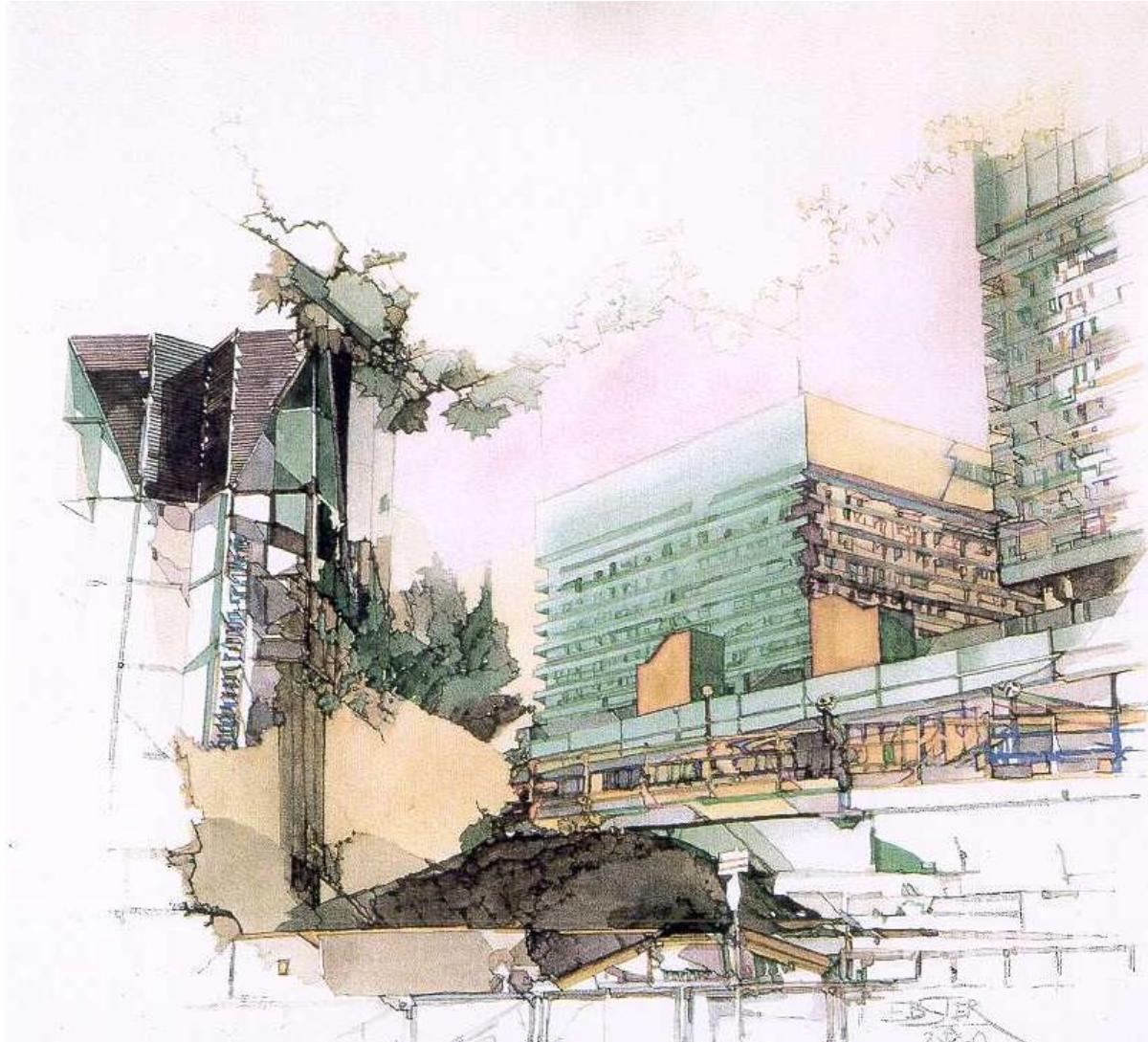
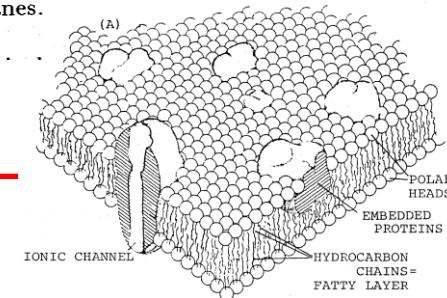


Workshop 8: FES in Rehabilitation – Practical Aspects

Role of Electrical Parameters





Functional Electrical Stimulation - FES

Induction of electrical fields in biological tissue -

- to influence voltage across excitable cell membranes
(mostly cylindrical surface of nerve or muscle fibers)

TOOL for

inducing action potentials in

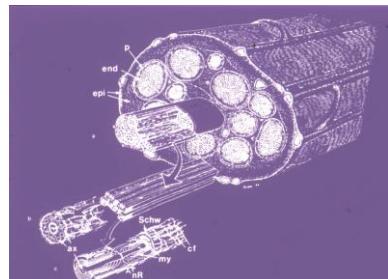
- Afferent neurons
- Efferent neurons
- Muscle fibers

or shifting

resting potential / altering excitability

Limitations in

- Spatial resolution
- Selective recruiting
- Temporal selectivity
- Bidirectional firing

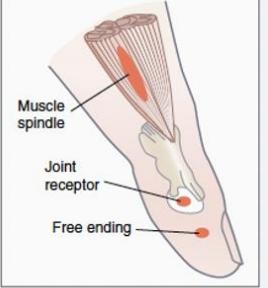
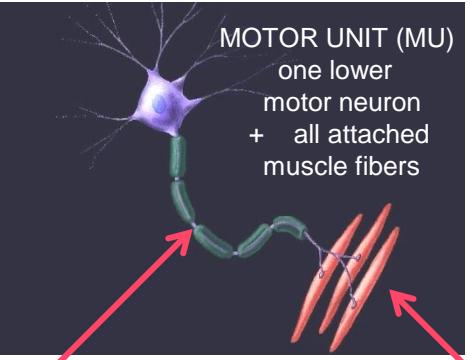
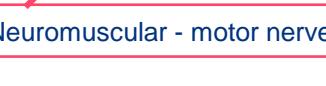
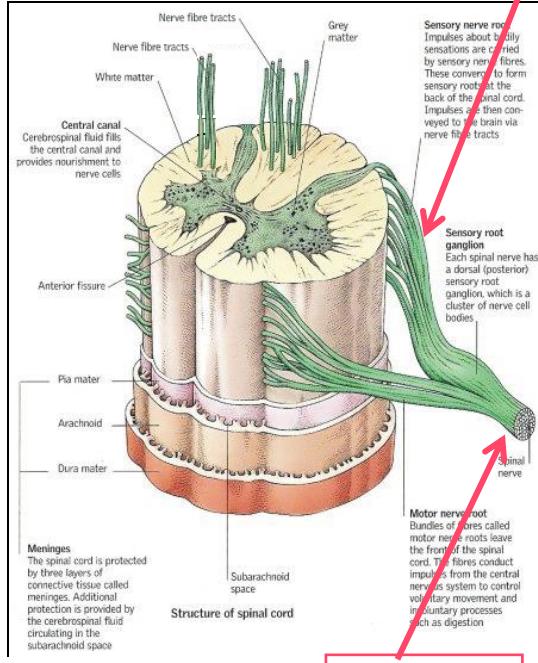


Systemic effects:

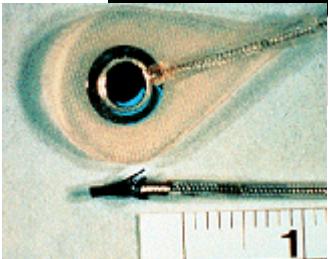
- NOT systemic eMedication !
- (rather alternative to systemic medication)
- NOT direct repair of neural damage
- BUT powerful tool for
- Support of recovery
- Support of tissue maintenance
- Prevention of secondary complications
- Augmentation or substitution of impaired functions (prostheses)

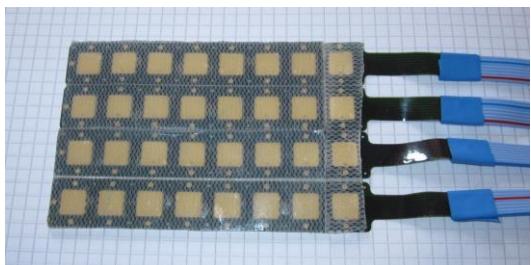
INTERFACING NEURONS AND MUSCLES

with Functional Electrical Stimulation / Neuromodulation

Afferent Nerves	Sensory Functions
	
	Afferent nerves
	Efferent nerves
	MOTOR UNIT (MU) one lower motor neuron + all attached muscle fibers
	Denervated muscle fibers (in absence of nerve only !)
Efferent Nerves	Motor Functions
	Afferent nerves
	Sensory nerve root Impulses about bodily sensations are carried by sensory nerve fibres. These converge to form sensory roots at the back of the spinal cord. Impulses are then conveyed to the brain via nerve fibre tracts.
	Sensory root ganglion Each spinal nerve has a dorsal (posterior) sensory root ganglion, which is a cluster of nerve cell bodies.
Muscle Fibers	Conditioning, Training
	Conditioning, Training
	Tissue Preservation
	Mixed Nerve
	Spasticity / Stiffness / Pain
	Motor Control
	Substitution of Functions

Non-invasive and invasive tools



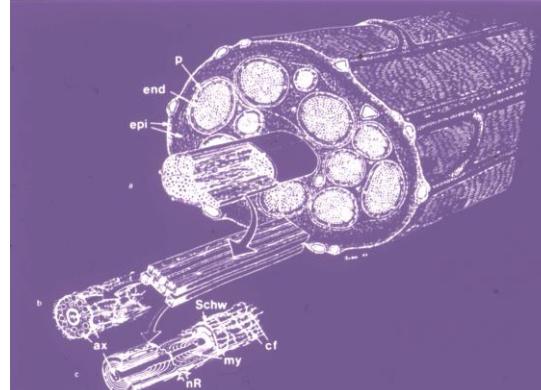


noninvasive

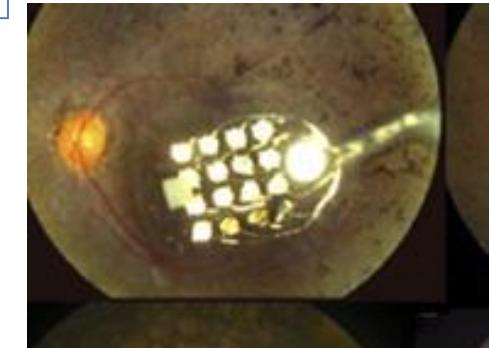
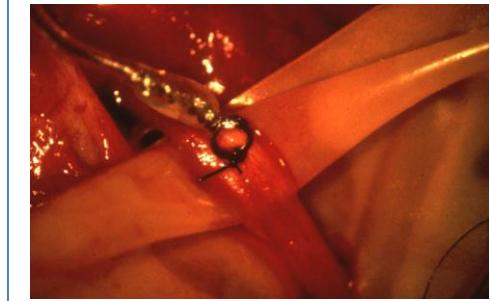
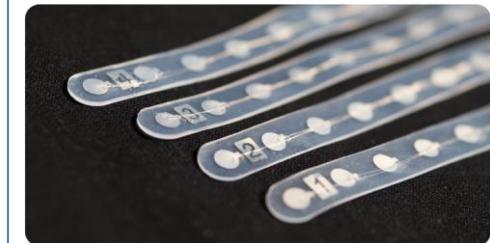
Decisive and limiting
compromise on
selectivity and safety
*

Generally coarse tool to
activate tiny structures
*

Integration of medical,
physiological and
engineering expertise

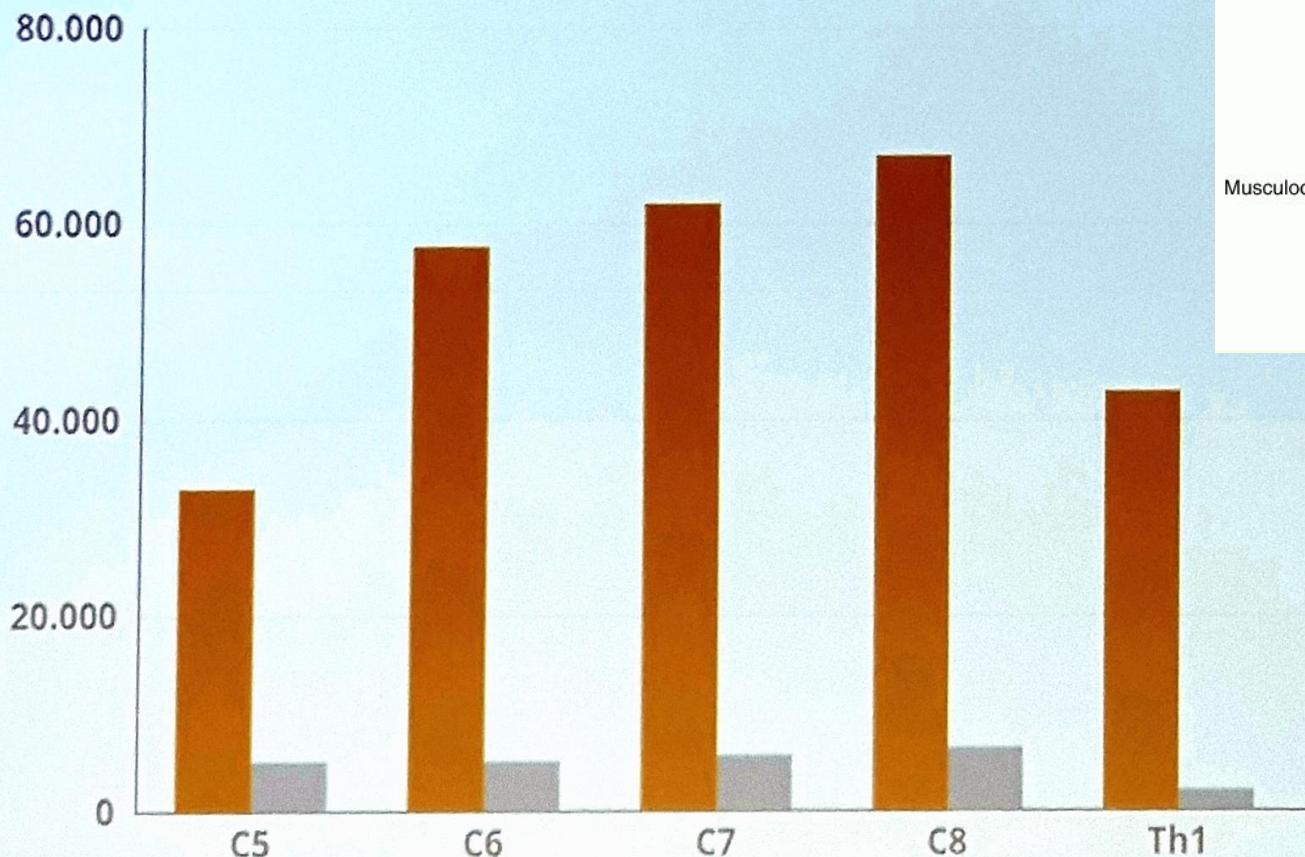


implanted

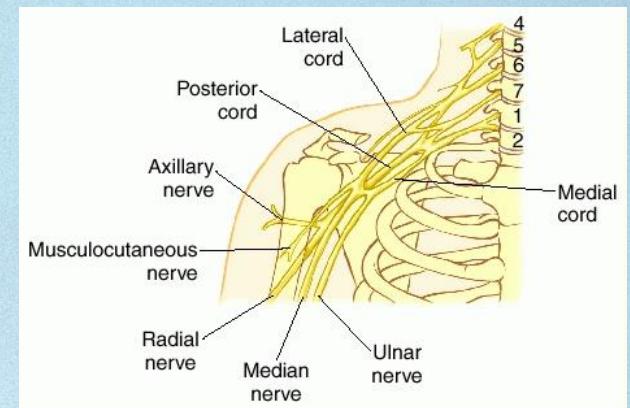


Neuron Recruitment

FIRST QUANTITATIVE DATA ON HUMAN BP



afferent – efferent
9 : 1

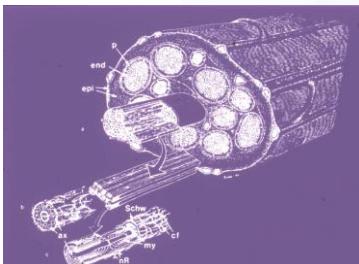


n=12

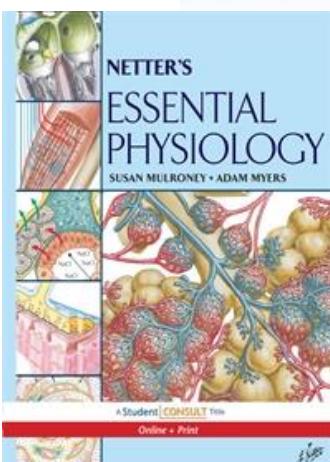
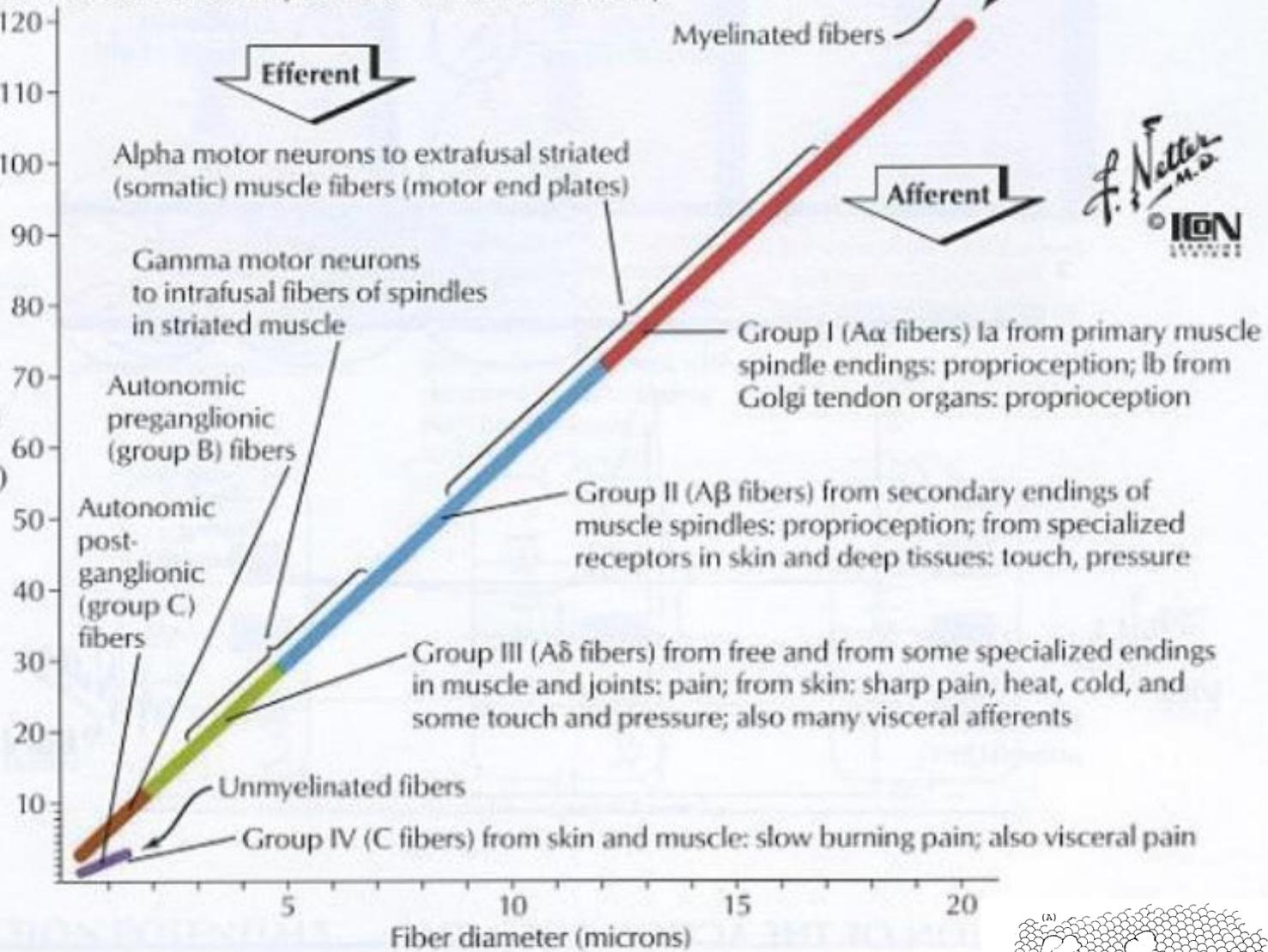
Afferents
Efferents

Gesslbauer B, et al.
Axonal components of nerves innervating the human arm.
Ann Neurol. 2017 Sep;82(3):396-408

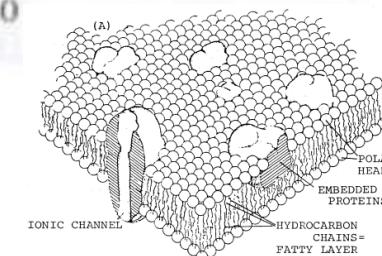
C. Classification of nerve fibers by size and conduction velocity

