Duty Cycle Optimization of Sensors in Wireless Body Area Network Based on Reinforcement Learning

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*Abstract*—Blood pressure (BP) is one of many rhythmic physiological indicators, and its home monitoring has great value and long-term significance. This paper establishes a two-dimensional blood pressure change model based on Circadian and Seasonal variation of blood pressure. We use the maximum and trend to characterize the state of blood pressure over a period of time. Blood pressure sensors can be used to sense the BP data in wireless body area network (WBAN). Our goal is to achieve a balance between power saving and low latency by optimizing the sensor duty cycle based on the BP model. To solve the problem, we establish it into a markov decision process (MDP) and then use the Deep Q-learning Network(DQN) method in Reinforcement Learning (RL) to find the best result. To test the validity of the algorithm, we simulated 180 days of blood pressure data for testing. Simulation results show that the algorithm can effectively reduce energy consumption and perform well in sensing delay.

*Index Terms*—blood pressure, duty cycle, Reinforcement Learning, wireless body area network

# INTRODUCTION

As the level of medical care continues to improve, the level of medical services that people enjoy continues to improve. In order to enable more people to enjoy the high-quality services brought by modern medical care, more and more high-tech is being used. The family health monitoring system allows patients to be physically monitored at home or in the office without having to stay in the hospital. At the same time, a more familiar and comfortable environment is also conducive to patient recovery. Wireless body area network (WBAN) is a technology commonly used to implement a home health monitoring system [1]. Taking BP monitoring as an example, Fig. 1 is a schematic diagram of the WBAN model.

The BP sensor is placed on the surface of the skin or embedded in the human body, and the data is collected and sent to the network coordinator. Finally, the data is sent over the wireless network to the home server and medical server. Patients and medical staff can analyze and process the collected data.

Like the general wireless sensor network (WSN), the sensor node battery life in the WBAN is limited, so it is also necessary to consider the service life of the sensor node [2]. In article [2] the duty cycle is defined as the ratio between the time during which a sensor node is in active state and the total time of active/dormant states. It considered the upper-bound of the WSN lifetime based on random duty cycle. This paper focuses on optimizing the duty cycle of the sensor to save energy while not damaging the immediacy of the induction by understanding the process of physiological index changes.

The major contributions of this paper can be summarized as follows:

* We establish a two-dimensional blood pressure change model based on circadian and seasonal variation of blood pressure, using the maximum and trend to characterize the state of blood pressure over a period of time.
* We design an algorithm based on DQN to optimize the duty cycle of the sensor for energy saving and low latency. It is verified by simulation that the algorithm is effective.

# blood Pressure Change Model

Human physiological indicators are mainly affected by nerves and body fluids (hormones), and have the characteristics of circadian and seasonal variation. We divide a change cycle into multiple observation windows, and calculate several statistics of physiological indicators in the windows, which can effectively help us understand the patient's physical condition. Due to the rhythm of physiological indicators, the corresponding statistics also have a certain change law.

## Circadian and Seasonal Variation

Ambulatory blood pressure measurement plays an important role in monitoring certain diseases. Article [3] studies the changes in BP in patients and gives some images of circadian pattern of systolic BP of normotensive and hypertensive patients. In most individuals, BP rises significantly after getting up in the morning and falls at night.

Article [4] studied the seasonal variation in BP over a longer span of time and concluded that systolic BP and diastolic BP are higher in winter than in summer. This process of seasonal variation can be seen as a process of gradual change between day and day, essentially related to climatic factors such as outdoor temperature.

## Observation Windows

As mentioned above, changes in physiological indicators are periodic, and the regularity of changes in each cycle is stable. For example, the change cycle of blood pressure is 24 hours, higher in the morning and lower in the evening. Since the range of blood pressure changes is relatively large, it is necessary to divide a cycle into smaller intervals. As a result the magnitude and complexity of the numerical changes in the interval are reduced, which is beneficial for us to observe the physiological condition of the patient.

As shown in Fig. 2, we divide a cycle T into several windows (i=1,2, ,N). The length of each window is determined according to the situation. Different window lengths may be equal or unequal. Each window has its own sensor duty cycle, which is the focus of our research.

