

## **NUFFT and Compressed Sensing**

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Friedrich-Alexander-Universität Erlangen-Nürnberg March 27, 2023





### **Outline**

Non-Uniform FFT (NUFFT)

Compressed Sensing (CS)

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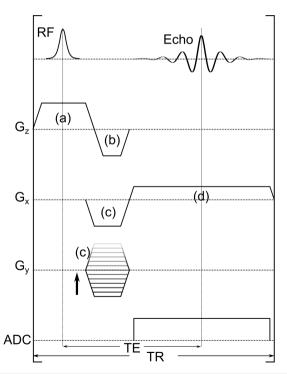


# 1 Non-Uniform FFT (NUFFT)



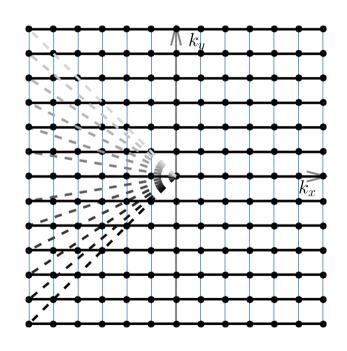


## Introduction: Cartesian Sampling (e.g. FLASH) <sup>1</sup>



#### **Gradients:**

- (a) Slice selection
- (b) Rewinder
- (c) Prephasing
- (d) Readout



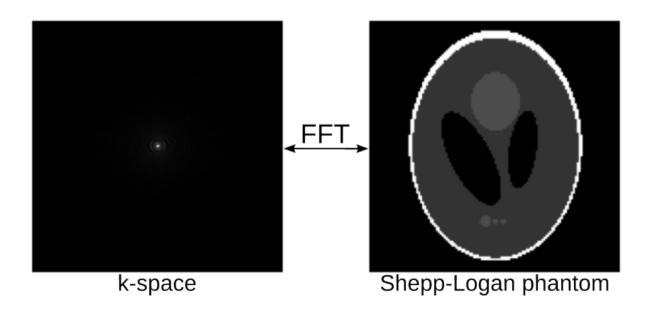
<sup>&</sup>lt;sup>1</sup>Haase A, Frahm J, Matthaei D, Hanicke W, Merboldt KD. FLASH imaging. Rapid NMR imaging using low flip-angle pulses. *J Magn Reson* (1986).

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### **Introduction: Fast Fourier Transform**

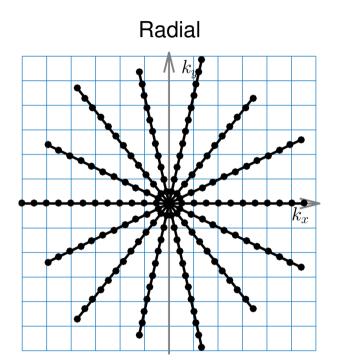
$$s(k_x, k_y) = \int \rho(x, y) \cdot e^{-i(k_x \cdot x + k_y \cdot y)} dx dy$$
 (1)

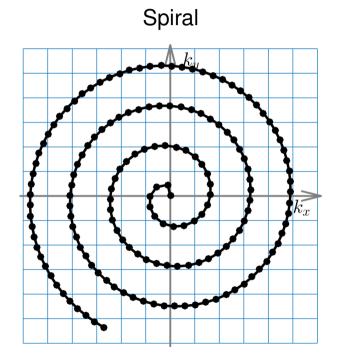


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## Non-Cartesian Sampling (e.g. Radial <sup>2</sup> and Spiral <sup>3</sup>)





<sup>&</sup>lt;sup>2</sup>Lauterbur PC. Image formation by induced local interactions: Examples employing nuclear magnetic resonance. *Nature* (1973).

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<sup>&</sup>lt;sup>3</sup>Nishimura DG, Irarrazabal P, Meyer C. A velocity k-space analysis of flow effects in echo-planar and spiral imaging. *Magn Reson Med* (1995).



### Image Reconstruction of Non-Cartesian Data Requires NUFFT

NUFFT: Non-Uniform FFT 4, 5, 6

- 1. Density compensation
- 2. Gridding: Convolution with the Kaiser-Bessel window
- 3. Deapodization & Inverse FFT

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<sup>&</sup>lt;sup>4</sup>OSulllivan J. A fast sinc function gridding algorithm for Fourier inversion in computed tomography. *IEEE Trans Med Imaging* (1985).