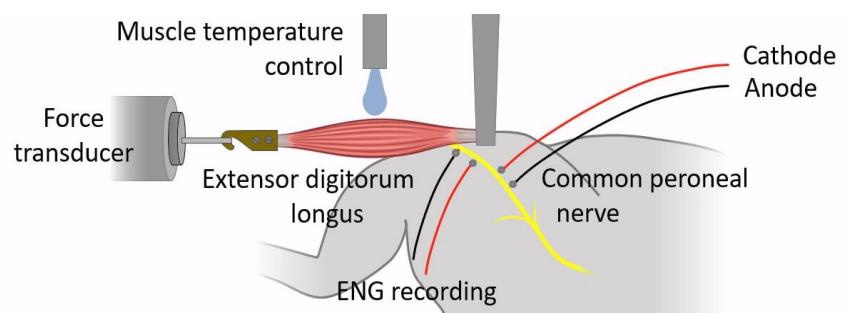
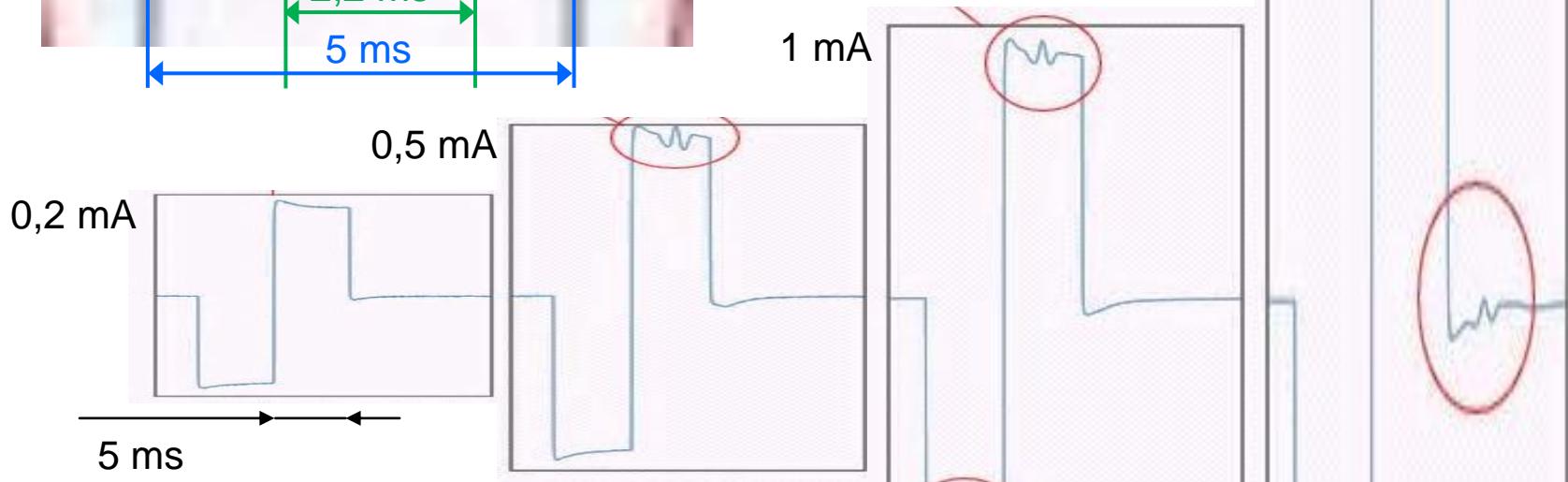
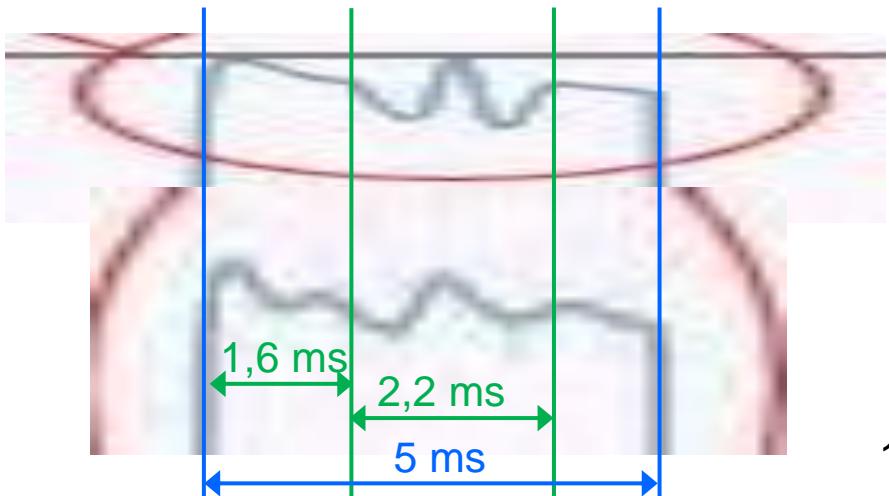


Conduction velocity (meters/sec)



Bretscher M.S. and Raff M.C. 1975. Mammalian plasma membranes.
Nature 258, 43-49





Steffen Eickhoff, Jonathan Jarvis – John Moores University, Liverpool
UNPUBLISHED DATA

SELECTIVITY

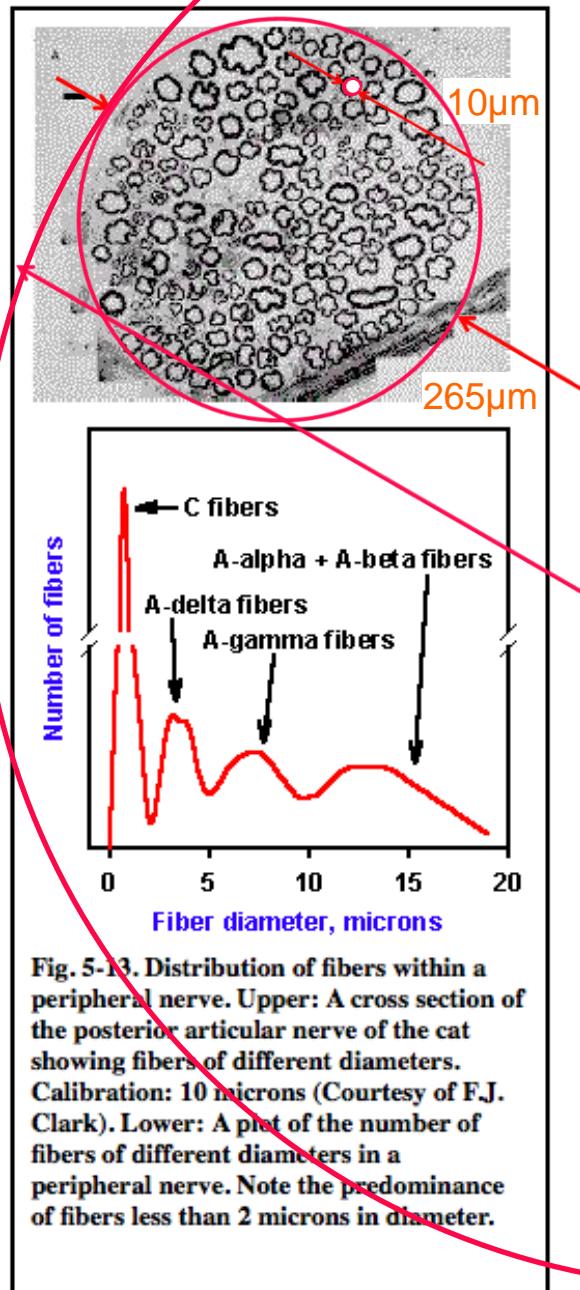
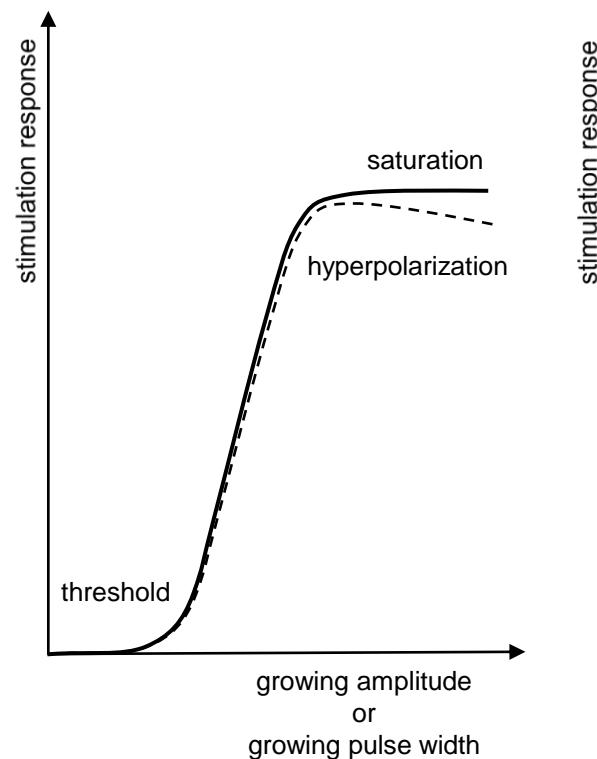


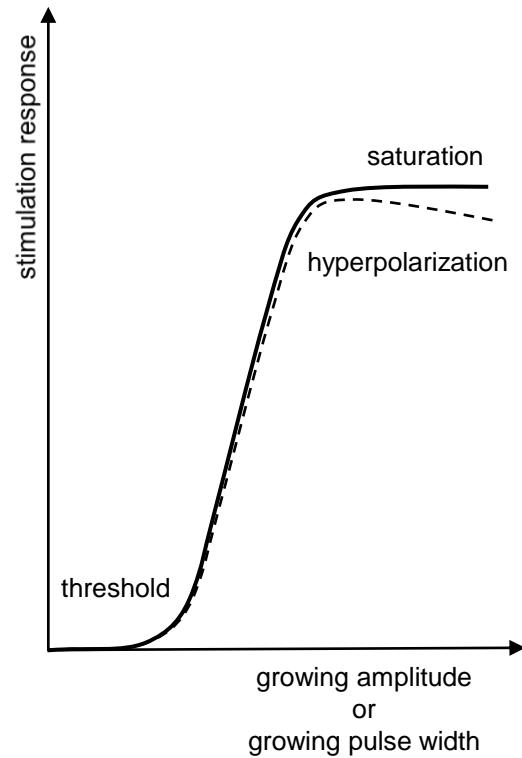
Fig. 5-13. Distribution of fibers within a peripheral nerve. Upper: A cross section of the posterior articular nerve of the cat showing fibers of different diameters. Calibration: 10 microns (Courtesy of F.J. Clark). Lower: A plot of the number of fibers of different diameters in a peripheral nerve. Note the predominance of fibers less than 2 microns in diameter.

THRESHOLDS / Depolarisation / Hyperpolarisation:

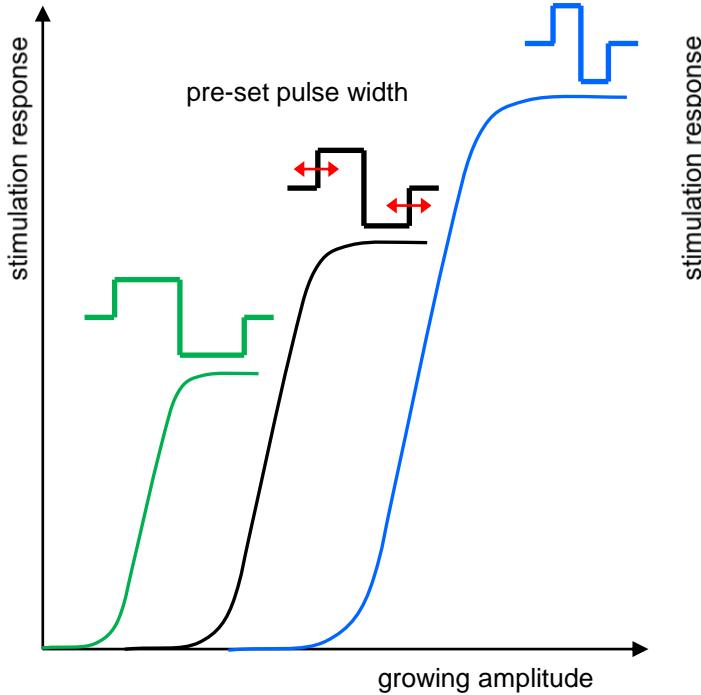
- Inverse proportional fiber size
- Prop. to square of distance



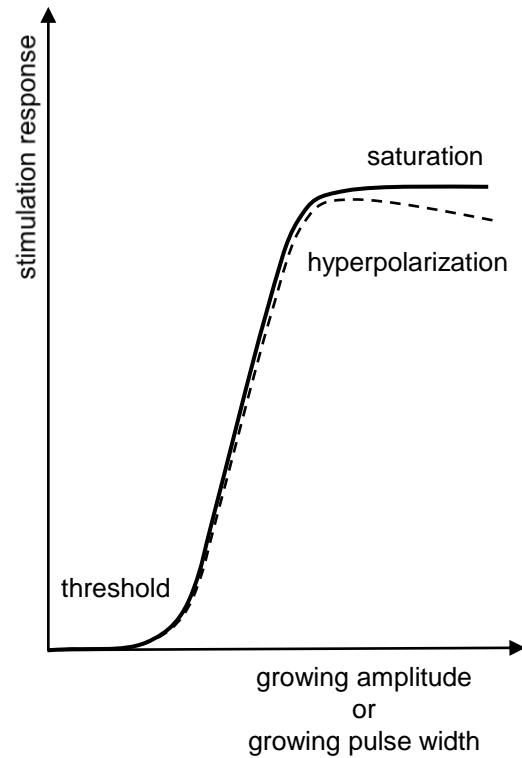
typical recruitment curve,
threshold to saturation



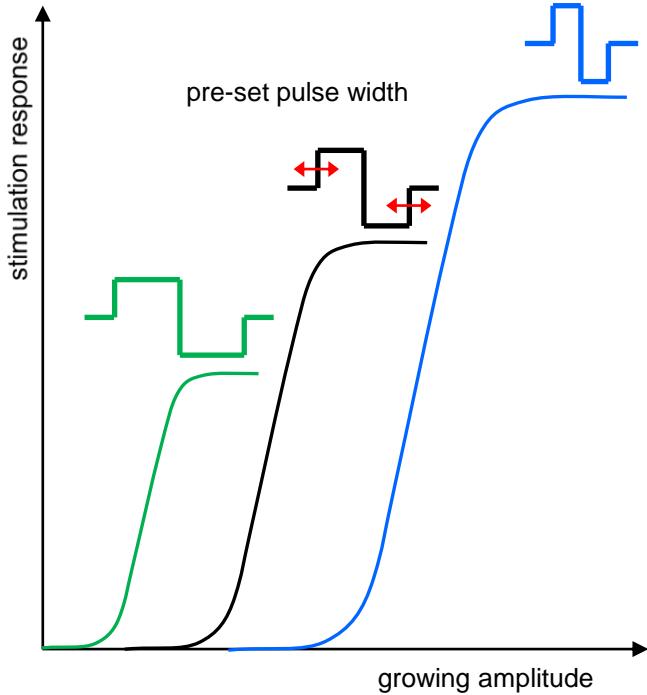
typical recruitment curve,
threshold to saturation



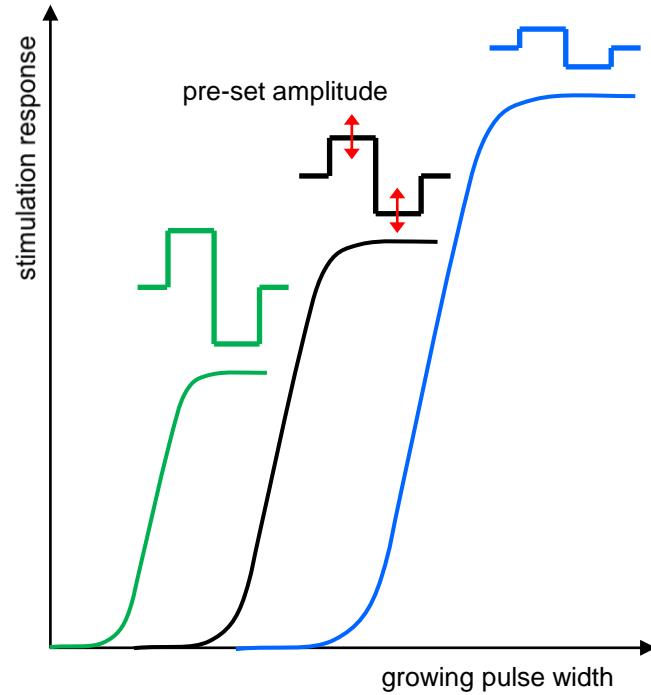
typical recruitment curve,
amplitude variation, constant pulse width



typical recruitment curve,
threshold to saturation

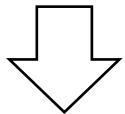


typical recruitment curve,
amplitude variation, constant pulse width

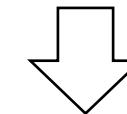


typical recruitment curve,
pulse width variation, constant amplitude

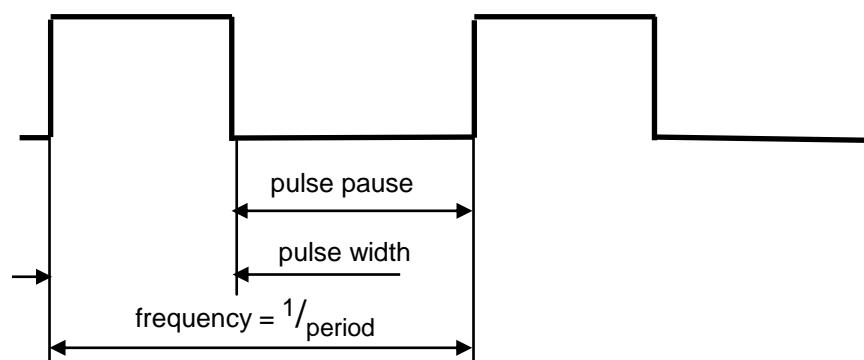
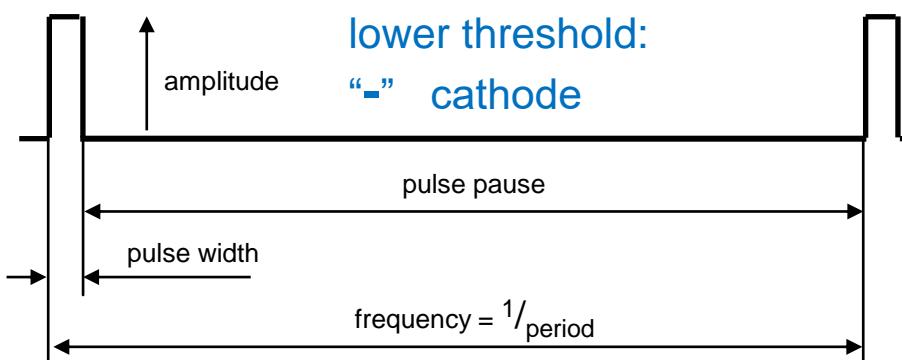
Nerve Stimulation



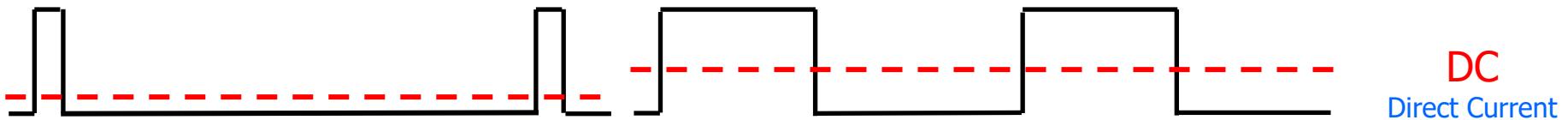
(Muscle Stimulation)



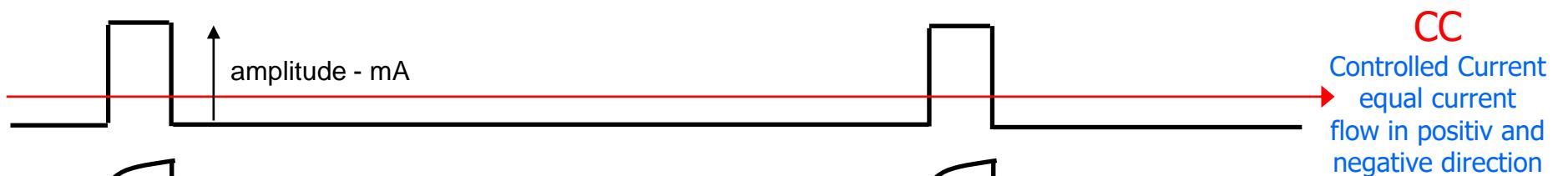
monophasic pulse shape



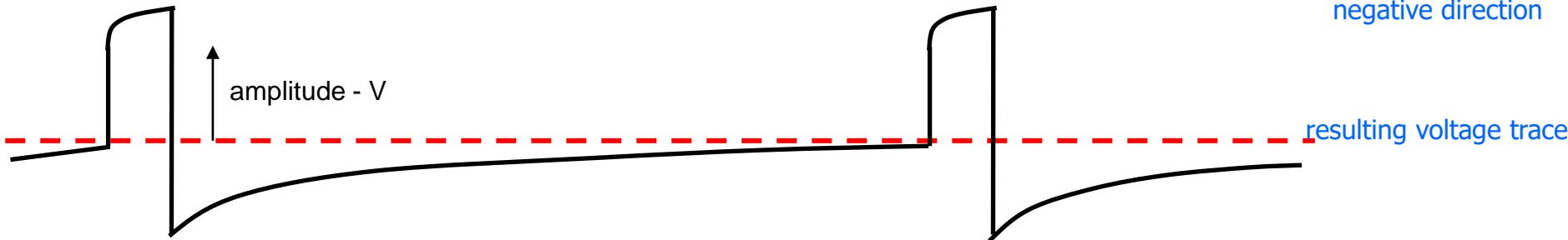
Cave: without DC-decoupling monophasic pulse trains have a DC-component !



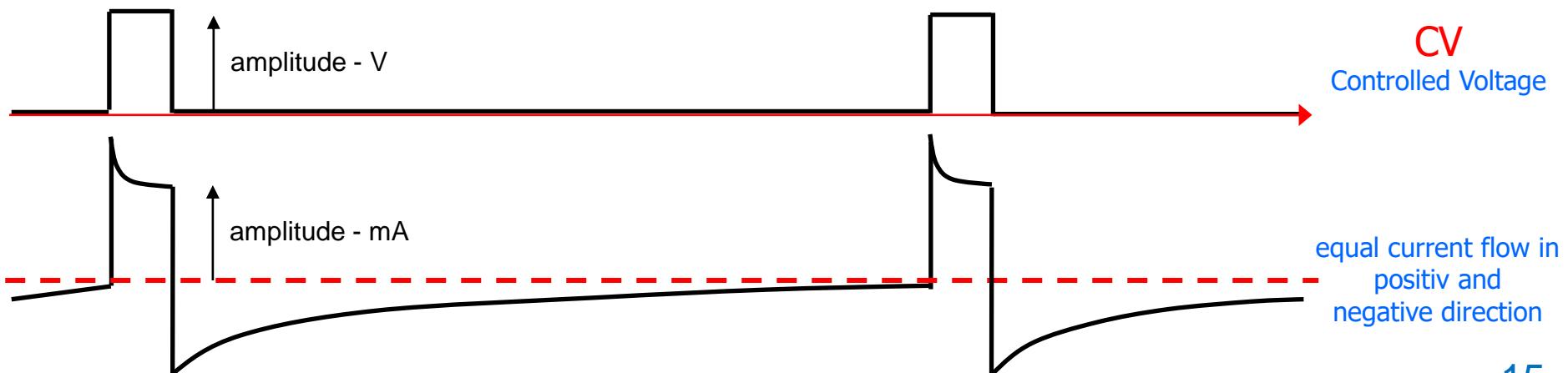
DC-decoupling forces charge balance !



