Assessing Regional Cerebral Oxygen Consumption (CMRO₂) in Preterm Neonates: A Quantitative MRI Cohort Study with Exploratory Analysis of Respiratory Support

Chen Shuang Zhu^{1,2} Natalie Chan³ Anil Chacko⁴ Liisa Holsti⁵ Ruth E Grunau*^{2,6} Alexander Mark Weber*^{1,2,6,*}

Source: Article Notebook

Keywords: cerebral metabolic rate of oxygen; cerebral blood flow; ventilation; preterm; respiratory support; arterial spin labeling; quantitative susceptibility mapping

ABBREVIATIONS: ASL = arterial spin labeling; $CMRO_2$ = cerebral metabolic rate of oxygen; $CSaO_2$ = cerebral arterial oxygen saturation; $CSvO_2$ = cerebral venous oxygen saturation; GA = gestational age; CGM = cortical grey matter; DGM = deep grey matter; Hct = hematocrit; NICU = neonatal intensive care unit; NIRS = near-infrared spectroscopy; OEF

¹ School of Biomedical Engineering, The University of British Columbia, Vancouver, BC, Canada

² BC Children's Hospital Research Institute, The University of British Columbia, Vancouver, BC, Canada

³ Department of Pediatrics, University of California San Francisco, San Francisco, California, USA

⁴ BC Women's Hospital, Vancouver, BC, Canada

Occupational Science & Occupational Therapy, University of British Columbia, Vancouver, BC, Canada

⁶ Department of Pediatrics, The University of British Columbia, Vancouver, BC, Canada

^{*} Correspondence: Alexander Mark Weber* <aweber@bcchr.ca>

^{*} Joint senior authors

= oxygen extraction fraction; PMA = post-menstrual age; PPM = parts per million; QSM = quantitative susceptibility mapping; T2-TRIR = T2 Prepared Tissue Relaxation Inversion Recovery; TRUST = T2-relaxation-under-spin-tagging;

Summary Section

PREVIOUS LITERATURE: Quantitative estimates of brain oxygen consumption can be achieved using oxygen-15 PET or xenon clearance techniques, which measure cerebral blood flow but are invasive and involve ionizing radiation, limiting their use in neonates. A less invasive option is near-infrared spectroscopy (NIRS), which estimates cerebral venous oxygen saturation ($CSvO_2$) but is limited to regional assessments and superficial brain tissue. Non-invasive MRI techniques have been explored, including venous oxygenation measurements with TRUST MRI, MR susceptometry, and T2-TRIR MRI pulse sequences, showing feasibility in neonates and correlating well with previous methods.

KEY FINDINGS: Using a novel, non-invasive MRI technique and analysis pipeline, CBF and CMRO₂ values were measured in very preterm neonates at TEA and found to align closely with reference values. CBF and CMRO₂ values were associated with time in room air and non-invasive ventilation.

KNOWLEDGE ADVANCEMENT: We introduced a novel MRI technique and analysis pipeline, and demonstrated that non-invasive respiratory support in very preterm infants is associated with increased cerebral oxygenation and consumption, while room air is linked to lower values. Regional brain analysis revealed that respiratory support impacts different brain structures uniquely.

Abstract

BACKGROUND AND PURPOSE: Developing a non-invasive method for measuring oxygen consumption at both regional and whole-brain levels in preterm infants is crucial for assessing brain development and neuronal injury in this vulnerable population. This study presents a multi-modal MRI technique and analysis pipeline designed for this purpose, which we employ in a cohort study to investigate how the duration of various respiratory supports in very preterm infants affects CBF and the cerebral metabolic rate of oxygen (CMRO₂).

METHODS: Infants (n=19) born <32 weeks gestational age were recruited in the neonatal intensive care unit. Infants were scanned at term-equivalent age using a 3T MRI sequence comprising of T_1 -weighted, T_2 -weighted, arterial spin labeling (ASL), and SWI. Days on three different categories of respiratory support, based on levels of invasiveness, were recorded. Using multiple linear regression, CBF and CMRO₂ were analyzed against days on: respiratory support, days in room air, and the proportion of days on respiratory support; GA and PMA were used as confounding factors.

RESULTS: Average CBF and CMRO₂ of cortical grey matter was $14.3 \pm 4.25 \,\text{mL}/100 \text{g/min}$ and $29.49 \pm 29.49 \,\mu\text{mol}/100 \text{g/min}$, respectively. CMRO₂ and CBF were positively correlated with days on non-invasive respiratory support, and negatively correlated with days in room air.

CONCLUSION: Using our novel method, CBF and CMRO_2 values aligned closely with literature values. Our exploratory findings suggest that the type of respiratory support may influence cerebral oxygenation during the neonatal period in infants born very preterm, with greater oxygen delivery and consumption associated with non-invasive respiratory support. Our regional brain analysis further highlights that different brain structures are impacted in distinct ways.

Introduction

The developing brains of preterm infants are vulnerable to injury and dysmaturation, which can result in long-term neurological deficits (Kiechl-Kohlendorfer et al. 2009). Infants born very preterm (32 weeks gestation) are particularly at risk for significant short and long-term respiratory problems, and the lower the gestational age at birth, the more likely the infant may be negatively impacted (Chung, Chou, and Brown 2020). To mitigate these risks, it is crucial to monitor brain hemodynamics, as instability in oxygen delivery and metabolism can contribute to these injuries (Dhillon et al. 2022). These infants are also at significant risk of respiratory disorders, such as respiratory distress syndrome (McPherson and Wambach 2018), and bronchopulmonary dysplasia (Yoder, Albertine, and Null 2016). Finding ways to prevent these respiratory disorders, and support lung development, is critically important as lung health helps determine the amount of oxygen the brain receives (Cannavò et al. 2020;

Guillot et al. 2020). Therefore, close monitoring of cerebral oxygenation is critical to identify these risks early and apply neuroprotective strategies that may mitigate long-term neurological consequences.

In the NICU, to aid in respiration and improve lung function, various strategies including different forms of ventilation can be used, where the general goal is to decrease days of invasive mechanical ventilation. Non-invasive modes of ventilation, such as continuous positive airway pressure and nasal intermittent positive pressure ventilation, have been shown to be effective in lowering rates of complications and mortality compared to intubation with mechanical ventilation (Kalikkot Thekkeveedu et al. 2022; Ho, Subramaniam, and Davis 2020; Ackermann et al. 2023; Shi et al. 2014). With advances in neonatal intensive care and the use of less invasive forms of respiratory support, the incidence of bronchopulmonary dysplasia and other respiratory complications in preterm neonates has decreased over time (Dumpa and Bhandari 2021). However, the optimal mode and timing of ventilation in preterm neonates with respiratory disorders are still being debated (Brown and DiBlasi 2011; Greenough and Sharma 2005; Ramaswamy et al. 2020; Kollisch-Singule et al. 2022)

Non-invasive MRI-based techniques are actively being explored to assess whole-brain oxygen consumption. One approach combines non-invasive venous oxygenation measurements from the sagittal sinus using T2-relaxation-under-spin-tagging magnetic resonance imaging (TRUST (Lu and Ge 2008)) with flow measurements from phase-contrast MR angiography, which has been used in adults (Xu, Ge, and Lu 2009) and has shown feasibility in neonates (Liu et al. 2014; Qi et al. 2018). Another method combines MR susceptometry to measure venous oxygenation in the sagittal sinus with phase-contrast MR angiography (Jain et al. 2011). Studies using this technique in neonates demonstrated that the results correlate well with those obtained through diffuse optical and correlation spectroscopy methods (Jain et al. 2014). Still another method applied in neonates is the T2 prepared tissue relaxation inversion recovery (T2-TRIR) MRI pulse sequence (Petersen, Lim, and Golay 2006), which measures the transverse and longitudinal relaxation rate of blood (T_{2b} and T_{1b}) in the sagittal sinus, and venous oxygenation subsequently derived from the T_{2b} and the T_{1b} -derived hematocrit (Lu et al. 2012).

