

# MRI algorithm outline

U. Chicago MRI Research Center

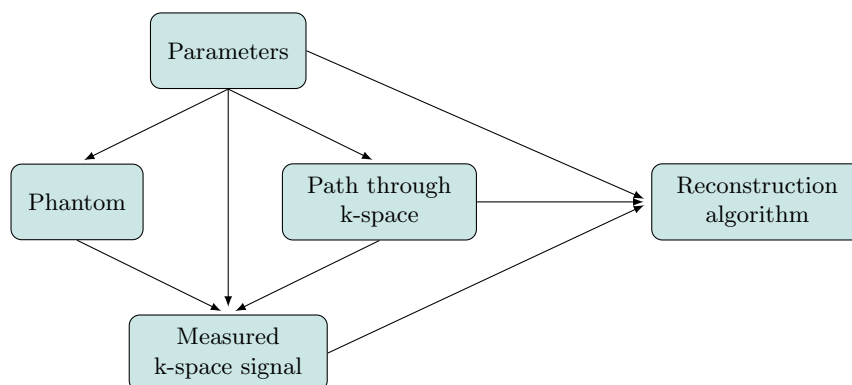
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## 1 Code outline

There are five main pieces of the code, pictured in the following dependency diagram:



### 1.1 Parameters

The parameters describe the settings of the scanner and reconstruction, and are stored in the structures `AcqPars` and `ReconPars`, respectively. `AcqPars` has the following fields:

- The dimensions and resolution of the spatial domain are expressed in three ways (only two of which need to be specified):
  - `AcqPars.nx`, `AcqPars.ny`, `AcqPars.nz` are positive integers specifying the dimensions of the reconstructed images, and of the corresponding Cartesian grid in k-space where we will acquire measurements.
  - `AcqPars.FOV` is a 3-dimensional vector encoding the size of the field of view in the spatial domain, in millimeters.
  - `AcqPars.Resolution` is a 3-dimensional vector encoding the size of each voxel in the reconstruction, in millimeters, which is equal to  $(\text{PhysSize}(1)/\text{nx}) \times (\text{PhysSize}(2)/\text{ny}) \times (\text{PhysSize}(3)/\text{nz})$ .

If any two are specified, we compute the third one; if all three are specified and do not agree, we overwrite `AcqPars.Resolution`.

- `AcqPars.stddev` is a  $n_x \times n_y \times n_z$  array of nonnegative values specifying the standard deviation of the noise at each point in k-space
- `AcqPars.FlipAngle` is the flip angle of the scanner, with value in  $[0, 2\pi]$
- `AcqPars.TR`, `AcqPars.TE` encode timing of the scanner (units = milliseconds). `TR` is the repetition time (milliseconds between each line acquisition) and `TE` is the echo time (milliseconds from center to edge of k-space and back along readout dimension)
- `AcqPars.randomseed` is the seed for the random number generator to produce the noise of the measurements in k-space.
- `AcqPars.acqtimeres` is the time resolution (in milliseconds) of the signal acquisition. When computing the measured k-space signal, we update the phantom at time resolution `acqtimeres` (and take a linear interpolation in between update times).
- The dimensions and resolution of the temporal domain are expressed in three ways (only two of which need to be specified):
  - `AcqPars.nscan`, the total number of passes through k-space
  - `AcqPars.totalscantime`, the duration of the scan (in milliseconds)
  - `AcqPars.onescantime`, the time duration of a single pass through k-space (in milliseconds), which is equal to `totalscantime ÷ nscan`

If any two are specified, we compute the third one; if all three are specified and do not agree, we overwrite `onescantime`. (Note that `onescantime` should, for real data, be a function of `TR`, `TE`, and the dimensions, but in the code is allowed to take an arbitrary value.)

