

# Polyp Classification and Clustering from Endoscopic Images Using Competitive and Convolutional Neural Networks

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**Abstract:** Understanding the type of Polyp present in the body plays an important role in medical diagnosis. This paper proposes an approach to classify and cluster the polyp present in an Endoscopic scene into malignant or benign class. CNN and Self Organizing Maps are used to classify and cluster from white light and Narrow Band (NBI) Endoscopic Images. Using Competitive Neural Network different polyps available from previous data are plotted with the new polyp according to their structural similarity. Such kind of presentation not only help the doctor in its easy understanding but also helps him to know what kind of medical procedures were followed in similar cases.

## 1 INTRODUCTION

According to the WHO, Cancer is the second leading cause of death globally, and is responsible for an estimated 9.6 million deaths in 2018. Globally, about 1 in 6 deaths is due to cancer. This report verifies that Late-stage presentation and inaccessible diagnosis and treatment are common reasons for these deaths. In 2017, only 26 percent of low-income countries reported having pathology services generally available in the public sector. More than 90 percent of high-income countries reported treatment services are available compared to less than 30 percent of low-income countries.

This provides a vast area of research so that diagnosis can be made easy and accessible. Many methods have been developed to know the existence of a polyp in an Endoscopic scene but the automatic classification of these into different classes is still complex (Y.Iwahori and K.Kasugai, 2013). This paper proposes a method to know whether the polyp detected in a patients body is benign or malignant because the first step after being diagnosed with a tumor is to find it's class. In short, the meaning of malignant is cancerous and the meaning of benign is non-cancerous that is why it is very important to have a proper verification and to decide the further treatment path. A timely understanding of the tumor can pre-

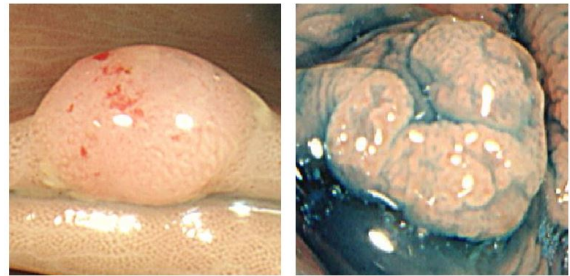


Figure 1: (i)White light Benign (ii)StainNBI Benign.

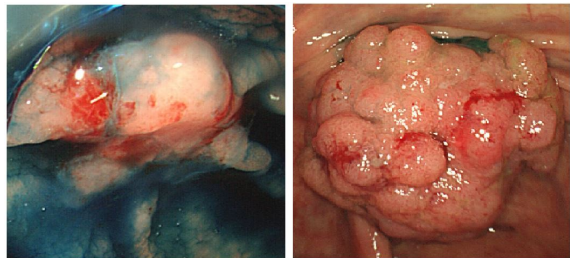


Figure 2: Malignant (i)StainNBI (ii)White Light.

vent deaths.

## 2 LITERATURE SURVEY

Present methods of image clustering mostly involve use of K-means algorithm and X-means algorithm (Coleman and Andrews, 1979). Using Self Organizing Maps with zero radius can provide similar results but with increased radius we can perform space approximation which will provide us with the minimum number of points that cover as much data as possible. The main issue with previous methods is that clusters do not know about the existence of other clusters therefore they tend to behave independently. Using SOM, we can enable more cooperative behaviour among these clusters. Due to this cooperation the cluster centres are more efficiently distributed. Even if some data points are removed, our model will give a good understanding about the shape of our original data. As the feature map spreads out over space, this method can generate smaller dataset which will keep the useful properties of the original dataset. (Zhao and Ma, 2014)

We used both CNN and Competitive Neural Networks to develop a self organizing map of the polyp data-set. This map consists of polyps from many previous cases along with the tumor of present patient. These polyps are positioned on the 2-D map according to their level of similarity. Such representation enables us to carefully examine the polyp and compare it with the other data. The lesser it's distance is from the other polyp, more are it's chances of similarity. This representation not only enables us to find it's class efficiently but can also be further modified to predict possible treatment procedures based on the previous cases in which the decisions were taken by actual doctors.

