

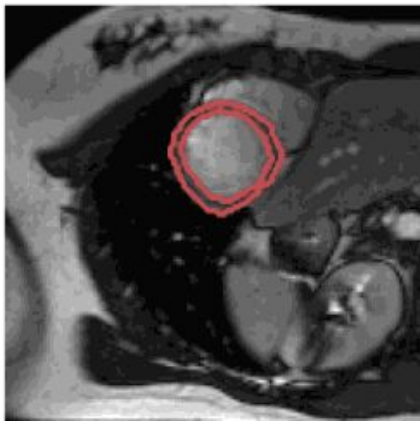


Adaptive Correspondence Scoring for Unsupervised Medical Image Registration

Xiaoran Zhang, John C. Stendahl, Lawrence Staib, Albert J. Sinusas, Alex Wong, James S. Duncan

Yale University

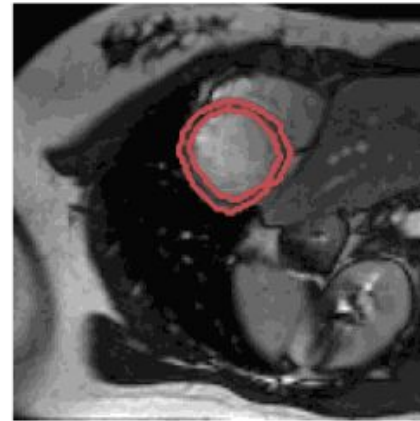
Tracking Anatomies Over Time



MRI video with only
ED label



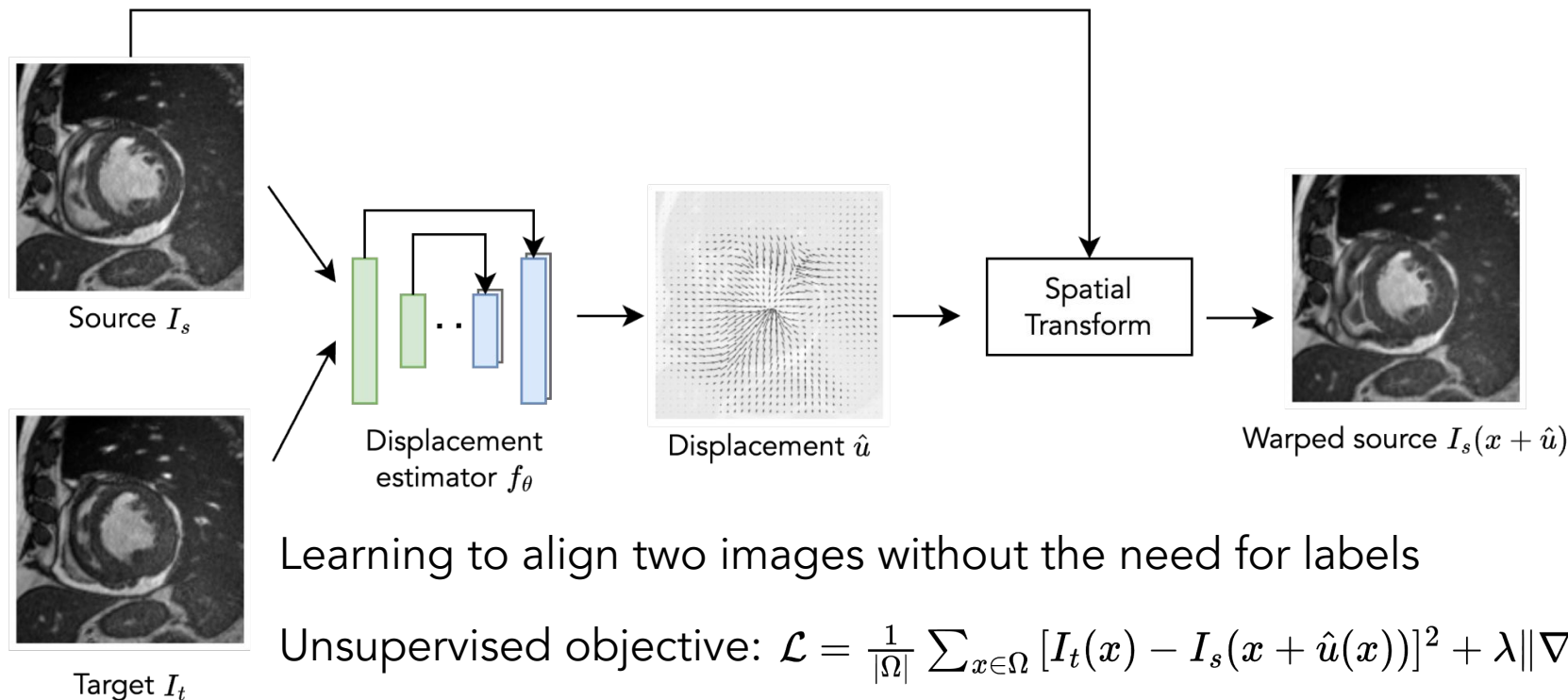
Estimated displacement



MRI video with
propagated labels

Unsupervised image registration enables accurate tracking of changes, label propagation, improved diagnosis, and enhanced treatment planning.

