

Biological Tissue Movement

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The mitral valve, also known as the bicuspid valve or left atrioventricular valve, is a valve with two flaps in the heart, that lies between the left atrium and the left ventricle. The mitral valve and the tricuspid valve are known collectively as the atrioventricular valves because they lie between the atria and the ventricles of the heart.

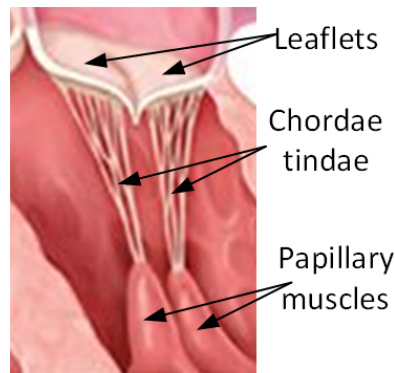


Figure 1: Mitral valve structure

Mitral valve has cyclic working conditions. In normal conditions, blood flows through an open mitral valve during diastole with contraction of the left atrium, and the mitral valve closes during systole with contraction of the left ventricle. The valve opens and closes because of pressure differences, opening when there is greater pressure in the left atrium than ventricle, and closing when there is greater pressure in the ventricle than atrium. In abnormal conditions, blood may flow backwards through the valve (mitral regurgitation) or the mitral valve may be narrowed (mitral stenosis). Rheumatic heart disease often affects the mitral valve; the valve may also prolapse with age, and be affected by infective endocarditis.

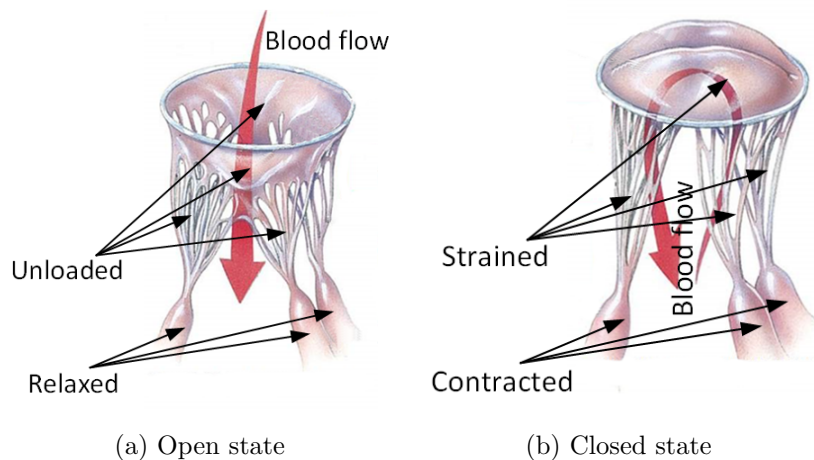


Figure 2: Mitral valve working cycle

Mitral valve prolapse (MVP) is a valvular heart disease characterized by the displacement of an abnormally thickened mitral valve leaflet into the left atrium during systole. By other words, it is a condition

in which the two flaps of the mitral valve doesn't close smoothly and evenly, but instead bulge (prolapse) upward into the left atrium.[1]

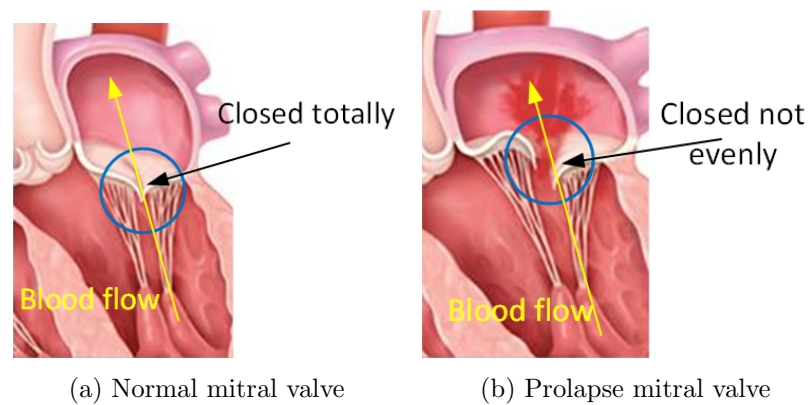


Figure 3: Comparison of the normal valve and prolapse

Providing the surgeon with an anatomically and biomechanically accurate computational model of a particular patient's mitral heart valve could enable preoperative surgical planning and potentially improve surgical outcome.

