

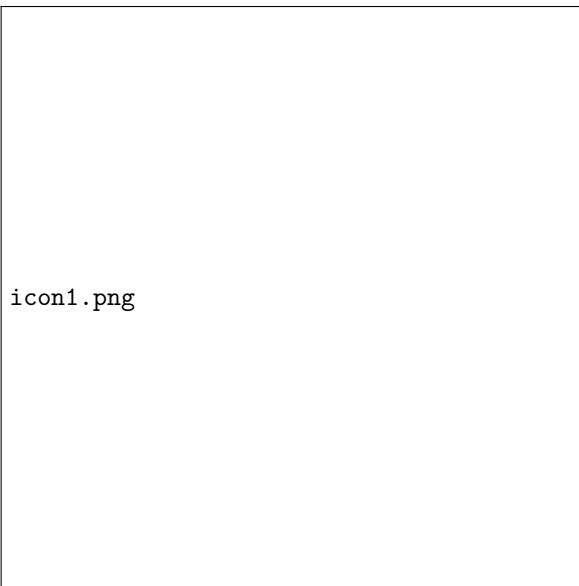
# Assignment4

## *Source localization*

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Biomedical Data Processing, Part II Course



# 1 Introduction

Brain is a network of  $10^{10}$  neurons. Each neuron could generate a small electrical activity which alone could not be picked up from the electrodes. This is due to the interference of other surrounding activities. In case of a big number of neurons simultaneously active, the outcome signal is sufficiently high to be picked from the scalp electrodes. This electrical activity could be modeled as a dipole. Brain electrical activity has been investigated via surface electrodes since 1930. Widely known as electroencephalogram (EEG) is the potential difference of electrodes in a time course. This readings has facilitated the diagnoses of many neurological diseases.

In simulation setup, dipole modeling could enable the generation of electrode potential via the solution of Poisson equation and Neuman boundary conditions. This is also known as the forward problem. Additionally, potential given the electrode, the underlying dipole localization and direction could also be estimated via different optimization setups. This is also known to be the inverse problem where the final outcome is source localization [?].

## 2 Forward problem

### 2.1 Theory

#### 2.1.1 Poisson's equation

Poisson's equations computes the potentials distribution in a volume conductor given the applied current source. The current density  $J(x, y, z)\{\frac{A}{m^2}\}$  is a vector field whereas its divergence defines the current source density  $I_m = \nabla J\{\frac{A}{m^3}\}$ . In case of a enclosed volume  $r_1(x_1, y_1, z_1)$  by current sink of positively charge represent the removal of positive ions. This yield a singularity current source density  $-I\delta(r - r_1)$ . A small volume around the current source  $r_2(x_2, y_2, z_2)$  is also constructed. Injection of positively charge ions into this volume is also another singular current source density  $I\delta(r - r_2)$ . Superposition of this cases outcome:

$$\nabla J = I\delta(r - r_2) - I\delta(r - r_1) \quad (2.1.1)$$

As regard to the current density  $J$  and the electrical field  $E$  Ohm's law gives the relation via:

$$J = E\sigma \quad (2.1.2)$$

where  $\sigma(r)$  is rank-1 tensor representation of the anisotropic conductivity which varies with the direction. Under the Faraday's law in quasi-static conditions ( $\nabla \times E = 0$ ) a relation between the electrical field and scalar potential field is given via gradient operation:

$$E = -\nabla V \quad (2.1.3)$$

The direction of  $\nabla V$  represents the most rapid increase of the potential  $V$  at a give point. It sign minus is based on the orientation flow from high to low potential. Poisson equation is obtained via combination of equations ??, ?? and ??.

$$\nabla(\sigma\nabla(V)) = -I_m = I\delta(r - r_2) - I\delta(r - r_1) \quad (2.1.4)$$

#### 2.1.2 Boundary conditions

Inability to diminish charge particles at the compartments interface is seen as the current leaving one region is equal to the current entering another region. Additionally the very low conductivity of the human head does not permit any charge to penetrate the head. These two conditions presented by Neuman are equationed below:

$$J_1 e_n = J_2 e_n \quad (2.1.5) \qquad J_1 e_n = 0 \quad (2.1.6)$$

#### 2.1.3 The current dipole

The current source and sink remove the same amount of charges  $I$  consequently dipole modeling is the best approach. Its momentum  $d$  is defined via  $d = I * p * e_d$  where  $\|d\| = \|I * p * e_d\|$  and  $e_d$  the orientation. Orthogonal projection of these dipole onto Cartesian axes is  $d = d_x e_x + d_y e_y + d_z e_z$ . Due to the linearity of Poisson equation it could be decomposed into:

$$V(r, r_{dip}, d) = d_x V(r, r_{dip}, e_x) + d_y V(r, r_{dip}, e_y) + d_z V(r, r_{dip}, e_z) \quad (2.1.7)$$

#### 2.1.4 Solution of the forward problem

Solution of the equation ?? with gives the scalp potential at an electrode due to a singular dipole with momentum  $d$ . A current dipole with momentum  $d = de_d$  positioned at  $r_{dip}$  in an infinite conductor with conductivity  $\sigma_i$  produces a potential field at distance  $r$  as:

$$V(r, r_{dip}, d) = \frac{d(r - r_{dip})}{2\pi\sigma\|r - r_{dip}\|^3} \quad (2.1.8)$$

which is also outlined in figure ?? The easiest model to solve the Poisson equation for a head model is a the spherical head model which is fast and easy to be implemented. More sophisticated approaches are Boundary Element Method (BEM), Finite Element Method (FEM) and Finite Difference Method (FDM) which are generally employed for realistic shape instead of spherical which is not realistic. Due to the difference in conductivity of skull from scalp and brain a three shell concentric spherical head has to been proposed for spherical head model. Semi-analytic solution for Poisson equation utilizing the proposed geometrical modelling is:

$$V = \frac{1}{4\pi SR^2} \sum_{i=1}^{\infty} \frac{X(2i+1)^3}{g_i(i+1)i} b^{i-1} \{id_r P_i(\cos\theta) + id_r P_i(\cos\theta)\} \quad (2.1.9)$$

given that:

$$g_i = \{(i+1)X + i\} \left\{ \frac{iX}{i+1} + 1 \right\} + (1-X) \{(i+1)X + i\} (f_1^{i_1} - f_2^{i_1}) - i(1-X)^2 \left\{ \frac{f_1}{f_2} \right\}^2 \quad (2.1.10)$$

where:

- $d_r$  is the radial component
- $d_t$  is the tangential component
- $R$  is the radius of the outer shell
- $S$  is the conductivity of the scalp and brain tissue
- $X$  is the ratio between the skull and soft tissue conductivity
- $b$  is the relative distance of the dipole from the center
- $\phi$  is the polar angle of the surface point
- $P_i(\cdot)$  is the Legendre polynomial
- $P_i^1(\cdot)$  is the associated Legendre polynomial
- $i$  is an index
- $i_1 = 2 * i + 1$
- $r_1$  is the radius of the inner shell
- $r_2$  is the radius of the middle shell
- $f_1 = \frac{r_1}{R}$
- $f_2 = \frac{r_2}{R}$

This is the equation for scalp potentials produced from an dipole located in the z axis. In case of an of an arbitrary dipole, Euler angles are employed for the rotation of the coordinate system accordingly.

## 2.2 EEG montage

Electrode placement is of great importance to display the EEG adequately. There is a big diversity of EEG montage which in same cases it should be adopted for specific applications. The most accepted model is 10/20 for classical EEG recording. There are symmetric placement between Nasion-Inion marked as Frontal pole ( $F_p$ ), Central (C), Parietal (P), occipital (O) and Temporal T. The electrodes named with zero (Z) are the ones corresponding at the central line. The odd numbers are used for points on the left hemisphere whereas the even number for points on the right of the hemisphere. There is a symmetry of the node placement respectively to the Nasion-Ion line ??.

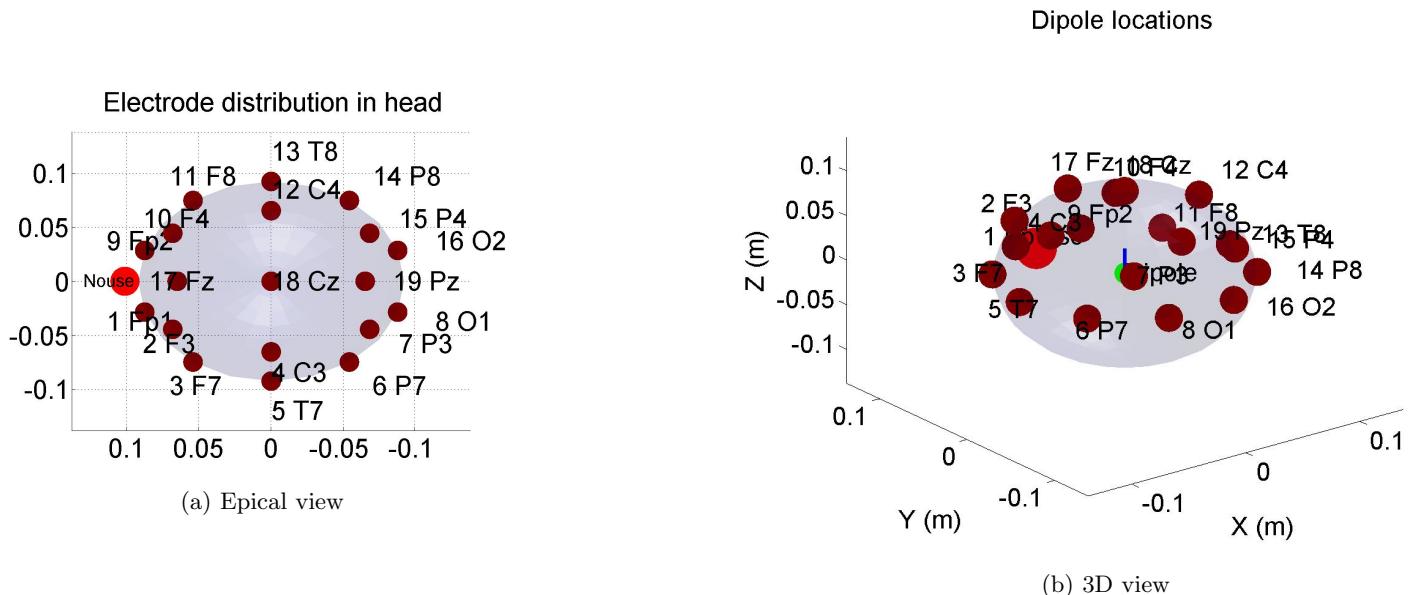


Figure 2.2.1: EEG montage for the simulation model

In figure ?? is the spherical model which will be used as well as the electrode placement as the most standard configuration. The spherical model we are using consist o a three shell model figure ?? with respective radius:

- $R_{skull} = 0.08[m]$
- $R_{scalp} = 0.086[m]$
- $R_{brain} = 0.092[m]$

### 2.3 Dipole location

The modeled dipole has two main parameters position and direction which are encoded into Cartesian coordinates. In figure ?? a simple dipole location at the center which is oriented towards z axis. This is acquired via command line *Show – Dipole – Placement([0, 0, 0, 0, 0, 1], hm, 4)* where *Show – Dipole – Placement([ $x_p, y_p, z_p, Ori_x, Ori_y, Ori_z$ ], Head – Model, NrFigure)*. In case it would be necessary to place an dipole half way from the center towards the right ear oriented towards z axis figure ?? that would be possible via command *Show – Dipole – Placement([0.05, 0, 0, 0, 0, 1], hm, 5)*.

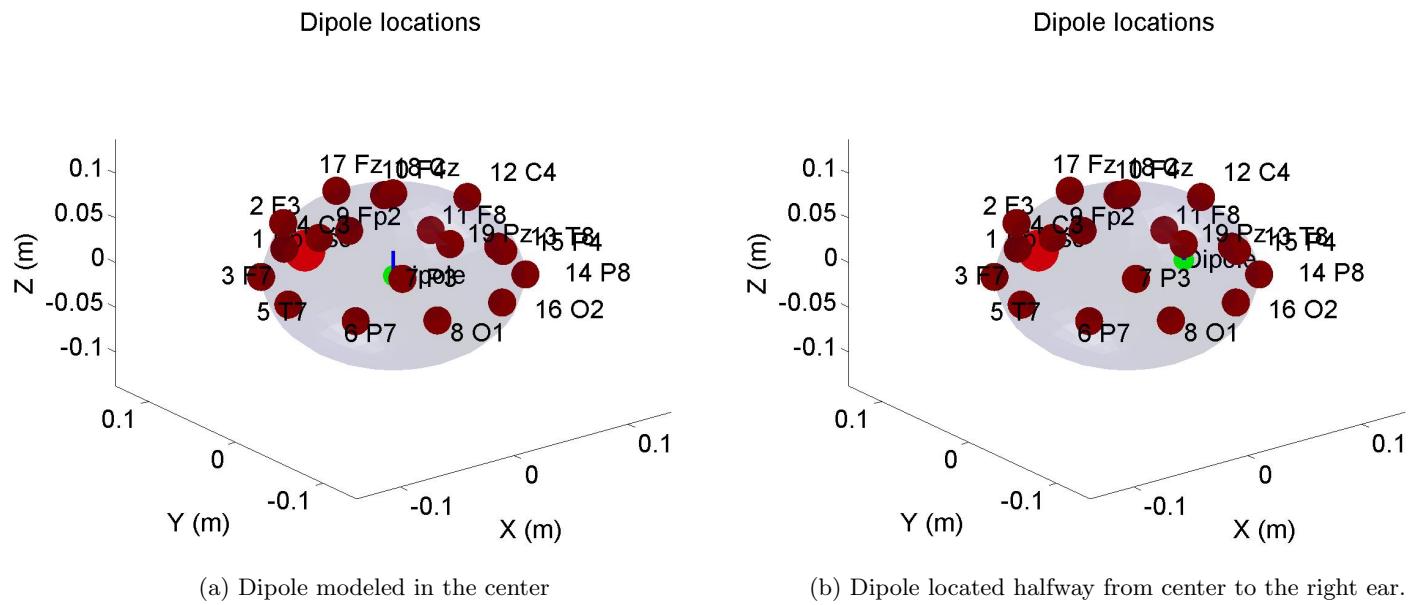


Figure 2.3.1: Dipole locations

#### 2.3.1 Potential computation

Spherical head model has been utilized to solve the Poisson equations and provides the potential distribution at particular coordinate due a dipole at particular direction and position. In case there will be a dipole located in the center oriented towards the  $x$  position the potential field distribution will be as in the figure ???. Since the dipole is not positioned along the  $z$  axis from [?] are all the necessary transformation needed to for the coordinates rotation which are also outlined in Appendix ???. The generalization of equation ?? for any dipole location can be written as:

$$V_x = T_x D_x \quad (2.3.1)$$

$$V_y = T_y D_y \quad (2.3.2)$$

$$V_z = T_z D_z \quad (2.3.3)$$

Figure 2.3.2: Voltage computation

whereas the potential  $V$  at  $R_2$  due to dipole  $D$  located at  $R_1$  is:  $V = V_x + V_y + V_z$ . Regarding the electrode potential values the plot in figure ?? outline individual values. The dipole location and orientation is plotted in figure ???. The potential field is therefore mostly oriented towards the right ear in the figure ?? which coincides with the orientation of the dipole inside the head.

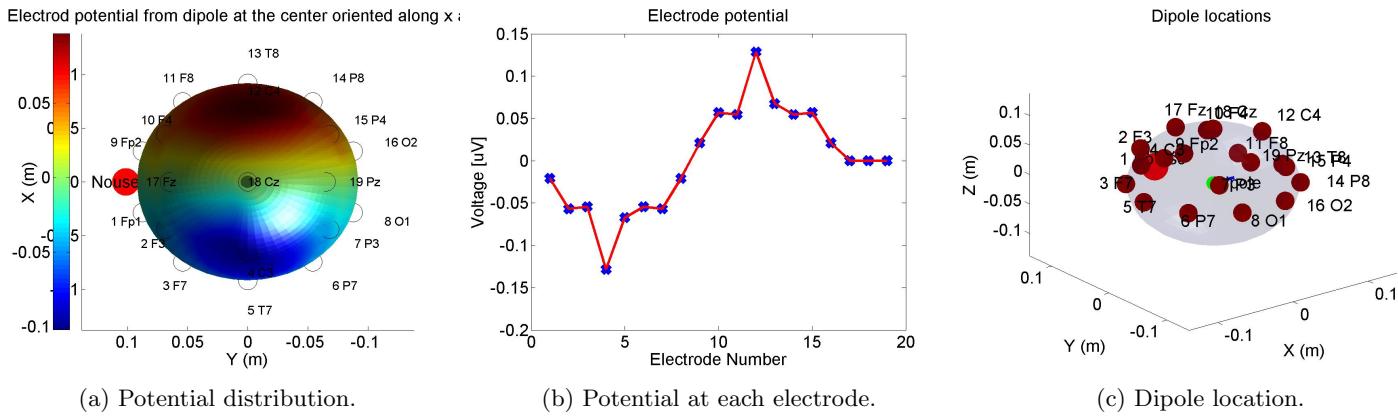


Figure 2.3.3: Potential distribution

## 2.4 Lead Field Matrix

The lead field matrix contains the potential intensity computed from the spherical model, oriented along x, y and z axis. The final potential distribution corresponding to the a particular dipole orientation is the superposition of each lead field matrix along each axis, whereby their contribution is proportional to the orientation of the dipole. In figure ?? are the potential distribution of each component where it is clearly noted maximum along X,Y and Z axis.