CC
Controlled Current
equal current
flow in positiv and
negative direction



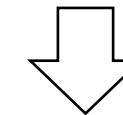
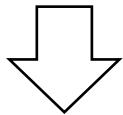
CV
Controlled Voltage



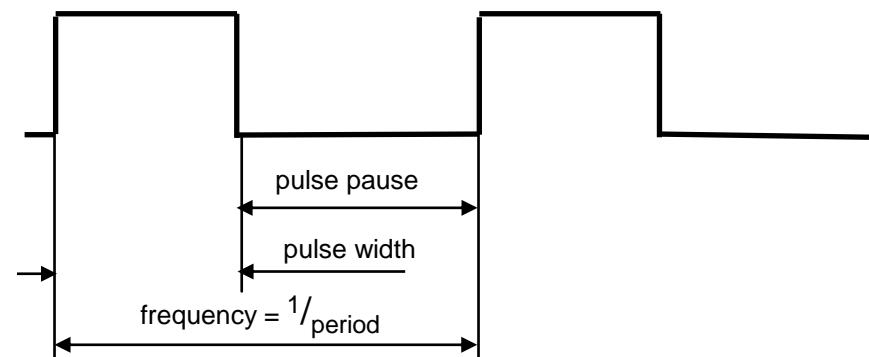
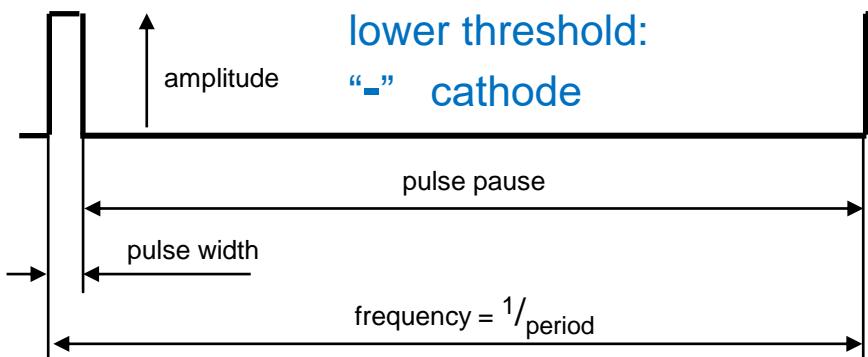
equal current flow in
positiv and
negative direction

Nerve Stimulation

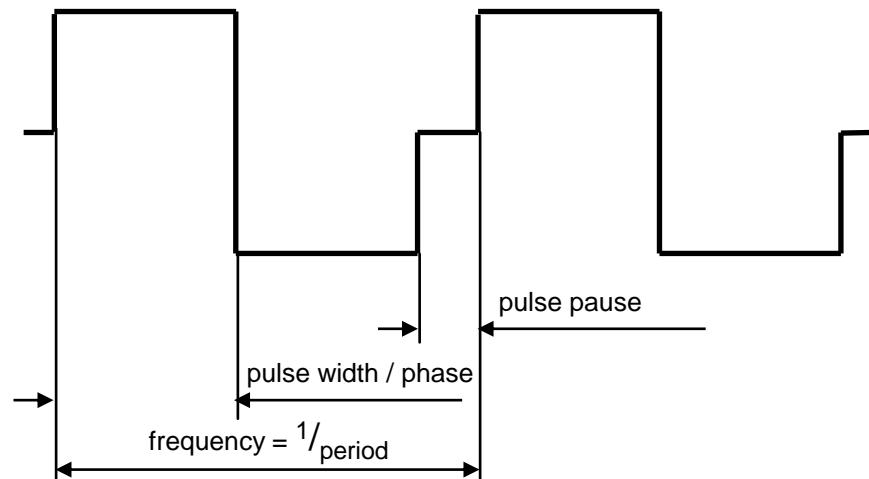
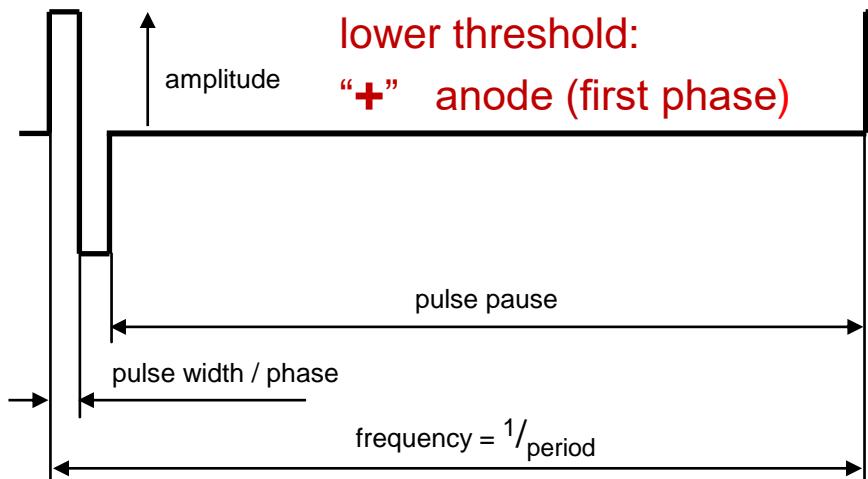
(Muscle Stimulation)



monophasic pulse shape



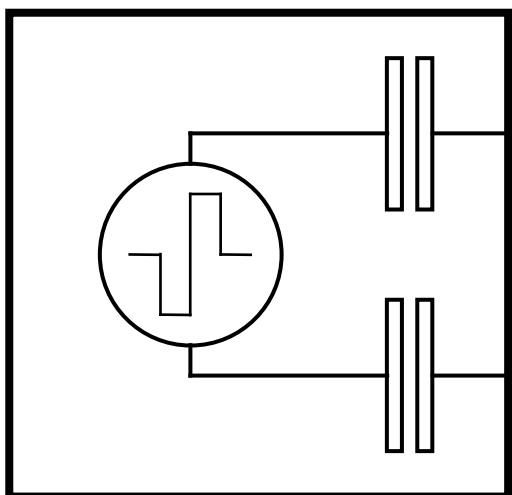
biphasic pulse shape



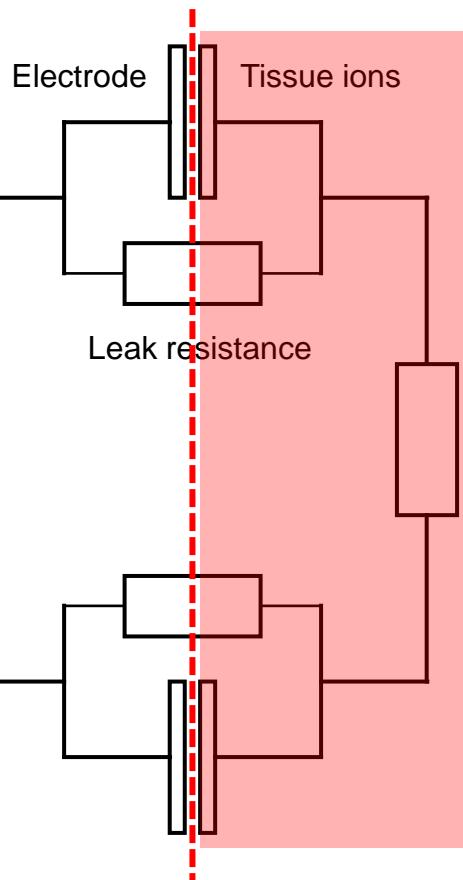
CV

Electrode / Skin

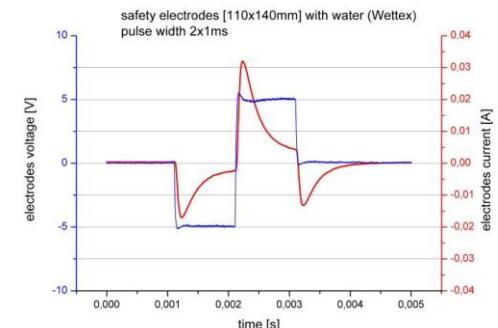
Stimulator



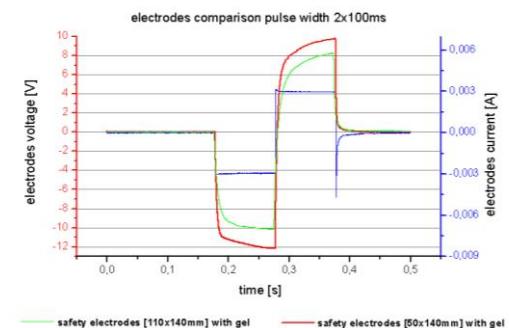
DC-decoupling
⇒ charge balance



Electrode / Skin



Subcutaneous
tissue



CC

Juan Capistrano, CA, USA). The stimulation waveform was biphasic, rectangular, 1 ms pulses at a frequency of 30 Hz, filled with a carrier frequency of 10 kHz (Fig. 2) [17]. This permitted stimulation intensities of 80–120 milliamperes (mA) to be delivered to the skin over the cervical spinal cord without discomfort.

Inanici F, et al.

Transcutaneous Electrical Spinal Stimulation Promotes
Long-Term Recovery of Upper Extremity Function
in Chronic Tetraplegia.
IEEE Trans Neural Syst Rehabil Eng. 2018
Jun;26(6):1272-1278

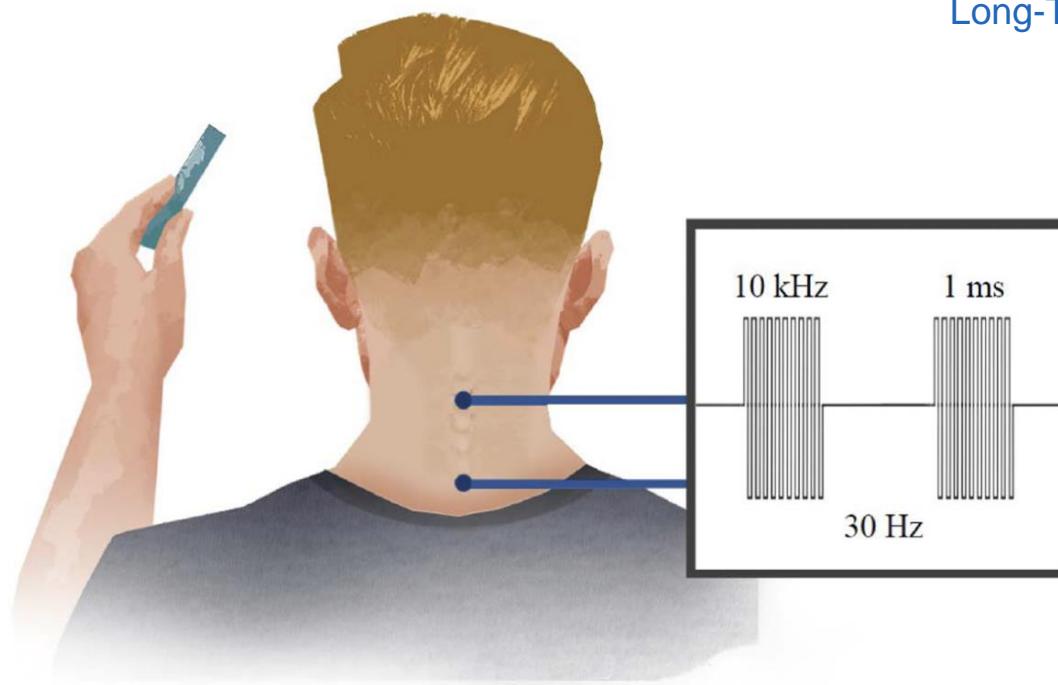


Fig. 2.

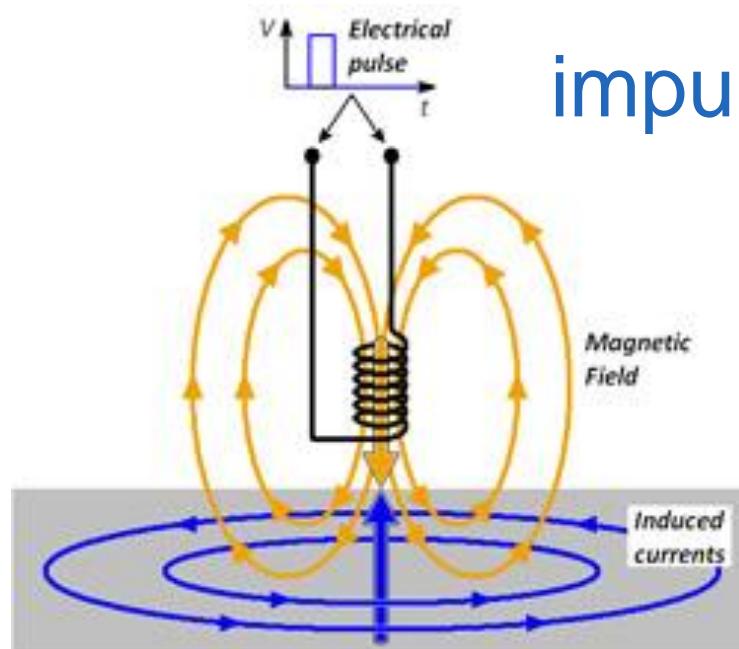
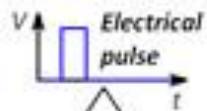
Schematic of the intervention showing electrical cervical spinal stimulation applied to the surface of the skin via electrodes placed midline at C3–4 and C6–7 bony landmarks. (Inset) Biphasic, rectangular, 1 ms pulses are delivered at a frequency of 30 Hz. Each pulse is filled with a carrier frequency of 10 kHz to permit stimulation intensities of 80–120mA to pass through the skin and reach the spinal cord without discomfort.

Stimulation was delivered via two 2.5 cm round electrodes placed midline at C3–4 and C6–7 spinous processes as cathodes and two 5 × 10 cm rectangular plates (Axelgaard Manufacturing Co., Ltd., USA) placed symmetrically over the iliac crests as anodes. A total of 1451 minutes of stimulation was applied over the five weeks (mean duration was 60 ± 20 minutes/session, range 25 – 120 minutes/session).

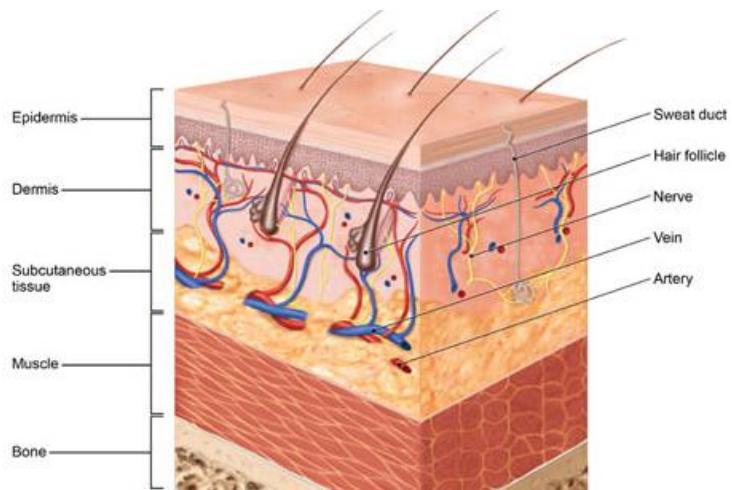


FMS

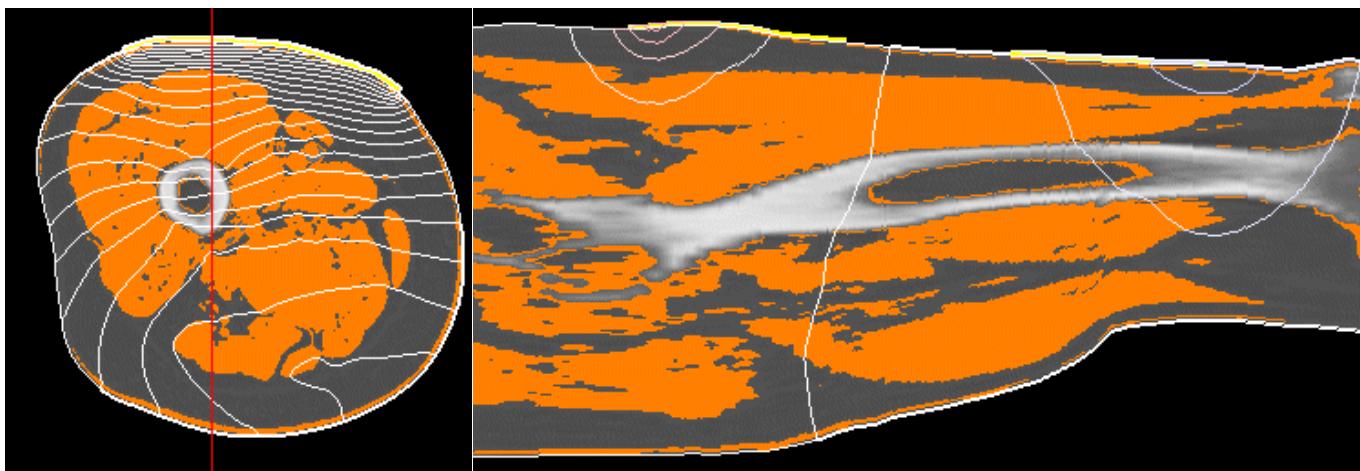
cave : “induction heating” !



impulses - up to 2 Tesla

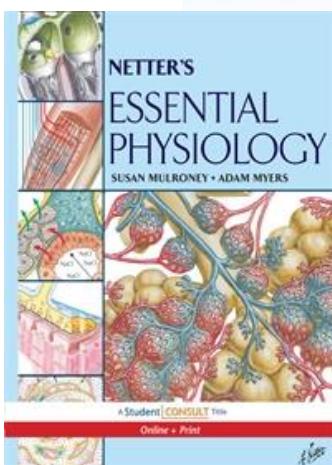
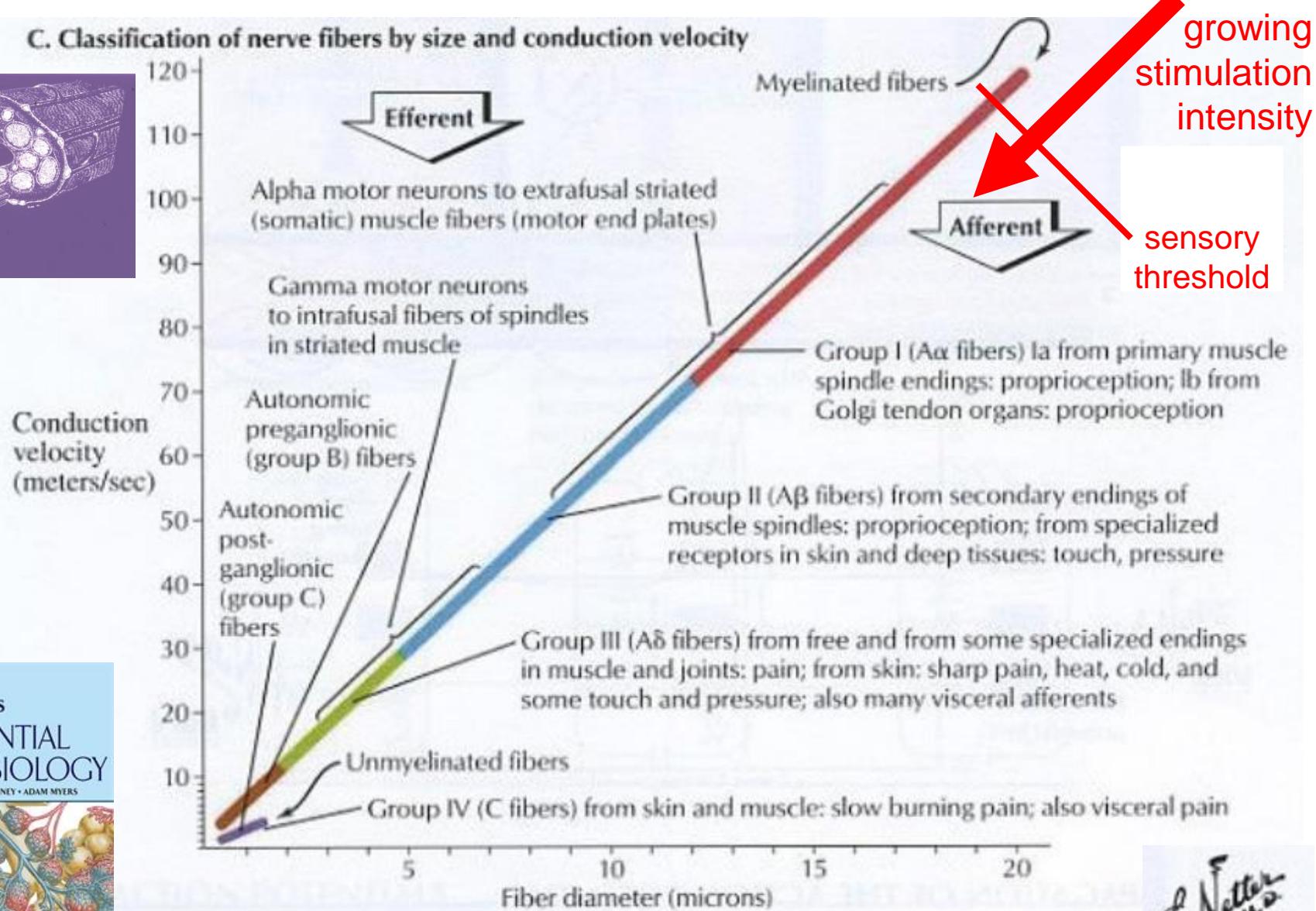
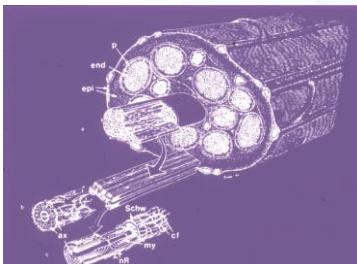


FES



Afferent Neurons

C. Classification of nerve fibers by size and conduction velocity



If we have an idea on fiber recruitment –

- what about neural processing / control of movement ?

