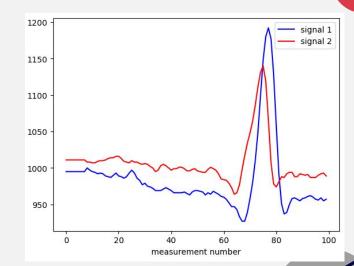
Gateway Data Science Project: Detecting Abnormal ECG Signals

Anna An, Jon Tchounguen, Victor Wu

The MIT-BIH Arrhythmia Dataset

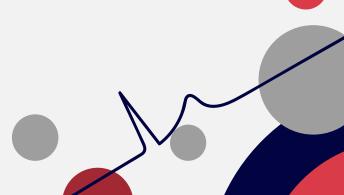
- Contains 48 30 minute ECG heartbeat samples
 - 100-series collected randomly from Boston hospital
 - 200-series selected to include clinically important rare arrhythmias
 - Beats have been annotated by cardiologists
- 20 specific standard classifications grouped as **5** broad categories:
 - Normal beats (N)
 - Fusion beats (F)
 - Supraventricular ectopic beats (S)
 - Ventricular ectopic beats (V)
 - Unclassified beats (Q)



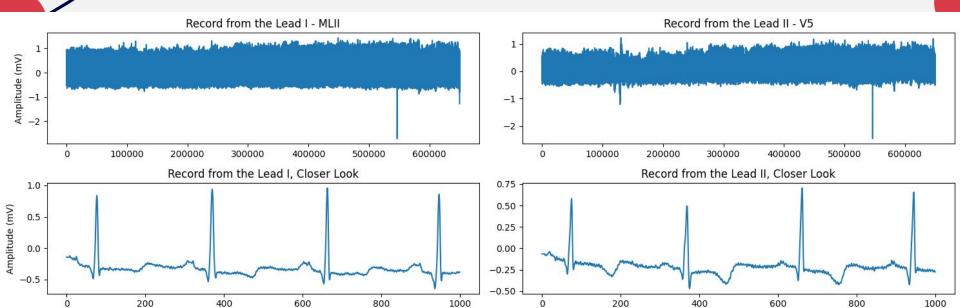


```
record = wfdb.rdsamp('mitdb/100')
    annotation = wfdb.rdann('mitdb/100', 'atr')
[ ] record
    (array([[-0.145, -0.065],
           [-0.145, -0.065],
           [-0.145, -0.065],
           [-0.675, -0.365],
           [-0.765, -0.335],
           [-1.28, 0.]
     {'fs': 360,
      'sig len': 650000,
      'n_sig': 2,
     'base date': None,
      'base_time': None,
     'units': ['mV', 'mV'],
     'sig_name': ['MLII', 'V5'],
      'comments': ['69 M 1085 1629 x1', 'Aldomet, Inderal']})
[ ] annotation.sample
                    77, 370, ..., 649484, 649734, 649991])
   print(annotation.symbol)
```

- First, we used a single file for EDA
 - A single file was found to have around 650,000 samples
 - 2274 R peaks
 - The recordings were digitized at 360 samples per second per channel with 11-bit resolution over a 10 mV range



EDA of Record 100



Sample Number

Sample Number



Descriptive analysis

Measures of Central Tendency Mean = -0.24866670384615372 Median = -0.27

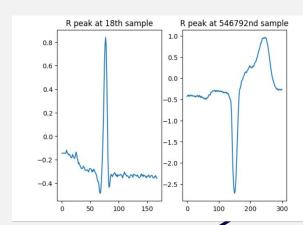
Measures of Dispersion

Minimum = -2.715 Maximum = 1.435 Range = 4.15 Variance = 0.032968090379058436 Standard Deviation = 0.18157117166295544

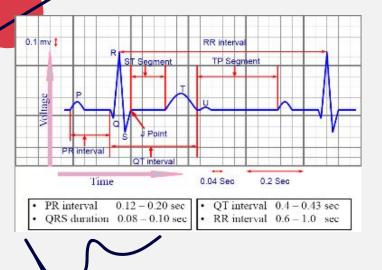
Are there missing values?

