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PD-Fuzzy Control of a Stair Climbing Wheelchair

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**Abstract**

This paper focuses on the development of a control strategy of a compact stair climbing wheelchair to maintain stable and balance while negotiating staircases in confined spaces for the elderly and disabled. The Visual Nastran 4D is used to develop a simulation models and linked with Matlab platform for control and visual assessment purposes. The challenges are to control front and rear motors as well as tilt angle to ensure system stability and maintain smoothness of the climbing process. PD-Fuzzy controls are developed, tested and associated performances are assessed through intensive visual approach.

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# Introduction

There are total of 11.2 million disabled persons, of whom 0.8 million are children, 5.2 million are working adults and 5.2 million are above their pension age according to 2010/2011 disability prevalence estimation data in Great Britain (Disability factsheet, 2011) [1]. This has caused high demand on some form of transport mechanism and thus wheelchairs continue to play a vital role. Common mobility assistive techniques and recent advances in curb and stair climbing devices are described in this paper. A proposal for a high step stair-

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climbing mechanism based on wheelchair in confined spaces and indoor usage is presented and its feasibility demonstrated in the paper.

There are several types of stair climbing wheelchair and the mechanical design in these three different categories are varies from one another. It can be classified into three categories; crawler type [2-6], wheeled type [7-9] and legged type [10].The approaches adopted in crawler types are non-slip rubber track based on a single and dual section track mechanisms. The control strategy used is fuzzy logic control as an optimal estimation algorithm to estimate the proportion of various factors that affect the track tension. However, it is hard to turn in narrow and small aisle due to its huge structure and the high pressure that exerted at the edge of each stairs can cause stairs damage. Stability control is not considered to the extensive level in a wheeled type and some of them are just based on the inverse kinematic derivation for motion planning. Nakajima has introduced a legged mechanism in 2011 with simulation and experiment validation [11]. It uses supporting polygon to maintain the level of the wheelchair body on at least three points while performing stair climbing. However this mechanism does not seem practical to be used in a place where it has more than two steps and high stairs slope.

Articulated wheel clusters has been used by iBOT 3000 Transporter to overcome the stairs climbing task [12]. The iBOT system then has been replicated by Japanese researchers from University of Tokyo, and they have introduced similar stair climbing wheelchair recently (NOBOROT 2012) [13]. Another recent development reported by the authors is a design using MSC Visual Nastran 4D (VN) environment in year 2012 [14], where actual weight of human and the overall stability of the wheelchair were taken into account. The mechanism is quite simple and thus can be used for indoor purposes without the user needing to hold the guardrails all the times or requiring an assistant. However, the climbing structure was based on pre- determined angle for link1 and link 2 in order to step up the first and further stairs respectively to perform stairs ascending task. The compact wheelchair design presented in this work improves in several ways but maintains the same behavior as in [14].

# Wheelchair model

The equation of motion of the stair climbing wheelchair is too complex to derive due to the nonlinearity of the system. All important variables might be left out when simplification approach is introduced when establishing a mathematical model of the system. A simplified equation of motion is not sufficient to represent a complex stair climbing mechanism with the changing of centre of gravity, COG of human mass. Therefore, the system is designed as close as the standard wheelchair and transformed in a 4D software called Visual Nastran (VN) so that all the nonlinear features will be maintained.

The VN software environment can provide a visualization including the motion of negotiating each stairs, stabilization of the overall wheelchair mechanism, and other functional features. It allows designing and simulation of rigid body dynamics, determining collision response, choosing materials type and identifying input/output of control signal for control purposes when integrating with Matlab/Simulink environment. The gravitational force is taken into consideration as well, thus approximating the real system. There are few researches which embark VN software as a first stage before deploy actual system [15]. A modified and simplified version of wheelchair model using wheels rotation instead of cluster mechanism [14] was designed using VN software. Fig 1 shows the schematic diagram and specific location of the motors required in the wheelchair model. All dimensions were taken from standard wheelchair size except the wheels which were adopted from the iBOT system due to its well known commercial stair climbing wheelchair mechanism.

