

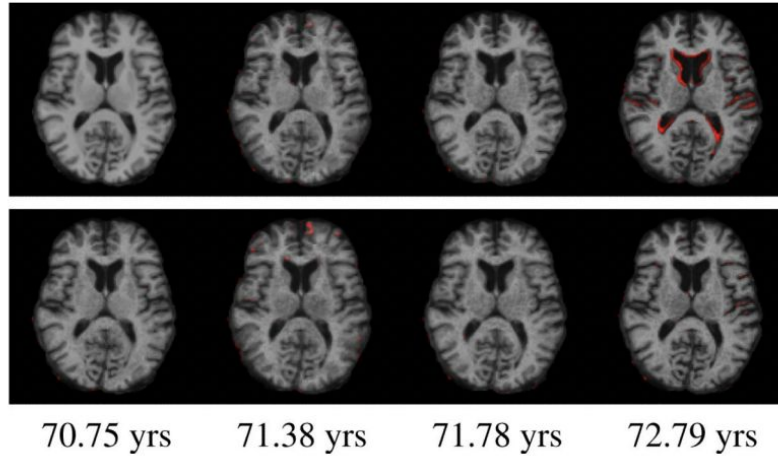
# Non-parametric Manifold Regression

Population Shape Regression from Random Design Data

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Presentation by Alexandre Cahill and Vincent Herfeld

# Initial Problem : Longitudinal study



*Brain MR Images templates*

# Statistical Method Overview

- Nadiya -Watson Manifold extension of Frechet Mean

$$\hat{I} = \arg \min_{I \in \mathcal{I}} \frac{\sum_{i=1}^N d_{\mathcal{I}}(I, y_i)^2}{N} \quad \longrightarrow \quad \hat{I}_h(t) = \arg \min_{I \in \mathcal{I}} \frac{\sum_{i=1}^N K_h(t - t_i) d_{\mathcal{I}}(I, y_i)^2}{\sum_{i=1}^N K_h(t - t_i)}$$

# Geometric Grounding : LDDMM

Shape Space :

- Manifold : Group action of Diffeomorphisms on the Space of Images
- Local Metric : Defined through kernel  $k$  on vector fields of a RKHS  $V$
- Computing geodesic distances :

$$Cost(\phi) = Length(\phi) + \lambda Fidelity(\phi(M_1), M_2)$$

$$d_{\mathcal{I}}(I, J)^2 = \min_{v: \dot{\phi}_t = v_t(\phi_t)} \int_0^1 \|v_t\|_V^2 dt + \frac{\|I(\phi^{-1}) - J\|_{L_2}^2}{\sigma^2}$$

# Method

## Single subject growth model

$$\min_{v: \dot{\phi}_t = v_t(\phi_t)} \int_0^1 \|v_t\|_V^2 dt + \frac{1}{\sigma^2} \int_0^1 \|I_\alpha(\phi^{-1}) - I_t\|_{L_2}^2 dt$$

$$Av_t = -\frac{1}{\sigma^2} \nabla(I_\alpha \circ \phi^{-1}) \int_t^1 (I_u(\phi_u \circ \phi_t) - I_\alpha(\phi^{-1})) |D(\phi_u \circ \phi_t^{-1})| du$$

## Population growth model

$$\min_{v: \dot{\phi}_t = v_t(\phi_t)} \int_0^1 \|v_t\|_V^2 dt + \frac{1}{\sigma^2} \int_0^1 \|I_\alpha(\phi^{-1}) - \hat{I}_t\|_{L_2}^2 dt$$

$$\hat{I}_h(t) = \arg \min_{I \in \mathcal{I}} \frac{\sum_{i=1}^N K_h(t - t_i) d_{\mathcal{I}}(I, y_i)^2}{\sum_{i=1}^N K_h(t - t_i)}$$

# Implementation

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**Algorithm 4.1** Intrinsic mean image: LDDMM solution

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**Input:** A collection of  $N$  images:  $\{I^i\}_{i=1}^N$

