

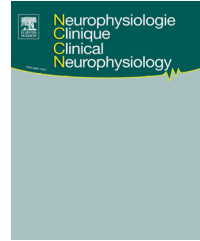


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## COMPREHENSIVE REVIEW

# The sensory role of the sole of the foot: Review and update on clinical perspectives



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**Summary** The feet constitute an important sensory structure in the mechanisms of postural control. As a direct and often only interface between the body and the ground, the feet allow us to sense and interact with our environment. Sensory information provided by muscle and cutaneous afferents in the foot contribute to our ability to stand upright, and postural sway is necessary to detect both position and motion of the body in space. A decline in foot sole skin sensitivity occurs naturally with aging and as a result of neurological disorders, including different peripheral neuropathies, the commonest etiologies of which are diabetes mellitus or effects of chemotherapy. This decline in sensitivity is frequently associated with poorer postural control and increased risk of falls in these populations. The purpose of this comprehensive review is to summarize the evidence that supports a functional role of foot sole sensory tactile and muscular feedback in standing balance, and the postural consequences when this feedback is impaired with aging or disease. This brings new clinical perspectives on the development of intervention strategies to improve the quality of foot sole cutaneous feedback. It also seems to be a promising approach in the management of patients with balance disorders, with specific chronic pain syndromes, with neurologic diseases or those at risk of falling.

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## Introduction

Human postural control is a complex process involving sensory inputs from visual, vestibular, proprioceptors and tactile receptors. It may be defined as the act of achieving, maintaining or restoring a state of balance during any

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posture or activity [132], and depends on a combination of both passive and active mechanical controls [191]. Passive control refers to the stiffness and kinematic proprieties of the joints, as well as the effect exerted on them by gravity. Active control is characterized by neural regulation of skeletal muscles responsible for sway detection and postural correction [9,140]. Postural instability seems to require a high hierarchical level of posture control and activation of different brain areas [144]. A facilitatory effect of postural instability on corticospinal pathways has been observed [154] and could depend on the existing level of background motor activity [81]. In addition, sensory transmission facilitation may occur depending on the motor task [14,109], and could play a critical role for feedforward mechanisms [109]. Automatic processes including sensory interaction (i.e., proprioceptive and tactile) and cutaneous reflexes contribute to control of posture [64,166]. Unavailable or disrupted signals from one or more sensors may result in a decrease in postural stability. When balance is disturbed, a postural adjustment by a series of cutaneous postural reflexes can be initiated by cutaneous mechanoreceptors [12,93,119].

It is clear that the feet constitute an important sensory structure in the mechanisms of postural control. As a direct and often unique interface between the body and the ground [63], the feet allow us to sense and interact with our environment. This ability results from the coordination between the motor system, which controls muscular activity and pressure exerted by the feet, and the somatosensory afferent system. Somatosensory feedback arises from a variety of sources, most notably the cutaneous mechanoreceptors in the skin, and muscle spindle endings found within most skeletal muscles that together provide tactile and proprioceptive feedback. Plantar cutaneous afferents transmit spatial and temporal feedback concerning the pressure variations and skin stretch exerted on the soles of the feet [58,63,179]. In response to this sensory feedback, corrective postural reactions are evoked by postural muscles [148,176,177]. The feet thus contribute to the upright stance in response to gravitational and ground reaction forces. The purpose of this comprehensive review is to summarize the evidence that supports a functional role of foot sole sensory tactile and muscular feedback in standing balance and the postural consequence when this feedback is impaired with aging or disease. Decline in foot sole skin sensitivity occurs naturally with aging [127,129] and as a result of neurological disorders, including different peripheral neuropathies (PN) [129,133,178]. This decline in sensitivity is associated with poorer postural control [94,153] and increased risk of falls in these populations [69,80,133,178]. Although PN may result from different etiologies such as traumatic injuries, infections, inflammatory and dysimmune processes, metabolic problems, inherited causes and exposure to toxins, PN related to diabetes mellitus and to chemotherapy are the most prevalent; as such, they will be particularly detailed later in this paper. The purpose of this review is first to describe the important relationship between the foot sole as a sensory structure and balance maintenance; secondly, to show how this sensory structure may be altered by aging or diseases. This review mostly concerns the peripheral processes of the foot sensory system, by highlighting the role of cutaneous and muscle receptors of the foot. neural mechanisms involved in the