Main motor namely front motor, *F* , rear motor, *R* and seat motors, *S* are shown in the figure. Three different sensors; one at the vertical cylinder rod for tilt angle control, distance sensor at each wheels to measure distance between wheels and stairs and angular sensor at each links for control measurement. The

input signals applied to the wheelchair model are both right and left front and rear motor torques,

*S*

*F L* / *FR* and

*R L* / *RR*

to lift link while the seat torque,

is to control the tilt angle. The measured outputs are angular

position of Link (degree) for climbing steps as well as tilt angle (degree).

*FL* ,  *FR*



Seat

Tilt

*FL* , *FR*

Link

*S*

Front wheels Rear wheels

Figure 1. Schematic diagram of wheelchair.

The humanoid model using the anthropometric data is approximated and designed [16]. In this work, the humanoid model is developed as a rigid body with 1.5 m in height and weight of approximately 71 kg. There are many types of stairs that have been used, and because they are inherently hazardous, the design must follow standard dimensions and structure to allow safe product manoeuvrability and feasibility (Canadian Centre for Occupational Safety and Health, 2010) [17]. Straight stairway with a slope of 500 was tested in this work and have a height of 8 inch, tread of 12.6 inch and width of 30 inch.

# Controller Structure

Fuzzy Logic control (FLC) is adopted in this wheelchair system and Mamdani-type fuzzy rules with multi- input single output, (MISO) structure is considered with error and change of error as the input as shown in Fig.

2. The angular position of two links (Link 1 and Link 2) are controlled independently with PD-fuzzy logic structures that have equal rule bases. Thus, there are two independent FLCs (FLC 1 and FLC2), one for each

link incorporating two inputs and one output for each FLC (

*R* , *L* ) ,while another FLC3 is for the tilt angle,

*S* . Both FLCs use angular position error, *e*1 and change of angular position error of Link 1, *e*1 . In order

to give smooth transition and response of the climbing task, Gaussian membership function was used. The five membership levels used are Positive Big (PB), Positive Small (PS), Zero (Z), Negative Small (NS) and Negative Big (NB) for both error and change of error. Fig. 3(a) shows the implemented 25 fuzzy rules. Noted that for this fuzzy control structure, the same design is used for all the FLCs, thus only one fuzzy logic controller need to be designed and implementable to all situations. The rules are typically fired as :

‘If *e*1 is **NB** and ‘If *e*1 is **NB** and ‘If *e*1 is **NB** and

.....

*e*1 is **NB** then the Torque is **PB**’ *e*1 is **PB** then the Torque is **Z**’ *e*1 is **PS** then the Torque is **PS**’

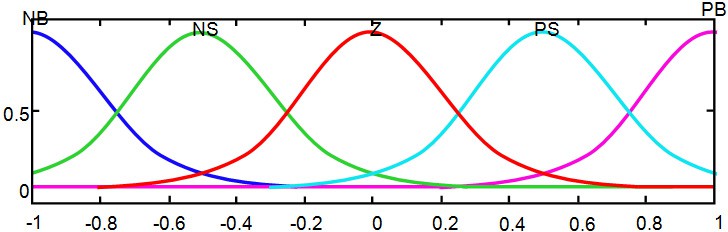
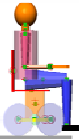


Figure 2:Input output structure and MFs of MISO system

Degree of membership

PD-Fuzzy Logic was implemented in Matlab integrated with VN, and the control structure is as shown in Fig. 3(b). The scaling factors for Fuzzy Logic and PD gains were tuned heuristically. The control objective is to produce sufficient torque to front and rear motors for lifting the rear wheels over the front wheels and the other wheels using cluster called ‘Link’ mechanism while maintaining the human body on the seat levelled. These tasks need to ensure that there will be no levitation or significant displacement of the overall wheelchair mechanism while performing stair climbing operation smoothly.



