_annotation.sample.size /
2)):
                    temp is seizure[
                        temp annotation.sample[i * 2] :
temp_annotation.sample[
                            i * 2 + 1
                    ] = 1
            temp len: int = temp_edf.n_times
            temp_is_seizure_ind: np.ndarray = np.array(
                    temp is seizure[i * step : i * step +
step window].sum()
                    / step window
                    for i in range((temp len - step window) //
step)
            temp 0 sample size = round(p *
np.where(temp is seizure ind = 0)[0].size)
            temp_1_sample_size = np.where(temp_is_seizure_ind > 0)
[0].size
            counter = counter + temp_0_sample_size +
temp_1_sample_size
        temp edf.close()
    # pyright: reportPossiblyUnboundVariable=false
    array signals: np.ndarray = np.zeros(
```

```
(counter, len(ch labels), step window), dtype=np.float32
    array_is_seizure: np.ndarray = np.zeros(counter, dtype=bool)
    counter: int = 0
    for n, temp f in enumerate(tqdm.tqdm(files train)):
        to_log: str = "No. {}: Reading. ".format(n)
        temp edf = mne.io.read raw edf(temp f)
        temp labels: List[str] = temp edf.ch names
        n label match: int = sum(
                any([0 \text{ if re.match}(c, l) = None else 1 for l in
temp_edf.ch_names])
                for c in ch_labels
        if n_label_match = len(ch_labels):
            ch mapping = {
                sorted([l for l in temp_edf.ch_names if re.match(c,
1) \neq None [0]: c
                for c in ch labels
            temp_edf.rename_channels(ch_mapping)
            # temp edf = temp edf.pick(ch labels)
            temp_is_seizure: np.ndarray =
np.zeros((temp edf.n times,))
            temp signals: np.ndarray =
temp edf.get data(picks=ch labels) * 1e6
            if os.path.exists(temp_f + ".seizures"):
                to_log: str = to_log + "seizure exists."
                temp annotation: wfdb.Annotation =
wfdb.rdann(temp_f, "seizures")
                for i in range(int(temp_annotation.sample.size /
2)):
                    temp is seizure[
                        temp_annotation.sample[i * 2] :
temp annotation.sample[
                             i * 2 + 1
                     ] = 1
            else:
                to_log = to_log + "No seizure."
            temp len: int = temp edf.n times
```

```
frequency: int = int(1 / (temp_edf.times[1] -
temp edf.times[0]))
            step window: int = time window * frequency
            step: int = time step * frequency
            temp_is_seizure_ind: np.ndarray = np.array(
                    temp is seizure[i * step : i * step +
step window].sum()
                    / step window
                    for i in range((temp len - step window) //
step)
                ]
            del temp_is_seizure
            temp 0 sample size: int = round(
                p * np.where(temp is seizure ind = 0)[0].size
            temp 1 sample size: int = np.where(temp is seizure ind
> 0)[0].size
            # seizure data
            temp ind: list = list(np.where(temp is seizure ind > 0)
[0]
            for i in temp ind:
                array signals[counter, :, :] = temp signals[
                    :, i * step : i * step + step_window
                array is seizure[counter] = True
                counter = counter + 1
            # no seizure data
            temp ind: list = random.sample(
                list(np.where(temp is seizure ind = 0)[0]),
temp 0 sample size
            for i in temp ind:
                array_signals[counter, :, :] = temp_signals[
                    :, i * step : i * step + step_window
                array is seizure[counter] = False
                counter = counter + 1
```

```
to log += "{} signals added: {} w/o seizure, {} w/
seizure.".format(
                temp 0 sample size + temp 1 sample size,
                temp 0 sample size,
                temp 1 sample size,
            )
        else:
            to log += "Not appropriate channel labels. Reading
skipped.".format(n)
        logger.info(to log)
        temp_edf.close()
        if n % 10 = 0:
            gc.collect()
    gc.collect()
   np.save("signal_samples", array_signals)
    np.save("is_seizure", array_is_seizure)
# Preprocessing
# The original signal frequency is 256 Hz, but to simplify the
data,
# it has been resampled to 128 Hz.
array signals = array signals[:, :, ::2]
# show a sample of extracted signals (the last one)
vertical width: int = 300
signals: np.ndarray = array_signals[-1, :, :]
fs: int = 128
fig, ax = plt.subplots()
for i in range(signals.shape[0]):
    ax.plot(
        np.arange(signals.shape[-1]) / frequency,
        signals[i, :] + i * vertical width,
        linewidth=0.5.
        color="tab:blue",
    ax.annotate(ch labels[i], xy=(0, i * vertical width))
ax.invert_yaxis()
plt.show()
```

```
# Checking how much of signals have seizure inside.
array_n: np.ndarray = np.where(array_is_seizure > 0.0)[0]
print("Number of all the extracted signals:
{}".format(array is seizure.size))
print("Number of signals with seizures: {}".format(array n.size))
print(
    "Ratio of signals with seizures: {:.3f}".format(
        array n.size / array is seizure.size
)
# Let's see samples with seizures.
for n in random.sample(list(array_n), 10):
    vertical width: int = 300
   temp_signals: np.ndarray = array_signals[n, :, :]
    frequency: int = 128
    fig, ax = plt.subplots(2, 1, figsize=(10, 6),
gridspec_kw={"height_ratios": [3, 1]})
    for i in range(temp signals.shape[0]):
        ax[0].plot(
            np.arange(temp_signals.shape[-1]) / frequency,
            temp signals[i, :] + i * vertical width,
            linewidth=0.5,
            color="tab:blue",
        ax[0].annotate(ch labels[i], xy=(0, i * vertical width))
    ax[0].invert yaxis()
    ax[0].set xlim(0, 8)
   ax[0].set_title("sample no. {}".format(n))
    ax[1].pcolormesh(
        np.arange(temp_signals.shape[-1]) / frequency,
        np.arange(len(ch_labels)),
        temp signals[:, :],
        cmap="gray",
    ax[1].invert yaxis()
    plt.show()
# Add a Channel dimension
array_signals: np.ndarray = array_signals[:, :, :, np.newaxis]
# splitting training data into training & validation data.
```