Unsupervised Image Registration

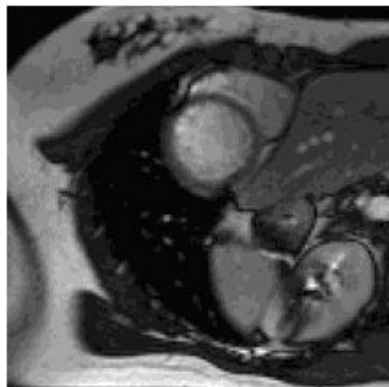


Learning to align two images without the need for labels

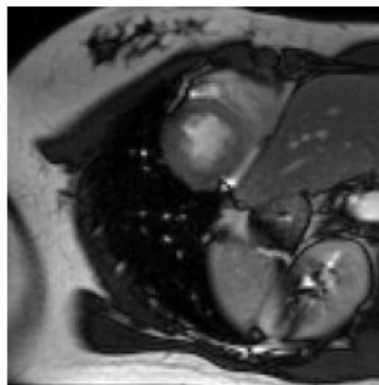
Unsupervised objective: $\mathcal{L} = \frac{1}{|\Omega|} \sum_{x \in \Omega} [I_t(x) - I_s(x + \hat{u}(x))]^2 + \lambda \|\nabla \hat{u}(x)\|^2$

Violations of Basic Assumptions

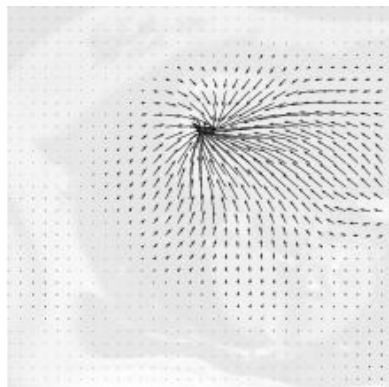
MRI video



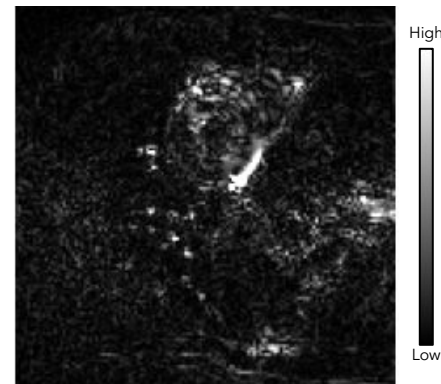
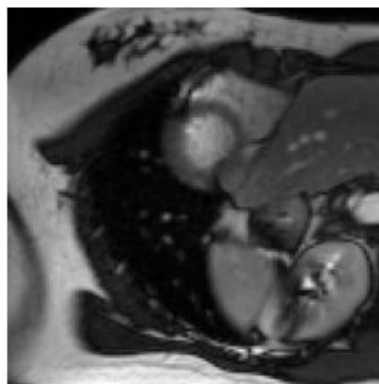
Target