Within each window we define multiple time slots of equal length and control the sensor for sampling or sleep in each time slot. Each window has its own unique sensor sampling scheme. Obviously, when the proportion of sampling is large, the monitoring effect is better but the energy consumption is larger. When the proportion of sleep is large, the energy consumption is small but has an effect on the monitoring effect. So our goal is to find a balance between energy consumption and monitoring effect. Fig. 3 is a schematic illustration of time slots.

## Two-dimensional Windows Model

Taking into account the circadian and seasonal variation of blood pressure, we consider the change in blood pressure within one day as one direction, and the change between day and day as another direction. Assuming that the lengths of the windows are equal, we can obtain the two-dimensional model of observation windows. Fig. 4 is a schematic diagram of the model.

As mentioned before, each window has a series of blood pressure data, and we will process the data in the window to extract features in later section.

# Window Feature Vector

The BP data in the window is usually too many and not intuitive. In order to better describe the state of BP during this time period, we performed statistical processing on BP data. This process involves calculating the maximum value and trend of the data. After obtaining the statistical results, we divide it into multiple intervals, corresponding to multiple maximum value states *v* and trend states *z*, and finally get the window feature vector (*v*, *z*).

## Maximum Value State

The maximum blood pressure data within the window characterizes the peak reached by the patient's blood pressure during that time period. For the patient, the maximum is the most dangerous moment in the period. When the maximum value is within the interval exceeding the normal value, both the medical staff and the patient should pay sufficient attention to it. Table 1 is the latest WHO standard, which divides systolic BP into multiple intervals. We decided to use a similar partitioning criterion to extract the feature from the maximum value and obtain the maximum value state *v*.

Table 1 shows that the patient is hypertension when the systolic BP exceeds 140 mmHg. 130 mmHg to 140mmHg is normal high BP, and 120 mmHg to 130mmHg is normal BP. Systolic BP of less than 120 mmHg is desirable. Considering that the hypotensive standard is generally less than 90 mmHg, we divide the peak of BP into multiple intervals, as shown in (3.1).

 (3.1)

The value of *v* can characterize the peak condition of the current window. Obviously, when *v* equals 4, it indicates that the patient's BP exceeds the normal value in this window，which needs to be vigilant. When *v* is equal to other values, it can also describe the peak situation to a certain extent, which is good for us to judge the physical condition.

## Trend State

There are many statistical tests that can be used to assess the importance of time series trends. One of the commonly used nonparametric trend tests is the Mann-Kendall trend test. It is widely used to distinguish whether a natural process is in natural fluctuations or there is a definite trend. This paper uses this test method to determine whether the BP in the windows shows a significant change trend.

The rank correlation test for a set of observations is formulated as follows. Eq. (3.2) is the calculation method of *S*:

 (3.2)

where

 (3.3)

When n is large enough, the statistic *S* tends to be normally distributed and the variance of *S* is calculated as in Eq. (3.4):

 (3.4)

The Mann-Kendall trend test is calculated as in Eq. (3.5):

 (3.5)

satisfies the standard normal distribution. When the absolute value of is greater than or equal to 1.28, 1.64, 2.32, it means that the confidence is 90%, 95%, and 99% significance test respectively.

With a confidence of 99%, we define three intervals for as three states, as in Eq. (3.6):

 (3.6)

Obviously, the data trend is decreasing when , the data trend is flat when , and the data trend is rising when . We use the value of z to determine the trend of blood pressure in the windows. Combined with the peak state *v* mentioned above, we obtain the window feature vector (*v*, *z*), which can effectively describe the blood pressure data in the windows. In the following sections, we use the vectors to study, so that the sensor adjusts the duty cycle according to the actual situation.

# Coupled Markov Chain Theory

In the section 2 we define the observation windows and in the section 3 define the feature vector describing the state of the data within the windows. Due to the circadian and seasonal variation of BP, the eigenvector sequence can be established as a Markov chain. Because blood pressure changes in two dimensions, the one-dimensional Markov chain cannot fully describe the process, so we need to establish a two-dimensional coupled Markov chain and list the transition probability. Article [5] gives the concept of a coupled Markov chain.

