

# G-Protein-Coupled Enzyme Cascades Have Intrinsic Properties that Improve Signal Localization and Fidelity

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**ABSTRACT** G-protein-coupled enzyme cascades are used by eukaryotic cells to detect external signals and transduce them into intracellular messages that contain biological information relevant to the cell's function. Since G-protein-coupled receptors that are designed to detect different kinds of external signals can generate the same kind of intracellular response, effective signaling requires that there are mechanisms to increase signal specificity and fidelity. Here we examine the kinetic equations for the initial three stages in a generic G-protein-coupled cascade and show that the physical properties of the transduction pathway result in two intrinsic features that benefit signaling. 1), The response to a single activated receptor is naturally confined to a localized spatial domain, which could improve signal specificity by reducing cross talk. 2), The peak of the response generated by such a signaling domain is limited. This saturation effect reduces trial-to-trial variability and increases signaling fidelity by limiting the response to receptors that remain active for longer than average. We suggest that this mechanism for reducing response fluctuations may be a contributing factor in making the single photon responses of vertebrate retinal rods so remarkably reproducible.

## INTRODUCTION

The functional viability of multicellular organisms depends on their constituent cellular building blocks being able to communicate with each other. This requires that cells have a way to detect and respond specifically to select external signals. One of the most common strategies for doing this makes use of a three-stage G-protein-coupled enzyme cascade (Lodish et al., 2000). In the first stage, a specialized membrane receptor protein,  $R$ , is activated by its interaction with a specific external signal, such as by binding a particular ligand or absorbing a photon of a particular wavelength. In the second stage, the activated receptor,  $R^*$ , turns on a heterotrimeric G-protein,  $G^*$ , by catalyzing GDP/GTP exchange on the  $\alpha$ -subunit of the protein. During the time it stays active,  $t_R$ , a single  $R^*$  will serially excite many G-proteins and thus amplify the original signal, i.e., one  $R^*$  to many  $G^*$ . In the third stage, each  $G^*$  associates with an effector protein,  $E$ , forming a  $G^*-E$  complex that stimulates the effector. We shall refer to the  $G^*-E$  complex as the active effector,  $E^*$ . Activated effector proteins are most commonly enzymes that control the level of an intracellular second messenger such as a cyclic nucleotide or  $\text{Ca}^{2+}$ . The resulting change in second messenger concentration represents the output signal of the transduction process and is further amplified by each activated enzyme,  $E^*$ , which turns over more than one substrate molecule.

The strength of the cascade's output signal, i.e., the size of the change in second messenger concentration, depends on how many effector enzymes are active and how long they

stay active. Thus the overall gain of the cascade depends on the rate of its inactivation. This involves shutting off the two catalytically active intermediates,  $R^*$  and  $E^*$ . The life of the activated receptor,  $R^*$ , and the steady production of  $G^*$  it catalyzes, are terminated after receptor phosphorylation. The catalytic activity of  $E^*$  is terminated when the GTPase activity of  $G^*$  within the  $G^*-E$  complex hydrolyzes GTP to GDP, leading to the dissociation of the complex and the shutting off of effector activity. The G-protein, in its inactive (GDP-bound) state is no longer able to excite the effector and  $E^*$  returns to its resting state. Additional elements, which control both  $R^*$  shutoff and the intrinsic activity of G-protein GTPase (Berman and Gilman, 1998; He et al., 1998; Makino et al., 1999; Arshavsky et al., 2002) provide a mechanism for gain control. Our treatment of the G-protein cascade considers the pathway only so far as the activation of effector enzyme; it does not include the dynamics of the second messenger signal.

The activated elements of the cascade ( $R^*$ ,  $G^*$ , and  $E^*$ ) that ultimately generate the second messenger signal are all membrane-associated and diffuse two-dimensionally on the membrane surface. Here we consider two inherent properties of signals that arise as a consequence of being generated by an amplified enzyme cascade that is confined to the membrane. By examining the first steps of G-protein signaling that follow the excitation of a single receptor we show that the resulting activity of the effector enzyme is naturally localized to a small  $\sim 1 \mu\text{m}$  radius response domain and the peak amplitude of the response is limited. Both of these built-in effects would serve to benefit the signaling process. The establishment of a localized signaling domain would reduce cross talk and improve signal specificity. Limiting the peak amplitude of the response would decrease

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trial-to-trial variability and thus increase response reproducibility and signal fidelity.

Our analysis is relevant to membrane-localized enzyme cascades in general, but our treatment is guided specifically by the phototransduction process in vertebrate retinal rods. We have chosen this as our model because it is the most thoroughly studied and best-understood example of G-protein-coupled signaling (Stryer, 1991; Baylor, 1996). The basic scheme is the same as the generic one described above. An external signal (a visible photon) activates a membrane receptor (rhodopsin, *Rh*). The light-activated receptor (*Rh*<sup>\*</sup>) serially activates many G-proteins (also known as transducin, or *T*) molecules. The activated transducin (*T*<sup>\*</sup>) stimulates one-to-one an equal number of effector enzymes (phosphodiesterase; i.e., PDE). The activated phosphodiesterase (PDE<sup>\*</sup>) hydrolyzes cyclic nucleotides (cyclic GMP; i.e., cGMP), generating an amplified second messenger signal consisting of a fall in the resting level of cGMP. In retinal rods the drop in cGMP closes ion channels that are opened by binding cGMP (cyclic nucleotide-gated channels). This reduces the standing inward cationic current that circulates through the rod in darkness and completes the phototransduction process that converts light into an amplified electrical signal, a change in cell membrane potential.