Research aim

Such physical structure imposes restrictions on the possible tools in the measurement. Another possible problem is the limited number of measurement attempts. Such limitations of physical measurements call into question the possibility of such activities in general. An alternative to physical experiments is the numerical simulation of these experiments. There are a large number of different numerical modeling methods. All of them are derivatives of Finite Element Method(FEM) and Discrete Element Method(DEM).

While general finite-element studies are helpful for the evaluation and development of MV repair surgery, patient-specific models are required for individual therapy planning.

article 1

The patient-specific mass-spring MV model uses a segmentation of 3D TEE images for the initialization of a mass-spring model of the closed MV under systolic pressure. An iterative approach is used to adjust the spring rest-length so that the model can accurately simulate the shape of the closed MV under systolic pressure. To simulate MV annuloplasty, the model can then be deformed, according to the annuloplasty ring to be used, to create a prediction of the shape of the closed MV after surgery.

Based on the properties of the material of biological tissues and review of existing projects, the most appropriate method is Mass - Spring modeling(MSM). This method based on ideas of DEM and basic element here is very know in mechanic simple one dimensional(1D) beam.

have to show so pic about MSM, with explanation what is going on

Computational complexity of MSM is much less compare to FEM-based methods, because of less number of equations to integrate on each time step. This important advantage and physics way have method describes basic element gave to MSM very wide using in computer games for calculating reality-looks hair or cloth movement in real time. Modelling by using MSM could be parallel calculated on each time step.[2] [3]

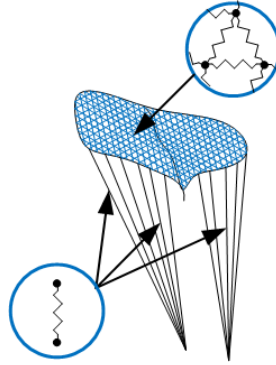


Figure 4: Displacement of papillary muscle over cardiac cycle

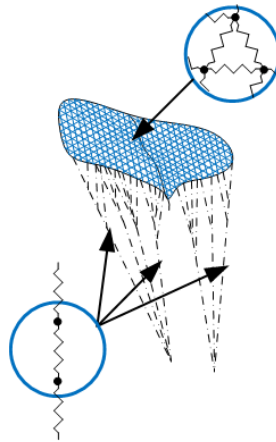


Figure 5: Displacement of papillary muscle over cardiac cycle

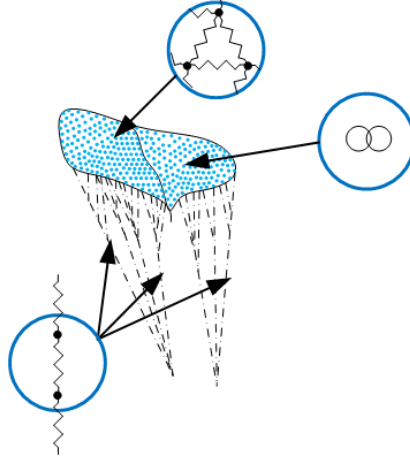


Figure 6: Displacement of papillary muscle over cardiac cycle

Mechanic equivalent of fibrous tissue could be described as system of 1D rods. Example of such flat 2D system are shown on figure 8.

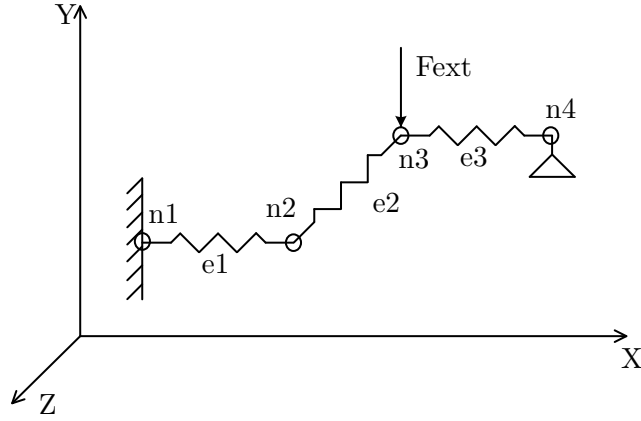


Figure 7: 1D Rod system in global coordinate system

System consists of discrete elements e_1 , e_2 and e_3 . All elements are connected to each other through nodes n_2 , n_3 and to special points through n_1 and n_4 . Each element e_n of system has own orientation in global coordinate system. From schematic representation of node comes that all vector variables of node should be calculated in global coordinate system and element variables in own local coordinate system (figure 8). For transformation between coordinate systems direction cosine matrix (DCM)(1) can be used.