Number of NaN values
Lead I: 0
Lead II: 0
annotation.sample: 0
annotation.sample: 0
Lead II: 0
annotation.sample: 0
annotation.sample: 0

Outliers?



About the Dataset: Data Wrangling



- Data Segmentation (Darmawahyuni et al., 2022)
 - The recordings were digitized at 360 samples per second per channel.
 - This implies that for every 36 samples, 0.1 seconds have elapsed.
 - Based on the time elapsed between different parts of an ECG wave, we were able to calculate that a single ECG wave should be 230 samples long (corresponding to 0.63 s)

Step 1. Preprocessing

Data set	N			S					V		F	Q		
	N	L R e j A				A	a J S			V E		F	f	Ç
DS1 ^a	38052	3946	3779	16	16	807	100	32	2	3664	105	414	0	8
	45777			973	3					3769		414	8	
DS2 ^b	36413	4123	3475	0	213	1735	50	51	0	3215	1	388	0	7
	44011			204	19					3216		388	7	

Table 1. Size of data sets DS1 and DS2 and the mapping between AAMI and MIT-BIH-AR labels.

- Records from patients 102, 104, 107 and 217 were excluded due to the majority of their beats being paced beats (is controlled by an electrical impulse from an artificial cardiac pacemaker)
- Segment: Data was segmented into individual arrays with 1 beat each
 - If an upside-down peak is observed, we neglected. (Outlier)
 - We observed that each record's baseline differed with each other. Therefore, we normalized the dataset (Kachuee et al., 2018).
- Classify: There are 42 unique symbols in annotation.symbol across the whole datasets (See the appendix 1 for more details)
 - They were classified based on AAMI labels mapping rules (Zhang et al., 2014)

	0	1	2	3	4	5	6	7	8	9		220	221	222	223	224	225	226	227	228	229
0	0.149153	0.152542	0.155932	0.155932	0.152542	0.159322	0.155932	0.166102	0.159322	0.159322		0.145763	0.149153	0.155932	0.155932	0.162712	0.145763	0.138983	0.155932	0.152542	0.159322
1	0.143791	0.143791	0.150327	0.156863	0.147059	0.147059	0.140523	0.143791	0.150327	0.156863		0.173203	0.166667	0.163399	0.160131	0.169935	0.173203	0.173203	0.163399	0.160131	0.173203
2	0.192691	0.192691	0.192691	0.179402	0.172757	0.192691	0.189369	0.192691	0.189369	0.189369	1555	0.232558	0.239203	0.242525	0.245847	0.232558	0.225914	0.229236	0.232558	0.232558	0.239203
3	0.133574	0.148014	0.148014	0.158845	0.158845	0.155235	0.151625	0.158845	0.169675	0.169675	***	0.194946	0.184116	0.176895	0.184116	0.180505	0.194946	0.191336	0.187726	0.191336	0.202166
4	0.150350	0.150350	0.150350	0.143357	0.143357	0.143357	0.153846	0.153846	0.153846	0.139860	***	0.174825	0.178322	0.185315	0.188811	0.188811	0.178322	0.178322	0.181818	0.192308	0.192308
	1751	57.53	570	(55)5	DIET	7.1	555)	550	25.55	1507	(1555)	1554	5550	200	8555	***	(555)	1710	2.00	(225)	0.00
100694	0.076555	0.076555	0.078947	0.083732	0.083732	0.081340	0.074163	0.069378	0.074163	0.071770		0.064593	0.059809	0.062201	0.052632	0.052632	0.045455	0.050239	0.057416	0.062201	0.066986
100695	0.095694	0.088517	0.090909	0.083732	0.083732	0.083732	0.086124	0.086124	0.088517	0.095694		0.059809	0.062201	0.059809	0.059809	0.064593	0.066986	0.071770	0.071770	0.071770	0.059809
100696	0.096447	0.088832	0.081218	0.078680	0.081218	0.081218	0.083756	0.083756	0.081218	0.091371	***	0.078680	0.081218	0.083756	0.088832	0.088832	0.093909	0.096447	0.096447	0.088832	0.096447
100697	0.054455	0.061881	0.056931	0.056931	0.061881	0.071782	0.069307	0.066832	0.059406	0.056931		0.071782	0.079208	0.076733	0.079208	0.079208	0.076733	0.071782	0.066832	0.061881	0.064356
100698	0.121655	0.121655	0.116788	0.114355	0.111922	0.114355	0.116788	0.116788	0.119221	0.119221	***	0.048662	0.048662	0.051095	0.055961	0.060827	0.063260	0.065693	0.063260	0.058394	0.063260