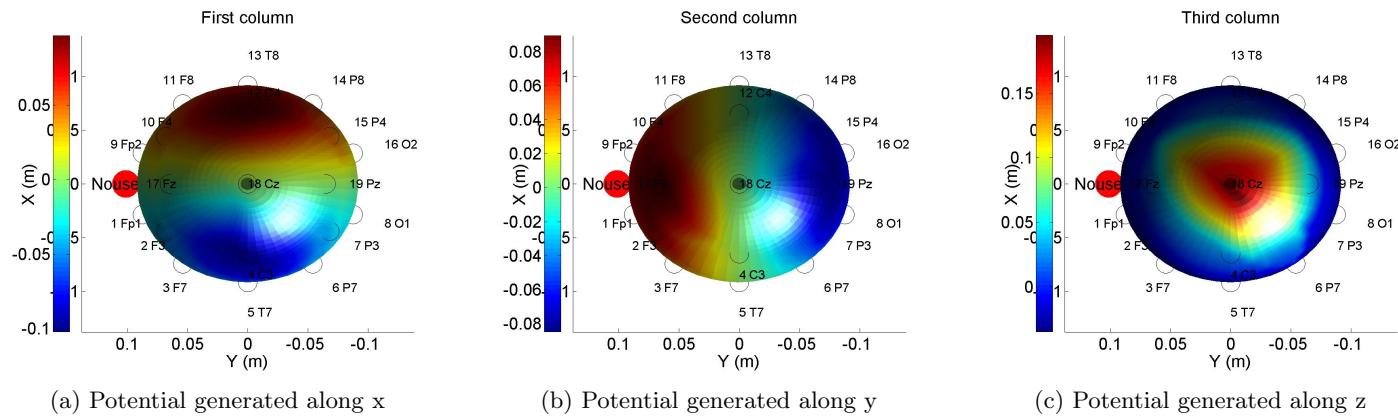
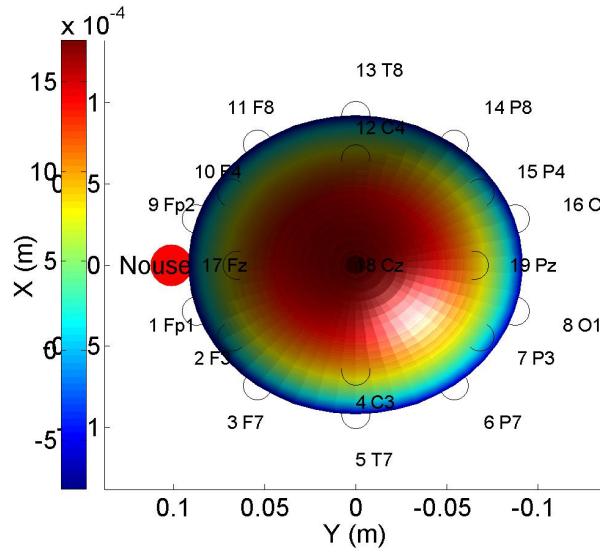


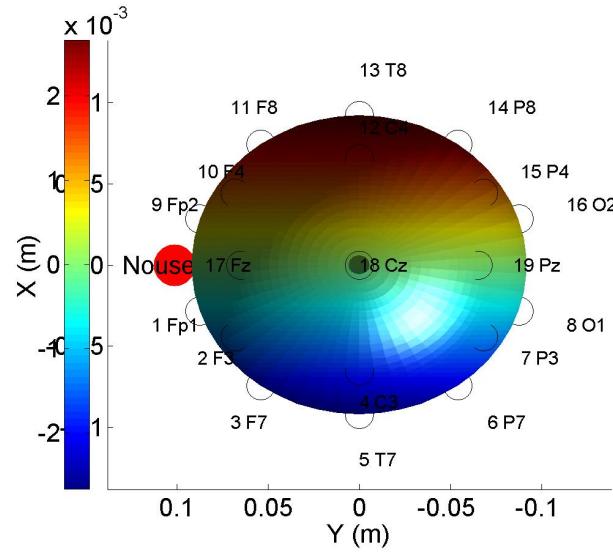
Figure 2.4.1: Lead field matrix

## 2.5 Linearity of Maxwell equation

The numerical version of the Maxwell equation is linear therefore the principle of superposition is applied. Therefore in this case, the potential produced from the dipole D1 and D2 located at the center where the first one oriented along  $x$  ?? and the second one along  $z$  in figure ?? produces the potentials in figure ?? and figure ???. Due to the linearity the final potential from these two dipoles will be as in figure ???. Differently this potential would be exactly the same as the potential distribution outcome from a single dipole where the orientation is the vectorial sum of dipole D1 and D2 figure ???. This equality is also testified from dipole distributions in figure ??.



(a) Voltage from dipole oriented along x



(b) Voltage from dipole oriented along y

Figure 2.5.1: Voltage distribution

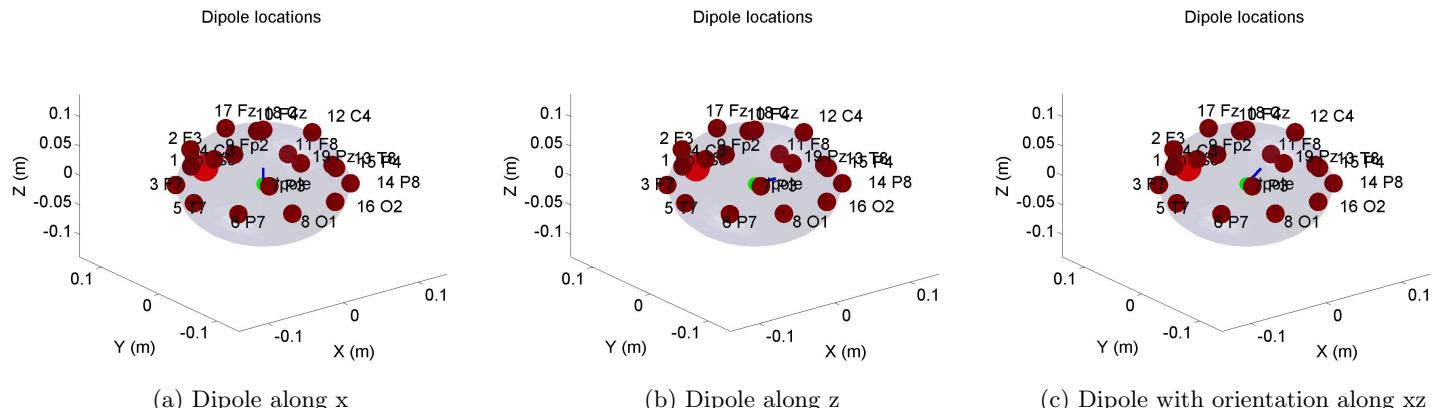
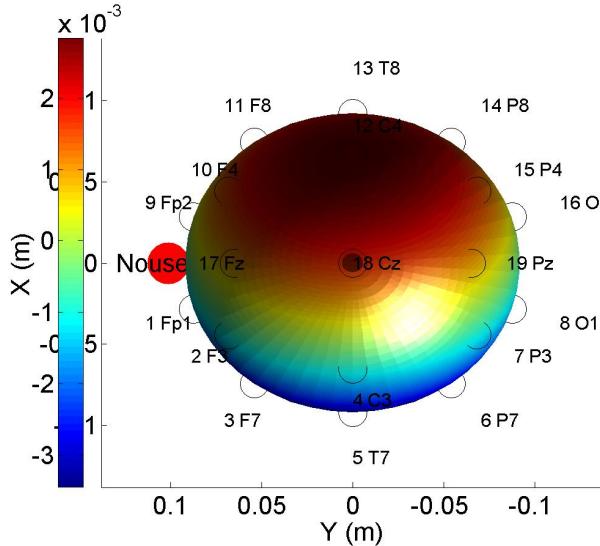
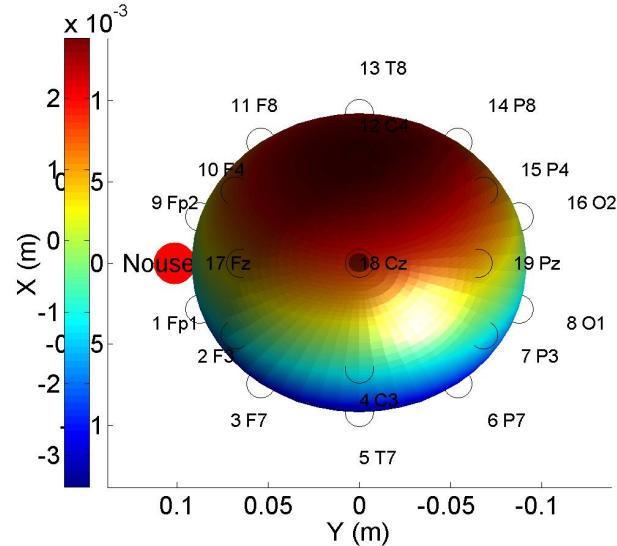


Figure 2.5.2: Dipole location



(a) Voltage superposition

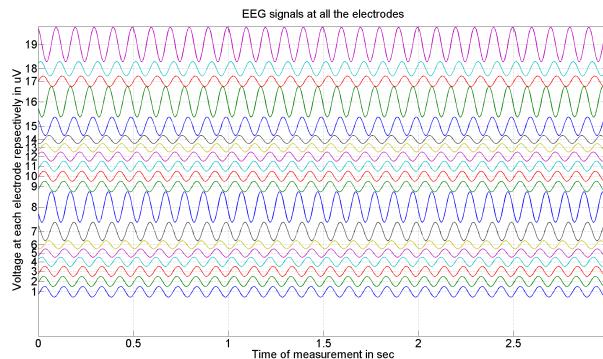


(b) Voltage from the dipole along xy

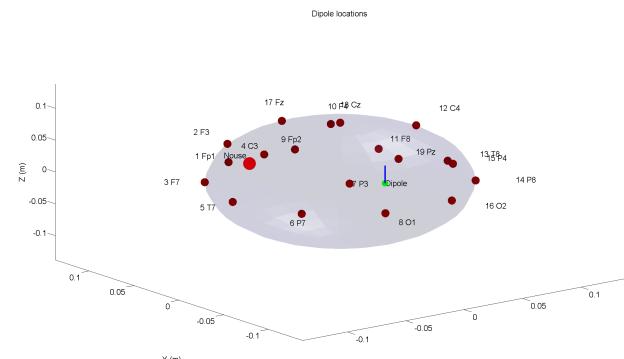
Figure 2.5.3: Potential distribution

## 2.6 EEG time series generation

Hereby EEG time series are being simulated by rotating along the xy plane the dipole located in the coordinates (0,-0.05,0.02) figure ???. The sampling frequency is 200 Hz which is much higher than the dipole rotation frequency which is 10 Hz in our case. After 3 sec EEG simulation from the time series values plotted in figure ?? what can be observed is that the electrodes near the dipole has a much higher amplitude comparing to the ones sitting further from the dipole.



(a) EEG plot



(b) Dipole

Figure 2.6.1: EEG simulation

### 3 Inverse problem

Inverse problem in EEG tends to estimate the source by its location and orientation given an instance measurement. This is an ill-posed problem due to its non-unique outcome and highly sensitive to the minor changes (unstable solution) [?]. Two set of methods in solving inverse problem in EEG exist including here, parametric and non-parametric. In this work parametric method is being utilized where it makes an exhaustive search upon a set of initial points for the best fit. The optimization is done iteratively until an arbitrary threshold is achieved.

#### 3.1 Estimation of a dipole using a single time instance

Inverse method has been applied on the on potential distribution outcomed from the dipole located in the coordinates (0.06,0,0.01) oriented along x. The dipole orientation error (DOR) equation ?? and dipole location error (DLE) equation ?? for this particular measurement are outlined in figure ?? whereas the RRE plot in figure ???. From these two figures a consistency of the errors is noted in both these scales for all the five trials. Whereas the potential to be used for this inverse problem is plotted in figure ??.

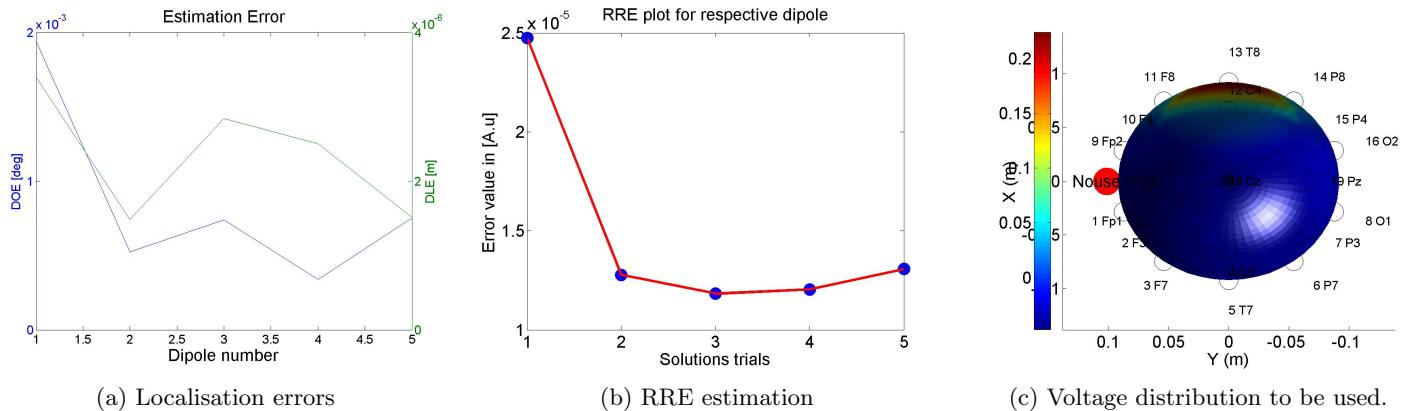


Figure 3.1.1: Inverse problem for a dipole located at (0.06,0,0) oriented along x

#### 3.2 Estimation of a dipole using the simulated EEG

Hereby a certain potential is read from the simulated EEG in figure ?? and the via inverse model the dipole is located from this particular time instance of the EEG. In the table ?? are the dipole locations data for this particular implementation.

Table 1: Inverse problem with electrode position altered

	<i>X</i>	<i>Y</i>	<i>Z</i>	<i>OriX</i>	<i>OriY</i>	<i>OriZ</i>	<i>RRE</i>
height	$4.74e - 07$	$-5.00e - 02$	$2.00e - 02$	$6.03e - 06$	$1.00e + 00$	$1.79e - 05$	$1.41e - 05$
<i>D1</i>	$4.74e - 07$	$-5.00e - 02$	$2.00e - 02$	$6.03e - 06$	$1.00e + 00$	$1.79e - 05$	$1.41e - 05$
<i>D2</i>	$4.23e - 02$	$-1.89e - 02$	$-7.85e - 02$	$3.65e - 01$	$8.89e - 01$	$-2.78e - 01$	$4.77e - 01$
<i>D3</i>	$3.50e - 07$	$-5.00e - 02$	$2.00e - 02$	$4.45e - 06$	$1.00e + 00$	$-3.92e - 05$	$2.64e - 05$
<i>D4</i>	$7.14e - 07$	$-5.00e - 02$	$2.00e - 02$	$9.08e - 06$	$1.00e + 00$	$2.79e - 06$	$1.56e - 05$
<i>D5</i>	$2.65e - 05$	$-5.00e - 02$	$2.00e - 02$	$3.38e - 04$	$1.00e + 00$	$9.32e - 05$	$3.92e - 04$

### 3.3 Error due to not incorporating a malfunctioning electrode

Hereby the importance of electrode functioning is verified. Using a dipole located at (0.06,0,0.01) oriented along x is used for this study. The potential distribution when all the electrodes are working is in figure ??, when the electrode P8 is off the potential distribution is as in the figure ?? whereas when the electrode F7 is off the potential distribution is as in the figure ??

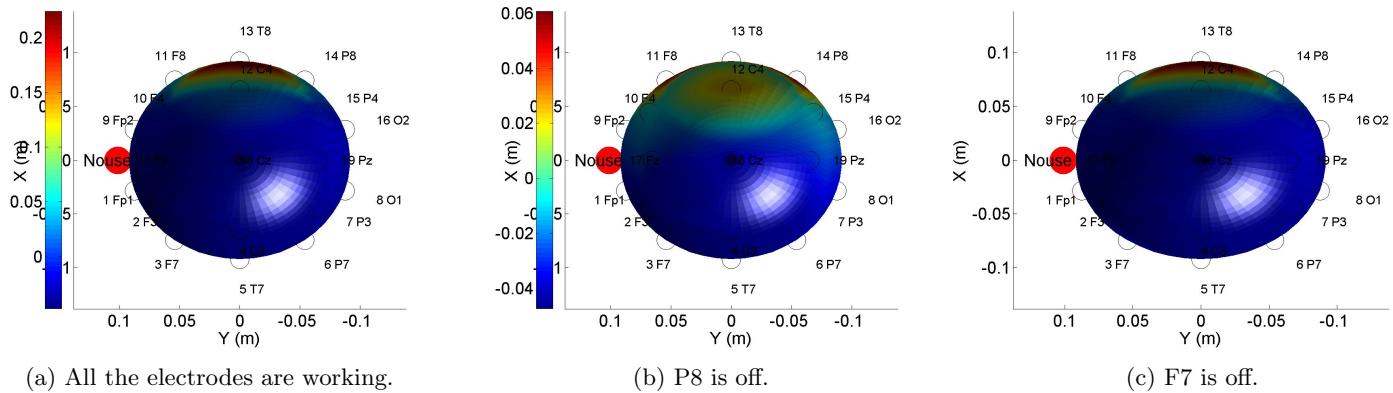


Figure 3.3.1: Voltage distribution measurement

The inverse problem is applied in all these three cases. DOE and DLE plots for respective method are outlined in figure ???. As it is excepted these error are at lower scale for the case of full electrode well functioning ?? whereas for the P8 case these errors are significantly higher compare to the F7 case respectively in figure ?? and ???. At similiar figure is also the RRE plots in figure ?? where is is easily observed the scale of error for the P8 case as compare to the F7 case. This is as a result that the P8 electrode location. This electrode is right in front of the main stream of the potential consequently being responsible for most flow. This flow is high in this direction due to the dipole orientation. Since the P8 is not functioning the potential measurement is measured dramatically wrong in this case.