In the current study, we propose a new method using quantitative susceptibility mapping (QSM) and arterial spin labeling (ASL) – in combination with hematocrit (Hct) and pulse oximetry – to determine regional whole-brain cerebral metabolic rate of oxygen (CMRO $_2$) and CBF. In order to investigate the validity of this new non-invasive approach we compared the obtained results to previously reported reference values (Altman et al. 1993; De Vis et al. 2014; Liu et al. 2014; Elwell et al. 2005; Skov et al. 1993; Yoxall and Weindling 1998; Qi et al. 2018). In addition, we conducted an exploratory analysis to evaluate if the technique can detect whether the degree of lung disease, as indicated by the duration of time on different levels of respiratory support in very-preterm neonates, is correlated with brain oxygenation measures CMRO $_2$ and CBF in different brain regions at term-equivalent age. We hypothesized the CMRO $_2$ and CBF would be negatively correlated with time on invasive respiratory support.

Methods

STROBE

The methodology and its reporting have followed the STrengthening the Reporting of OBservational studies in Epidemiology (STROBE) standards. We include the checklist for a cohort study in our Supplementary Materials.

Patients

The study was approved by the Clinical Research Ethics Board at the *** and written informed consent was obtained from the parent/guardian for each infant.

Preterm neonates born <32 weeks gestational age (GA) (n=20) admitted to the level III neonatal intensive care unit (NICU) at *** in *** were recruited by a research nurse from February 2021 to January 2022. Our sample size was determined based on similar recruitment numbers from previous studies (Altman et al. 1993; De Vis et al. 2014; Liu et al. 2014; Elwell et al. 2005; Skov et al. 1993; Yoxall and Weindling 1998; Qi et al. 2018). Inclusion criteria were infants born less than 32 weeks GA. Infants were excluded if there was evidence of a congenital malformation or syndrome, a TORCH infection, or ultrasound evidence of large periventricular hemorrhagic infarction (>2 cm, Grade 4 intra-ventricular hemorrhage). Parents were approached by the research nurse about the study shortly before being discharged from the NICU. Infants returned to the hospital for the study at TEA (37-44 weeks PMA) for the MRI scan. One infant remained in hospital on respiratory support at 44 weeks PMA, and was withdrawn from the study. The final number of infants scanned was 19. The clinical characteristics of the subjects are shown in Table 1.

MRI data acquisition

All scans took place at the *** 's MRI Research Facility and were performed on a 3.0 Tesla General Electric Discovery MR750 (scanner software version DV26.0_R03) with a SREE Medical Systems single channel neonatal head coil. Infants were fed and swaddled by a research nurse prior to being placed in an MRI compatible incubator for imaging (SREE Medical Systems). Molded foam was placed around the infant's body and head to minimize head movement and ear plugs were used for ear protection. Arterial oxygen saturation and heart rate were monitored and measured continuously throughout the scan using a pulse oximeter placed on the foot of the infant. A neonatologist *** and primary investigator *** were present throughout the scan.

MRI scans were performed using a protocol consisting of a T1-weighted scan, a T2-weighted scan, a pseudo-continuous ASL scan to measure CBF, an SWI scan to generate QSM maps, and a diffusion weighted imaging spin echo EPI sequence (not included in this report). Sequences

were repeated when large motion artifacts were detected. If an infant awoke or was moving during the scan, the scanning was stopped, and a research nurse entered the MRI room to monitor and ensure the infant fell back to sleep.

The T1-weighted coronal 3D-FSPGR parameters were: 2.97ms TE, 7.74ms TR, 12 degrees flip angle, 20cm FOV, 512x512 matrix, 0.39x0.39 mm in-plane resolution, 1mm slice thickness, 126 slices, and a scan duration of 4min39 s. The T2-weighted sagittal 3D-CUBE parameters were: 66.29ms TE, 2,300ms TR, 90 degrees flip angle, 20cm FOV, 256x256 matrix, 0.78x0.78 mm in-plane resolution, 1mm slice thickness, 106 slices, and a scan duration of 5min1s.

The pseudo-continuous ASL axial multi-shot spiral 3D fast spin-echo parameters were: 10.55ms TE, 4.68s TR, 111 degrees flip angle, 24cm FOV, 128x128 matrix, 1.875x1.875 mm in-plane resolution, 4mm slice thickness, 50 slices, 1,450ms label period, 2,025ms pulse label delay, 24 control-label pairs, and a scan duration of 5min26 s.

The SWI axial 3D spoiled GRE flow compensated parameters were: five equally spaced echoes, 5ms first TE, 5.24ms echo spacing, 30.9ms TR, 20 degrees flip angle, 25cm FOV, 256x256 matrix, 0.977mm in-plane resolution, 2mm slice thickness, 92 slices, and a scan duration of 5min29s.

A DWI spin-echo EPI sequence was also acquired, but was not analyzed for this study.

Clinical data collection

Hct values were acquired retrospectively from chart review. Hct values for the day of scan were predicted using a four-parameter Weibull function (drc; fct=W1.4; Supplementary Figure 1). Clinical variables were obtained from the ***. Days on respiratory support were categorized into three groups: Category 1 (invasive ventilation) included high frequency jet ventilation, high frequency oscillatory ventilation, and intermittent positive-pressure ventilation (either volume or pressure targeted); Category 2 (non-invasive ventilation) included non-invasive positive pressure ventilation and continuous positive airway pressure; and Category 3 included high-flow and low-flow nasal cannula. The three categories represented the invasiveness of respiratory support, with Category 1 being the highest, and Category 3 being the lowest.

MRI data processing

Imaging data was processed using an in-house pipeline written in Bash shell script by *** with minor edits by ***. A step-by-step summary of the pipeline can be found in the Supplementary Materials.

Statistics

Statistical analysis was performed using R (v. 4.4.3) (R Core Team 2022) and R studio (v. 2022.12.0 Build 353) (RStudio Team, n.d.). A multiple linear regression analysis was conducted to examine relationships between dependent variables CBF or $CMRO_2$ and independent variables (e.g. days on Category 1 support). GA at birth and post-menstrual age (PMA) at time of scan were included as confounding factors. The correlation coefficient, p-value, and beta value was determined for each individual analysis. Significant relationships were considered with a p-value of 0.05. Multiple comparison corrections were not applied as our analysis was primarily exploratory.

Using a multiple linear regression analysis including GA and PMA as confounding factors, CBF and $\rm CMRO_2$ were analyzed separately against days on: the three separate categories of respiratory support, the number of days in room air (total days in the NICU minus total days on respiratory support), and the proportion of days on respiratory support (total days on respiratory support divided by total days in the NICU). Previous studies have shown a significant negative relationship between the brainstem volume of very preterm neonates at TEA and prolonged days on mechanical ventilation (Guillot et al. 2020); thus the days on Category 1 respiratory support was analyzed with brainstem volumes.