The Markov chain is a probabilistic model that exhibits special dependencies. The future depends on the current and has a transition probability, but is not associated with the past. In the model of this paper, the Markov property is expressed as: the future window feature vector *W* depends on the current *W.* For a single-dimensional Markov chain, such a property can be expressed as in Eq. (4.1):



(4.1)

where is the sequence of window feature vectors and is the state space.

Obviously, represents the probability of transitioning from state to state , where n is the number of states in the model. Thus we can use to represent the one-dimensional state transition probability, and there are two constraints expressed as shown in Eq. (4.2):

 (4.2)

The coupled Markov chain describes the joint behavior of Markov chains in both directions. The current state depends on the previous state in both directions and has a joint transition probability. Similar to the one-dimensional Markov chain, we describe the Markov chain in the horizontal direction as shown in Eq. (4.3):

 (4.3)

where is the window feature vector of the jth window of the ith day.

The Markov chain in the vertical direction is described as shown in Eq. (4.4):

 (4.4)

Coupled Markov chains are obtained by coupling horizontal and vertical chains, but forcing the chains in both directions to reach an equal state. Thus we get the joint transition probability:

 (4.5)

where *C* is a normalizing constant whose value is equal to that shown in Eq. (4.6):

 (4.6)

Thus we get the joint transition probability by combining Eq. (4.5) and Eq. (4.6):

 (4.7)

The joint state transition probability indicates the effect of the window state of the previous day and the previous period on the current state. This means that the current state can be predicted to some extent. In the following sections we will use the RL method to optimize the sensor duty cycle based on the window feature and joint transition probability.

# Optimization Goal

The goal of this paper is to optimize the duty cycle of the sensors based on the state of the windows and the transition probability. In general, the duty cycle of a sensor is the ratio of the length of sampling to the period in a period. A higher duty cycle means that the sleep time is shorter in the same amount of time. As mentioned before, the patient's BP is generally low at night, and if the high duty cycle is still used, the energy of the sensor is wasted. Therefore, we use the RL method to adaptively optimize the duty cycle to reduce energy consumption without affecting the use effect.

In order to facilitate us to judge the effect of a certain duty cycle, we specify the cycle mode of sensors sampling and sleep as shown in Fig. 5. In the window, it is assumed that the number of time slots collected in one cycle is , and the number of time slots in sleep is . The acquisition starts from the first time slot of the window, and after collecting slots, it sleeps, and after slots, it starts sampling again. Loop through this mode until the end of the window.

Since and are small relative to the length of the window, we calculate the duty cycle of the window as shown in Eq. (5.1):

 (5.1)

In this paper, we use two calculations when we judge whether the duty cycle in the window is appropriate: energy consumption and delay *.* The final goal is to find the optimal duty cycle based on these two calculations.

Article [2] introduced a formula for calculating the energy consumption (J/s) of a sensor for WSN as shown in Eq. (5.2):

 (5.2)

where is the average sensing rate, is the energy consumption to sense a bit of data, is the transceiver relay data rate, is energy consumed per bit by the transmitter electronics, is the energy consumed per bit in the transmit op-amp, is the transmission distance and is the sleep state energy consumption per second.

In general, the energy consumed by the sensor during sleep is relatively low, so the energy consumption of the sensor is positively related to the duty cycle . When the is large, the energy consumption is large, and vice versa. For most sensor nodes in WSN, the energy of transmitting per bit of data is much greater than the energy consumed by sensing per bit of data. The energy consumption by a sensor node in WSN per second across a distance *d* with path loss exponent *n* is as shown in Eq. (5.3).

 (5.3)

In a specific scenario and application, the transmission power has a maximum and minimum limit as shown in Eq. (5.4).

 (5.4)

After the duty cycle in a window is determined, according to our specified cycle mode of sensors sampling and sleep, we can define the delay as the interval between the time when sensor first senses the abnormal blood pressure and the time when the blood pressure actually reaches abnormal in one window. Obviously, the delay indicates the degree of danger of the current duty cycle. If the is high, the current duty cycle may cause the patient's condition to be undetected and processed in a timely manner. This can be very dangerous for the patient. So we want to control the delay within the allowed range as shown in Eq. (5.5).

