

Using Virtual Reality to Assess the Street Crossing Behavior of Pedestrians with Simulated Macular Degeneration at a Roundabout

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2 ABSTRACT

3

4 This work investigates how pedestrian street crossing behavior at a virtual traffic roundabout is
5 affected by central visual field loss. We exposed participants with normal vision to a first-person
6 virtual experience of central visual field loss of variable size in the form of a simulated scotoma,
7 an area of the visual field with degraded visual acuity. A larger size of scotoma influenced people
8 to select longer gaps between traffic, and to wait longer before initiating a crossing. In addition, a
9 gender difference was found for risk taking behavior. Male subjects tended to take more risk, as
10 indicated by the selection of shorter gaps in traffic and a shorter delay before the initiation of a
11 crossing. Our findings generally replicate those of studies done in real-world conditions using
12 participants afflicted with genuine central vision loss, supporting the hypothesis that virtual reality
13 is a safe and accessible alternative for investigating similar issues of public concern.

14 **Keywords:** macular degeneration, immersive traffic simulation, visual deficit simulation, gap affordances, perception, street crossing,
15 roundabout

1 INTRODUCTION

16 Virtual Reality (VR) provides an effective medium for the study of human behavior. The appeal of this
17 technology lies in its capacity to control environmental factors. VR also finds applications in research where
18 conducting an experiment may be too dangerous or infeasible for real-world execution. Thus, VR has been
19 used to investigate pedestrian behavior at intersections (Clancy et al., 2006; Seward et al., 2007; Bernhard
20 et al., 2008; Morrongiello et al., 2015; Meir et al., 2015). Real traffic scenarios present unnecessary risk to
21 participants and are difficult to control with accuracy. Contributing to previous virtual traffic research, we
22 conducted an investigation into the ability of pedestrians to make street-crossing decisions under simulated
23 visual impairment. In contrast to prior studies, our virtual environment consists of a roundabout, rather

24 than a traditional, linear intersection, because the ability of a pedestrian to judge sufficient openings, or
25 gaps, in traffic is essential for crossing the street at circular junctions safely. For the visually impaired
26 and other vulnerable populations, this ability may be compromised, resulting in unsafe decision making
27 at these special crossroads. This concern is motivated by real-world studies (Ashmead et al., 2005; Guth
28 et al., 2005), which have established that blind individuals make poor gap judgments at traffic roundabouts.
29 Accordingly, these populations have been of interest for behavioral analysis within the domain of pedestrian
30 safety.

31 We are interested in how macular degeneration in particular affects performance and safety in pedestrian
32 situations. Macular degeneration is a medical condition that primarily affects older populations and results
33 in vision loss to the center of the visual field. This loss is due to the deterioration of the macula, which lies
34 near the center of the eye's retina. The resulting degradation of visual acuity, or scotoma, may present itself
35 as a partial vision loss or complete occlusion. Clear central vision is essential for observing fine detail, and
36 central vision deficits affect performance in daily activities such as reading and walking (Ergun et al., 2003;
37 Hassan et al., 2002). At present macular degeneration accounts for 8.7% of all blindness worldwide and is
38 the most common cause of blindness in developed countries (Wong et al., 2014). Alarmingly, the number
39 of people worldwide with age-related macular degeneration alone is projected to rise to 196 million by
40 2020, advancing to 288 million by 2040.

41 In an effort to aid in determining the extent to which macular degeneration affects the movement and
42 safety of afflicted pedestrians, we analyzed pedestrian performance at a roundabout intersection without
43 traffic signal guidance. To achieve this goal, we embedded a simulation of our desired visual deficit into an
44 immersive virtual reality application. Both our experimental setup and virtual environment were inspired
45 by prior literature, which analyzes gap crossing judgments in order to evaluate pedestrian safety (Wu et al.,
46 2009). We define gap crossing as the selection of a break in the traffic stream followed by traversal of
47 an intersection. By exposing normally sighted individuals to this first-person experience and assessing
48 their gap crossing behavior, we were able to investigate the effect of macular degeneration on gap crossing
49 judgments.

50 Thus, this study simulates a visual impairment (macular degeneration) in a virtual traffic crossing to assess
51 a vulnerable population's ability to make critical judgments on issues of safety. Recruiting a population
52 with actual visual impairments for either real-world or virtual studies is problematic as this population
53 is often elderly and may have balance issues that limit use of head-mounted displays (HMDs); also, the
54 limited contrast range of most HMDs makes viewing difficult for such a group. It may therefore be more
55 effective to simulate the visual impairment and use healthy subjects. Likewise, the virtual traffic simulation
56 itself provides a safe means of studying a dynamic and potentially hazardous phenomena under controlled
57 conditions. We show that our macular degeneration simulation offers a controlled and well defined model
58 of real visual impairment; and our roundabout traffic simulation provides a realistic and safe environment.

59 Our head-mounted display (HMD) based virtual environment consisted of a roundabout, a controllable
60 traffic simulation, a 3D acoustic subsystem, and a vision deficit simulation. The virtual environment
61 modeled a single lane roundabout accompanied with crosswalks and splitter islands. The simulated traffic
62 reproduced vehicle acceleration and deceleration patterns as well as other natural traffic interactions, such
63 as collision avoidance and pedestrian yielding.

2 BACKGROUND AND RELATED WORK

64 Plumert et al. (2004, 2007) studied street crossings and gap affordances at linear intersections in a large
65 screen virtual environment in the context of cycling safety, with particular attention to children. They
66 found children and adults chose the same-size gaps and yet children ended up with less time to spare
67 when they cleared the path of the approaching car, providing evidence of a significant developmental
68 change in affordance judgments for adolescents. Their work has also studied pedestrian behavior at such
69 intersections O’Neal et al. (2017) and judgments involving two lanes of traffic Grechkin et al. (2013). In
70 contrast to their work, our work takes place in the context of the exit lane of a roundabout, where traffic
71 decisions can be more complex, and involves visual impairment.