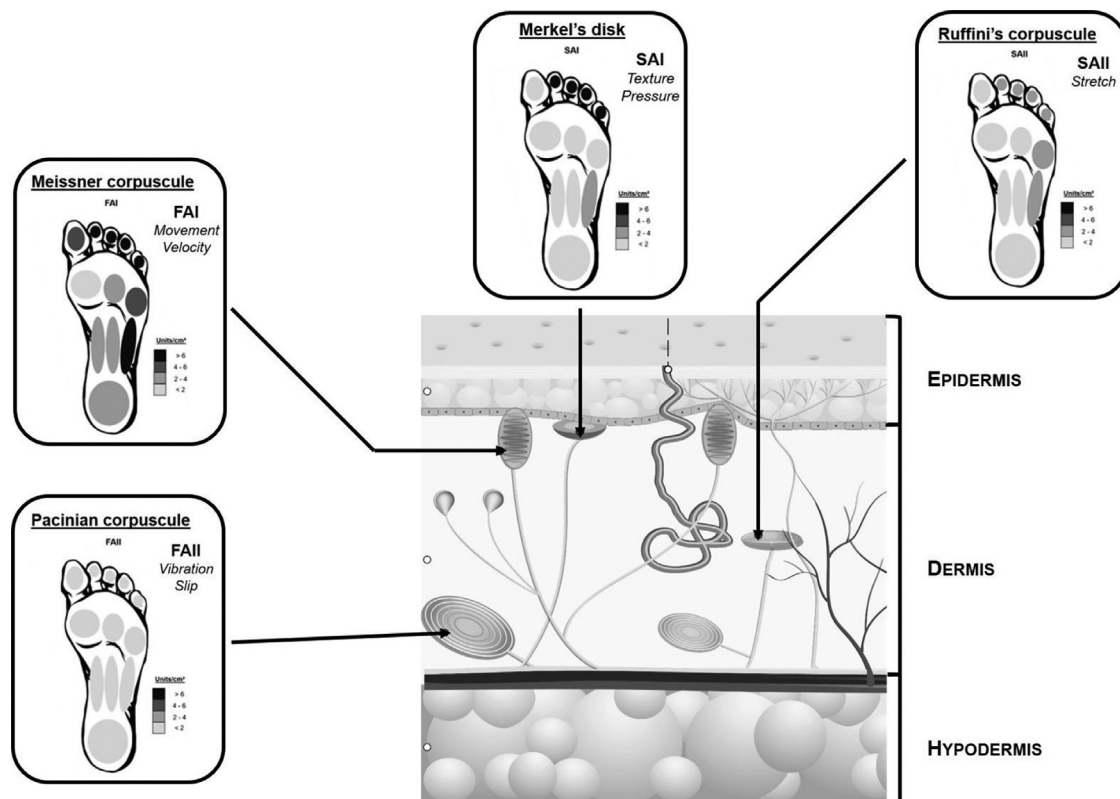
sensory processes to maintain balance are not described here. For additional reviews on cutaneous and muscle spindle feedback the author recommends the following works: Strzalkowski et al., [164], Proske and Gandevia [137] and Macefield and Knellwolf [89]. This review aims to provide scientific support for new clinical perspectives concerning the foot sole as a sensory structure and emphasizes how several intervention programs aimed at stimulating the foot sole can improve standing balance.

## The foot sole as a sensory structure

Sensory information provided by muscle and cutaneous afferents in the foot [87] contribute to our ability to stand upright. The intrinsic muscles of the foot and the glabrous skin of the sole are supplied by the tibial nerve. The tibial nerve is a mixed nerve that extends from the arcade of the soleus muscle to the calcaneal canal as it travels along the posteromedial aspect of the ankle. Distally, it bifurcates into the lateral plantar nerve and medial plantar nerve which supply the majority of the cutaneous innervation of the plantar surface of the foot. Tibial nerve efferents also provide extensive motor innervation for the foot. This innervation contributes to movement of all toes, excluding extension, as well as assisting with maintenance of the longitudinal arches of the foot [73].

## Muscular afferents

Muscle spindles are mechanosensory endings found within skeletal muscles. They are sensitive to muscle stretch as well as the rate of stretch and encode joint angular position and the velocity of movement [137]. Primary spindle fibers convey feedback about the velocity of muscle length changes using large diameter type Ia sensory neurons, whereas secondary fibers provide information about static muscle length using smaller type II neurons [89]. By providing proprioceptive feedback of muscle length, muscle spindles located in the intrinsic muscles of the foot contribute to control of upright stance [89]. The role of the medial arch has been suggested to be important for maintaining posture when performing standing balance [66]. EMG responses in tibialis anterior and gastrocnemius have been reported during manipulations of the digits and metatarsals, arguing that sensory input from the foot can trigger responses in muscles acting about the ankle [192]. This could relate to the function of the intrinsic muscles as toe-flexors [42], and muscle spindles within these muscles would be able to report the position of the body over the base of support. The majority of these spindle afferents are silent in the natural resting position [73] but during standing, spindles display a tonic discharge and respond to transient perturbations in position [73,150]. Recruitment of sensory afferents is a specific coding mechanism within the somatosensory nervous system; increase in the number of active muscle spindle endings seems to constitute an important source of sensory feedback from the foot [73]. In this context, muscle spindles in the intrinsic foot muscles provide useful proprioceptive feedback that play a role in the control of natural upright stance [74].