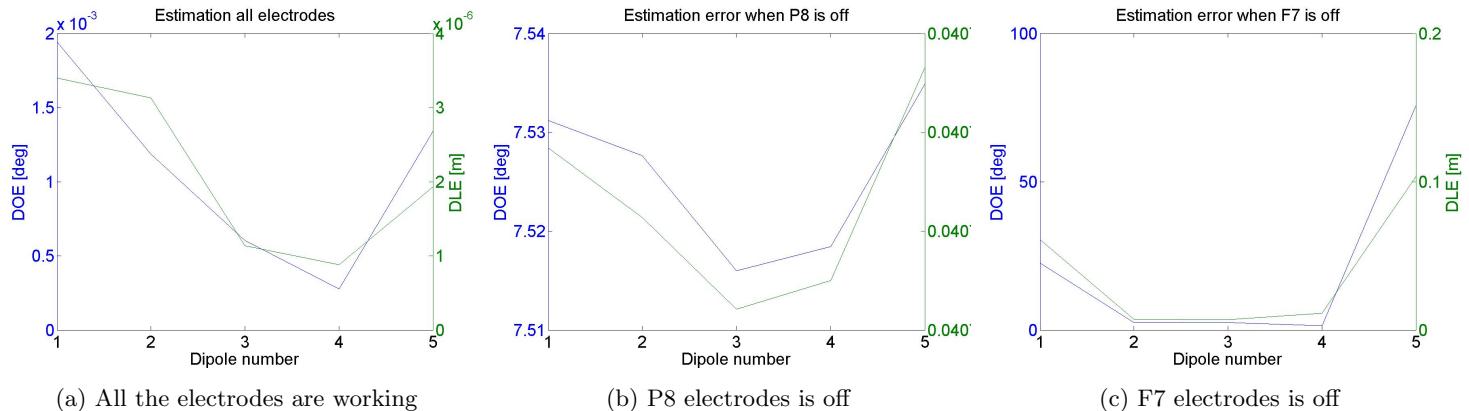


Figure 3.3.2: Localisation error for the three cases

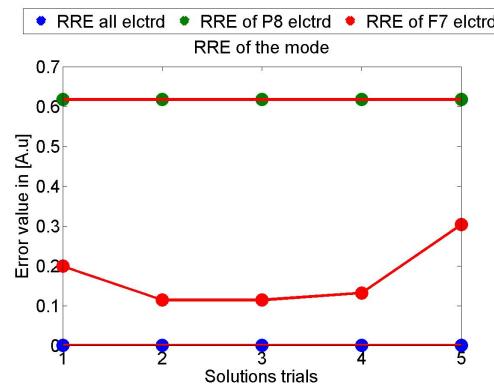


Figure 3.3.3: RRE estimation for the three cases

### 3.4 Error by different conductivity of the tissues

Skull conductivity is also an important parameter for the inverse model. Hereby an experimental study is being conducted where the inverse problem is being uplied over a head model with different skull conductivity as compare to the head model where the forward problem is being computed. Hereby 10 different dipole are being tested where 5 different trials are tested for each dipole in the inverse problem. In the table ?? the solution are listed where Trial1D1 stands for trial 1 dipole 1. Whereas the DOE and DLE are plotted respectively in table ?? and ?? for each dipole trial over five different estimation for each trial.

Table 2: Inverse problem with skull conductivity altered

	<i>X</i>	<i>Y</i>	<i>Z</i>	<i>OriX</i>	<i>OriY</i>	<i>OriZ</i>	<i>RRE</i>
height							
Tria1D1	4.69e - 02	1.66e - 02	3.00e - 02	7.07e - 01	7.07e - 01	-6.10e - 06	1.59e - 05
Tria1D2	4.69e - 02	1.66e - 02	3.00e - 02	7.07e - 01	7.07e - 01	4.15e - 06	9.22e - 06
Tria1D3	4.69e - 02	1.66e - 02	3.00e - 02	7.07e - 01	7.07e - 01	1.15e - 05	1.41e - 05
Tria1D4	4.69e - 02	1.66e - 02	3.00e - 02	7.07e - 01	7.07e - 01	-1.62e - 05	2.08e - 05
Tria1D5	4.69e - 02	1.66e - 02	3.00e - 02	7.07e - 01	7.07e - 01	2.45e - 06	1.81e - 05
Tria2D1	2.81e - 02	4.19e - 02	2.04e - 02	7.07e - 01	7.07e - 01	7.42e - 06	1.41e - 05
Tria2D2	2.81e - 02	4.19e - 02	2.04e - 02	7.07e - 01	7.07e - 01	-3.32e - 05	2.12e - 05
Tria2D3	2.81e - 02	4.19e - 02	2.04e - 02	7.07e - 01	7.07e - 01	4.10e - 06	1.55e - 05
Tria2D4	2.82e - 02	4.19e - 02	2.04e - 02	7.07e - 01	7.07e - 01	1.53e - 05	3.80e - 05
Tria2D5	2.81e - 02	4.19e - 02	2.04e - 02	7.07e - 01	7.07e - 01	-1.69e - 05	2.00e - 05
Tria3D1	5.51e - 03	1.09e - 02	2.57e - 02	1.43e - 06	7.07e - 01	7.07e - 01	8.37e - 06
Tria3D2	5.51e - 03	1.09e - 02	2.57e - 02	3.05e - 06	7.07e - 01	7.07e - 01	1.58e - 05
Tria3D3	5.51e - 03	1.09e - 02	2.57e - 02	6.80e - 07	7.07e - 01	7.07e - 01	2.41e - 05
Tria3D4	5.51e - 03	1.09e - 02	2.57e - 02	1.20e - 06	7.07e - 01	7.07e - 01	8.06e - 06
Tria3D5	5.51e - 03	1.09e - 02	2.57e - 02	5.60e - 06	7.07e - 01	7.07e - 01	2.41e - 05
Tria4D1	1.10e - 02	3.03e - 02	4.06e - 02	-2.45e - 06	-9.83e - 06	1.00e + 00	2.06e - 05
Tria4D2	1.10e - 02	3.03e - 02	4.06e - 02	-5.84e - 06	5.67e - 06	1.00e + 00	2.29e - 05
Tria4D3	1.10e - 02	3.03e - 02	4.06e - 02	-7.02e - 07	-7.14e - 06	1.00e + 00	1.27e - 05
Tria4D4	1.10e - 02	3.03e - 02	4.06e - 02	-1.46e - 06	-1.00e - 05	1.00e + 00	1.84e - 05
Tria4D5	1.10e - 02	3.03e - 02	4.06e - 02	-6.65e - 06	9.30e - 07	1.00e + 00	2.24e - 05
Tria5D1	3.73e - 02	7.99e - 02	-1.53e - 02	-1.35e - 01	-6.77e - 01	7.24e - 01	2.93e - 01
Tria5D2	3.16e - 02	4.56e - 02	2.72e - 02	7.07e - 01	1.69e - 06	7.07e - 01	2.15e - 05
Tria5D3	3.16e - 02	4.56e - 02	2.72e - 02	7.07e - 01	2.04e - 06	7.07e - 01	4.44e - 06
Tria5D4	3.16e - 02	4.56e - 02	2.72e - 02	7.07e - 01	-1.17e - 05	7.07e - 01	1.64e - 05
Tria5D5	3.16e - 02	4.56e - 02	2.72e - 02	7.07e - 01	-6.21e - 06	7.07e - 01	1.68e - 05
Tria6D1	1.64e - 02	3.60e - 02	6.53e - 02	1.00e + 00	-1.37e - 05	-2.43e - 05	1.73e - 05
Tria6D2	1.64e - 02	3.60e - 02	6.53e - 02	1.00e + 00	-2.75e - 08	1.05e - 06	6.29e - 06
Tria6D3	1.64e - 02	3.60e - 02	6.53e - 02	1.00e + 00	2.70e - 06	9.33e - 06	1.36e - 05
Tria6D4	1.64e - 02	3.60e - 02	6.53e - 02	1.00e + 00	5.41e - 06	8.77e - 06	8.85e - 06
Tria6D5	1.64e - 02	3.60e - 02	6.53e - 02	1.00e + 00	3.07e - 06	1.72e - 06	1.25e - 05
Tria7D1	5.98e - 02	6.93e - 03	5.01e - 02	5.77e - 01	5.77e - 01	5.77e - 01	5.85e - 05
Tria7D2	8.88e - 02	-6.78e - 03	1.20e - 02	6.94e - 01	1.68e - 01	7.00e - 01	2.55e - 01
Tria7D3	5.99e - 02	6.93e - 03	5.01e - 02	5.77e - 01	5.77e - 01	5.77e - 01	1.73e - 05
Tria7D4	5.99e - 02	6.93e - 03	5.01e - 02	5.77e - 01	5.77e - 01	5.77e - 01	1.38e - 05
Tria7D5	5.99e - 02	6.93e - 03	5.01e - 02	5.77e - 01	5.77e - 01	5.77e - 01	1.38e - 05
Tria8D1	1.67e - 02	3.58e - 02	5.08e - 02	1.00e + 00	1.10e - 07	-5.77e - 06	1.28e - 05
Tria8D2	1.67e - 02	3.58e - 02	5.08e - 02	1.00e + 00	3.36e - 06	8.28e - 06	9.94e - 06
Tria8D3	1.67e - 02	3.58e - 02	5.08e - 02	1.00e + 00	-9.13e - 06	-1.84e - 05	2.87e - 05
Tria8D4	1.67e - 02	3.58e - 02	5.08e - 02	1.00e + 00	-5.01e - 06	-1.73e - 05	2.50e - 05
Tria8D5	1.67e - 02	3.58e - 02	5.08e - 02	1.00e + 00	-4.31e - 06	-7.02e - 06	1.06e - 05
Tria9D1	6.59e - 03	5.97e - 03	3.87e - 02	-7.46e - 07	7.07e - 01	7.07e - 01	4.04e - 05
Tria9D2	6.59e - 03	5.97e - 03	3.87e - 02	6.57e - 07	7.07e - 01	7.07e - 01	1.04e - 05
Tria9D3	6.59e - 03	5.97e - 03	3.87e - 02	-1.38e - 07	7.07e - 01	7.07e - 01	9.16e - 06
Tria9D4	6.59e - 03	5.97e - 03	3.87e - 02	1.38e - 06	7.07e - 01	7.07e - 01	2.04e - 05
Tria9D5	6.59e - 03	5.97e - 03	3.87e - 02	2.78e - 06	7.07e - 01	7.07e - 01	1.22e - 05
Tria10D1	7.13e - 04	4.09e - 02	1.30e - 03	-1.21e - 06	1.00e + 00	-5.74e - 07	1.09e - 05
Tria10D2	7.12e - 04	4.09e - 02	1.30e - 03	7.88e - 06	1.00e + 00	-4.78e - 05	3.57e - 05
Tria10D3	7.13e - 04	4.09e - 02	1.30e - 03	-3.34e - 06	1.00e + 00	-1.23e - 05	1.19e - 05
Tria10D4	7.14e - 04	4.09e - 02	1.30e - 03	-6.28e - 06	1.00e + 00	-1.39e - 06	1.43e - 05
Tria10D5	7.13e - 04	4.09e - 02	1.30e - 03	-5.90e - 06	1.00e + 00	-2.32e - 05	1.69e - 05

Table 3: DOE for skull

	<i>D</i> 1	<i>D</i> 2	<i>D</i> 3	<i>D</i> 4	<i>D</i> 5
height					
<i>Trial</i> 1	$3.78e - 04$	$3.18e - 04$	$6.87e - 04$	$9.83e - 04$	$5.82e - 04$
<i>Trial</i> 2	$5.65e - 04$	$1.91e - 03$	$3.02e - 04$	$1.15e - 03$	$1.12e - 03$
<i>Trial</i> 3	$1.98e - 04$	$7.40e - 04$	$5.63e - 04$	$4.09e - 04$	$4.72e - 04$
<i>Trial</i> 4	$5.80e - 04$	$4.66e - 04$	$4.11e - 04$	$5.79e - 04$	$3.85e - 04$
<i>Trial</i> 5	$6.54e + 01$	$7.27e - 04$	$2.30e - 04$	$1.02e - 03$	$6.47e - 04$
<i>Trial</i> 6	$1.60e - 03$	$6.03e - 05$	$5.56e - 04$	$5.90e - 04$	$2.01e - 04$
<i>Trial</i> 7	$3.52e - 03$	$2.56e + 01$	$3.40e - 03$	$5.79e - 04$	$8.32e - 04$
<i>Trial</i> 8	$3.31e - 04$	$5.12e - 04$	$1.18e - 03$	$1.03e - 03$	$4.72e - 04$
<i>Trial</i> 9	$7.26e - 05$	$3.60e - 04$	$1.11e - 04$	$8.11e - 04$	$1.77e - 04$
<i>Trial</i> 10	$7.67e - 05$	$2.78e - 03$	$7.32e - 04$	$3.69e - 04$	$1.37e - 03$

Table 4: DLE for skull

	<i>D</i> 1	<i>D</i> 2	<i>D</i> 3	<i>D</i> 4	<i>D</i> 5
height					
<i>Trial</i> 1	$2.16e - 06$	$8.69e - 07$	$1.05e - 06$	$1.63e - 06$	$1.53e - 06$
<i>Trial</i> 2	$9.94e - 07$	$2.02e - 06$	$1.06e - 06$	$3.29e - 06$	$1.50e - 06$
<i>Trial</i> 3	$6.71e - 07$	$1.85e - 06$	$2.42e - 06$	$9.89e - 07$	$2.35e - 06$
<i>Trial</i> 4	$2.24e - 06$	$1.53e - 06$	$9.52e - 07$	$1.72e - 06$	$1.54e - 06$
<i>Trial</i> 5	$5.49e - 02$	$2.28e - 06$	$3.64e - 07$	$1.69e - 06$	$1.71e - 06$
<i>Trial</i> 6	$2.47e - 06$	$9.20e - 07$	$1.50e - 06$	$5.06e - 07$	$9.78e - 07$
<i>Trial</i> 7	$1.54e - 05$	$4.97e - 02$	$4.18e - 06$	$3.60e - 06$	$3.19e - 06$
<i>Trial</i> 8	$7.02e - 07$	$6.77e - 07$	$2.66e - 06$	$2.20e - 06$	$8.37e - 07$
<i>Trial</i> 9	$3.42e - 06$	$7.23e - 07$	$6.98e - 07$	$2.09e - 06$	$1.17e - 06$
<i>Trial</i> 10	$1.61e - 06$	$3.05e - 06$	$1.06e - 06$	$1.84e - 06$	$1.89e - 06$

In case the skull conductivity is not given the setup in figure ?? could be utilized for a particular measurement.

### 3.5 Inverse problem with electrode position altered

Similarly to the case when the skull conductivity was changed hereby a altering in the electrode position is performed. In table ?? are the result listed accordingly. Whereas the DOE and DLE are plotted respectively in table ?? and ?? for each dipole trial over five different estimation for each trial. The spherical angle is changed as in equation ?? for a particular displacement.