```
X_train, X_val, y_train, y_val = model_selection.train_test_split(
    array_signals, array_is_seizure, test_size=0.3,
stratify=(array is seizure > 0)
del array signals, array is seizure
# Initialize the deep learning model
model = keras.models.Sequential()
# Add the first convolutional layer with input shape
# Ensure input shape matches the expected dimensions (channels,
height, width)
model.add(
    layers.Input(shape=(18, 1024, 1)),
)
model.add(
    layers.Conv2D(filters=64, kernel_size=(2, 4), padding="same",
activation="relu")
model.add(
    layers.Conv2D(
        # filters=64,
        filters=32,
        kernel_size=(2, 4),
        padding="same",
        activation="relu",
        input shape=(18, 1024, 1),
) # Modify input shape as needed
# Add more convolutional layers and pooling layers
model.add(
    layers.Conv2D(
        filters=32,
        kernel_size=(2, 4),
        strides=(1, 2),
        padding="same",
        activation="relu",
    )
)
model.add(layers.MaxPooling2D(pool_size=(1, 2)))
model.add(
```

```
layers.Conv2D(filters=64, kernel_size=(2, 4), padding="same",
activation="relu")
model.add(
    layers.Conv2D(
        filters=64,
        kernel_size=(2, 4),
        strides=(1, 2),
        padding="same",
        activation="relu",
    )
)
model.add(layers.MaxPooling2D(pool size=(2, 2)))
model.add(
    layers.Conv2D(filters=128, kernel_size=(4, 4), padding="same",
activation="relu")
model.add(
    layers.Conv2D(
        filters=128,
        kernel size=(4, 4),
        strides=(1, 2),
        padding="same",
        activation="relu",
    )
)
model.add(layers.MaxPooling2D(pool size=(1, 2)))
# Add a global average pooling layer
model.add(layers.GlobalAveragePooling2D())
# Add fully connected layers
model.add(layers.Dense(256, activation="relu"))
model.add(layers.Dropout(0.25)) # Dropout for regularization
model.add(layers.Dense(128, activation="relu"))
model.add(layers.Dense(64, activation="relu"))
model.add(layers.Dropout(0.25)) # Another dropout layer
model.add(
    layers.Dense(1, activation="sigmoid")
   # Output layer for binary classification
model.compile(optimizer="adam", loss="binary_crossentropy",
metrics=["accuracv"])
model.summary()
```

```
plot_model(model, show_shapes=True, to_file="model.png")
plot model(model, show shapes=True, dpi=70)
LEARNING RATE: float = 1e-4
OPTIMIZER: tf.keras.optimizers =
tf.keras.optimizers.Adam(learning rate=LEARNING RATE)
model.compile(optimizer=OPTIMIZER, loss="binary crossentropy",
metrics=["accuracy"])
# callbacks
VERBOSE: int = 1
# Define the early stopping callback
es = EarlyStopping(
    monitor="val loss",
    patience=20,
    verbose=VERBOSE,
    mode="auto".
    restore best weights=True,
)
# Define the learning rate reduction callback
lr = ReduceLROnPlateau(
    monitor="val loss", factor=0.75, patience=5, verbose=1,
min lr=1e-8
)
callbacks: List = [es, lr]
# Nvidia thing, allows using float16 instead of float32
mixed_precision.set_global_policy("mixed_float16")
# Clear any previous session
tf.keras.backend.clear_session()
# Train the model
hist = model.fit(
    x=X train,
    y=y train,
    validation data=(X_val, y_val),
    # epochs=200, # lets not use this
    epochs=50.
    # batch_size=256, # does not work
    batch size=128,
    callbacks=callbacks.
```

