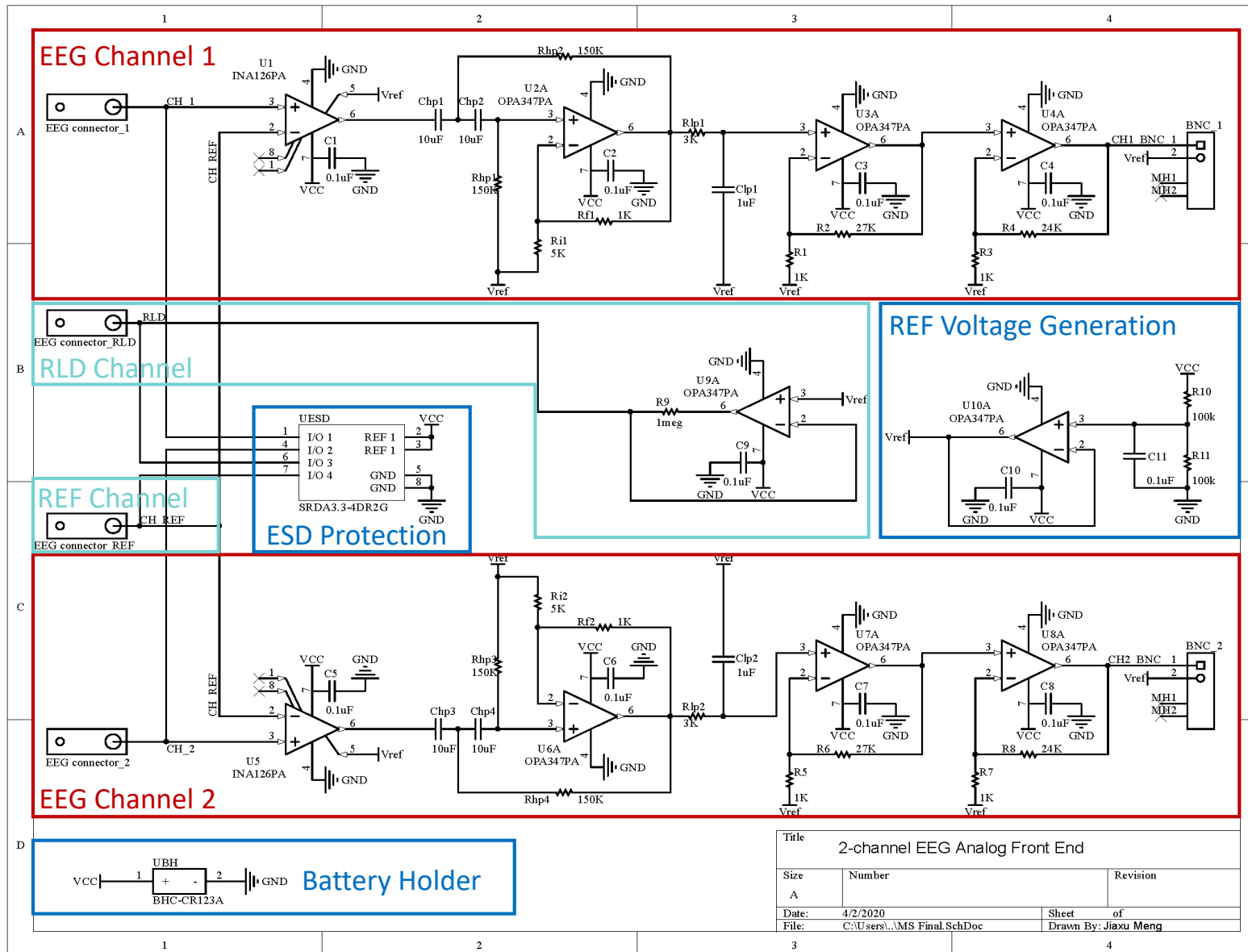


# 2-Channel Low-Power Wireless Scalp EEG System Analog Front End PCB Design

Jiaxu Meng

# Full Schematic



## 2 EEG channels

- 1<sup>st</sup> stage: EEG signal acquisition
- 2<sup>nd</sup> stage: band pass filtering 0.1-50Hz
- 3<sup>rd</sup> and 4<sup>th</sup> stage: amplification
- Gain: 72.5dB (x4200)
- High input impedance
- High CMRR