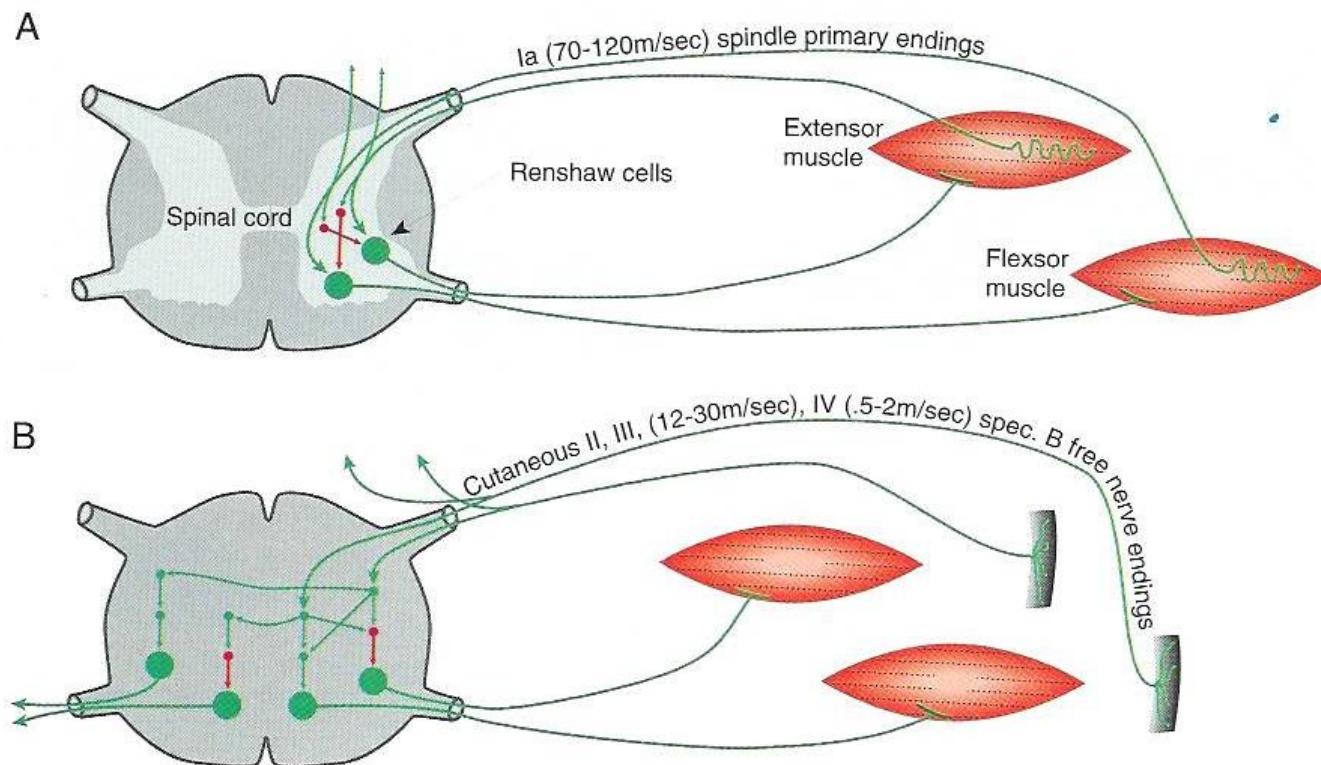
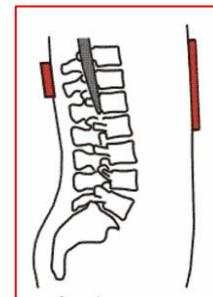
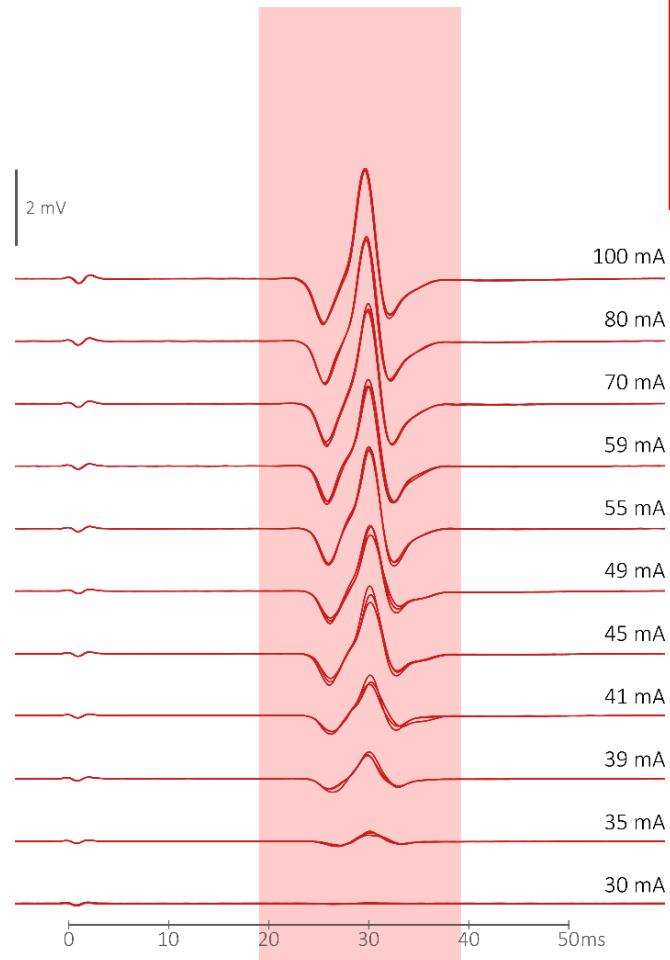


FIGURE 29.3 Circuitry for segmental spinal reflexes. Ia spindle reflexes are activated by stretch of the muscle and cause excitation of that muscle and its synergists and reciprocal inhibition of its antagonists. Skin reflexes (activated by a noxious stimulus) may cause withdrawal of the limb away from the stimulus with a supporting reaction in the opposite limb. Adapted from Thach and Montgomery, *Neurobiology of Disease*, Oxford University Press, New York, 1990.

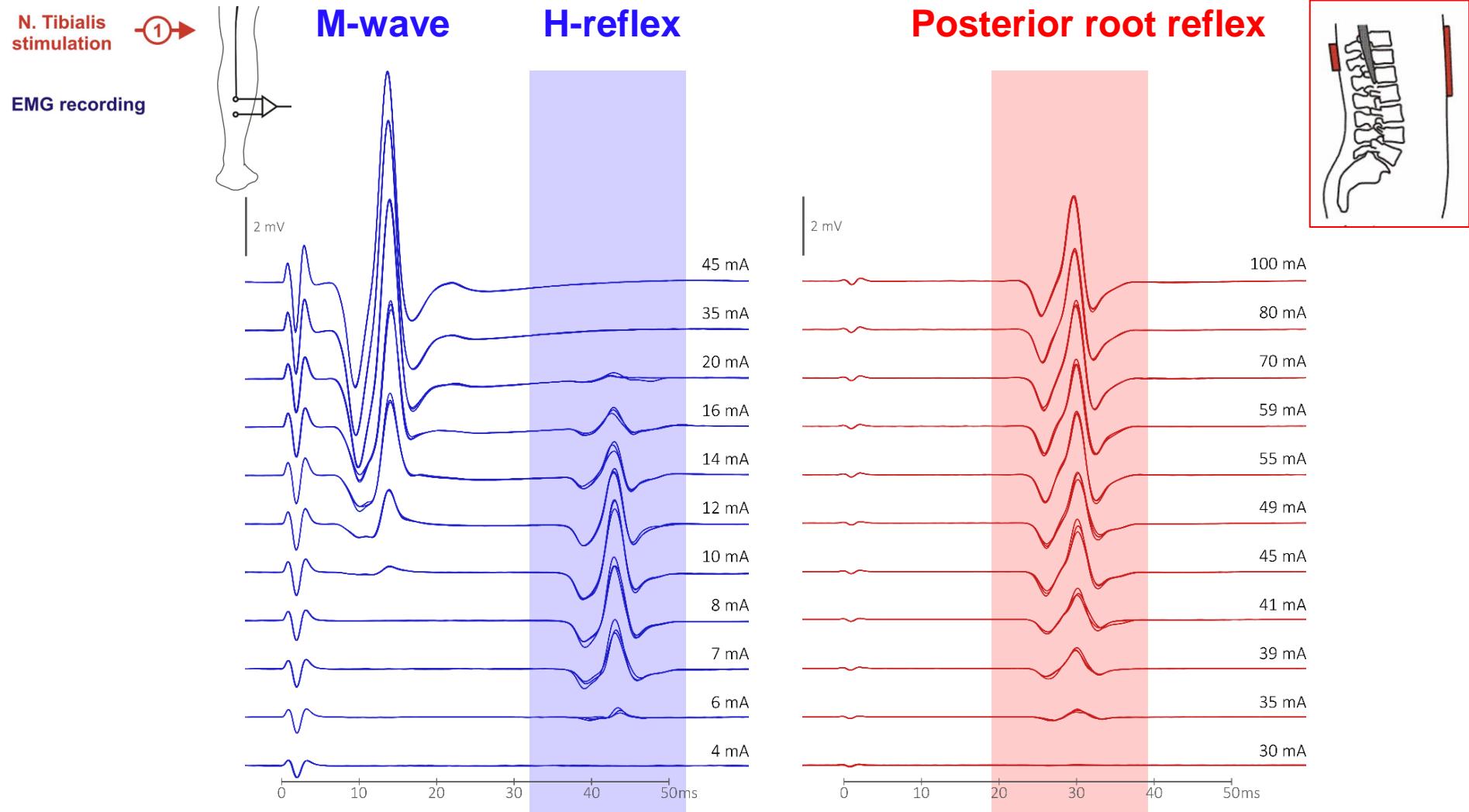
Electrical stimulation of peripheral nerves or posterior roots can activate monosynaptic and polysynaptic reflex arcs

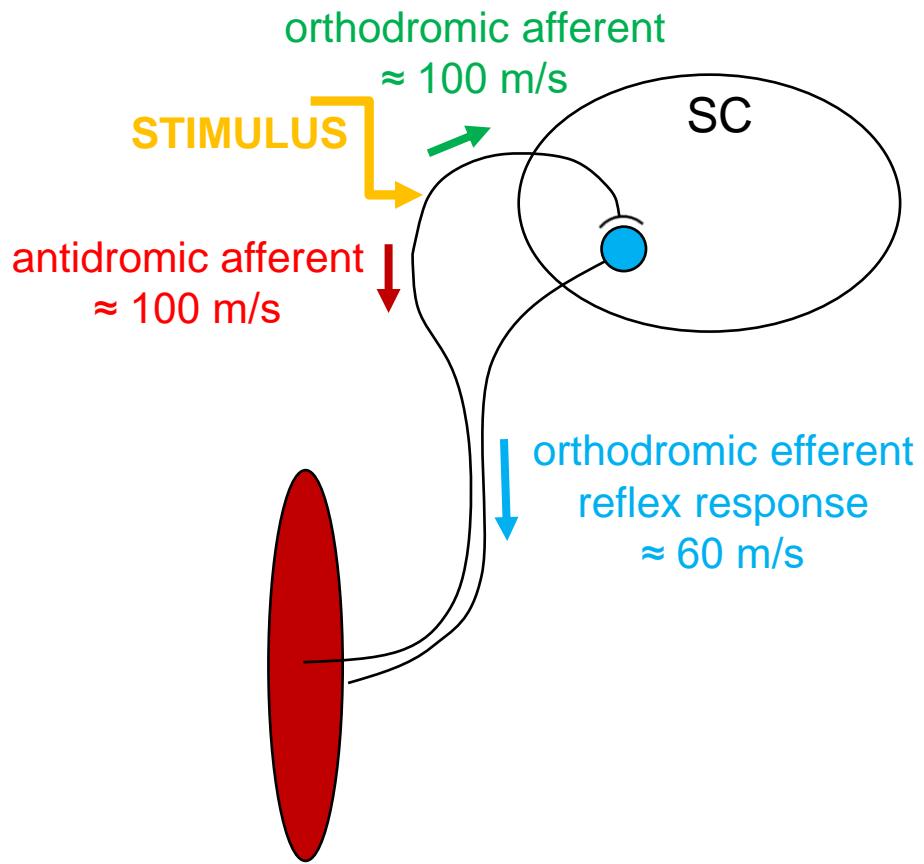
H-reflex and posterior root reflex in the soleus muscle

Posterior root reflex

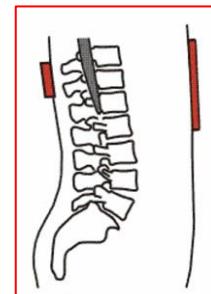
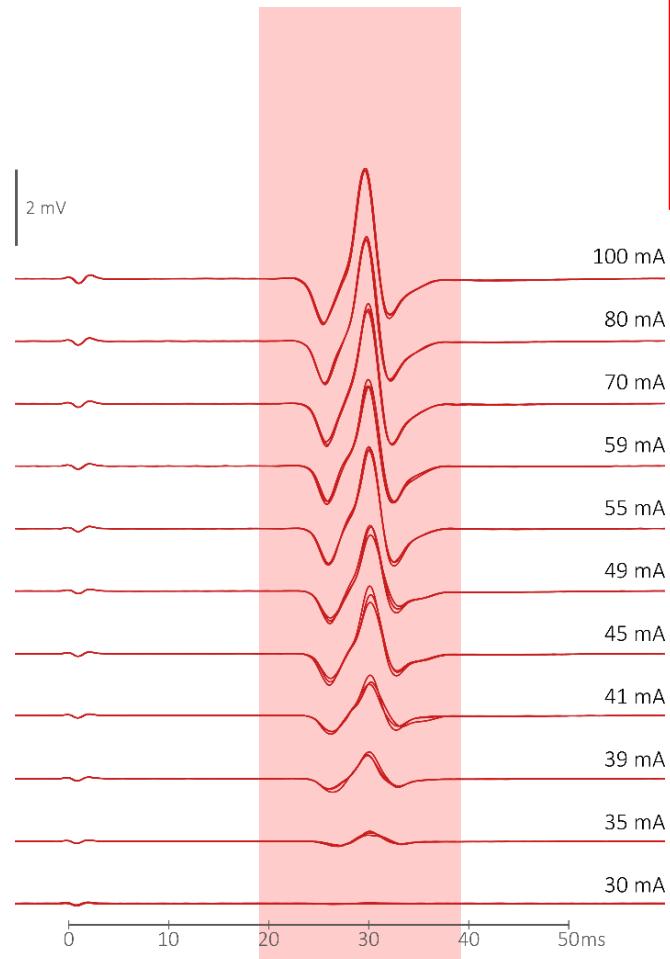


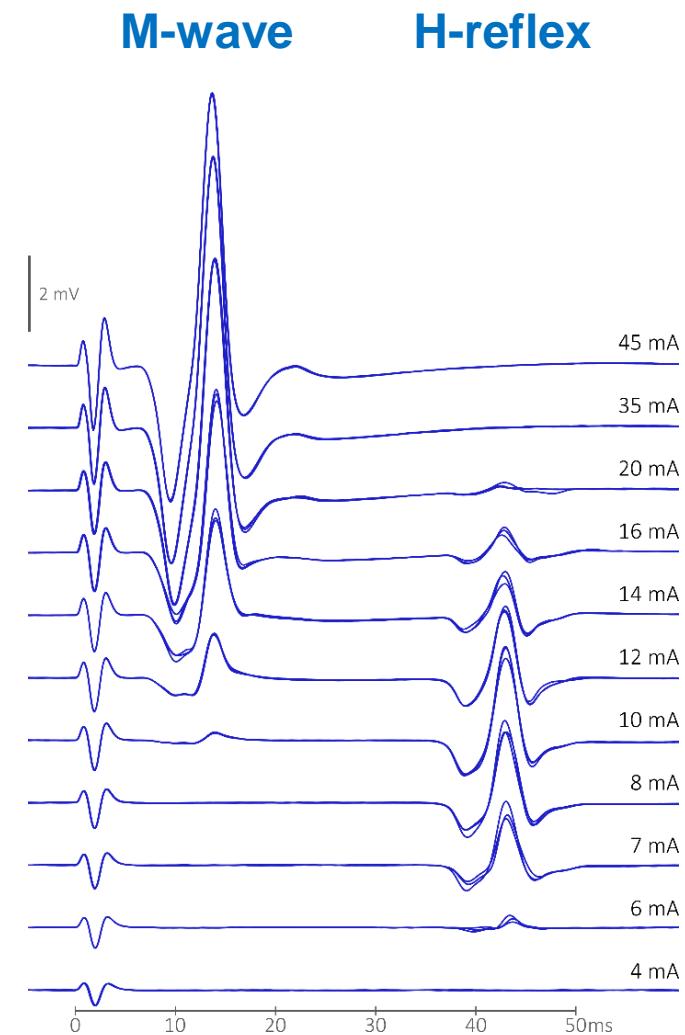
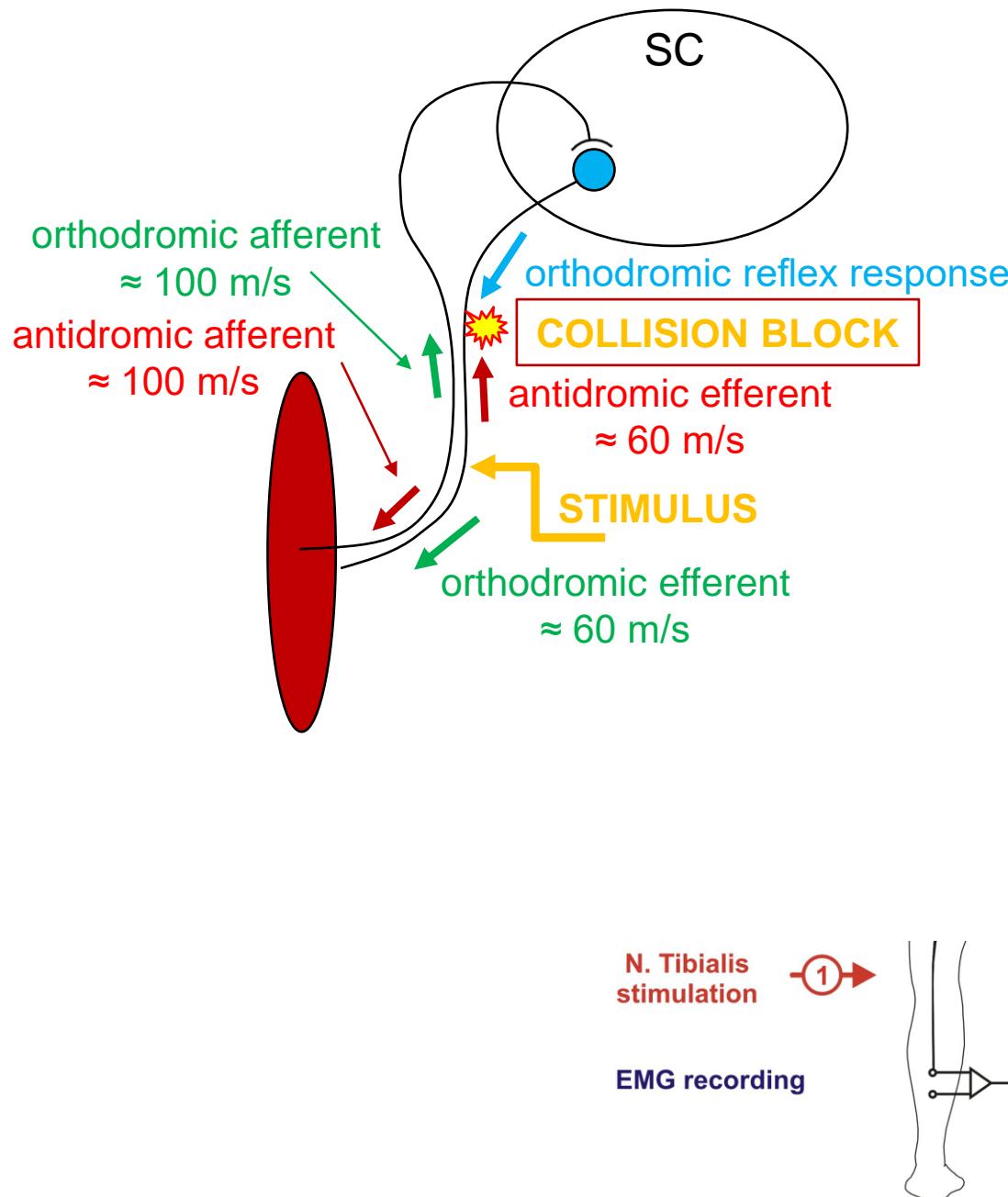
H-reflex and posterior root reflex in the soleus muscle



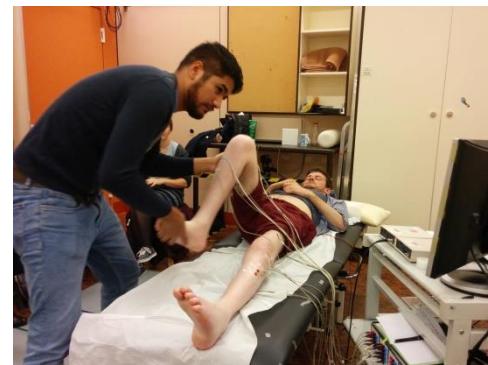
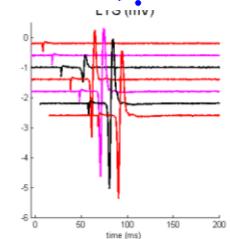
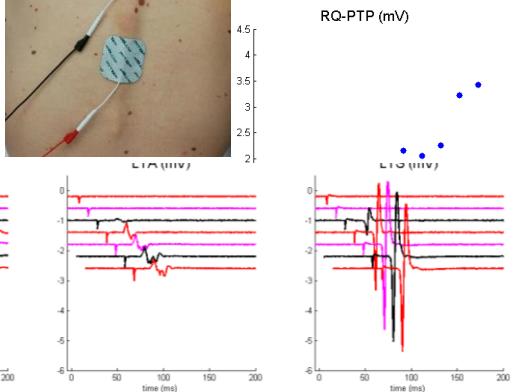
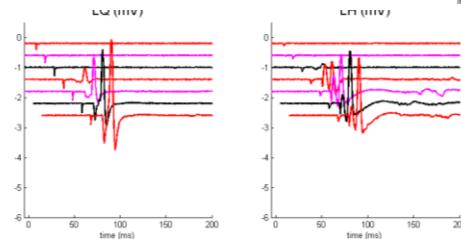
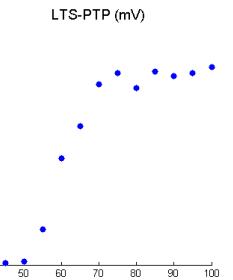
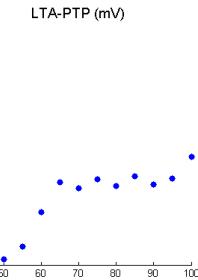
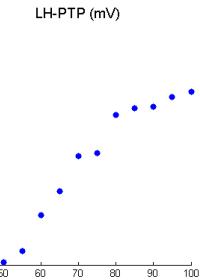
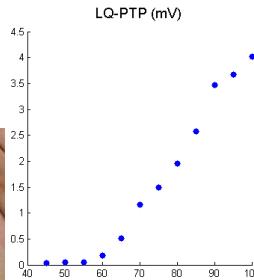