Displacement between
first and last frame



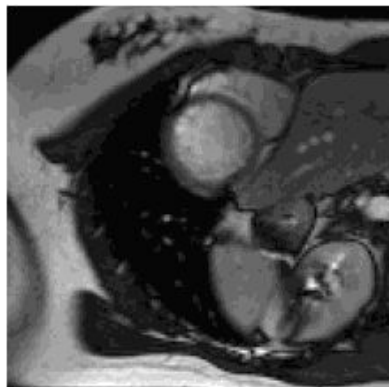
Reconstructed target



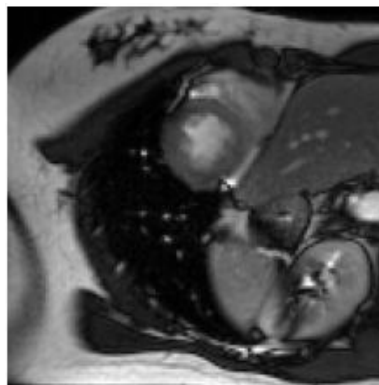
Error map

Violations of Basic Assumptions

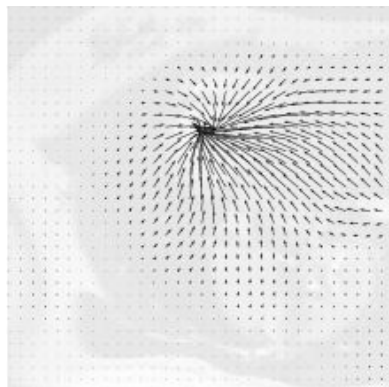
MRI video



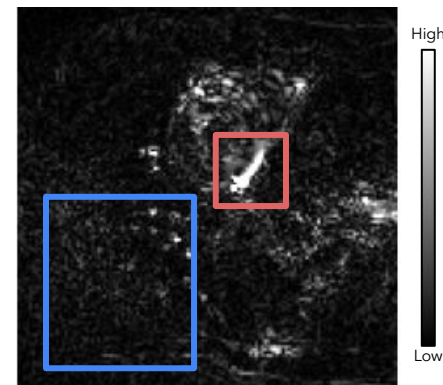
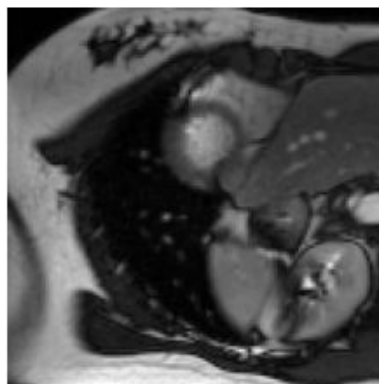
Target