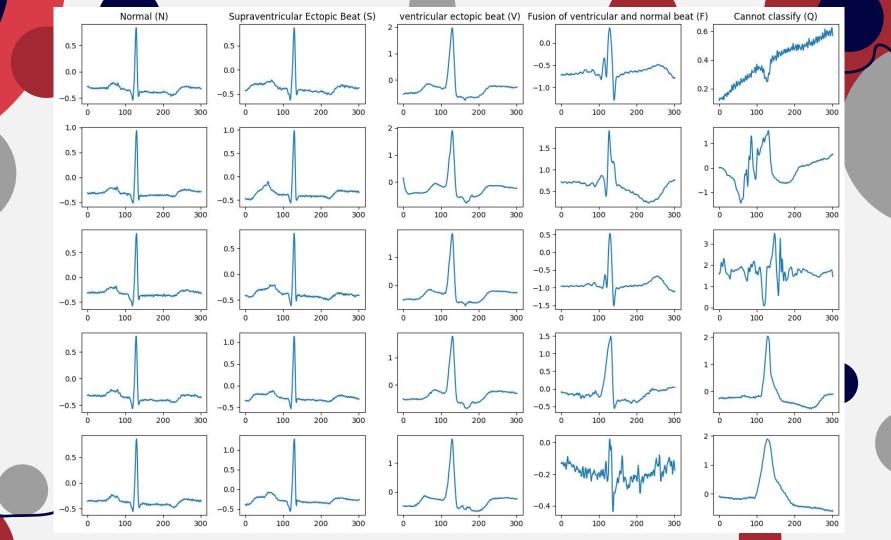
Variable 1. 230*100698 Table Formed; Columns represent a sample (230 samples = 0.63 seconds), rows represent one wave (N, S, V, F, or Q), and values represent an amplitude for a wave at a specific sample (mV).

```
['N' 'N' 'N' ... 'N' 'N' 'N']
(100699,)
```

Variable 2. Wave label

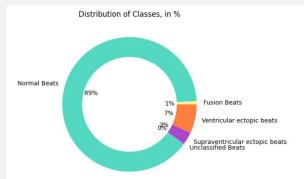
```
[3.70000e+02 6.62000e+02 9.46000e+02 ... 6.49292e+05 6.49536e+05 6.49772e+05]
(100699,)
```

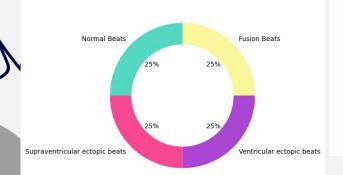
Variable 3. Wave's R peak location



Step 2. Balancing Dataset





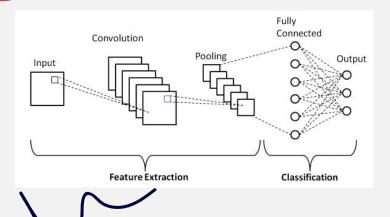


- Dataset is imbalanced across 5 classes
 - Normal: 89848
 - Supraventricular: 3026
 - Ventricular: 7008
 - Fusion: 802
 - Unclassified: 15
- Smaller classes were resampled so that all classes have same number of samples in the training set
 - Unclassified classes were neglected because 1. No specific pattern observed, 2. small size of sample
- All 4 classes now have 31727 samples
- Data was split into 2 sets: 70% training (56% train, 14% validate), 30% test sets.