Results

Median (Q1-Q3) GA at birth and PMA at scan were 28.86 (27.79–29.93) and 40.57 (39.29–41.36), respectively. Median (Q1-Q3) days on Categories 1, 2, and 3 respiratory support, in room air, and length of stay in the NICU were 2 (0–4), 19 (11.5–32), 7 (5.5–12), 11 (3.5–23), and 53 (37–60), respectively (Table 1 and Figure 1).

A subject-by-subject distribution of days on different categories of respiratory support is shown in Figure 2.

Gestational age at birth was found to be negatively correlated with both days on Category 1 (invasive ventilation) and Category 2 (non-invasive ventilation) respiratory support, but not Category 3 (high-flow/low-flow; Figure 3).

A sample of results of the MRI analysis, including a sample brain segmentation, CBF map, QSM map, and CMRO₂ map are shown in Figure 4.

Mean whole-brain $CSvO_2$, $CSaO_2$, Hct and oxygen extraction fraction (OEF) values were 63.9 \pm 4, 98.3 \pm 1.5, 29.7 \pm 3.5, and 34.9 \pm 4.3, respectively. Regional mean CBF and $CMRO_2$ values are shown in Table 2. The lowest CBF and $CMRO_2$ values were found in the WM, while the highest CBF and $CMRO_2$ values were found in the brainstem.

Multiple linear regression analysis of regional CMRO_2 and CBF showed significant positive correlations with proportion of days on respiratory support (Figure 5), days on Category 2

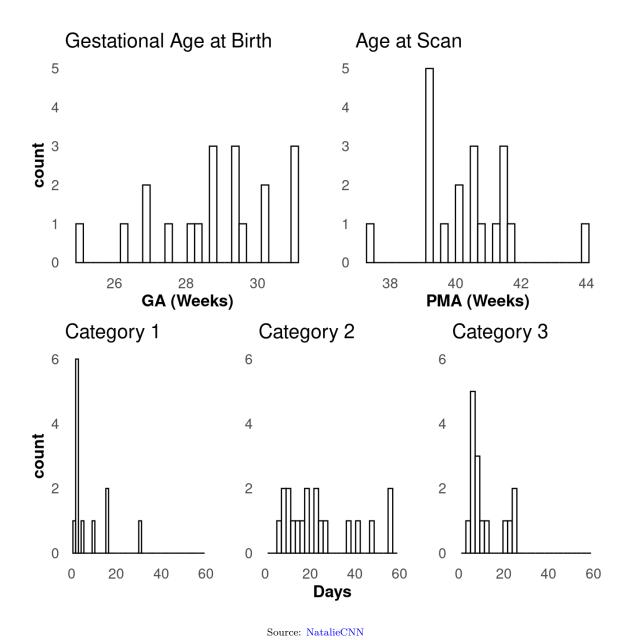


Figure 1. Types of respiratory support in relation to gestational age at birth, postmenstrual age (PMA) at scan, and days on each type of respiratory support. Note, counts of 0 days on respiratory support are not shown. Category 1 = invasive ventilation; category 2 = noninvasive ventilation; category 3 = high-flow and low-flow support.

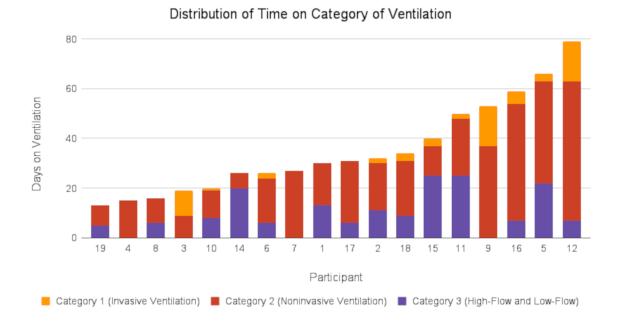


Figure 2. Days on the three levels of respiratory support for each study subject.

respiratory support (Figure 6), and significant negative correlations with days in room air (Figure 7). Results are summarized in Table 3.

No significant relationships were found between respiratory support categories and OEF, CSvO₂, CSaO₂, Hct (Table 3). No significant relationship was observed between brainstem volume and days on Category 1 respiratory support.

Discussion

We presented the initial results of a novel, non-invasive MRI method and analysis pipeline to evaluate CSvO_2 , OEF and CMRO_2 in preterm neonates. The values we found agreed well with earlier reported reference values. In addition, our technique allowed us to examined the effects of various forms of respiratory support on CBF and CMRO_2 in neonates born very preterm. We found that the proportion of days on respiratory support was positively associated with both CBF and CMRO_2 in all brain regions, a negative association was found for both CBF (some brain regions) and CMRO_2 (all brain regions) with days in room air, and non-invasive ventilation showed a positive association with CBF in all regions, and a positive association with CMRO_2 in the brainstem and cerebellum.

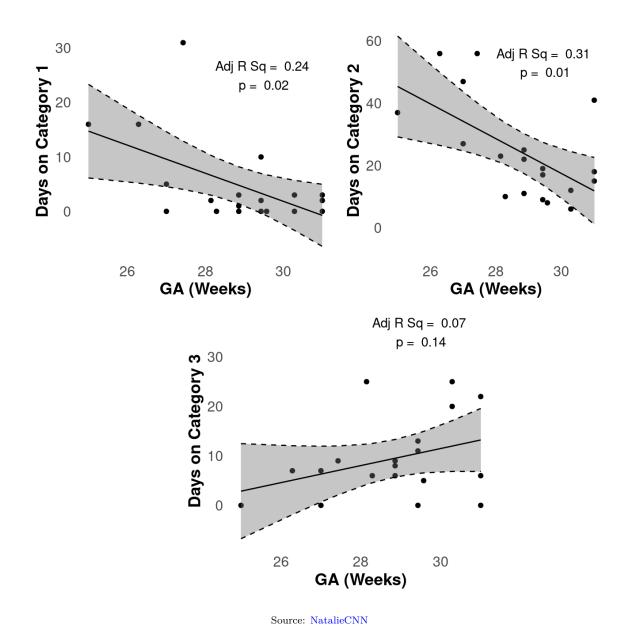


Figure 3. Linear regression of days on the three categories of respiratory support vs gestational age.

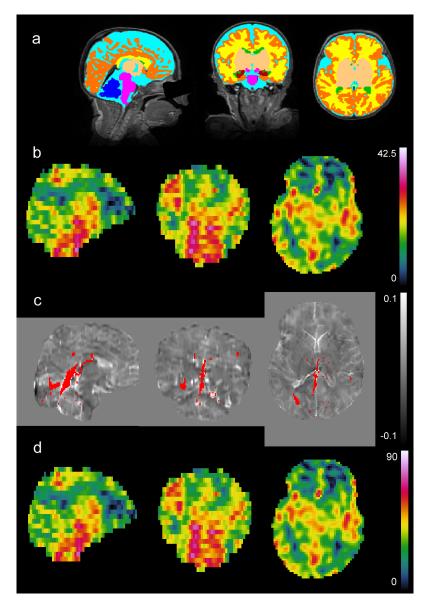


Figure 4. Sample images from a subject of various MRI results. All images show a sagittal, coronal and axial slice from left to right. A) is a T2w image in the background with segmentation overlaid in various colors: dark blue = cerebellum; pink = brainstem; light blue = CSF; yellow = white matter; dark orange = cortical grey matter; green = ventricles; light orange = deep grey matter; dark red = hippocampus and amygdala. B) is a processed CBF map from 0 to 47.5 mL/100g/min. C) is a QSM image in the background from -0.1 to 0.1 ppm susceptibility overlaid with a venous mask in red. D) is a processed CMRO₂ image from 0 to 93 µmol/100g/min. Note that B) and D) look identical as D is simply B multiplied by a value determined by CSaO₂, CSvO₂, and Hct. However, this value will be different for every subject.