Displacement between
first and last frame



Reconstructed target



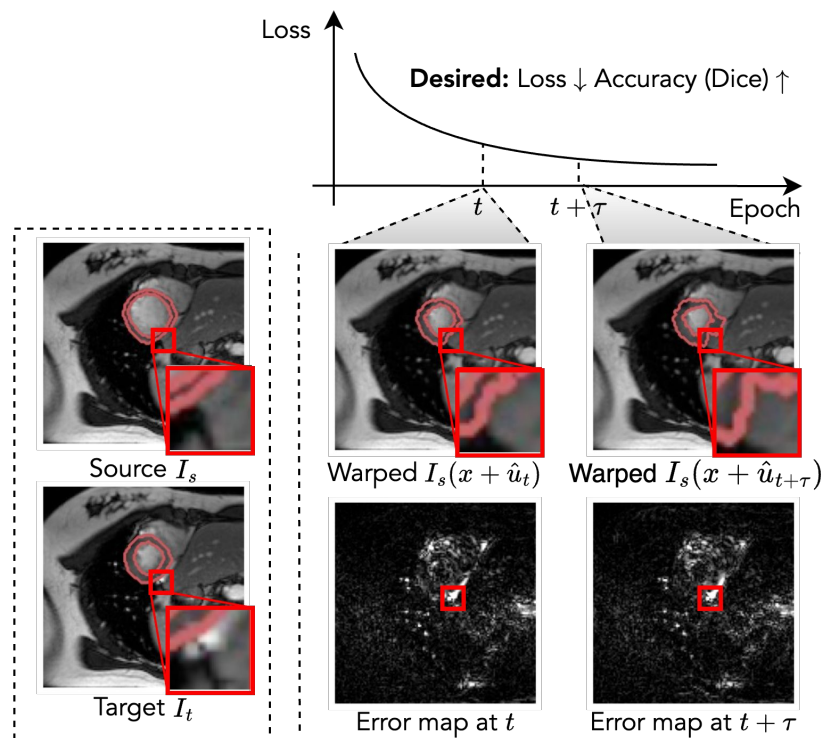
Error map

Occlusions

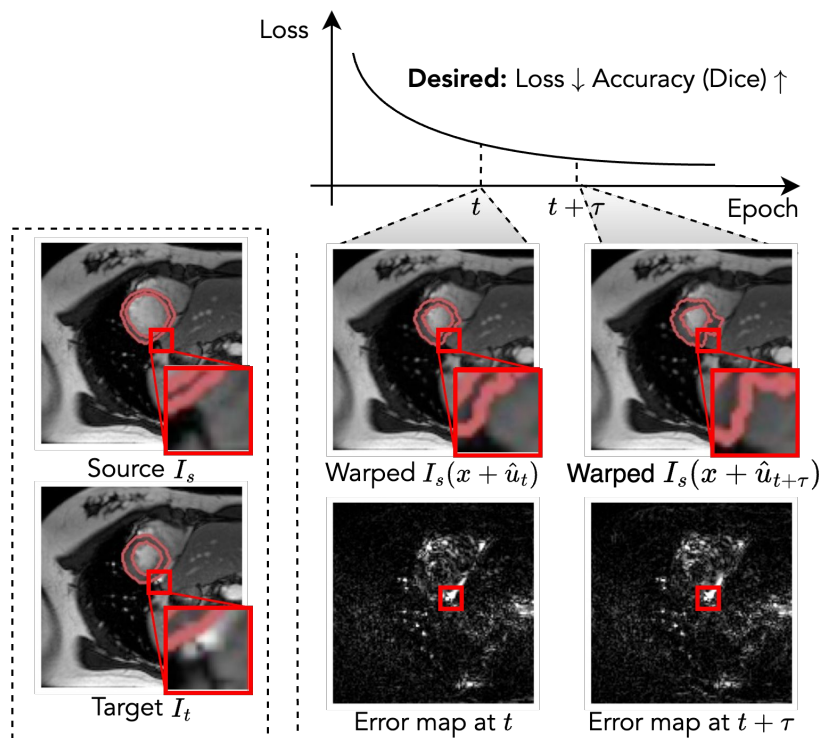
Heteroscedastic noise

... and many others

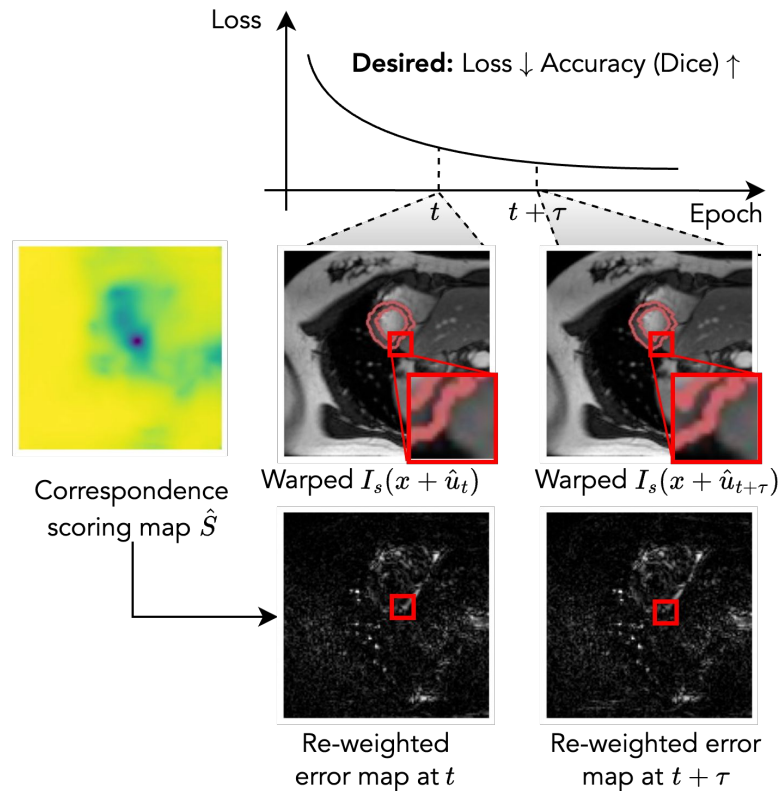
A Closer Look