72 Geruschat et al. (2006) found that macular degeneration patients appear to have different gaze behavior
73 in comparison to fully-sighted people during high-risk activities. Geruschat et al. (2011) compared traffic
74 gap detection among pedestrians with normal vision, central vision loss, and peripheral vision loss. While
75 their results suggested that all groups could identify crossable and uncrossable gaps accurately, there was a
76 significant effect of low vision in measures of latency and safety. The study also found that decisions at the
77 exit lane of a roundabout are more difficult than those at the entry lane. These experiments, done in the
78 real world at an uncontrolled intersection with a handheld trigger as the indicator of deciding to cross are
79 best viewed as complementary to ours, which involve real locomotion in a controlled traffic simulation in a
80 virtual environment.

81 Hassan (2012) compared normally sighted, visually impaired, and blind pedestrians’ street crossing
82 decisions, and found that visually impaired participants’ performance was as accurate and reliable as
83 normally sighted participants. Unsurprisingly, blind pedestrians were the least accurate in making street
84 crossing decisions. Hassan and Snyder (2012) continued this investigation among elderly people with
85 macular degeneration, elderly people with normal vision, and young normally sighted pedestrians. Again,
86 no significant differences were found between macular degeneration and age-matched, normally-sighted
87 pedestrians in street crossing decisions. However, the study found a risky tendency for macular degeneration
88 pedestrians to make unsafe street-crossing decisions. Our study seeks to provide a simulation that provides
89 normally sighted people with an understanding of the difficulties faced by these visual deficits and is
90 behaviorially equivalent. This work is again best viewed as complementary to ours since it involved
91 decisions at simpler traffic intersections (the single lane of a one-way street), and used a handheld trigger
92 as an indicator of deciding to cross. It is likely that our simulation presented visual impairments that were
93 in a broader range of impairment than those studied by this body of work as well, as Hassan and colleagues
94 focused on subjects with mild to moderate visual impairments.

95 Virtual reality has been applied to simulate visual impairments for medical training and education
96 purposes, as well. These simulations provide first-person experiences for medical professionals to better
97 understand the daily difficulties encountered by patients. Ai et al. (2000) and Jin et al. (2005) simulated
98 various forms of eye diseases in the context of a virtual apartment and received positive user response.
99 They simulated macular degeneration through the application of an opacity mask and a wavy mask. Banks
100 and McCrindle (2008) created a similar, specialized visual eye disease simulator for architects to view their
101 designs through the perspective of a visually impaired onlooker. This work provides engineers with a better
102 understanding of how to design public spaces for better accessibility and easier navigation. In the study
103 presented by Lewis et al. (2012), a Gaussian blur and a distortion shader were applied to simulate macular
104 degeneration. They also conducted an effectiveness test which showed that using their visual impairment
105 simulator improved users understanding of visual impairments in general. Expanding the virtual microcosm,
106 Väyrynen et al. (2016) designed a navigation task amidst a city environment that allowed for participants

107 to experience various visual impairments such as macular degeneration, cataracts, glaucoma, and myopia
108 in a dynamic setting.

109 In augmented reality, various types and levels of visual impairment have also been simulated. Through
110 the coupling of head-mounted displays and stereoscopic cameras, Ates et al. (2015) and Werfel et al. (2016)
111 produced simulation tools to generate experiences using real-time video feedback. Both developments focus
112 primarily on user experience, invoked empathy, and understanding as metrics for evaluation. While most
113 studies recreate computational estimations of low vision experiences, an assessment tool was designed by
114 Pamplona et al. (2011) to capture retinal information from a high-contrast light-field display. Although this
115 information is not displayed in real-time, it is able to create an accurate depiction of the visual occlusion
116 experienced by a participating subject.

3 THE ROUNDABOUT VIRTUAL ENVIRONMENT

117 A roundabout is a circular intersection in which an entering vehicle must adjust direction and speed in
118 order to merge into a uni-directional traffic circle. Our environment is modeled after the Pullen-Stinson
119 roundabout, at North Carolina State University. Figure 1 shows a bird's eye view of the scene. Upon
120 approach to the roundabout, a vehicle in the system gradually reduces momentum from a default speed
121 (15m/s) to a circulating speed (7.5m/s), maintaining the circulating speed for the duration of its roundabout
122 traversal. Upon exiting, the vehicle gradually accelerates back to the original, default speed of 15m/s. A
123 vehicle must also avoid collisions, although our subjects were instructed not to "force" such yielding.

124 Our system controls travel paths, start times, and velocities for all vehicles so that a variable stream of
125 virtual automobiles may be scheduled and launched for each trial. These trials can therefore represent
126 a variety of traffic scenarios by providing a series of time gaps between moving vehicles, based on a
127 specified distribution. In our procedure each traffic stream includes a maximum of eight vehicles, which
128 are randomly selected from eight distinct vehicle models.

129 To include both auditory and visual cues in our environment, we added a three-dimensional (3D) acoustic
130 subsystem capable of synthesizing the spatialized sound associated with moving vehicles in real-time. Our
131 spatialized audio rendering uses a non-individual head-related transfer function (HRTF) (Begault, 1994;
132 Kapralos et al., 2008), derived from the anthropomorphic audio logical research mannequin KEMAR
133 (Knowles Electronics) (Gardner and Martin, 1995).

134 Within this HMD-based virtual environment, users can safely interact with controlled traffic streams,
135 which allocate sufficient time for street traversal upon the event of a designated, safe time gap in traffic. A
136 sample rendering of the pedestrian's viewpoint of the roundabout with traffic is shown in Figure 2. More
137 details about the roundabout environment can be found in Wu et al. (2009).

4 SIMULATING MACULAR DEGENERATION

138 4.1 Optical Distortions

139 Induced by retinal damage, macular degeneration often results in scotomas, or areas of reduced light
140 sensitivity, in the retina. A relative scotoma, which can be simulated by blurring images, refers to an area
141 that retains some residual light sensitivity. An absolute scotoma, which can be simulated as an opaque spot,
142 describes the absence of any light perception. The shape and size of scotomas vary across patients. In this
143 simulation, we generalize a model of macular degeneration through the combination of a blur and opacity
144 filter, which is expressed by a circle of black area within a circle of a blurred region. Figure 3 provides a



Figure 1. An overview of a roundabout virtual environment



Figure 2. Traffic view within the roundabout



Figure 3. Macular Degeneration simulation (a black area, 10° of visual angle, surround by a blurred area, 20° of visual angle)

145 sample rendering of the low-vision simulation for clarification. Our filter was implemented via the OpenGL
146 Shading Language (GLSL) embedded in Vizard.