## 3 DATA-SET

The Data-set used for the experimentation purposes is 'Polyp-CVC-CliniDB (Bernal, 2015). CVC-

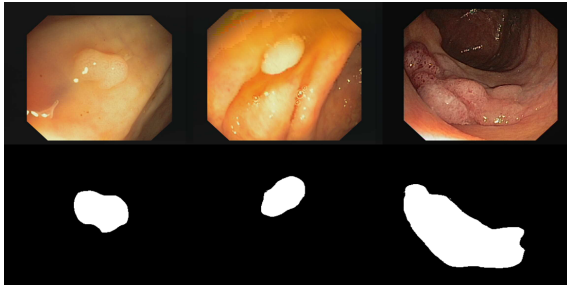


Figure 3: Content of CVC-ClinicDB database.

ClinicDB is a database of frames extracted from

colonoscopy videos. These frames contain several examples of polyps. In addition to the frames, it consists of the ground truth for the polyps. This ground truth consists of a mask corresponding to the region covered by the polyp in the image. CVC-ClinicDB database consists of two different types of images: Original images and Polyp mask. CVC-ClinicDB is the official database used in the training stages of MICCAI 2015 Sub-Challenge on Automatic Polyp Detection Challenge in Colonoscopy Videos

Sequence	1	2	3	4	5	6	7	8
Frames	1-25	26-50	51-67	68-78	79-103	104-126	127-151	152-177
Sequence	9	10	11	12	13	14	15	16
Frames	178-199	200-205	206-227	228-252	253-277	278-297	298-317	318-342
Sequence	17	18	19	20	21	22	23	24
Frames	343-363	364-383	384-408	409-428	429-447	448-466	467-478	479-503
Sequence	25	26	27	28	29			
Frames	504-528	529-546	547-571	572-591	592-612			

Figure 4: Correspondence between number of frames and video sequences in CVC-ClinicDB.

## 4 PROPOSED METHODS

This paper proposes two methods to classify and cluster the Endoscopic polyp images. One method is using self organizing map. This method uses principles of competitive learning. Competitive learning is a form of learning in artificial neural network in which nodes compete for the right to respond to a subset of the input data. Competitive learning works by increasing the specialization of each node in the network. In contrast to other standard Neural networks, it only has input and output layers. There are no hidden layers in between, instead there is a SOM layer. Training is done by competitive learning where the weights associated with output layer nodes compete for activation. Therefore we can understand a high dimensional data in less dimensions and these observations can be classified into clusters. The second method involves use of CNN. A new CNN model was generated to classify Stain Narrow Band Endoscopic images into Benign and Malignant classes. Images are pre-processed using combination of Bilateral and Guided filter which are then used as inputs to the network.

### 4.1 Convolutional Neural Network

A Convolutional Neural Network (CNN) is comprised of one or more convolutional layers (often with a subsampling step) and then followed by one or more fully connected layers as in a standard multilayer neural network. The architecture of a CNN is designed

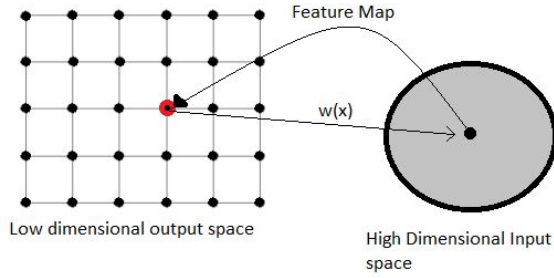


Figure 5: Working of SOM.

to take advantage of the 2D structure of an input image. This is achieved with local connections and tied weights followed by some form of pooling which results in translation invariant features.(A. Krizhevsky and Hinton, 2012)

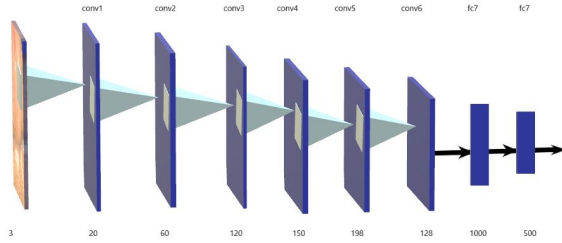


Figure 6: Designed Neural Network structure.