`ReconPars` has the following fields:

- The reconstruction algorithm is based on a linear system, which is solved via preconditioned conjugated gradient descent, using Matlab's `pcg` function. We use two convergence parameters:
  - `ReconPars.convergethresh` is a convergence threshold parameter, e.g.,  $10^{-8}$ .
  - `ReconPars.maxiter` is the maximum number of iterations allowed, e.g., 1000.
- `ReconPars.smoothing` is a smoothing parameter, which takes a small positive value, e.g.,  $10^{-5}$ . It's added to the eigenvalues of the smoothing-over-time matrix in order to ensure this matrix is invertible.
- `ReconPars.weights` is a  $n_x \times n_y \times n_z$  of positive weights. A higher weight corresponds to a voxel where we expect the signal to be more smooth over time.
- The time resolution of the reconstruction is expressed by two parameters:
  - `ReconPars.nimage` is the number of images in the reconstruction
  - `ReconPars.recontimeres` is the time resolution of the reconstruction (in milliseconds), i.e., one image is produced every `recontimeres` milliseconds. It is equal to `scantime ÷ nimage`.

Only one of these needs to be specified. If both are specified and do not agree, then we overwrite `recontimeres`. Note that the problem is underdetermined only when `recontimeres < onescantime` (equivalently, `nimage > nscan`), which is assumed in the implementation.

## 1.2 Phantom

The phantom is not constructed directly, but instead is specified via a function that can return the 3D phantom at any specified time, along with any parameters needed for calling this function.

- **PhantomPars** holds any parameters or objects needed for calling the phantom evaluation function. If no parameters are needed, **PhantomPars** is an empty variable.
- **PhantomEvalFn** is a function handle for evaluating the parameter at a time (between 0 and **totalscantime**). The times are measured in milliseconds, with zero being a reference time at the start of the scan. The function returns a real-valued array of dimension **nx**×**ny**×**nz** containing the signal at each point in the spatial grid, at time **time**.  
The function is called with the command **PhantomEvalFn(PhantomPars,AcqPars,time)**.
  - Workflow: in order to construct a particular phantom, we create a custom function:  
`function PhantomAtTime = MyPhantomFunction(PhantomPars,AcqPars,time)`  
stored in `MyPhantomFunction.m`. Then, we store its handle with the command:  
`PhantomEvalFn=@MyPhantomFunction;`
  - If the function **PhantomEvalFn** requires access to any helper functions, libraries, etc, this can be achieved by adding a path name to the parameter structure. For example, the first line of the **PhantomEvalFn** function definition might be  
`addpath(genpath(PhantomPars.filepathname))`  
where set **PhantomPars.filepathname** is defined as a string giving the necessary path.

## 1.3 Path through k-space

The path through k-space is specified by a **nx**×**ny**×**nz**×**nscan** array. The entries of this array specify the time (in milliseconds, since the start of the scan) when each point in k-space is reached, during each pass through k-space.

## 1.4 Measured signal

The measured signal is a **nx**×**ny**×**nz**×**nscan** complex-valued array called **KspaceSignal**, storing the noisy value measured at each point in k-space, during each pass of the scanner.

- The array **KspaceSignal** is created by the function **GenerateKspaceSignal**, of the format:  
`function KspaceSignal = GenerateKspaceSignal(PhantomEvalFn,PhantomPars,Path,AcqPars).`  
To produce the k-space measurement **KspaceSignal(ix,iy,iz,iscan)**, the function performs the following steps:
  - This value in k-space is measured at time **Path(ix,iy,iz,iscan)**. Since the phantom is updated only once every **AcqPars.acqtimeres** milliseconds, find update times  $t_{\text{pre}}, t_{\text{post}}$  such that  $t_{\text{pre}} \leq \text{Path}(\text{ix}, \text{iy}, \text{iz}, \text{iscan}) \leq t_{\text{post}}$ , i.e., the update times immediately before and after the measurement time. Find the value  $0 \leq c \leq 1$  so that  $\text{Path}(\text{ix}, \text{iy}, \text{iz}, \text{iscan}) = c \cdot t_{\text{pre}} + (1 - c) \cdot t_{\text{post}}$ .
  - Let **kspace\_pre** be the Fourier transform of the phantom evaluated at time  $t_{\text{pre}}$ , and **kspace\_post** at time  $t_{\text{post}}$ . Then, using a linear interpolation, the measured signal is:  
 $c \cdot \text{kspace\_pre}(\text{ix}, \text{iy}, \text{iz}) + (1 - c) \cdot \text{kspace\_post}(\text{ix}, \text{iy}, \text{iz}) + \text{noise}$ ,  
where the noise is a complex Gaussian with standard deviation **AcqPars.stddev(ix,iy,iz)**.