Another reason we have focused our attention on phototransduction is that our analysis considers the events that follow the activation of a single receptor molecule. Detailed information about the signal that G-protein-coupled cascades produce in response to a single activated receptor molecule is only available for photoreceptors, which produce a robust response to the absorption of a single photon (Baylor, 1984).

### The G-protein module

The analysis begins by considering the rate equations that describe the localized activation and deactivation of G-protein and effector enzyme caused by activated receptor *R*<sup>\*</sup>:

$$\frac{d[G^*]}{dt} = k_1[R^*] - k_2[E][G^*] + D_G \nabla^2 [G^*], \quad (1)$$

$$\frac{d[E^*]}{dt} = k_2[E][G^*] - k_H[E^*] + D_E \nabla^2 [E^*]. \quad (2)$$

In addition to formation and destruction of active species these equations describe their diffusion on the membrane, away from their sites of production. The G-protein and effector enzyme are membrane-associated proteins and their concentrations are expressed as areal densities (number per  $\mu\text{m}^2$ ) denoted by the bracket [...]. Their diffusion coefficients  $D_G$  and  $D_E$  are reported (Pugh and Lamb, 1993; Lamb, 1994) to have similar values in the 1–2  $\mu\text{m}^2/\text{s}$  range. The constant  $k_1$  is the rate of activation of  $G^*$  by  $R^*$ . More generally this process obeys Michaelis-Menten kinetics,  $k_1[R^*]/(1+K_m/[G])$ , which we assume operates in the

saturation limit when  $[G] \gg K_m$ , as is apparently the case for phototransduction. The kinetic constant  $k_2$  describes the formation of the  $G^*-E$  complex and thus the production of  $E^*$ . The rate of  $E^*$  decay is governed by  $k_H$ , the rate of  $G^*$  inactivation due to GTP hydrolysis by the G-protein's GTPase activity within the  $G^*-E$  complex. We assume that  $E$  and  $E^*$  have the same diffusivity ( $D_E$ ). As a result, the total  $E$  concentration,  $[E_{\text{tot}}] = [E] + [E^*]$ , satisfies a simple diffusion equation, and is taken to be a constant in this study.

The kinetic equations (Eqs. 1 and 2) do not describe the full G-protein cycle, nor do they consider the possible dissociation of  $G^*$  from the membrane, which might become important under conditions of prolonged strong excitation (Chabre and Deterre, 1989; Heck and Hofmann, 1993, 2001). Nevertheless, they can be used to describe the response evoked by the activation of a single receptor molecule. In the continuum kinetic equation description employed here, single receptor activation is represented as a density of active receptor,  $[R^*] = A(t)\delta(r-r^*)$ , sharply peaked at the location,  $r^*$ , of the active receptor molecule and non-zero only over the time interval  $0 < t < t_R$ , where  $t_R$  denotes the shutoff time of the activated receptor (note  $A(t) = 1$  for  $0 < t < t_R$ ). The shutoff of the active receptor is a random variable with an average lifetime,  $\tau_R$ , which is controlled by the rate of receptor phosphorylation and arrestin binding (Chabre and Deterre, 1989; Stryer, 1991; Helmreich and Hofmann, 1995). The difference between  $t_R$  (the shutoff time of a single activated receptor for a single trial) and lifetime  $\tau_R$  (defined as the average  $t_R$  taken over many trials) is important, and will come up later in the analysis.

Note that this description does not prevent the incorporation of other general properties of G-protein signaling. For example, multistep deactivation of  $R^*$  may be accommodated by endowing  $t_R$  with an appropriate sub-Poisson statistical distribution, whereas the diffusion of  $R^*$  may be represented by making the locus of activity,  $r^*$ , follow a random trajectory and averaging  $E^*$  activation patterns over all possible trajectories.

### Localization of G-protein signaling

Let us consider a response defined as the effector activity generated by a single catalytically active receptor molecule acting as a point source of  $[G^*]$ . The details of the analysis can be found in the Appendix. In the text we describe the physical mechanism of signal localization and saturation and then describe the relationships between particular parameters and the properties of the localization and saturation process. A full quantitative description obtained by the numerical solution of Eqs. 1 and 2, as described in the Appendix, is presented in the figures. To simplify the discussion we shall presently ignore effector diffusion, for it does not affect the key aspects of the mechanism.

Free  $G^*$  will spread spatially from its site of production with a characteristic length,  $l_d$ , that represents a competition

between its outward diffusion and its sequestration, upon binding with free  $E$ , into a  $G^*-E$  complex. This length can be expressed as

$$l_d = \sqrt{\frac{D_G}{k_2[E]}}, \quad (3)$$

and is quite short ( $<100$  nm using the parameters in Table 1, and assuming that free effector concentration is of the order of total effector concentration  $[E_{\text{tot}}]$ .) The one-to-one association of  $G^*$  and  $E$  to produce  $E^*$ , reduces free  $[E]$ .