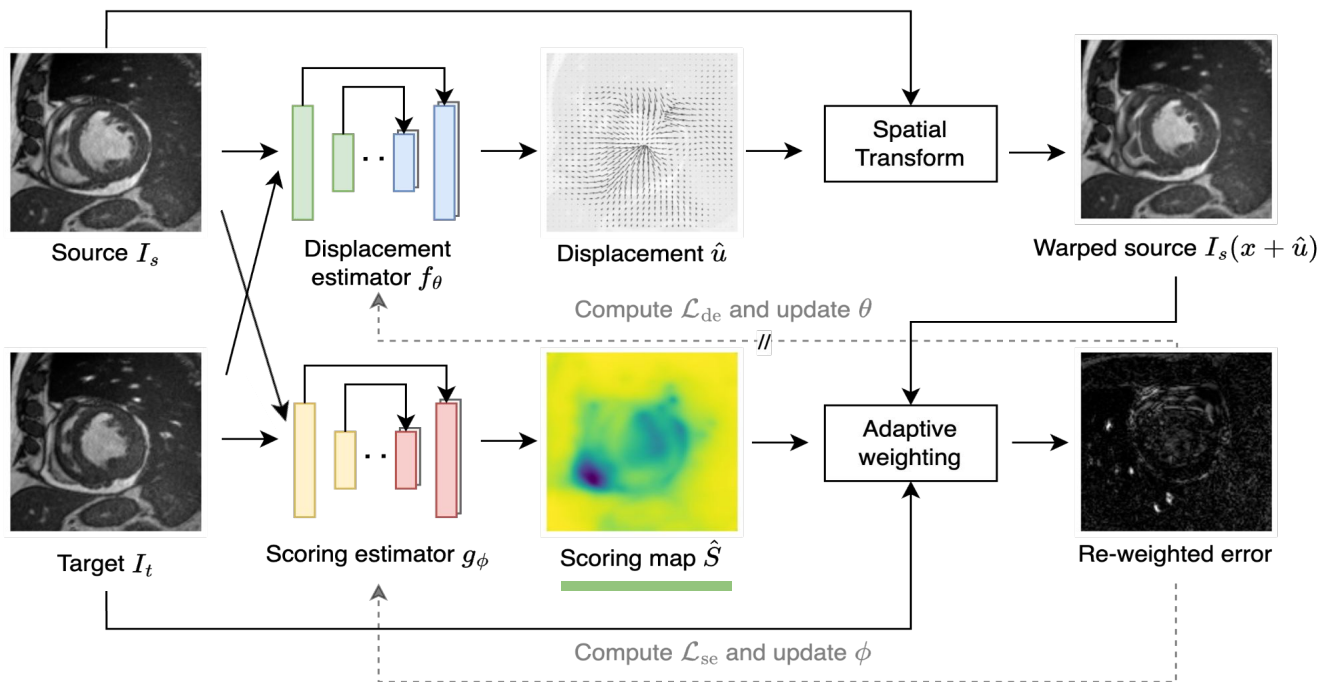
A Closer Look



Our approach:



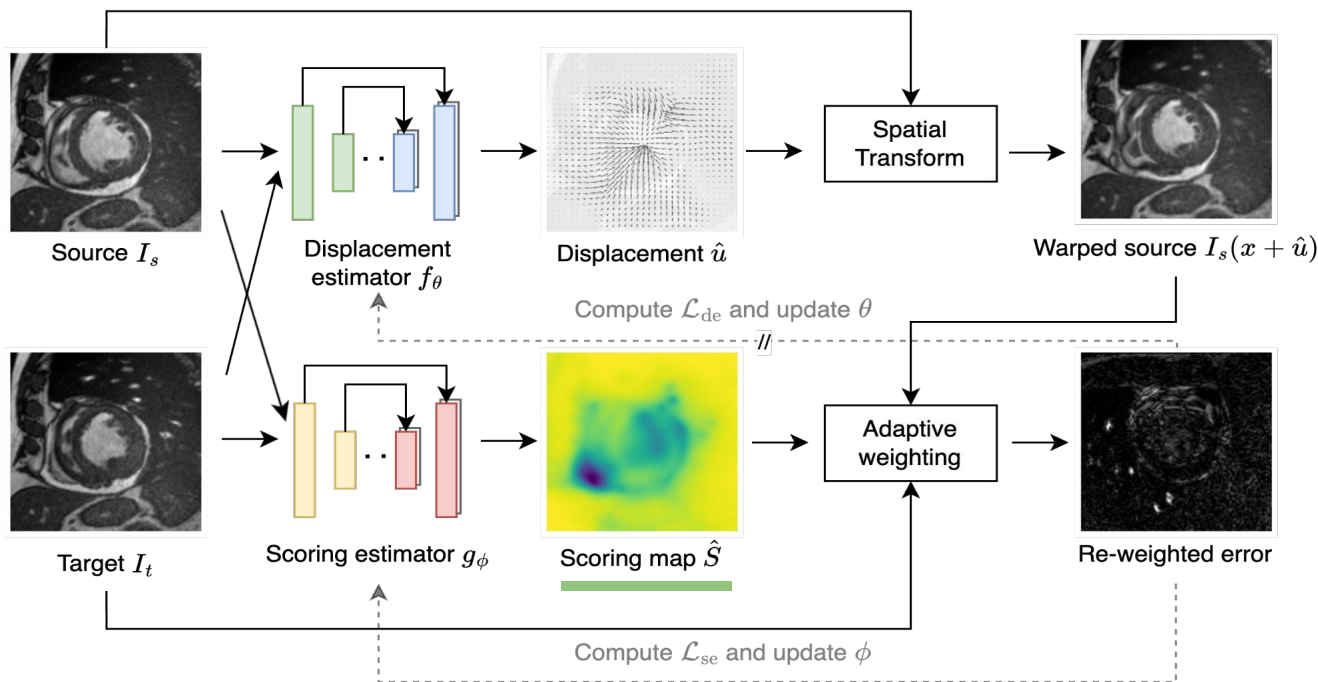
Method



But there is a trivial solution...

Displacement estimator loss:
$$\frac{1}{|\Omega|} \sum_{x \in \Omega} [\hat{S}(x)] [I_t(x) - I_s(x + \hat{u}(x))]^2 + \lambda \|\nabla \hat{u}(x)\|^2$$