Table 5: Inverse problem with electrode position altered

	<i>X</i>	<i>Y</i>	<i>Z</i>	<i>OriX</i>	<i>OriY</i>	<i>OriZ</i>	<i>RRE</i>
heightTria1D1	7.56e - 03	9.50e - 03	7.13e - 02	-1.85e - 02	7.24e - 01	6.89e - 01	7.67e - 02
Tria1D2	2.56e - 03	1.51e - 02	1.43e - 04	-5.90e - 02	3.64e - 01	9.30e - 01	6.28e - 01
Tria1D3	7.62e - 03	9.50e - 03	7.13e - 02	-1.86e - 02	7.24e - 01	6.90e - 01	7.67e - 02
Tria1D4	7.60e - 03	9.51e - 03	7.13e - 02	-1.84e - 02	7.24e - 01	6.89e - 01	7.67e - 02
Tria1D5	7.59e - 03	9.48e - 03	7.13e - 02	-1.86e - 02	7.24e - 01	6.89e - 01	7.67e - 02
Tria2D1	2.05e - 02	2.05e - 03	5.95e - 02	-3.05e - 02	9.99e - 01	-4.48e - 02	1.28e - 01
Tria2D2	2.05e - 02	2.05e - 03	5.95e - 02	-3.05e - 02	9.99e - 01	-4.48e - 02	1.28e - 01
Tria2D3	2.05e - 02	2.03e - 03	5.95e - 02	-3.07e - 02	9.99e - 01	-4.52e - 02	1.28e - 01
Tria2D4	2.05e - 02	2.05e - 03	5.95e - 02	-3.06e - 02	9.99e - 01	-4.47e - 02	1.28e - 01
Tria2D5	2.05e - 02	2.03e - 03	5.95e - 02	-3.06e - 02	9.99e - 01	-4.51e - 02	1.28e - 01
Tria3D1	8.00e - 02	2.63e - 02	-2.84e - 02	-5.45e - 01	2.11e - 02	8.38e - 01	1.50e - 01
Tria3D2	7.80e - 02	1.91e - 02	1.18e - 02	6.15e - 01	5.83e - 01	5.31e - 01	5.56e - 02
Tria3D3	7.81e - 02	1.90e - 02	1.18e - 02	6.15e - 01	5.83e - 01	5.31e - 01	5.56e - 02
Tria3D4	7.81e - 02	1.90e - 02	1.19e - 02	6.16e - 01	5.83e - 01	5.30e - 01	5.56e - 02
Tria3D5	7.80e - 02	1.91e - 02	1.18e - 02	6.15e - 01	5.83e - 01	5.31e - 01	5.56e - 02
Tria4D1	1.28e - 02	3.53e - 02	6.78e - 02	5.32e - 01	5.84e - 01	6.14e - 01	9.88e - 02
Tria4D2	1.28e - 02	3.53e - 02	6.79e - 02	5.31e - 01	5.83e - 01	6.14e - 01	9.88e - 02
Tria4D3	1.28e - 02	3.53e - 02	6.78e - 02	5.32e - 01	5.84e - 01	6.14e - 01	9.88e - 02
Tria4D4	1.28e - 02	3.53e - 02	6.79e - 02	5.32e - 01	5.84e - 01	6.14e - 01	9.88e - 02
Tria4D5	1.28e - 02	3.53e - 02	6.78e - 02	5.31e - 01	5.84e - 01	6.14e - 01	9.88e - 02
Tria5D1	8.87e - 03	2.86e - 02	1.75e - 02	1.00e + 00	7.73e - 03	-1.38e - 02	7.10e - 02
Tria5D2	8.90e - 03	2.86e - 02	1.74e - 02	1.00e + 00	7.64e - 03	-1.35e - 02	7.10e - 02
Tria5D3	8.91e - 03	2.85e - 02	1.75e - 02	1.00e + 00	7.92e - 03	-1.36e - 02	7.10e - 02
Tria5D4	8.90e - 03	2.86e - 02	1.74e - 02	1.00e + 00	7.55e - 03	-1.34e - 02	7.10e - 02
Tria5D5	8.92e - 03	2.86e - 02	1.74e - 02	1.00e + 00	7.66e - 03	-1.32e - 02	7.10e - 02
Tria6D1	4.08e - 02	8.09e - 02	-1.52e - 02	4.60e - 01	8.11e - 02	8.84e - 01	3.34e - 01
Tria6D2	4.16e - 02	3.58e - 02	3.48e - 02	6.93e - 01	7.20e - 01	-2.01e - 02	9.23e - 02
Tria6D3	4.16e - 02	3.57e - 02	3.48e - 02	6.93e - 01	7.20e - 01	-1.98e - 02	9.23e - 02
Tria6D4	5.37e - 03	6.32e - 02	5.94e - 02	5.68e - 01	8.23e - 01	2.11e - 03	3.51e - 01
Tria6D5	-9.01e - 04	6.87e - 02	5.87e - 02	3.87e - 01	8.89e - 01	2.46e - 01	3.06e - 01
Tria7D1	-2.19e - 03	5.94e - 02	3.50e - 02	6.89e - 01	7.68e - 04	7.25e - 01	1.58e - 01
Tria7D2	-1.03e - 03	9.09e - 02	2.45e - 03	6.14e - 01	-5.40e - 01	5.76e - 01	2.24e - 01
Tria7D3	-2.17e - 03	5.95e - 02	3.50e - 02	6.89e - 01	2.26e - 04	7.25e - 01	1.58e - 01
Tria7D4	-2.19e - 03	5.95e - 02	3.50e - 02	6.89e - 01	1.01e - 04	7.25e - 01	1.58e - 01
Tria7D5	-2.19e - 03	5.95e - 02	3.50e - 02	6.89e - 01	3.12e - 04	7.25e - 01	1.58e - 01
Tria8D1	4.33e - 02	7.98e - 02	-1.58e - 02	9.15e - 02	2.12e - 01	9.73e - 01	3.37e - 01
Tria8D2	4.63e - 02	5.08e - 02	3.50e - 02	-1.32e - 02	7.21e - 01	6.93e - 01	4.11e - 02
Tria8D3	4.63e - 02	5.08e - 02	3.50e - 02	-1.33e - 02	7.21e - 01	6.93e - 01	4.11e - 02
Tria8D4	7.03e - 03	9.09e - 02	1.32e - 02	5.55e - 01	-2.65e - 01	7.88e - 01	2.55e - 01
Tria8D5	6.48e - 02	2.29e - 02	6.02e - 02	7.69e - 03	9.15e - 01	4.03e - 01	2.94e - 01
Tria9D1	9.54e - 03	5.58e - 02	3.10e - 02	6.54e - 01	7.52e - 01	-8.26e - 02	1.80e - 01
Tria9D2	9.61e - 03	5.58e - 02	3.09e - 02	6.54e - 01	7.52e - 01	-8.14e - 02	1.80e - 01
Tria9D3	9.55e - 03	5.58e - 02	3.10e - 02	6.54e - 01	7.52e - 01	-8.26e - 02	1.80e - 01
Tria9D4	9.55e - 03	5.58e - 02	3.10e - 02	6.54e - 01	7.52e - 01	-8.26e - 02	1.80e - 01
Tria9D5	9.58e - 03	5.58e - 02	3.09e - 02	6.54e - 01	7.52e - 01	-8.25e - 02	1.80e - 01
Tria10D1	5.21e - 03	1.50e - 02	3.05e - 03	7.01e - 01	2.35e - 02	7.12e - 01	1.46e - 01
Tria10D2	5.17e - 03	1.50e - 02	3.06e - 03	7.02e - 01	2.39e - 02	7.12e - 01	1.46e - 01
Tria10D3	5.22e - 03	1.50e - 02	3.06e - 03	7.01e - 01	2.35e - 02	7.12e - 01	1.46e - 01
Tria10D4	5.20e - 03	1.50e - 02	3.05e - 03	7.01e - 01	2.36e - 02	7.12e - 01	1.46e - 01
Tria10D5	5.19e - 03	1.49e - 02	3.01e - 03	7.01e - 01	2.39e - 02	7.12e - 01	1.46e - 01

As it could be noted, the error due to the electrode displacement sits at much higher values as compare to the case when the skull conductivity is changed. This infer a great importance of electrode placement in source localisation via inverse methods.

Table 6: DOE for electrode misplacement

	<i>D1</i>	<i>D2</i>	<i>D3</i>	<i>D4</i>	<i>D5</i>
height	$1.78e + 00$	$2.39e + 01$	$1.75e + 00$	$1.75e + 00$	$1.77e + 00$
<i>Trial1</i>	$3.11e + 00$	$3.11e + 00$	$3.13e + 00$	$3.10e + 00$	$3.12e + 00$
<i>Trial2</i>	$7.95e + 01$	$3.43e + 00$	$3.47e + 00$	$3.53e + 00$	$3.45e + 00$
<i>Trial3</i>	$3.37e + 00$	$3.39e + 00$	$3.35e + 00$	$3.36e + 00$	$3.38e + 00$
<i>Trial4</i>	$9.09e - 01$	$8.88e - 01$	$9.03e - 01$	$8.83e - 01$	$8.77e - 01$
<i>Trial5</i>	$6.75e + 01$	$1.59e + 00$	$1.59e + 00$	$1.04e + 01$	$2.56e + 01$
<i>Trial6</i>	$1.45e + 00$	$3.27e + 01$	$1.48e + 00$	$1.47e + 00$	$1.45e + 00$
<i>Trial7</i>	$3.31e + 01$	$1.34e + 00$	$1.34e + 00$	$6.83e + 01$	$2.13e + 01$
<i>Trial8</i>	$6.18e + 00$	$6.12e + 00$	$6.17e + 00$	$6.17e + 00$	$6.17e + 00$
<i>Trial9</i>	$1.42e + 00$	$1.43e + 00$	$1.42e + 00$	$1.42e + 00$	$1.44e + 00$
<i>Trial10</i>					

Table 7: DLE for electrode misplacement

	<i>D1</i>	<i>D2</i>	<i>D3</i>	<i>D4</i>	<i>D5</i>
height	$1.27e - 03$	$7.11e - 02$	$1.30e - 03$	$1.29e - 03$	$1.29e - 03$
<i>Trial1</i>	$3.68e - 03$	$3.69e - 03$	$3.71e - 03$	$3.68e - 03$	$3.66e - 03$
<i>Trial2</i>	$3.90e - 02$	$2.85e - 03$	$2.89e - 03$	$2.96e - 03$	$2.87e - 03$
<i>Trial3</i>	$6.26e - 03$	$6.28e - 03$	$6.23e - 03$	$6.25e - 03$	$6.26e - 03$
<i>Trial4</i>	$2.17e - 03$	$2.15e - 03$	$2.20e - 03$	$2.16e - 03$	$2.15e - 03$
<i>Trial5</i>	$6.49e - 02$	$3.12e - 03$	$3.10e - 03$	$5.09e - 02$	$5.78e - 02$
<i>Trial6</i>	$5.24e - 03$	$4.61e - 02$	$5.21e - 03$	$5.22e - 03$	$5.21e - 03$
<i>Trial7</i>	$5.59e - 02$	$3.44e - 03$	$3.45e - 03$	$5.71e - 02$	$4.51e - 02$
<i>Trial8</i>	$3.78e - 03$	$3.71e - 03$	$3.77e - 03$	$3.76e - 03$	$3.74e - 03$
<i>Trial9</i>	$4.56e - 03$	$4.54e - 03$	$4.58e - 03$	$4.55e - 03$	$4.54e - 03$
<i>Trial10</i>					

## A Forward problem appendix

### A.1 Head models

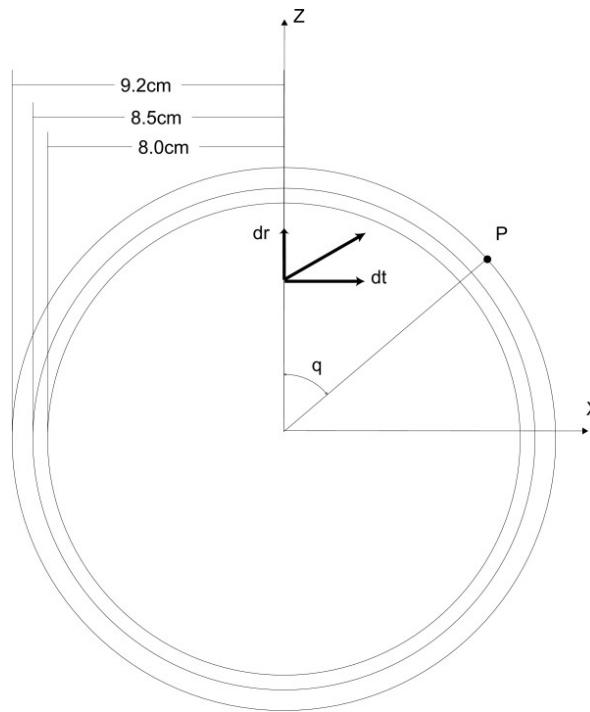


Figure A.1.1: Spherical head model

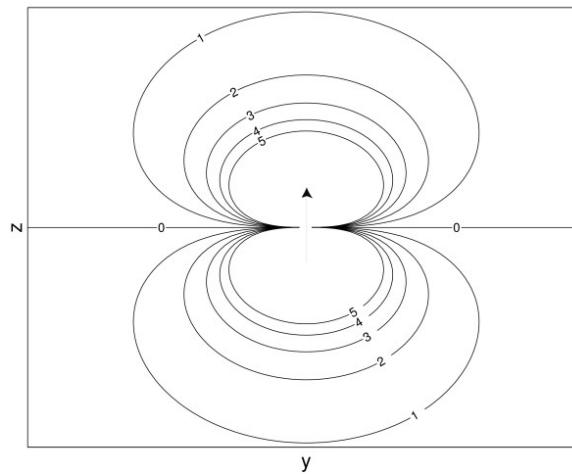


Figure A.1.2: Dipole electrical field

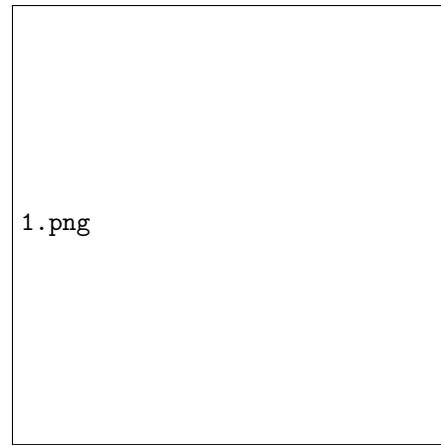


Figure A.1.3: Dipole modeling

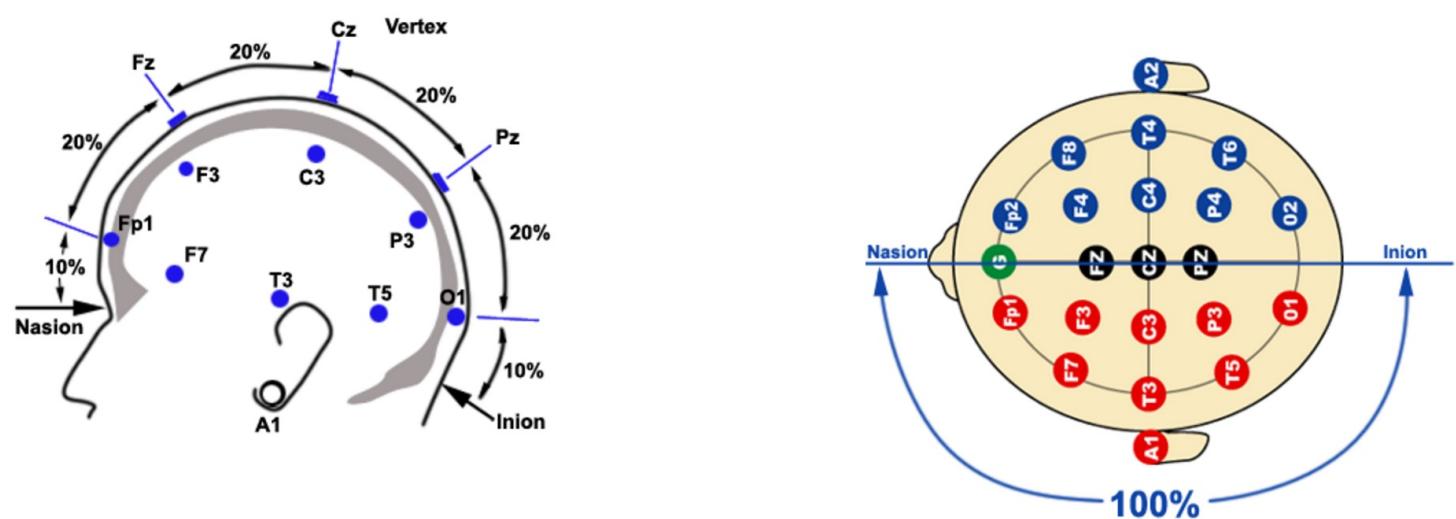


Figure A.1.4: EEG montage

## A.2 The Potential of a General Dipole

Consider a dipole with a dipole moment  $\vec{D} = (D_x, D_y, D_z)$  located at  $\vec{R}_1 = (X_1, Y_1, Z_1)$ , and a point on the scalp  $\vec{R}_2 = (X_2, Y_2, Z_2)$ . The radius vectors  $\vec{R}_1$  and  $\vec{R}_2$  define a plane in space, which will be called the major plane. The cross product  $\vec{N} = \vec{R}_1 \times \vec{R}_2$  is perpendicular to the major plane. The cross product  $\vec{t} = \vec{N} \times \vec{R}_1$  is in the major plane, and perpendicular to  $\vec{R}_1$ . Based on an identity from algebra,  $\vec{t} = \vec{R}_2(\vec{R}_1 \cdot \vec{R}_1) - \vec{R}_1(\vec{R}_1 \cdot \vec{R}_2)$ , or by components

$$t_x = X_2 \cdot p - X_1 \cdot q \quad (\text{A.2.1}) \qquad t_y = Y_2 \cdot p - Y_1 \cdot q \quad (\text{A.2.2}) \qquad t_z = Z_2 \cdot p - Z_1 \cdot q \quad (\text{A.2.3})$$

where  $p = X_1^2 + Y_1^2 + Z_1^2$  and  $q = X_1 \cdot X_2 + Y_1 \cdot Y_2 + Z_1 \cdot Z_2$ .  $\vec{T} = (T_x, T_y, T_z)$  is the unit vector in the  $\vec{t}$  direction, which is the tangential direction to  $\vec{R}_1$  in the major plane. Its components are