The resulting initial response domain will have different properties depending on whether the rate of  $G^*$  activation is large or small compared to the rate of  $E^*$  (i.e.,  $G^*-E$  complex) deactivation. If the recovery of free  $E$ , which follows GTP hydrolysis within the complex, is faster than the rate of  $G^*$  production, then there will always be free  $E$  on hand to bind to free  $G^*$  and prevent its outward spread. For this to happen  $k_1$  must be less than the maximum rate of  $E$  recovery within the activated area ( $\pi l_d^2$ ), which we estimate as  $\pi l_d^2 [E^*] k_H = (\pi D_G k_H / k_2)([E^*]/[E])$ —note that, in the subsaturated condition,  $[E^*] < [E]$ . Thus a single molecule of activated receptor ( $R^*$ ) will give rise to a spatially localized subsaturated response domain when  $k_1 < (\pi D_G k_H / k_2)([E^*]/[E]) < \pi D_G k_H / k_2$ . It is convenient to define a saturation parameter ( $S$ ) as

$$S = k_1 k_2 / \pi D_G k_H. \quad (4)$$

The subsaturated response domain described above corresponds to  $S < 1$ . When  $S > 1$ , the deactivation of  $E^*$ , and recovery of free  $E$ , is slower than the rate of  $G^*$  production. Under these conditions after a time,  $t_i \approx \pi l_d^2 [E]/k_1 = \pi D_G/k_2 k_1$  ( $\sim 3-10$  ms for rod phototransduction), nearly all the effector molecules in the initial response domain will be excited, forming an area of saturated activity. This means that if  $R^*$  remains active for a time longer than  $t_i$ ,  $G^*$  will no longer be completely absorbed by free  $E$  within the  $l_d$  region. Molecules of  $G^*$  will spill out of the initial response domain and proceed to expand with a radius,  $r$ , growing with time as

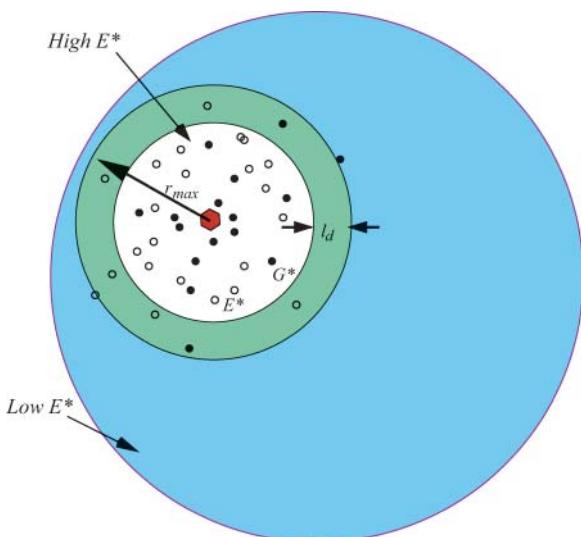
$$r(t) = \sqrt{\frac{k_1 t}{\pi [E_{\text{tot}}]}}, \quad (5)$$

**TABLE 1** Rod phototransduction parameter values

Description	Value	Reference
$D_G$	$1.2 \mu\text{m}^2/\text{s}$	Pugh and Lamb (1993)
$k_H$	$10 \text{ s}^{-1}$	Chen et al. (2000)
$k_1$	$100-1000 \text{ s}^{-1}$	Pugh and Lamb (1993); Kahler and Hofmann (1991); Leskov et al. (2000)
$k_2$	$1 \mu\text{m}^2/\text{s}$	Pugh and Lamb (1993)
[Rhodopsin]	$25,000 \mu\text{m}^{-2}$	Hamm and Bownds (1986)
[Transducin]	$2500 \mu\text{m}^{-2}$	Pugh and Lamb (1993)
[Phosphodiesterase]	$200 \mu\text{m}^{-2}$	Dumke et al. (1994)

so that the total number of activated effectors,  $E^*$ , will increase as  $k_1 t$ . This process is illustrated in Fig. 1. The expansion of the response domain continues until it reaches a maximum radius,  $r_{\text{max}}$ , which is on the order of  $\sqrt{k_1/\pi k_H [E_{\text{tot}}]}$ . We refer to this process as *spot formation*. It develops with a characteristic time,  $t_S$ , which is on the order of  $1/k_H$ . The internal consistency of this argument requires that the time for spot formation,  $t_S$ , be longer than the time it takes for  $G^*$  to spread by free diffusion over a distance on the same scale as  $r_{\text{max}}$ . This time is  $\sim r_{\text{max}}^2 / 4D_G$ , provided  $r_{\text{max}}^2 k_H / 4D_G = k_1 / 4\pi D_G [E_{\text{tot}}] < 1$ . This condition is satisfied for the rod parameters in Table 1.

Fig. 2 shows the space and time evolution of the effector response triggered by a single active receptor molecule. The traces present the results of the numerical solution of Eqs. 1 and 2 for  $S > 1$ . They show snapshots of the spatial profile of the response at different times. As time increases, the response (the spatial distribution of  $[E^*]$ ) converges to a stationary profile and does not change further with time. This illustrates the process of spot formation discussed above and shows that the limiting profile of the response is a saturated area of effector activity. Total effector activation in the case of continuous receptor activity is shown as a function of time in Fig. 3. As the saturated spot forms, the total number of active effectors  $E^*$  approaches a limit (Fig. 3 a) equal to  $k_1/k_H$  — a result derived in the Appendix. Fig. 3, b and c, compare the effect for two different values of  $k_1$  and three different values of  $k_H$ . In these figures the active effector number is normalized to the amplitude of the saturated response ( $k_1/k_H$ ) and time is measured in the units



**FIGURE 1** Localization of G-protein and effector activation. Hexagon represents location of single active receptor molecule, which activates G-proteins. Active G-protein (solid circles) diffuses outward, binds to the effector and activates it (open circles). Green denotes the activation front which moves out with time and if receptor activity persists, eventually converging to the stationary active spot boundary. See text for details.