Method



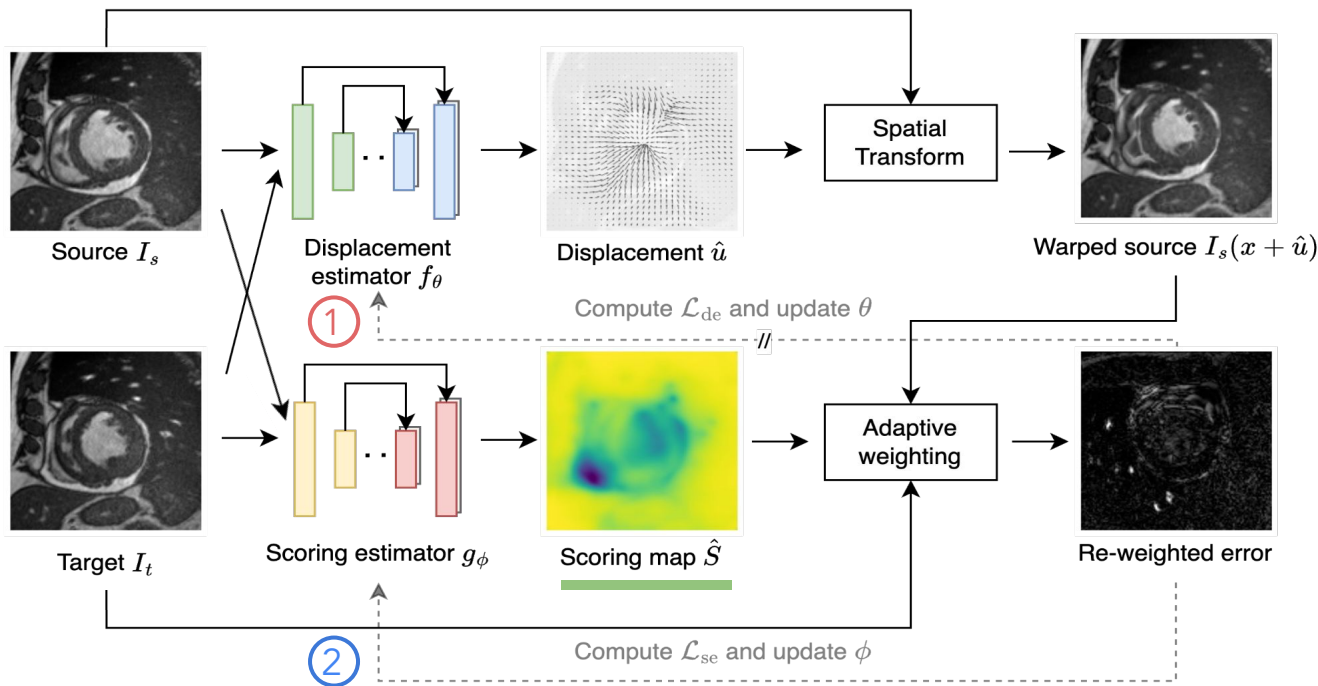
Avoid trivial solution:

$$\frac{1}{|\Omega|} \sum_{x \in \Omega} [1 - \hat{S}(x)]^2$$

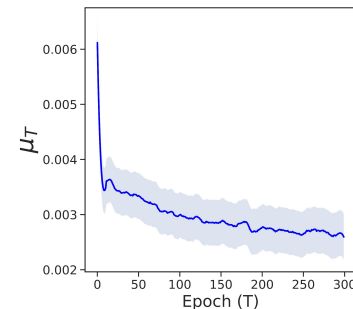
Scores correspond to surfaces that are locally smooth:

$$\frac{1}{|\Omega|} \sum_{x \in \Omega} \|\nabla \hat{S}(x)\|^2$$

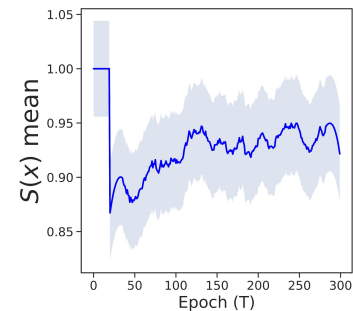
Method



Average residuals:



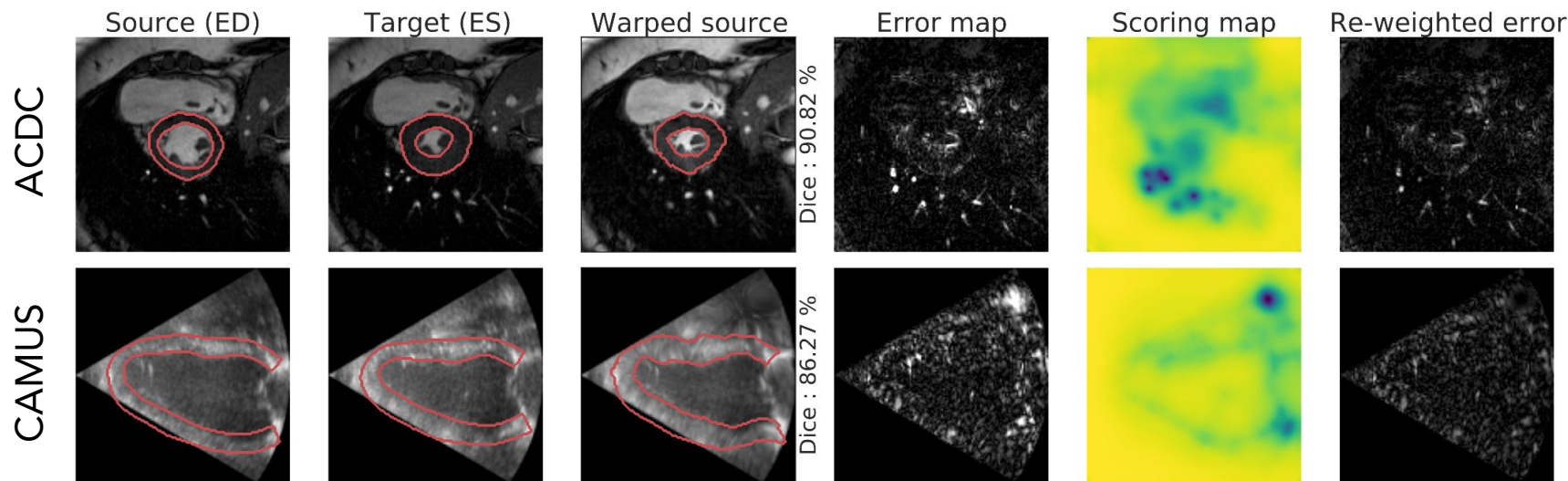
Average scores:



Momentum term: $b_T = \cos \frac{\pi}{2} \mu_T; m_T = \gamma m_{T-1} + (1 - \gamma) b_T$

**Note: The displacement and scoring estimators are optimized in separate alternating steps ① and ②

Results on ACDC and CAMUS



Our estimated scoring map identifies spurious error residuals and prevents parameter drift during training.

Results on ACDC and CAMUS

Quantitative evaluation

		ACDC			CAMUS		
		DSC ↑	HD ↓	ASD ↓	DSC ↑	HD ↓	ASD ↓
CNN	Undeformed	47.98	7.91	2.32	66.77	10.87	2.61
	Elastix	77.26	4.95	1.28	80.18	10.02	1.81
	Voxelmorph	79.48	4.79	1.27	81.50	8.72	1.74
	NLL	76.49	5.46	1.45	75.24	11.05	2.20
	β -NLL	78.74	5.07	1.33	79.75	9.39	1.93
	AdaFrame	66.38	5.80	1.67	77.88	10.54	1.93
	AdaReg	78.75	5.13	1.33	79.31	9.78	1.88
	AdaCS (Ours)	80.50	4.69	1.23	81.74	8.55	1.72
	Transmorph	76.94	5.51	1.30	79.24	10.30	1.79
	NLL	73.12	7.22	1.27	75.08	11.60	1.79
Transformer	β -NLL	75.74	6.12	1.29	77.39	10.99	1.86
	AdaFrame	67.95	5.72	1.59	78.06	9.86	1.91
	AdaReg	76.22	5.68	1.29	78.12	10.62	1.84
	AdaCS (Ours)	78.39	5.40	1.32	79.64	9.85	1.79
	Diffusemorph	67.38	5.80	1.67	75.23	9.80	2.07
Diffusion	NLL	66.24	5.84	1.73	74.78	10.62	2.15
	β -NLL	66.31	5.93	1.74	73.27	9.85	2.25
	AdaFrame	59.78	6.46	1.93	75.04	10.41	2.10
	AdaReg	69.41	6.25	1.78	74.36	10.66	2.21
	AdaCS (Ours)	72.09	5.35	1.53	77.65	9.82	1.99

Comparison to robust losses

		ACDC			CAMUS		
		DSC ↑	HD ↓	ASD ↓	DSC ↑	HD ↓	ASD ↓
vxm	NCC	78.55	4.94	1.29	77.01	10.23	1.89
	MI	78.04	5.25	1.35	78.18	9.83	1.99
	TBL	79.31	4.64	1.23	81.18	8.91	1.72
	MAE	78.27	5.36	1.43	78.59	10.23	1.97
	MSE	79.48	4.79	1.27	81.50	8.72	1.74
	AdaCS	80.50	4.69	1.23	81.74	8.55	1.72
tsm	NCC	73.77	6.64	1.12	73.03	11.87	1.70
	MI	73.57	6.57	1.11	74.83	11.94	1.83
	TBL	78.23	5.11	1.27	79.12	9.75	1.84
	MAE	74.30	6.36	1.28	75.96	11.35	1.89
	MSE	76.94	5.51	1.30	79.24	10.30	1.79
	AdaCS	78.39	5.40	1.32	79.64	9.85	1.79
dfm	NCC	70.25	5.29	1.58	75.67	10.75	2.06
	MI	71.16	5.40	1.56	76.19	10.09	2.16
	TBL	69.12	5.73	1.63	76.05	9.54	2.06
	MAE	66.30	5.75	1.71	77.30	10.36	2.09
	MSE	67.38	5.80	1.67	75.23	9.80	2.07
	AdaCS	72.09	5.35	1.53	77.65	9.82	1.99