```
# Save the model
keras.saving.save_model(model, "CHB_MIT_sz_detec demo.keras")
fig, ax = plt.subplots(1, 2, figsize=(12, 4))
ax[0].plot(hist.history["loss"], label="loss")
ax[0].plot(hist.history["val_loss"], label="val_loss")
ax[0].set xlabel("epoch")
ax[0].set ylabel("loss")
ax[0].axvline(x=es.best_epoch, label="early stopping",
color="tab:red", alpha=0.5)
r = 0.2
temp y = r * min(hist.history["loss"]) + (1 - r) *
max(hist.history["loss"])
ax[0].annotate(" early stopping:\n best epoch", xy=(es.best_epoch,
temp y))
ax[0].set title("Loss")
ax[0].legend()
ax[1].plot(hist.history["accuracy"], label="accuracy")
ax[1].plot(hist.history["val accuracy"], label="val accuracy")
ax[1].set xlabel("epoch")
ax[1].set ylabel("accuracy")
r = 0.8
temp y = r * min(hist.history["accuracy"]) + (1 - r) *
max(hist.history["accuracy"])
ax[1].axvline(x=es.best epoch, label="early stopping",
color="tab:red", alpha=0.5)
ax[1].annotate(" early stopping:\n best epoch", xy=(es.best_epoch,
temp y))
ax[1].set_title("Accuracy")
ax[1].legend()
plt.show()
```

Results:

fig1: database information after processing and splitting into test and train

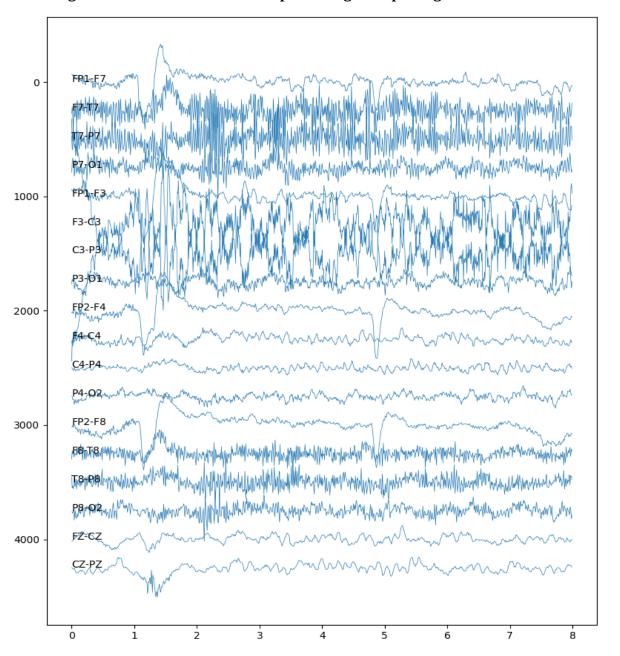
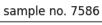
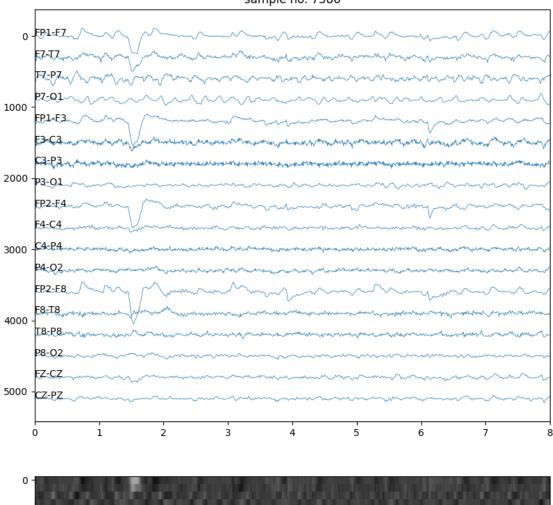
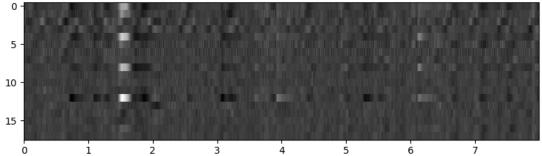
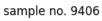


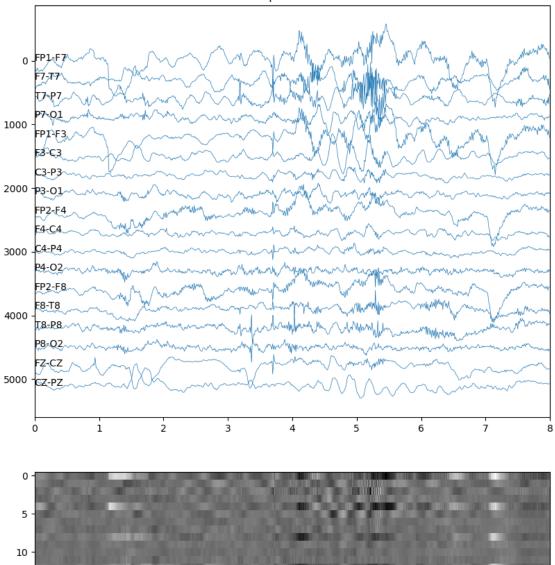
fig2: A sample of extracted signals

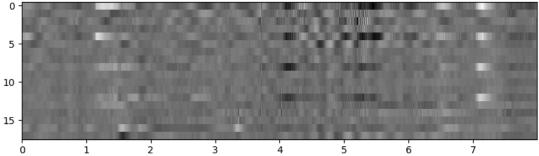


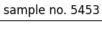