$$T_x = t_x/|t| \quad (\text{A.2.4}) \qquad T_y = t_y/|t| \quad (\text{A.2.5}) \qquad T_z = t_z/|t| \quad (\text{A.2.6})$$

where  $|t| = (t_x^2 + t_y^2 + t_z^2)^{1/2}$ . The unit vector  $\vec{RR} = (R_x, R_y, R_z)$  in the radial direction  $\vec{R}_1$  is

$$R_x = X_1/|\vec{R}_1| \quad (\text{A.2.7}) \qquad R_y = Y_1/|\vec{R}_1| \quad (\text{A.2.8}) \qquad R_z = Z_1/|\vec{R}_1| \quad (\text{A.2.9})$$

where  $|\vec{R}_1| = (X_1^2 + Y_1^2 + Z_1^2)^{1/2}$ . The cosine of the angle between  $\vec{R}_1$  and  $\vec{R}_2$  is

$$\cos\alpha = q/|\vec{R}_1| \cdot |\vec{R}_2| \quad (\text{A.2.10})$$

where  $|\vec{R}_2| = (X_2^2 + Y_2^2 + Z_2^2)^{1/2}$ . The potential that the dipole  $\vec{D}$  generates at the scalp point  $\vec{R}_2$  is the sum of the potentials contributed by  $D_x$ ,  $D_y$  and  $D_z$ . When these expressions are substituted in equation ?? the potential at  $\vec{R}_2$  due to  $D_x$  turns to be

$$V_x = \left\{ \frac{1}{4\pi SR^2} \sum_{i=1}^{\infty} \frac{X(2n+1)^3}{d_n(n+1)n} \cdot b^{n-1} \{nR_x P_n(\cos\alpha) + T_x P_n^{-1}(\cos\alpha)\} \right\} D_x \quad (\text{A.2.11})$$

and similarly, the potential due to  $D_y$  and  $D_z$  would be

$$V_y = \left\{ \frac{1}{4\pi SR^2} \sum_{i=1}^{\infty} \frac{Y(2n+1)^3}{d_n(n+1)n} \cdot b^{n-1} \{nR_y P_n(\cos\alpha) + T_y P_n^{-1}(\cos\alpha)\} \right\} D_y \quad (\text{A.2.12})$$

$$V_z = \left\{ \frac{1}{4\pi SR^2} \sum_{i=1}^{\infty} \frac{Z(2n+1)^3}{d_n(n+1)n} \cdot b^{n-1} \{nR_z P_n(\cos\alpha) + T_z P_n^{-1}(\cos\alpha)\} \right\} D_z \quad (\text{A.2.13})$$

where  $b = |\vec{R}_1|/R_1$  and  $\cos\alpha$  is given by equation ???. The potential  $V$  at  $\vec{R}_2$  due to  $\vec{D}$  at  $\vec{R}_1$  is  $V = V_x + V_y + V_z$ . Assigning a Reference Electrode

1) An arbitrary convenient point on the surface, denoted by  $\vec{R}_0$ , is declared as the reference. All potentials are measured with respect to the electrode at this point. (If the potentials have already been measured with respect to a different point, such as left earlobe, they have to be adjusted accordingly. The measured potential at  $\vec{R}_0$  (with respect to the earlobe) should be subtracted from the measured potential at each point).

2) Equations ?? are corrected for the new reference point, and become

$$V'_x = (T_{x12} - T_{x10}).D_x \quad (\text{A.2.14}) \qquad V'_y = (T_{y12} - T_{y10}).D_y \quad (\text{A.2.15}) \qquad V'_z = (T_{z12} - T_{z10}).D_z \quad (\text{A.2.16})$$

where  $T_{x10}$ ,  $T_{y10}$ ,  $T_{z10}$  are the transfer coefficients from a dipole at  $\vec{R}_1$  onto surface point  $\vec{R}_0$ .  $V'$ , the theoretical potential at  $\vec{R}_2$  with respect to  $\vec{R}_0$  due to a dipole at  $\vec{R}_1$  is given by

$$V' = V'_x + V'_y + V'_z. \quad (\text{A.2.17})$$

## B Inverse problem appendix

### B.1 Formulas

$$DLE = \sqrt{(x_{orig} - x_{est})^2 - (y_{orig} - y_{est})^2 - (z_{orig} - z_{est})^2} \quad (\text{B.1.1})$$

$$DOE = \arccos \left\{ \frac{Or_{xorig} * x_{est} + Or_{yorig} * y_{est} + Or_{zorig} * Or_{zest}}{\sqrt{Or_{xest}^2 - Or_{yest}^2 - Or_{zest}^2} * \sqrt{Or_{xorig}^2 - Or_{yorig}^2 - Or_{zorig}^2}} \right\} \quad (\text{B.1.2})$$

Spherical coordinate for the electrode displacement:

$$\text{Angle} = \frac{360 * \text{Displacement}}{2 * \pi * \text{Radius}} \quad (\text{B.1.3})$$

### B.2 Skull conductivity measurement

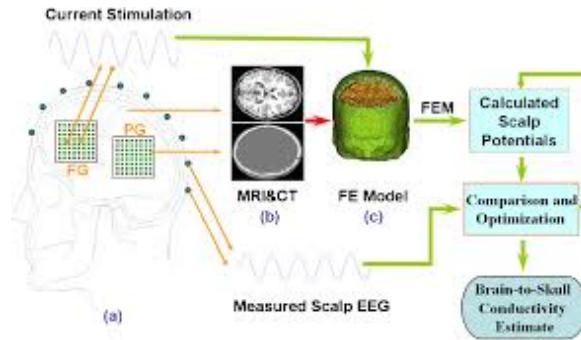
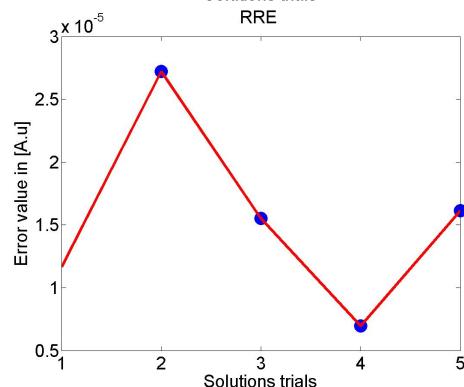
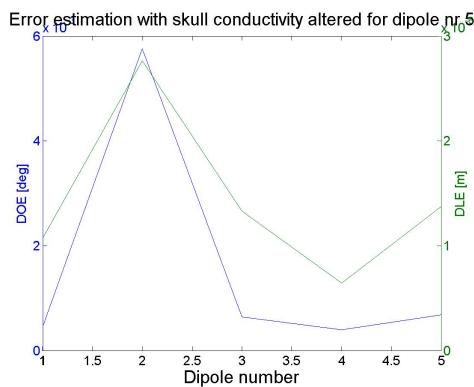
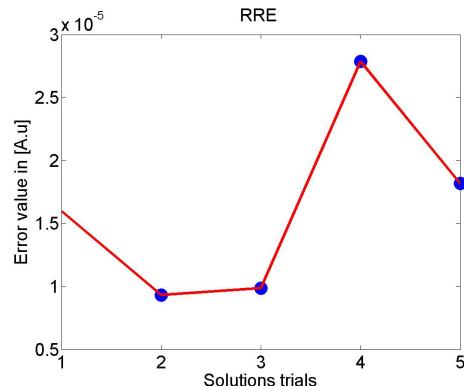
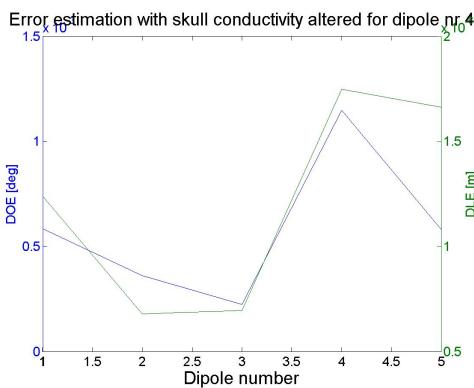
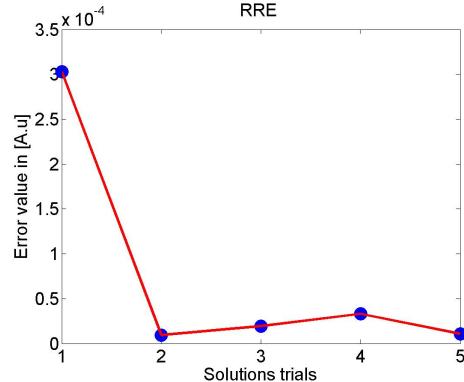
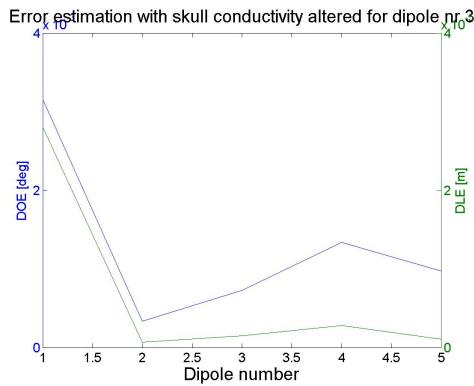
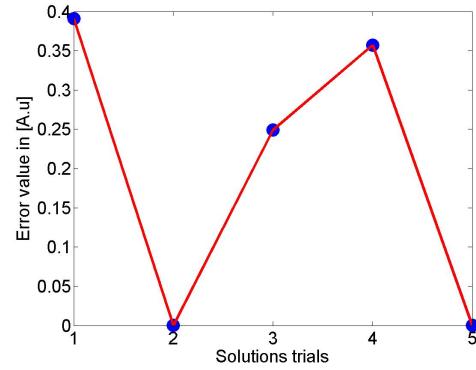
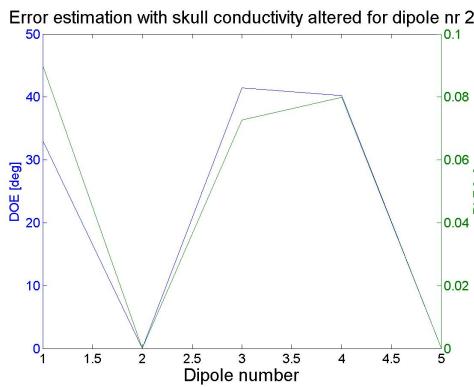
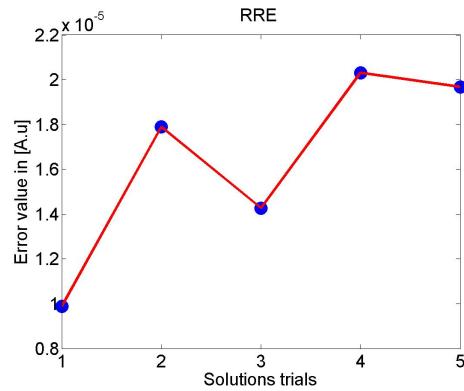
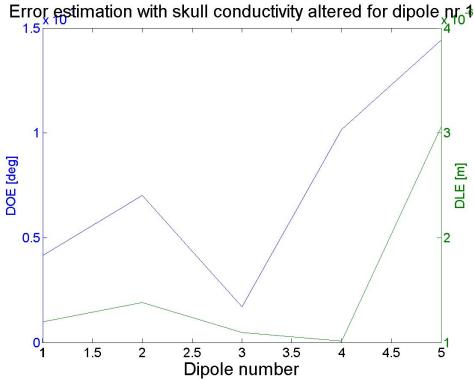
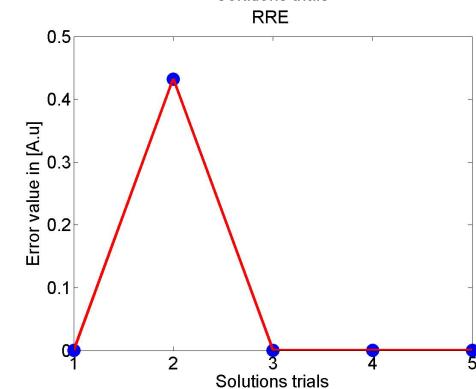
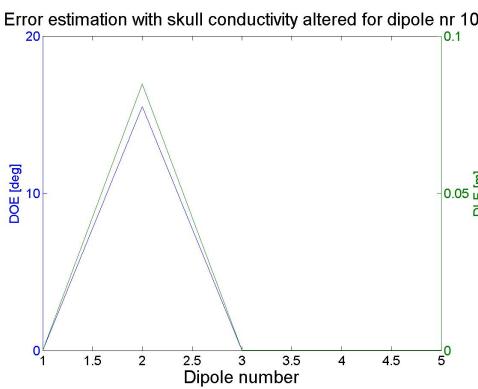
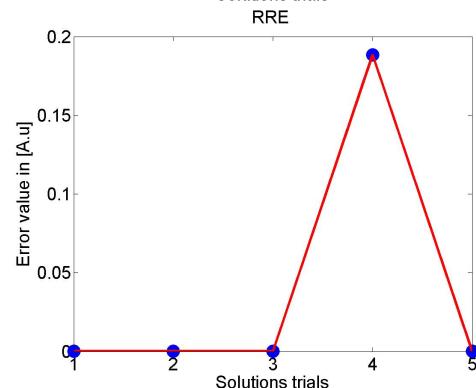
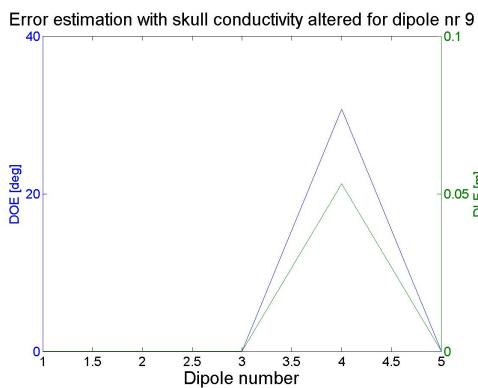
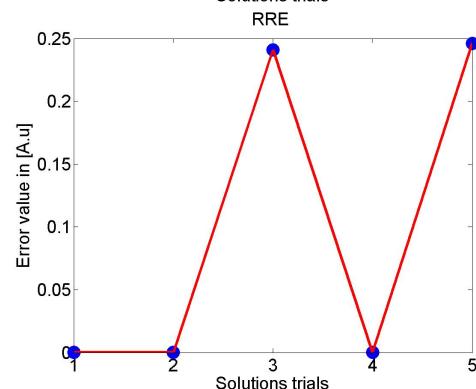
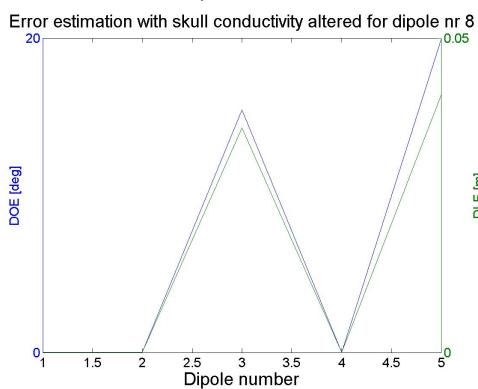
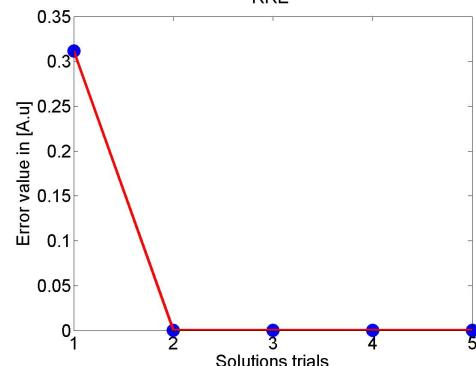
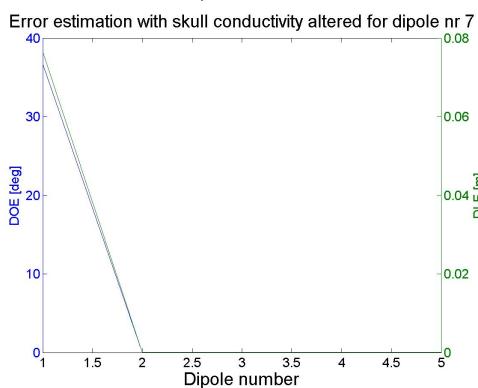
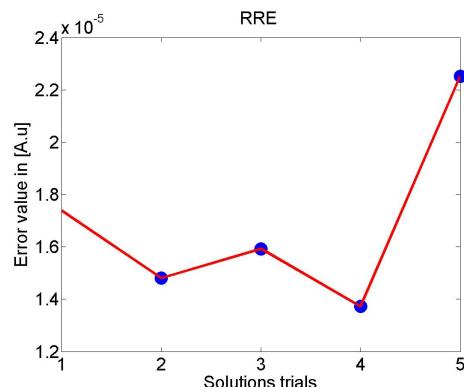
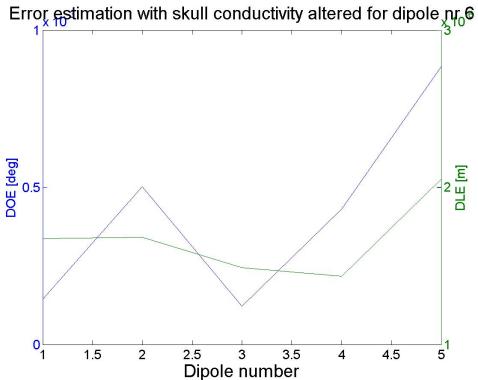