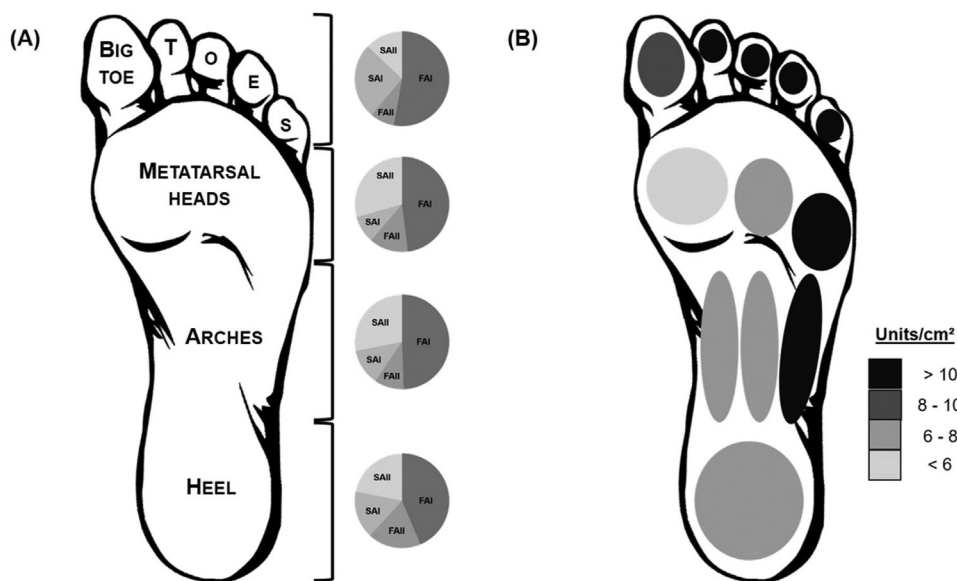


**Figure 1** Organisation of cutaneous mechanoreceptors from the foot sole (Adapted with permission from Strzalkowski et al., 2018). Four classes of cutaneous mechanoreceptors are distributed in the depths of the glabrous skin of the foot sole. They inform the central nervous system via large diameter A $\beta$  myelinated afferents. Representation of proximal-distal gradient and medial-lateral gradient in innervation density (Units/cm<sup>2</sup>), of each afferent type across the foot. Greater innervation density are in Black and lower innervation density are in Light grey. FAI, fast-adapting type I; FAII, fast-adapting type II; SAI, Slowly adapting type I; SAII, Slowly adapting type II.

### Cutaneous afferents

Cutaneous sensitivity characterizes a set of perceived sensations following tactile stimuli such as pressure, stretch, or vibration experience by the skin [58,62,63,180]. Specialized foot sole cutaneous mechanoreceptors [2,27,67,85], transduce these mechanical forces to the central nervous system (CNS) in the form of action potentials. The quality of this feedback depends on the biomechanical properties of the mechanoreceptors and tissue in which they reside. In the context of standing balance, tactile information arises from foot sole skin deformations induced by contact between the foot and the ground. The combination of cutaneous mechanoreceptors and sensory afferents constitute the fundamental functional unit for the transduction and transmission of tactile information to the CNS. The development of microneurography has allowed detailed analyses of the different mechanoreceptive afferents from the skin and muscles [73,88]. From a morphological point of view, cutaneous receptors consist of free or encapsulated nerve endings of first-order sensory neurons [98]. There are four subtypes of cutaneous mechanoreceptors (Fig. 1). Ruffini endings and Merkel discs maintain their firing for a longer duration during indentation; their afferents are classified as slowly adapting (SA). In contrast, Pacinian corpuscles and Meissner's corpuscles rapidly discontinue firing

after the initial contact, and their afferents are classified as fast adapting (FA) [75,88,98]. Cutaneous afferents are further subdivided by receptive field characteristics. Type I afferents have small receptive fields with well demarcated borders. Type II afferents have large receptive fields with diffuse borders [67,139,179]. Afferents innervating Merkel discs and Meissner's corpuscles are classified as Type I, while afferents innervating Ruffini endings and Pacinian corpuscles are classified as Type II. Merkel discs (SA I) and Meissner's corpuscles (FA I) are the most superficial and are located at the level of the dermal-epidermal junction, while Pacinian corpuscles (FA II) and Ruffini endings (SA II) are located deeper within the skin [55,61] (Fig. 1). Each class of cutaneous afferent is sensitive and responds to specific mechanical deformations of the skin [161,163]. When vibration, pressure or stretch is applied to the skin, the skin receptors produce a generating potential by ion channel opening and membrane depolarization. If the generating potential reaches the excitation threshold, it triggers one or more action potentials or impulses that then propagate along the axon to the CNS [147]. FA afferents provide information about changes in the pressure distribution exerted on the foot skin [63]. FA type I afferents generally provide information about shear forces tangential to the skin or information about normal contact to the skin. They can also be activated by joint movements that induce skin stretch



**Figure 2** Distribution and Innervation density estimate of cutaneous afferents across the foot sole (Adapted with permission from Strzalkowski et al., 2018). According to Strzalkowski et al. [164], the distribution of foot sole cutaneous afferents increases from the heel to the toes, and from the medial to lateral aspects, driven primarily by type FAI afferents. (A) Pie chart illustrates the percentage distribution of each afferent type at the toes, metatarsal heads, arches, and heel. (B) Representation of proximal-distal gradient and medial-lateral gradient in innervation density, with greater innervation density (black) in the toes and in the lateral region, and lower innervation (Light grey) in the heel and in the medial region, FAI, fast-adapting type I; FAII, fast-adapting type II; SAI, Slowly adapting type I; SAIL, Slowly adapting type II.

or compression when their receptive field is situated close to that joint [37,38] and FA type II afferents predominantly code skin stretch over compression [3,4]. Stretch and compression of skin seems to be important for kinesthesia [85]. Since FA receptors are sensitive to dynamic deformation of the skin [60], they are thought to play a dynamic role in balance control and stability. By providing spatial information about the pressure distribution between the feet and the ground [62,116,126], SA afferents are therefore particularly sensitive to static mechanical pressure stimuli [54,61]. They are thought to provide a tonic response in relation to the position of the body over the feet. However, they also provide dynamic cues.