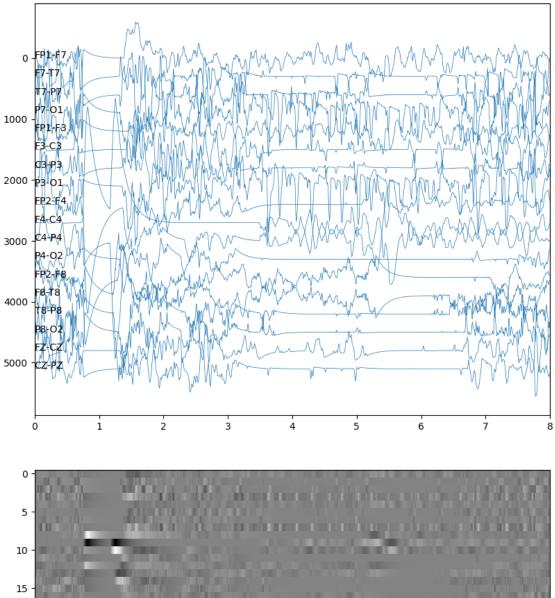


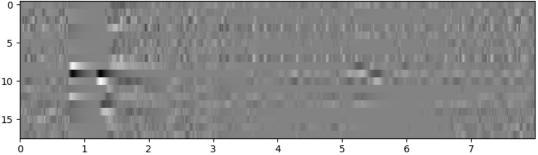


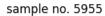


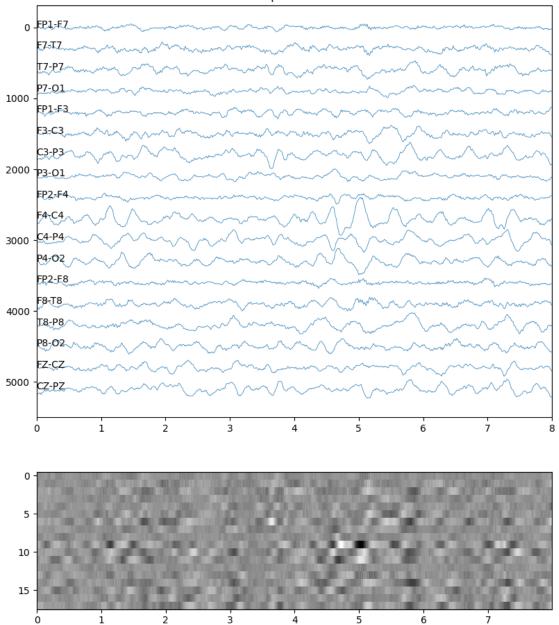


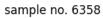


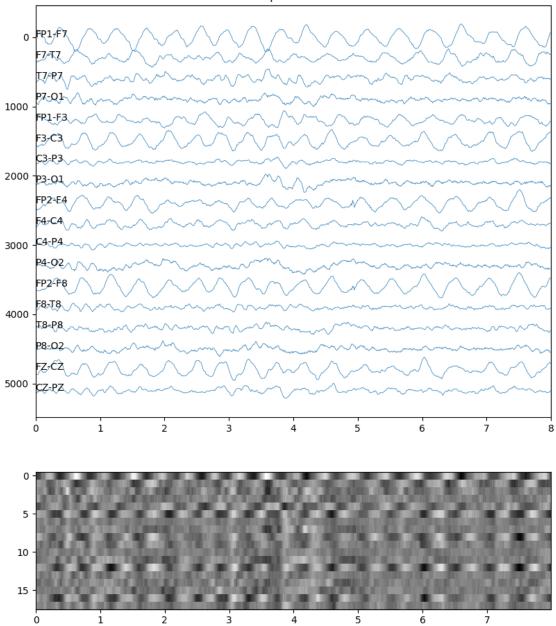


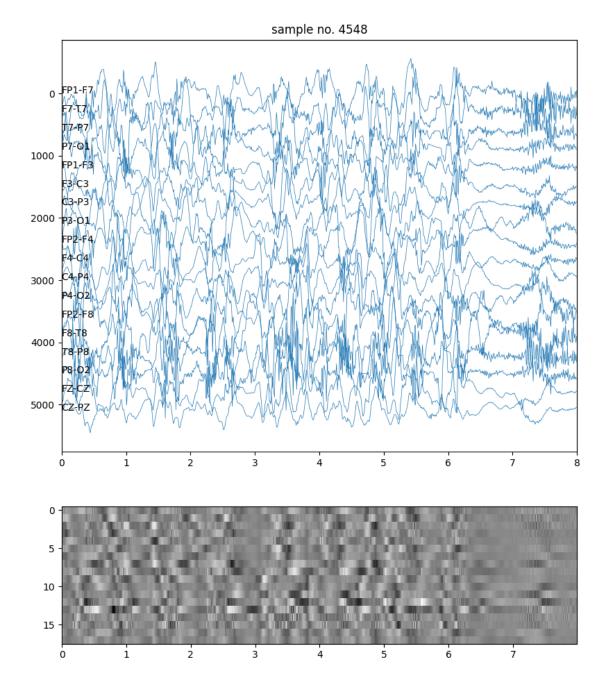


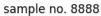


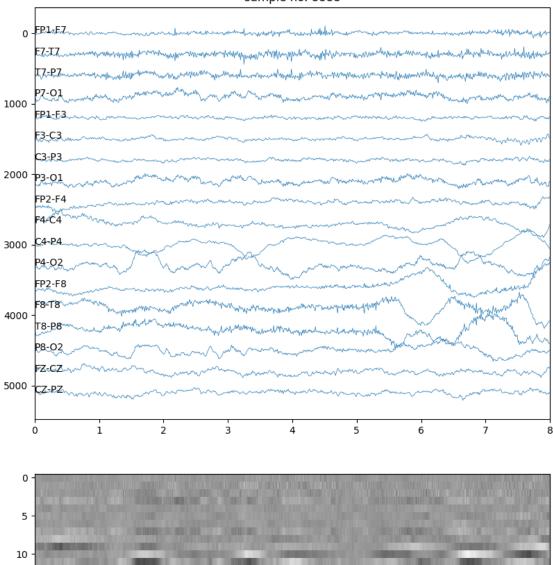


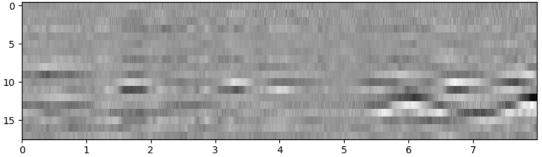


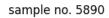


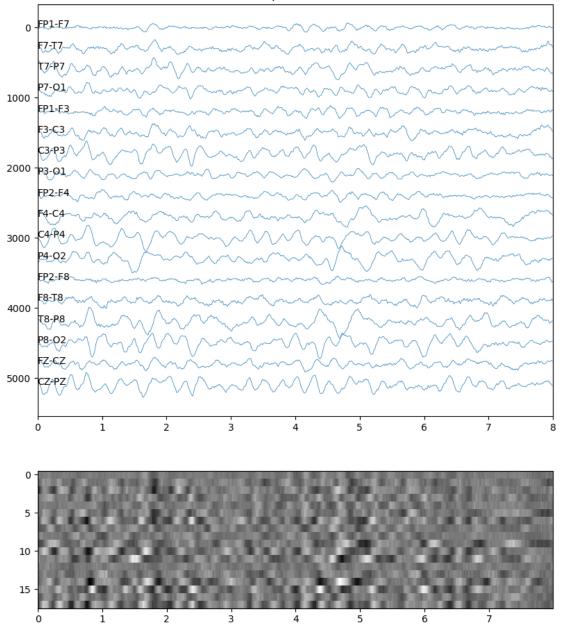


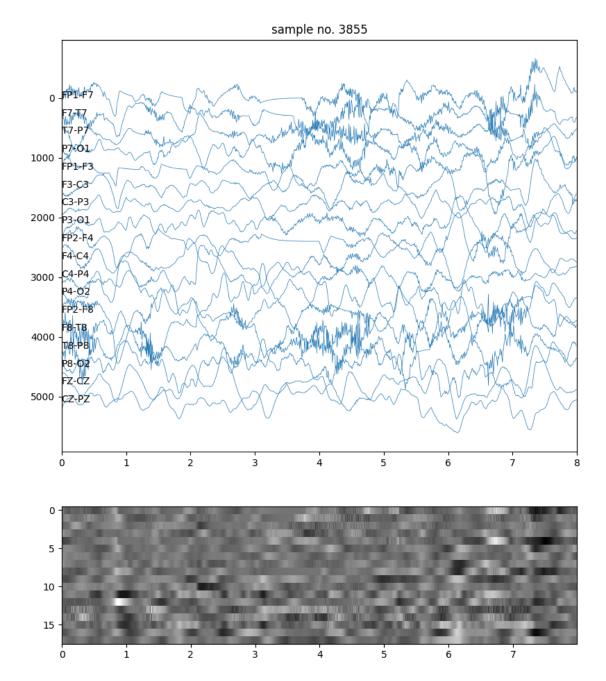


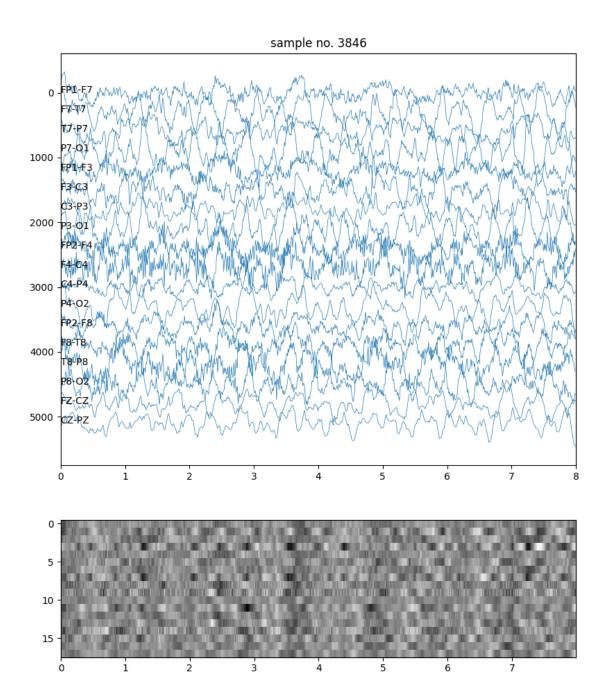


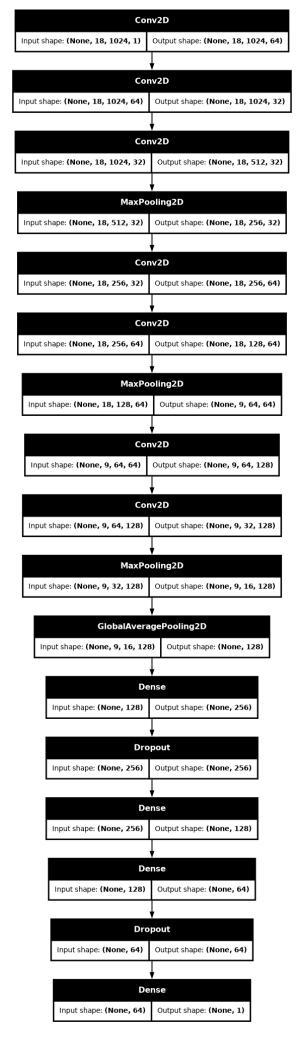












Layer (type)	Output Shape	Param #
conv2d (Conv2D)	(None, 18, 1024, 64)	576
conv2d_1 (Conv2D)	(None, 18, 1024, 32)	16,416
conv2d_2 (Conv2D)	(None, 18, 512, 32)	8,224
<pre>max_pooling2d (MaxPooling2D)</pre>	(None, 18, 256, 32)	0
conv2d_3 (Conv2D)	(None, 18, 256, 64)	16,448
conv2d_4 (Conv2D)	(None, 18, 128, 64)	32,832
<pre>max_pooling2d_1 (MaxPooling2D)</pre>	(None, 9, 64, 64)	0
conv2d_5 (Conv2D)	(None, 9, 64, 128)	131,200
conv2d_6 (Conv2D)	(None, 9, 32, 128)	262,272
<pre>max_pooling2d_2 (MaxPooling2D)</pre>	(None, 9, 16, 128)	0
<pre>global_average_pooling2d (GlobalAveragePooling2D)</pre>	(None, 128)	0
dense (Dense)	(None, 256)	33,024
dropout (Dropout)	(None, 256)	0
dense_1 (Dense)	(None, 128)	32,896
dense_2 (Dense)	(None, 64)	8,256
dropout_1 (Dropout)	(None, 64)	0
dense_3 (Dense)	(None, 1)	65

Fig: Model summary

Code for prediction:

```
from scipy.signal import find_peaks
from sklearn import metrics
from typing import List
import matplotlib.pyplot as plt
import mne
import numpy as np
import os
import glob
import random
import re
import tqdm
import wfdb
from tensorflow.keras.models import load_model
# Define channel labels
ch labels: List[str] = [
  "FP1-F7",
  "F7-T7",
  "T7-P7",
  "P7-O1".
  "FP1-F3",
  "F3-C3".
  "C3-P3",
  "P3-O1",
  "FP2-F4",
  "F4-C4",
  "C4-P4",
  "P4-O2",
  "FP2-F8",
  "F8-T8".
  "T8-P8",
  "P8-O2",
  "FZ-CZ",
  "CZ-PZ",
# Define base path to data
base_path: str = "/home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit/"
# Walk through the directory and print all filenames
def list_files_in_directory(path: str) -> None:
  for dirname, _, filenames in os.walk(path):
    for filename in filenames:
       print(os.path.join(dirname, filename))
```

```
list_files_in_directory(base_path)
# Gather folders and extract patient numbers
folders: List[str] = sorted(glob.glob(f"{base_path}/*/"))
n_patient: List[str] = [folder.rstrip("/").split("/")[-1][-2:] for folder in folders]
print("Patients:", *n_patient)
# Set seed for reproducibility
random.seed(2024)
# Split patients into train and test sets
# Patients are assigned to training and test groups through a random selection process.
ratio train: float = 0.3
test_patient_str: List[str] = sorted(
  random.sample(n_patient, round(ratio_train * len(n_patient)))
print("Test PT:", *test_patient_str)
# Collect file paths for train and test sets
def collect_files(patient_str_list: List[str], path: str) -> List[str]:
  return [
     edf_file
     for patient in patient_str_list
     for edf_file in glob.glob(f"{path}/chb{patient}/*.edf")
  ]
files_test: List[str] = collect_files(test_patient_str, base_path)
print("Number of test files:", len(files_test))
# Model: CHB_MIT_sz_detec_demo.keras
model = load_model("CHB_MIT_sz_detec_demo.keras")
def sampling_data_pred(f, verbose=True):
  if verbose == True:
     print("{}: Reading. ".format(f))
  temp_edf = mne.io.read_raw_edf(f)
  temp_array_signals, temp_is_seizure_ind = np.array([]), np.array([])
  if sum(
       any([0 \text{ if re.match}(c, l) == \text{None else 1 for l in temp\_edf.ch\_names}])
```