<sup>&</sup>lt;sup>5</sup>Jackson J, Meyer CH, Nishimura DG, Macovski A. Selection of a convolution function for Fourier inversion using gridding. *IEEE Trans Med Imaging* (1991).

<sup>&</sup>lt;sup>6</sup>Fessler JA, Sutton BP. Nonuniform fast Fourier transforms using min-max interpolation. *IEEE Trans Med Imaging* (2003).



### **NUFFT Step 1: Density Compensation**

- $\triangleright$  Non-Cartesian samples are usually not uniformly acquired in k-space.
- ightharpoonup e.g. In radial sampling, the central k-space points are more densely acquired than peripheral k-space points.
- Analytical density compensation function (DCF) in radial sampling.

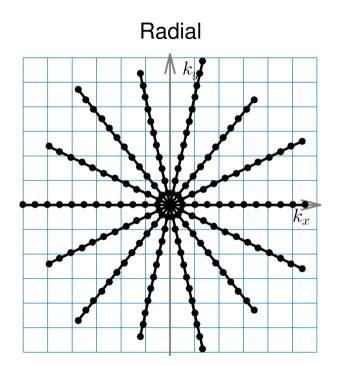
Given 
$$ktrj = k_x + 1i * k_y$$
,

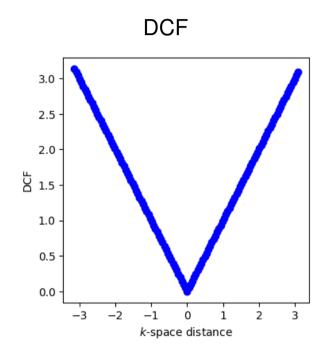
$$DCF = \sqrt{k_x^2 + k_y^2} \tag{2}$$

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### **DCF in Radial Sampling**

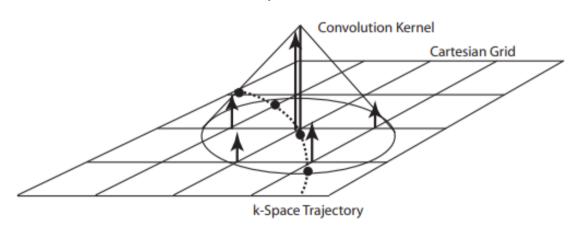






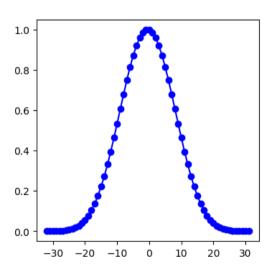
### NUFFT Step 2: Gridding (Interpolation) with the Kaiser-Bessel Window

#### Interpolation <sup>a</sup>



ahttps://users.fmrib.ox.ac.uk/~karla/reading\_group/lecture\_notes/AdvRecon\_Pauly\_ read.pdf

#### Kaiser-Bessel Window



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### **NUFFT Step 3: Deapodization**

► The gridded signal on Cartesian grids can be written as the convolution between the non-Cartesian signal and the Kaiser-Bessel window,

$$s_{\text{Cart}} = s_{\text{non-Cart}} \circledast W_{\text{kb}}$$
 (3)

with FFT, it becomes

$$\mathcal{F}\{s_{\text{Cart}}\} = \mathcal{F}\{s_{\text{non-Cart}}\} \cdot \mathcal{F}\{W_{\text{kb}}\}$$
(4)

► Then deapodization is

$$I = \mathcal{F}\{s_{\text{Cart}}\}./\mathcal{F}\{W_{\text{kb}}\}\tag{5}$$

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### **NUFFT Recap**

- ► Any questions with regard to NUFFT?
- ► Any question with regard to NUFFT exercises?

▶ What if the density compensation function is unknown?