 (5.5)

Therefore, our goal is to find the right duty cycle to achieve the best balance of energy consumption and delay. To quantify the plausibility of the duty cycle of each window, we define a reward function based on energy consumption and delay as shown in Eq. (5.6).

 (5.6)

The function  is a decreasing function with respect to and . When the values of and are small, the value of the reward function is large. So our goal is to maximize the sum of the reward functions of all windows and meet some constraints, as shown in Eq. (5.7).

 (5.7)

# Algorithm based on reinforcement learning

Reinforcement Learning is a common machine learning method. For the specific problem, it obtains the influence of each action on the state and the reward obtained by the action through the reward function. The goal is to get the optimal policy , which is the sequence of best actions. We designed an algorithm based on DQN in RL and used it to solve our optimization problem.

## Deep Q-Learning Network

A Markov decision process (MDP) can be characterized by the following variables: state space (which is a finite set), action space (a set of finite actions), state transition probability matrix, reward function, and discount factor. State refers to the state in which the agent is currently located, usually consisting of a series of discrete values that make up its state space. Action is an action taken by agent that affects the state and is usually a limited set. The state transition probability describes the probability of a transition between states. The state transition probability is one of the components describing the Markov process. The reward function is used to describe the degree of advantage of the state, usually a positive value indicates an acceptable state and a negative value indicates a state that should be avoided.

Using several elements of MDP, we can create a Q-table as shown in Fig. 6.

In Fig. 6, Q-table maps the state space to the action space one by one, and the values in the table represent the maximum future reward expectations for taking the action in that state. The initial value is set to 0. Based on this table, the agent can choose the appropriate decision for each action.

In order to get a Q-table with good enough effect, we use the DQN method. In each episode, we explore the action by using the *ε*-greedy strategy. This strategy chooses exploitation with the probability of *ε* and chooses exploration with a probability of .If it is the exploration phase, we randomly select an action corresponding to the current state. If it is the exploitation phase, we select the action with the largest . After the action selection, the next state and the corresponding reward function are obtained, and the of the current state in the Q-table is updated by Eq. (6.1)

 (6.1)

where is the reward for taking that action at that state, is the maximum expected future reward given the new state and all possible actions at that new state,α is learning rate and is discount rate.

## Optimization Algorithm

Based on the DQN, we designed an optimization algorithm to solve our problem. According to the principle of the algorithm, we initialize the Q-table and each coefficient, and set the *ε-*greedy algorithm to be related to the number of episode. When the number of episode increases, the probability of exploitation will be higher. The reward function is calculated during the episodes and the Q-table is updated according to Eq. (6.1) until the training is completed.

In our algorithm, the state vector *s* is set as (*v*, *z*,,). For a particular window feature vector (*v*, *z*), the final goal of our training is to have a specific duty cycle expressed as a specific combination of and . Action *a* is set to multiple values, corresponding to changing and . At the beginning of the algorithm, the parameters are initialized, and the values in the Q-table are all set to 0. In each episode, we start from the first observation window and calculate *v* and *z*. Then we find the corresponding state vector *s* in the Q-table. We set *ε* to the expression associated with episode as shown in Eq. (6.2).

 (6.2)

where is a constant used to control the change rate of *ε* and σ is a constant used to control the initial value of *ε*.

A random number is generated each episode and compared with *ε* to determine the selection strategy of the action. According to the *ε*-greedy strategy, if in the exploration phase, one action is randomly selected, and in the exploitation phase, the action with the largest  is selected. After that, the and of the next window are changed according to the action. Then slide the window backwards and calculate the reward function r, which can be used to update the .Repeat this process until the number of episode reaches the maximum value N we set at the beginning.

# Simulation results

Human physiological indicators are mainly affected by nerves and body fluids (hormones), and have the characteristics of circadian and seasonal variation. We divide a change cycle into multiple observation windows, and calculate several statistics of physiological indicators in the windows, which can effectively help us understand the patient's physical condition. Due to the rhythm of physiological indicators, the corresponding statistics also have a certain change law.