147 Central scotomas are represented by a variety of shapes including: circles, ellipses, ring-shapes, and
148 horseshoes, as well as more irregular geometries. The majority of macular degeneration studies (Guez
149 et al., 1993; Hassan et al., 2002) use diameters to infer scotomas, so we have generated a circle-based
150 approximation to provide a reasonable comparison. The macula refers to an area of approximately 5-6 mm
151 in diameter, centered on the fovea, which corresponds to the central 15°-20° of visual angle (Cheung and
152 Legge, 2005). Our HMD has field of view 44° horizontally and 35° vertically, so there is a wide range to
153 the visual angles of scotomas it can generate. Previous studies (Hassan et al., 2002; Ergun et al., 2003)
154 have revealed that the size of the absolute scotoma correlates significantly with one's ability to perform
155 daily tasks. Therefore, for the efficacy of our simulation, it is imperative to provide an allowance for any
156 size of potential scotoma.

157 Visual acuity is another indication of a person's ability to perform a range of vision-dependent daily living
158 tasks (McClure et al., 2000). In our system, changing the amount of blur for the relative scotoma can control

159 visual acuity. We asked 8 people to report letters binocularly using a Snellen chart in a virtual environment.
 160 The acuity estimates were systematically related to the blur factor and fit to an exponential curve, as shown
 161 in Figure 4. The image transitions from clear to blur or opacity needs to be smoothed without sharp edges.
 162 A Gaussian function was applied to define the level of blur or opacity over the transition on edges. This
 163 type of simulation of visual deficit is consistent with other simulations of such phenomenon (Cornelissen
 164 et al., 2005; Geringswald et al., 2012).

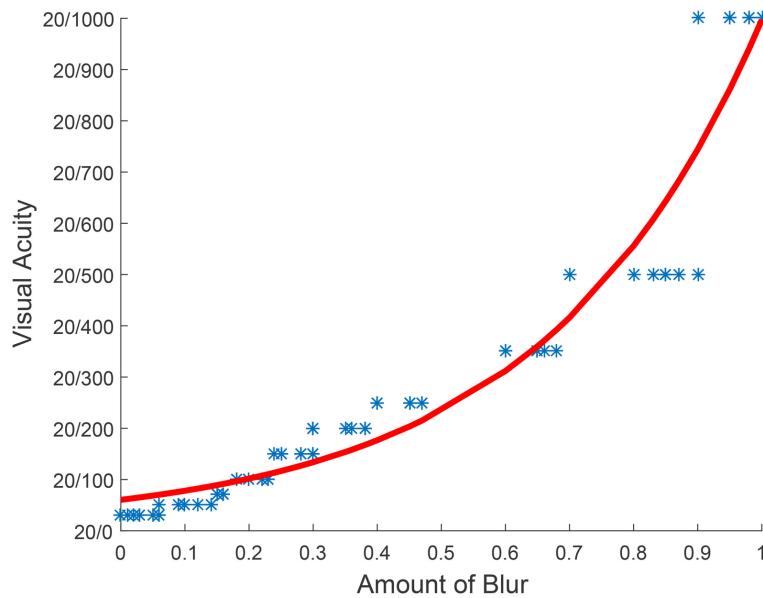


Figure 4. Visual acuity tested by a Snellen chart (X axis represents the scale of the blur. Scale 1 makes the scene opaque and scale 0 makes the scene clear. Y axis represents Snellen fraction.)

165 4.2 Gaze-contingent

166 Scotomas frequently affect the same region of the visual field in both eyes (Cheung and Legge, 2005) and
 167 shift with eye movement in real-time. This type of degradation to the visual field in the foveal region can
 168 be simulated with a stereoscopic head-mounted display (HMD) equipped with an eye-tracker. With only a
 169 static occlusion in the middle of the display, subjects may circumvent visual occlusions by looking at the
 170 clear, peripheral portion of the viewport. However, by using an eye-tracker, gaze position is provided in
 171 real-time so that the system can link simulated scotomas with current gaze position. This allows scotomas
 172 to shift with real-time gaze movement and provides a dynamic occlusion at the center of the user's visual
 173 field. In this paper we used an NVis SX60 HMD equipped with an Arrington eye-tracker. The Nvisor SX-60
 174 HMD provides 1280×1024 resolution per eye, a field of view (FOV) of approximately 47° (horizontal)
 175 by 37° (vertical) degrees, full binocular overlap, and a frame rate of 60 Hz. The HMD weighs approximately
 176 1kg. The Arrington eyetracker provides eye tracking with infrared video. The accuracy is approximately
 177 $0.25^\circ - 1.0^\circ$ visual arc with spatial resolution approximately 0.15° visual arc. The system records the
 178 (X, Y) position of gaze at a rate between 60Hz and 30Hz. This rate is faster than the 50 milliseconds of
 179 average saccadic suppression (Volkmann, 1986). The position data can be transmitted in real-time to other
 180 software applications.

181 The eye-tracker requires calibration, which was done at two levels. Initially, a calibration to the user was
 182 done at the system level. However, optimal calibration was difficult to maintain given the unavoidable

183 slippage of the HMD on the head as people turned their heads to track vehicles and as they crossed the road.
 184 To minimize this, we had subjects wear silicone swimming caps before wearing the HMD, and we secured
 185 the cable of the HMD to each subject with a belt. Additionally, a second, application layer calibration was
 186 conducted within the virtual environment on a per trial basis. This calibration application involved subjects
 187 fixating on the center of the visual field and adjusting the eyetracking to match this position.