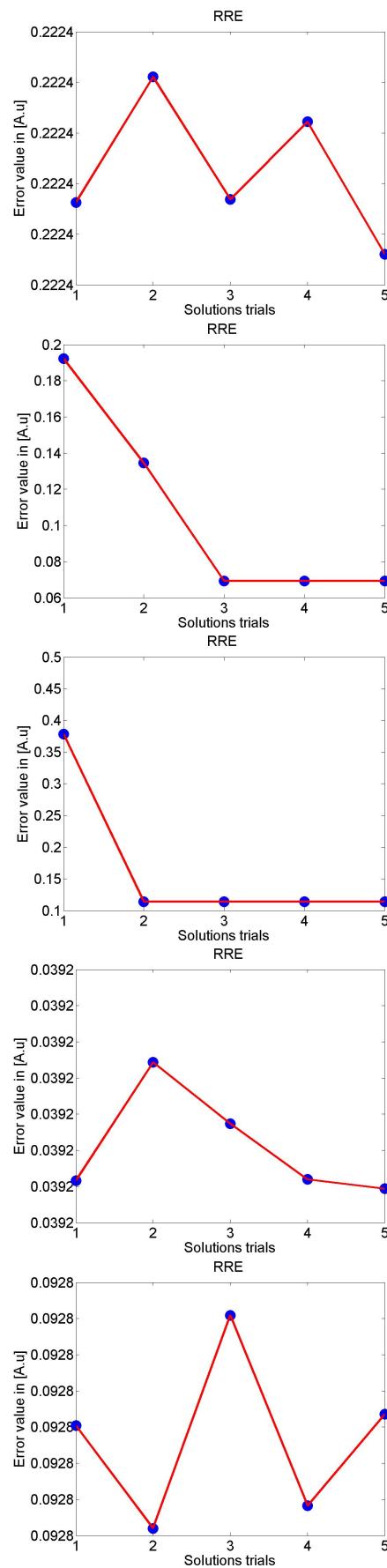
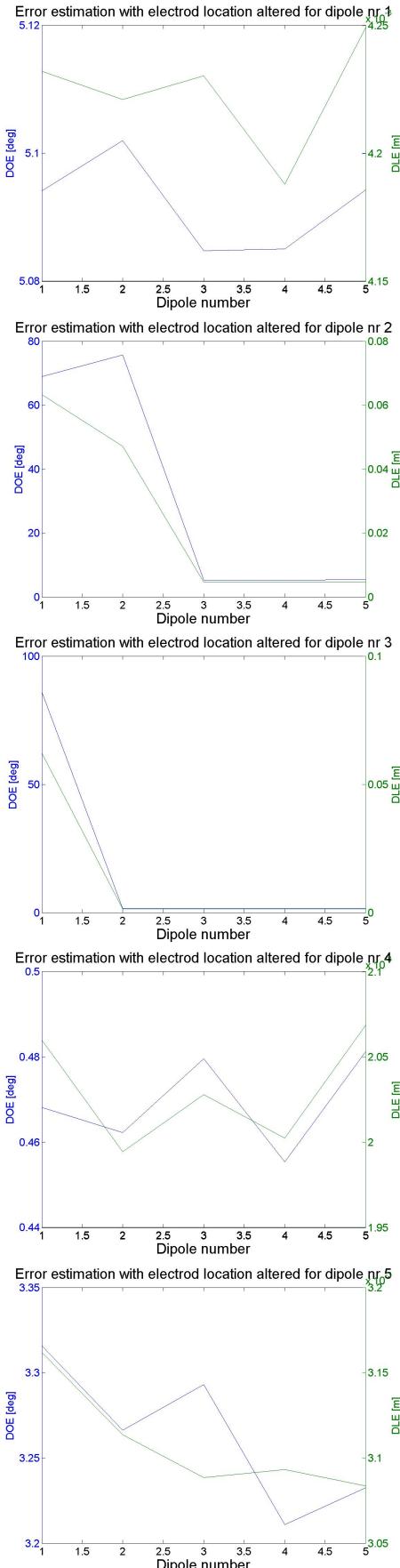
Figure B.2.1: Skull conductivity measurement[?]

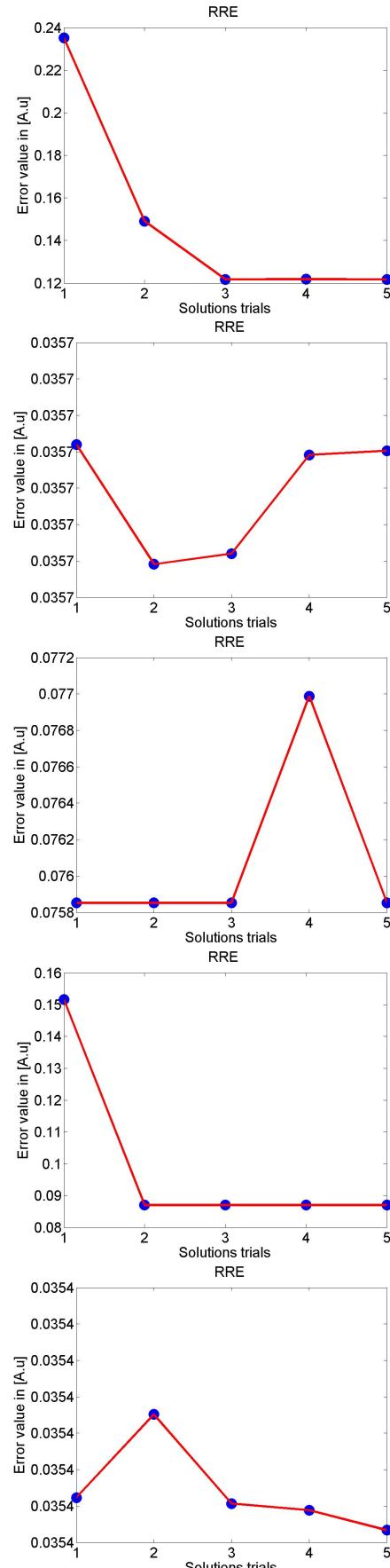
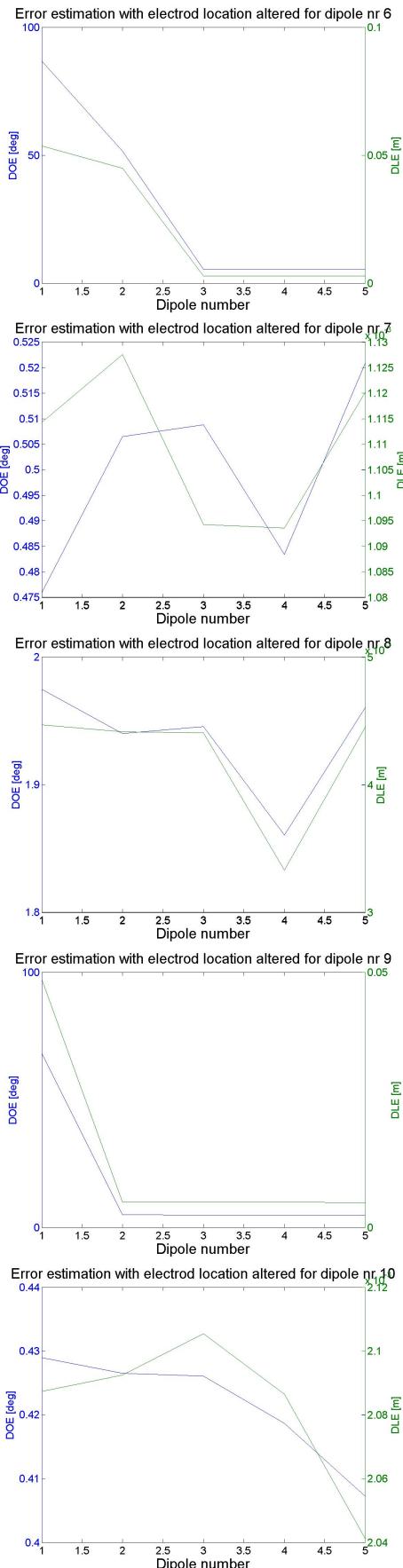
### B.3 Skull conductivity error plots





## B.4 Electrode misplacement error plots





## C Main code session

### C.1 First part

```

1
2 clear all
3 close all
4 clc
5 %%
6 % 1
7 load headmodel19           % Load the head model
8 %%
9 index=1;
10 %% 2 Show electrode position
11 Electrode_Position_V(hm,3)% Plot the location of the electrodes
12 [index]=Save_Image(index);
13 %% index=2;
14
15 %%
16 %% 3
17 Show_Dipole_Placement([0 0 0 0 0 1],hm,4)    % Show the dipole at the center orientation towards z
18 [index]=Save_Image(index);
19 Show_Dipole_Placement([-0.05 0 0 0 0 1],hm,5)  % Show the dipole at the middle of center towards the right ear
   orientation towards z
20 [index]=Save_Image(index);
21 %%
22 %% 4 dipole at the center orinted along x axis
23 source.loc=[0 0 0.05];          % Input a source at the center
24 source.ori=[1 0 0];            % Input the orientation towards x axis
25 [V1,L]=Spherical_Head_Model(hm,source);% Comput the voltage at the electrodes from this dipole with the
   forward solution
26 Potential_Distribution(V1,hm,6,1)        % Show the potential distribution in the electrodes
27 title('Electrod potential from dipole at the center oriented along x axis')
28 [index]=Save_Image(index);
29 Plot_Electrode_Potential(V1,9)
30 [index]=Save_Image(index);
31 Show_Dipole_Placement([0 0 0 1 0 0],hm,8)    % The dipole location and its orientation has been plot
32 [index]=Save_Image(index);
33 %%
34 %% 5 study the composition of L
35 Potential_Distribution(L(:,1),hm,17,1)
36 title('First column')
37 [index]=Save_Image(index);
38 Potential_Distribution(L(:,2),hm,18,1)
39 title('Second column')
40 [index]=Save_Image(index);
41 Potential_Distribution(L(:,3),hm,19,1)
42 title('Third column')
43 [index]=Save_Image(index);
44 %%
45 %% 6 two potential at the center , where one along the x axis the other along the z axis
46 source1.loc=[0 0 0];          % Input a source at the center
47 source1.ori=[0 0 1];          % Input the orientation towards z axis
48
49 source2.loc=[0 0 0];          % Input a source at the center
50 source2.ori=[1 0 0];          % Input the orientation towards x axis
51
52 source3.loc=[0 0 0];          % Input a source at the center
53 source3.ori=[1 0 1];          % Input the orientation towards x axis
54 %%
55 [V1,L1]=Spherical_Head_Model(hm,source1); % Comput the voltage at the electrodes from this dipole with the
   forward solution
56 [V2,L2]=Spherical_Head_Model(hm,source2); % Comput the voltage at the electrodes from this dipole with the
   forward solution
57 [V3,L2]=Spherical_Head_Model(hm,source3); % Comput the voltage at the electrodes from this dipole with the
   forward solution
58 VT=V1+V2;                      % Superimpose the voltages since the Maxwell equation is a linear
   relatoin
59 Potential_Distribution(VT,hm,20,1)      % Show the potential distribution in the electrodes
60 [index]=Save_Image(index);
61 Potential_Distribution(V1,hm,20,1)      % Show the potential distribution in the electrodes
62 [index]=Save_Image(index);
63 Potential_Distribution(V2,hm,20,1)      % Show the potential distribution in the electrodes
64 [index]=Save_Image(index);
65 Potential_Distribution(V3,hm,20,1)      % Show the potential distribution in the electrodes
66 [index]=Save_Image(index);
67 Show_Dipole_Placement([0 0 0 0 0 1],hm,8)  % The dipole location and its orientation has been plot
68 [index]=Save_Image(index);
69 Show_Dipole_Placement([0 0 0 1 0 0],hm,8)  % The dipole location and its orientation has been plot

```

```

70 [index]=Save_Image(index);
71 Show_Dipole_Placement([0 0 0 1 0 1],hm,8) % The dipole location and its orientation has been plot
72 [index]=Save_Image(index);
73 %%%
74 % 7 Simulate EEG
75 sourceEEG.loc=[0 -0.05 0.02]; % Input a source at the indicated location
76 sourceEEG.ori=[0 0 1]; % Input the orientation towards z axis
77 f=200; % Sampling frequency
78 RotateFreq=10; % Rotation frequency in time domain
79 Duration=3; % Duration of the EEG signal
80 [EEG]=Simulate_EEG(sourceEEG,hm,f,RotateFreq,Duration);
81 %%
82 [dim1,dim2]=size(EEG);
83 t=linspace(0,3,dim1);
84 figure('units','normalized','outerposition',[0 0 1 1])
85 Vangjush_PlotEEG(EEG',t)
86 title('EEG signals at all the electrodes','FontSize',30)
87 xlabel('Time of measurement in sec','FontSize',30)
88 ylabel('Voltage at each electrode respectively in uV','FontSize',30)
89 set(gca,'FontSize',30);
90 [index]=Save_Image(index);
91 Show_Dipole_Placement([0 -0.05 0.02 0 0 1],hm,8) % The dipole location and its orientation has been plot
92 [index]=Save_Image(index);
93 %%
94 % Potential_Movie(hm,EEG,f)

```

## C.2 Second part

```

1 clear all
2 close all
3 clc
4 %%
5 %
6 load headmodel19 % Load the head model
7 %%
8 sourceEEG1.loc=[0.06 0 0.01]; % Input a source at the indicated location
9 sourceEEG1.ori=[1 0 0]; % Input the orientation towards x axis
10 [V_EEG1,L_EEG1]=Spherical_Head_Model(hm,sourceEEG1); % Compute the voltage done by this potential
11 [Result]=Solve_Inverse_Problem(V_EEG1,hm);% Solve the inverse problem meaning the computation of the dipole
     parameters from the computed dipole
12 index=100;
13 Plot_EE(Result,sourceEEG1,index)
14 [index]=Save_Image(index);
15 PlotRRE(Result(:,7),index) % Plot the set of the RRE values
16 [index]=Save_Image(index);
17 Potential_Distribution(V_EEG1,hm,index,1) % Plot the potential at each electrode
18 [index]=Save_Image(index);
19 %
20 %%
21 sourceEEG2.ori=[1 0 0]; % Input the orientation towards x axis
22 sourceEEG2.loc=[0.06 0 0.01]; % Input a source at the indicated location
23 %
24 [VEEG2,LEEG2]=Spherical_Head_Model(hm,sourceEEG2); % Compute the voltage done by this potential
25 Potential_Distribution(VEEG2,hm,index,1) % Show the computed voltages at each electrode
26 [index]=Save_Image(index);
27 VEEG2Error=VEEG2;
28 VEEG2Error(13)=0; % The P8 electrode is shut down to see the impact
29 Potential_Distribution(VEEG2Error,hm,index,1) % Show the computed voltages at each electrode and the impact of the down electrode
30 [index]=Save_Image(index);
31 VEEG2Error1=VEEG2;
32 VEEG2Error1(3)=0; % The third electrode is shut down to see the impact
33 Potential_Distribution(VEEG2Error1,hm,5,index) % Show the computed voltages at each electrode and the impact of the down electrode
34 [index]=Save_Image(index);
35 %
36 result_point_error=Solve_Inverse_Problem(VEEG2,hm); % The inverse problem is computed in the case when all electrodes are working
37 result_point_error1=Solve_Inverse_Problem(VEEG2Error,hm); % The inverse problem is computed in the case when the p8 electrode is down
38 result_point_error2=Solve_Inverse_Problem(VEEG2Error1,hm); % The inverse problem is computed in the case when the third electrode is down
39 %%
40 PlotRRE([result_point_error(:,7),result_point_error1(:,7),result_point_error2(:,7)],index)
41 legend('RRE all elctrd','RRE of P8 elctrd','RRE of F7 elctrd','Location','northoutside','Orientation','horizontal')
42 title('RRE of the mode')
43 [index]=Save_Image(index);