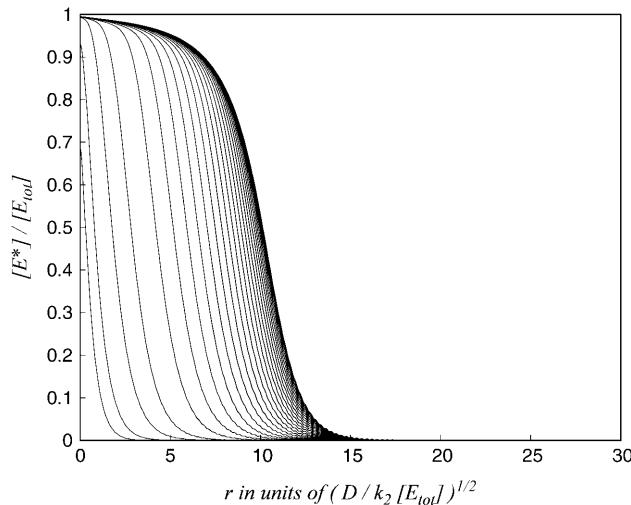


FIGURE 2 The fraction of activated effector is shown as a function of the distance from the excited receptor molecule at various times. The outermost curve corresponds to the saturated spot profile corresponding to stationary response to continuous receptor activity, and the inner curves represent the snapshots of the profile at earlier times, as this stationary profile is approached. Snapshots are taken at  $t = 0.015, 0.02, 0.025, 0.05, 0.1, 0.15, 0.2, 0.25, \dots, 3.0$  in units of  $1/k_H$ . Parameters are  $k_H = 3 \text{ s}^{-1}$ ,  $k_1 = 10^3 \text{ s}^{-1}$ , and  $k_2 = D_G = 1 \mu\text{m}^2/\text{s}$ ; the total effector density is  $[E_{\text{tot}}] = 200 \mu\text{m}^{-2}$ .

of  $1/k_H$ . Normalizing the response and time axes in this way shows that the characteristic time of saturation,  $t_S$ , (defined quantitatively as the time for half-maximum effector activation), scales with (and is approximately equal to)  $k_H^{-1}$ , with only a weak dependence on  $k_1$ . The maximal active domain size,  $r_{\max}$ , as a function of  $k_H$ , is shown in Fig. 4. Spot size scales as  $\sqrt{k_1/k_H}$ .

The effect of this localized saturation on the actual response depends on the duration of receptor activity. The plots in Fig. 3, *b* and *c*, show the growth of normalized effector activity ( $E^*(t)$ ) in response to a maintained step of receptor activation. The effector response to a pulse of receptor activity staying on for time  $t_R$ , would depart from the time course of the response to a step, only after receptor shutoff at  $t_R$  — at which time the growth of  $E^*$  would slow, reach a peak and begin to decline as recovery took over. Hence, the peak amplitude of the response, as a function of time ( $E_p^*(t)$ ), closely follows the behavior of  $E^*(t)$ . Fig. 5 presents  $E_p^*(t)$  determined from the numerical solution of Eqs. 1 and 2, as described in the Appendix. Since the timescale in this figure is in units of  $1/k_H$ , which, as discussed above, is on the order of  $t_S$ , it can also be read as the ratio of  $t_R$  to  $t_S$ . Thus, for example, when  $t_R$  is equal to  $t_S$ , the peak amplitude of the response would be  $\sim 55\%$  saturated.

Our analysis has, for simplicity's sake, ignored the diffusion of  $R^*$  and  $E^*$ . These additional diffusive processes are similar in effect to an increase in  $D_G$  and lead to the reduction of the saturation parameter  $S$ . Yet, since our estimated value of  $S$ , based on Table 1 parameters, is in the

range of 10–100 and thus is much larger than 1, its reduction — even by a factor of 2 or 3 — would not take the system out of the  $S > 1$  regime analyzed above. Note also that in the regime corresponding to this condition, the size of the spot and the peak amplitude of effector activity are independent of diffusivity and are determined by the balance of  $k_1$  and  $k_H$ .

### Response fidelity

The output signal of a generic G-protein-coupled enzyme cascade is a change in the level of a soluble second messenger, e.g., a change in cGMP in the case of the retinal rod. The amplitude of the output signal evoked by a single activated receptor depends on how many effector enzymes are activated and how long they stay active. Since the output of an amplified enzymatic cascade is more strongly influenced by changes in upstream events than downstream events, which pass through fewer amplified stages, variations in the amplitude of the output signal would be dominated by noise in the earliest stage of the cascade, i.e., activation of  $G^*$  by  $R^*$ . The trial-to-trial variation in the signal generated by a single molecule of  $R^*$  has only been studied in photoreceptors. This is because the phototransduction cascade is highly amplified and responses evoked by single photon absorptions, i.e., single  $R^*$  responses, can be identified and recorded. Rod single photon responses are robust and remarkably reproducible; their mean amplitude is 4–5 times larger than the standard deviation of the fluctuations in their amplitude (Baylor et al., 1979, 1980, 1984; Rieke and Baylor, 1996, 1998; Whitlock and Lamb, 1999; Field and Rieke, 2002; Hamer et al., 2003). The explanation(s) for this exceptionally low variability has not been fully established, but the trial-to-trial variation in the amplitude of the single photon response is recognized to arise predominantly from randomness in shutting off receptor activity. If receptor shutoff were a single-step process occurring at a certain rate, the fluctuations of the shutoff time  $t_R$  would have Poisson statistics so that the standard deviation of  $t_R$  would be equal to its mean. To suppress noise down to the level observed at the output would require shutoff to be a much less noisy process, which would be the case if it involved multiple steps occurring sequentially with equal rates. If this were the only mechanism for noise suppression in the transduction pathway, 16  $R^*$  shutoff steps would be required for a rod to produce single photon responses with a coefficient of variation,  $Q$  — defined as the ratio of the standard deviation to the mean — of 0.25 as observed (number of steps =  $(1/Q)^2$ ) (Rieke and Baylor, 1998).