A self designed and trained layer structure as shown in figure 4 was used to classify Benign and Malignant polyps. Input images were processed using smoothing filters and edges were detected. This network was trained using 500 images of both kinds. K-fold cross validation (Burman, 1989) was used on this set. k-fold cross validation is a procedure used to estimate the skill of the model on new data. In this case we used 10-fold cross validation. In k-fold

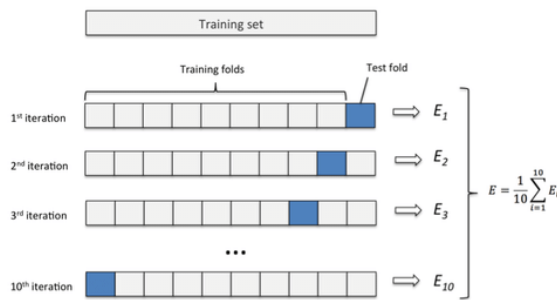


Figure 7: 10-fold cross validation

cross-validation, the original sample is randomly partitioned into k equal sized subsamples. Of the k sub-

samples, a single subsample is retained as the validation data for testing the model, and the remaining subsamples are used as training data. The cross-validation process is then repeated k times, with each of the k subsamples used exactly once as the validation data. The k results can then be averaged to produce a single estimation. The advantage of this method over repeated random sub-sampling is that all observations are used for both training and validation, and each observation is used for validation exactly once.

Results when compared with other pre-existing networks were found to be less accurate than this network. Accuracy of around 91 percent was achieved while no other model could give accuracy of more than 90 percent.

Table 1: Accuracy using different network architectures.

Network Architecture	Accuracy
Lenet	82.7%
VGG 16	79.3%
VGG 19	87.8 %
Proposed Architecture	90.8%

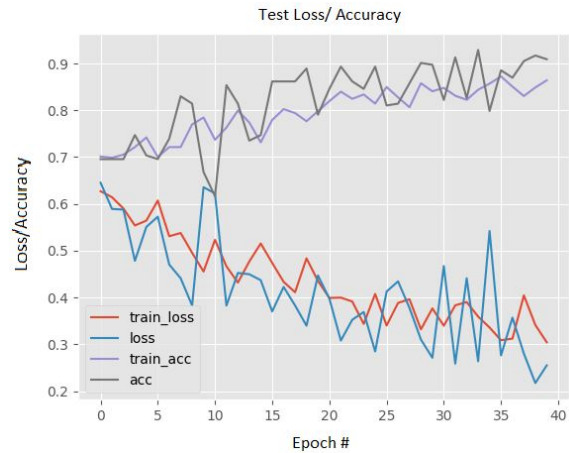


Figure 8: Results using CNN.

## 4.2 Self Organizing Map

The SOM algorithm (Kohonen, 2013) is based on competitive learning. It provides a topology preserving mapping from the high dimensional space to neurons. Our brain is subdivided into specialized areas, they specifically respond to certain stimuli i.e. stimuli of the same kind activate a particular region of the brain. The idea is transposed to a competitive learning system where the input space is "mapped" in a small (often rectangular) space with the following principle: similar individuals in the initial space will be pro-

jected into the same neuron or, at least, in neighboring neurons in the output space (preservation of proximity). Neurons usually form a two-dimensional lattice and forms a mapping from high dimensional space onto a 2-dimensional plane in our case. Topology preserving property means that the mapping preserves the relative distance between the points. Points that are near each other in the input space are mapped to nearby map units in the SOM. The SOM can thus serve as a cluster analyzing tool of high-dimensional data. Also, the SOM has the capability to generalize. Generalization capability means that the network can recognize or characterize inputs it has never encountered before.