**Output:** A Fréchet mean image  $\hat{I}$  and a collection of diffeomorphic transformations  $\{\phi^i\}_{i=1}^N$  such that  $\phi^i$  maps  $I^i$  onto  $\hat{I}$

```
1: // Initialize deformations with identity
2: for  $i = 1 : N$  do
3:    $\phi^i \leftarrow \text{Id}_{\text{Diff}_V(\Omega)}$ 
4: end for
5: // Perform gradient descent optimization
6: repeat
7:    $\hat{I} = \frac{1}{N} \sum_{i=1}^N I_{\phi^i}^i$  // Update mean image
8:   for  $i = 1 : N$  do
9:     // Compute gradient of functional at each discretized timepoint  $s$ 
10:    for  $j = 1 : T$  do
11:       $s \leftarrow \frac{j-1}{T}$ 
12:       $\nabla_{v_t^i} E_t \leftarrow 2v_t^i - K \left( \frac{2}{\sigma_2} |D\phi_{s,1}^i| |\nabla I_{\phi_{0,s}^i}^i| (I_{\phi_{0,s}^i}^i - \hat{I}_{\phi_{1,s}^i}^i) \right)$ 
13:    end for
14:     $v^i \leftarrow v^i - \epsilon \nabla_{v^i} E$  // Step along gradient
15:  end for
16: until convergence
```

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*LDDMM algorithm to solve regression on 2D images*

# Implementation

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**Algorithm 4.2** Intrinsic mean image: Greedy solution

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**Input:** A collection of  $N$  images:  $\{I^i\}_{i=1}^N$

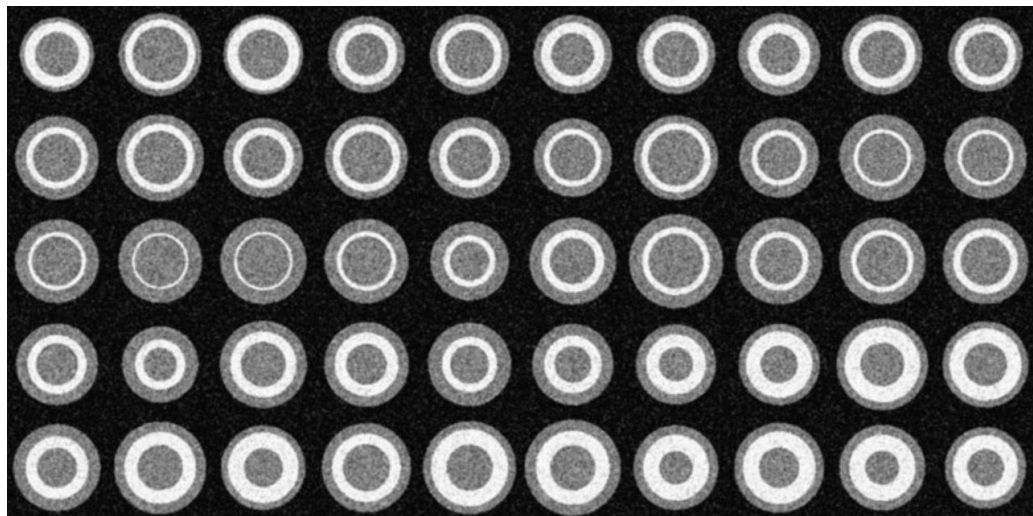
**Output:** A Fréchet mean image  $\hat{I}$  and a collection of diffeomorphic transformations  $\{\phi^i\}_{i=1}^N$  such that  $\phi^i$  maps  $I^i$  onto  $\hat{I}$

```
1: // Initialize deformations with identity
2: for  $i = 1$  : number of images do
3:    $\phi^i \leftarrow \text{Id}_{\text{Diff}_V(\Omega)}$ 
4: end for
5: repeat
6:    $\hat{I} = \frac{1}{M} \sum_{i=1}^M I_{\phi^i}^i$  // Update mean image
7:   for  $i = 1$  : number of images do
8:      $v_{\text{inc}} \leftarrow K \left( \frac{2}{\sigma^2} \nabla I_{\phi_{0,1}^i}^i (I_{\phi_{0,1}^i}^i - \hat{I}) \right)$  // Compute locally optimal velocity
9:      $\phi^i \leftarrow \text{Exp}_{\phi^i}(\epsilon v_{\text{inc}})$  // Step in direction of incremental velocity
10:  end for
11: until convergence
```