Another mechanism that would act to reduce response variability and arises as a natural consequence of the properties of a G-protein-coupled enzyme cascade is spot formation, described above. As illustrated in Fig. 2, the effector response to a single  $R^*$  converges on a stable response profile which ceases to depend on  $R^*$  lifetime. This would reduce the overall variability of the responses by making all the

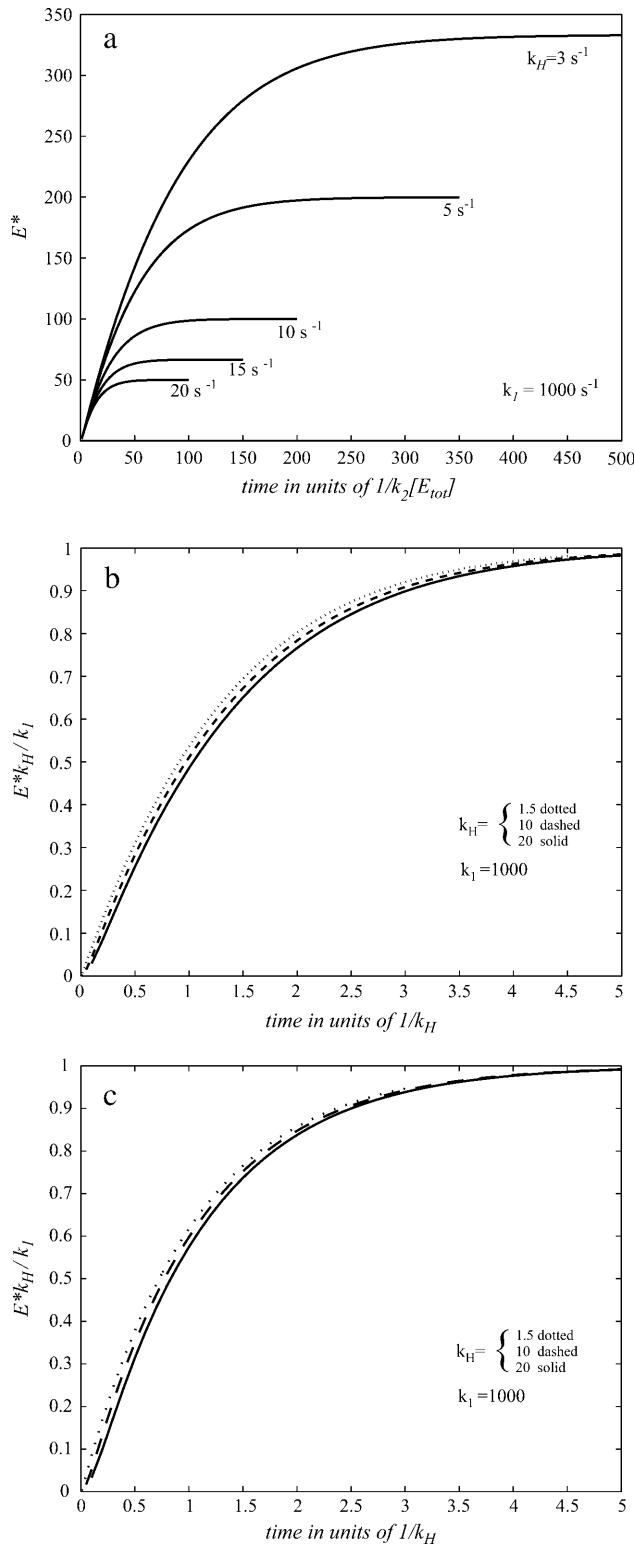


FIGURE 3 (a) Total effector activation as a function of time for a set of different  $k_H$  values and fixed  $k_I = 10^3 \text{ s}^{-1}$  (and other parameters the same as in Fig. 2). Maximal activation and the characteristic time of saturation ( $t_S$  defined as time corresponding to half-maximal activation) both decrease with increasing  $k_H$ . (b) Same as a but with  $E^*$  scaled with  $k_I/k_H$  and time in units of  $1/k_H$ . The fact that they asymptotically approach 1, shows that maximal

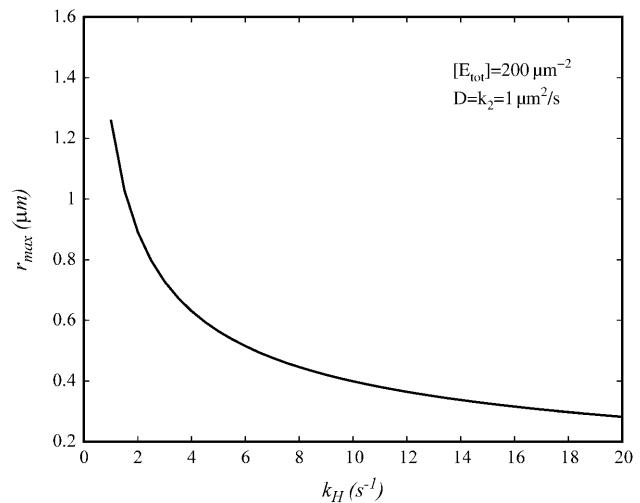


FIGURE 4 Radius of the saturation spot,  $r_{\max}$ , as a function of  $k_H$ , with  $k_I = 10^3 \text{ s}^{-1}$ .

responses evoked by  $R^*$ s that lived longer than a certain time, essentially identical.