## Circadian and Seasonal Variation

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|  |  |
| --- | --- |
| **Algorithm** DQN-Based optimization window duty cycle scheme | |
| 1: | Initial Q-table and *s*; |
| 2: | Initial α,γ,β and N; |
| 3: | Initial ; |
| 4: | Initial ,; |
| 5: | repeat |
| 6: | Initial the sum of the reward ; |
| 7: | Initial and ; |
| 8: | ; |
| 9: | Randomly generate ; |
| 10: | Calculate *v* and *z* of ; |
| 11: | repeat |
| 12: | If : |
| 13: | Choose a randomly; |
| 14: | If: |
| 15: | ; |
| 16: | ove to next window; |
| 17: | Change and according to a; |
| 18: | Obtain *s*’ and *r*; |
| 19: | ; |
| 20: | Update Q-table by Eq. (6.1); |
| 21: | until( is the last observation window) |
| 22: | ; |
| 23: | Until() |

Article [4] studied the seasonal variation in BP over a longer span of time and concluded that systolic BP and diastolic BP are higher in winter than in summer. This process of seasonal variation can be seen as a process of gradual change between day and day, essentially related to climatic factors such as outdoor temperature.

## Observation Windows

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## Two-dimensional Windows Model

Taking into account the circadian a

# MATH

If you are using *Word,* use either the Microsoft Equation Editor or the *MathType* add-on (http://www.mathtype.com) for equations in your paper (Insert | Object | Create New | Microsoft Equation *or* MathType Equation). “Float over text” should *not* be selected.

## Equations

Number equations consecutively with equation numbers in parentheses flush with the right margin, as in (1). First use the equation editor to create the equation. Then select the “Equation” markup style. Press the tab key and write the equation number in parentheses. To make your equations more compact, you may use the solidus ( / ), the exp function, or appropriate exponents. Use parentheses to avoid ambiguities in denominators. Punctuate equations when they are part of a sentence, as in

(1)

Be sure that the symbols in your equation have been defined before the equation appears or immediately following. Italicize symbols (*T* might refer to temperature, but T is the unit tesla). Refer to “(1),” not “Eq. (1)” or “equation (1),” except at the beginning of a sentence: “Equation (1) is ... .”

# Units

Use either SI (MKS) or CGS as primary units. (SI units are strongly encouraged.) English units may be used as secondary units (in parentheses). This applies to papers in data storage**.** For example, write “15 Gb/cm2 (100 Gb/in2).” An exception is when English units are used as identifiers in trade, such as “3½-in disk drive.” Avoid combining SI and CGS units, such as current in amperes and magnetic field in oersteds. This often leads to confusion because equations do not balance dimensionally. If you must use mixed units, clearly state the units for each quantity in an equation.

The SI unit for magnetic field strength *H* is A/m. However, if you wish to use units of T, either refer to magnetic flux density *B* or magnetic field strength symbolized as µ0*H*. Use the center dot to separate compound units, e.g., “A·m2.”

# Some Common Mistakes

The word “data” is plural, not singular. The subscript for the permeability of vacuum µ0 is zero, not a lowercase letter “o.” The term for residual magnetization is “remanence”; the adjective is “remanent”; do not write “remnance” or “remnant.” Use the word “micrometer” instead of “micron.” A graph within a graph is an “inset,” not an “insert.” The word “alternatively” is preferred to the word “alternately” (unless you really mean something that alternates). Use the word “whereas” instead of “while” (unless you are referring to simultaneous events). Do not use the word “essentially” to mean “approximately” or “effectively.” Do not use the word “issue” as a euphemism for “problem.” When compositions are not specified, separate chemical symbols by en-dashes; for example, “NiMn” indicates the intermetallic compound Ni0.5Mn0.5 whereas “Ni–Mn” indicates an alloy of some composition NixMn1-x.

Be aware of the different meanings of the homophones “affect” (usually a verb) and “effect” (usually a noun), “complement” and “compliment,” “discreet” and “discrete,” “principal” (e.g., “principal investigator”) and “principle” (e.g., “principle of measurement”). Do not confuse “imply” and “infer.”