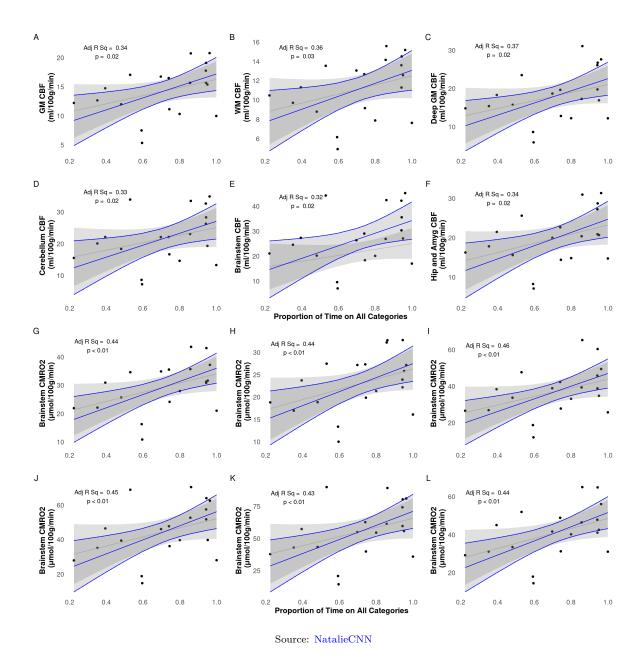


Figure 5. CBF (A-F) and CMRO₂ (G-L) vs proportion of time on all categories while in the NICU. Raw data points as filled black circles. Grey line and ribbon represent linear model of raw data points and 95% interval, respectively. Blue line and ribbon represent adjusted multiple linear regression including GA and PMA as confounding factors.

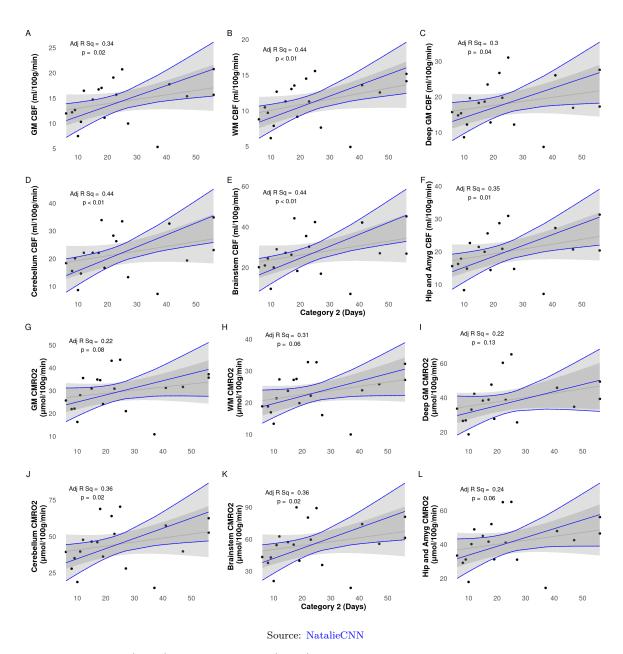


Figure 6. CBF (A-F) and CMRO₂ (G-L) values against Days on Noninvasive Ventilation (Category 2). Raw data points as filled black circles. Grey line and ribbon represent linear model of raw data points and 95% interval, respectively. Blue line and ribbon represent adjusted multiple linear regression including GA and PMA as confounding factors.

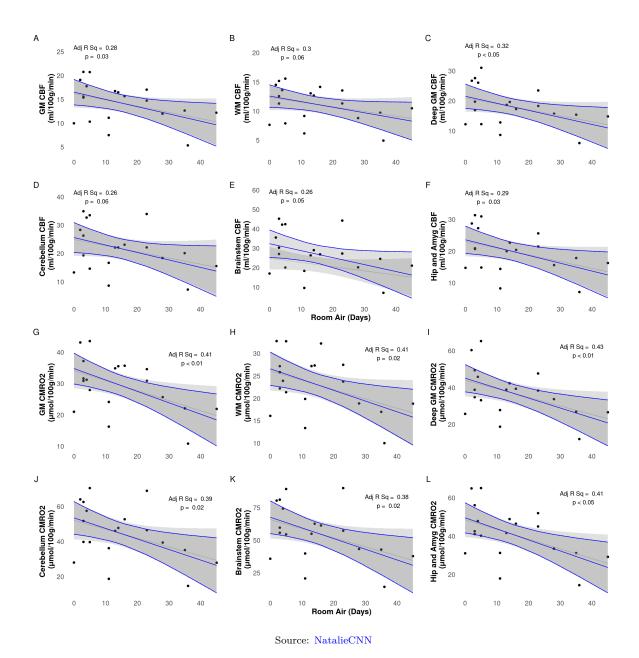


Figure 7. CBF () and CMRO₂ (b) values vs days in room air. Raw data points as filled black circles. Grey line and ribbon represent linear model of raw data points and 95% interval, respectively. Blue line and ribbon represent adjusted multiple linear regression including GA and PMA as confounding factors.

Comparison of MRI methods with previous literature

The results from previous neonatal studies are summarized in Table 4. The global CMRO₂, CBF, OEF and $CSvO_2$ values from this study align well with the literature from MRI, NIRS and PET studies reported for TEA infants.

One strength of using ASL compared to similar studies that used phase-contrast to calculate CBF is the ability to look at regional changes in CBF as opposed to a single number for the whole-brain (Liu et al. 2014; Qi et al. 2018). This is best demonstrated in the difference we see when looking at correlations with Category 2, where all regions were found to have a positive correlation with CBF, but only the brainstem and cerebellum were found to be positively correlated with CMRO₂. This discrepancy is discussed more below. However, using ASL in infants also has drawbacks that should be considered, including low signal-to-noise ratio, quantification difficulties due to uncertainty in labelling efficiency and bolus arrival time, and the rapid changes that occur in such young populations that make single-imaging-protocol difficult (Liu et al. 2019).

Similarly, a strength of using QSM to study CSvO₂ rather than previous MRI methods that used the TRUST (Liu et al. 2014; Qi et al. 2018) or T2-TRIR (De Vis et al. 2014), is that QSM produces a whole-brain map with high spatial resolution. By producing a whole-brain map, we were able to measure the CSvO₂ by averaging over all internal veins. This is likely to produce a more robust measurement than acquiring a single slice and averaging within the superior sagittal sinus (SSS) as TRUST and T2-TRIR do. For the current study, our QSM maps were reconstructed to a 0.9x0.9x0.9mm³ resolution, but future studies would benefit from acquiring and reconstructing up to 0.5x0.5x0.5 mm₃. Indeed, greater spatial resolution would likely improve CSvO₂ measurements as χ values could be better isolated to venous tissue without including non-venous sources. Finally, QSM could also allow for regional analysis of CSvO₂ values, which we did not attempt here. Unfortunately, as our method for calculating QSM requires removing brain tissue along the edge of the brain (an eroded brain mask), we could not measure CSvO₂ values in the SSS for more direct comparisons. Future work should be directed at acquiring QSM values in the SSS.