## Reference voltage

- single power supply: +3V battery
- rise subject's baseline voltage up to +1.5V for signal integrity

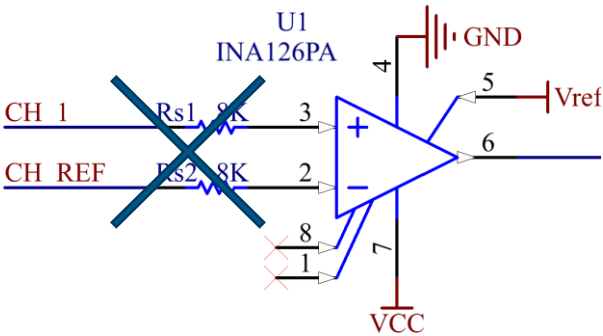
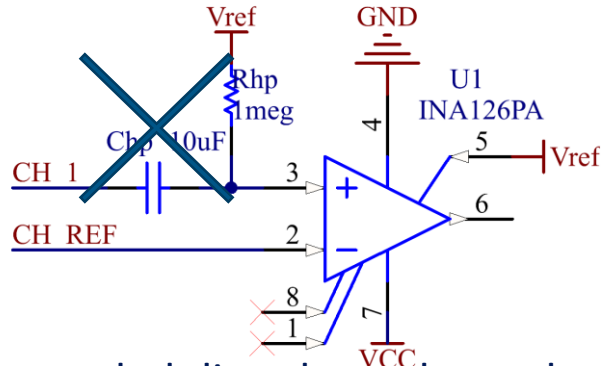
## RLD channel

- reduce  $V_{cm}$ : negative feedback
- safety:  $1M\Omega$  resistance in case of leakage

# Signal Acquisition and Output



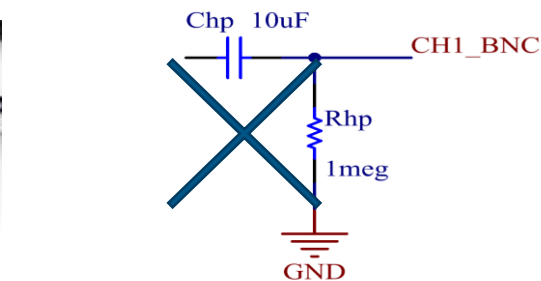
- EEG electrodes
- coupled directly to electrodes