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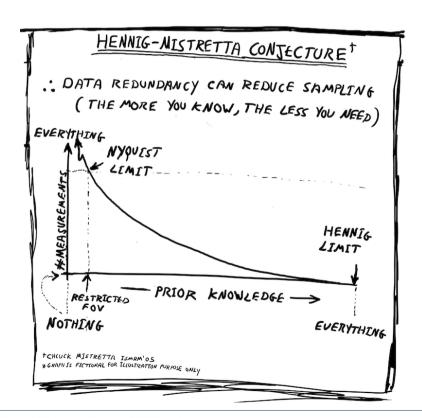


## 2 Compressed Sensing (CS)





### **Compressed Sensing**



- Candes EJ, Romberg JK, Tao T. Stable signal recovery from incomplete and inaccurate measurements. Commun Pure Appl Math (2006).
- ► Lustig M, Dohono D, Pauly JM. Sparse MRI: The application of compressed sensing for rapid MR imaging. *Magn Reson Med* (2007).
- ▶ Block KT, Uecker M, Frahm J. Undersampled radial MRI with multiple coils. Iterative image reconstruction using a total variation constraint. *Magn Reson Med* (2007).
- ► Comics from http://people.eecs.berkeley. edu/~mlustig/comics1.html

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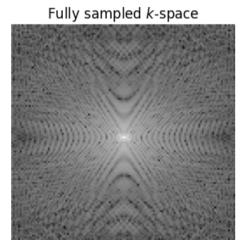


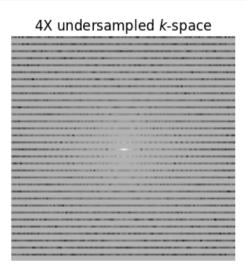
### What is Nyquist Limit?

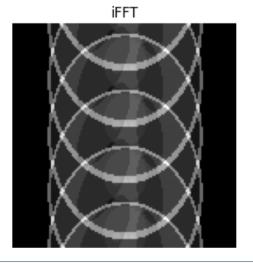
#### **Nyquist Sampling Requirement**

Given an imaging field-of-view (FOV), the sampling in k-space must satisfy

$$\Delta k \le 1/\text{FOV}$$
 (6)



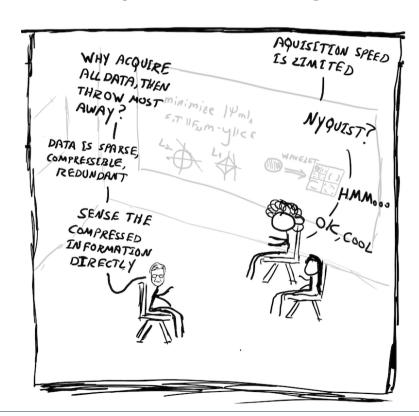




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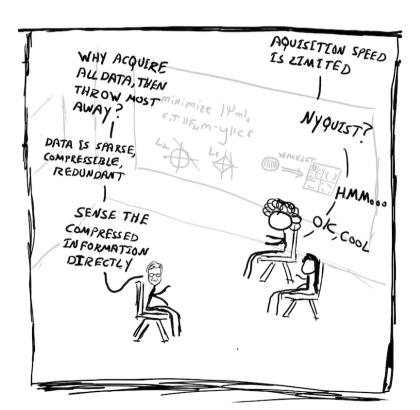
### **How Compressed Sensing Goes Beyond Nyquist?**

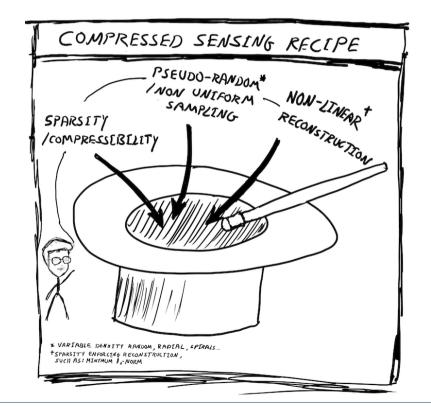


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### **How Compressed Sensing Goes Beyond Nyquist?**

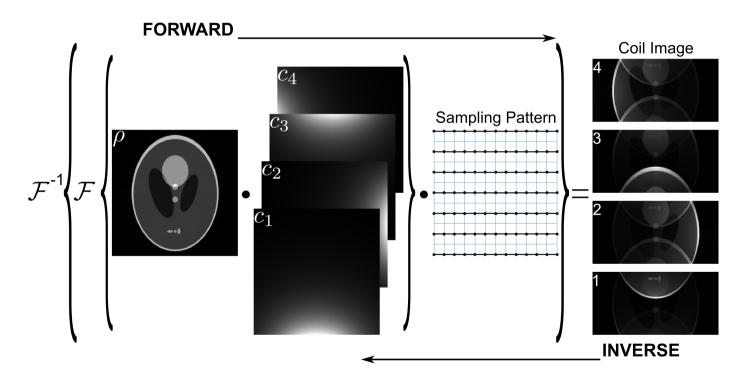




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### Before Compressed Sensing: Parallel Imaging as SENSE 7



<sup>&</sup>lt;sup>7</sup>Pruessmann KP, Weiger M, Scheidegger MB, Boesiger P. SENSE: sensitivity encoding for fast MRI. *Magn Reson Med* (1999).