- The goal is to classify ECG beats with one of four labels
 - Normal beats, fusion beats, supraventricular ectopic beats, ventricular ectopic beats
 - As there is a large variation in unclassified beats, we decided to exclude them from the classification task

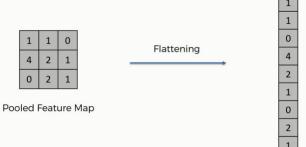
Step 3. Classification: CNN



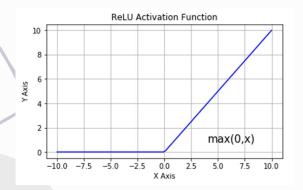
- We used two methods to classify the data, convolutional neural network (CNN) and support vector machine (SVM)
- Convolutional neural network:
 - A classification algorithm with layers made of functions that take multiple inputs and produce a single output
 - Each function has different weights that can extract features that distinguish different classes
 - Here, we applied a 1-dimensional convolution operation to the input data by sliding a small window (known as a filter) over the input data and performing a dot product between the filter and the data within the window.

12	20	30	0			
8	12	2	0	2×2 Max-Pool	20	30
34	70	37	4		112	37
112	100	25	12			

<u>Max Pooling:</u> a downsampling technique that reduces the spatial dimensionality of the input data. This reduces the size of the data, while preserving the most important features.



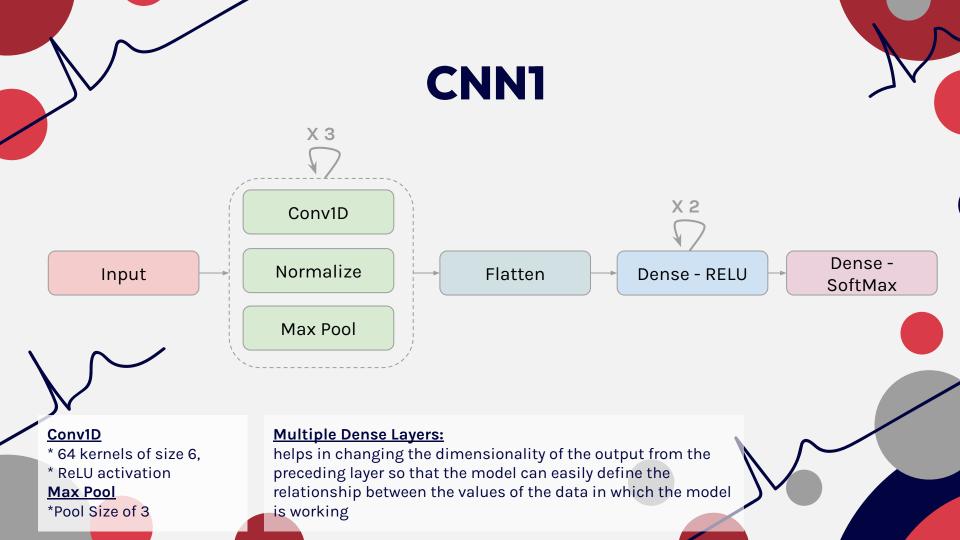
<u>Flatten:</u> Flatten is a layer that simply reshapes the input data into a 1-dimensional vector.