Prefixes such as “non,” “sub,” “micro,” “multi,” and “ultra” are not independent words; they should be joined to the words they modify, usually without a hyphen. There is no period after the “et” in the Latin abbreviation “*et al.*” (it is also italicized). The abbreviation “i.e.,” means “that is,” and the abbreviation “e.g.,” means “for example” (these abbreviations are not italicized).

A general IEEE styleguide is available at [www.ieee.org/authortools](http://www.ieee.org/authortools).



Fig. 1. Magnetization as a function of applied field. Note that “Fig.” is abbreviated. There is a period after the figure number, followed by two spaces. It is good practice to explain the significance of the figure in the caption.

TABLE I

Units for Magnetic Properties

|  |  |  |
| --- | --- | --- |
| Symbol | Quantity | Conversion from Gaussian and  CGS EMU to SI a |
| Φ | magnetic flux | 1 Mx → 10−8 Wb = 10−8 V·s |
| *B* | magnetic flux density,  magnetic induction | 1 G → 10−4 T = 10−4 Wb/m2 |
| *H* | magnetic field strength | 1 Oe → 103/(4π) A/m |
| *m* | magnetic moment | 1 erg/G = 1 emu  → 10−3 A·m2 = 10−3 J/T |
| *M* | magnetization | 1 erg/(G·cm3) = 1 emu/cm3  → 103 A/m |
| 4π*M* | magnetization | 1 G → 103/(4π) A/m |
| σ | specific magnetization | 1 erg/(G·g) = 1 emu/g → 1 A·m2/kg |
| *j* | magnetic dipole  moment | 1 erg/G = 1 emu  → 4π × 10−10 Wb·m |
| *J* | magnetic polarization | 1 erg/(G·cm3) = 1 emu/cm3  → 4π × 10−4 T |
| χ*,* κ | susceptibility | 1 → 4π |
| χρ | mass susceptibility | 1 cm3/g → 4π × 10−3 m3/kg |
| μ | permeability | 1 → 4π × 10−7 H/m  = 4π × 10−7 Wb/(A·m) |
| μr | relative permeability | μ → μr |
| *w, W* | energy density | 1 erg/cm3 → 10−1 J/m3 |
| *N, D* | demagnetizing factor | 1 → 1/(4π) |

Vertical lines are optional in tables. Statements that serve as captions for the entire table do not need footnote letters.

aGaussian units are the same as cg emu for magnetostatics; Mx = maxwell, G = gauss, Oe = oersted; Wb = weber, V = volt, s = second, T = tesla, m = meter, A = ampere, J = joule, kg = kilogram, H = henry.

# Guidelines for Graphics Preparation and Submission

## Types of Graphics

The following list outlines the different types of graphics published in IEEE journals. They are categorized based on their construction, and use of color / shades of gray:

### *Color/Grayscale figures*

### Figures that are meant to appear in color, or shades of black/gray. Such figures may include photographs, illustrations, multicolor graphs, and flowcharts.

### *Line Art figures*

### Figures that are composed of only black lines and shapes. These figures should have no shades or half-tones of gray, only black and white.

### *Author photos*

### Head and shoulders shots of authors that appear at the end of our papers.

### *Tables* Data charts which are typically black and white, but sometimes include color.

## Multipart figures

Figures compiled of more than one sub-figure presented side-by-side, or stacked. If a multipart figure is made up of multiple figure types (one part is lineart, and another is grayscale or color) the figure should meet the stricter guidelines.

## File Formats For Graphics

Format and save your graphics using a suitable graphics processing program that will allow you to create the images as PostScript (PS), Encapsulated PostScript (.EPS), Tagged Image File Format (.TIFF), Portable Document Format (.PDF), or Portable Network Graphics (.PNG) sizes them, and adjusts the resolution settings. If you created your source files in one of the following programs you will be able to submit the graphics without converting to a PS, EPS, TIFF, PDF, or PNG file: Microsoft Word, Microsoft PowerPoint, or Microsoft Excel. Though it is not required, it is strongly recommended that these files be saved in PDF format rather than DOC, XLS, or PPT. Doing so will protect your figures from common font and arrow stroke issues that occur when working on the files across multiple platforms. When submitting your final paper, your graphics should all be submitted individually in one of these formats along with the manuscript.