```
for c in ch_labels
  ) == len(ch_labels):
    ch_mapping = {
       sorted([l for l in temp_edf.ch_names if re.match(c, l) != None])[0]: c
       for c in ch labels
    temp_edf.rename_channels(ch_mapping)
    temp is seizure = np.zeros((temp edf.n times,))
# pyright: reportOperatorIssue=false
     temp signals = temp edf.get data(picks=ch labels) * 1e6
    if os.path.exists(f + ".seizures"):
       if verbose == True:
          print("seizure exists.", end=" ")
       temp_annotation = wfdb.rdann(f, "seizures")
       for i in range(int(temp_annotation.sample.size / 2)):
          temp_is_seizure[
            temp annotation.sample[i * 2]: temp annotation.sample[i * 2 + 1]
         ] = 1
    temp_len = temp_edf.n_times
    time window = 8
    time step = 4
     fs = int(1 / (temp_edf.times[1] - temp_edf.times[0]))
    step_window = time_window * fs
    step = time_step * fs
    # sampling all signals
    temp_array_signals = np.array(
       Γ
          temp_signals[:, i * step : i * step + step_window]
          for i in range((temp_len - step_window) // step)
       1
    )
     temp_is_seizure_ind = np.array(
          temp_is_seizure[i * step : i * step + step_window].sum() / step_window
          for i in range((temp_len - step_window) // step)
       1
  else:
    if verbose == True:
       print("EEG {}: Not appropriate channel labels. Reading skipped.".format(n))
  return temp_array_signals, temp_is_seizure_ind
```

```
# reading files and prediction
list pred = []
list_true = []
for f in tqdm.tqdm(files_test):
  array_signals, array_is_seizure = sampling_data_pred(f, verbose=False)
  array_signals = array_signals[:, :, ::2, np.newaxis]
  list_pred.append(model.predict(array_signals, verbose=0))
  list true.append(array is seizure)
# threshold = 0.5
report = metrics.classification_report(
  np.concatenate(list_true) > 0, np.concatenate(list_pred) > 0.5
print(report)
# threshold = 0.9
report = metrics.classification_report(
  np.concatenate(list_true) > 0, np.concatenate(list_pred) > 0.9
print(report)
roc = metrics.roc_curve(np.concatenate(list_true) > 0, np.concatenate(list_pred))
auc = metrics.roc_auc_score(np.concatenate(list_true) > 0, np.concatenate(list_pred))
plt.figure(figsize=(4, 4))
plt.plot(
  roc[0][np.argmin(np.abs(roc[2] - 1)) :], roc[1][np.argmin(np.abs(roc[2] - 1)) :]
plt.xlabel("FPR: false positive rate")
plt.ylabel("TPR: true positive rate")
plt.title("ROC curve: AUC score = {:.2f}".format(auc))
th = [0.1, 0.2, 0.5, 0.9, 0.95, 1.0]
ind = [np.argmin(np.abs(roc[2] - 1)) for 1 in th]
plt.scatter(roc[0][ind], roc[1][ind], s=15)
for i, l in enumerate(ind):
   plt.annotate("{}".format(th[i]), xy=(roc[0][l], roc[1][l]))
# plt.plot([0, 1, 1, 0, 0], [0, 0, 1, 1, 0], color='black', linewidth=1)
plt.ylim(-0.05, 1.05)
plt.xlim(-0.05, 1.05)
plt.grid()
# plt.axis('off')
plt.show()
```