### Foot sole innervation characteristics

Recently, Strzalkowski et al. [164] combined published [41,67,85,161] and unpublished microneurography tibial nerve recordings to investigate cutaneous afferent firing threshold and distribution across the foot sole. A total of 364 foot sole cutaneous mechanoreceptors were identified in this study. This sample consisted of 63 slow adapting type I (17%), 74 slow adapting type II (20%), 184 fast adapting type I (51%), and 43 fast adapting type II (12%). Across the foot sole, FA afferents consistently have lower firing thresholds than SA afferents (foot median: FAI 0.69 g, FA II 0.5 g, SA I 1.74 g, and SA II 10.0 g) [163]. Threshold afferents from the foot are higher than those in the hand (hand median: FAI 0.06 g, FA II 0.05 g, SAI 0.13 g, and SA II 0.76 g) [59,60] and may reflect their tuning to the high forces of standing balance. Strzalkowski et al. [164] found the distribution of foot sole cutaneous afferents to increase from the heel

to the toes, and from the medial to lateral aspects, driven primarily by type I afferents (Fig. 2). The distribution of cutaneous afferents across the foot sole could indicate areas of relative tactile importance (Fig. 1). It may be that type I afferent feedback from the toes and lateral border play a particularly important role in the control of standing balance (Fig. 2). With high receptor populations, the toes are identified as important sensory locations with populations able to delineate the physical limits of the base of support, evoking appropriate postural responses [192]. The toes dictate the anterior limit of the base of support [164,192]. Through toe muscle activation, it is possible to control the movement of the centre of pressure (CoP) in the sagittal plane within the confines of the base of support [121,176]. In the same way, the lateral borders of both feet define the boundary of the base of support in the frontal plane. When the centre of mass (CoM) moves beyond the lateral limit of the base of support, a stepping reaction can occur to prevent a fall [99]. Since FAI afferents have strong synaptic coupling to lower [41] and to upper [10] limb motor neurons, their relatively large density in the toes and lateral foot sole border [164] (Fig. 2) may help facilitate reflexive loops important in balance control. In fact, increasing cutaneous feedback from the foot sole border [128] or from the toes [185,187] has been shown to change balance ability in different categories of people.

### Cutaneous reflexes

Cutaneous reflexes in lower limb muscles play an important role in posture [30,48]. Several studies provide evidence of underlying reflexes arising from cutaneous afferents in humans from the sole of the foot. Afferents from



mechanoreceptors in the foot sole have multi-synaptic reflex connections with the neuron pools innervating the muscles that act at the ankle [6,41]. Cutaneous afferents from different nerves enter spinal cord through dorsal horn, converge and synapse on a common spinal interneuron to modulate excitability and produce excitation and inhibition in functionally related groups of motoneurons [115]. Non-noxious electrical stimulation of cutaneous afferents from the foot, innervated by the sural or tibial nerve, evoked a sequence of waves with onset latencies as early as 40 ms and lasting up to 200 ms [6] that produced complex excitatory and inhibitory effects of muscles acting about the ankle [6,41,196]. For example, a short latency inhibitory pathway from plantar cutaneous afferents to ankle extensors following mild stimulation to the tibial nerve is enabled in subjects when the foot sole makes contact with a surface [1]. Excitation of cutaneous afferents arising from the foot sole induces long-lasting facilitation of the ipsilateral extensor motoneurons [41] and induces crossed inhibitory postsynaptic potentials in the knee and ankle extensors [36]. These effects may be related to:

- the action of plantar cutaneous afferents on the presynaptic inhibition acting on Ia afferent terminals [56];
- their interaction with the reciprocal innervation [146];
- their actions on Ib inhibitory pathways [130,131].

In addition, plantar foot reflexes innervating lower leg muscles appear to be organized in a highly location-specific manner in humans [41,113,194,195] and the magnitude of these cutaneous reflexes is strongly altered depending on the posture [1,21,77]. Gradual changes in the magnitude and reversal of the reflex sign occurred when the locus of the stimulation systematically moved from the toe to heel. For the soleus and the tibialis anterior, there appears to be a boundary at approximately the mid-lateral plantar region of the foot, in which the sign of the reflex is switched to the opposite direction [113]. Forefoot stimulation produced inhibitory responses in the soleus and medial gastrocnemius, but excitatory responses in tibialis anterior muscles. Following heel stimulation, an opposite effect was evoked [113]. Systemic stimulations from the fifth toe to the heel on the lateral margin of the plantar foot demonstrated that the border of this soleus and tibialis anterior reflex reversal occurred roughly around the middle of the foot sole, providing greater resolution in the fine sculpting of motor output than previously revealed by sural or tibial nerve stimulation. A functional organization of excitatory and inhibitory cutaneous reflexes in the tibialis anterior and soleus by non-painful electrical stimulation to the plantar foot was demonstrated during voluntary contraction [155]. In addition, the middle latency component of cutaneous reflexes in lower leg muscles was significantly larger when the reflex was recorded during voluntary contraction of the muscle rather than when the muscle was posturally active [47]. It was also observed that stimulation at the lateral forefoot and heel evoked excitatory responses in peroneus longus but following medial forefoot stimulation an inhibitory response was evoked [113,114]. It was suggested that tactile stimulation mimics a destabilization of posture and thus modulates peroneus longus responses to counteract uneven terrain through stabilization of the ankle joint [113,114]. Finally,

when these muscles are active in standing, cutaneous feedback may play a role in modulating motoneuron output and thereby contribute to stabilization of stance [6].