#### 4.2.1 Learning Algorithm

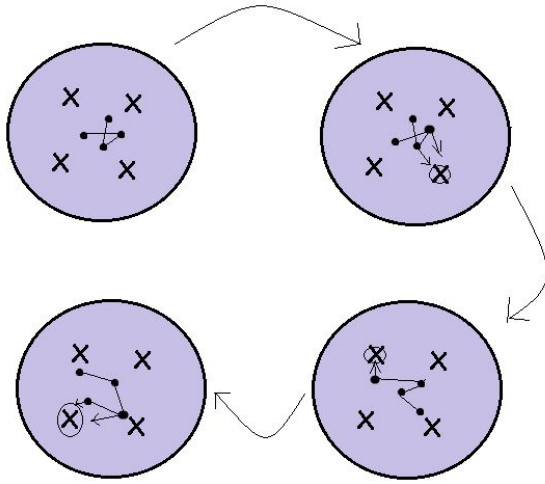


Figure 9: Forming of Map.

These following steps are implemented so that the weight vectors can represent the input data.

Step I: Randomly initialize the weights.

Step II: From the Input data, randomly choose a point (marked in circle).

Step III: Find the weight vector which is closest to the point chosen in previous step. This is considered as the winning neuron.

Step IV: The winning neuron and its closest neighbouring neuron move closer to this chosen point. Neurons which are closer to this point are supposed to take larger steps than their neighbouring neurons.

Step V: These steps are repeated many times

and it results in the weight vectors to settle into stable zones that represent the patterns in the input data.

The step size for updating the weights and the amount of weights to be updated decreases across iterations

For finding the Best matching unit, we iterate through all the nodes and compare the Euclidean distance between every node's weight vector and present input vector. Node with weight vector closest to input vector is termed as the best matching unit for that particular input. This Euclidean distance can be calculated using:

$$dist = \sqrt{\sum_{i=0}^n (V_i - W_i)^2}$$

where  $V$  is current input vector and  $W$  is node's weight vector.

Once this best matching unit is decided, we find all the other node's which are in its neighbourhood because in next step all their weights will be altered. Number of node's coming in a BMU's neighbourhood depends on the radius of neighbourhood chosen. This area of neighbourhood will keep on shrinking with every iteration. This property is visualized by the exponential decay function.

$$\sigma(t) = \sigma_0 e^{-t/\lambda}$$

where  $\sigma_0$  denotes the width of the lattice at time  $t=0$ ,  $\lambda$  denotes the time constant and  $t$  represents current iteration of the loop.

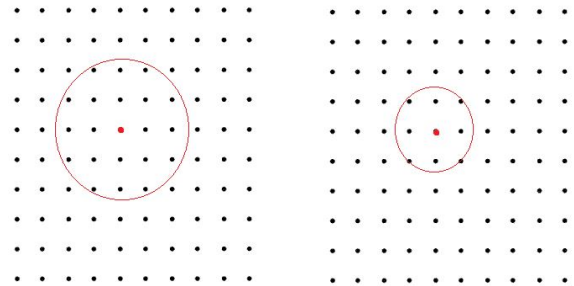


Figure 10: Shrinking of radius.

This radius will keep shrinking until only one neuron that is the BMU is present inside the neighbourhood. Weight vector of every node present inside the current neighbourhood is updated using

$$W(t+1) = W(t) + \theta(t)L(t)(V(t) - W(t))$$

where  $t$  is the time step,  $L$  is the learning rate which decays with time using

$$L(t) = L_0 e^{-t/\lambda}$$



Now practical use suggests that not only the Learning rate should decay with iteration but also it's effect should decrease as the distance from the best matching unit increase. There should barely be any effect at edges of the neighbourhood. To fade the amount of learning with increasing distance Gaussian decay function is used.  $\theta$  defines the amount of influence on learning rate of a node with distance 'dist' from BMU will have.

$$\theta(t) = e^{-dist^2/2\sigma(t)^2}$$

Neuron grid that is used is 2 dimensional rectangular grid. Therefore each neuron is connected directly to 4 other neurons which are it's close neighbours. Every neuron possess two properties that is connection to other neurons and position. Connections are defined before the start of training and that remain same in all the iterations whereas the positions keep on changing. Positions of these neurons were initialized randomly. At the end of every iteration the position of the winning neuron and all the neurons in it's neighbourhood are updated.