$$DCM = \begin{bmatrix} \cos(X, x) & \cos(X, y) & \cos(X, z) \\ \cos(Y, x) & \cos(Y, y) & \cos(Y, z) \\ \cos(Z, x) & \cos(Z, y) & \cos(Z, z) \end{bmatrix} \quad (1)$$

where $\{X, Y, Z\}$ is global coordinate system and $\{x, y, z\}$ is local coordinate system.

According to primitive scheme of node 8, mass of each node can be calculated, like sum of half mass of each element, which acting in node. $m_n = \sum_e m_e / 2$

In case that node does not have external interrupt, like pressure or other applied force, schematic represent of node can be as on figure 8.

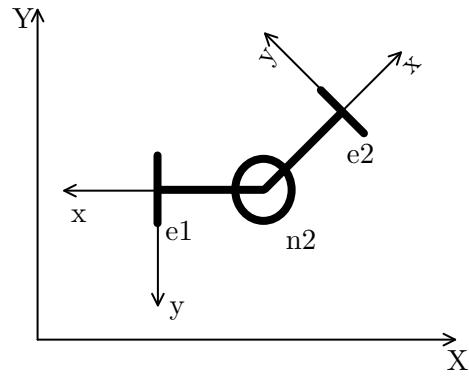


Figure 8: Extracted node from system

Mathematical model of discrete system is expressed by equations of nodes motion. As elements are 1D, nodes will be 1D as well. All system acting in global coordinate system $\{X, Y, Z\}$ and each element acting in own local coordinate system $\{x, y, z\}$.

Mass Spring Model

Linear deformation

For investigating motion of any mechanical system comes to integration motion equation of discrete parts of this system. In case of MSM, system described as nodes connected to each other by 1D rod elements⁸. (5). For this propose need to express all acting forces in node(2) for each node in relation to their application place.

$$\vec{F}_n = \vec{F}_{ext} + \sum \vec{F}_{elem} \times [DCM] + \vec{F}_{press} \times [DCM] \quad (2)$$

F_{ext} is external load force, applied to node in global coordinates. Value of this force for each time step is loaded from list of loads.

F_{press} is external pressure and can be described like force applied to element in local coordinates.

F_{elem} is sum of internal forces of each element, which acting in node. From each element counts only half of force to node, other half going to neighbour node. In case of 1D element system, internal force of each element can be express like axial force and it is equal to integral of stress over area:

$$N(x) = \int_A \sigma dA \quad (3)$$

For 1D rod system F_{elem} can be expressed like:

Is it has to be divided by 2? in this case how to calc mass of node?

$$F_{elem} = \sum_e N_e(x)/2 \quad (4)$$

The motion of nodes can be expressed by Newton's equation of motion⁵. As 1D element was selected as discrete element, only the normal component of the translational motion is considered, the equation reduces to

$$m\ddot{x} + k\dot{x} + c\ddot{x} = \vec{F}_n \quad (5)$$

where F_n is force acting in node n , m – mass of node and \ddot{x} is acceleration, k – stiffness coefficient of node, x is displacement of node and c – damping coefficient of node, \dot{x} is velocity of node, initial conditions are: $x(0) = 0$ and $\dot{x}(0) = V_0$. According to 2, kx are described by $\sum F_{elem}$, $c\dot{x}$ are described by F_{press} and motion equation will become to:

$$\vec{F}_{press} + \sum F_{elem} + m\ddot{x} = \vec{F}_n \quad (6)$$

where F_{elem} is sum of node's elements forces, m – mass of node and \ddot{x} is acceleration. In static case $m\ddot{x}$ equal to zero, due zero acceleration, because no external force is applied and equation of node is balanced. But if external force are applied, motion will start, motion equation will become not balanced⁷, mass start to act as inertia.