## Sensory contributions of the foot sole: a proprioceptive and tactile interaction

Sensory feedback from the foot sole is important for perceiving changes to body orientation [64], and to regulate postural sway [100,120,193,197]. The spatial coding of body verticality by plantar inputs results from the ever-changing contrast between the pressures exerted on different parts of one foot or between the two feet [63,145]. Cutaneous afferents from the foot are encoded in a pressure scale and decoded as spatially relevant cues about body orientation [145]. Change in skin pressure under the sole could inform how the foot is in contact with the ground and subsequently how far the body position has to be adjusted [145]. Cutaneous mechanoreceptors feedback supply information about surface contact pressure and help sense continuous changes of posture [105]. Cutaneous mechanoreceptors may be functionally involved in exteroceptive [97] and proprioceptive processing by informing the central nervous system (CNS) about body position and support state [145].

Ankle proprioceptive feedback also provides sensitive means for detecting postural sway while standing [43,44], and there is strong evidence supporting the contribution of both cutaneous [3,85,103] and spindle [5] cues to the awareness of ankle position and movement. Information from the skin surrounding the ankle is necessary for kinesthetic tasks at the ankle joint, in both dorsi- and plantarflexion angles [85]. Furthermore, a transient reduction in skin sensitivity on the foot dorsum and anterior lower leg in healthy young adults has been shown to impair passive joint position sense [85,86] and alter lower limb kinematics during gait [53]. In the same way, Mildren and Bent [103] showed that cutaneous input from the foot generated by both low and high frequency vibration could influence proprioception at the ankle joint, and that this influence was modulated by ankle joint angle. These results emphasized robust interactions between FA cutaneous input [103] from the foot sole and proprioceptive signals from the ankle [85,103]. Although the observed effects were small, they had functional significance, and it has been suggested that this similarity facilitates coprocessing [4], making it likely that muscle and skin information influence each other. Postural responses of both cutaneous and proprioceptive origin were found to be frequency dependent [64].

Finally, proprioceptive and tactile feedback might be differentially involved in human postural control according to body or environmental constraints [64] and could subserve complementary functions for postural purposes.

## Changes with age and disease

Somatosensory information is important to the control of upright standing, and postural sway is necessary to detect both position and motion of the body in space. The relatively small body movements during quiet standing are sufficient to stimulate the various sensory receptors, especially plantar cutaneous mechanoreceptors, which constitute the

direct interface between the body and the ground. Studies have found changes in receptor morphology (reduction in receptor density and elasticity) or physiology (slower nerve conduction) with age or disease. A decline in foot sole skin sensitivity occurs naturally with aging [128,129] and as a result of neurological disorders, including different peripheral neuropathy [129,133,178]. This decline in sensitivity is associated with poorer postural control [94,153] and an increased risk of falls in these populations [69,80,133,178].

## Aging

Accurate detection and integration of somatosensory information from the feet is important for balance control [20], and degeneration of peripheral sensory receptors, can lead to a diminished capacity to detect information from the soles of the feet during interactions with the external environment [57,127]. Normal aging leads to changes in mechanical properties of the skin, as well as cutaneous receptor density, morphology and physiology. Age-related sensory deterioration of cutaneous afferents has been hypothesized as contributing to the increased risk of falling [57,142] as well as gait and balance disorders [32,84,101]. FA receptors exhibit structural modifications and are reduced in number with aging [13,23,46,151,157]. Several studies have compared sensory threshold testing in young and elderly groups of healthy subjects. Elderly feet were significantly less sensitive to mechanical stimuli (tactile and vibration) than the young [68,104]. Tactile thresholds in the elderly are significantly increased [174]. This is possibly due to a decrease in the density and distribution of Pacinian and Meissner corpuscles and Merkel's discs in the skin causing decreased spatial acuity [13,46,151,157]. This decrease in the density and distribution of cutaneous mechanoreceptors has been associated clinically with declines in vibration perception or touch thresholds [13,104], especially in the great toe [13]. Meissner's corpuscles of the plantar surface of the big toe of 30 persons were investigated histologically with respect to age [151]. The number of corpuscles decreases exponentially with increasing age. During the first decades of life the corpuscles exhibit a steady lateral and longitudinal growth, whereas at an advanced age an atrophy of Meissner's corpuscles occurs. In spite of considerable individual variations, a distinct dependency on age can be noticed. The deterioration of acuity in the great toe (averaging 400% between youth and advanced age) may adversely affect such diverse activities as maintaining balance [158]. This degradation of tactile acuity in the plantar aspect of the toe was significantly greater in fallers than in non-fallers [101].