- compensation RES sacrifices Zin



- BNC

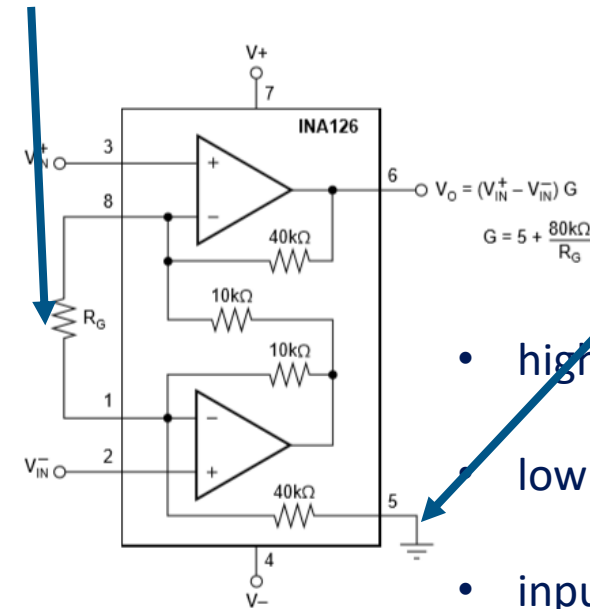


- NI ADC can use floating point

- INA126 circuitry

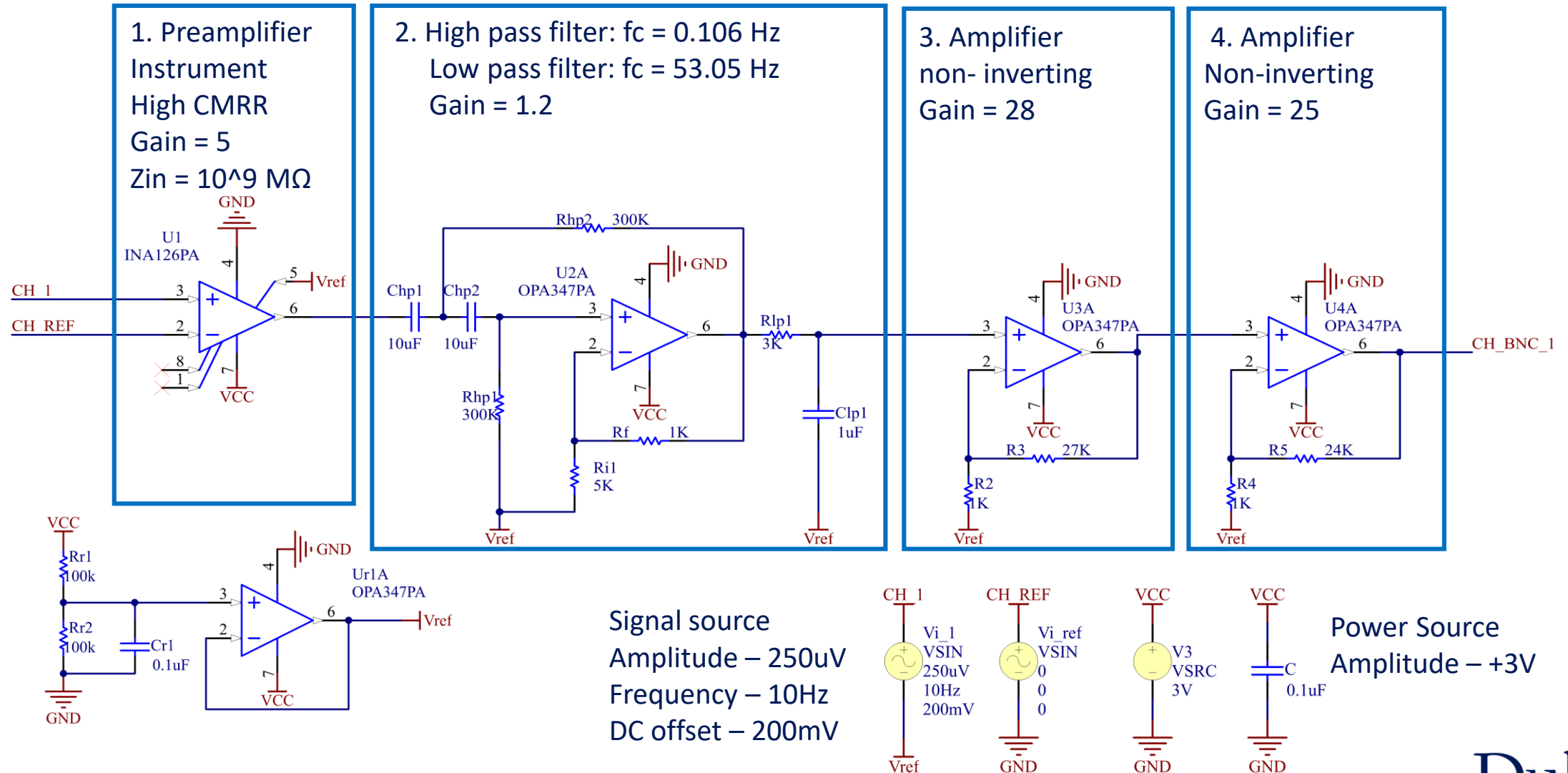
INA operates on Vref by feeding Vref voltage into pin5