## 1.5 Reconstruction algorithm

The reconstructed signal is a **nx**×**ny**×**nz**×**ntime** complex-valued array called **EstSignal**, where the number of time points is **ntime = nscan·nhighres**.

- The array `EstSignal` is computed with the function `ReconAlg`, of the format:  
`function EstSignal = ReconAlg(KspaceSignal,Path,AcqPars,ReconPars).`

The reconstruction algorithm is described below.

## 2 Reconstruction algorithm

Next we give the details of the reconstruction algorithm implemented in the function `ReconAlg`. A glossary for translating between the algorithm and the code outline:

$n = \mathbf{nx} \cdot \mathbf{ny} \cdot \mathbf{nz}$ , the total number of voxels in the discretized grid  
 $T$  = the number of timepoints in the reconstructed image, `nimage`  
 $X$  = the phantom produced by `PhantomEvalFn`  
 $Y$  = the measured k-space signal `KspaceSignal`  
 $\hat{X}$  = the estimated signal `EstSignal` computed by the function `ReconAlg`  
 $W = \text{diag}(w_1, \dots, w_n)$  where  $w_1, \dots, w_n$  are specified by `weights`  
 $\lambda$  = the smoothing parameter `smoothing`  
 $\Omega$  = specifies which points in k-space are observed at which time, as determined by `Path`

### 2.1 Measurement model

Let  $n = n_x \cdot n_y \cdot n_z$ . At each time  $t = 1, \dots, T$ , the signal is given by  $X_t \in \mathbb{C}^n$ , which contains the true  $n_x \times n_y \times n_z$  discretized signal reshaped into a vector. We will write  $X \in \mathbb{C}^{n \times T}$  to be the matrix with  $t$ -th column  $X_t$ .

Let  $\Omega_t \subset \{1, \dots, n\}$  index the points in k-space where we take measurements at time  $t$ , and let

$$\Omega = \cup_{t=1}^T (\Omega_t \times \{t\}) \subset \{1, \dots, n\} \times \{1, \dots, T\}$$

index the observed points in k-space at their observed times. While the number of timepoints  $T$  is higher than the total number of scans, it is still an approximation to the continuous-time measurements taken by the scanner. To assign each measurement in k-space to a time  $t = 1, \dots, T$ , we simply divide the total scan time into  $T$  time bins of equal length, and then all measurements in k-space acquired during time bin  $t$  are assigned to  $\Omega_t$ .

Next, let  $Y \in \mathbb{C}^{n \times T}$  be a matrix containing our measured entries, with zeros elsewhere. Specifically, in the  $t$ -th column, we have

$$(Y_t)_{\Omega_t} = [\mathcal{F}X_t]_{\Omega_t} + \text{noise}, \quad (Y_t)_{(\Omega_t)^c} = 0,$$

where  $\mathcal{F}$  is the 3D discrete Fourier transform (rearranged into a  $n \times n$  matrix, so that it acts on vectorized 3D signals, i.e.,  $\mathcal{F}$  is a map from  $\mathbb{C}^n$  to  $\mathbb{C}^n$ ). The entries of the noise are independent complex normals with variance corresponding to the location in k-space (variance is highest near the center of k-space).

### 2.2 Smoothed optimization

We will solve a smoothed optimization problem:

$$\min \{ \langle W, XDX^* \rangle : (\mathcal{F}X)_{\Omega} = Y_{\Omega} \}, \quad (1)$$

where  $D \in \mathbb{C}^{T \times T}$  and  $W \in \mathbb{C}^{d \times d}$  are positive definite matrices chosen such that  $D$  induces smoothness over time while  $W$  controls the penalty over the spatial domain.

For the matrix  $W$ , we will use a diagonal matrix  $W = \text{diag}(w_1, \dots, w_n)$ , where  $w_i > 0$  is the smoothness penalty acting on voxel  $i$  (larger  $w_i$  corresponds to enforcing more smoothness on that voxel's trajectory over time).