```
for i, f in enumerate(files_test):
  if os.path.exists(f + ".seizures"):
     print("Index = {} has seizures: {}".format(i, f))
def moving_ave(a, n):
  if len(a.shape) != 1:
     print("Not 1 dimension array. return nothing.")
     return
  temp = np.zeros(a.size - n)
  for i in range(n):
     temp = temp + a[i : -n + i]
  temp = temp / n
  return temp
# get signals and labels from test data.
n = 100
array_signals, array_is_seizure = sampling_data_pred(files_test[n])
# preprocess
array_signals = array_signals[:, :, ::2, np.newaxis]
if model is None:
  print("Model not found. Exit.")
  exit()
# use deep learning model
pred = model.predict(array_signals)
time_window = 8
time\_step = 4
mv_win = 3
fig, ax = plt.subplots(figsize=(12, 2))
ax.plot(
  np.arange(pred.size) * time_step,
  pred.flatten(),
  alpha=0.7,
  label="deep learning model pred",
ax.plot(np.arange(pred.size) * time_step, array_is_seizure, alpha=0.7, label="True label")
pred_moving_ave = moving_ave(pred.flatten(), mv_win)
pred_peaks, _ = find_peaks(pred_moving_ave, height=0.95, distance=6)
```

```
ax.plot(
  np.arange(pred.size - mv win) * time step,
# pyright: reportArgumentType=false
  pred_moving_ave,
  alpha=0.9,
  label="pred - moving ave",
  color="tab:pink",
  zorder=0.
)
# pyright: reportOptionalSubscript=false
ax.scatter(pred_peaks * time_step, pred_moving_ave[pred_peaks], s=20, color="tab:red")
ax.set_xlabel("time (s)")
ax.set_ylabel("p")
ax.set_xlim(0, pred.size * time_step + 500)
ax.legend(loc="upper right")
plt.show()
if pred peaks.size == 0:
  print("No seizure detected.")
else:
  f = files_test[n]
  temp_edf = mne.io.read_raw_edf(f)
  temp_labels = temp_edf.ch_names
  temp_signals = None
  if sum(
    ſ
       any([0 \text{ if re.match}(c, l) == \text{None else 1 for l in temp edf.ch names}])
       for c in ch_labels
  ) == len(ch_labels):
    ch_mapping = {
       sorted([l for l in temp_edf.ch_names if re.match(c, l) != None])[0]: c
       for c in ch_labels
    temp_edf.rename_channels(ch_mapping)
    # temp_edf = temp_edf.pick(ch_labels)
    temp_is_seizure = np.zeros((temp_edf.n_times,))
    temp_signals = temp_edf.get_data(picks=ch_labels) * 1e6
  fs = int(1 / (temp_edf.times[1] - temp_edf.times[0]))
  for n_peak in range(pred_peaks.size):
     ind_peak = pred_peaks[n_peak] * time_step * fs
    backward steps = 30 * fs
    forward steps = 15 * fs
    vertical_width = 500
```