Posterior root reflex





Augmentation of residual neural control by non-invasive spinal cord stimulation to modify spasticity in spinal cord injured people



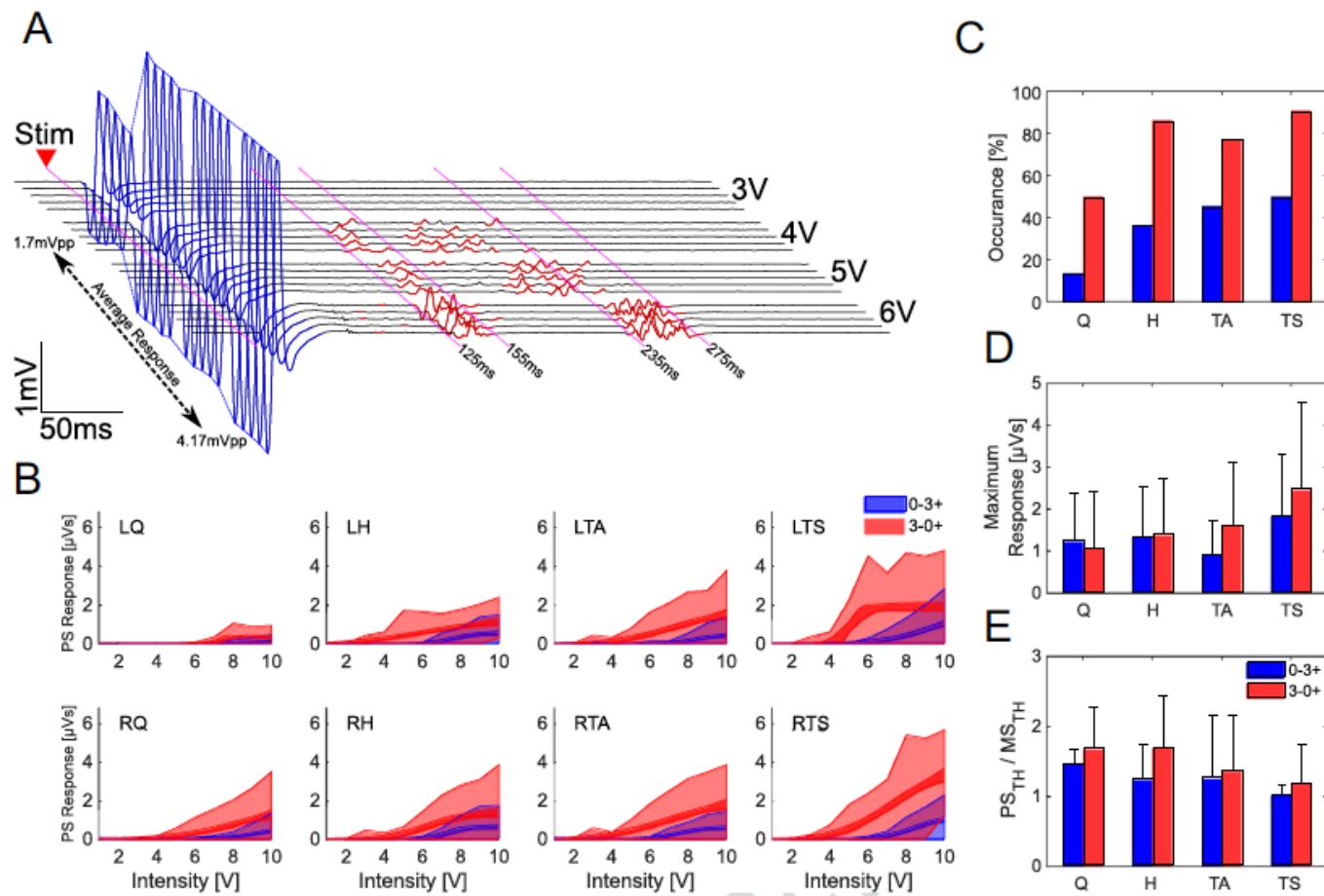
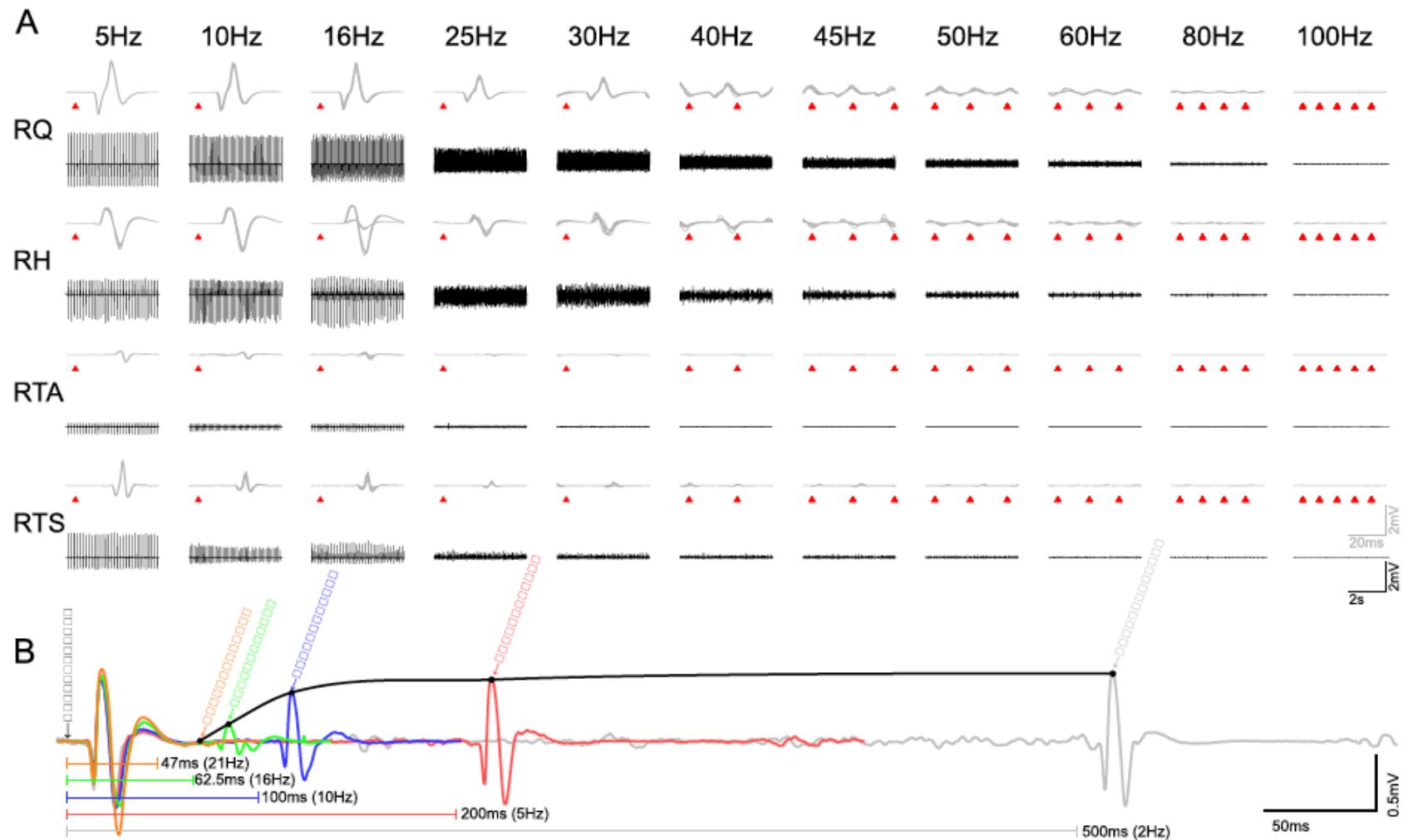
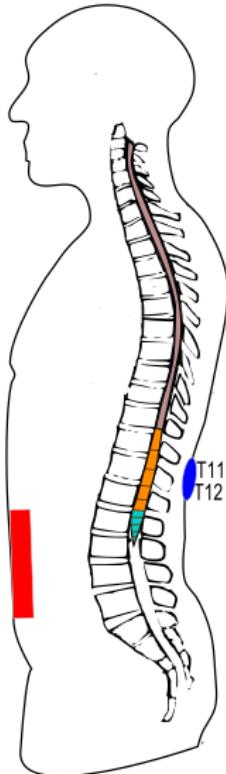


Fig. 2 Characteristics of the Polysynaptic responses. **A** Exemplary responses from RH on SID 10 with 3–0+ electrode configuration. The sEMG show in blue the short-latency (monosynaptic) responses, appearing after ~7 ms, and, in red, the long-latency (polysynaptic) responses, which appear in two groups with latencies of around 130 ms and 260 ms. Both types of responses evolve when the stimulus intensity is increased. **B** Estimated recruitment curve for eight subjects (SID2 and SID8 excluded), showing the 95% confidence interval for the mean amplitude (narrowband) and standard devia-

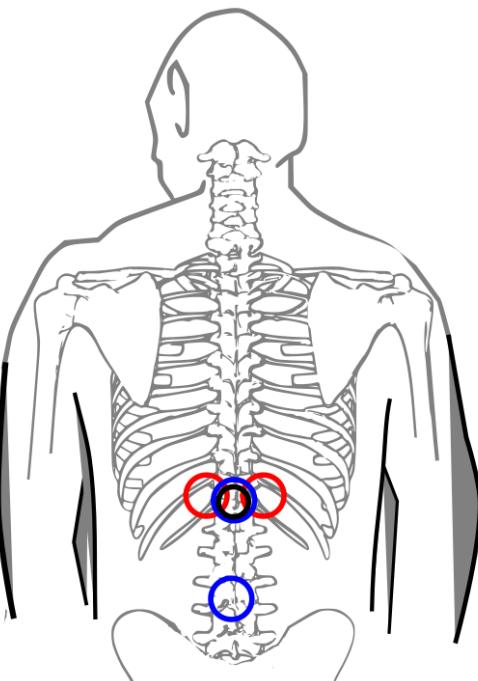
tion of the samples at each intensity (shadowed area) for the lower limbs with both electrode configurations. **C** Shows the percentage of polysynaptic activity occurrence on each muscle group (both sides grouped together). **D** shows the mean maximum response for each muscle and electrode configuration (SID8 excluded due to continuous activity not associated with the stimulation). Finally, **E** Shows the relative threshold of the polysynaptic activity compared to the monosynaptic activity



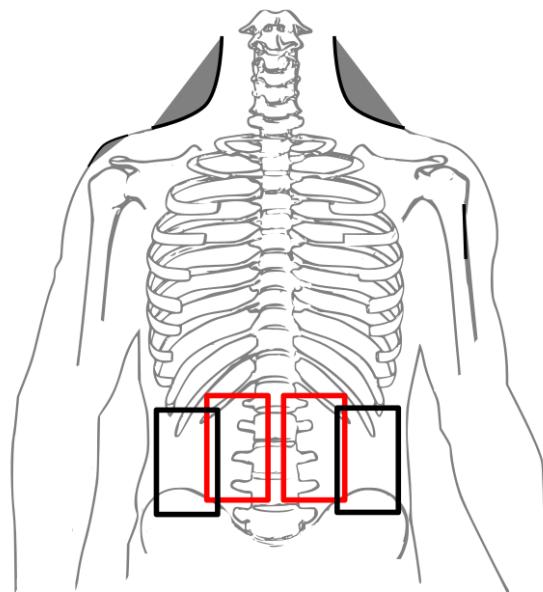
Surface electrode configuration



Stimulation electrode
- Dimension: 2 x 5 cm



Reference electrode
- Dimension: 8 x 13 cm



Transversal setup

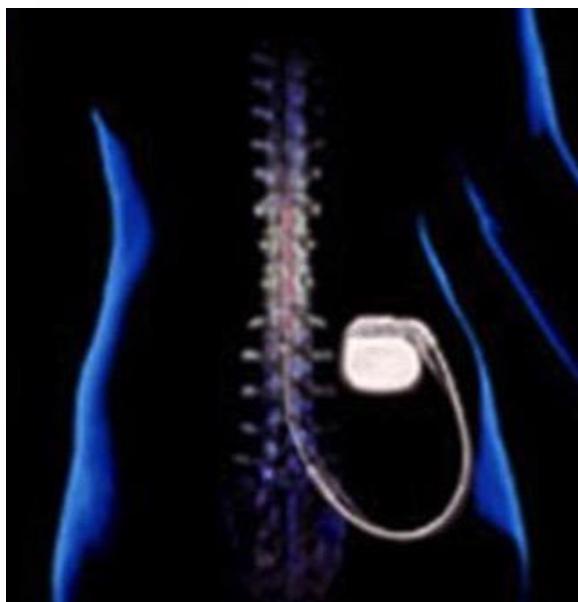
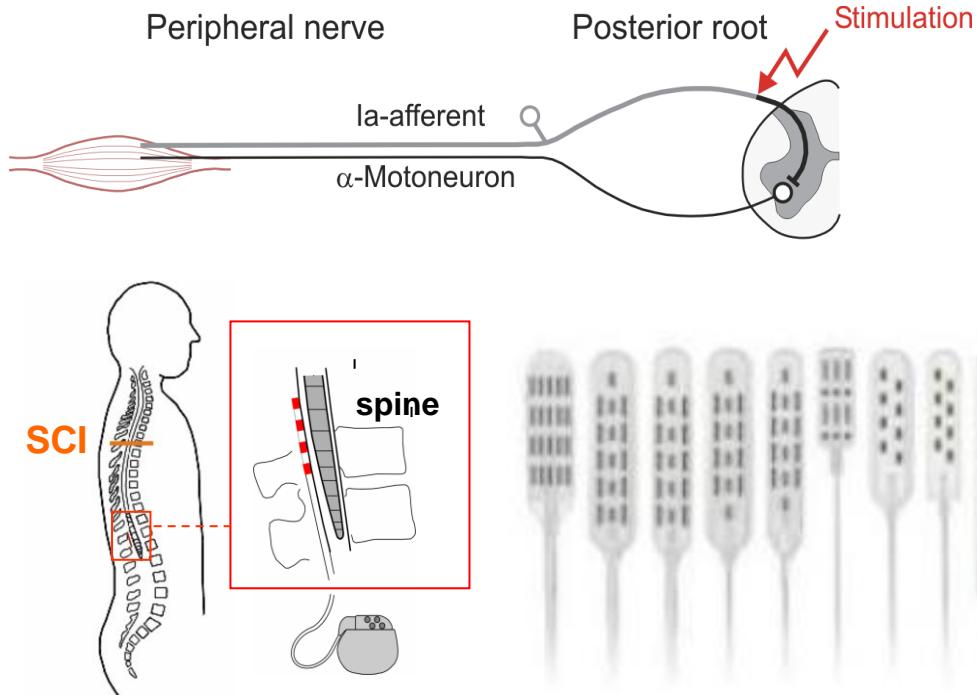
- Lower thresholds
- Flexibility on reference electrode position
- necessary option for adipose persons



Bipolar setup

- Avoids abdominal muscle contractions
- Avoids issues with percutaneous catheters
- Minimize breathing problems

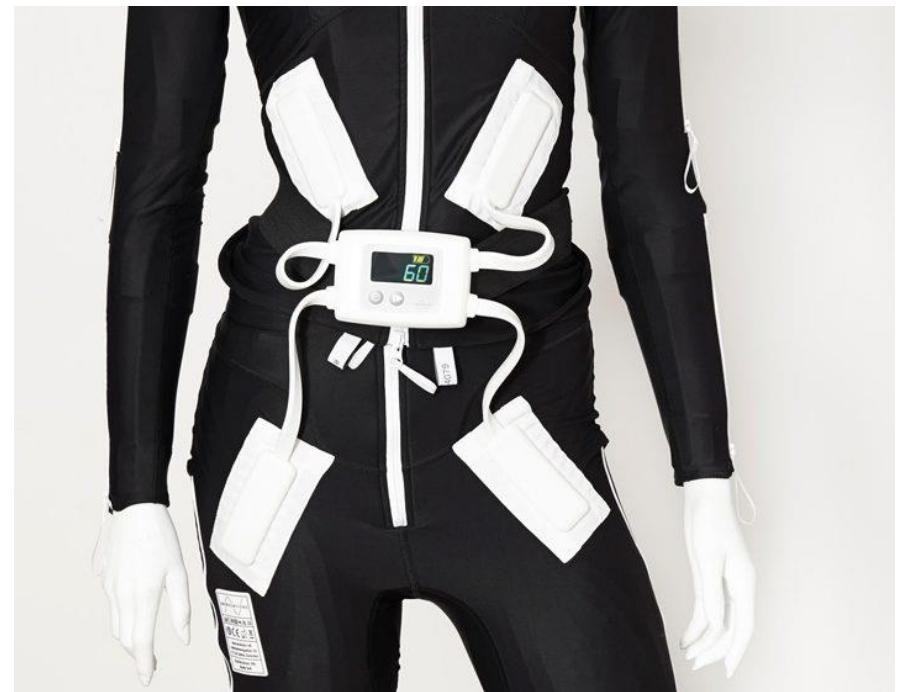
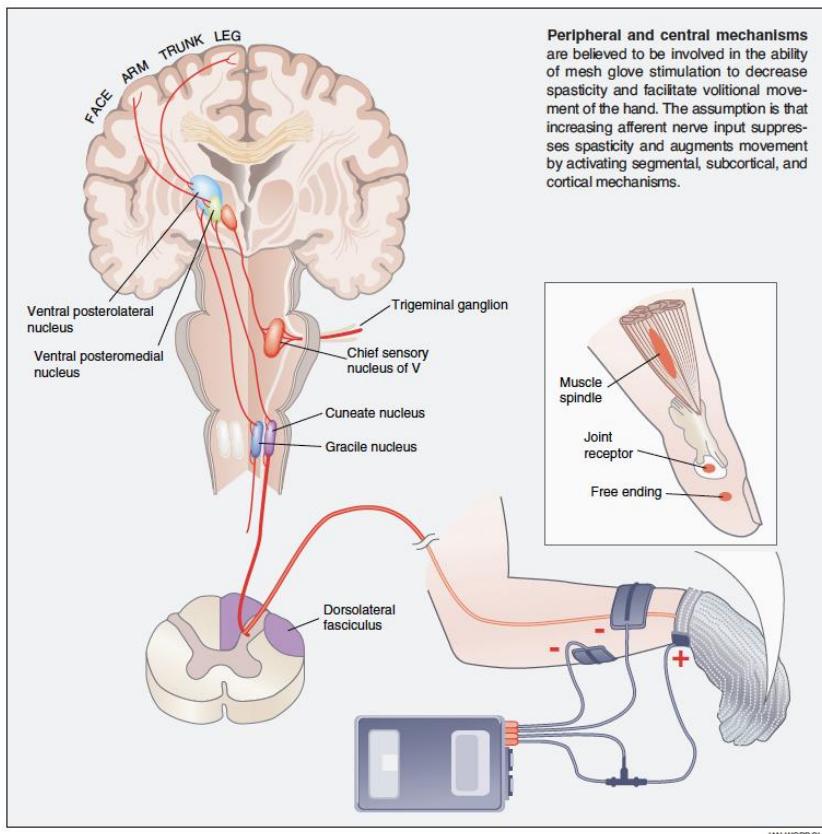




4-pole electrode
Pisces-Quad
3487A Medtronic
(T11/L1)
3625 Test
Stimulator or
implanted Itrel3
7425, Medtronic
2,1 – 120 Hz
0 – 12 V

Examples for available systems





EXOPULSE Mollii Suit
Stockholm, Sweden

Mesh Glove Electrical Stimulation

by M. Meta Dimitrijević, Nachum Soroker,
and Fabian E. Pollo

SCIENCE & MEDICINE

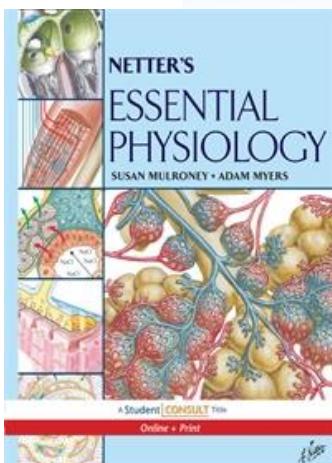
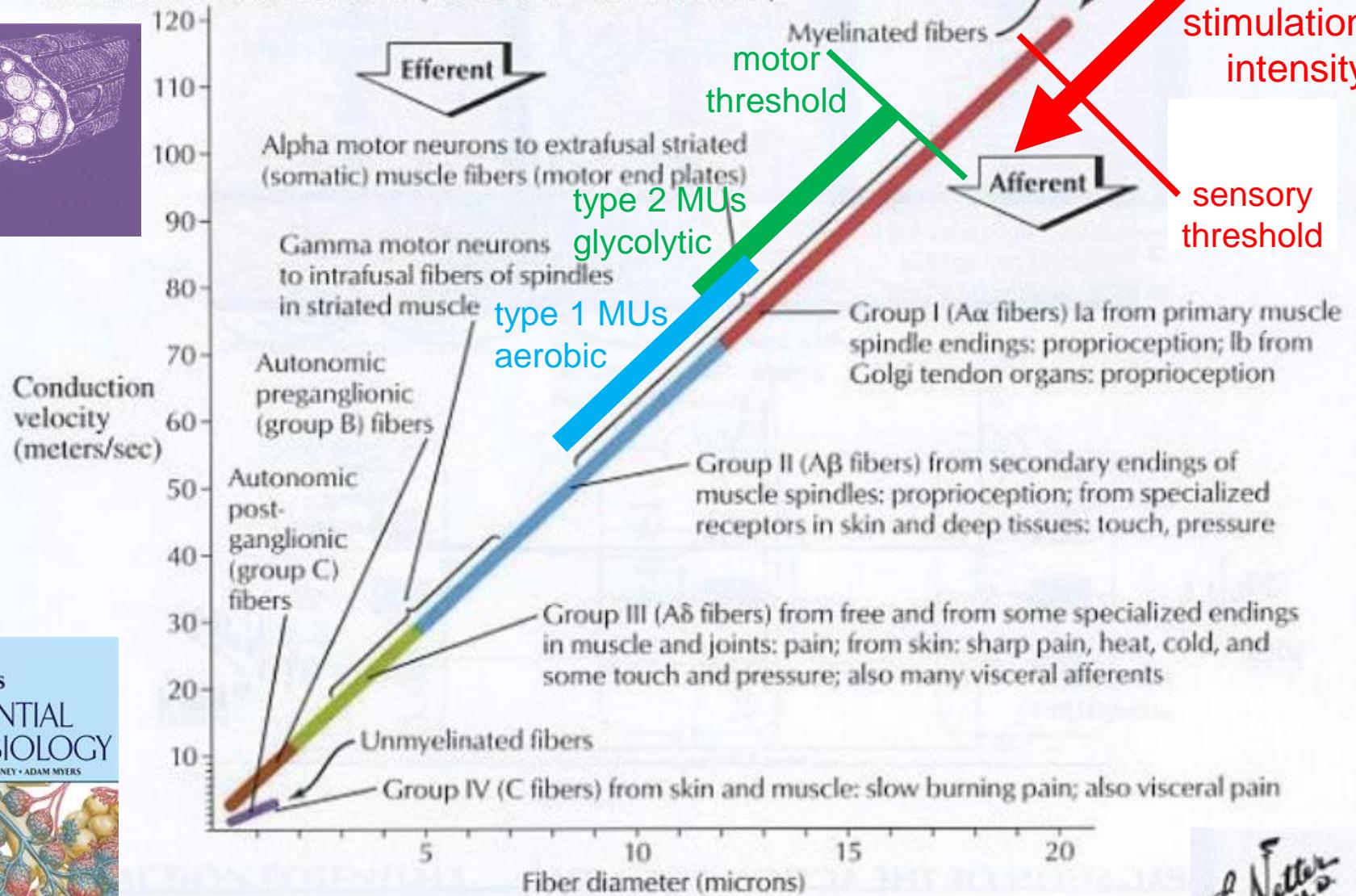
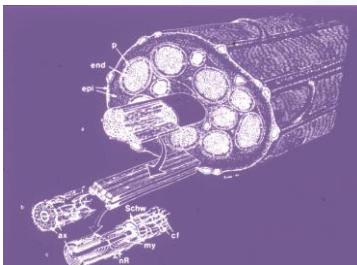
May/June 1996

 EXOPULSE

ottobock.