In our analysis, response variability was estimated from the dependence of the peak effector response on the shut-off time  $t_R$  (see Fig. 5). The coefficient of variation,  $Q = \sqrt{\langle E_p^{*2} \rangle - \langle E_p^* \rangle^2} / \langle E_p^* \rangle$ , was used to evaluate response variability, where  $E_p^*$  represents the peak effector response. The averaging  $\langle \dots \rangle$  is taken over  $t_R$ , which is governed by the probability distribution of shutoff times,  $P_n(t_R)$ , with the average shutoff time  $\langle t_R \rangle = \tau_R$ ,

$$P_n(t_R) = \frac{t_R^{n-1} (n/\tau_R)^n}{(n-1)!} \exp[-nt_R/\tau_R]. \quad (6)$$

This probability distribution corresponds to deactivation via  $n$  steps with equal rates  $n/\tau_R$  and is a generalization of the simple Poisson distribution of shutoff times ( $n = 1$ ). Fig. 6 plots  $Q$  for the peak effector response as a function of  $\tau_R k_H$  obtained from the numerical solution of Eqs. 1 and 2, as illustrated in Fig. 5. The different curves in Fig. 6 show the decrease in  $Q$ , i.e., the decrease in noise, due to spot formation for  $R^*$  shutoff with different numbers of shutoff steps. The decrease in variability is due to the sublinearity and saturation of the effector response. The quantitative contribution of this effect is evident from comparing  $Q(\tau_R k_H; n)$  with  $Q(0; n)$  which corresponds to the limit where response is directly proportional to on-time  $E_p^* = k_I t_R$ .

activation is equal to  $k_I/k_H$  (as derived in the Appendix). Near-collapse of the curves also shows that the characteristic time of saturation ( $t_S$ ) scales with  $1/k_H$ . Furthermore, to the extent that half-activation occurs at  $t k_H \approx 1$ , we have  $t_S \approx k_H$ . (c) Same as b, but with  $k_I = 10^2 \text{ s}^{-1}$ . Similarity of b and c indicates that the effect of decreasing  $k_I$  is mostly limited to decreasing the total activation level absorbed (in b and c) by rescaling the ordinate ( $E^*$ ) with  $k_I/k_H$ .

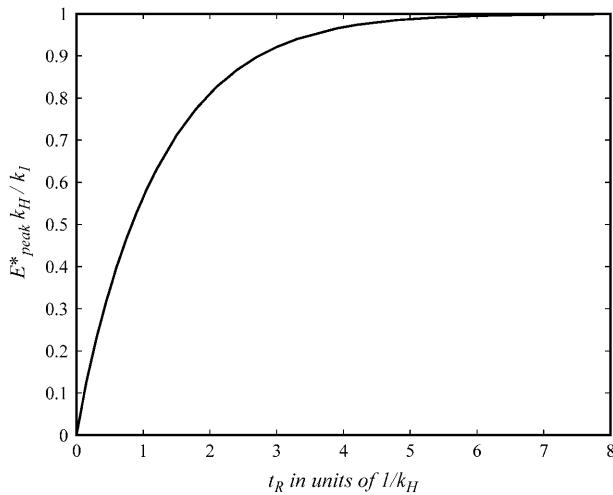


FIGURE 5 Peak effector activation in response to single receptor activity with duration  $t_R$ . The curve is a result of a numerical simulation with the same parameters as in Fig. 2.

## DISCUSSION

G-protein-coupled pathways are designed to couple the activation of a surface membrane receptor to the stimulation of an intracellular effector enzyme. We analyzed the kinetic equations (Eqs. 1 and 2) constituting a simplified model for the enzyme cascade that underlies generic G-protein-coupled signaling focusing on the response to single receptor activation. The results show that the three-step cascade has

two features: 1), localization of effector activation and 2), signal saturation—which arise as a natural consequence of the physical properties of signaling. These features could benefit the signaling process by acting to reduce cross talk and increase response fidelity, respectively.

## Cross talk

Typical mammalian cells have a large number of different G-protein-coupled receptors that converge to control a much smaller population of different effector enzymes. By virtue of this arrangement it is possible for the same type of effector to be stimulated by different surface receptors that respond to different external signals (Birnbaumer, 1990; Gundermann et al., 1996). In addition, the three principal elements in the cascade ( $R$ ,  $G$ , and  $E$ ) are all membrane-associated and diffuse two-dimensionally on its surface. This would be expected to further confuse signal specificity by providing an opportunity for diffusion to drive promiscuous interactions between the three components of the cascade, thus making it harder to use a nonspecific change in effector enzyme activity as a message about the detection of a specific external signal. Despite these expected signaling problems, it is well documented that G-protein-coupled signaling pathways are commonly used to produce selective cellular responses to specific stimuli (Gilman, 1987). This shows that there are cell mechanisms to increase signal specificity. One well-recognized mechanism that biology uses to limit the confusion due to cross talk is to physically contain the elements of a cascade that are coupled to a specific receptor. This is done either by fencing them in (by forming a molecular corral made of distinct lipid and protein elements; Okamoto et al., 1998; Fagan et al., 2000; Steinberg and Brunton, 2001) or by tying them up (with scaffolding proteins to tether the components together into a multimolecular transduction complex; Steinberg and Brunton, 2001; Colledge and Scott, 1999; Brady and Limbird, 2002; Albert and Robillard, 2002).