For the matrix  $D$ , we will use

$$D = \begin{pmatrix} 1 & -2 & 1 & 0 & \dots & 0 & 0 & 0 \\ -2 & 5 & -4 & 1 & \dots & 0 & 0 & 0 \\ 1 & -4 & 6 & -4 & \dots & 0 & 0 & 0 \\ 0 & 1 & -4 & 6 & \dots & 0 & 0 & 0 \\ \vdots & \vdots & \vdots & \vdots & \ddots & \vdots & \vdots & \vdots \\ 0 & 0 & 0 & 0 & \dots & 6 & -4 & 1 \\ 0 & 0 & 0 & 0 & \dots & -4 & 5 & -2 \\ 0 & 0 & 0 & 0 & \dots & 1 & -2 & 1 \end{pmatrix} + \lambda \mathbf{I}_T.$$

The first term penalizes the squared magnitude of the discretized second derivative, while  $\lambda \mathbf{I}_T$  ensures that  $D$  is invertible (here  $\mathbf{I}_T$  is the  $T \times T$  identity matrix, while  $\lambda > 0$  is some small smoothing parameter).

We can see that (1) is a simple optimization problem, minimizing a convex quadratic objective subject to some linear constraints.

### 2.2.1 Solving for the minimizer

With some rearranging, we can find a closed-form solution to (1). First we rearrange into vector form, and equivalently rewrite the optimization problem (1) as:

$$\min \{ \text{vec}(X)^* (\bar{D} \otimes W) \text{vec}(X) : [(\mathbf{I}_T \otimes \mathcal{F}) \cdot \text{vec}(X)]_\Omega = [\text{vec}(Y)]_\Omega \}, \quad (2)$$

where, abusing notation, we are now treating  $\Omega$  as a subset of indices  $\{1, \dots, nT\}$  (i.e., the indices after vectorizing our  $n \times T$  matrices). The solution is then given by

$$\text{vec}(\hat{X}) = [\bar{D}^{-1} \otimes (W^{-1} \mathcal{F}^*)]_{*,\Omega} \cdot \left( [\bar{D}^{-1} \otimes (\mathcal{F} W^{-1} \mathcal{F}^*)]_{\Omega,\Omega} \right)^{-1} \cdot [\text{vec}(Y)]_\Omega. \quad (3)$$

In terms of computation cost, the main step is solving the  $|\Omega| \times |\Omega|$  linear system. Note that, in the notation of our code outline,  $|\Omega|$  is given by

$$|\Omega| = \text{nx} \cdot \text{ny} \cdot \text{nz} \cdot \text{nscan},$$

i.e., it's the total number of measurements acquired.

Now we verify that (3) solves the optimization problem (2). First we check feasibility:

$$\begin{aligned} [(\mathbf{I}_T \otimes \mathcal{F}) \cdot \text{vec}(\hat{X})]_\Omega &= [\bar{D}^{-1} \otimes (\mathcal{F} W^{-1} \mathcal{F}^*)]_{*,\Omega} \cdot \left( [\bar{D}^{-1} \otimes (\mathcal{F} W^{-1} \mathcal{F}^*)]_{\Omega,\Omega} \right)^{-1} \cdot [\text{vec}(Y)]_\Omega \\ &= [\bar{D}^{-1} \otimes (\mathcal{F} W^{-1} \mathcal{F}^*)]_{\Omega,\Omega} \cdot \left( [\bar{D}^{-1} \otimes (\mathcal{F} W^{-1} \mathcal{F}^*)]_{\Omega,\Omega} \right)^{-1} \cdot [\text{vec}(Y)]_\Omega \\ &= [\text{vec}(Y)]_\Omega. \end{aligned}$$