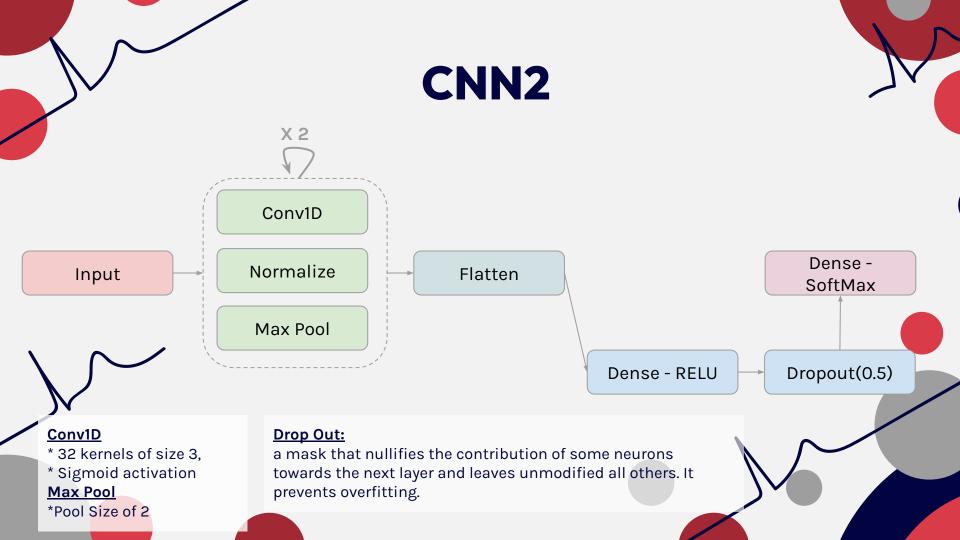


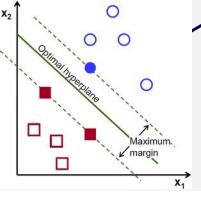
ReLu: allows the decision boundary to be non-linear. (It applies the function f(x) = max(0,x))

<u>Sigmoid</u>: It applies the function $f(x) = 1 / (1 + \exp(-x))$ to each element of the input tensor, squashing the output values between 0 and 1.

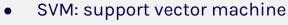
<u>SoftMax</u>: Exponential functions are used to make sure outputs sum to 1. (Applies $f(x) = \exp(x_i) / \sup(\exp(x_j))$)



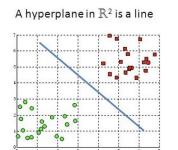


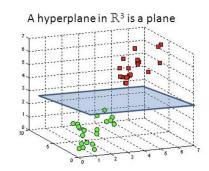


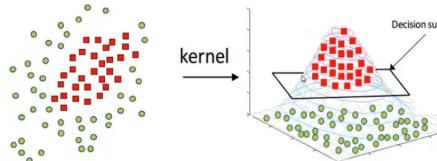
Step 3. Classification: SVM

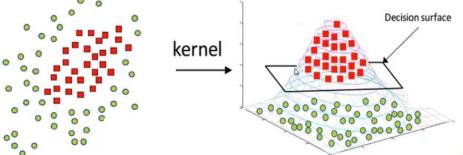


- An algorithm that finds a linear boundary between two classes
 - In 2D a line, in 3D a plane, in nD a n-1 D hyperplane (hard to imagine)
- The boundary location is found by maximizing the distance between the points close to the boundary and the boundary
- A kernel function is used to transform data that is not linearly separable to a higher dimension where it is
- We used an rbf kernel (projects into a Gaussian distribution)







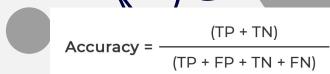




- Four metrics: accuracy, precision, sensitivity, specificity
 - Accuracy: the percentage of correct classifications
 - Precision: out of all the classifications of a certain class, what proportion were correct
 - Sensitivity (recall), specificity: true positive and true negative rate
 - **Confusion matrix**: shows the number of each class correctly and incorrectly classified



$$Precision = \frac{True\ Positive}{True\ Positive + False\ Positive}$$





Both our CNN and SVM model scored excellently, with testing and training scores ≥ 0.95.