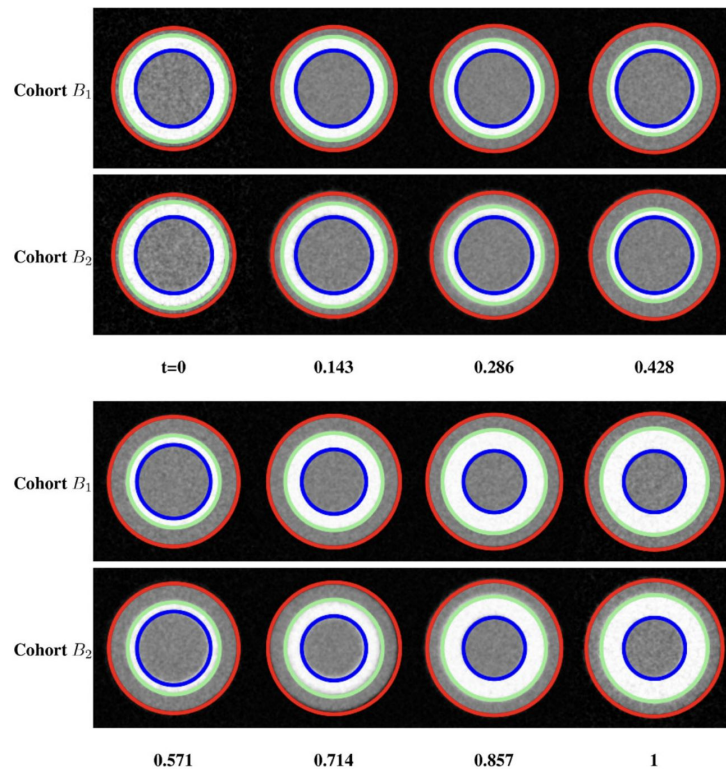
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*Greedy algorithm to solve regression on 3D images*

# Results



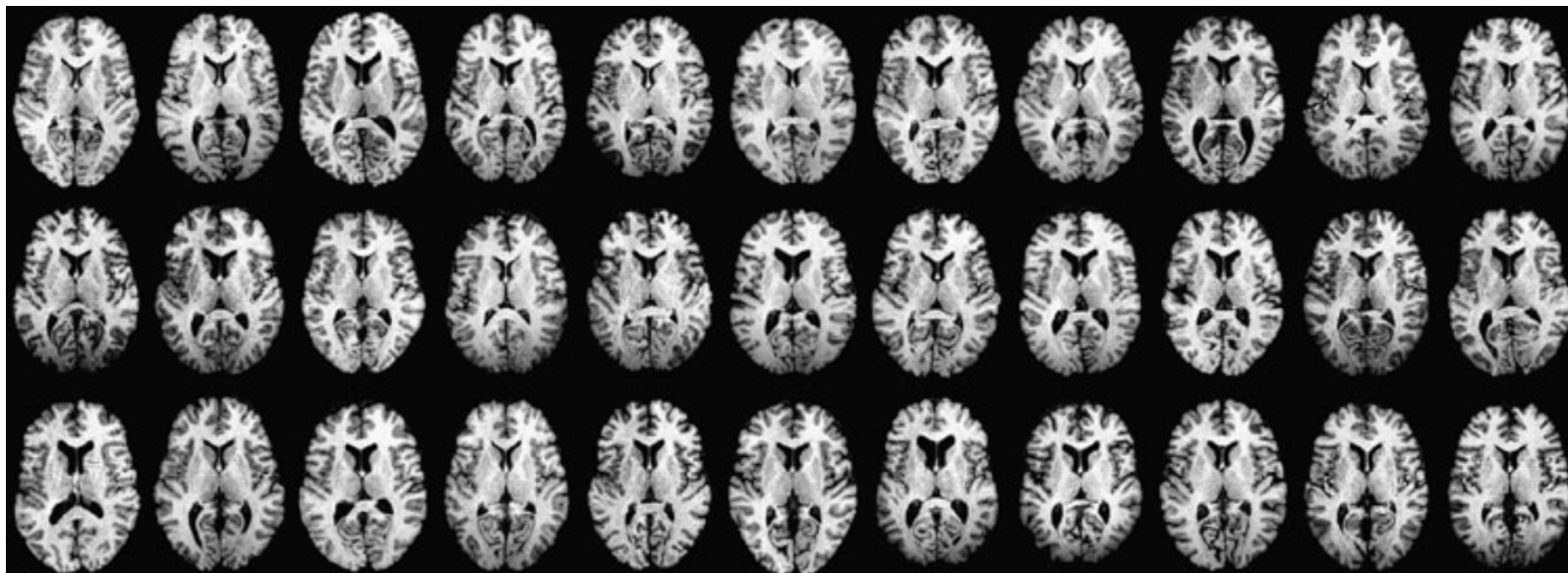
*Synthesised images of bull's-eyes as observation data*