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### Parallel Imaging as SENSE: Solving a Linear Inverse Problem

Objective function:

$$\operatorname{argmin}_{x} \|y - \mathcal{PFS}x\|_{2}^{2} \tag{7}$$

- ► Solver: gradient descent, or conjugate gradient, or ADAM, ...
- ▶ Data update via gradient method, e.g. FISTA 8:

$$x^{(t+1)} = x^{(t)} + \alpha \cdot \mathcal{S}^H \mathcal{F}^{-1} \mathcal{P}^H (y - \mathcal{P} \mathcal{F} \mathcal{S} x^{(t)})$$

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<sup>&</sup>lt;sup>8</sup>Beck A, Teboulle M. A fast iterative shrinkage-thresholding algorithm for linear inverse problems. SIAM J Imaging Sciences (2009).



#### What is Linear Inverse Problem and What is Gradient?

Objective function:

$$\operatorname{argmin}_{x} \|2 - x\|_{2}^{2}$$
 (8)

Given initial guess  $x_{\text{prev}} = 0$  and learning rate  $\alpha = 0.1$ ,

Iteration	$x_{ m prev}$	grad = 2 * (2 - x)	$x_{\text{curr}} = x_{\text{prev}} + \alpha * \text{grad}$
0	0	4	0.4
1	0.4	3.2	0.72
:	:	:	:
47	1.9999	0.0001	2

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#### What is Linear Inverse Problem and What is Gradient?

```
x_prev = 0

for n in range(50):

    g = 2 * (2 - x_prev)

    x_curr = x_prev + 0.1 * g

    print(' iter %2d x_prev %6.4f grad %6.4f x_curr %6.4f'%(n, x_prev, g, x_curr))

    x_prev = x_curr
```

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### Inverse Problems can Become Under-determined / III-posed

Objective function:

$$\operatorname{argmin}_{x_1, x_2} \|2 - x_1 - x_2\|_2^2 \tag{9}$$

➤ You can't find an unique solution for this function.

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- ..., however, when there is prior knowledge, e.g.

s.t. 
$$x_1 = x_2$$
 (10)

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s.t. 
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 $\blacktriangleright$  We can easily solve it,  $x_1 = x_2 = 1$ .

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### We can write this toy example in a matrix format

Objective function:

$$\operatorname{argmin}_{x_1, x_2} \|2 - x_1 - x_2\|_2^2 \tag{11}$$

It is equivalent to

$$\operatorname{argmin}_{\mathbf{x}} \|\mathbf{y} - \mathbf{A}\mathbf{x}\|_{2}^{2} \tag{12}$$

where 
$$\mathbf{x} = \begin{pmatrix} x_1 \\ x_1 \end{pmatrix}$$
,  $\mathbf{y} = \begin{pmatrix} 2 \\ 2 \end{pmatrix}$  and  $\mathbf{A} = \begin{pmatrix} 1 & -1 \\ 1 & -1 \end{pmatrix}$ 

Does it look similar to the inverse problem in MRI?

$$\operatorname{argmin}_{x} \|y - \mathcal{PFS}x\|_{2}^{2} \tag{13}$$

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### **Prior is the Game Changer in Compressed Sensing**

▶ Prof. Dr. Gary Golver from Stanford: "We eventually only need to measure one point in k-space!!!"

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### **Prior is the Game Changer in Compressed Sensing**

- ▶ Prof. Dr. Gary Golver from Stanford: "We eventually only need to measure one point in k-space!!!"
- ► People like me: "What is going on here??? Is there anyone who would like to share their codes???"

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- ► People like me: "What is going on here??? Is there anyone who would like to share their codes???"
- Prof. Dr. Mike Lustig from Berkeley: "Sparsifying transformation changes the game!!!"

$$\operatorname{argmin}_{x} \|y - \mathcal{PFS}x\|_{2}^{2} + \lambda \|\Phi x\|_{1}$$
 (14)

where  $\Phi$  is wavelet transform, total variation, ...