Several studies have highlighted age-related changes in large fiber structure and decline in sensory nerve conduction velocity [16,182]. There is a decline in sensory nerve conduction velocity and in the amplitude of the sensory action potential with age [143]. Electrophysiological studies showed that sensory fibers are affected prior to motor fibers with aging [16]. Sensory nerve conduction velocities and response amplitudes peaked at age 40 years and subsequently declined [16]. Rivner et al. [143] found strong correlation of ageing with amplitude of the sensory action potential and a small but definite negative relation between

age and sensory nerve conduction velocity. For example, the sensory response from the sural nerve was absent in 23% of subjects between the ages of 70 and 79 years and in 40% over the age of 80 years [143]. It has been speculated that age-related changes in myelination may cause decreased nerve conduction velocity. Thus, the longer conduction distances to the feet would induce greater vibrotactile sense dysfunction and higher thresholds [68].

There are well-documented age-related changes in postural stability as measured via quiet standing on a force plate, including increased sway amplitude, centre of pressure velocity, and whole-body acceleration [78,96]. Sensory impairment (i.e., vibration sense, discriminative touch, or sensory nerve conduction velocity) in older adults is associated with functional decline and fall risk [65]. Peripheral sensation seems to be the single most important factor in maintenance of static postural stability in an older adult population [84] and reduced foot tactile sense in the elderly contributes to postural instability along with deprivation of feedback [168,169]. Endo et al. [39], reported a strong correlation between force plate measures of toe plantar flexor strength and the anterior limit of the functional base of support. Toe muscle function may play a particularly important role in the maintenance of balance in older people. Tanaka et al. [168,169] have shown that when standing, older people exert greater pressure with their toes than younger people, possibly in an attempt to intensify sensory information to maintain balance in the setting of reduced muscle and cutaneous information [168].

In this context, vibratory perception threshold testing may provide a sensitive measure to detect the onset of age-related plantar insensitivity [127]. Discriminative touch (i.e., 2-point sensation) of the feet should be considered when screening for distal sensory impairments in older adults [127,183] and could have a clinically relevant role as an assessment measure in aging. Although peripheral sensory loss is generally irreversible, there is emerging evidence that augmenting tactile sensory information from the sole of the foot using insoles with raised projections [91] or vibrating pads [135] may improve balance in older people. Foot characteristics, particularly tactile sensitivity and toe strength [102], are important determinants of balance and functional ability in older people. Intervention studies to reduce risk of falling may possibly benefit from augmenting sensory information from the foot.

## Peripheral neuropathy

Peripheral neuropathy (PN) is a complex disorder that arises from damage to peripheral nerves. PN can arise due to a variety of conditions, and the most common of which are diabetes mellitus [106] or effects of chemotherapy [25]. Peripheral nerve damage is characterized by abnormal conduction velocities and amplitudes [7] that typically progress in a distal to proximal manner [19]. Most cases of PN do involve pathology in the smaller sensory fibers such as A $\beta$ , A $\delta$  and unmyelinated C-fibers that transmit cutaneous sensations like touch, vibration and temperature [167]. Patients with PN describe several sensations such burning, tingling, hyperalgesia or allodynia, and loss of tactile sensation, proprioception, and thermal sensitivity [7]. In this context, PN frequently results in specific functional impairment, such as

loss of balance and with marked increase in risk of falling [24,160].

**Diabetes.** Peripheral neuropathy is a pathology that affects sensory and/or motor nerves and degrades perception and action abilities [141]. The most common cause of these neuropathies is diabetes [184]. Diabetic peripheral neuropathy (DPN) is the result of a number of disturbances in the peripheral nervous system as a consequence of hyperglycemia [173]. Rapidly reversible abnormalities of nerve conduction may occur in patients with recent transiently poorly controlled diabetes and may be accompanied by uncomfortable distal sensory symptoms [18,173]. Duration and severity of exposure to hyperglycemia are related to the severity of neuropathy [124,156]. The most common clinical presentation of DPN is sensorimotor neuropathy [35,122]. DPN involves either or both small and large nerve fibers in limbs in a length-dependent pattern [184]. Small nerve fiber injuries classically occur earlier [92] than large ones [198]. Nevertheless, plantar vibration sense and/or distal tendon reflexes are also altered very early in the course of DPN [110,198], but these correspond to dysfunction in large diameter fibers. Although the pathophysiology of DPN remains unclear, peripheral mechanisms have been suggested, such as neural ion channels (Na<sup>+</sup> and Ca<sup>2+</sup>), abnormal glycemic flux-related damage to the spinal cord, and central mechanisms, such as impaired central pain processing secondary to functional and structural brain remodeling [152].