Efferent Neurons

C. Classification of nerve fibers by size and conduction velocity



SELECTIVITY

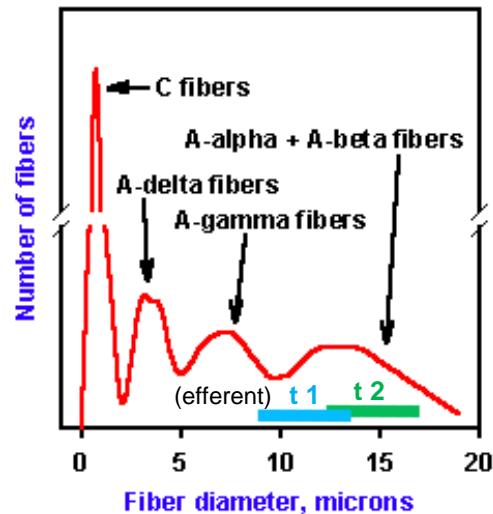
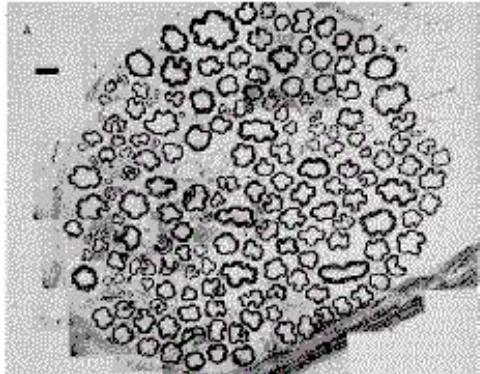
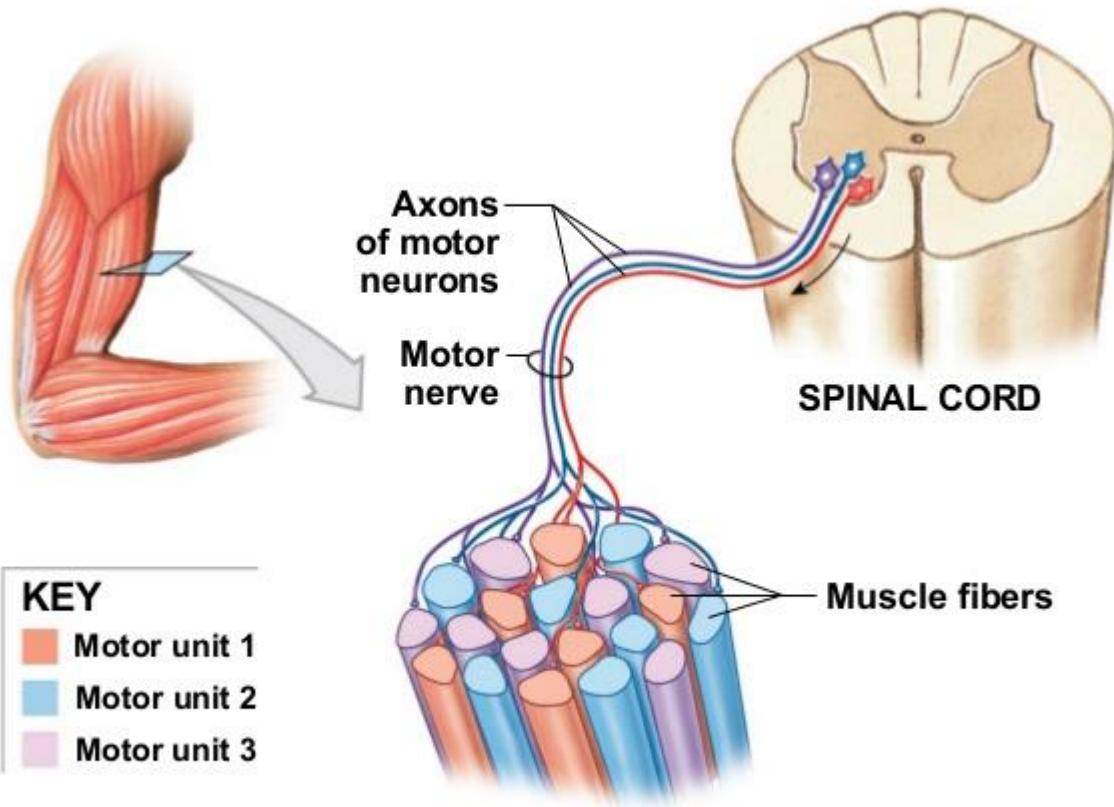


Fig. 5-13. Distribution of fibers within a peripheral nerve. Upper: A cross section of the posterior articular nerve of the cat showing fibers of different diameters. Calibration: 10 microns (Courtesy of F.J. Clark). Lower: A plot of the number of fibers of different diameters in a peripheral nerve. Note the predominance of fibers less than 2 microns in diameter.

Figure 9.12 The Arrangement of Motor Units in a Skeletal Muscle



© 2012 Pearson Education, Inc.

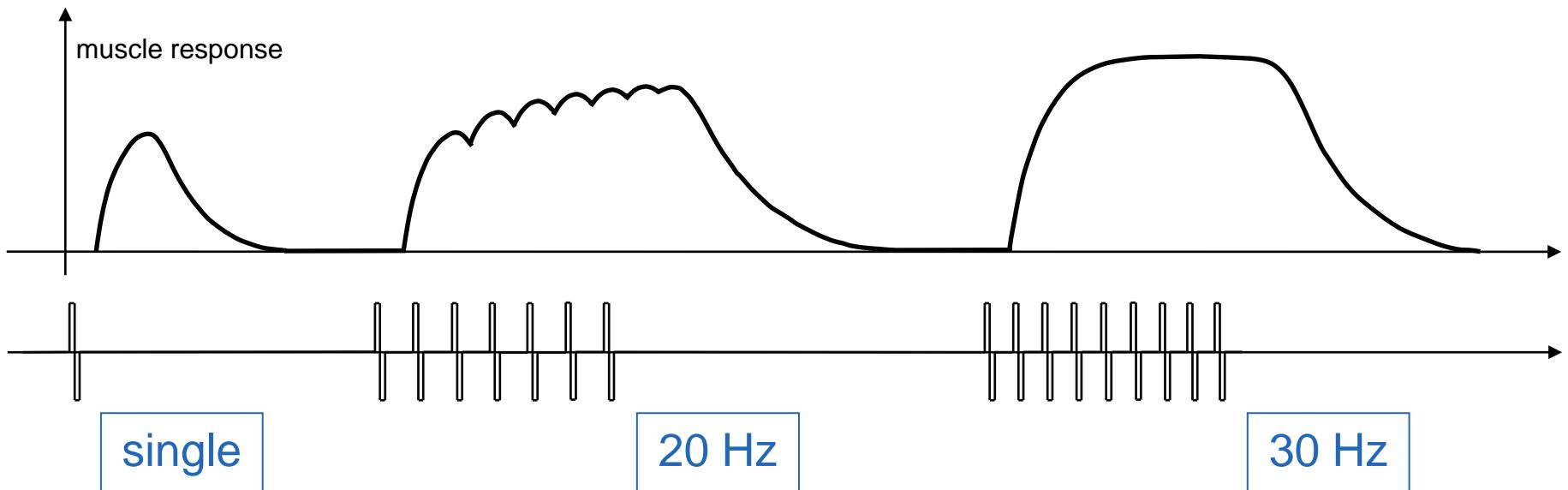
Michael D. Mann:
The Nervous System in Action
<http://michaeldmann.net>

MIXED NERVE, predominantly afferent

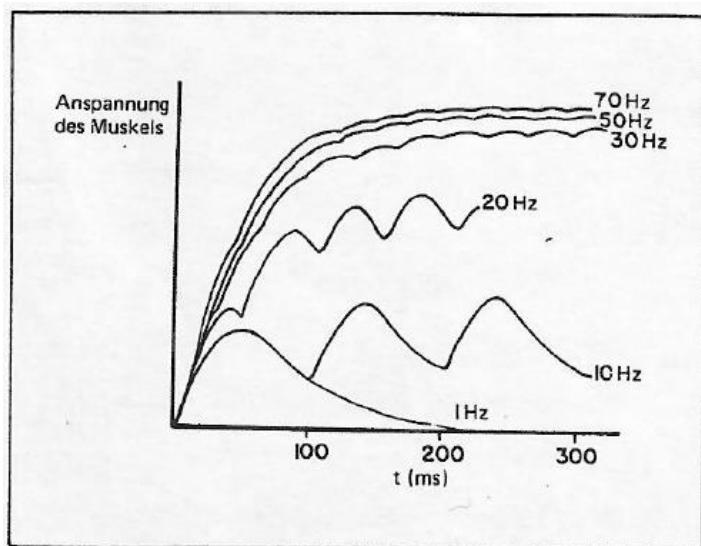
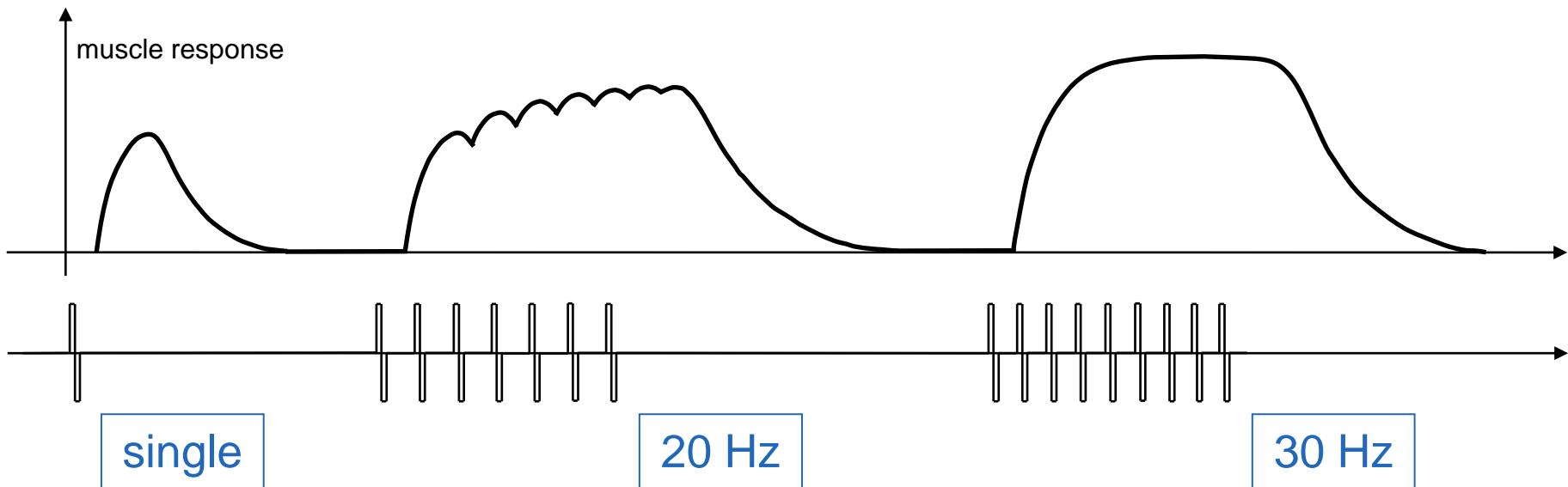
Glycolytic & aerobic motor units –
- mixed morphology in nerve and muscle

Control-, metabolic and biomechanical issues

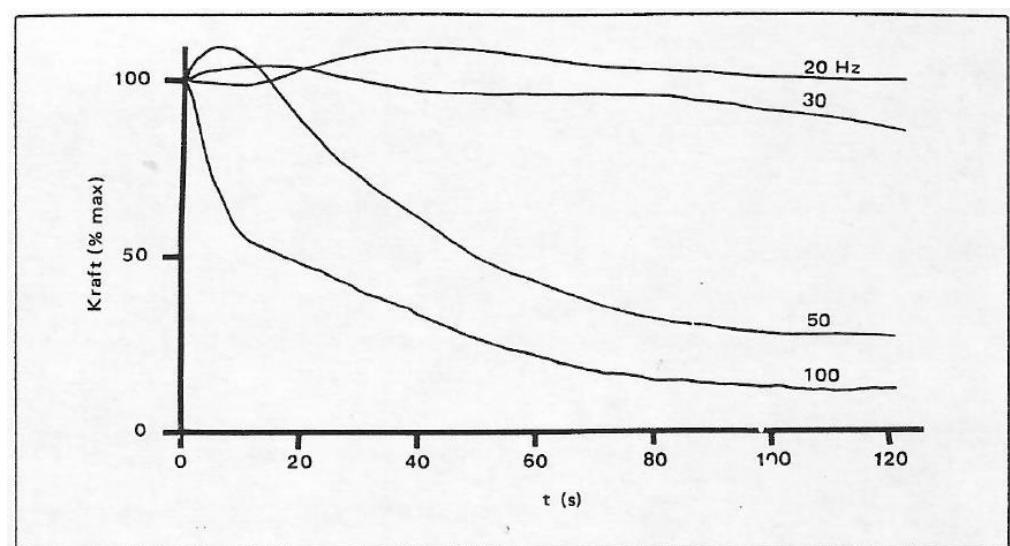
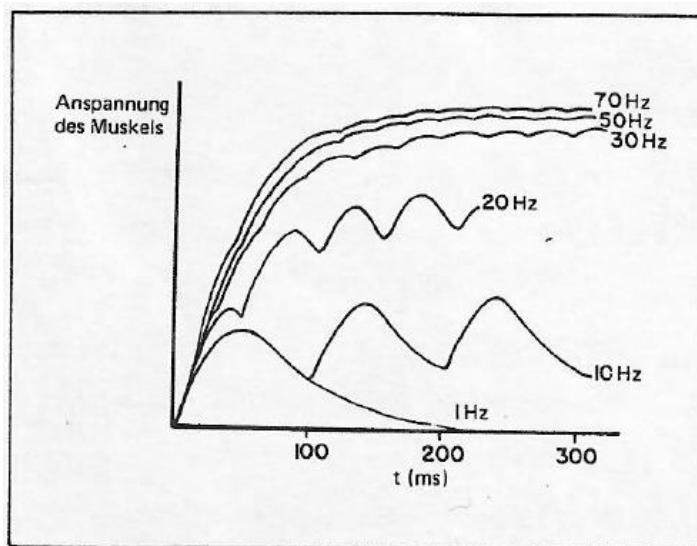
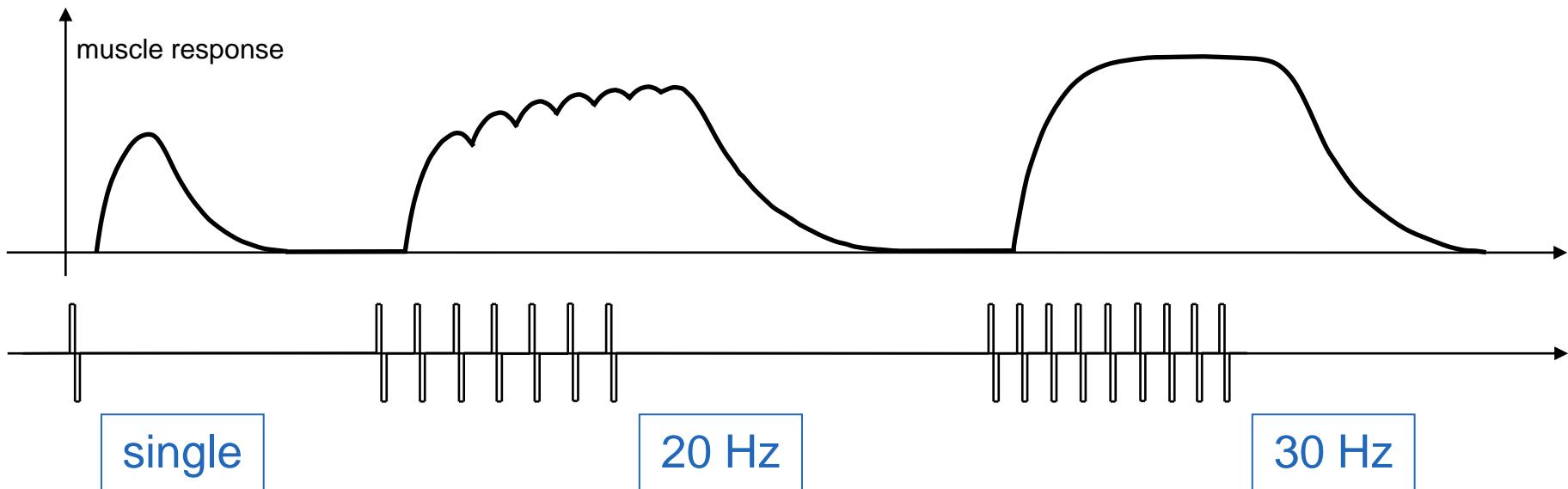
Frequency dependence of neuromuscular stimulation: contraction force development versus muscle fatigue



Frequency dependence of neuromuscular stimulation: contraction force development versus muscle fatigue

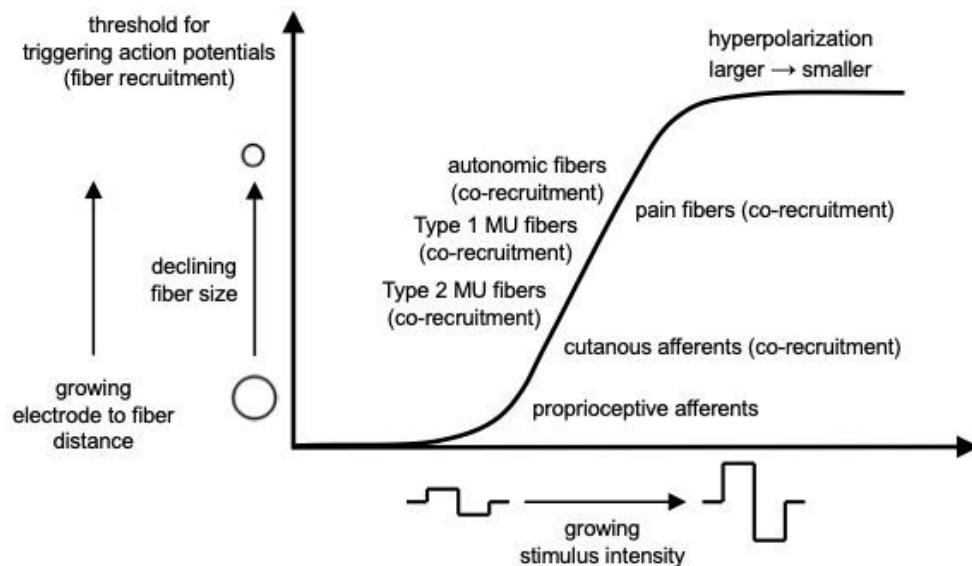


Frequency dependence of neuromuscular stimulation: contraction force development versus muscle fatigue