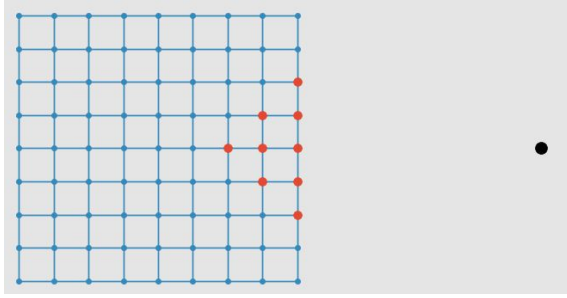


Figure 11: Feature map before training

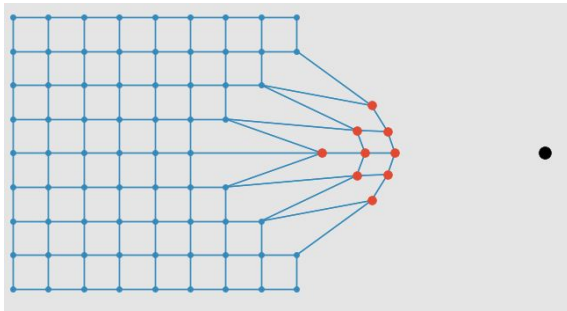


Figure 12: Feature map after training

## 5 RESULTS

### 5.1 Using CNN

Around 500 images of Benign and Malignant Polyps were used as input to Neural networks after neces-

sary pre-processing. Different kinds of architectures of neural networks were used to compare the results. K-fold Cross Validation was used on this set. k-fold cross validation is a procedure used to estimate the skill of the model on new data. In this case we used 10-fold cross validation. Accuracy achieved using these networks is shown in Table 1. Maximum accuracy was achieved using the proposed Network structure while minimum accuracy was achieved using VGG16.

Table 2: Accuracy using different network architectures.

Network Architecture	Accuracy
Lenet	82.7%
VGG 16	79.3%
VGG 19	87.8 %
Proposed Architecture	90.8%

## 5.2 Clustering

### 5.2.1 Implementation

The grid structure proposed in our method is Rectangular grid - Rectangular neighbourhood. The notion of neighborhood is essential in SOM, especially for the updating of weights and their propagation during the learning process.

Rectangular grid - Rectangular neighborhood

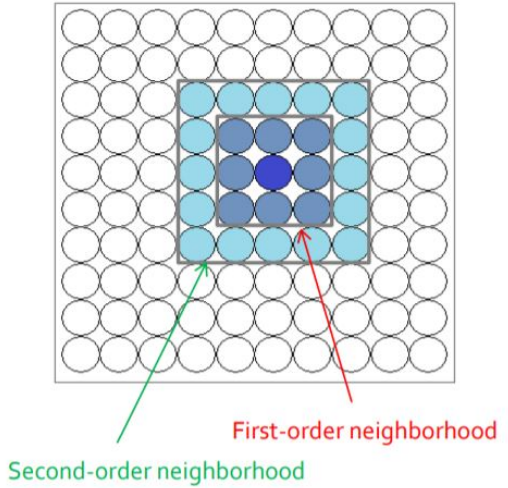


Figure 13: Rectangular grid

The further the neighbouring neuron is from winning neuron, smaller it's learning rate will be and smaller the std parameter, smaller will be learning rate for neighbouring neurons.

Table 3: Image data statistics for 2 class clustering

Image Type	No. of samples
White Light Benign	104
White Light Malignant	92

Table 4: Image data statistics for 4 class clustering

Image Type	No. of samples
White Light Benign	60
White Light Malignant	60
Stain NBI Benign	60
Stain NBI Malignant	60

Parameters used for the Competitive Neural network:

- i) Initial Learning Radius: 6
- ii) Reduce radius after: 5 Epochs
- iii) std = 1
- iv) reduce std after: 5 Epochs
- v) step= 0.1
- vi) Reduce step after: 5 Epochs