Degradation of the somatosensory system occurs with DPN and can be determined by nerve conduction velocity and perception thresholds of different modalities such as pressure or vibration [19,141]. Typical symptoms of DPN are symmetric numbness, paresthesia, or pain in the distal lower limbs involving more than a single nerve distribution, which progresses in a centripetal direction [171]. Symmetrical sensory loss ("stocking or glove sensory loss") in the feet above the ankles is evident on clinical examination. The ankle and Achilles reflexes are usually reduced or absent, which can result in foot abnormalities. These symptoms collectively result in disturbed proprioception and abnormal muscle sensory function. Increased vibration and thermal thresholds occur early during the course of the disease in both patients with type 1 and type 2 diabetes [198]. However, DPN symptoms may develop much earlier in the course of type 1 than in type 2 [124], suggesting a difference in the natural history or different mechanisms of nerve injury in DPN between diabetes types: predominant involvement of small nerve fibers in patients with type 2 versus large myelinated fibers in patients with type 1 diabetes, respectively, even in those with a similar severity of neuropathy [110]. Consequently, the degradation of the somatosensory system, including decrease in nerve conduction velocity and sensory threshold, patients with peripheral neuropathy have balance disorders [49]. The pathological findings of DPN are axonal loss, axonal regeneration, and demyelination in some patients [33]. The nerve conduction study is a reliable and objective diagnostic method to evaluate the DPN [40]. It is used to measure the speed of both motor and sensory conduction, amplitude, distal latency, distance, F wave latency, and other factors [34]. More precisely, several studies using electromyography [116–118] showed that decreased nerve conduction velocity associated with loss of

sensory feedback may delay the onset of postural corrections in response to environmental disturbances [49,51]. In addition, Nardone and Schieppati [117] established correlation between postural oscillations and nerve conduction velocity in diabetic patients with both Ia and II fiber neuropathy. There was a significant relationship between postural instability and type II fiber involvement [118]. In the same way, a decrease in sensory thresholds [11] could induce postural instability [11,24]. It would appear that loss of information from the CoP position is the most important parameter for postural control [52]. From a clinical point of view, quantitative sensory testing (QST) represents a quantitative method usually graded using a continuous numerical scale to detect the threshold of thermal perception (cold or warm), vibration perception, current perception, pressure pain and sudomotor function [22,33]. Vibration thresholds are particularly sensitive to detect mild or subclinical neuropathy and correlate well with other QST measures [19]. The QST is probably effective for documenting sensory abnormalities and changes in sensory thresholds during longitudinal evaluation of patients with DPN. This should be complementary to thorough clinical assessment [34].

**Chemotherapy.** Chemotherapy, such as taxanes or oxaliplatin, is often used to treat different types of cancer [108]. One of the most important side effects of chemotherapy is painful peripheral neuropathy [25,31,188] with decreased sensory nerve action potential amplitudes on electrodiagnostic testing [25], increased vibration thresholds, dysesthesias and paresthesia in a glove and stocking distribution [25,45]. Peripheral neuropathy following chemotherapy correlates with a loss of proprioception and is associated with postural instability [52,118] and higher risk of falls [141,165,175], and can have a significant impact on physical function. Taxanes among other chemotherapeutic agents are well known to cause selective injuries to the peripheral nervous system, notably inflammation in the dorsal root ganglion and peripheral nerves involved in processing somatosensory information [95]. Large myelinated afferent fibers such as Ia fibers are injured by these neurotoxic agents [95] and may be responsible for balance disorders [188]. Neuropathy-induced loss of somatosensory information and processing leads to postural instability [15]. In this context, CoP parameters were significantly higher for patients with breast cancer compared with healthy controls [170,188]. These balance disorders tend to progress with cumulative chemotherapy and may be partially explained by somatosensory change, notably on the soles of the feet [76].

The effect of chemotherapy on patient balance appears to be clinically relevant when compared to balance impairments observed in diabetic patients [17] or in elderly adults [134]. The balance measures provide an objective approach to quantify changes in patient function by assessing postural control. These results support the clinical interest of implementing balance measures during routine oncology clinic flow to longitudinally quantify postural instability in breast cancer patients [107].

## Clinical interest and interventions

Previous research has provided some evidence that experimental modulation cutaneous information can change

postural sway. More precisely, artificially reducing somatosensory information by cooling [90], local anesthetics [51] or standing on a foam surface [125] can reduce the reliability of somatosensory information and increase postural sway.

In recent years, studies have demonstrated that additional somatosensory input has positive effects on postural control by using various stimulation methods [186]. These findings confirm that mechanical stimulation of the plantar sole have an impact on the mechanoreceptors of the feet, and this relevant tactile information helps in upright standing. Nevertheless, the effect of mechanical stimulation on postural control in patients with reduced cutaneous sensory acuity remains unclear.

Previous studies have used mechanical noise to improve standing balance [50,82,83,135,199], movement sensation [29] and tactile sensation [26,190] in elderly people [82,83,135], in people with peripheral diabetic neuropathy [50,83,136,199] or stroke [83,136]. Application of mechanical noise to the feet, administered as random vibrations from specific elements, induces stochastic resonance, which can transform previously unfelt subthreshold stimuli into suprathreshold stimuli that do produce action potentials [136,190]. Mechanical noise improves the vibration perception threshold of the plantar side of the foot in patients with diabetic neuropathy and may be helpful in preventing foot ulceration in patients with diabetic neuropathy [70,199].

Another potential aid to improve balance in patients with loss of sensation is application of low-level electrical stimulation [111,112] under the feet. These authors suggested that daily home use of plantar electrical stimulation was effective to enhance balance [172] and plantar sensation, as quantified by significant reduction in vibration perception threshold [111].