Rg is open circuit  $\rightarrow G = 5$

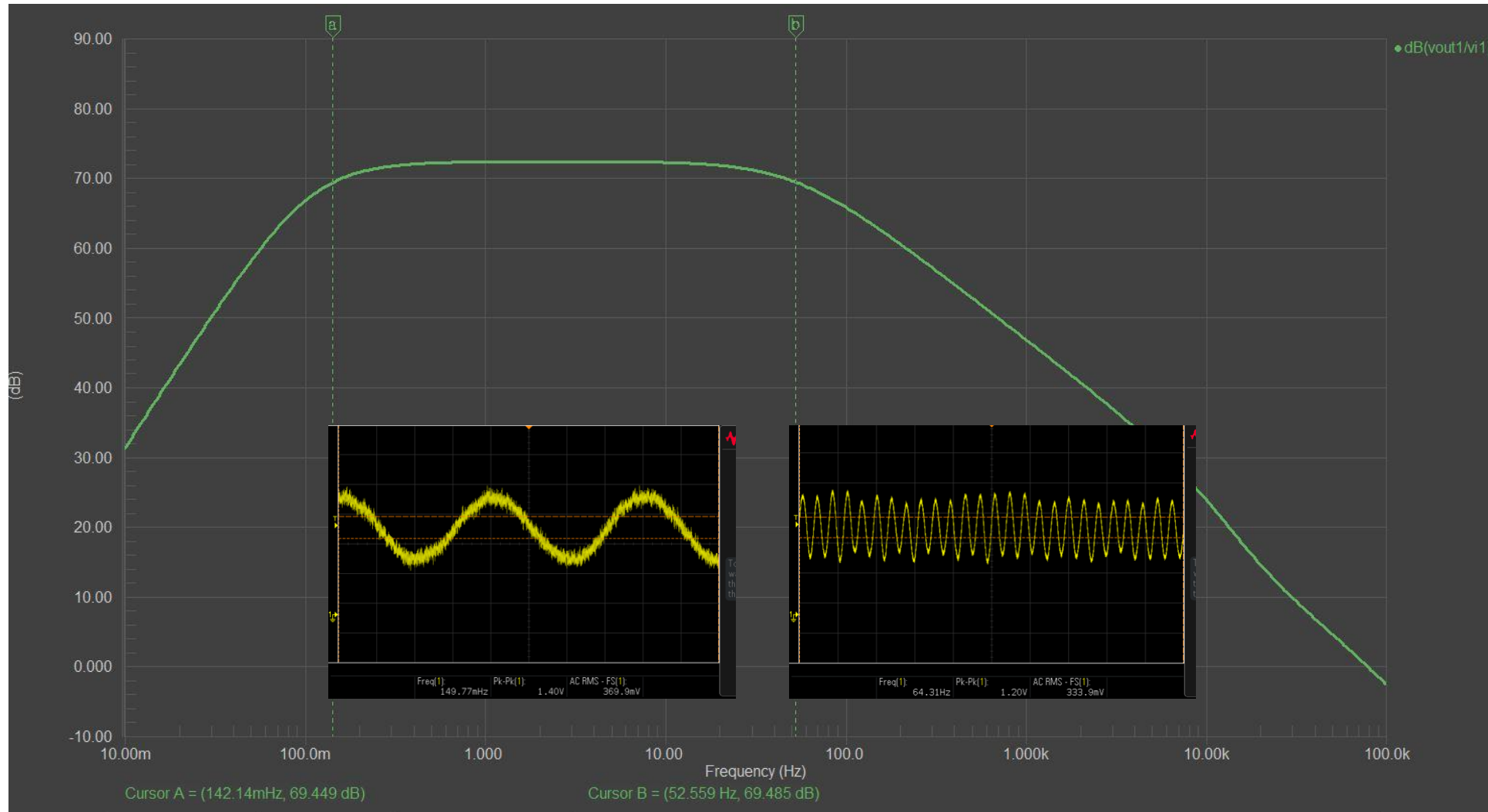


- high CMRR
- low input bias current
- input buffering  $\rightarrow$  high Zin
- adjustable differential gain by Rg