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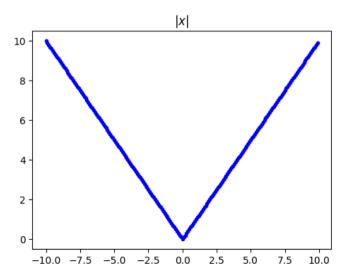


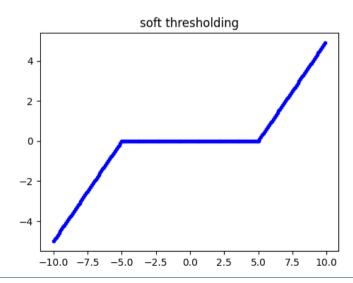
#### **How to Solve this Problem?**

#### Objective function:

$$\operatorname{argmin}_{x} \|y - \mathcal{PFS}x\|_{2}^{2} + \lambda \|\Phi x\|_{1}$$
 (15)

- ▶ the regularization term  $\lambda \| \Phi x \|_1$  is not differentiable; ▶ soft thresholding  $\mathcal{T}_{\lambda}(x) = (x \lambda)_{+} \mathrm{sign}(x)$





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### **Compressed Sensing: Iterative Soft Thresholding**

1. Gradient update:

$$\dot{x}^{(t+1)} = x^{(t)} + \alpha \cdot \mathcal{S}^H \mathcal{F}^{-1} \mathcal{P}^H (y - \mathcal{P} \mathcal{F} \mathcal{S} x^{(t)})$$

2. Soft thresholding:

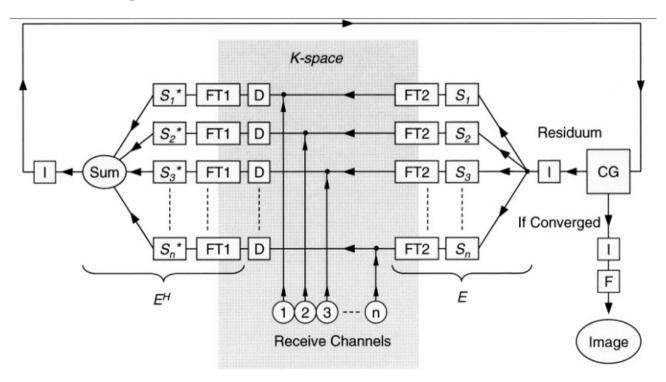
$$x^{(t+1)} = \Phi^{-1} \mathcal{T}_{\lambda}(\Phi x^{(t+1)})$$

- $\blacktriangleright$  This suffices when  $\Phi$  is wavelet transform.
- ▶ When you use total variation, you may need a more general solver such as ADAM.

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## What is Gradient Update in Parallel MRI? 9



<sup>&</sup>lt;sup>9</sup>Pruessmann KP, Weiger M, Börnert P, Boesiger P. Advances in sensitivity encoding with arbitrary *k*-space trajectories. *Magn Reson Med* (2001).

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- ▶ density correction *D*:
  - $D=1/d\mathbf{k}$ ,  $\mathbf{k}$  is the relative density of the k-space sampling pattern at the position  $\vec{k}$ .
- ▶ this changes the system equation:

$$(E^H DE)\mathbf{v} = E^H D\mathbf{m}$$

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- Exercise 1: run the gradient step many times without soft thresholding, are you able to get a similar reconstruction as the NUFFT reconstruction with density compensation?

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- ▶ this speeds up the iterative procedure in practice. However, mathematicians don't like it ...
- ► Exercise 1: run the gradient step many times without soft thresholding, are you able to get a similar reconstruction as the NUFFT reconstruction with density compensation?
- ► Exercise 2: try to tune the soft thresholding parameter, and show how it affects the reconstruction

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#### It is not the end ...

► Prof. Dr. Florian Knoll <sup>10</sup>: "Instead of hand-crafted sparsifying transform, neural network learns it!!!"

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<sup>&</sup>lt;sup>10</sup>Hammernik K, Klatzer T, Kobler E, Recht MP, Sodickson DK, Pock T, Knoll F. Learning a variational network for reconstruction of accelerated MRI data. *Magn Reson Med* (2018).