Next we check first-order optimality conditions—we need to see that  $(\bar{D} \otimes W) \text{vec}(\hat{X})$  (the gradient of the objective function) lies in the span of  $[\mathbf{I}_T \otimes \mathcal{F}^*]_{*,\Omega}$  (the gradient of the constraints):

$$\begin{aligned} (\bar{D} \otimes W) \text{vec}(\hat{X}) &= (\bar{D} \otimes W) \cdot [\bar{D}^{-1} \otimes (W^{-1} \mathcal{F}^*)]_{*,\Omega} \cdot \left( [\bar{D}^{-1} \otimes (\mathcal{F} W^{-1} \mathcal{F}^*)]_{\Omega,\Omega} \right)^{-1} \cdot [\text{vec}(Y)]_\Omega \\ &= [(\bar{D} \otimes W) \cdot (\bar{D}^{-1} \otimes (W^{-1} \mathcal{F}^*))]_{*,\Omega} \cdot \left( [\bar{D}^{-1} \otimes (\mathcal{F} W^{-1} \mathcal{F}^*)]_{\Omega,\Omega} \right)^{-1} \cdot [\text{vec}(Y)]_\Omega \\ &= [\mathbf{I}_T \otimes \mathcal{F}^*]_{*,\Omega} \cdot \left( [\bar{D}^{-1} \otimes (\mathcal{F} W^{-1} \mathcal{F}^*)]_{\Omega,\Omega} \right)^{-1} \cdot [\text{vec}(Y)]_\Omega, \end{aligned}$$

as desired. This proves that (3) is optimal. (Since  $D$  and  $W$  are positive definite, the solution is also unique.)

### 2.2.2 Special case: constant weights

If  $W = \text{diag}(w_1, \dots, w_n)$  where the weights  $w_1 = \dots = w_n$  are constant across the  $n$  voxels of the image, this is a special case that can be solved much more efficiently. The solution is given by

$$\hat{X} = \mathcal{F}^* \tilde{Y},$$

where  $\tilde{Y}$  is the smoothed signal in k-space. Specifically, for each voxel  $i = 1, \dots, n$ , let  $\Omega_{(i)} \subset \{1, \dots, T\}$  be the time points when voxel  $i$  is measured, and let  $Y_{(i)}$  and  $\tilde{Y}_{(i)}$  denote the  $i$ -th row of the matrix  $Y$ , expressed as column vector (i.e., the measurements at voxel  $i$ , and zeros at the unmeasured time points). We define the smoothed k-space signal with rows  $\tilde{Y}_{(i)}$ ,

$$\tilde{Y}_{(i)} = [\overline{D}^{-1}]_{*, \Omega_{(i)}} \cdot \left( [\overline{D}^{-1}]_{\Omega_{(i)}, \Omega_{(i)}} \right)^{-1} \cdot [Y_{(i)}]_{\Omega_{(i)}}. \quad (4)$$

Note that

$$[\tilde{Y}_{(i)}]_{\Omega_{(i)}} = [\overline{D}^{-1}]_{\Omega_{(i)}, \Omega_{(i)}} \cdot \left( [\overline{D}^{-1}]_{\Omega_{(i)}, \Omega_{(i)}} \right)^{-1} \cdot [Y_{(i)}]_{\Omega_{(i)}} = [Y_{(i)}]_{\Omega_{(i)}},$$

that is, the measured values at the observed voxels stay the same.

Now we verify that  $\hat{X}$  is the right solution. Referring back to equation (3) for the general case, note that in this special case we have  $W^{-1} = w_1^{-1} \mathbf{I}_n$ , and so  $\mathcal{F}W^{-1}\mathcal{F}^* = w_1^{-1}\mathcal{F}\mathcal{F}^* = w_1^{-1}\mathbf{I}_n$ . Therefore, the solution is given by

$$\text{vec}(\hat{X}) = [\overline{D}^{-1} \otimes w_1^{-1}\mathcal{F}^*]_{*, \Omega} \cdot \left( [\overline{D}^{-1} \otimes w_1^{-1}\mathbf{I}_n]_{\Omega, \Omega} \right)^{-1} \cdot [\text{vec}(Y)]_{\Omega}.$$

This can be rearranged to

$$\hat{X} = \mathcal{F}^* \tilde{Y} \text{ where } \text{vec}(\tilde{Y}) = [\overline{D}^{-1} \otimes \mathbf{I}_n]_{*, \Omega} \cdot \left( [\overline{D}^{-1} \otimes \mathbf{I}_n]_{\Omega, \Omega} \right)^{-1} \cdot [\text{vec}(Y)]_{\Omega},$$

and we can verify that this definition of  $\tilde{Y}$  is equivalent to the solution given above in (4).