```
fig, ax = plt.subplots(figsize=(10, 6))
  if temp_signals is not None:
     for i in range(temp_signals.shape[0]):
       ax.plot(
          np.arange(ind_peak - backward_steps, ind_peak + forward_steps) / fs,
          temp_signals[i, ind_peak - backward_steps : ind_peak + forward_steps]
          + i * vertical_width,
          linewidth=0.5,
          color="tab:blue",
       ax.annotate(
          ch_labels[i], xy=((ind_peak - backward_steps) / fs, i * vertical_width)
       )
     ax.axvline(
       x=ind_peak / fs, color="tab:red", alpha=0.5, label="Seizure detection point"
     )
     ax.invert_yaxis()
     ax.legend(loc="upper right")
     plt.show()
# ax.set_xlim(0, 8)
temp_edf.close()
```

100%				
	precision	recall	f1-score	support
False	1.00	0.97	0.98	293126
True	0.05	0.93	0.10	502
accuracy			0.97	293628
macro avg	0.53	0.95	0.54	293628
weighted avg	1.00	0.97	0.98	293628
	precision	recall	f1-score	support
False	1.00	0.99	1.00	293126
True	0.17	0.82	0.28	502
accuracy			0.99	293628
macro avg	0.58	0.91	0.64	293628
weighted avg	1.00	0.99	1.00	293628

Fig: model metrics summary

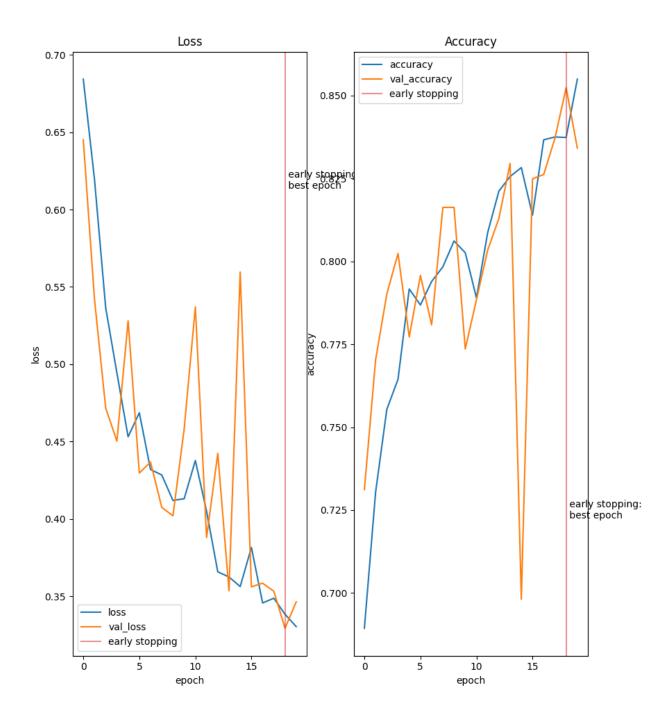


Fig: Loss and Accuracy graph

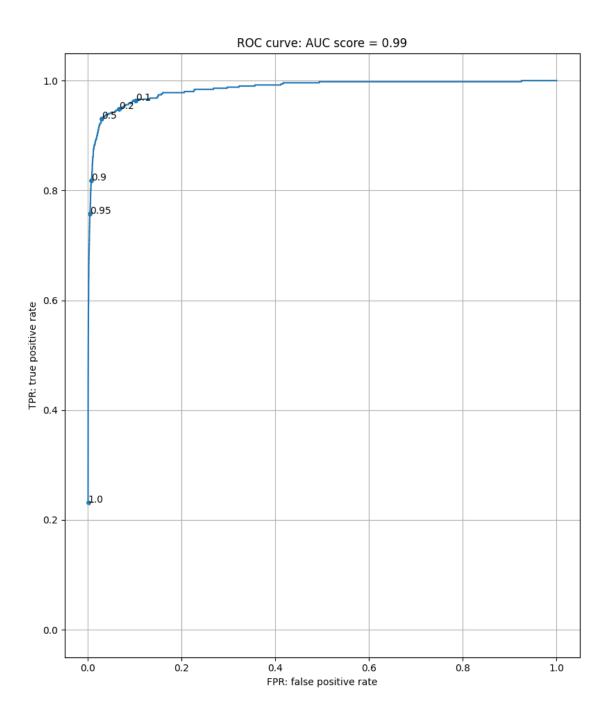


Fig: ROC curve with AUC score

```
Index = 0 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming Lab/chbmit//chb06/chb06 01.edf
Index = 0 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb06/chb06_04.edf
Index = 3 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb06/chb06_09.edf
Index = 8 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb06/chb06_10.edf
Index = 9 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb06/chb06_11.edf
Index = 12 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb06/chb06_13.edf
Index = 15 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb06/chb06_24.edf
Index = 29 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb07_chb07_13.edf
Index = 30 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb07/chb07_12.edf
Index = 36 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb07/chb07_12.edf
Index = 36 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb07/chb07_12.edf
 Index = 36 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb07/chb07_12.edf
Index = 36 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb07/chb07_19.edf
Index = 42 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb09/chb09_06.edf
Index = 44 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb09/chb09_08.edf
Index = 44 has seizures: /nome/utsav/work/academic/NIIM-T24CS003/Programming_Lab/chbmit//chb09/chb09_08.edf
Index = 54 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb10/chb10_12.edf
Index = 64 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb10/chb10_20.edf
Index = 71 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb10/chb10_20.edf
Index = 74 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb10/chb10_27.edf
Index = 76 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb10/chb10_31.edf
 Index = 76 has seizures: /home/utsav/work/academit/NITM-T24C3003/Programming_Lab/chbmit//chb10/chb10_31edf
Index = 77 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb10/chb10_38.edf
Index = 80 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb10/chb10_89.edf
Index = 80 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb10/chb10_89.edf
Index = 83 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb14/chb14_03.edf
Index = 84 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb14/chb14_06.edf
Index = 85 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb14/chb14_11.edf
Index = 86 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb14/chb14_17.edf
 Index = 92 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb14/chb14_18.edf
Index = 100 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb14/chb14_27.edf
                        116 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb16/chb16_10.edf
 Index =
 Index = 117 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb16/chb16_11.edf
Index = 120 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb16/chb16_14.edf
Index = 122 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb16/chb16_16.edf
 Index = 123 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb16/chb16_18.edf
Index = 124 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb16/chb16_17.edf
Index = 124 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb16/chb16_17.edf
Index = 153 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb19/chb19_28.edf
Index = 154 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb19/chb19_29.edf
Index = 155 has seizures: /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb19/chb19_30.edf
/home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit//chb14_27.edf: Reading.

Extracting EDF parameters from /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit/chb14/chb14_27.edf ...
 EDF file detected
  /home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit/chb2_pred.py:89: RuntimeWarning: Channel names are n
 or duplicates.
 temp_edf = mne.io.read_raw_edf(f)
/home/utsav/work/academic/NITM-T24CS003/Programming_Lab/chbmit/chb2_pred.py:89: RuntimeWarning: Scaling factor is no
       0, --1, --2, --3, --4
       temp_edf = mne.io.read_raw_edf(f)
  Setting channel info structure...
  Creating raw.info structure...
                                                                                 0s 13ms/step
 29/29
 No seizure detected.
  (chb)

♦ v3.12.7  ● 00:35
```

Fig: Prediction results of the model