Two of the studies that measured $CMRO_2$, CBF and $CSvO_2$ in sick newborns requiring ventilatory support did not investigate associations between these values and days on various forms of respiratory support. Therefore, we were not able to directly compare these findings.

Respiratory support

In the present study, more days in room air without any type of respiratory support was associated with lower CMRO_2 and CBF values. If the assumption of higher CMRO_2 and CBF are indications of more optimal brain health, then this may suggest that the use of some form of respiratory support may be more beneficial to very preterm infants than weaning to room air. Indeed, CMRO_2 and CBF were positively related to the proportion of time on respiratory

support compared to the total time in the NICU. However, caution must be advised when interpreting these findings. Our study was observational, therefore, we cannot exclude various confounding factors, such as various levels of illness which would have dictated the form of respiratory support the infant received. We may be observing a compensatory effect, wherein infants who were sicker may have over-compensated for CBF and CMRO₂ to provide adequate oxygen. This would imply that increased CMRO₂ and CBF are a reflection of higher illness severity. It is critical for future studies to further explore this relationship because, if on the other hand, being in room air indicates suboptimal cerebral oxygenation and metabolism, it may significantly influence how infants in the NICU are managed.

Furthermore, while all brain regions were found to have a negative correlation between days in room air and CMRO₂, this was not the case for CBF, where only the cortical grey matter, deep grey matter, and hippocampus & amygdala were found to be negatively correlated with days in room air. Specific brain structures appear to regulate the level of CBF differently and independently of CMRO₂, suggesting that these brain regions may be more susceptible to or protected from hypoxia. Indeed, evidence for physiological uncoupling of CBF and CMRO₂ has been reported previously (Fox and Raichle 1986; Henriksen et al. 2021; Ishii et al. 1996). However, caution should be exercised when drawing strong conclusions from our exploratory analysis.

Invasive ventilation was not found to have to be associated with CMRO₂ or CBF in any tissue regions. This was unexpected as we hypothesized that infants who required more days on invasive ventilatory support would have lower CMRO₂ values at TEA. We also did not find a relationship between invasive mechanical ventilation and brain stem volume at TEA, unlike a previous study by Guillot et al. (2020) (Guillot et al. 2020). Our results are likely limited by the low exposure of this population to invasive mechanical ventilation, as only one infant required invasive support for a prolonged period of time (> 28days).

Non-invasive ventilation support was associated with increased CMRO_2 and CBF in preterm neonates at TEA. The observed increase in CMRO_2 and CBF with non-invasive ventilation suggests that prioritizing non-invasive over invasive ventilation may improve brain health outcomes in preterm neonates. However, caution should be exercised as our findings are exploratory in nature. Future studies on respiratory support strategies should incorporate CMRO_2 and CBF measurements to better understand their relationship with cerebral oxygenation and include a healthy term control cohort to establish comparative baseline values.

The difference between elevated CMRO_2 and CBF was also observed within regional tissues where CBF increased in all regional tissues for infants on non-invasive ventilation, but CMRO_2 only increased in the brainstem and cerebellar tissue. One possibility for this observation could be that compensatory mechanisms are activated in response to respiratory distress or regional brain injuries that hinder the uptake of oxygen. As with our findings in room air, this suggests that specific brain regions respond to respiratory support differently and may be more susceptible to damage. However, further research is first required to reproduce our exploratory findings.

Limitations

There are several limitations that are worth highlighting. Our CSvO₂ processing pipeline filtered out χ values below 0.15 ppm in order to obtain realistic values. Future studies may wish to use smaller voxel sizes, as well as a technique to decompose paramagnetic and diamagnetic values in order to avoid this step (Shin et al. 2021). See a recent study of ours for an attempt at this technique (Carmichael et al. 2025). Furthermore, in order to reduce QSM artifacts, the exterior of the brain mask was eroded, making it impossible to measure CSvO₂ in the SSS. Future studies may find a way to measure QSM in the SSS, which would also allow researchers to determine if CSvO₂ values are different in the SSS compared to the central cerebral veins. Again, see a recent study of ours that attempted this (Carmichael et al. 2025). Het levels were not collected on the day of the scan, but instead were predicted based on past values. Our respiratory support analysis was exploratory with a small sample size. Thus, the positive correlation we found in Category 2 may be spurious or a result of an unaccounted factor. Future studies using large sample randomized controlled trials would provide a clearer understanding of the relationship between respiratory support and cerebral oxygenation. Imaging was performed at term-equivalent age after the infants had been discharged from the NICU, meaning the scans were performed weeks after the infants were last on respiratory support. Obtaining scans while the infants are still receiving respiratory support could provide a more robust mechanistic connection. Our study did not include a healthy control cohort to compare the expected physiological measures at TEA. This would be important to include, as too much oxygen can be just as harmful as not enough (Rantakari et al. 2021). Finally, due to our sample size, this study did not explore supplementary variables, such as medications, that may affect respiratory uptake and oxygen metabolism, and patterns of oxygen saturations infants experience during their NICU stay.

Acknowledgments

We wish to acknowledge the work of and thank *** (Research Nurse); *** (Research Nurse); *** (Neonatologist); and *** (Radiologist).

Funding

Authors *** were co-primary investigators on a *** Catalyst Grant (\$20,000). *** were supported by an establishment award from *** . Scanning was partly funded through a special award to *** from *** .

References

- Ackermann, Benjamin W., Daniel Klotz, Roland Hentschel, Ulrich H. Thome, and Anton H. Van Kaam. 2023. "High-Frequency Ventilation in Preterm Infants and Neonates." Pediatric Research 93 (7): 1810–18. https://doi.org/10.1038/s41390-021-01639-8.
- Altman, D. I., J. M. Perlman, J. J. Volpe, and W. J. Powers. 1993. "Cerebral Oxygen Metabolism in Newborns." *Pediatrics* 92 (1): 99–104.
- Brown, Melissa K, and Robert M DiBlasi. 2011. "Mechanical Ventilation of the Premature Neonate." Respiratory Care 56 (9): 1298–1313. https://doi.org/10.4187/respcare.01429.
- Cannavò, Laura, Immacolata Rulli, Raffaele Falsaperla, Giovanni Corsello, and Eloisa Gitto. 2020. "Ventilation, Oxidative Stress and Risk of Brain Injury in Preterm Newborn." *Italian Journal of Pediatrics* 46 (1): 100. https://doi.org/10.1186/s13052-020-00852-1.
- Carmichael, Thomas Gavin, Alexander Rauscher, Ruth E. Grunau, and Alexander Mark Weber. 2025. "The Application of Magnetic Susceptibility Separation for Measuring Cerebral Oxygenation in Preterm Neonates." *Pediatric Research*, March. https://doi.org/10.1038/s41390-025-03966-6.
- Chung, Estefani Hee, Jesse Chou, and Kelly A. Brown. 2020. "Neurodevelopmental Outcomes of Preterm Infants: A Recent Literature Review." *Translational Pediatrics* 9 (S1): S3–8. https://doi.org/10.21037/tp.2019.09.10.
- De Vis, J. B., E. T. Petersen, T. Alderliesten, F. Groenendaal, L. S. de Vries, F. van Bel, M. J. N. L. Benders, and J. Hendrikse. 2014. "Non-Invasive MRI Measurements of Venous Oxygenation, Oxygen Extraction Fraction and Oxygen Consumption in Neonates." NeuroImage 95 (July): 185–92. https://doi.org/10.1016/j.neuroimage.2014.03.060.
- Dhillon, Simerdeep K., Eleanor R. Gunn, Benjamin A. Lear, Victoria J. King, Christopher A. Lear, Guido Wassink, Joanne O. Davidson, Laura Bennet, and Alistair J. Gunn. 2022. "Cerebral Oxygenation and Metabolism After Hypoxia-Ischemia." Frontiers in Pediatrics 10 (July): 925951. https://doi.org/10.3389/fped.2022.925951.
- Dumpa, Vikramaditya, and Vineet Bhandari. 2021. "Non-Invasive Ventilatory Strategies to Decrease Bronchopulmonary Dysplasia—Where Are We in 2021?" *Children* 8 (2): 132. https://doi.org/10.3390/children8020132.
- Elwell, Clare E., Julian R. Henty, Terence S. Leung, Topun Austin, Judith H. Meek, David T. Delpy, and John S. Wyatt. 2005. "Measurement of CMRO2 in Neonates Undergoing Intensive Care Using Near Infrared Spectroscopy." In Oxygen Transport to Tissue XXVI, edited by Paul Okunieff, Jacqueline Williams, and Yuhchyau Chen, 566:263–68. New York: Springer-Verlag. https://doi.org/10.1007/0-387-26206-7_35.
- Fox, P T, and M E Raichle. 1986. "Focal Physiological Uncoupling of Cerebral Blood Flow and Oxidative Metabolism During Somatosensory Stimulation in Human Subjects." *Proceedings of the National Academy of Sciences* 83 (4): 1140–44. https://doi.org/10.1073/pnas.83.4. 1140.
- Greenough, Anne, and Atul Sharma. 2005. "Optimal Strategies for Newborn Ventilation—a Synthesis of the Evidence." Early Human Development 81 (12): 957–64. https://doi.org/10.1016/j.earlhumdev.2005.10.002.