*Regressed images*

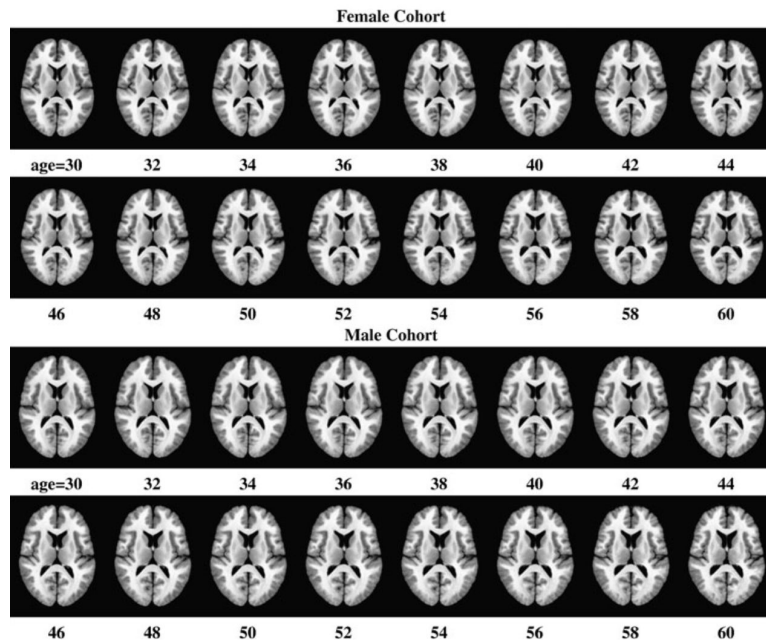


# Results



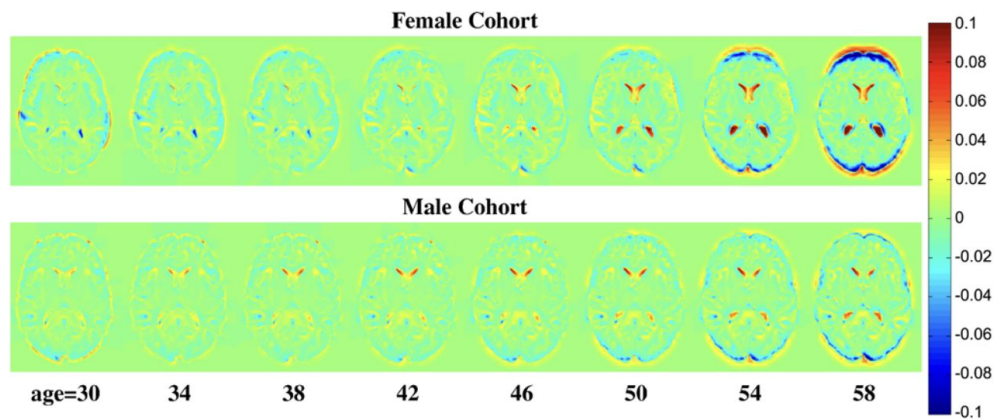
*Healthy brain MRIs data set*

# Results



*Slices of regressed 3D images*

$$\log \begin{vmatrix} \frac{\partial \dot{g}_t^1}{\partial x^1}(x) & \frac{\partial \dot{g}_t^1}{\partial x^2}(x) & \frac{\partial \dot{g}_t^1}{\partial x^3}(x) \\ \frac{\partial \dot{g}_t^2}{\partial x^1}(x) & \frac{\partial \dot{g}_t^2}{\partial x^2}(x) & \frac{\partial \dot{g}_t^2}{\partial x^3}(x) \\ \frac{\partial \dot{g}_t^3}{\partial x^1}(x) & \frac{\partial \dot{g}_t^3}{\partial x^2}(x) & \frac{\partial \dot{g}_t^3}{\partial x^3}(x) \end{vmatrix}$$