# Schematic for Simulation



# Simulation vs Bench Testing – Frequency Response

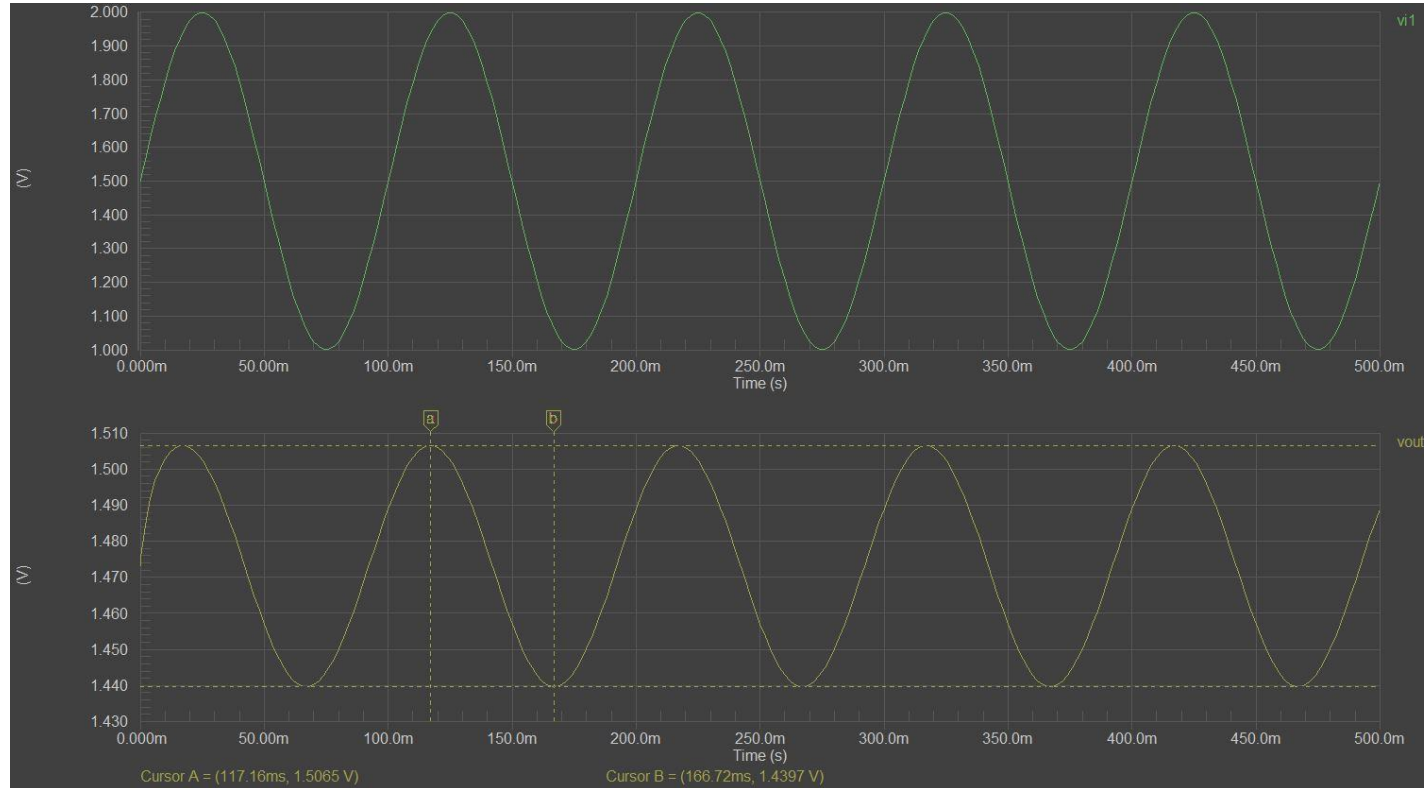


Method: The passband is obtained by manually adjusting input signal frequency until the output signal magnitude decreased by 3dB (became 0.707 times of  $V_{out}/V_i$ ) through filtering stage

Simulation: passband is 0.071Hz – 53Hz

Bench Testing: passband is 0.15Hz – 64Hz

# Simulation vs Bench Testing – CMRR



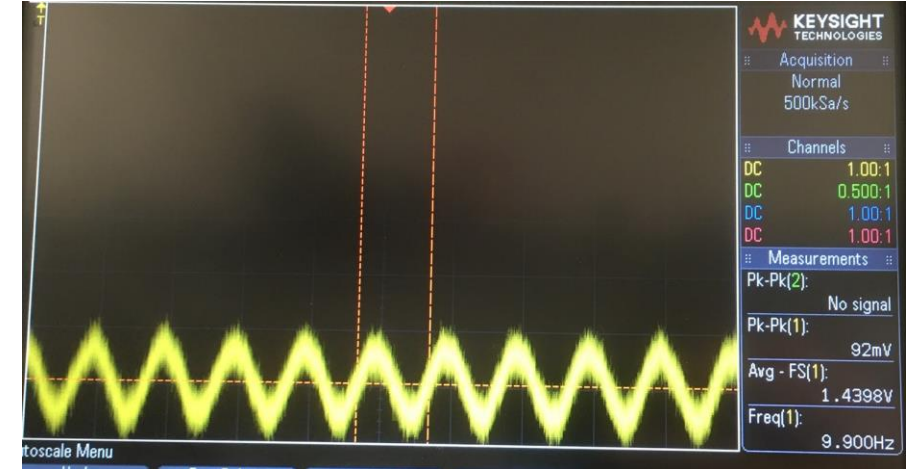
CMRR calculation:

$$A_d = 5 \times 1.2 \times 28 \times 25 = 4200$$

$$V_{cm\_in} = 500\text{mV}$$

$$A_{cm} = \frac{V_{cm\_out}}{V_{cm\_in}} = \frac{1.5065 - 1.4397}{1} = 0.0668$$

$$\text{CMRR} = 20\log \frac{A_d}{A_{cm}} = 20\log \frac{4200}{0.0668} = 96\text{dB}$$



Method: Input a  $V_{cm}$  with magnitude of 500mV to both INA input pins and record the output signal for calculation

CMRR calculation:

$$A_d = 3860$$

$$V_{cm\_in} = 500\text{mV}$$

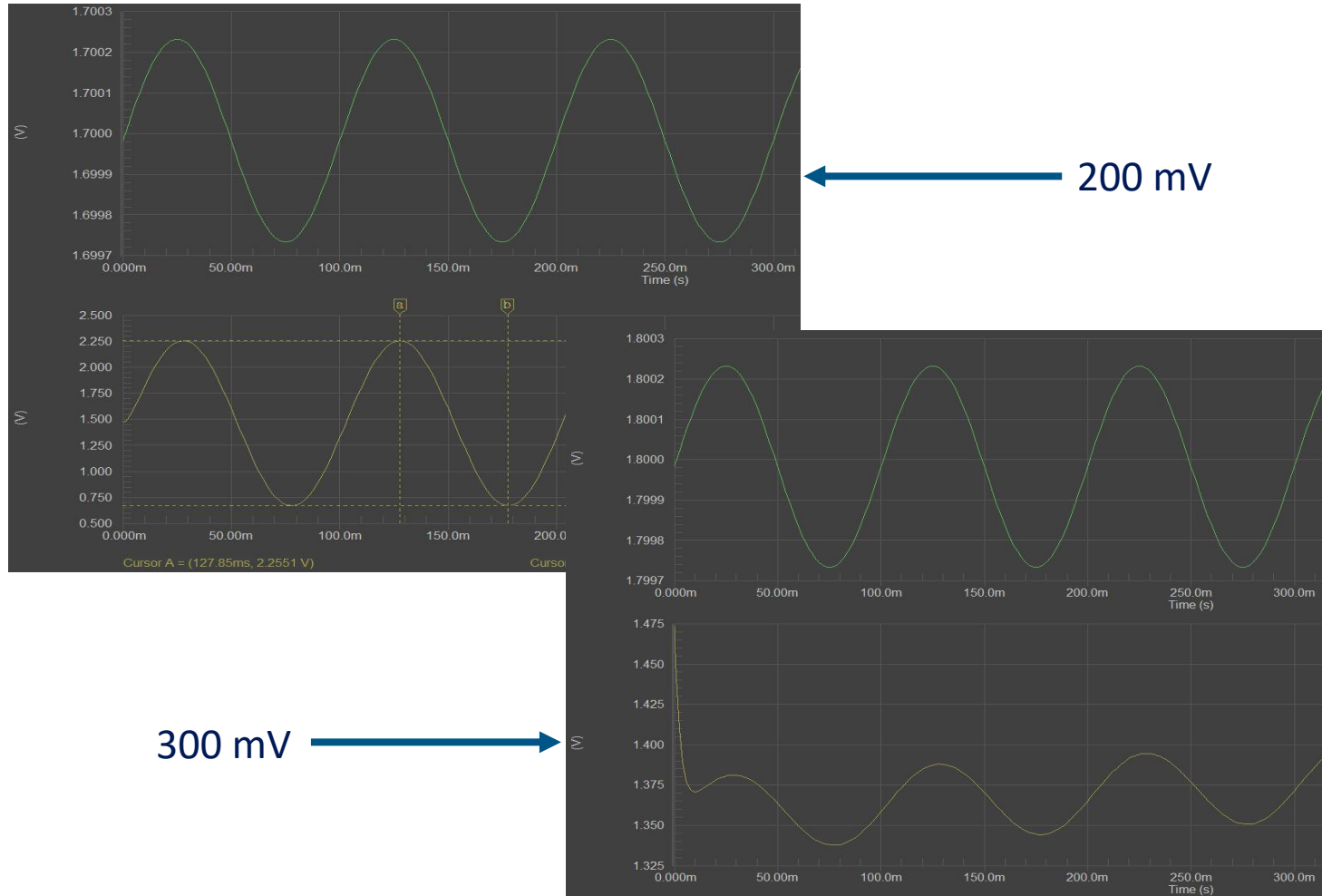
$$A_{cm} = \frac{V_{cm\_out}}{V_{cm\_in}} = \frac{0.092}{1} = 0.092$$