- Guillot, Mireille, Ting Guo, Steven Ufkes, Juliane Schneider, Anne Synnes, Vann Chau, Ruth E. Grunau, and Steven P. Miller. 2020. "Mechanical Ventilation Duration, Brainstem Development, and Neurodevelopment in Children Born Preterm: A Prospective Cohort Study." The Journal of Pediatrics 226 (November): 87–95.e3. https://doi.org/10.1016/j.jpeds.2020.05.039.
- Henriksen, Otto M., Albert Gjedde, Kim Vang, Ian Law, Joel Aanerud, and Egill Rostrup. 2021. "Regional and Interindividual Relationships Between Cerebral Perfusion and Oxygen Metabolism." *Journal of Applied Physiology* 130 (6): 1836–47. https://doi.org/10.1152/japplphysiol.00939.2020.
- Ho, Jacqueline J, Prema Subramaniam, and Peter G Davis. 2020. "Continuous Positive Airway Pressure (CPAP) for Respiratory Distress in Preterm Infants." Edited by Cochrane Neonatal Group. Cochrane Database of Systematic Reviews 2020 (10). https://doi.org/10.1002/14651858.CD002271.pub3.
- Ishii, K., M. Sasaki, H. Kitagaki, S. Sakamoto, S. Yamaji, and K. Maeda. 1996. "Regional Difference in Cerebral Blood Flow and Oxidative Metabolism in Human Cortex." *Journal of Nuclear Medicine: Official Publication, Society of Nuclear Medicine* 37 (7): 1086–88.
- Jain, Varsha, Erin M. Buckley, Daniel J. Licht, Jennifer M. Lynch, Peter J. Schwab, Maryam Y. Naim, Natasha A. Lavin, et al. 2014. "Cerebral Oxygen Metabolism in Neonates with Congenital Heart Disease Quantified by MRI and Optics." Journal of Cerebral Blood Flow and Metabolism: Official Journal of the International Society of Cerebral Blood Flow and Metabolism 34 (3): 380–88. https://doi.org/10.1038/jcbfm.2013.214.
- Jain, Varsha, Michael C Langham, Thomas F Floyd, Gaurav Jain, Jeremy F Magland, and Felix W Wehrli. 2011. "Rapid Magnetic Resonance Measurement of Global Cerebral Metabolic Rate of Oxygen Consumption in Humans During Rest and Hypercapnia." Journal of Cerebral Blood Flow & Metabolism 31 (7): 1504–12. https://doi.org/10.1038/jcbfm. 2011.34.
- Kalikkot Thekkeveedu, Renjithkumar, Ahmed El-Saie, Varsha Prakash, Lakshmi Katakam, and Binoy Shivanna. 2022. "Ventilation-Induced Lung Injury (VILI) in Neonates: Evidence-Based Concepts and Lung-Protective Strategies." *Journal of Clinical Medicine* 11 (3): 557. https://doi.org/10.3390/jcm11030557.
- Kiechl-Kohlendorfer, U, E Ralser, U Pupp Peglow, G Reiter, and R Trawöger. 2009. "Adverse Neurodevelopmental Outcome in Preterm Infants: Risk Factor Profiles for Different Gestational Ages." *Acta Paediatrica* 98 (5): 792–96. https://doi.org/10.1111/j.1651-2227.2009.01219.x.
- Kollisch-Singule, Michaela, Harry Ramcharran, Joshua Satalin, Sarah Blair, Louis A. Gatto, Penny L. Andrews, Nader M. Habashi, Gary F. Nieman, and Adel Bougatef. 2022. "Mechanical Ventilation in Pediatric and Neonatal Patients." Frontiers in Physiology 12 (March): 805620. https://doi.org/10.3389/fphys.2021.805620.
- Liu, Peiying, Hao Huang, Nancy Rollins, Lina F. Chalak, Tina Jeon, Cathy Halovanic, and Hanzhang Lu. 2014. "Quantitative Assessment of Global Cerebral Metabolic Rate of Oxygen (CMRO2) in Neonates Using MRI." *NMR in Biomedicine* 27 (3): 332–40. https://doi.org/10.1002/nbm.3067.
- Liu, Peiying, Ying Qi, Zixuan Lin, Qiyong Guo, Xiaoming Wang, and Hanzhang Lu. 2019.