## Sizing of Graphics

Most charts, graphs, and tables are one column wide (3.5 inches / 88 millimeters / 21 picas) or page wide (7.16 inches / 181 millimeters / 43 picas). The maximum depth a graphic can be is 8.5 inches (216 millimeters / 54 picas). When choosing the depth of a graphic, please allow space for a caption. Figures can be sized between column and page widths if the author chooses, however it is recommended that figures are not sized less than column width unless when necessary.

There is currently one publication with column measurements that do not coincide with those listed above. Proceedings of the IEEE has a column measurement of 3.25 inches (82.5 millimeters / 19.5 picas).

The final printed size of author photographs is exactly   
1 inch wide by 1.25 inches tall (25.4 millimeters x 31.75 millimeters / 6 picas x 7.5 picas). Author photos printed in editorials measure 1.59 inches wide by 2 inches tall (40 millimeters x 50 millimeters / 9.5 picas x 12 picas).

## Resolution

The proper resolution of your figures will depend on the type of figure it is as defined in the “Types of Figures” section. Author photographs, color, and grayscale figures should be at least 300dpi. Line art, including tables should be a minimum of 600dpi.

## Vector Art

In order to preserve the figures’ integrity across multiple computer platforms, we accept files in the following formats: .EPS/.PDF/.PS. All fonts must be embedded or text converted to outlines in order to achieve the best-quality results.

## Color Space

The term color space refers to the entire sum of colors that can be represented within the said medium. For our purposes, the three main color spaces are Grayscale, RGB (red/green/blue) and CMYK (cyan/magenta/yellow/black). RGB is generally used with on-screen graphics, whereas CMYK is used for printing purposes.

All color figures should be generated in RGB or CMYK color space. Grayscale images should be submitted in Grayscale color space. Line art may be provided in grayscale OR bitmap colorspace. Note that “bitmap colorspace” and “bitmap file format” are not the same thing. When bitmap color space is selected, .TIF/.TIFF/.PNG are the recommended file formats.

## Accepted Fonts Within Figures

When preparing your graphics IEEE suggests that you use of one of the following Open Type fonts: Times New Roman, Helvetica, Arial, Cambria, and Symbol. If you are supplying EPS, PS, or PDF files all fonts must be embedded. Some fonts may only be native to your operating system; without the fonts embedded, parts of the graphic may be distorted or missing.

A safe option when finalizing your figures is to strip out the fonts before you save the files, creating “outline” type. This converts fonts to artwork what will appear uniformly on any screen.

## Using Labels Within Figures

### Figure Axis labels

Figure axis labels are often a source of confusion. Use words rather than symbols. As an example, write the quantity “Magnetization,” or “Magnetization *M*,” not just “*M*.” Put units in parentheses. Do not label axes only with units. As in Fig. 1, for example, write “Magnetization (A/m)” or “Magnetization (Am−1),” not just “A/m.” Do not label axes with a ratio of quantities and units. For example, write “Temperature (K),” not “Temperature/K.”

Multipliers can be especially confusing. Write “Magnetization (kA/m)” or “Magnetization (103 A/m).” Do not write “Magnetization (A/m) × 1000” because the reader would not know whether the top axis label in Fig. 1 meant 16000 A/m or 0.016 A/m. Figure labels should be legible, approximately 8 to 10 point type.

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2. E. P. Wigner, “Theory of traveling-wave optical laser,”   
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3. P. Kopyt *et al., “*Electric properties of graphene-based conductive layers from DC up to terahertz range,” *IEEE THz Sci. Technol.,* to be published. DOI: 10.1109/TTHZ.2016.2544142.

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Dr. Author was a recipient of the International Association of Geomagnetism and Aeronomy Young Scientist Award for Excellence in 2008, and the IEEE Electromagnetic Compatibility Society Best Symposium Paper Award in 2011.

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Mr. Author’s awards and honors include the Frew Fellowship (Australian Academy of Science), the I. I. Rabi Prize (APS), the European Frequency and Time Forum Award, the Carl Zeiss Research Award, the William F. Meggers Award and the Adolph Lomb Medal (OSA).

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