5 EXPERIMENT AND RESULTS

188 5.1 General Design

189 The purpose of this experiment was to observe how our simulation affected normal-sighted individuals'
 190 street crossing decisions at roundabout intersections. In particular, we examined the time gap between
 191 vehicles where pedestrians select to cross the street — the gap threshold — under different vision conditions.

192 In the roundabout virtual environment, subjects were asked to cross the street in an exit lane. This area is
 193 shown as the shaded area between point A and point B in Figure 5. For that particular position, there are six
 194 paths along which vehicles travel must be checked. These paths are depicted by yellow curves on the same
 195 figure: (1) M ->N ->C; (2) M ->N ->E ->F; (3) J ->K ->N ->C; (4) J ->K ->N ->E ->F; (5) G ->H
 196 ->K ->N ->C; (6) G ->H ->K ->N ->E ->F. The system creates traffic streams by randomly selecting
 197 travel paths for each of eight vehicles from these six paths, allowing half of the vehicles to exit at point C
 198 and half of them to exit at point F.

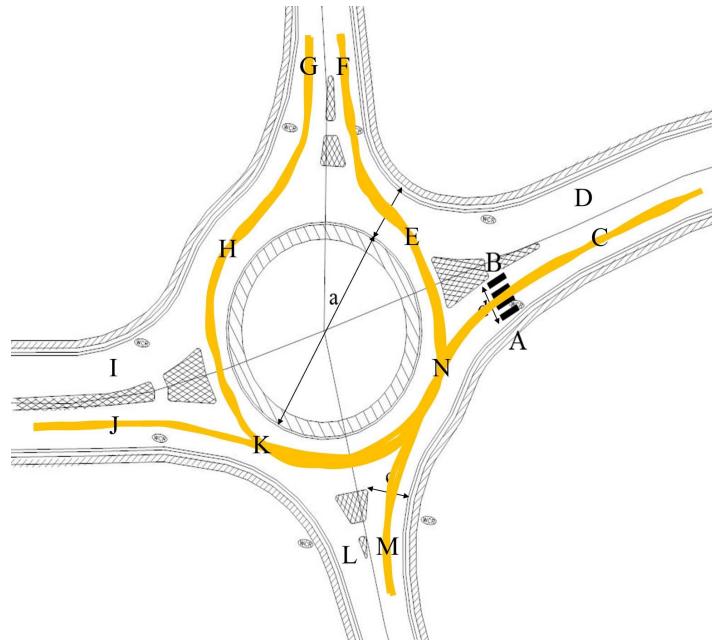


Figure 5. The architectural model of the roundabout, showing the pedestrians crossing area and vehicle travel paths

199 The system creates the traffic stream so that there is a gap between vehicles such that a pedestrian at A or
 200 B might choose to cross. This gap is the target gap. Each traffic stream is scheduled based on a specified
 201 time gap between every two adjacent vehicles. Most of these time gaps represent non-target intervals,
 202 which are set to less than 1.5 seconds. Only one randomly selected gap in the stream is set to the target
 203 gap value, which can range between a minimum of 2 seconds and a maximum of 10 seconds. We were

204 interested in analyzing street-crossing decisions made at this interval, which simulated a safe crossing
205 interval.

206 As in our previous study (Wu et al., 2009), we applied a maximum-likelihood stimulus procedure (MLP)
207 (Grassi and Soranzo, 2009) as an evaluation methodology to obtain the minimal threshold of gap selection.
208 Each pedestrian crossed the street 20 times, either from point A to B or from point B to A as seen in Figure
209 5. Each time they either crossed the street in a target gap or in a non-target gap. Based on the specified
210 target gap duration and the pedestrians crossing outcome, MLP found a minimal gap duration that says this
211 participant chose to cross the street 75% of the time.

212 Participants were instructed to find a safe and comfortable gap in traffic to cross the street without running
213 and without wasting any chances to cross, just as they would in the real world. Participants were instructed
214 to wait until the first car passed before attempting to cross. In addition, they were asked to assume that
215 vehicles would not yield in response to their crossing. We desired participants to assume responsibility
216 for their safety through this assumption even though virtual vehicles in the environment would yield to
217 pedestrians in practice. Participants were encouraged to finish after initiating a crossing, even if they
218 believed that their decision was unsafe. Based in pilot testing, each subject completed 20 trial crossings,
219 which was enough to insure convergence of the maximum likelihood procedure.

220 The outcome in a trial was deemed a “go” if the pedestrian started crossing during the target gap for
221 a given stream of traffic. A “no-go” outcome occurred if the target gap passed without the pedestrian
222 initiating a cross. Under “go” conditions a safe crossing indicates the subject successfully crossed before
223 the target gap passed, otherwise it fell into the unsafe crossing category. An invalid outcome occurred if the
224 pedestrian started crossing during a gap preceding the target gap, in which case that stream was invalidated
225 and repeated in later trials.

226 For all go outcomes, the system recorded the time points when a pedestrian started crossing and finished
227 crossing the street. With this system we recorded two other dependent variables in addition to the gap
228 threshold. One was the curb delay, which was the time elapsed from the beginning of the target gap to
229 the start of crossing behavior, meaning how long the pedestrian delayed on the curb before they actually
230 initiated their crossing. The other was the crossing time, which was the elapsed time between the start of a
231 crossing and the finish of that crossing. More details of the general design of street crossing are in Wu et al.
232 (2009).

233 5.2 Hypotheses

234 The independent variable for this experiment was scotoma size, which generated three visual conditions:
235 normal vision (zero scotoma), which provided base line results; 10° of visual angle of absolute scotoma
236 with 20° of visual angle of relative scotoma; and 20° of visual angle of absolute scotoma with 40° of visual
237 angle of relative scotoma. Each subject was randomly assigned to one of these three viewing conditions.

238 Our size decision was based on the research of Sunness et al. (2007). They showed a progression of
239 increasing scotoma size at different stages of macular degeneration, from less than 10° of visual angle near
240 the onset of the disease, to up to 20° of visual angle for late stage. We selected a small and large size of
241 absolute scotoma and doubled the size of relative scotoma to compare the effect.