- "Assessment of Cerebral Blood Flow in Neonates and Infants: A Phase-Contrast MRI Study." *NeuroImage* 185 (January): 926–33. https://doi.org/10.1016/j.neuroimage.2018.03.020.
- Lu, Hanzhang, and Yulin Ge. 2008. "Quantitative Evaluation of Oxygenation in Venous Vessels Using T2-Relaxation-Under-Spin-Tagging MRI." *Magnetic Resonance in Medicine* 60 (2): 357–63. https://doi.org/10.1002/mrm.21627.
- Lu, Hanzhang, Feng Xu, Ksenija Grgac, Peiying Liu, Qin Qin, and Peter van Zijl. 2012. "Calibration and Validation of TRUST MRI for the Estimation of Cerebral Blood Oxygenation." Magnetic Resonance in Medicine 67 (1): 42–49. https://doi.org/10.1002/mrm.22970.
- McPherson, Christopher, and Jennifer A. Wambach. 2018. "Prevention and Treatment of Respiratory Distress Syndrome in Preterm Neonates." *Neonatal Network* 37 (3): 169–77. https://doi.org/10.1891/0730-0832.37.3.169.
- Petersen, Esben Thade, Tchoyoson Lim, and Xavier Golay. 2006. "Model-Free Arterial Spin Labeling Quantification Approach for Perfusion MRI." *Magnetic Resonance in Medicine* 55 (2): 219–32. https://doi.org/10.1002/mrm.20784.
- Qi, Ying, Peiying Liu, Zixuan Lin, Hanzhang Lu, and Xiaoming Wang. 2018. "Hemodynamic and Metabolic Assessment of Neonates With Punctate White Matter Lesions Using Phase-Contrast MRI and T2-Relaxation-Under-Spin-Tagging (TRUST) MRI." Frontiers in Physiology 9: 233. https://doi.org/10.3389/fphys.2018.00233.
- R Core Team. 2022. "R: A Language and Environment for Statistical Computing." Vienna, Austria: R Foundation for Statistical Computing.
- Ramaswamy, Viraraghavan Vadakkencherry, Kiran More, Charles Christoph Roehr, Prathik Bandiya, and Sushma Nangia. 2020. "Efficacy of Noninvasive Respiratory Support Modes for Primary Respiratory Support in Preterm Neonates with Respiratory Distress Syndrome: Systematic Review and Network Meta-Analysis." *Pediatric Pulmonology* 55 (11): 2940–63. https://doi.org/10.1002/ppul.25011.
- Rantakari, Krista, Olli-Pekka Rinta-Koski, Marjo Metsäranta, Jaakko Hollmén, Simo Särkkä, Petri Rahkonen, Aulikki Lano, et al. 2021. "Early Oxygen Levels Contribute to Brain Injury in Extremely Preterm Infants." *Pediatric Research* 90 (1): 131–39. https://doi.org/10.1038/s41390-021-01460-3.
- RStudio Team. n.d. "RStudio: Integrated Development Environment for R." Boston, MA: RStudio, PBC.
- Shi, Yuan, Shifang Tang, Jinning Zhao, and Jie Shen. 2014. "A Prospective, Randomized, Controlled Study of NIPPV Versus nCPAP in Preterm and Term Infants with Respiratory Distress Syndrome: NIPPV Vs. nCPAP in Preterm and Term Infants." *Pediatric Pulmonology* 49 (7): 673–78. https://doi.org/10.1002/ppul.22883.
- Shin, Hyeong-Geol, Jingu Lee, Young Hyun Yun, Seong Ho Yoo, Jinhee Jang, Se-Hong Oh, Yoonho Nam, et al. 2021. "χ-Separation: Magnetic Susceptibility Source Separation Toward Iron and Myelin Mapping in the Brain." NeuroImage 240 (October): 118371. https://doi.org/10.1016/j.neuroimage.2021.118371.
- Skov, L., O. Pryds, G. Greisen, and H. Lou. 1993. "Estimation of Cerebral Venous Saturation in Newborn Infants by Near Infrared Spectroscopy." *Pediatric Research* 33 (1): 52–55. https://doi.org/10.1203/00006450-199301000-00011.

- Xu, Feng, Yulin Ge, and Hanzhang Lu. 2009. "Noninvasive Quantification of Whole-Brain Cerebral Metabolic Rate of Oxygen (CMRO2) by MRI." *Magnetic Resonance in Medicine* 62 (1): 141–48. https://doi.org/10.1002/mrm.21994.
- Yoder, Bradley A., K. H. Albertine, and D. M. Null. 2016. "High-Frequency Ventilation for Non-Invasive Respiratory Support of Neonates." Seminars in Fetal and Neonatal Medicine 21 (3): 162–73. https://doi.org/10.1016/j.siny.2016.02.001.
- Yoxall, C. W., and A. M. Weindling. 1998. "Measurement of Cerebral Oxygen Consumption in the Human Neonate Using Near Infrared Spectroscopy: Cerebral Oxygen Consumption Increases with Advancing Gestational Age." *Pediatric Research* 44 (3): 283–90. https://doi.org/10.1203/00006450-199809000-00004.

Tables

Table 1. Neonatal and maternal characteristic of the study sample.

Maternal Characteristics	(n=19)	Neonatal Characteristics
Gestational Diabetes	6 (31.6%)	Male (n)
Delivery Mode		Female (n)
Cesarean	16 (84.2%)	Birth weight (g)
Vaginal	3 (15.8%)	GA at Birth (weeks)
Maternal Fever		PMA on Scan Day (weeks)
Yes	1 (5.3%)	Weight on Scan Day (g)
No	6 (31.6%)	Head Circumference on Scan Day (cm)
Unknown	12 (63.2%)	Days in NICU
Chorioamnionitis		Days on Sedatives
Yes	4 (21%)	Days on Narcotic Infusion
No	12 (63.2%)	Days on Category 1 (invasive ventilation)
Unknown	3 (15.8%)	Days on Category 2 (non-invasive ventilation)
Leukocytosis		Days on Category 3 (high-flow/low-flow)
Yes	1 (5.3%)	Total Days on Respiratory Support
No	4 (21%)	Days in Room Air
Unknown	14 (73.7%)	
Gestational Hypertension	3 (15.8%)	
Pre-Existing Hypertension	1 (5.3%)	
Systemic Antibiotic	cs	
Yes	15 (78.9%)	
No	1 (5.3%)	
Unknown	3 (15.8%)	

Median(Q1-Q3) is shown for continuous variables and n (%) for categorical variables. GA = gest postmenstrual age on the day of the scan.

Source: Article Notebook

Table 2. Regional mean \pm standard deviation CBF and CMRO2 values. White matter tissue was found to have the lowest CBF/CMRO2 values, while the brainstem had the highest. CBF = cerebral blood flow; CMRO2 = cerebral metabolic rate of oxygen; ROI = region of interest; CGM = cerebral grey matter; WM = white matter; DGM = deep grey matter.

ROI	CBF $(mL/100g/min)$	$CMRO2~(\mu mol/100 g/min)$
CGM	14.3 ± 4.25	29.49 ± 8.62
WM	11.18 ± 3.11	23.08 ± 6.47
DGM	18.1 ± 6.63	37.22 ± 13.23
Brainstem	27.16 ± 11.05	55.69 ± 21.34
Cerebellum	21.78 ± 8.27	44.68 ± 15.98
Hippocampus and Amygdala	19.98 ± 6.85	41.14 ± 13.69

Table 3. Results from linear regression of physiological parameters with days on various forms of respiratory support. All analyses included GA and PMA as confounding variables. CGM = cortical grey matter; WM = white matter; DGM = deep grey matter; BS = brainstem; Cereb = cerebellum; H&A = hippocampus and amygdala.