### 5.2.2 Formation of Clusters

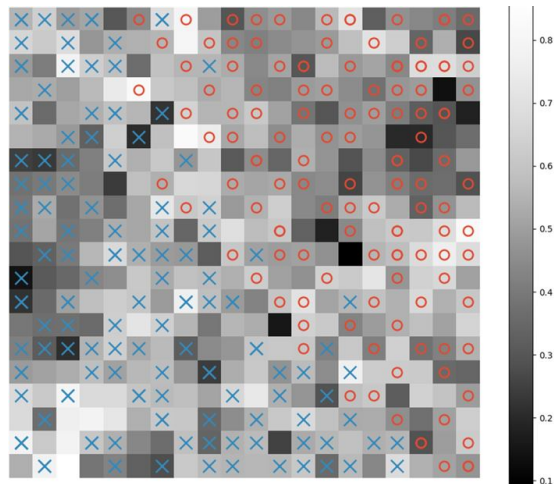


Figure 14: Clustering of White Light Benign and Malignant polyp

Where square represents StainNBI Benign, pentagon is StainNBI Malignant, cross represent White Light Benign and Circle shows White Light Malignant. Each Cell in this heatmap has a number associated with it which represents its average distance to neighbour clusters. This number can be interpreted from the color bar. White color means that this cluster is far from its neighbours.

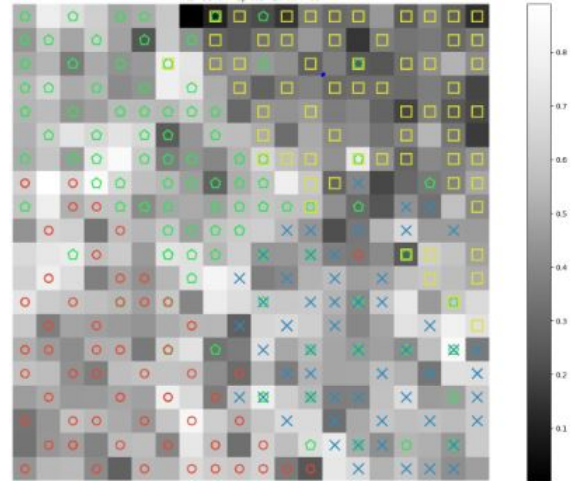


Figure 15: Clustering of White Light Benign, Malignant, Stain NBI Benign, Malignant Polyp

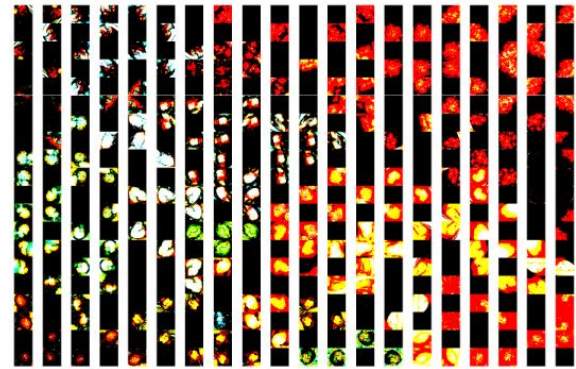


Figure 16: 4-class original cluster

Figure 10 and 11 shows the formation of clusters according to the similarity in the structure of input polyps. Different symbols are used to represent polyps belonging to different classes. Polyp structures which are predicted to be of similar shapes tend to remain closer than those with different shapes. Figure 12 contains original images from the reduced data set. This figure can be used to carefully understand the relation between a new polyp data with those which occurred in past.

## 6 Conclusion

Thus the CNN Architecture proposed in this paper can be used for efficient classification of Benign and Malignant Polyps from the Endoscopic scene. Such kind of automatic classification can lead to easy diagnosis of tumor at early stage and further course of treatment can be decided effectively. Figure 12 shown above can be further used for real time treatment pre-

diction if proper data is provided.

Further development in this approach can be made so that a doctor can see similar past cases and makes a judgment depending on the outcomes of previous decision thus decreasing the chances of fatality. The kind of treatment given in previous cases can also be provided as input to facilitate automatic prediction of course of treatment using the information on how the actual doctor proceeded in the previous cases of similar polyp structure

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