242 In pilot studies conducted with full screen visual acuity variations, we found that varying acuity alone did
243 not significantly change gap estimation performance, possibly because it is easy to estimate moving blobs
244 in a static background. This finding held even at severe degradations in acuity of 20/1,000. We did not,

245 therefore, plan to vary the acuity in this study but set the relative scotoma at a fixed value of 20/500 for
246 both simulated conditions.

247 By simulating a controllable scotoma coupled with low visual acuity, we were able to simulate the main
248 characteristics foveal vision loss characteristic of macular degeneration. We hypothesized that simulated
249 macular degeneration would cause subjects to select a longer target gap to cross, experience a longer curb
250 delay, and experience a longer gap crossing time in comparison to subjects who do not experience the
251 simulated impairment. There is some suggestion in the literature — e.g., Simpson et al. (2003); Holland
252 and Hill (2007) — of males making riskier road crossing decisions than females, and we hypothesized that
253 this will be the case regardless of visual condition.

254 5.3 Participants

255 A pilot study revealed that some participants experienced difficulties with the eye-tracking solution. While
256 most participants could be calibrated in approximately ten minutes, some could not be accurately calibrated
257 at all with the eye-tracker, due to imperfect fit of the HMD and eye-tracker on the head. Therefore, we
258 conducted pre-screening sessions prior to the experiment to train subjects to use the eye-tracking HMD. If a
259 participant's pupil still evaded detection by the eye-tracker, then they were eliminated from the experiment.

260 We recruited 41 subjects in total. Three subjects were excluded because of inability to calibrate the
261 eye-tracker. Another two subjects were excluded due to motion sickness during the experiment. Our final
262 results are derived from the remaining 36 subjects. The subject group included 18 males and 18 females
263 aged from 18 to 31 years old. All subjects were normally sighted without eyeglasses, although subjects
264 who were corrected to normal with contact lenses were allowed.

265 Subjects were randomly assigned to one of the visual conditions of no simulated scotoma, a 10° of visual
266 angle of absolute scotoma with 20° of visual angle of relative scotoma (10/20), or a 20° of visual angle
267 of absolute scotoma with 40° of visual angle of relative scotoma (20/40). A between groups design was
268 chosen to minimize overall time in the HMD and to avoid the possibility of carry-over effects from one
269 condition to another.

270 5.4 Apparatus

271 The experiment was conducted in a 29 x 23 ft. room. We used the Vizard (Worldviz, Santa Barbara,
272 CA) platform to develop the virtual roundabout environment. Our system includes a WorldViz rendering
273 computer, Precision Position Tracker server with 4 cameras, an audio rendering computer with a pair of
274 Klipsch S4 earbuds. The HMD and eye tracker were described previously in Section 4.2.

275 An InterSense IS-900 precision motion tracker is used to update the participants rotational movements
276 with six degrees of freedom. Position is updated using 4 optical tracking cameras working in coordination
277 with 2 LED lights at 60Hz. For the ViewPoint EyeTracker, the expected difference in degrees of visual
278 angle between true eye position and mean computed eye position is approximately 0.25° to 1.0° visual arc.
279 The smallest change in eye position that can be measured is approximately 0.15° visual arc.

280 As mentioned previously, in order to preserve proper calibration and prevent slipping of the HMD, we
281 required subjects to don a silicone-swimming cap before using the HMD and we required subjects to wear
282 a belt to secure the HMD's tethered cable. In addition, throughout the experiment a helper, carrying a
283 backpack which held the HMD machine, followed the subjects to ensure that the cable would not be pulled
284 or pushed.

285 5.5 Procedure

286 Participants started by completing a written consent form and questionnaire asking about prior experience
287 with video games and virtual reality. The experimental protocols were approved the Institutional Review
288 Board at our University. In particular, subjects were assured that they could take a break or quit at any point
289 if they desired or if they began to feel sick. Next, participants were shown a Google map depiction of
290 the real world roundabout from which the virtual model was derived. The direction of traffic flow was
291 depicted. The experimental task (safe road crossing in the face of traffic) was explained to the participant
292 and they were informed that their vision would be obstructed if they were in one of the visual impairment
293 conditions. Subjects were told that they would be crossing the street 20 times with traffic over the course
294 of the experiment. Subjects then donned ear buds, swim cap, HMD, and belt. The eye cameras were
295 calibrated in a process taking between five and ten minutes. The HMD was adjusted to be secure before
296 calibration and subjects were asked not to touch the HMD unless they wanted to take a break or quit the
297 experiment, as the calibration procedure would need to be repeated. Subjects were then introduced to
298 the virtual environment with full vision and crossed the street once without traffic to introduce them to
299 locomotion in the HMD. After each street crossing, a quick recalibration of the eyetracker as described
300 in Section 4.2 was performed. At this point, subjects were introduced to their specific visual condition.
301 Subjects were asked to inform the experimenter if the central scotoma was not in line with their gaze, at
302 which time another recalibration was performed. The traffic simulation was started, and the participant
303 began to cross the street in traffic. After 20 crossings, subjects were compensated for their time in the
304 experiment.

305 5.6 Results

306 Figure 6 shows the overall gap crossing distributions, grouped by vision condition and gender, for the 36
307 subjects in their 20 crossings. This diagram illustrates the various conditions defined in Section 5.1 for the
308 gaps in traffic: “go and safe” represents the percentage of trials where participants selected a target gap and
309 crossed the street safely; “go but unsafe” represents the percentage of trials in which participants selected
310 an unsafe gap to cross the street; and “no-go” represents the percentage of trials in which participants
311 elected to not cross the street during the presented traffic stream.