```

```

44 %
45 Plot_EE(result_point_error,sourceEEG2,index)
46 title('Estimation all electrodes','FontSize',20)
47 [index]=Save_Image(index);
48 Plot_EE(result_point_error1,sourceEEG2,index)
49 title('Estimation error when P8 is off','FontSize',20)
50 [index]=Save_Image(index);
51 Plot_EE(result_point_error2,sourceEEG2,index)
52 title('Estimation error when F7 is off','FontSize',20)
53 [index]=Save_Image(index);
54 %
55 index=110;
56 hm1=hm;
57 hm1.condkull=(1/80)*hm1.condsoft; % The conductivity of the skull is altered to see the impact
58 Nr_Dipoles=10; % The total number of the random dipoles around the
      head is computed
59 [Random_Dipoles]=Generate_Random_Dipole(hm,Nr_Dipoles);
60
61 for i=1:10
62 sourceEEGS.loc(1:3)=Random_Dipoles(i,1:3); % Location of the sources in inputed
63 sourceEEGS.ori(1:3)=Random_Dipoles(i,(1:3)+3); % Orientation of the sources in inputed
64 [A,~]=Spherical_Head_Model(hm1,sourceEEGS); % Voltage at each electrode for this specific dipole is
      computed
65 Estimation1{i}=Solve_Inverse_Problem(A,hm); % Dipole parameters for the computed volatage
      are computed
66 [DOE(i,:),DLE(i,:)]=Plot_EE(Estimation1{i},sourceEEGS,index);
67 a=sprintf('Error estimation with skull conductivity altered for dipole nr %d',i);
68 title(a,'FontSize',20)
69 [index]=Save_Image(index);
70 close all
71 Temp=Estimation1{i};
72 PlotRRE(Temp(:,7),index)
73 a=sprintf('RRE ');
74 title(a);
75 [index]=Save_Image(index);
76 end
77 %
78 str1='Skull';
79 Vangjush_Parameter_2_Latex_Table(Estimation1,str1)
80
81 str1='Skull1';
82 Vangjush_Parameter_2_Latex_Table1(DOE,str1)
83
84 str1='Skull2';
85 Vangjush_Parameter_2_Latex_Table1(DLE,str1)
86 %
87 clear all
88 index=200;
89 load headmodel19
90 hm1=hm;
91 Nr_Dipoles=10; % The total number of the random dipoles around the
      head is computed
92 [Random_Dipoles]=Generate_Random_Dipole(hm,Nr_Dipoles);
93 offset=1e-3;
94 phi=offset*360/2*pi/hm.radius(3);
95 hm1.elpos(1,2)=hm1.elpos(1,2)+1; % The first electrode is displaced by 1 cm
96 for i=1:Nr_Dipoles
97 sourceEEGS.loc(1:3)=Random_Dipoles(i,1:3); % Location of the sources in inputed
98 sourceEEGS.ori(1:3)=Random_Dipoles(i,(1:3)+3); % Orientation of the sources in inputed
99 [A,~]=Spherical_Head_Model(hm1,sourceEEGS); % Voltage at each electrode for this specific dipole is
      computed
100 Estimation1{i}=Solve_Inverse_Problem(A,hm); % Dipole parameters for the computed volatage
      are computed
101 [DOE(i,:),DLE(i,:)]=Plot_EE(Estimation1{i},sourceEEGS,index);
102 a=sprintf('Error estimation with electrode location altered for dipole nr %d',i);
103 title(a,'FontSize',20)
104 [index]=Save_Image(index);
105 close all
106 Temp=Estimation1{i};
107 PlotRRE(Temp(:,7),index)
108 a=sprintf('RRE ');
109 title(a);
110 [index]=Save_Image(index);
111 end
112 str1='Electrode';
113
114 Vangjush_Parameter_2_Latex_Table(Estimation1,str1)
115
116 str1='Electrode1';

```

```

117 Vangjush_Parameter_2_Latex_Table1(DOE,str1)
118
119 str1='Electrode2';
120 Vangjush_Parameter_2_Latex_Table1(DLE,str1)
121 %% 2
122 % Simulate EEG
123 sourceEEG.loc=[0 -0.05 0.02]; % Input a source at the indicated location
124 sourceEEG.ori=[0 0 1]; % Input the orientation towards z axis
125 f=200; % Sampling frequency
126 RotateFreq=10; % Rotation frequency in time domain
127 Duration=3; % Duration of the EEG signal
128 [EEG]=Simulate_EEG(sourceEEG,hm,f,RotateFreq,Duration);
129 %%
130 [dim1,dim2]=size(EEG);
131 t=linspace(0,3,dim1);
132 figure('units','normalized','outerposition',[0 0 1 1])
133 Vangjush_PlotEEG(EEG',t);
134 title('EEG signals at all the electrodes','FontSize',30)
135 xlabel('Time of measurement in sec','FontSize',30)
136 ylabel('Voltage at each electrode respectively in uV','FontSize',30)
137 set(gca,'FontSize',30);
138 [x,y]=ginput(1);
139 V=EEG';
140 Temp=V(:,round(x*f));
141 %%
142 result_point_error=Solve_Inverse_Problem(Temp,hm);
143 str1='EEG';
144 Vangjush_Parameter_2_Latex_Table2(result_point_error,str1)

```

### C.3 Aid functions

```

1 function Bounding(scale,r)
2 %%
3 Bounds=[-scale*r scale*r];
4 xlim(Bounds);
5 ylim(Bounds);
6 zlim(Bounds);
7 end

1 function [RRE,V_in]=CalculateRRE(Results,V_EEG,hm)
2 [dim1,~]=size(Results); % Extract the dimensions of the results , number of dipoles dim1 and
3 % data length dim2
4 for i=1:dim1
5   for j=1:3
6     source.loc(j)=Results(i,j); % Input the location of the source from the first 3 data values
7     source.ori(j)=Results(i,j+3); % Input the orientation of the source from the last 3 data values
8   end
9   [V, ~]=solve_forward(hm,source); % Calculate the forward problem meaning the computation of the
10  voltage
11  V_in(i,:)=V; % Store this values
12  RRE(i)=sum((V-V_EEG).^2)./sum(V.^2); % Compute the RRE value for respective computation
13 end
14 end

1 function [DLE]=Dipole_Location_Error(Loc1,Loc2)
2 %%
3 DLE=sqrt(sum((Loc1-Loc2).^2));
4 end

1 function [DOE]=Dipole_Orientation_Error(Loc1,Loc2)
2 %%
3 d1=sqrt(sum(Loc1.^2));
4 d2=sqrt(sum(Loc2.^2));
5 DOE=acosd(sum(Loc1.*Loc2)/d1/d2);
6 end

1 function c=Dipole_Position_Inverse(dp,hm,V)
2 %%
3 ndip=size(dp,1);
4 L=zeros(size(V,1),3*ndip);
5 for i=1:ndip
6   source.loc=dp(i,:);
7   [~,L]=Spherical_Head_Model(hm,source);
8 end
9 c=norm((eye(size(V,1))-L*pinv(L))*V,'fro')/norm(V,'fro');
10 return;

```

```

1 function Draw_Nouse(r,Font1)
2 %
3 plot3(r*0,r*1.1,r*-0.2,'r.','MarkerSize',100)
4 text(r*0,r*1.41,r*-0.2,'Nouse','FontSize',Font1);
5 end

1 function DrawSphere(Nr_Points,r)
2 %
3 [X,Y,Z]=sphere(Nr_Points);
4 s1=surf(r*X,r*Y,r*Z);
5 set(s1,'FaceColor',[0.9 0.9 0.9],'EdgeColor','green');
6 set(s1,'FaceColor',[0 1 1],'EdgeColor','red');
7 set(s1,'FaceAlpha', 0.1)
8 shading interp
9 light
10 end

1 function Electrode_Names(Head_Model,r,Font)
2 %
3 Element_Position=Head_Model.elpos;
4 Electrode_Names=Head_Model.meas;
5 %
6 Electr_Position_Cartesian=Spherical_To_Cartesian_Coordinate([Element_Position, r*ones(length(Element_Position),1)]');
7 Electr_Position_Cartesian.text=Spherical_To_Cartesian_Coordinate([Element_Position, r*(ones(length(Element_Position),1)+0.3)]);
8
9 for i=1:size(Electr_Position_Cartesian,2)
10   text(Electr_Position_Cartesian.text(1,i)',Electr_Position_Cartesian.text(2,i)',...
11     Electr_Position_Cartesian.text(3,i)' + r*0.011,...[num2str(i) ' ', Electrode_Names.el.lbl{i}], 'FontSize',Font);
12 end
13 end

1 function Electrode_Position_V(Head_Model,~)
2 %
3 % figure(nr_fig)
4 figure('units','normalized','outerposition',[0 0 1 1])
5 r=Head_Model.radius(end);
6 Nr_Points=20;
7 Font1=20;
8 Font=30;
9 scale=1.5;
10 manner='filled';
11
12 DrawSphere(Nr_Points,r)
13 hold on
14
15 Position_Of_Electrodes(Head_Model,r,manner);
16 Electrode_Names(Head_Model,r,Font)
17
18 Draw_Nouse(r,Font1);
19
20 Labeling(Font)
21 title('Electrode distribution in head','FontSize',Font);
22 Bounding(scale,r);
23 set(gca,'FontSize',Font);
24 end

1 function [DOE,DLE]=Estimation_Error(Result,sourceEEG1)
2 %
3 for i=1:min(size(Result))
4   DOE(i)=Dipole_Orientation_Error(Result(i,4:6),sourceEEG1.ori);
5   DLE(i)=Dipole_Location_Error(Result(i,1:3),sourceEEG1.loc);
6 end
7 end

1 function [Random_Dipoles]=Generate_Random_Dipole(hm,Nr_Dipoles)
2 %
3 Random_Dipoles=zeros(Nr_Dipoles,3);
4 center=hm.center;
5 h=waitbar(0,'Generating random dipoles inside head model');
6 for l=1:Nr_Dipoles
7   i=hm.radius(1);
8   j=hm.radius(1);
9   k=hm.radius(1);
10  while(sqrt(sum(([i-center(1),j-center(2),k-center(3)].^2)))>hm.radius(1))
11    i=rand(1);
12    j=rand(1);

```

```

13     k=rand(1);
14 end
15 Random_Dipoles(1,1:3)=[i j k];
16 Random_Dipoles(1,4:6)=[randi([0 1],1,1) randi([0 1],1,1) randi([0 1],1,1)];
17
18 waitbar(1/Nr_Dipoles ,h)
19 end
20 delete(h)
21 end

```

```

1 function [Random_Dipoles]=Generate_Random_Dipoles(hm,Nr_Dipoles)
2 %
3 Random_Dipoles=zeros(Nr_Dipoles,3);
4 center=hm.center;
5 Random_Dipoles(1,1:3)=center;
6 h=waitbar(0,'Generating random dipoles inside head model');
7 for l=2:Nr_Dipoles
8     i=hm.radius(1);
9     j=hm.radius(1);
10    k=hm.radius(1);
11    while(sqrt(sum(([i-center(1),j-center(2),k-center(3)].^2)))>hm.radius(1))
12        i=rand(1);
13        j=rand(1);
14        k=rand(1);
15    end
16    Random_Dipoles(l,1:3)=[i j k];
17    waitbar(1/Nr_Dipoles ,h)
18 end
19 delete(h)
20 end

```

```

1 function [R,d]=GenerateDipole(x,r)
2 R=zeros(x,6); % Initialization of the dipole data consistently to the dimensions
3 for i=1:x
4     [y,d(i)]=RandomInsideSphere(r); % Generate randomly location coordinate of the dipole within the sphere
        where the radius is the smalles in the Head Modes
5     for j=1:3
6         R(i,j)=y(j); % Input data into the matrix
7     end
8     for j=1:3
9         x=randsample(1*1000,1)/1000;% Generate randomly the orientation of the dipole
10        R(i,j+3)=x; % Input data into the matrix
11    end
12 end
13 end

```

```

1 function [RotateFreqRad_Inter,TimeArray]=GenerateTimeSeries(f, RotateFreq, Duration)
2 % f=200; % Compt the period of sampling from the sampling frequency
3 T=1/f; % Time array of the sampling
4 TimeArray=0:T:Duration; % Removing the last sample in time since we start from 0 sec
5 TimeArray(end)=[]; % %
6 % T_Retota=1/ RotateFreq; % Compute the rotation period in sec
7 RotateAngle=0:T_Retota:20*Duration; % Compute the array of the rotation in sec
8 RotateAngle(end)=[]; % Removing the last sample in time since we start from 0 sec
9 RotateFreqRad=RotateAngle*pi; % Compute the array of rotation angle in rad
10 % %
11 A=length(RotateFreqRad); % Length of the rotate angle array
12 B=length(TimeArray); % Length of the time array
13 % A1=rem(B,A); % Division residue between this data
14 B1=round(B/A); % The scale of data size between this two data
15 RotateFreqRad_Inter=interp(RotateFreqRad,B1);
16 end

```

```

1 function Labeling(FontSize)
2 xlabel('X (m)', 'FontSize',FontSize);
3 ylabel('Y (m)', 'FontSize',FontSize);
4 zlabel('Z (m)', 'FontSize',FontSize);
5 set(gca, 'FontSize',FontSize);
6 end

1 function [Control]=Localization_Error(Dipole,HeadModel,Voltage)
2 %
3 Number_Dipoles=size(Dipole,1);
4 % Lead_Field_Matrix=zeros(size(V,1),3*Number_Dipoles);
5 %
6 for i=1:Number_Dipoles
7     source.loc=Dipole(i,:);
8     [~,Lead_Field_Matrix]=solve_forward(HeadModel,source);

```

```

9 Control(i)=norm((eye(size(Voltage,1))-Lead_Field_Matrix*pinv(Lead_Field_Matrix))*Voltage,'fro')/norm(
10 Voltage,'fro');
11 end
12 Control=sum(Control(i));
13 end

1 function [Result]=Minimize_Function(Random_Dipoles,HeadModel,V)
2 %
3 h=waitbar(0,'Locating the sources');
4 Nr_Dipoles=size(Random_Dipoles,1);
5 for i=1:Nr_Dipoles
6 % Location calculation
7 [Result(i,1:3),Voltage]=fminsearch('Localization_Error',Random_Dipoles(i,1:3),optimset('TolX',1.e-4,
8 'TolFun',1.e-5,'Display','off','MaxFunEvals',100000,'MaxIter',10000),HeadModel,V);
9 % Orientation calculation
10 source.loc=Result(i,1:3);
11 [~,L]=solve_forward(HeadModel,source);
12 Orientation=pinv(L)*V;
13 Orientation_Nomalized=Orientation./norm(Orientation);
14 Result(i,4:6)=[Orientation_Nomalized(1),Orientation_Nomalized(2),Orientation_Nomalized(3)];
15 Result(i,7)=Voltage;
16 waitbar(i/Nr_Dipoles,h);
17 end
18 delete(h);
19 end

1 function Poly_Leng_L=PLG(Leng, mode, Value)
2 %
3 if (mode < 0 || mode > Leng || abs(Value) > 1.0)
4 disp('Bad arguments in routine plgndr')
5 Poly_Leng_L=NaN;
6 return ;
7 end
8 temp4=1;
9 if (mode > 0)
10 somx2=sqrt(1-Value.^2);
11 temp=cumsum([1,2*ones(1,mode-1)]);
12 temp1=-somx2*(temp);
13 temp3=cumprod(temp1);
14 temp4=temp3(end);
15 end
16 if (Leng== mode)
17 Poly_Leng_L=temp4;
18 return ;
19 else
20 temp5=Value*(2*mode+1)*temp4;
21 if (Leng == (mode+1))
22 Poly_Leng_L=temp5;
23 return ;
24 else
25 for i=mode+2:Leng
26 Poly_Leng_L=(Value*(2*i-1)*temp5-(i+mode-1)*temp4)/(i-mode);
27 temp4=temp5;
28 temp5=Poly_Leng_L;
29 end
30 end
31 end

1 function [DOE,DLE]=Plot_EE(Result,sourceEEG1,~)
2 %
3 [DOE,DLE]=Estimation_Error(Result,sourceEEG1);
4 figure('units','normalized','outerposition',[0 0 1 1])
5 X=1:length(DOE);
6 [hAx,~,~]=plotyy(X,DOE,X,DLE);
7 title('Estimation Error','FontSize',20)
8 xlabel('Dipole number','FontSize',20)
9 ylabel(hAx(1),'DOE [deg]','FontSize',15) % left y-axis
10 ylabel(hAx(2),'DLE [m]','FontSize',15) % right y-axis
11 set(hAx,'FontSize',15);
12
13 end

1 function Plot_Electrode_Potential(V,nr)
2 figure(nr),plot(V,'x','LineWidth',13),hold on,plot(V,'r','LineWidth',3)
3 xlabel('Electrode Number','FontSize',20)
4 ylabel('Voltage [uV]','FontSize',20)
5 title('Electrode potential','FontSize',20)
6 set(gca,'fontsize', 20);
7 end

```

```

1 function PlotEEG(sig ,t)
2 % t = linspace(0,2,1024);
3 % sig = rand(32,1024);
4 [dim1,dim2]=size(sig);
5 % calculate shift
6 mi = min(sig,[],2);
7 ma = max(sig,[],2);
8 shift = cumsum([0; abs(ma(1:end-1))+abs(mi(2:end))]);
9 shift = repmat(shift ,1 ,dim2);
10
11 %plot 'eeg' data
12 plot(t,sig+shift)
13
14 % edit axes
15 set(gca , 'ytick' ,mean(sig+shift ,2) , 'yticklabel' ,1:dim1)
16 grid on
17 % ylim ([mi(1) max(max(shift+sig))])
18
19 end

```

```

1 function PlotPotemtialMap(V_in,hm)
2 [dim1, ~]=size(V_in);
3 for i=1:dim1
4 a=sprintf('Estiantion %d',i);
5 showpotentials(V_in(i,:)',hm)
6 title(a)
7 end
8 end

```

```

1 function PlotRRE(RRE,~)
2 %
3 % figure(Nr)
4 figure('units','normalized','outerposition',[0 0 1 1])
5 plot(RRE,'x','LineWidth',10)
6 hold on
7 plot(RRE,'o','LineWidth',10)
8 hold on
9 plot(RRE,'r','LineWidth',3)
10 xlabel('Solutions trials','FontSize',20);
11 ylabel('Error value in [A.u]','FontSize',20);
12 title('RRE plot for respective dipole','FontSize',20);
13 set(gca , 'FontSize',20);
14 end