$$\vec{F}_{press} + \sum \vec{F}_{elem} + m\ddot{x} = F_n + \vec{F}_{ext} \quad (7)$$

Equations of motion for Euler's scheme of integration can be described like:

$$\ddot{x}(t + \Delta t) = \vec{F}_n/m \quad (8)$$

$$\dot{x}(t + \Delta t) = \dot{x}(t) + \ddot{x}(t)\Delta t \quad (9)$$

$$x(t + \Delta t) = x(t) + \dot{x}(t)\Delta t \quad (10)$$

Element force becomes from physical deformation of element. In linear case of study, deformation of element much less compare to element dimensions. It is expressed by linear geometry equation(11), which showing relation between initial length of element and length in Δt state.

$$\varepsilon = \frac{dU}{dx} = \frac{l(\Delta t) - l(t)}{l(t)} \quad (11)$$

According to Hook law $\sigma = \varepsilon E$ and linear geometry equation (11), inner force can be described as:

$$N(x) = \int_{Al} \varepsilon E dl dA = EA \int_l \varepsilon dl = \frac{EA}{l(t)} * (l(t + \Delta t) - l(t)) \quad (12)$$

where $l(\Delta t)$ is current length of element, $l(t)$ length of element at previous time moment, E – Young's modulus for element material, A – volume of element. To be able to integrate equation of motion, need to express deformation in equation (12) by differences between displacements of nodes, to which element is connected:

$$N(x) = \frac{EA}{l(t)} * (x_i(t) - x_j(t)) \quad (13)$$

To words about mechanical properties of valve components, poisson ratio ν is same, 0.49 for all. Mean value of chordae length L 0,025m and diameter d 0,001m. Chordae has density $\rho = 1040$ kg/m³ and stiffness $E = 2000$ N/m, when leaflets has $\rho = 1.06$ E3 kg/m³ and $E = 2$ MPa (Anterior leaflet), $E = 1$ MPa (Posterior leaflet)