312 The first row of Figure 6 displays the data broken out by vision condition. Qualitatively, it demonstrates
313 that a larger size of simulated scotoma results in a lower percentage of safe crossings. In particular, this is
314 indicated by a decrease in the percentage of go and safe crossings, which drops from 25% to 18% between
315 the no scotoma and the 20°/40° scotoma conditions. This result is consistent with the hypothesis that
316 subjects with simulated macular degeneration will have fewer safe crossings. In addition, the percentage of
317 no-go trials increased from 45% to 55%, indicating that participants with larger sizes of simulated scotomas
318 missed more chances to cross the street. However, the percentage of unsafe crossings did not increase.
319 These results suggest that participants became more conservative with their risk taking behavior as the size
320 of scotoma increased. In the second row of the figure, which displays the data as grouped by gender, we
321 observe that male subjects had fewer “no-go” trials and that they perform fewer safe crossings, indicating
322 that male subjects have a greater propensity for risk taking than their female counterparts.

323 There are two between-subjects independent variables: gender (two levels: male, female) and vision
324 condition (three levels: no scotoma, 10°/20° of absolute/relative scotoma, 20°/40° of absolute/relative
325 scotoma). Table 1 lists the complete breakdown of mean and standard error values for these three dependent
326 variables in the experiment: gap threshold (the discrimination threshold of crossing gaps), curb delay (the
327 time elapsed from the beginning of the designated gap to the start of actual street crossing), and crossing

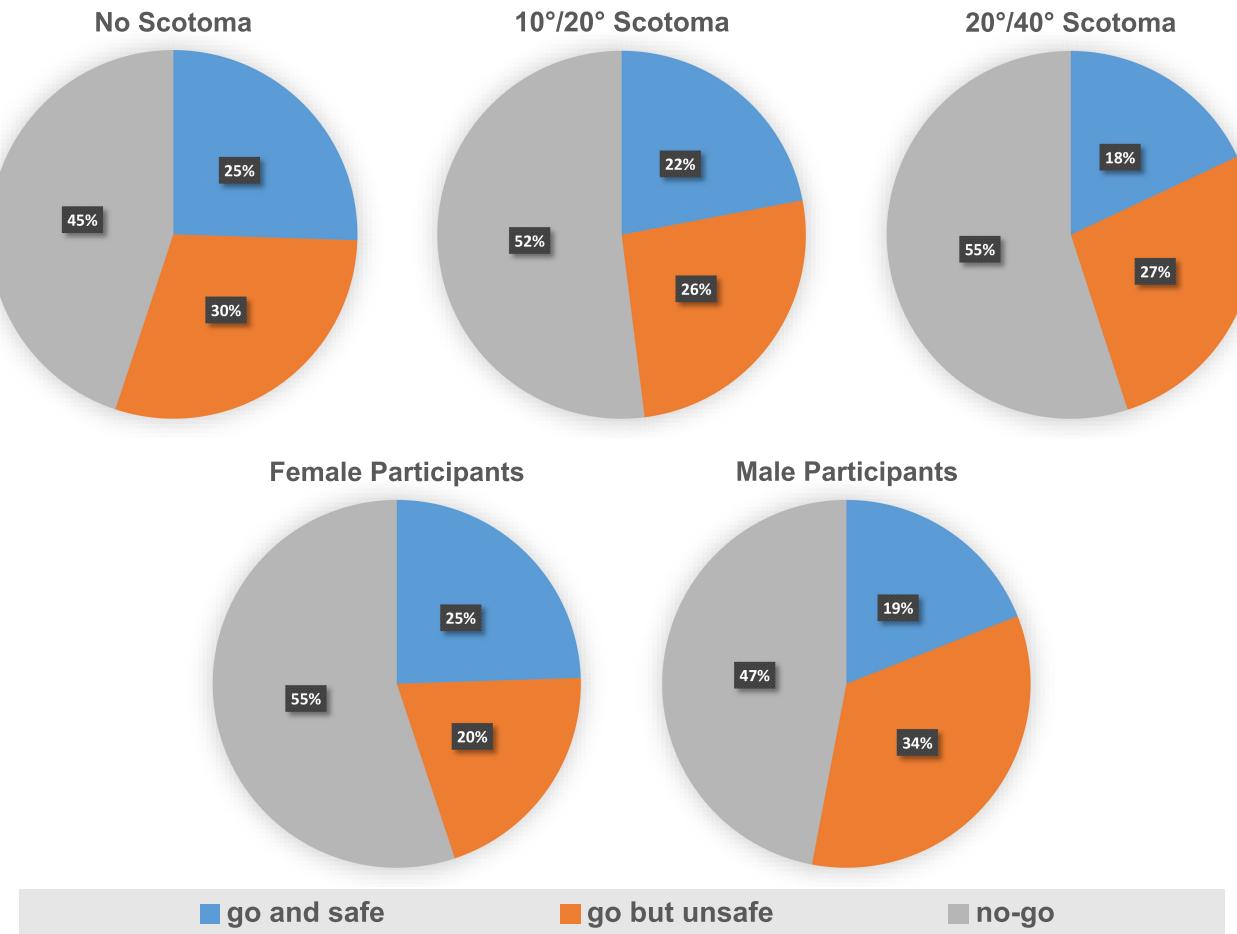


Figure 6. Crossing distribution by group and crossing distribution by gender in experiment.

328 time (the time elapsed from the start of street crossing to the finish of street crossing). The no scotoma
 329 participants had the smallest gap threshold (4.204 seconds) with smallest curb delay (1.661 seconds);
 330 and participants with 20°/40° of absolute/relative scotoma had largest gap threshold (6.177 seconds) with
 331 largest curb delay (2.639 seconds).

332 Figure 7 shows the mean gap thresholds, mean curb delays, and mean crossing times broken out by both
 333 vision condition and gender. We analyzed our results using a two-way between-subjects analysis of variance
 334 (ANOVA). For the gap threshold, there are main effects of vision condition, $F(2, 30) = 5.4415, p = 0.0096$,
 335 and of gender, $F(1, 30) = 5.7624, p = 0.023$. A post hoc Tukey test showed that the no scotoma, 10°/20°
 336 scotoma, and 20°/40° scotoma all differed significantly. Also males had significantly shorter gap thresholds
 337 than females. Likewise, for curb delay, ANOVA there were main effects of both vision condition, $F(2, 30)$
 338 = 5.6694, $p = 0.0082$, and gender, $F(1, 30) = 5.1099, p = 0.031$. A post hoc Tukey test showed that the no
 339 scotoma condition had a significantly shorter curb delay than the 20°/40° scotoma condition; the 10°/20°
 340 scotoma condition was not significantly different from either, but lay somewhere in the middle. Crossing
 341 time was not statistically different between groups.