*Age-indexed local expansion and contraction*

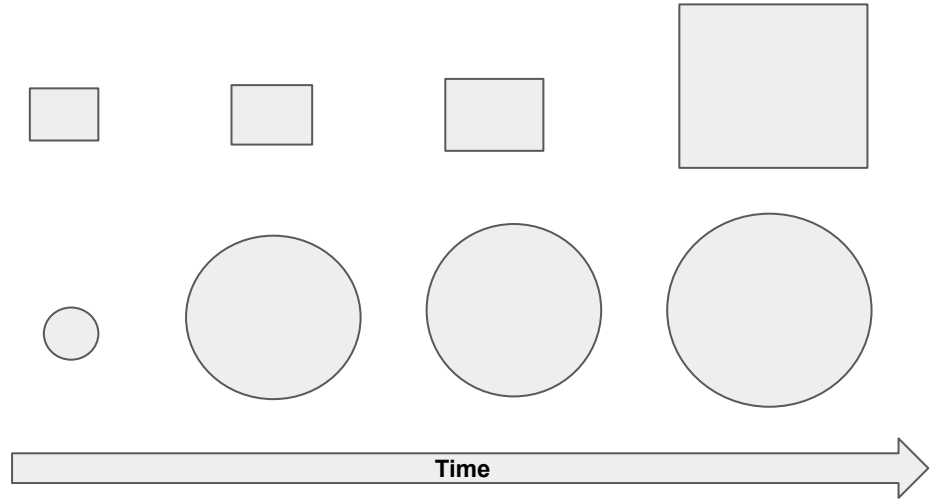
*Red : expansion    Blue : contraction*

# Statistical Limitations

1. No Subject-Specific information:

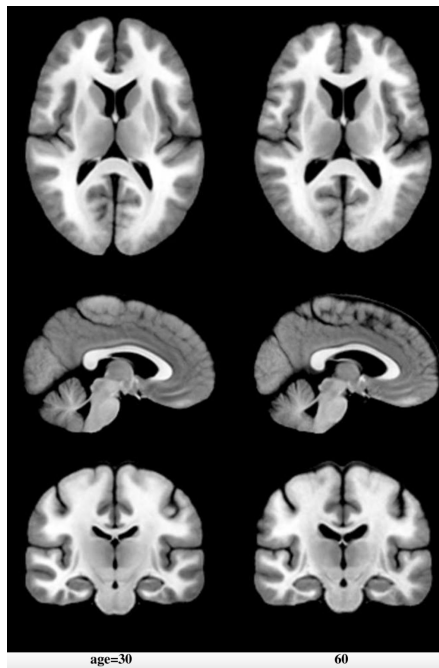
=> Loss of Information

2. Time deformation :

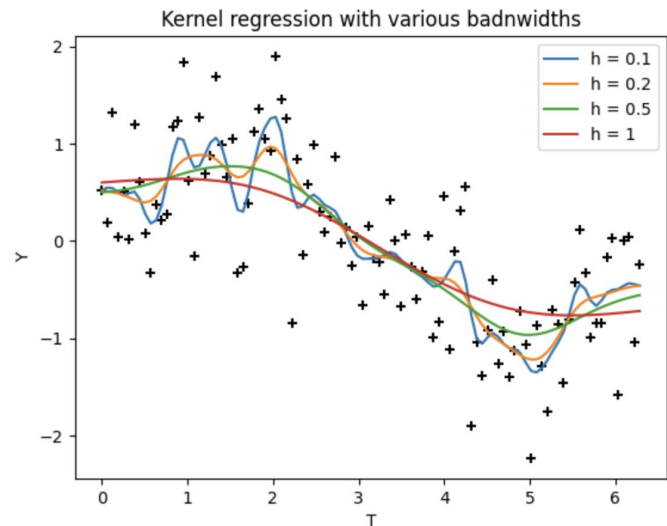


*Schematic Growth Scenarios*

# Computational Limitations



*Regressed images of mixed cohorts*



Finding best kernel bandwidth can be complicated and/or subjective.

≈ 2 hours of computation time / regressed image

$O(MN \log n)$  M iterations,  
N images

n voxels along largest dimension

## Sources :

Images where taken from the article and Brad C. Davis's thesis