Considering the sensory deficits presented by subjects with Parkinson's disease, several studies have proposed automated mechanical peripheral stimulation applied under the foot, as a potential rehabilitation strategy [71,72,123,159]. Mechanical pressure applied, in sequence, under the feet has shown positive effects in terms of improving functional mobility and gait parameters [71,72,159], and postural control [138]. Low pressure-based stimulation (range of 0.3–0.9 N/mm<sup>2</sup>) applied simultaneously in two target areas (head of the great toe and base of the first metatarsal bone) under both feet [138] could improve dynamic balance [71,159] and spatiotemporal parameters of gait [71,72,159]. In the same way, autonomic changes were observed following stimulation of the feet, either using low pressure (0.58 kg/mm<sup>2</sup>) applied to the tip of the hallux and the lower great toe first metatarsal joint plantar surface [8], or vibration [162]. Autonomic changes resulting in diminished resting blood pressure values may help in controlling orthostatic hypertension, which often is present in patients with Parkinson's disease [8]. In addition, effective stimulation re-established the capacity to increase cardiac and vascular sympathetic modulation in response to the gravity stimulus and widened the functionality of the arterial baroreceptor mechanism [8].

Finally, stimulation of the plantar surface of the foot using vibration could represent an interesting and original way to assist the navigation of people with visual impairment [181]. Using vibrating motors, inexpensive and practicable

devices have been proposed for stimulating the plantar surface and transmitting tactile information to people with visual impairment [181]. Results showed that people were capable of navigating environments using the directions provided by tactile interfaces for the foot [181].

## Summary and conclusions

The sole of the foot is an important sensory structure in the control of standing balance. Specialized mechanoreceptors transmit tactile and proprioceptive feedback used by the CNS for reflexive and conscious adjustments to posture. This ability results from the coordination between a tactile system that permanently provides information about sway and weight distribution under the feet, and a motor system that initiates corrective postural reaction controlling muscular activity. Cutaneous receptors and associated afferents constitute the fundamental functional units that enables the transduction and transmission of tactile feedback to the CNS. Providing additional sensory information useful for postural control seems relevant to improve postural stability and balance. Plantar cutaneous inputs enhance the detection and transmission of weakened cutaneous signals and this region appears to be a good candidate for improving the postural stability in older adults or subjects with neurological disorders [189]. In this perspective, several interventions have been proposed and studied in the elderly [127] and patients with neurological diseases, such as peripheral neuropathy [94], Parkinson's disease [133] or multiple sclerosis [28].

The increased distribution of cutaneous afferents in the toes [164] may reflect the postural significance of feedback from the toes in the control of standing balance. In addition, the toe plantar flexion muscles contribute to controlling posture. Both amplitude and velocity of postural sway could be controlled by toe plantar flexion muscles [148]. In fact, the toes play a unique and important role in standing balance [121,168,169,176,185,187]. In order to maintain balance, the toes can be flexed and extended to apply pressure to the ground and correct for postural disturbance. During quiet standing, we can frequently feel that the movement of the toes helps in maintaining balance. Additionally, links were found between decreased toe sensitivity and increased body sway during quiet standing [168]. Tanaka et al. [169] proposed the idea that people with less toe sensitivity might use great toe pressure in order to intensify sensory input from the great toe as well as to maintain balance. In the same way, some authors [121,176] showed that the toe muscle stimulation was capable of regulating CoP displacement and this approach may be a good candidate for controlling balance. In these studies, forward movement of the CoP was induced by different intensity of electrical stimulation applied to the toe muscles. Furthermore, body acceleration could be controlled during quiet standing by regulating the intensity of stimulation applied to the toe muscles [176].

Finally, Viseux et al. [185,187] observed that small focal additional thickness placed under the toes has an effect on the CoP measures used to assess postural control during unperturbed stance. A significant change of balance was obtained with the lowest thickness (0.8 mm), even though the contact forces induced by the lowest thickness were



probably too small to mechanically stabilize the body. In this context, it was believed that cutaneous mechanoreceptors of the toes were activated by a low focal additional thickness and seem to be consistent with tactile hypothesis of Tortolero et al. [176]. Since the foot is the only body part in contact with the surface during quiet standing, it is very likely that toe movements play an important role in balance control [148,192]. The toes provide a stable surface area that remains in contact with the ground and serve to relay relevant sensory information to the central nervous system [79]. It is clear that sensory information from the toes is used to perform postural corrections when balance disturbances occur [176] and their use can improve the feeling of stability [1,149,176]. These findings highlight the important functional role of the foot sole, where tactile feedback from the toes and plantar muscle activity may be more meaningful for the control of standing balance. This comprehensive review advances how the foot sole is viewed as a sensory structure that communicates with the CNS to help us balance and stand up. This brings new clinical perspectives for development of intervention strategies to improve the quality of foot sole cutaneous feedback (i.e. customized postural insoles) and seems to be an interesting and promising approach for the management of patients with balance disorders, with specific chronic pain syndromes, with neurologic diseases or those at risk of falling.

## Disclosure of interest

The author declares that he has no competing interest.

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