342 There is a linear correlation between these dependent variables. Pearson's coefficient of correlation
 343 between gap threshold and curb delay is 0.888 ($t = 11.259, df = 34, p < 0.001$). Likewise, the Pearson's
 344 coefficient of correlation between gap threshold and crossing time is 0.533 ($t = 3.6763, df = 34, p < 0.001$);
 345 and the coefficient of correlation between curb delay and crossing time is 0.595 ($t = 4.3208, df = 34,$

Table 1. Key measures in seconds

Condition	Gap Threshold		Curb Delay		Crossing Time	
	<i>Mean</i>	<i>SE</i>	<i>Mean</i>	<i>SE</i>	<i>Mean</i>	<i>SE</i>
No Scotoma	4.204	0.363	1.661	0.143	3.267	0.109
<i>Male</i>	3.741	0.279	1.424	0.073	3.283	0.144
<i>Female</i>	4.667	0.644	1.897	0.250	3.251	0.176
10°/20°	5.660	0.510	2.224	0.202	3.933	0.258
<i>Male</i>	4.612	0.648	1.933	0.227	3.936	0.497
<i>Female</i>	6.707	0.536	2.515	0.306	3.929	0.211
20°/40°	6.177	0.511	2.639	0.270	3.907	0.189
<i>Male</i>	5.864	0.769	2.357	0.414	3.924	0.196
<i>Female</i>	6.490	0.719	2.922	0.344	3.889	0.346

346 $p < 0.001$). Thus high gap threshold tends to be paired with relatively high curb delay and high crossing
 347 time.

348 In summary, we found statistically significant differences between vision conditions. A larger size
 349 scotoma resulted in a longer gap threshold, and a longer curb delay. However, the most dramatic differences
 350 were typically found between the presence and the absence of a scotoma. These findings are consistent
 351 with our hypotheses that subjects with simulated macular degeneration will select a longer gap to cross and
 352 experience a longer curb delay. We also found gender differences in some measures. Male subjects tended
 353 to take more risk, which was demonstrated by the selection of shorter gaps and shorter waiting times prior
 354 to crossing. This finding is consistent with our second hypothesis. However, the males in our sample group
 355 were also more familiar with video games as self-reported in their responses to our questionnaire, with 10
 356 of 18 subjects reporting regularly playing video games an average of 7 hours per week ($SD=5.2$ hours); in
 357 contrast, only one of 18 females reported playing video games regularly, an average of 7 hours per week. It
 358 is possible that increased familiarity with the virtual environment leads to increased risk-taking, although
 359 Spearman's rank-order correlation did not achieve significance.

6 DISCUSSION

360 We simulated central visual field loss and assessed the affect of this loss on normally sighted individuals
 361 making road crossing decisions at a roundabout. We found support for our hypothesis that this loss would
 362 increase the gap threshold and result in increased curb delay, but did not find a statistically significant
 363 difference in crossing times for subjects once they had selected a gap to cross. Compared to no scotoma,
 364 each level of increased scotoma size that we implemented resulted in a longer gap threshold selection, but
 365 our only significant difference in the curb delay was between the no scotoma and the largest scotoma size