ROI	Invasive Ventilation (Category 1) [95% CI] / Adj R ²	Noninvasive Ventilation (Category 2) [95% CI] / Adj R ²	High-flow and low-flow air (Category 3) [95% CI] / Adj R ²	Proportion Of Days On All Categories [95% CI] / Adj R ²	Room Air [95% CI] / Adj R ²
$\overline{ ext{CBF}}$					
CGM	0.05 [-0.31 to 0.41] / 0.02	$0.2 \; [0.05 \; { m to} \ 0.36] \; / \; 0.34$	0.13 [-0.14 to 0.4] / 0.08	$10.27 \; [2.17] \ ext{to} \; 18.37] \; / \ 0.34$	-0.15 [-0.29 to -0.02] / 0.28
WM	0.08 [-0.17 to 0.32] / 0.13	$egin{array}{ll} 0.15 & [0.05\ au & 0.26] \ / \ 0.44 \end{array}$	0.07 [-0.12 to 0.26] / 0.14	6.7 [0.86 to 12.55] / 0.36	-0.1 [-0.19 to 0] / 0.3
DGM	-0.05 [-0.59 to 0.5] / 0.06	0.28 [0.02 to 0.53] / 0.3	0.16 [-0.26 to 0.57] / 0.1	15.82 [3.51 to 28.13] / 0.37	-0.23 [-0.44 to -0.03] / 0.32
Cereb	0.18 [-0.5 to 0.87] / 0.07	$egin{array}{lll} 0.43 & [0.14] \ ext{to } 0.72] \ / \ 0.44 \end{array}$	$0.21 [-0.31 \text{ to} \\ 0.73] / 0.09$	18.81 [2.98 to 34.64] / 0.33	-0.26 [-0.53 to 0.01] / 0.26
BS	0.17 [-0.75 to 1.09] / 0.05	0.59 [0.2 to 0.97] / 0.44	$0.21 [-0.49 \text{ to} \\ 0.92] / 0.06$	25.22 [3.9 to 46.53] / 0.32	-0.36 [-0.72 to 0] / 0.26
H&A	0.05 [-0.53 to 0.63] / 0.02	0.33 [0.08 to 0.59] / 0.35	0.13 [-0.31 to 0.57] / 0.04	16.73 [3.73 to 29.73] / 0.34	-0.25 [-0.47 to -0.03] / 0.29
$CMRO_2$		0.00		0.01	0.20
CGM	0.04 [-0.68 to 0.77] / 0.04	0.31 [-0.04 to 0.66] / 0.22	$0.25 \ [-0.29 \ to \ 0.79] \ / \ 0.1$	23.31 [8.19 to 38.44] / 0.44	-0.36 [-0.62 to -0.11] / 0.41
WM	0.13 [-0.39 to 0.64] / 0.14	0.24 [-0.01 to 0.48] / 0.31	0.15 [-0.24 to 0.54] / 0.16	15.68 [4.38 to 26.98] / 0.44	-0.36 [-0.62 to -0.11] / 0.41
DGM	-0.19 [-1.27 to 0.89] / 0.09	0.41 [-0.13 to 0.95] / 0.22	0.3 [-0.52 to 1.12] / 0.12	34.74 [11.97 to 57.5] / 0.46	-0.54 [-0.92 to -0.16] / 0.43

ROI	Invasive Ventilation (Category 1) [95% CI] / Adj R ²	Noninvasive Ventilation (Category 2) [95% CI] / Adj R ²	High-flow and low-flow air (Category 3) [95% CI] / Adj R ²	Proportion Of Days On All Categories [95% CI] / Adj R ²	Room Air [95% CI] / Adj R ²
Cereb	0.27 [-1.03 to 1.56] / 0.1	0.7 [0.11 to 1.29] / 0.36	0.39 [-0.59 to 1.38] / 0.13	40.71 [12.88 to 68.54] / 0.45	-0.6 [-1.08 to -0.12] / 0.39
BS	0.2 [-1.55 to 1.96] / 0.07	0.96 [0.17 to 1.75] / 0.36	0.4 [-0.95 to 1.74] / 0.09	54.63 [16.85 to 92.4] / 0.43	-0.82 [-1.46 to -0.18] / 0.38
H&A	0 [-1.15 to 1.15] / 0.04	0.52 [-0.03 to 1.07] / 0.24	0.25 [-0.63 to 1.13] / 0.06	37.23 [13.28 to 61.17] / 0.44	-0.58 [-0.98 to -0.17] / 0.41
CSvO ₂ (%)				0.44	
Wholebrain	-0.16 [-0.51 to 0.2] / -0.1	0.06 [-0.14 to 0.25] / -0.13	-0.06 [-0.34 to 0.22] / -0.15	-0.68 [-10.72 to 9.36] / -0.16	-0.02 [-0.19 to 0.14] / -0.15
$CSaO_2$ (%)			0.10	0.10	0.10
n/a	-0.05 [-0.18 to 0.08] / 0.06	-0.06 [-0.12 to 0] / 0.23	$0.02 [-0.08 \text{ to} \\ 0.12] / 0.03$	0.34 [-3.23 to 3.91] / 0.02	-0.01 [-0.07 to 0.05] / 0.02
OEF (%)					
Wholebrain	0.13 [-0.26 to 0.52] / -0.14	-0.1 [-0.31 to 0.11] / -0.1	0.07 [-0.23 to 0.38] / -0.15	0.83 [-10.03 to 11.68] / -0.17	0.02 [-0.16 to 0.19] / -0.17
Hct (%)					
n/a	-0.19 [-0.49 to 0.12] / -0.07	-0.02 [-0.2 to 0.15] / -0.18	-0.05 [-0.3 to 0.19] / -0.17	2.35 [-6.48 to 11.17] / -0.16	-0.09 [-0.23 to 0.05] / -0.05

Table 4. Comparison of the arterial oxygenation, venous oxygenation, oxygen extraction fraction, cerebral blood flow, and cerebral metabolic rate of oxygen obtained from this study with that of previous reports. CBF = cerebral blood flow; CMRO2 = cerebral metabolic rate of oxygen; CSvO2 = cerebral venous oxygen saturation; CSaO2 = cerebral arterial oxygen saturation; OEF = oxygen extraction fraction; Hct = hematocrit ^*^Median and interquartile range reported.

	Number of	PMA CSaO2CSvO2OEF CBF CMRO2
Study	Meth Sdbjects	(weeks) (%) (%) (%) (mL/100 $g/minl$) 100g/
This study	MRI 19 preterm at	$40.4 98.3 63.9 34.9 14.3 \pm 29.5 \pm$
	term	$\pm \pm \pm 4 \pm 4.3 \qquad 4.2 \qquad 8.6$
		1.4 1.5
Altman et al., (1993) (Altman et al. 1993)	PET 11 HIE and other conditions	35.1 ± 6 M/A $21.6\pm21606\pm132$ 2.6 $\pm21.21.4\pm16.4$
De Vis et al., (2014) (De Vis et al. 2014)	MRI 10 preterm at term	$39 97 \pm 1 52 \pm 12 49 \pm 12 14 \pm 3 \qquad 30 \pm 6$
	9 HIE	$38 96 \pm 3 65 \pm 13 32 \pm 12 12 \pm 4 24 \pm 12$
Liu et al., (2014) (Liu et al. 2014)	MRI 12 healthy	37.4±2.95.8±22.6±8.N/A 13.4±4.238.3±17.7
Elwell et al., (2005) (Elwell et al. 2005)	NIRS9 ventilatory support	29.2±5.N/A N/A N/A N/A 45.9±12.3
Skov et al., (1993) (Skov et al. 1993)	NIRS10 asphyxiated (full term)	$38.8 \pm 1.944 \pm 7 \ 67.3 \pm 928.4 \pm 0.26.5 \pm 17.562.6 \pm 35.8$
`	22 Respiratory Distress Syndrome (RDS) (preterm)	$29.8 \pm 2.96.5 \pm 53.4 \pm 15446 \pm 2.11.9 \pm 5.244.7 \pm 17.9$
Yoxall & Weindling, (1998) (Yoxall and Weindling 1998)	NIRS9 ventilatory support	23- N/A 62.6±8.N/A 13.4±4.238.3±17.7 37
Qi et al, (2018) (Qi	MRI 38 healthy	35.71 95 63.85 32.35 15.35 38.09
et al. 2018)*	v	(5.36) (2) (4.8) (6.26) (9.13) (18.84)
,	23 Punctate	35.14 95 68.7 27.53 12.63 29.11
	White Matter Lesions (PWML)	(3.29) (2) (16.3) (18.94) (7.83) (16.8)