• CNN1 Overall accuracy scores: 0.9987

- CNN1 Accuracy scores by classes:
 - O N: 0.991
 - S: 0.823
 - O V: 0.968
 - o F: 0.798

 CNN2 Overall accuracy scores: 0.9886

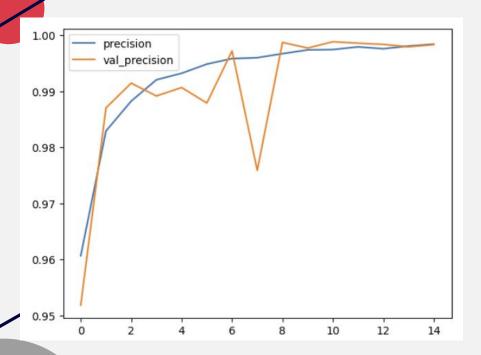
- CNN2 Accuracy scores by classes:
 - O N: 0.991
 - S: 0.809
 - V: 0.960
 - o F: 0.855

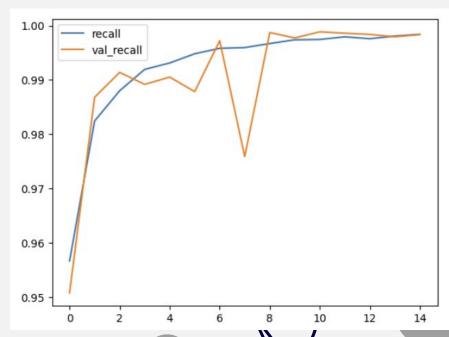
SVM Overall accuracy scores: 0.9485

- SVM Accuracy scores by classes:
 - o N: 0.950
 - o S: 0.904
 - O V: 0.954
 - o F: 0.957

The CNN scored slightly better than the SVM, and both had high testing scores, meaning the models generalize well to new data.

Precision, Recall-CNN1

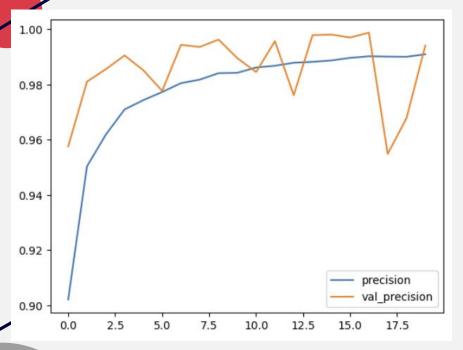


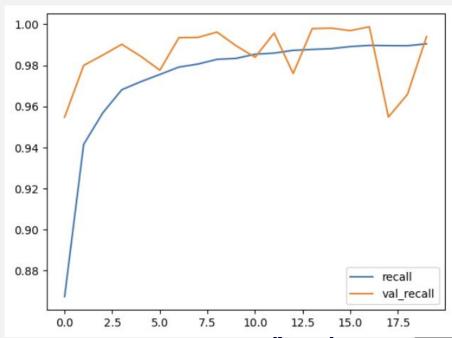


Precision Graph: 0.9987 at Epoch 15

Recall Graph: 0.9987 at Epoch 15

Precision, Recall-CNN2



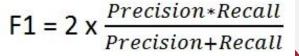


Precision Graph: 0.9890 at Epoch 20

Recall Graph: 0.9884 at Epoch 20

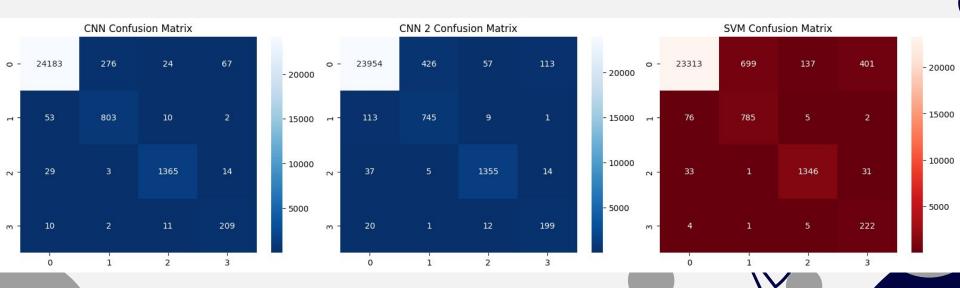
Precision, Recall — SVM

			precision	recall	f1-score
 Normal beats (N) Supraventricular e Ventricular ectopic Fusion beats (F) 	•	0 1 2 3	1.00 0.53 0.90 0.34	0.95 0.90 0.95 0.96	0.97 0.67 0.93 0.50
	accurad macro av	/g	0.69 0.97	0.94 0.95	0.95 0.77 0.96