$$\text{CMRR} = 20\log \frac{A_d}{A_{cm}} = 20\log \frac{3860}{0.092} = 92.45\text{dB}$$

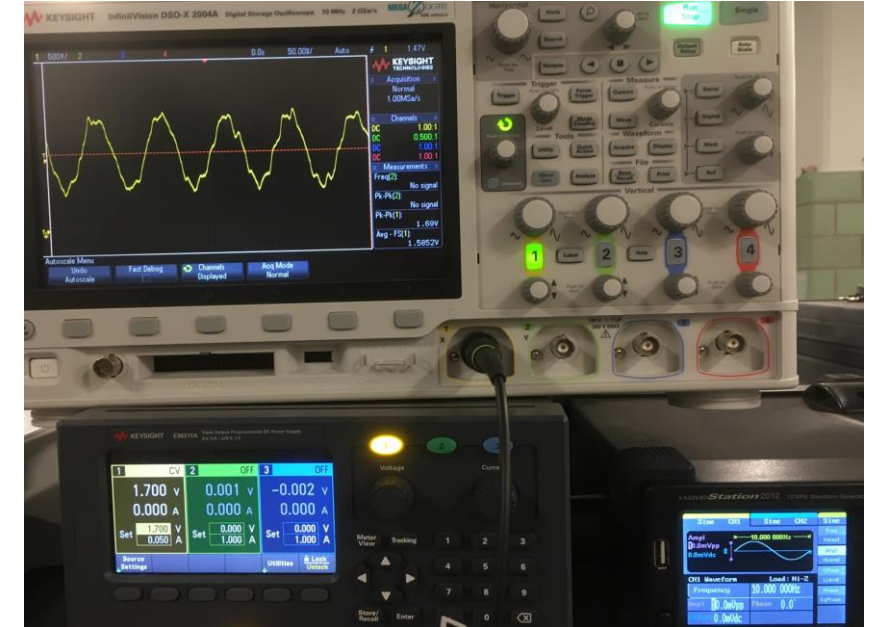
Duke



# Simulation vs Bench Testing – DC Offset Tolerance



Simulation tolerance: +/-200 mV

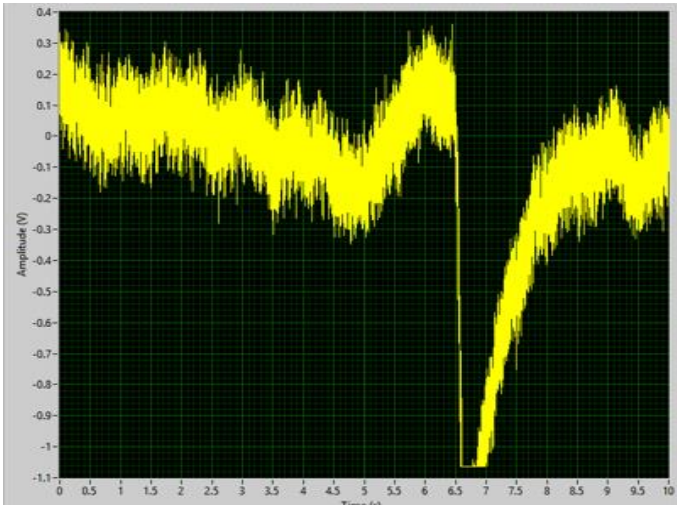


Bench testing tolerance: +/-170 mV

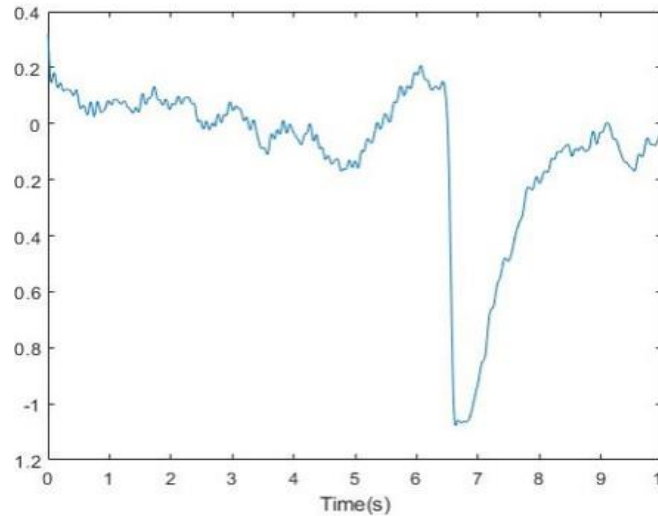
Method: increase the amplitude of DC offset voltage on input signals until the output signal is distorted

Duke

# EEG Testing



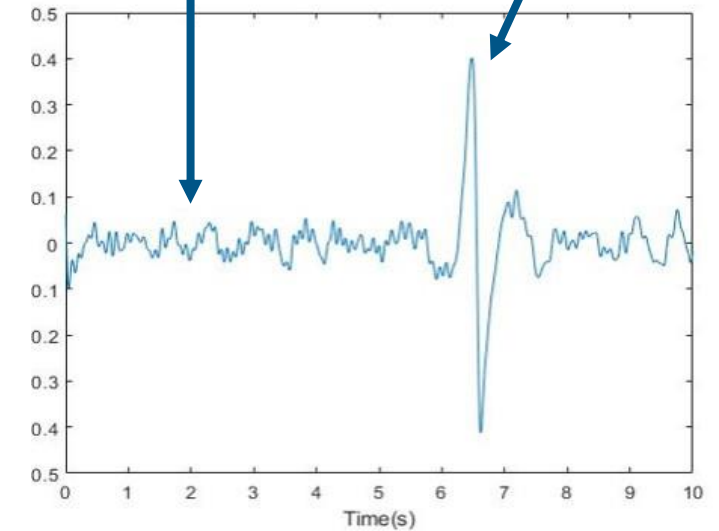
Raw EEG signal obtained from P300 speller BCI2000 system



Low pass filter with cut off frequency 10Hz

higher frequency bands  
beta and gamma

alpha rhythm



Band pass filter within 1 – 10Hz



# Result

Specification	Design Value	Simulation Result	Measured Result
Gain	72.5dB = x4200	72.5dB = x4194	71.73dB = x3860
Noise (input-referred)	3.6 $\mu$ V rms from 0.1 to 50 Hz	Max=0.228 $\mu$ V rms	3.1 $\mu$ V rms
Input voltage range	+/- 250 $\mu$ V	+/- 250 $\mu$ V	+/- 250 $\mu$ V
High pass filter -3 dB	0.106 Hz	0.142 Hz	0.149 Hz
Low pass filter -3 dB	53.05 Hz	52.5 Hz	64.3 Hz
Input offset range	+/- 300 mV	+/- 200 mV	+/- 170 mV
Power consumption	33mW	5.96mW	120mW
CMRR (dB)	> 60 dB	96dB	92.45dB
Input Impedance	> 10 M $\Omega$	10 <sup>9</sup> M $\Omega$	10 <sup>9</sup> M $\Omega$
Leakage Current	< 1 $\mu$ A	0.12 $\mu$ A	0.02 $\mu$ A
Distortion	< 1%	0.04%	

- Low pass filter should have lower cut off frequency
- Input offset range should be enlarged without sacrificing input impedance
- EEG testing for suddenly opening eyes in bright light