```

```

1 function PlotSIR(SNR,F1)
2 figure
3 plot(SNR,F1,'x')
4 hold on
5 plot(SNR,F1,'o')
6 hold on
7 plot(SNR,F1,'r')
8 xlabel('SNR trial'),ylabel('SIR')
9 end

```

```

1 function Position_Of_Electrodes(hm,r,manner)
2 %
3 Elect_Postion=Spherical_To_Cartesian_Coordiante([hm.elpos(:,1)'; hm.elpos(:,2)'; r*ones(size(hm.elpos(:,2)))']);
4 X_el=Elect_Postion(1,:);
5 Y_el=Elect_Postion(2,:);
6 Z_el=Elect_Postion(3,:);
7 S = 500*ones(size(X_el));
8 C = 500*ones(size(X_el));
9 scatter3(X_el,Y_el,Z_el,S,C,manner),view(-90,90)
10 end

```

```

1 function Potential_Distribution(V,Head_Model,~,barcolor)
2 %
3 scale=1.5;
4 Font=20;
5
6 % figure(Nr_Fig)
7 figure('units','normalized','outerposition',[0 0 1 1])
8 set(axes , 'NextPlot' , 'add');
9 r=Head_Model.radius(end);
10 [X,Y,Z]=sphere(50);
11 fvc=surf2patch(r*X,r*Y,r*Z);
12 manner='ko';
13

```

```

14 Position_Of_Electrodes(Head_Model,r,manner)
15 Electrode_Names(Head_Model,r,Font-5)
16
17 Se=Spherical_To_Cartesian_Coordinate([Head_Model.elpos(:,1)'; Head_Model.elpos(:,2)'; r*1.17*ones(size(Head_Model.elpos(:,2)))']);
18 F=TriScatteredInterp(Se(1,:)',Se(2,:)',Se(3,:)',V);
19 VI=F(fvc.vertices(:,1),fvc.vertices(:,2),fvc.vertices(:,3));
20 pl=patch(fvc);
21 set(pl,'FaceColor','interp','EdgeColor','none','FaceVertexCData',VI);
22
23
24 lightangle(-45,30)
25 h.FaceLighting='gouraud';
26 h.AmbientStrength=0.3;
27 h.DiffuseStrength=0.8;
28 h.SpecularStrength=0.9;
29 h.SpecularExponent=25;
30 h.BackFaceLighting='unlit';
31
32 if barcolor==1
33 c=colorbar('westoutside');
34 % c=colorbar('AxisLocation','in')
35 c.Label.String='Potential distribution';
36 end
37 Draw_Nouse(r,Font);
38 Labeling(Font)
39 Bounding(scale,r);
40 view(-90,90)
41 end

```

```

1 function Potential_Movie(Head_Model,EEG,fs)
2 %
3 a=size(EEG);
4 for i=1:max(a);
5 Potential_Distribution(EEG(i,:)',Head_Model,30,0)
6 drawnow;
7 pause(1/fs);
8 end
9 end

```

```

1 function [x,y]=RandomInsideSphere(r)
2 for i=1:3
3 x(i)=randsample(r*9000,1)/10000; %Randomly generate three different value within the range o to the
radius which has been put as an input
4 end
5
6 while(sqrt(sum(x.^2))>=r) % If the initial distance from the center [0 0 0] is outside the sphere
, re initialize another sample.
7 for i=1:3 %Keep on doing this till the condition is meet
8 x(i)=randsample(r*9000,1)/10000;
9 end
10 end
11 y=sqrt(sum(x.^2));
12 end

```

```

1 function [B]=RotateDipole(A,x,y,z)
2
3 Rotate_y=[cos(-y) 0 -sin(-y);0 1 0;sin(-y) 0 cos(-y)];
4 Rotate_x=[1 0 0;0 cos(x) sin(x);0 -sin(x) cos(x)];
5 Rotate_z=[0 cos(z) -sin(z);sin(z) cos(z) 0;0 0 1];
6 Total_Rotation_Matrix=Rotate_x;%*Rotate_y;%*Rotate_z;
7 B=Total_Rotation_Matrix*A;
8
9
10 end

```

```

1 function [index]=Save_Image(index)
2 %
3 File=sprintf('.jpg');
4 Name=strcat('C:\Users\vkomin1\Dropbox\Apps\ShareLaTeX\Katholieke university of Leuven\Bio-Medical Data
Processing part II\A4\Images4\',num2str(index),File);
5 % saveas(gcf,Name)
6 index=index+1;
7 close all
8 end

1 function Show_Dipole_Placement(dipole,Head_Model,Nr_Fig)
2 %
3 Font=20;

```

```

4 Nr_Points=20;
5 scale=1.5;
6 manner='filled';
7 % figure(Nr_Fig)
8 figure('units','normalized','outerposition',[0 0 1 1])
9 r=Head_Model.radius(end);
10 set(axes,'NextPlot','add');
11
12 DrawSphere(Nr_Points,r)
13 Draw_Nouse(r,Font);
14
15 Position_Of_Electrodes(Head_Model,r,manner)
16 Electrode_Names(Head_Model,r,Font)
17
18 %plot dipoles
19 for i=1:size(dipole,1)
20     dipole(i,4:6)=0.3*r*dipole(i,4:6)./norm(dipole(i,4:6));
21     plot3(dipole(i,1),dipole(i,2),dipole(i,3),'g','MarkerSize',50);
22     plot3([dipole(i,1) dipole(i,1)+dipole(i,4)],...
23            [dipole(i,2) dipole(i,2)+dipole(i,5)],...
24            [dipole(i,3) dipole(i,3)+dipole(i,6)],'b','LineWidth',3);
25     a=8e-4*max([dipole(i,1),dipole(i,2),dipole(i,3)]);
26     text(dipole(i,1)+a,dipole(i,2)+a,dipole(i,3)+a,'Dipole','FontSize',Font);
27 end
28
29 Labeling(Font)
30 title('Dipole locations','FontSize',Font);
31 Bounding(scale,r);
32 set(gca,'FontSize',Font);
33 view(3)
34 end

```

```

1 function [EEG]=Simulate_EEG(sourceEEG,hm,f,RotateFreq,Duration)
2 %
3 [RotateFreqRadRelicated,~]=GenerateTimeSeries(f, RotateFreq, Duration); % Compute the array of the rotation
4 angles
5 for i=1:length(RotateFreqRadRelicated)
6     Rotation=[0 sin(RotateFreqRadRelicated(i)) cos(RotateFreqRadRelicated(i))];%RotateDipole(sourceEEG.ori
7 , RotateFreqRadRelicated(i),0,0) % Rotation the dipole consistently to the rotation angles
8 sourceEEG.ori=Rotation;
9 [EEG(:, :) ,~]=Spherical_Head_Model(hm,sourceEEG); % Compute the voltage done by this
10 potential
11 end
12 end

```

```

1 function [Result]=Solve_Inverse_Problem(V,Head_Model)
2 %
3 % Generate 5 random dipoles
4 n=5;
5 [Random_Dipole]=Generate_Random_Dipoles(Head_Model,n);
6 for i=1:n
7     [Result(i,1:3),RRE]=fminsearch('Dipole_Position_Inverse',Random_Dipole(i,1:3),optimset('TolX',1.e-4,
8 'TolFun',1.e-5,'Display','off','MaxFunEvals',100000,'MaxIter',10000),Head_Model,V);
9     source.loc=Result(i,1:3);
10    % source.ori=Result(i,4:3);
11    [~,L]=Spherical_Head_Model(Head_Model,source);
12    Orientation=pinv(L)*V;
13    Orientation=Orientation./norm(Orientation);
14    Result(i,4:6)=Orientation;
15    Result(i,7)=RRE;
16 end

```

```

1 function Result=Solve_Inverse_Problem_Dipole_Ana(V,hm)
2 %
3 n=5;
4 [Random_Dipoles]=Generate_Random_Dipoles(hm,n);
5 [Result]=Minimize_Function(Random_Dipoles,hm,V);
6 end

```

```

1 function [V,L]=Spherical_Head_Model(Head_Model,source)
2 %
3 Location=source.loc;
4 Electrode_position=Head_Model.elpos;
5 Radiuses=Head_Model.radius;
6 X=Head_Model.condratio;
7 S=Head_Model.condsoft;
8 rhead=Radiuses(3);
9 r2=rhead;

```

```

10
11 f1=Radiuses(1)/Radiuses(3);
12 f2=Radiuses(2)/Radiuses(3);
13
14 K1=1/(4*pi*S*rhead^2);
15
16
17
18 NOFTERMS=80;
19
20 theta=Electrode_position(:,1);
21 phi=Electrode_position(:,2);
22 Nr_Of_Electrodes=length(theta);
23
24
25
26
27 Tx=zeros(Nr_Of_Electrodes,1);% Tangent component along X
28 Ty=zeros(Nr_Of_Electrodes,1);% Tangent component along Y
29 Tz=zeros(Nr_Of_Electrodes,1);% Tangent component along Z
30
31 t=zeros(Nr_Of_Electrodes,1);
32 q=zeros(Nr_Of_Electrodes,1);
33 R2=zeros(Nr_Of_Electrodes,3);
34 cosalpha=zeros(Nr_Of_Electrodes,1);
35
36 V=zeros(Nr_Of_Electrodes,1);
37 Vx=zeros(Nr_Of_Electrodes,1);
38 Vy=zeros(Nr_Of_Electrodes,1);
39 Vz=zeros(Nr_Of_Electrodes,1);
40
41 for i=1:Nr_Of_Electrodes
42     R2(i,1)=rhead*sin(theta(i))*cos(phi(i));
43     R2(i,2)=rhead*sin(theta(i))*sin(phi(i));
44     R2(i,3)=rhead*cos(theta(i));
45 end
46
47
48 R1=Location;
49 r1=sqrt( R1(1)^2+R1(2)^2+R1(3)^2 );
50 if r1~=0
51     %% Computation of Tangential and Radial components
52     b=r1/rhead;
53     p=r1^2;
54     for i=1:Nr_Of_Electrodes
55         q(i)=R1(1)*R2(i,1) + R1(2)*R2(i,2)+ R1(3)*R2(i,3);
56         cosalpha(i)=q(i)./r1./r2;
57         if (abs(cosalpha(i))>1.0)
58             cosalpha(i)=cosalpha(i)/abs(cosalpha(i));
59         end
60         Tx(i)=R2(i,1)*p - R1(1)*q(i);
61         Ty(i)=R2(i,2)*p - R1(2)*q(i);
62         Tz(i)=R2(i,3)*p - R1(3)*q(i);
63         t(i)=sqrt(sum([Tx(i) Ty(i) Tz(i)].^2));
64         if (t(i)~=0)
65             Tx(i)=Tx(i)/t(i);
66             Ty(i)=Ty(i)/t(i);
67             Tz(i)=Tz(i)/t(i);
68         end
69     end
70     Rx=R1(1)/r1;% Radial component along X
71     Ry=R1(2)/r1;% Radial component along Y
72     Rz=R1(3)/r1;% Radial component along Z
73
74     %% 
75     for i=1:NOFTERMS
76         i1=2*i+1;
77         gi=((i+1)*X+i)*(i*X/(i+1)+1) + (1-X)*((i+1)*X+i)*(f1^i1-f2^i1) - ...
78         i*(1-X)*(1-X)*(f1/f2)^i1;
79         fact1=X*i1^3*b^(i-1)/gi/(i+1)/i;
80         for j=1:Nr_Of_Electrodes
81             fact2=i*PLG(i,0,cosalpha(j));
82             fact3=-PLG(i,1,cosalpha(j));
83             % fact2=i*legendre(i,cosalpha(j));
84             % fact3=-legendreP(i,cosalpha(j));
85             Vx(j)=Vx(j)+fact1*(fact2*Rx+fact3*Tx(j));
86             Vy(j)=Vy(j)+fact1*(fact2*Ry+fact3*Ty(j));
87             Vz(j)=Vz(j)+fact1*(fact2*Rz+fact3*Tz(j));
88         end

```

```

89     end
90 else
91     i=1; i1=2*i+1;
92     gi=((i+1)*X+i)*(i*X/(i+1)+1) + (1-X)*((i+1)*X+i)*(f1^i1-f2^i1) -...
93         i*(1-X)*(1-X)*(f1/f2)^i1;
94     fact1=X*i1^3^(i-1)/gi/(i+1)/i;
95     for j=1:Nr_Of_Electrodes
96         Vx(j)=fact1*PLG(1,0,R2(j,1)/r2);
97         Vy(j)=fact1*PLG(1,0,R2(j,2)/r2);
98         Vz(j)=fact1*PLG(1,0,R2(j,3)/r2);
99         % Vx(j)=fact1*legendre(1,R2(j,1)/r2);
100        % Vy(j)=fact1*legendre(1,R2(j,2)/r2);
101        % Vz(j)=fact1*legendre(1,R2(j,3)/r2);
102    end
103 end
104 %% 
105 Voltage_Ref=zeros(Nr_Of_Electrodes,3);
106 for i=1:Nr_Of_Electrodes
107     Voltage_Ref(i,:)=[Vx(i) Vy(i) Vz(i)];
108 end
109
110 % average referencing
111 Voltage_Ref = Voltage_Ref-ones(Nr_Of_Electrodes,1)*sum(Voltage_Ref)/Nr_Of_Electrodes;
112 L=K1*Voltage_Ref*1e-3;
113 if 1 < length(fieldnames(source))
114     V=L*source.ori';
115 else
116     V=[];
117 end
118 end

```

```

1 function Cartesian_Coordinates=Spherical_To_Cartesian_Coordiante(Sphere_Coord)
2 Azimuth=Sphere_Coord(1,:);
3 Elevation=Sphere_Coord(2,:);
4 Radius=Sphere_Coord(3,:);
5 %% 
6 x=Radius.*cos(Elevation).*sin(Azimuth);
7 y=Radius.*sin(Elevation).*sin(Azimuth);
8 z=Radius.*cos(Azimuth);
9 %% 
10 Cartesian_Coordinates(1,:)=x;
11 Cartesian_Coordinates(2,:)=y;
12 Cartesian_Coordinates(3,:)=z;
13 end

```

```

1 function Vangjush_Parameter_2_Latex_Table(Control,str1)
2 %% LLE
3 name_file=strcat('C:\Users\vkomin1\Dropbox\Apps\ShareLaTeX\Katholieke university of Leuven\Bio-Medical Data
4 Processing part II\A4\Files\',str1,'.txt');
4 fileID = fopen(name_file,'w');
5 fprintf(fileID, '%s', '\hline');
6 for i=1:10
7     Temp=Control{i};
8     for j=1:5
9         fprintf(fileID, '$Tria%d%d$&$', i,j);
10        for k=1:7
11            if k<7
12                fprintf(fileID, '%6.2e$&$',Temp(j,k));
13            end
14            if k==7
15                fprintf(fileID, '%6.2e$\backslash\backslash\backslash$',Temp(j,k));
16            end
17        end
18        fprintf(fileID, '%s', '\hline');
19    end
20 end
21 fprintf(fileID, '\n');
22 fclose(fileID);
23 %% 
24 end

```

```

1 function Vangjush_Parameter_2_Latex_Table1(Control,str1)
2 %% 
3 name_file=strcat('C:\Users\vkomin1\Dropbox\Apps\ShareLaTeX\Katholieke university of Leuven\Bio-Medical Data
4 Processing part II\A4\Files\',str1,'.txt');
4 fileID = fopen(name_file,'w');
5 fprintf(fileID, '%s', '\hline');
6 for j=1:10
7     fprintf(fileID, '$Trial%d$&$', j);

```

```

8   for k=1:5
9     if k<5
10       fprintf(fileID , '%6.2e$$' , Control(j ,k));
11     end
12     if k==5
13       fprintf(fileID , '%6.2e$\backslash\backslash' , Control(j ,k));
14     end
15   end
16   fprintf(fileID , '%s' , ' \hline ');
17 end
18 fprintf(fileID , '\n');
19 fclose(fileID);
20 %%
21 end

1 function Vangjush_Parameter_2_Latex_Table2(Control ,str1)
2 %%
3 name_file=strcat ('C:\Users\vkomin1\Dropbox\Apps\ShareLaTeX\Katholieke university of Leuven\Bio-Medical Data
4 Processing part II\A4\Files\' ,str1 ,'.txt');
5 fileID = fopen(name_file , 'w');
6 fprintf(fileID , '%s' , ' \hline ');
7 for j=1:5
8   fprintf(fileID , '$D%d$$' ,j );
9   for k=1:7
10     if k<7
11       fprintf(fileID , '%6.2e$$' , Control(j ,k));
12     end
13     if k==7
14       fprintf(fileID , '%6.2e$\backslash\backslash' , Control(j ,k));
15     end
16   end
17   fprintf(fileID , '%s' , ' \hline ');
18 end
19 fprintf(fileID , '\n');
20 fclose(fileID);
21 %%
22 end

1 function Vangjush_PlotEEG(sig ,t)
2 %%
3 % t=0:size(sig ,2)-1;
4 [dim1 ,dim2]=size(sig );
5 mi = min(sig ,[] ,2);
6 ma = max(sig ,[] ,2);
7 shift1 = cumsum([0; abs(ma(1:end-1))+abs(mi(2:end))]);
8 shift = repmat(shift1 ,1 ,dim2);
9 plot(t ,sig+shift , 'LineWidth' ,2)
10 set(gca , 'ytick' ,mean(sig+shift ,2) , 'yticklabel' ,1:dim1)
11 grid on
12 end

```