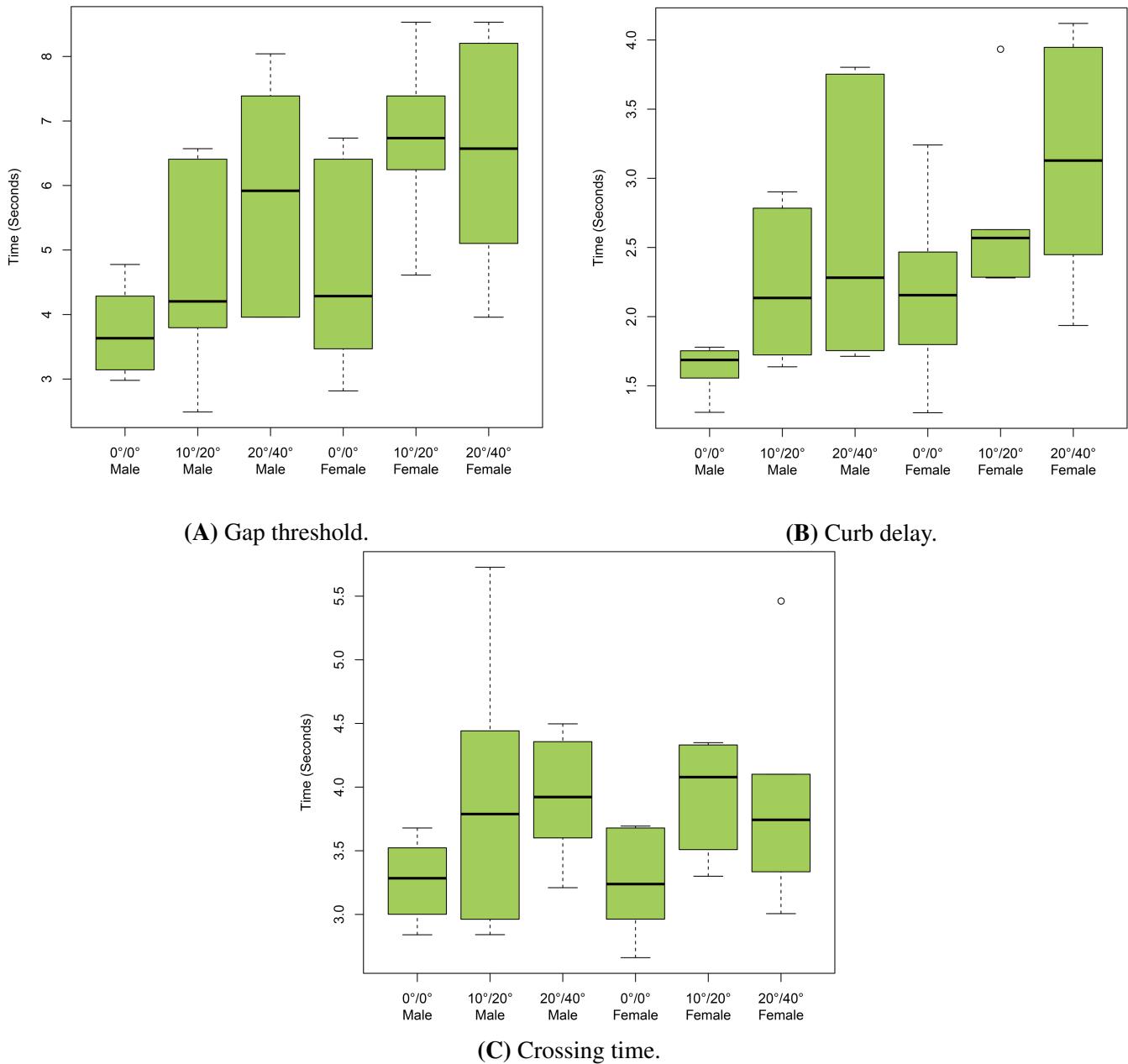


Figure 7. Medians and quartiles of the various measures broken out by vision condition and gender.

366 (20/40). Regarding crossing times, it may be that once subjects decide to cross the street, their walking pace
 367 is not strongly subject to visual feedback and thus visual field impairment may result in only incidental
 368 increases. We also found support for our hypothesis that there would be gender differences in the data.
 369 Male subjects tended to take more risk, which was demonstrated by the selection of shorter gaps and shorter
 370 waiting times prior to crossing. This gender difference was not due to faster crossing times by males, since
 371 both genders crossed in about 3.9 seconds on average.

372 Hassan et al. (2002) studied macular degeneration patients and found that mobility performance, such as
 373 walking speed, decreased as the size of a binocular central scotoma increased. In our study, normal-sighted
 374 participants exposed to central vision loss selected a longer gap threshold with increasing scotoma size. Our
 375 gap thresholds and crossing times are in accord with those of our prior work (Wu et al., 2009). O'Neal et al.

376 (2017) used a linear intersection and large screen immersive display environment and found gap thresholds
377 generally consistent with ours but crossing times that were faster, possibly an artifact in our work of subjects
378 wearing an HMD. It is potentially interesting to note that their simulation involved a wide, naturalistic field
379 of view in a linear intersection, and ours involved a restricted field of view in a roundabout, and yet the gaps
380 chosen by their adult population (approximately 4.45s) and our no scotoma adult population (4.2s) were
381 close. It is always important to examine field of view as an ecological factor in assessing simulation validity
382 when using HMDs, and the NVIS SX60 has limited field of view compared to commodity level devices
383 available today, but it may not be an important factor in this area of investigation. Our work showing that
384 males make riskier choices is consistent with a large body of literature that indicates male gender as a
385 risk factor in pedestrian injury, e.g., Schiff and Oldak (1990); Assailly (1997); Rosenbloom et al. (2004);
386 Barton and Schwebel (2007).

387 Our simulation allowed us to explore the effect central vision loss on these gap thresholds. The simulation
388 is configurable to allow a variety of visual impairments to be implemented. We chose extreme central
389 vision loss as a test case since with moderate blur locomotion and road crossing seem to be unaffected
390 (although such things as reading would be severely affected), as evidenced by Figure 4. Future work will
391 model foveal deficits and maculopathies in more detail, with the goal of examining mechanisms of disease
392 progression through behavior. Some limitations in the present simulation that may hinder this work are that
393 it is difficult to characterize the accuracy of eye-tracker given the two-step calibration procedure used and
394 the slippage of the HMD on the head. Our assessment criterion in this study was behavioral, and did not
395 require more accurate assessment of the eye tracking system's limits, c.f., Geringswald et al. (2013), but
396 that may not be true of future work.

397 Our simulation incorporated spatialized audio as a component of the experience. It was not tested as a
398 factor in any of these experiments, but sound is known to be a cue for making crossing decisions in the real
399 world. Geruschat et al. (2011) found that pedestrians with full sight were more sensitive when their hearing
400 was occluded, whereas in the low vision groups hearing occlusion did not affect sensitivity. Hassan (2012)
401 was also noted that the visually impaired participants traffic gap detection performance was unaffected
402 by hearing occlusion. There is significant interest in how audio cues are used by the visually impaired,
403 particularly with the increase of quieter hybrid and electric vehicles on the street Emerson et al. (2011),
404 and such investigation is a topic of future research.

405 The use of virtual reality in this work was critical. Virtual reality provides an environment in which a
406 dangerous scenario — traffic crossing with visual impairment — can be investigated in a controlled and
407 rigorous manner. Testing subjects with true visual impairment in true traffic situations is difficult, and
408 some form of proxy is often used. For example, Geruschat et al. (2011) used subjects with actual macular
409 degeneration or peripheral vision loss at a live intersection with real traffic, but had them press triggers
410 to indicate when they would cross rather than actually cross. Our results are nonetheless consistent with
411 theirs, with ours having considerably easier recruitment, ease of execution, no real danger, and containing
412 actual locomotion. This suggests that our traffic crossing scenario allows us to design and conduct effective
413 research in perception and action in dynamic situations. The simulation of visual impairment for normally
414 sighted individuals can provide an important educational tool to investigate a significant social problem.
415 The result of this research could deliver important insight in how to improve structures for the safety of
416 those with visual impairments. In particular, the first-person experience provided by our simulation could
417 provide important insights for safe design in engineering intersections and more.

7 ACKNOWLEDGMENTS

418 This material is based upon work supported by the National Eye Institute, National Institutes of Health,
419 under R01 EY12894-04, and by the National Science Foundation under grant 0821640 and 1526448. Any
420 opinions, findings, and conclusions or recommendations expressed in this material are those of the authors
421 and do not necessarily reflect the views of the sponsors.

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