Our analysis shows that in addition to these molecular mechanisms for physical containment, the spatial spread of the effector response of a generic  $G$ -protein cascade is self-limiting and naturally forms a restricted signaling domain in the vicinity of the activated membrane receptor. The properties of the localization domain depend essentially on the ratio of the rate of  $G^*$  production,  $k_1$ , to the rate of  $E^*$  inactivation,  $k_H$ , which enters the saturation parameter  $S$  (defined by Eq. 4). Saturation parameter  $S$  controls the crossover to the saturated spot response, where a local domain of activated effector forms with an area increasing with the time that the receptor has been active until saturating at the maximal radius  $r_{max}$  (given by Eq. 5). Using photoreceptor parameters we estimate the maximum radius of the signaling domain to be  $\sim 1 \mu\text{m}$ . We note that the size of the signaling domain and the maximal signal amplitude can be controlled by  $k_1$  and  $k_H$  parameters and hence by

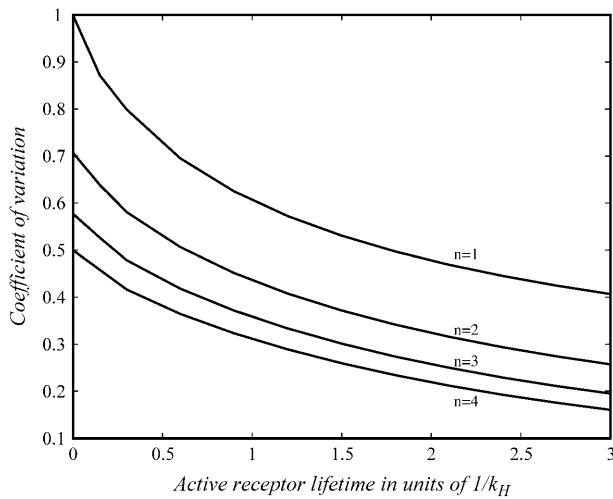


FIGURE 6 Coefficient of variation (ratio of standard deviation to the mean) for peak response as a function of  $t_R$ . Averages are taken in the ensemble of responses with random shutoff times governed by  $n = 1, 2, 3, 4$  step Poisson processes with the average shutoff time given by  $\tau_R$ . Note that with  $\tau_R k_H$  value of, say, 1.5, there is a significant reduction of the coefficient of variation (denoted by  $Q$  in the text) even for  $n = 2$ . This reduction occurs because the sublinear behavior of the peak response, as a function of the shutoff time ( $t_R$ ) (see Fig. 5), reduces the contribution of the events with late receptor shutoff times to the trial-to-trial variability of the responses.

controlling, respectively, the G-protein concentration and the concentration (or activity) of the RGS proteins (Berman and Gilman, 1998; He et al., 1998; Makino et al., 1999; Arshavsky et al., 2002), which modulate the GTPase activity of  $G^*$  to influence  $k_H$ . These regulatory knobs could provide cells with a mechanism for adapting their response to the stimulus. In any case, to the extent that local signaling domains can reduce cross talk, our analysis shows that cross-talk suppression is an intrinsic feature of the G-protein-coupled enzyme cascade.

### Response fidelity

The effector activation process results in a sublinear, saturating dependence of peak effector activity on the on-time of a single  $R^*$  so that for long on-times the response becomes independent of the duration of  $R^*$  activity. This acts to decrease the fluctuations in peak amplitude that would normally arise from random variation in the shutoff time ( $t_R$ ) of  $R^*$ s and thus serves to increase signal fidelity. This effect, which we have referred to as *spot formation*, may be a contributing factor in the remarkable reproducibility of the single photon response.

Its influence on the trial-to-trial variability of single  $R^*$  responses, as measured by the coefficient of variation of the responses, is shown in Fig. 6 for different values of the  $\tau_R$ . The coefficient of variation of rod single photon responses is  $\sim 0.25$  (Baylor et al., 1979; Rieke and Baylor, 1998; Whitlock and Lamb, 1999; Hamer et al., 2003). Fig. 6 shows that this level of reproducibility can be achieved if the  $\tau_R k_H$  is sufficiently large and that the value required for a given  $Q$  decreases with increasing number of  $R^*$  deactivation steps,  $n$ . Thus for  $n = 4$ , we find that  $Q = 0.25$  can be obtained for  $\tau_R k_H \approx 2$ . On the other hand, looking at Fig. 5 we note that for  $\tau_R$  this large, typical responses—ones with  $t_R \approx \tau_R$ —would have peak response within  $\sim 20\%$  of saturation. A somewhat shorter lifetime, such that  $\tau_R k_H = 1.5$ , would keep the average response further from saturation, yet decrease  $Q$  to 0.6 for  $n = 1$  and to 0.3 for  $n = 4$ .