Confusion Matrix

- Shows for each class the amount of correct and incorrect classifications
- x axis: actual class, y axis: predicted class





Sensitivity/Specificity

$$Sensitivity = \frac{True\ Positives}{True\ Positives + False\ Negatives}$$

$$Specificity = \frac{True\ Negatives}{True\ Negatives + False\ Positives}$$

- Sensitivity (recall): Sensitivity or recall refers to a test's ability to designate an individual with disease as positive. (Known as True Positive Rate)
- Specificity: The specificity of a test is its ability to designate an individual who does not have a disease as negative. (Known as True Negative Rate)



Findings: Sensitivity/Specificity

CNN1	CNN2	<u>SVM</u>
CIVILI	CIVINE	<u>3 V IVI</u>

class	sensitivity	specificity
0	0.953007	0.989124
1	0.991181	0.900922
2	0.998441	0.970234
3	0.998845	0.892241
Avg:	0.985	0.938

class	sensitivity	specificity
0	0.952210	0.984114
1	0.989310	0.898618
2	0.997778	0.964564
3	0.996683	0.922414
Avg:	0.984	0.942

class	sensitivity	specificity
0	0.954998	0.949613
1	0.973237	0.904378
2	0.994269	0.953933
3	0.983823	0.956897
Avg:	0.976	0.941

Summary

	Accuracy	Precision	Recall	Specificity	Time
CNN1	0.9987	0.9984	0.9984	0.938	10 mins
CNN2	0.9818	0.9819	0.9818	0.942	9 mins
SVM	0.9485	0.97	0.95	0.941	29 mins



Pros/Cons



CNN

- Takes less time to train
- Slightly more accurate
- Is more precise across all classes
- Is less accurate for some classes
- Can create non-linear decision boundaries

SVM

- Takes longer to train
- Still very accurate (0.95)
- Is not precise across all classes
- Accuracy is consistent across all classes
- Can only transformed using the kernel function



Conclusions / Recommendations

- After using both CNN and SVM models to classify arrhythmia data, we conclude that the CNN is a more effective classification model than the SVM. This is because the CNN takes less time to run than the SVM while also having scoring higher in measures of model accuracy.
- Therefore, for classification of different types of heartbeats, we would recommend using a convolutional neural network.



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Appendix

l desc	cription
Not an actual and	notation
Norr	mal beat
Left bundle branch blo	
Right bundle branch blo	ock beat
Aberrated atrial premate	ure beat
/ Premature ventricular conf	traction
Fusion of ventricular and norm	mal beat
Nodal (junctional) premate	ure beat
A Atrial premature cont	traction
5 Premature or ectopic supraventricula	lar beat
Ventricular esca	ape beat
j Nodal (junctional) esca	ape beat
	ced beat
Q Unclassifiab	ble beat
Signal quality	y change
Isolated QRS-like	artifact
	T change
	e change
*	Systole
]	Diastole
" Comment and	notation
= Measurement and	notation
P-wa	ave peak
B Left or right bundle brand	
Non-conducted pace	
	ave peak
	m change
	ave peak
	Learning
! Ventricular flut	
Start of ventricular flutter/fibr:	
End of ventricular flutter/fibr	
Atrial esca	
Supraventricular esca	
Link to external data (aux_note conta:	
Non-conducted P-wave (block	
f Fusion of paced and norm	
	rm onset
	form end
R-on-T premature ventricular conf	
on a premature venter reutal con-	