Let's try to describe minimal possible way to get simulation of such structure as shown on figure 7.

```

initialization;
// Preform integration nodes movement over time
// Initial state is  $x(0) = \dot{x}(0) = \ddot{x}(0) = 0$ 
// Iterate over time
while  $t < t_{end} - 1$  do
    // Iterate over nodes
    foreach node in nodes do
        // get external force loading
         $F_{ext} = \text{getFext}(\text{node}, t)$ ;
        // push  $F_{ext}$  into current node force  $F_n$ 
         $F_n = F_n + F_{ext}$ ;
        // calc  $F_{elm}$  from previous displacement
        foreach link in neighbours do
             $F_{elm} = \text{getFelm}(\text{node}, \text{link})$ ;
            // convert  $F_{elm}$  from local to global coordinates
             $F_{elm}G = F_{elm} \times [DCM]$ ;
            // push  $F_{elm}G$  into current node force  $F_n$ 
             $F_n = F_n + F_{elm}G$ ;
        end
        // calc pressure force
         $F_{press} = \text{getFpress}(\text{node}, t)$ ;
        // convert  $F_{elm}$  from local to global coordinates
         $F_{press}G = F_{press} \times [DCM]$ ;
        // push  $F_{elm}G$  into current node force  $F_n$ 
         $F_n = F_n + F_{press}G$ ;
        // integrate collected  $F_n$  to get derivatives of  $x$  for  $t + \Delta t$ 
         $[x(t + \Delta t), \dot{x}(t + \Delta t), \ddot{x}(t + \Delta t)] = \text{integrate}(F_n, x(t), \dot{x}(t), \ddot{x}(t))$ 
    end
end
end

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Integration schemes

Euler first order explicit

$$\begin{aligned} v(t + \Delta t) &= v(t) + a(t) * \Delta t \\ x(t + \Delta t) &= x(t) + v(t) * \Delta t \end{aligned} \quad (14)$$

The central difference scheme, also known as velocity Verlet is a very widely used integration method of second order. This was initially proposed by Cundall and Strack (1979) and adopted by several other authors. Velocities in the upcoming time step $t + \Delta t/2$ and positions at $t + \Delta t$ are calculated as

$$\begin{aligned} v(t + \Delta t/2) &= v(t + \Delta t/2) + a(t - \Delta t/2) * \Delta t \\ x(t + \Delta t) &= x(t) + v(t + \Delta t/2) * \Delta t \end{aligned} \quad (15)$$

predictor–corrector schemes very commonly used for molecular dynamics and discrete element applications are Gear’s schemes. They are based on three stages, whereas in addition to the predictor and corrector step known from the Adams-method an evaluation step is added. Schemes considered here are the third order Gear’s method (GPC3) and the fourth order Gear’s method (GPC4). In the prediction step positions and their higher derivatives are calculated based on Taylor series expansions as

$$\begin{aligned} c(t + \Delta t, p) &= c(t) \\ b(t + \Delta t, p) &= b(t) + c(t) * \Delta t \\ a(t + \Delta t, p) &= a(t) + b(t) * \Delta t + \frac{1}{6} * c(t) * \Delta t^2 \\ v(t + \Delta t, p) &= v(t) + a(t) * \Delta t + \frac{1}{2} * b(t) * \Delta t^2 + \frac{1}{6} * c(t) * \Delta t^3 \\ x(t + \Delta t, p) &= x(t) + v(t) * \Delta t + \frac{1}{2} * a(t) * \Delta t^2 + \frac{1}{6} * b(t) * \Delta t^3 + \frac{1}{24} * c(t) * \Delta t^4 \end{aligned} \quad (16)$$

with the first and second derivative of the accelerations calculated as
for GPC3:

$$b(t) = \frac{\Delta a(t)}{\Delta t} \quad (17)$$

$$c(t) = 0$$

for GPC4:

$$\begin{aligned} b(t) &= \frac{\Delta a(t)}{\Delta t} \\ c(t) &= \frac{\Delta b(t)}{\Delta t} \end{aligned} \quad (18)$$

In the evaluation step the difference in the accelerations calculated based on the acceleration $a(t + \Delta t, p)$ and the acceleration $a(t + \Delta t)$ calculated from positions $x(t + \Delta t, p)$ and velocities $v(t + \Delta t, p)$ is obtained by

$$\Delta a = a(t + \Delta t) - a(t + \Delta t, p) \quad (19)$$

In the following, correction step positions and their higher derivatives are calculated based on their values from the previous time step and the obtained difference in acceleration as

$$\begin{aligned} x(t + \Delta t) &= x(t + \Delta t, p) + k1 * \Delta a * \Delta t^2 \\ v(t + \Delta t) &= v(t + \Delta t, p) + k2 * \Delta a * \Delta t \\ a(t + \Delta t) &= a(t + \Delta t, p) + k3 * \Delta a \\ b(t + \Delta t) &= b(t + \Delta t, p) + k4 * \frac{\Delta a}{\Delta t} \\ c(t + \Delta t) &= c(t + \Delta t, p) + k5 * \frac{\Delta a}{\Delta t^2} \end{aligned} \quad (20)$$

Gear's scheme parameters k1-k5

for GPC3: $k_1 = 1/12, k_2 = 5/12, k_3 = 1, k_4 = 1, k_5 = 0$

for GPC4: $k_1 = 19/240, k_2 = 3/8, k_3 = 1, k_4 = 3/2, k_5 = 1$

Results

List of literature

- [1] Emil Hayek, Christian N Gring, and Brian P Griffin. “Mitral valve prolapse”. In: *The Lancet* 365.9458 (Feb. 2005), pp. 507–518. ISSN: 0140-6736. DOI: 10.1016/S0140-6736(05)17869-6. URL: <https://www.sciencedirect.com/science/article/pii/S0140673605178696?via%7B%5C%7D5C=ihub>.
- [2] Allan Rasmusson, Jesper Mosegaard, and Thomas Sangild Sørensen. “Exploring parallel algorithms for volumetric Mass-Spring-Damper models in CUDA”. In: *Lecture Notes in Computer Science (including subseries Lecture Notes in Artificial Intelligence and Lecture Notes in Bioinformatics)*. 2008. ISBN: 3540705201. DOI: 10.1007/978-3-540-70521-5_6.
- [3] Ronan Mendonça Amorim et al. “An electro-mechanical cardiac simulator based on cellular automata and mass-spring models”. In: *Lecture Notes in Computer Science (including subseries Lecture Notes in Artificial Intelligence and Lecture Notes in Bioinformatics)*. 2012. ISBN: 9783642333491. DOI: 10.1007/978-3-642-33350-7-45.