In a previous study Rieke and Baylor (1998) considered the possibility that response saturation suppresses variability and plays a role in the reproducibility of single photon responses. They dismissed this idea, however, by arguing that responses were not saturated because an experimental manipulation that prolonged the lifetime of  $R^*$ , i.e., increased  $\tau_R$ , also increased the peak amplitude of the response. Our results are in fact consistent with this observation, since we see in Fig. 5 that the peak response corresponding to  $\tau_R k_H = 1.5$  is well below saturation. The reduction of variability that we are talking about comes from a more subtle effect than outright total effector saturation. The crossover to saturation as a function of the shutoff time selectively suppresses the peaks of the responses evoked by  $R^*$  activation events with long on-times. These are the events that correspond to the tail of the  $t_R$  distribution,  $P(t_R)$ , when  $t_R > \tau_R$ . Thus the variability

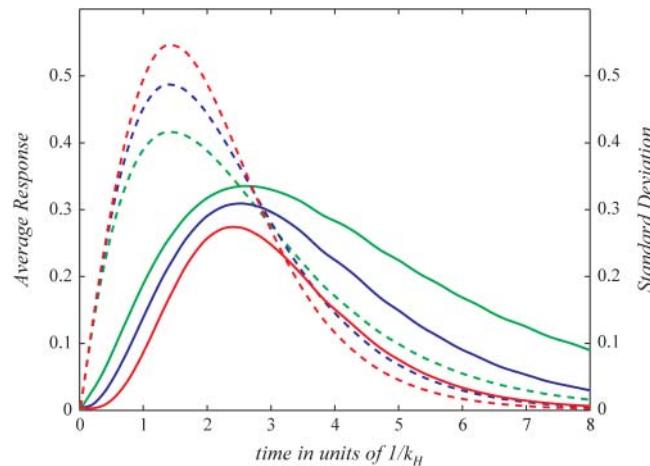
can be suppressed even while the typical events with  $t_R \approx \tau_R$  are relatively unaffected by saturation.

To further evaluate our analysis with respect to the observed statistical properties of rod single photon responses (Whitlock and Lamb, 1999; Field and Rieke, 2002), we consider a time-resolved measure of response variability. Fig. 7 compares the time courses of the average response with the trial-to-trial standard deviation of the response all computed numerically in ensembles of simulated responses to receptor activation events with  $P_n(t_R)$  distribution of shutoff times and  $\tau_R k_H = 1.5$ . The results show that the peak of  $Q(t)$  lags behind the peak of the mean response, consistent with the results of Field and Rieke (2002).

We conclude, although we cannot prove here, that the spot-formation mechanism contributes to the high fidelity of single photon responses in rod cells. We have demonstrated that: 1), suppression of response variability is a natural consequence of the G-protein-mediated signaling cascade and 2), the proposed mechanism is not inconsistent with experimental observations of single photon response variability. Finally, we note that reduction of the coefficient of variation down to 0.25 is likely to be a multifactorial phenomenon with the abovementioned mechanism being one of several components.

### APPENDIX: LOCALIZATION OF G-PROTEIN SIGNALING

In this Appendix we present the details of the calculations of the  $E^*$  spot formation by analyzing Eqs. 1 and 2.  $[G^*]$  and  $[E^*]$  are, respectively, the areal density of activated G-proteins and of activated effector, whereas  $[E] = [E_{\text{tot}}] - [E^*]$  is the areal density of inactive or free effector. We are interested in the effect of a single activated receptor molecule, which we assume to be at the origin of our coordinate system,  $r = 0$ , and to stay active



**FIGURE 7** The time course of the trial-to-trial standard deviation (solid line) of the responses is compared to the time course of the average response (dashed line). Based on the same numerical simulation as Fig. 6 with  $\tau_R k_H = 1.5$ . Red, blue, and green curves correspond respectively to  $n = 1, 2, 4$  shutoff steps. Note that the peak of standard deviation is delayed relative to the peak of the average response.

for time  $t$ ,  $0 < t < t_R$ . Then active receptor areal density  $[R^*] = \delta^{(2)}(r)\theta(t_R - t)\theta(t)$  where  $\delta^{(2)}(r)$  denotes a two-dimensional Dirac delta function and function  $\theta(t) = 1$  for  $t \geq 0$  and equal to 0 for  $t < 0$ . In our further analysis, for the sake of simplicity we neglect the diffusion of  $E$ , since it does not qualitatively change the results. To produce full time-dependent solutions, equations were integrated numerically in MatLab (The MathWorks, Natick, MA).

Axially symmetric solutions are conveniently described in polar coordinates. To deal with the diffusion term, the solution was sought as a linear superposition of Bessel functions  $J_0(\beta_m r)$  (Abramowitz and Stegun, 1965) where  $\beta_m$  forms the root of  $J_0(z)$ :

$$G^*(r, t) = \sum_m a_m(t) J_0(\beta_m r), E(r, t) = \sum_m b_m(t) J_0(\beta_m r).$$

Since Bessel functions are the eigen-functions of the Laplacian  $\nabla^2 J_0(\beta r) = -\beta^2 J_0(\beta r)$ , the partial differential equations (Eqs. 1 and 2) in the Bessel basis (i.e., in terms of  $a_m$  and  $b_m$ ) reduce to a system of ordinary differential equations which are integrated numerically using an Adams-Basforth (Stoer and Bulirsch, 1992) method with the linear terms of Eq. 1 advanced in time using an implicit scheme (Stoer and Bulirsch, 1992). The nonlinear ( $k_2$  term) is evaluated at the preceding time step by going back to  $r$ -space, i.e., by recomputing  $G^*(r, t)$  and  $E(r, t)$ . Keeping 200 Bessel modes will provide sufficient convergence and allow rapid integration in MatLab.

Let us consider the stationary state, which can be reached in the absence of receptor deactivation:

$$\begin{aligned} k_1 \delta^{(2)}(r) - k_2 [E][G^*] + D_G \nabla^2 [G^*] &= 0, \\ k_2 [E][G^*] - k_H [E^*] + D_E \nabla^2 [E^*] &= 0. \end{aligned}$$

Eliminating the  $k_2 [E][G^*]$  term and integrating the resulting equation over space removes the diffusion terms and yields an exact expression for the maximal number of activated  $E^*$  molecules in a saturated spot:  $k_1/k_H$ .

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