Smoothness

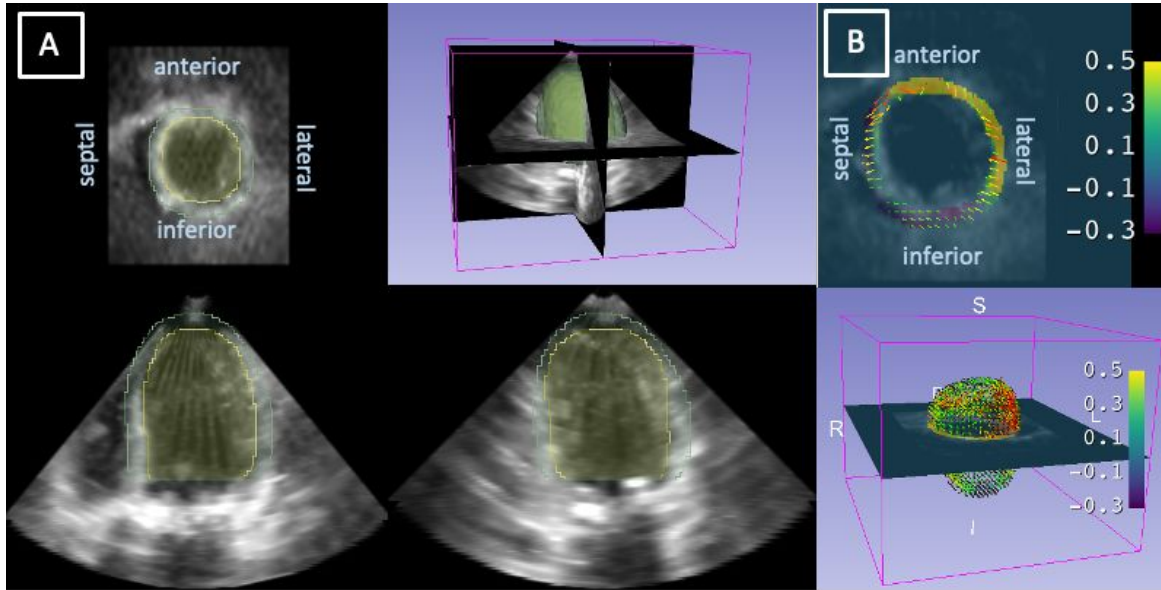
		ACDC			CAMUS		
		DSC ↑	$ J_{\hat{a}} \leq 0 \downarrow T_{\text{train}}$		DSC ↑	$ J_{\hat{a}} \leq 0 \downarrow T_{\text{train}}$	
Voxelmorph		79.48 ± 9.23	0.29	0.26	81.50 ± 5.58	0.60	0.26
	AdaCS (Ours)	80.50 ± 8.58	0.22	0.43	81.74 ± 5.36	0.30	0.43
Transmorph		76.94 ± 8.93	0.76	0.60	79.24 ± 6.06	1.41	0.59
	AdaCS (Ours)	78.39 ± 9.06	0.57	0.87	79.64 ± 6.37	0.70	0.70
Diffusemorph		67.38 ± 15.65	0.05	1.08	75.23 ± 8.71	0.05	1.06
	AdaCS (Ours)	72.09 ± 13.60	0.06	1.86	77.65 ± 7.64	0.08	1.91

Ablation

		Loss		ACDC			CAMUS		
		\mathcal{L}_{reg}	$\mathcal{L}_{\text{smooth}}$	DSC ↑	HD ↓	ASD ↓	DSC ↑	HD ↓	ASD ↓
vxm	✓	✗		80.24	4.64	1.23	81.58	8.89	1.74
	✓	✓		80.50	4.69	1.23	81.74	8.55	1.72
tsm	✓	✗		77.84	5.41	1.33	79.58	10.17	1.81
	✓	✓		78.39	5.40	1.32	79.64	9.85	1.79
dfm	✓	✗		71.62	5.56	1.58	77.32	9.71	2.00
	✓	✓		72.09	5.35	1.53	77.65	9.82	1.99

Our proposed approach consistently outperforms baselines in various architectures and datasets and produces reasonably smooth displacement.

Application - Cardiac Strain Analysis



(A) Segmented clinical echo (rest)

(B) Rest radial strain overlaid with estimated displacement revealing akinetic septal and inferior walls

Conclusion

- We identify the limitation of the widely used unsupervised training objective
- We address this by proposing an adaptive correspondence scoring framework during training
- Our proposed approach can be plugged-and-played into existing frameworks with no extra cost during inference



Xiaoran Zhang

<https://xiaoranzhang.com/>



Project page



Paper

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