Summary

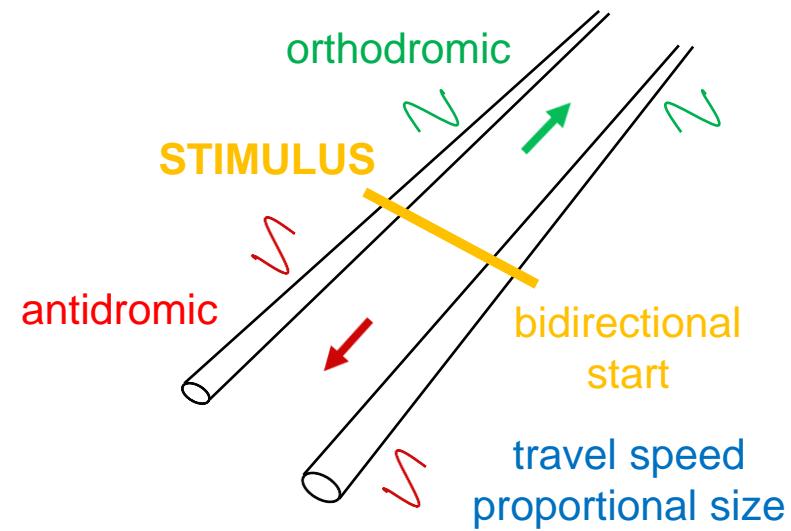
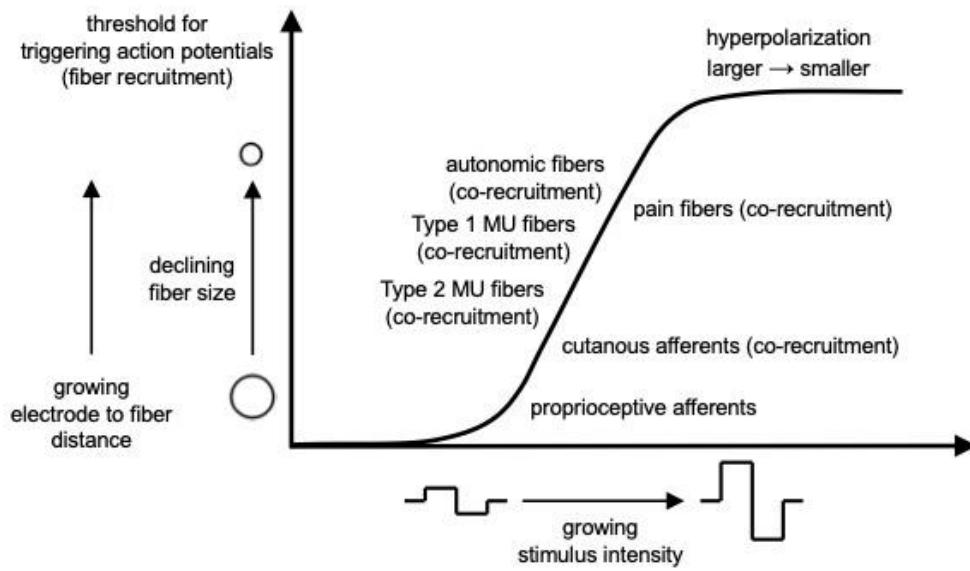
on interaction of stimuli with neuron pools



Stimulation interface – neuron activation

Size and distance dependent **recruitment** of fibers (in groups)

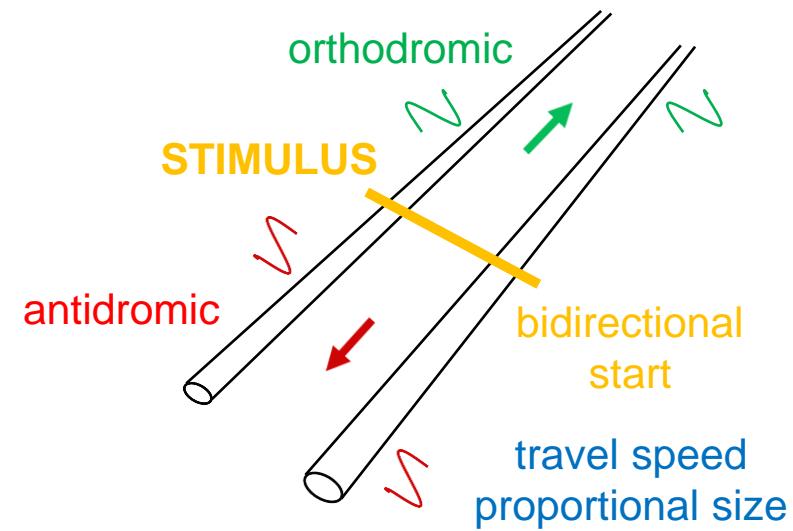
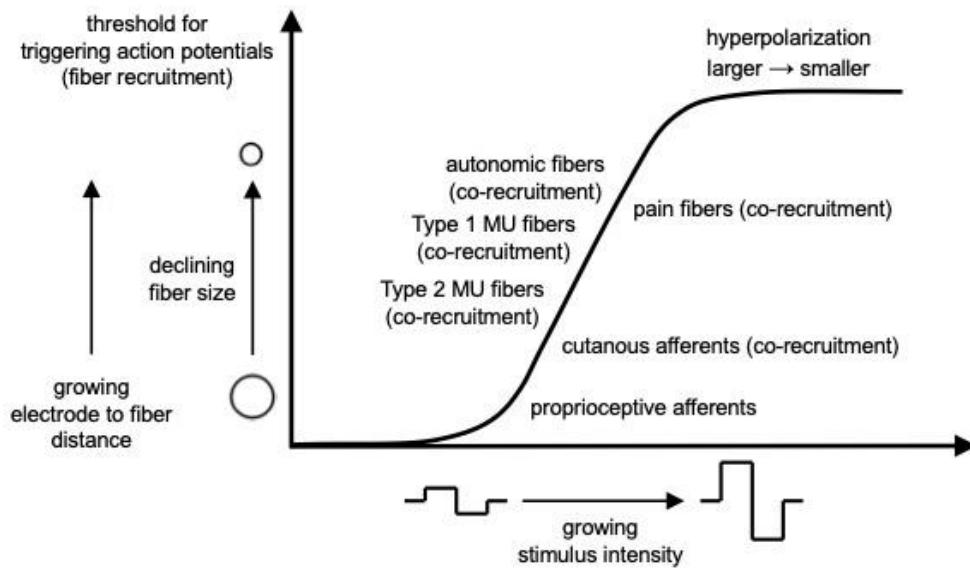
- Lowest threshold – large afferents
- Growing intensity co-recruits smaller fibers gradually



Stimulation interface – neuron activation

Size and distance dependent **recruitment** of fibers (in groups)

- Lowest threshold – large afferents
- Growing intensity co-recruits smaller fibers gradually
- Synchronous **start** – dispersion by distance and conduction velocity
 - bidirectional

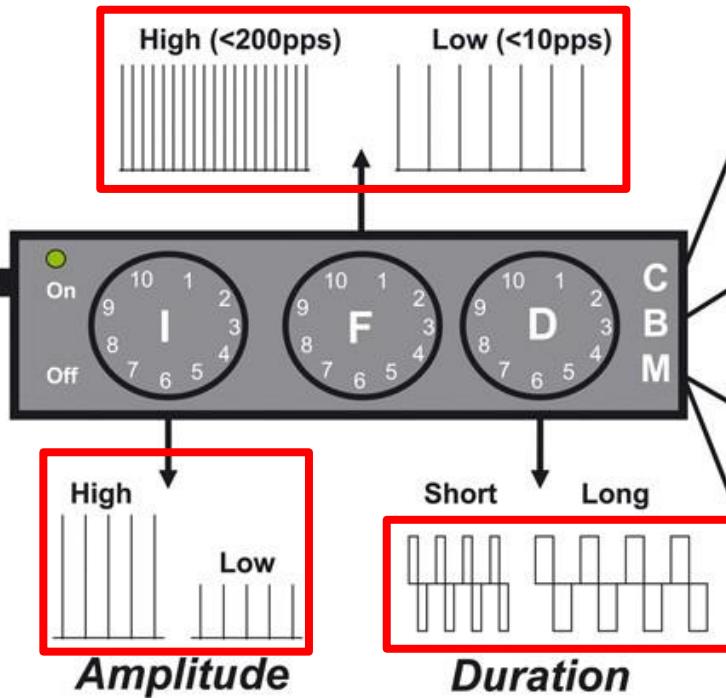


Stimulation interface – neuron activation

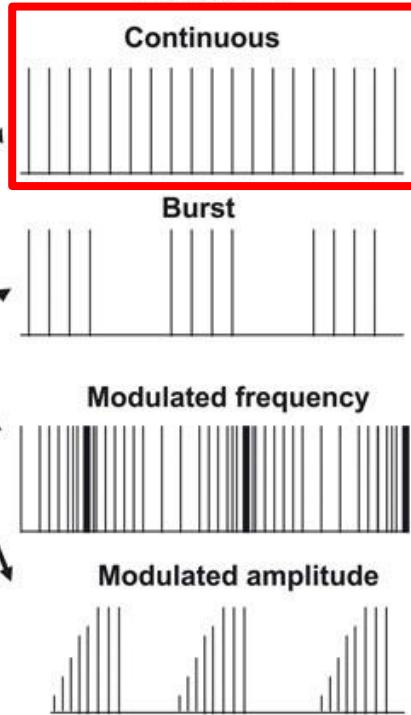
Size and distance dependent **recruitment** of fibers (in groups)

- Lowest threshold – large afferents
- Growing intensity co-recruits smaller fibers gradually
- Synchronous **start** – dispersion by distance and conduction velocity
 - bidirectional
- Beyond recruitment with intensity - **frequency** influences
 - central interneuron processing as afferent input
 - contraction properties in efferent neuromuscular activation

Frequency



Pattern



Examples for available systems

- AFFERENT NERVE STIMULATION:**
- Continuous biphasic pulses
 - 1 – 120 Hz,
 - 0,1-1ms per phase (100-1000µs)
 - Posterior roots: up to 120mA
 - Peripheral nerves: < 50 mA

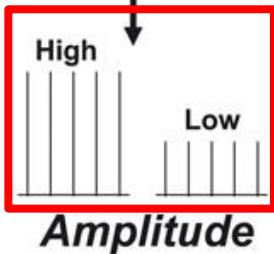
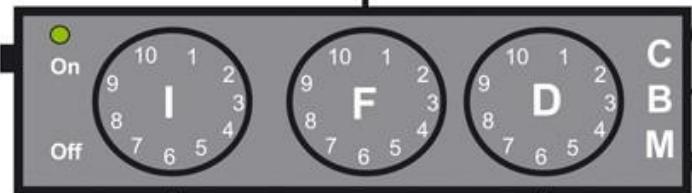
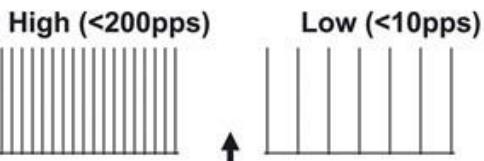
NEUROMUSCULAR STIMULATION:

- Phasic pattern, var. on-/off-time
- 10 – 50 Hz,
- 0,1-1ms per phase (100-1000µs)

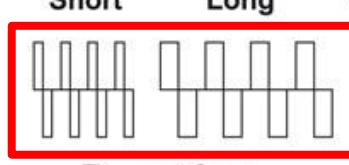


Essential device feature: resolution of amplitude adjustment finer than 0,5 mA !!!

Frequency



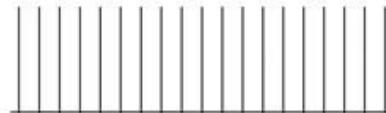
Amplitude



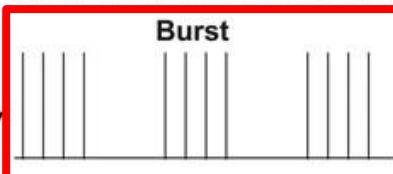
Duration

Pattern

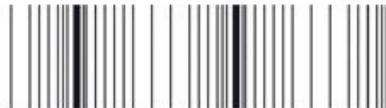
Continuous



Burst



Modulated frequency



Modulated amplitude

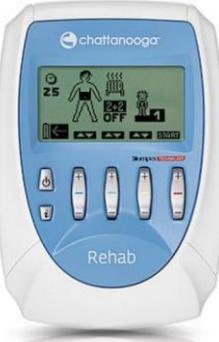


AFFERENT NERVE STIMULATION:

- Continuous biphasic pulses
- 1 – 120 Hz,
- 0,1-1ms per phase (100-1000µs)
- Posterior roots: up to 120mA
- Peripheral nerves: < 50 mA

NEUROMUSCULAR STIMULATION:

- Phasic pattern, var. on-/off-time
- 10 – 50 Hz,
- 0,1-1ms per phase (100-1000µs)



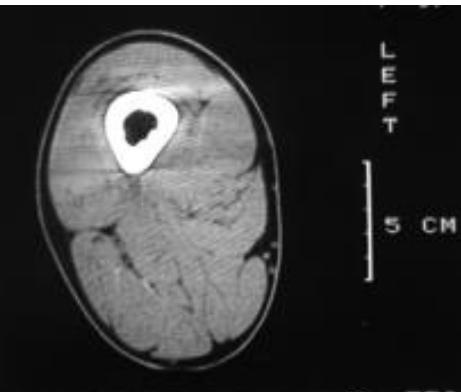
TAKING
ELECTROTHERAPY
A STEP FURTHER

Examples for available systems

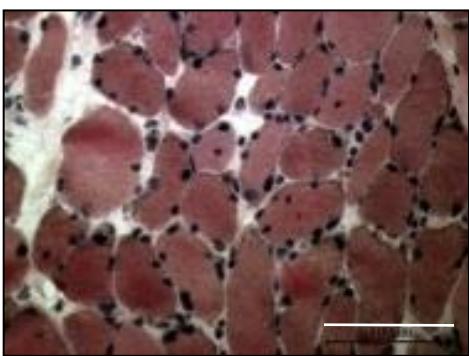
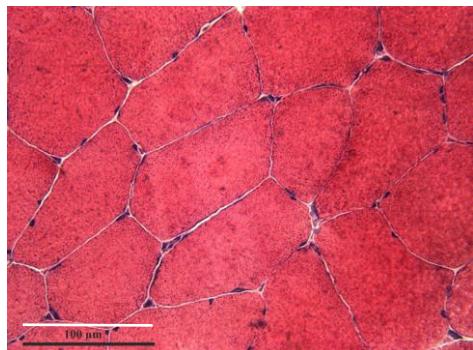
Muscle Stimulation

Consequences of muscle denervation

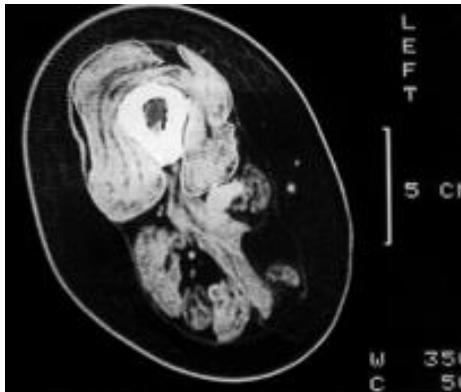
Healthy thigh



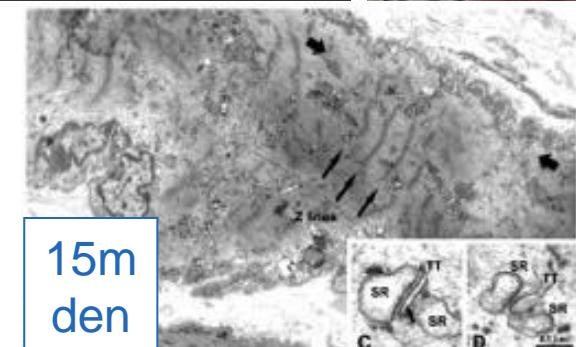
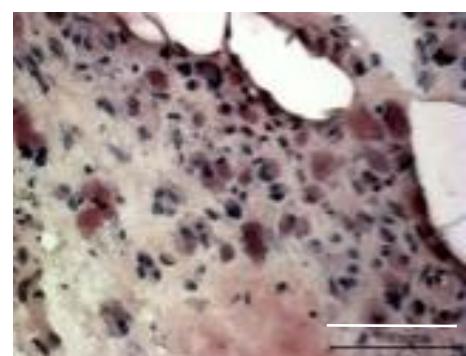
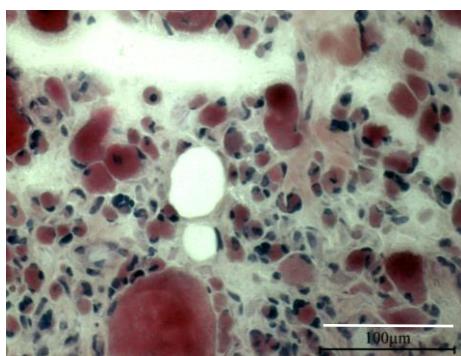
0,9y
den



4 years denervated



8,7 years denerv.



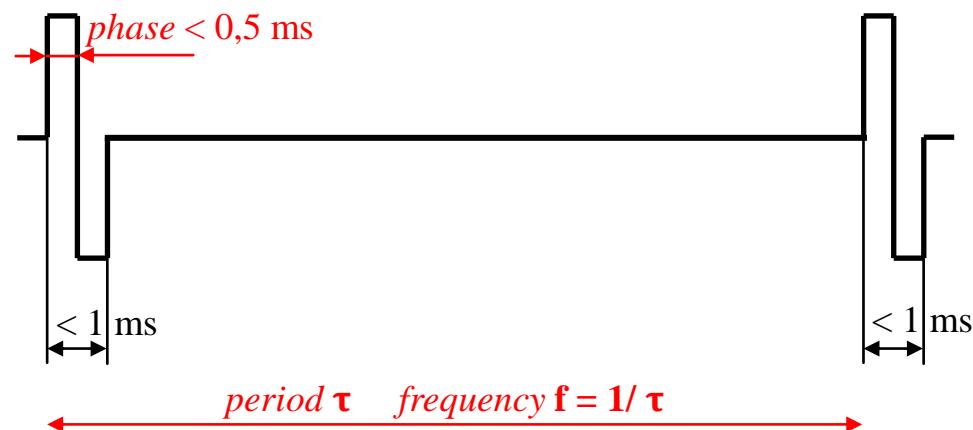
15m
den

MFCV_{max} vastus lat:
healthy 4,48 m/s
10mo den 2,40 m/s
30mo den 1,20 m/s

Stimulation parameter ranges

Nerve stimulation:

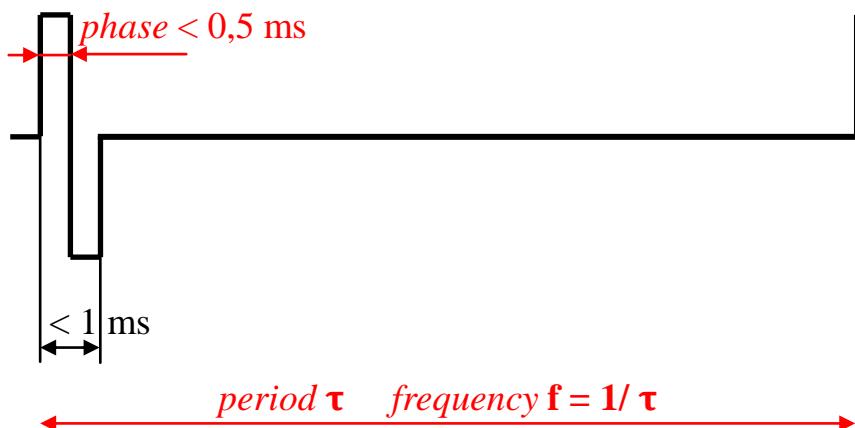
- Pulse width (biphasic)
typ. < 0.5ms per phase
- Frequency (fused contr.)
25 Hz
- Amplitude range (Surface)
 $\Rightarrow \pm 100V / \Rightarrow \pm 300mA$
- Amplitude range (Implant)
 $\Rightarrow \pm 10V / \Rightarrow \pm 30mA$



Stimulation parameter ranges

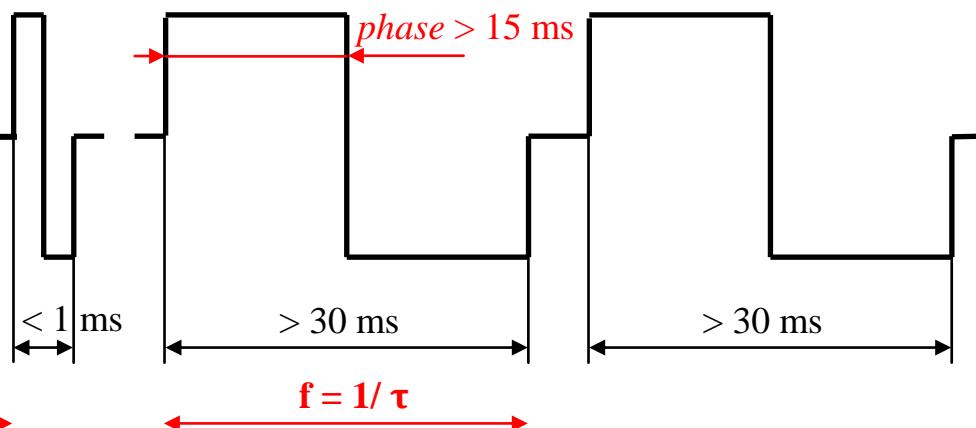
Nerve stimulation:

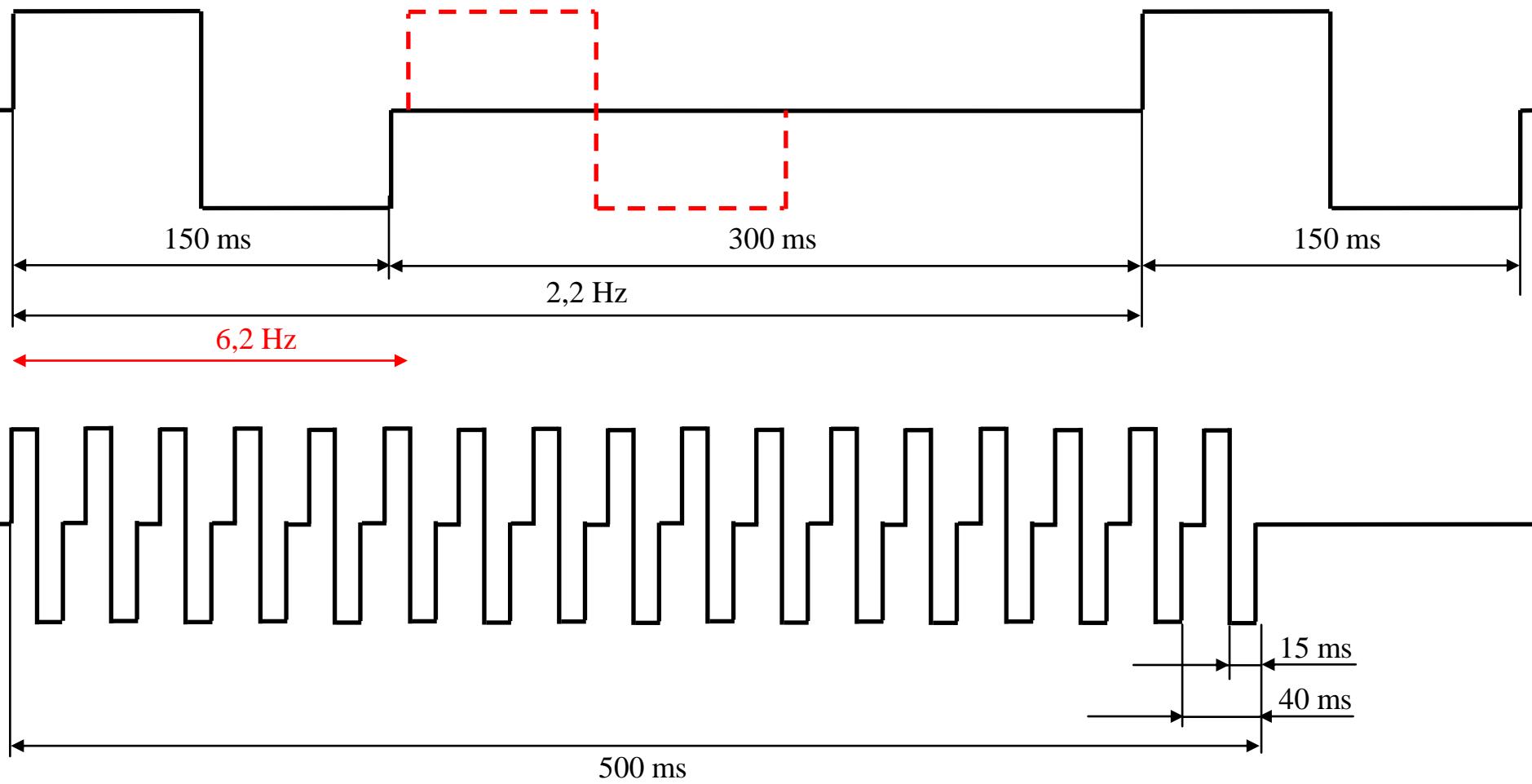
- Pulse width (biphasic)
typ. < 0.5ms per phase
- Frequency (fused contr.)
25 Hz
- Amplitude range (**Surface**)
 $\Rightarrow \pm 100V / \Rightarrow \pm 300mA$
- Amplitude range (**Implant**)
 $\Rightarrow \pm 10V / \Rightarrow \pm 30mA$