Position of front wheel

Set point

-

+

*F*

Set point

+

*R*

-

PD-Fuzzy Control

*S*

Tilt angle

Set point

+

*v C*

Cluster angle

+

-

Set point

-

Matlab/Simulink

Visual Nastran

Position of rear wheel

Figure 3: Control system structure

# Simulations

Fig. 4 shows visualization of the wheelchair performance while ascending step 1 and step 2. Initially, the wheelchair stays in four-wheeled configuration on the ground as shown in Fig. 4 (a), then front motor torque, *F* lifts link 1 for positioning rear wheels on the upper step, Fig. 4(b). This mechanism is a two-wheeled

configuration during which stabilization of the system is realized as in Fig. 4(c). Then, rear motor torque, *R*

will lift link 2 in order to transfer the whole wheelchair to the second step as shown in Fig. 4 (d-f). At this

stage, the rear motor cater for stability of the overall mechanism and maintain both wheels at the same position. The challenges are to develop suitable control torques for the respective motors and prevent the whole system including human (amounting up to 100kg) from falling or slipping. As can be seen, seat motor torque, *S* stabilized the seat in the upright position during the whole process at all times. The whole process

is then repeated for climbing on further steps. The associated simulations can be seen in Fig. 5 where Fig. 5(a- b) shows the orientation of the control input signal, link 1 and link 2 for both steps respectively which were set to the desired angle depending on specifications of the stairs. It took the system a total of approximately

2.7s to climb the first staircase before continue to climb second staircase for up to 6s. Fig. 5(c-d) shows the front and rear wheel positions while climbing step 1 and step 2 whereas both wheels only got affected when front motor was performed during climbing step 1 and vice versa. It shows that both wheels maintained stable at the same position without levitating during the overall operation. Furthermore, the tilt angle was maintained levelled throughout the process with a small variation, (-0.5o to 0.5o) as in Fig. 5 (e). Figure 5(f) shows the simulation of the wheelchair during completing final step after performing few stair ascending task. The acting wheels are shown as highlighted in green colour as in Fig. 4 (g) it has some travelled distance in order to perform the final landing process due to the wheel rotation.

# Conclusion

A stair climbing wheelchair has been successfully developed in VN using a standard sized wheelchair. A humanoid model with approximate weight of 71kg and standard sized stairs have been adopted. A Fuzzy control approach has been implemented to perform stair climbing task in an automatic mode wheelchair system. The results presented proved that the FLC works well in controlling highly interchangeable systems which incorporated front and rear motors to perform stair climbing task. It has been demonstrated that the control system is able to perform effectively in order to ensure user comfort and smoothness of the manoeuvring tasks. Future work will look at the stairs descending process, optimization of the control scaling parameters and linear motion.

Perform stair climbing task

|  |
| --- |
| (a) |
| (b) |
| (c) |
| (d)  *S* |
| (e) |
| (f) |
| (g)  ***d*** |

Figure 4. Ascending stairs

Complete final step

100

Angular position of link 1 (degree)

50

200

100

Step1

Step2

Angular position of link 2 (degree)

0 0

-50 -100

-100

0 2 4 6

Time (s)

-200

0 2 4 6

Time (s)

0.1

0

Front wheel position (m)

-0.1

-0.2

-0.3

-0.4

-0.5

(a) Angular positions of link 1 (b) Angular positions of link 2

0.6

Step1

left wheel right wheel

left wheel

right wheel

Step2

0.4

Rear wheel position (m)

0.2

0

-0.2

-0.6

0 2 4 6

Time (s)

-0.4

0 1 2 3 4 5 6

Time (s)

(c) Front wheel position (d) Right wheel position

1

Step1 Step2

0.5

0

0.5

Tiltangle(degree)

Tilt angle, (degree)

-

-1

0 2 4 6

Time (s)

(e) Tilt angle during climbing steps

0.5

TAinlgtulaarnpogsliteio,no(fdtieltganrgelee()degree)

-

0

0.5

-1

0 1 2 3 4 5

Time (s)

(f) Tilt angle in completing final step Figure 5. Wheelchair performance in completing ascending task

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