Muscle stimulation:

- Pulse width (biphasic)
typ. >15ms ($\Rightarrow 250ms$) per phase
- Frequency (fused contr.)
25 Hz
- Amplitude range (**Surface**)
 $\Rightarrow \pm 100V / \Rightarrow \pm 300mA$
- Amplitude range (**Implant**)
 $\Rightarrow \pm 10V / \Rightarrow \pm 30mA$



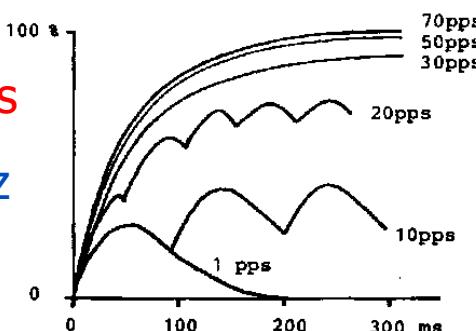


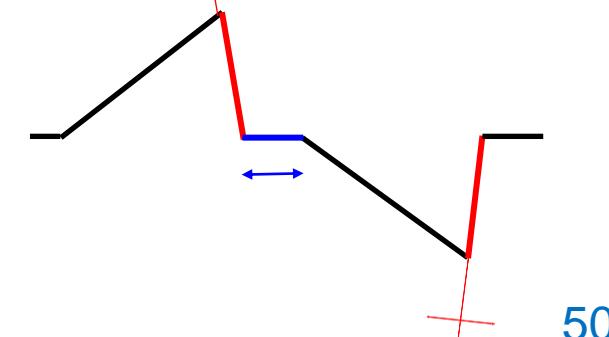
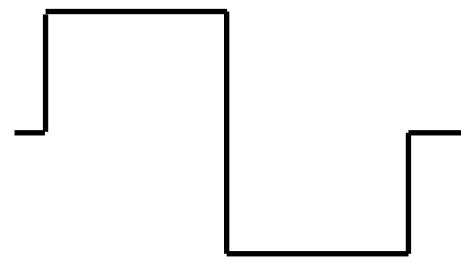
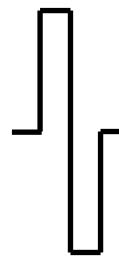
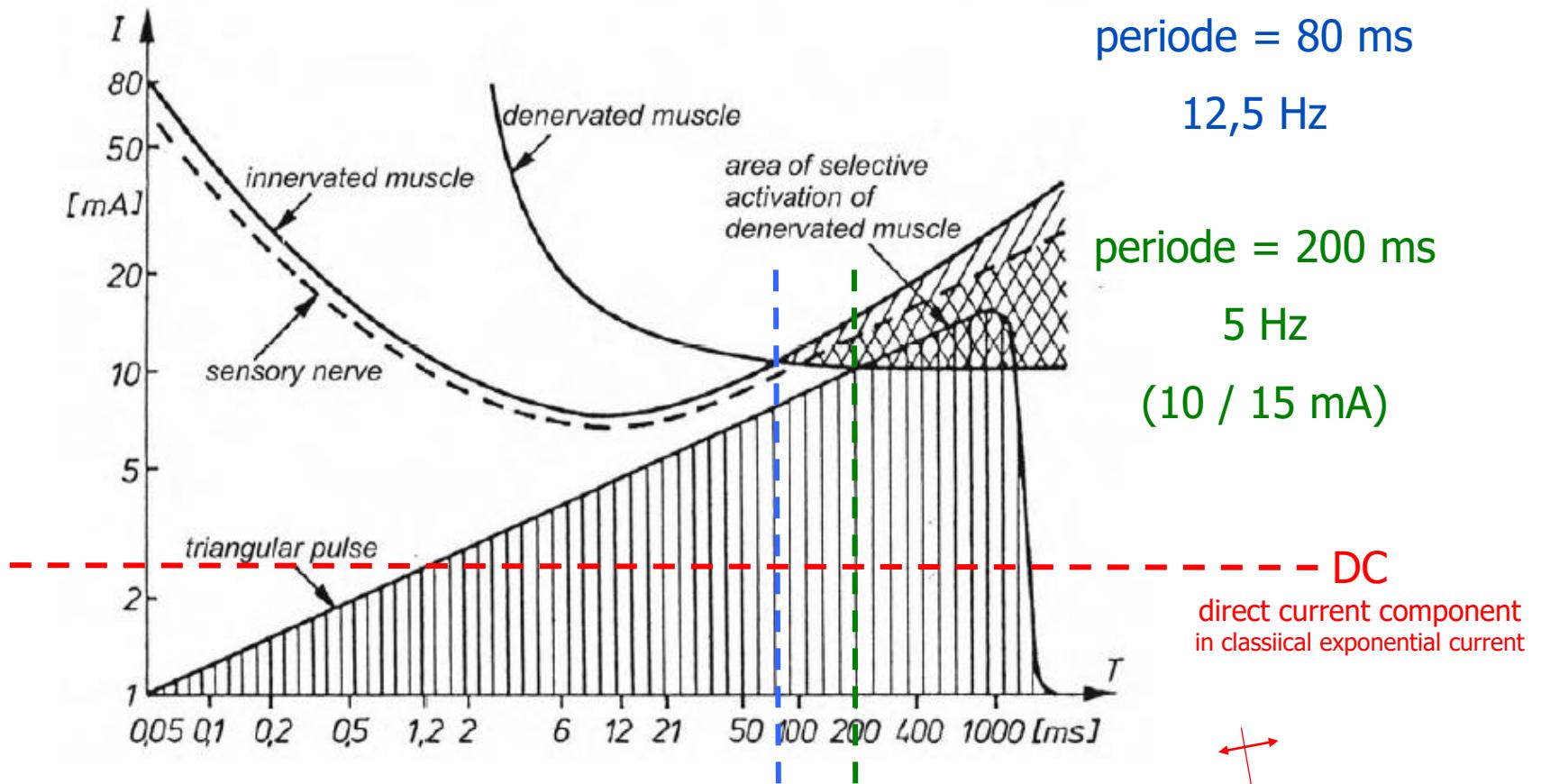
Excitability
conditioning

Period < 50 ms
> 20 Hz

Pulse phase > 15 ms
Period 40ms / 25 Hz

Single twitch \Rightarrow unfused tetanus \Rightarrow fused tetanus



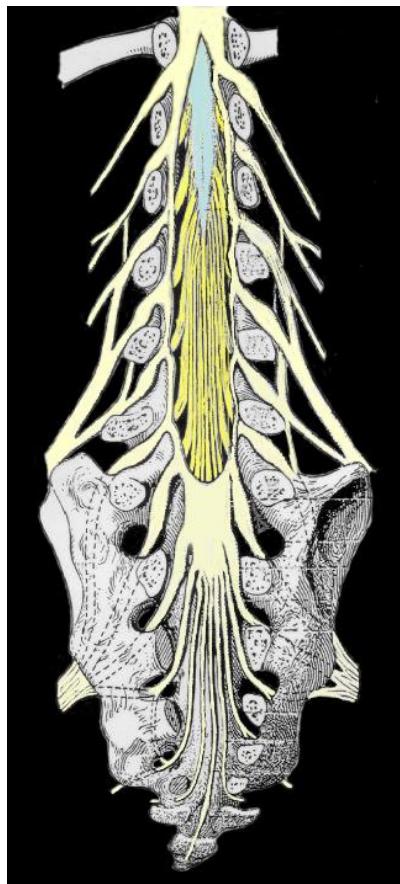


nerve stimulation

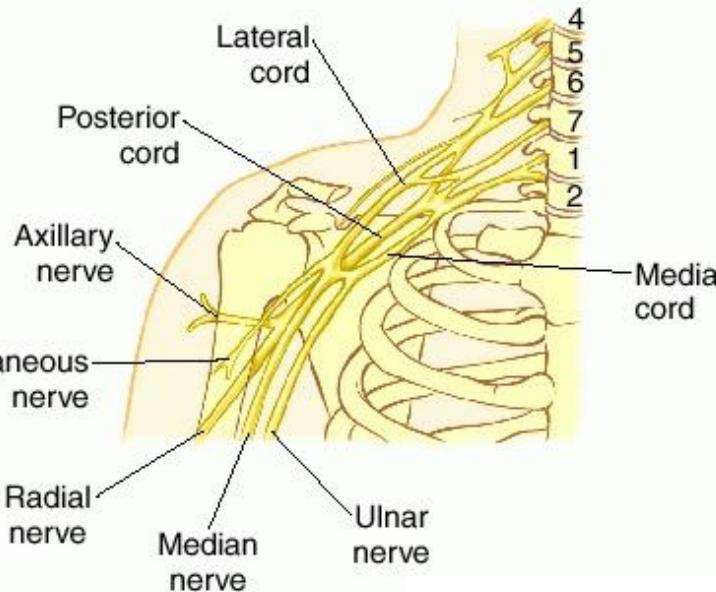
muscle stimulation

muscle stimulation,
reduced nerve stimulation

Temporary or chronic denervation



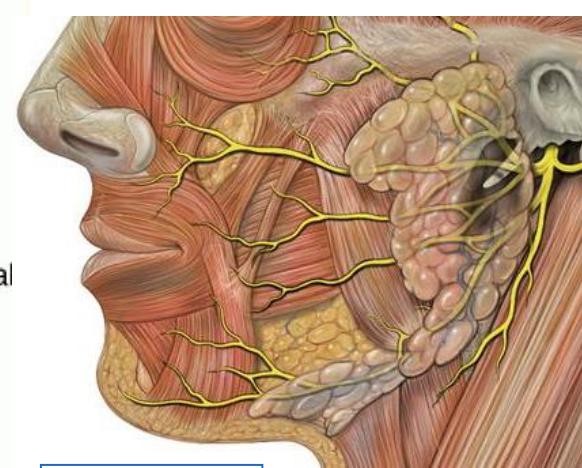
Plexus



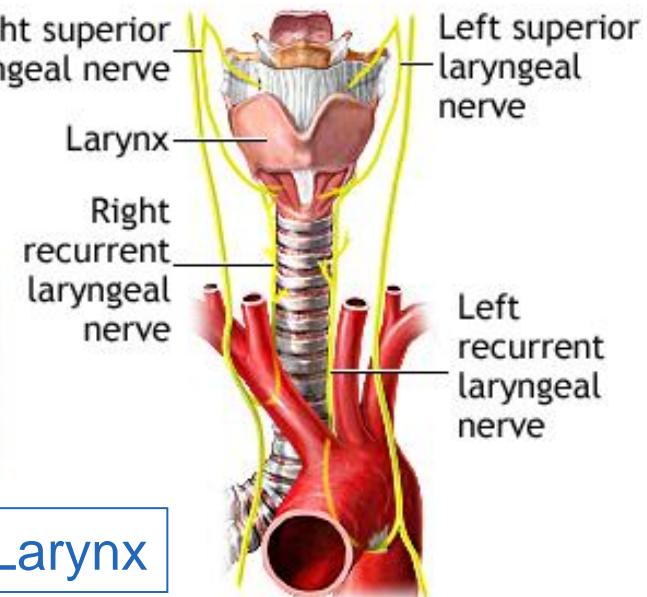
Cauda



Recovery support
Reconstructive surgery



Facialis

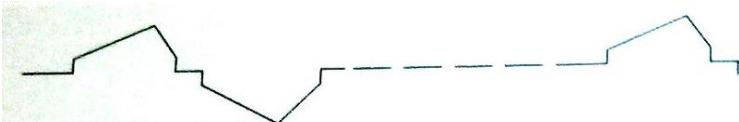
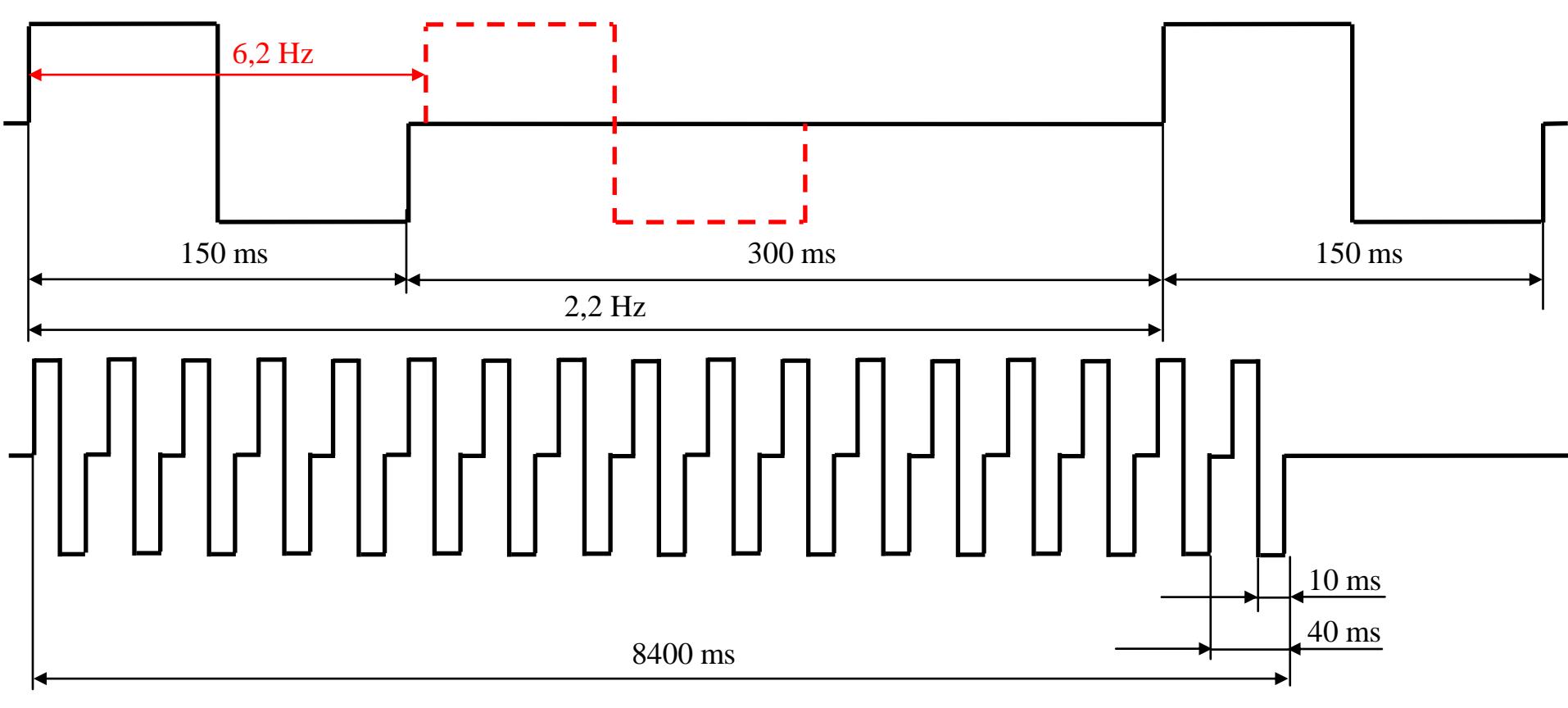


Larynx

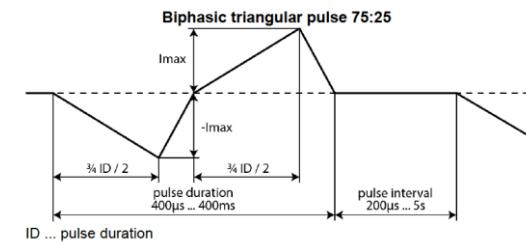
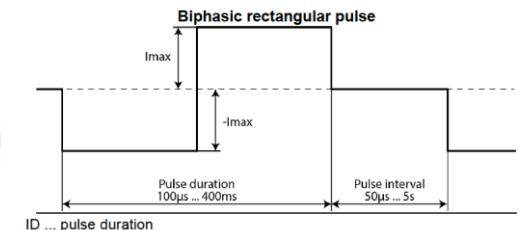
ADAM.

Electrodes





Examples for available systems





ASIA IMPAIRMENT SCALE

A – Complete: No motor or sensory function preserved in the sacral segments S4-S5.

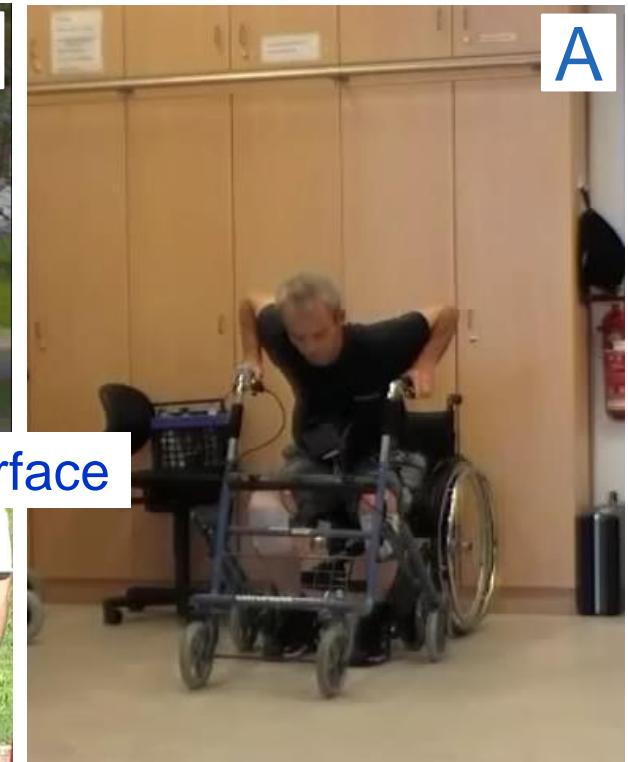
B – Incomplete: Sensory but not motor function preserved below neurological level and includes the sacral segments S4-S5.

C – Incomplete: Motor function preserved below neurological level, and more than half of key muscles below the neurological level have muscle grade below 3.

D – Incomplete: Motor function preserved below neurological level, and more than half of key muscles below the neurological level have muscle grade of 3 or more.

E – Normal: Motor and sensory function normal

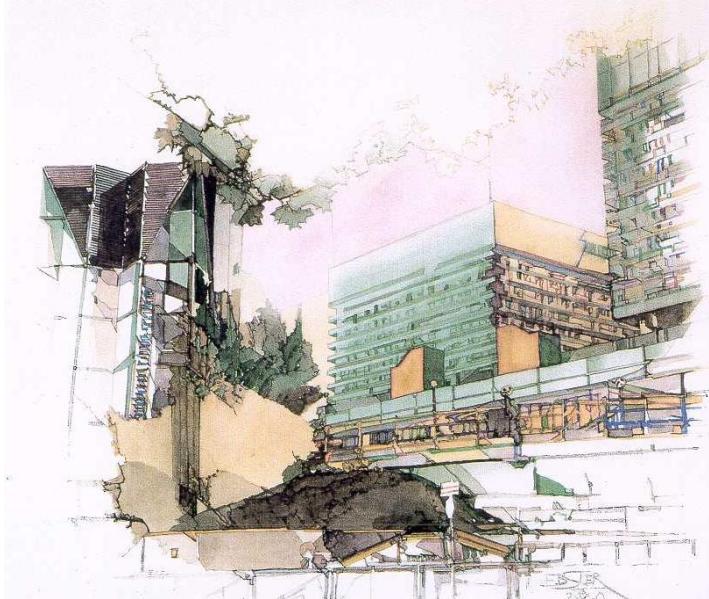
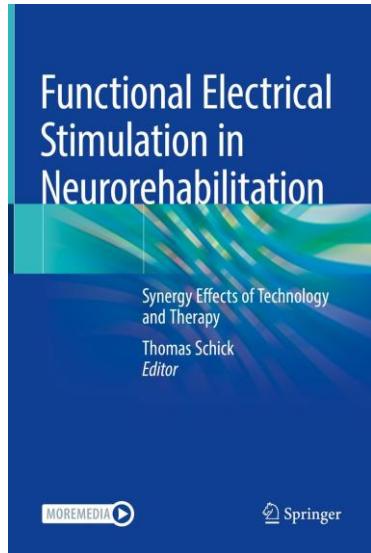
implant



surface

Paraplegia

Role of Technical Tools and Electrical Parameters in Functional Electrical Stimulation



<https://link.springer.com/book/10.1007/978-3-030-90123-3>

Chapters:

- *Role of Electrical Parameters in Functional Electrical Stimulation*
- *Absolute and Relative Contraindications*

winfried.mayr@meduniwien.ac.at

https://www.meduniwien.ac.at/web/index.php?id=688&res_id=235&name=Winfried_Mayr

55