



# Analysis of Electrocardiograms via Artificial Neural Networks For a Reliable Assessment of a Possible Myocardial Infarction

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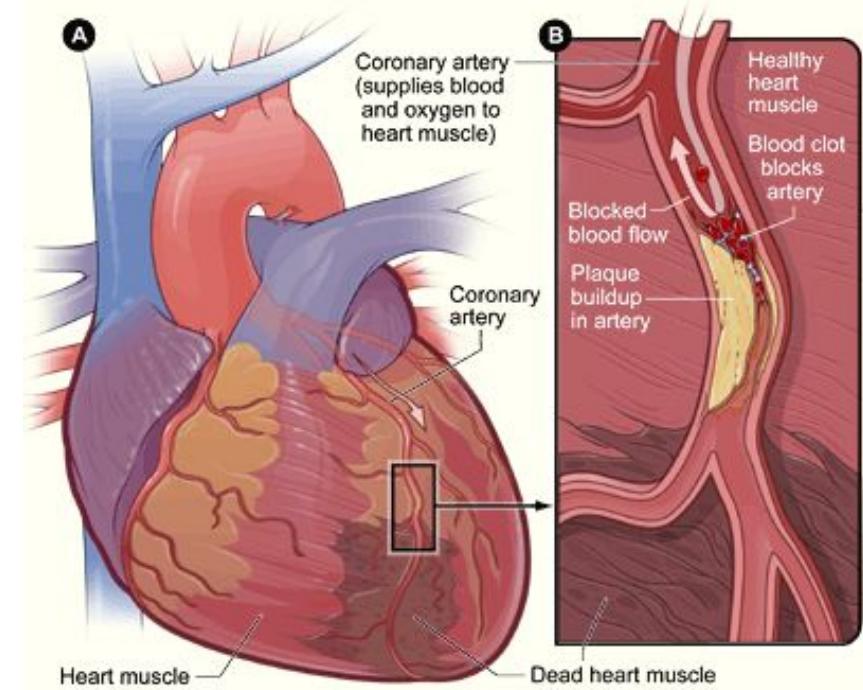
# 1.1 Problem Setting

## What is Myocardial Infarction?

The presence of acute myocardial injury, detected by abnormal cardiac biomarkers in the setting of evidence of acute myocardial ischemia.



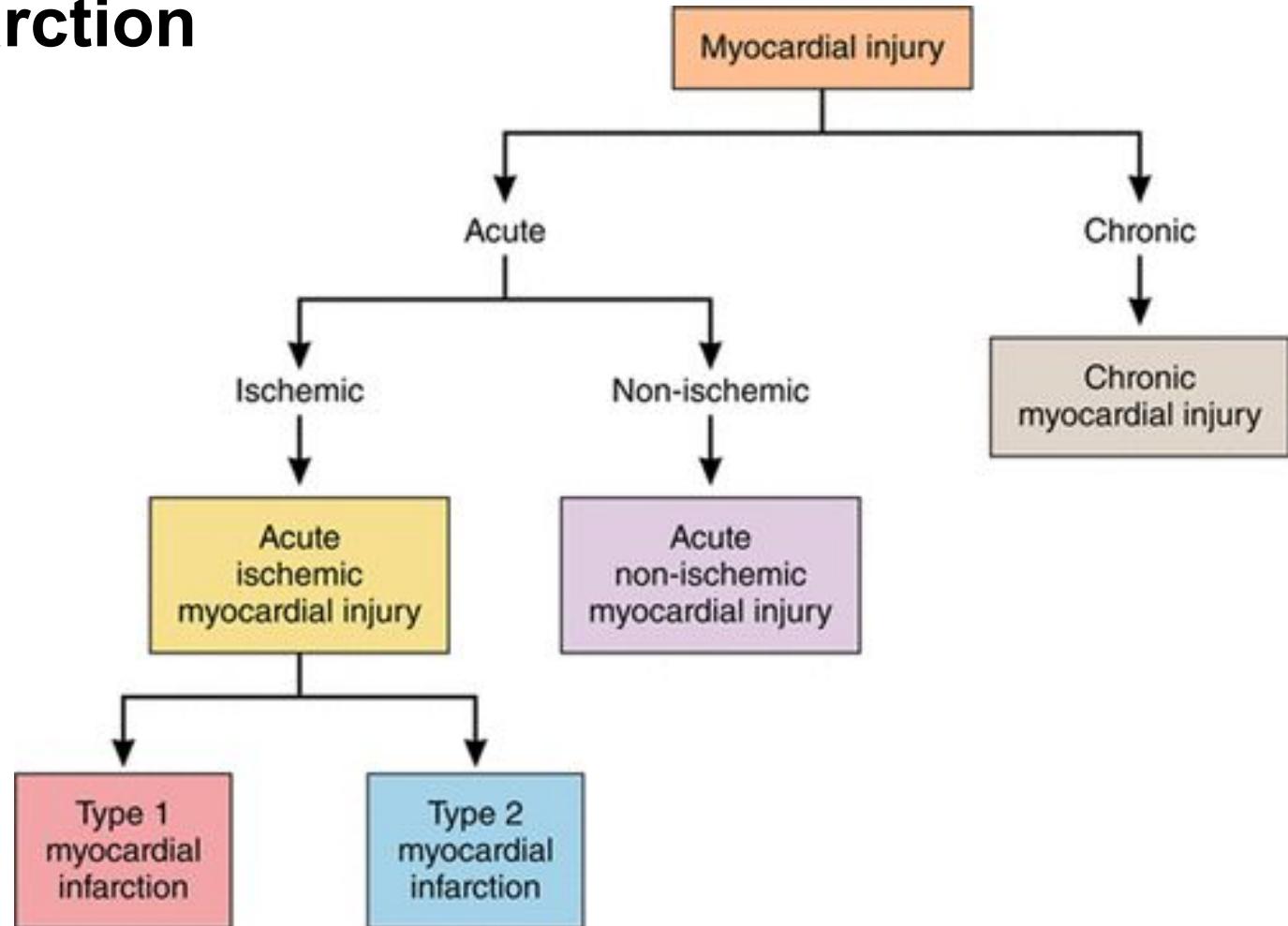
Happens when one or more areas of the heart muscle don't get enough oxygen. This happens when blood flow to the heart muscle is blocked.



# 1.1 Problem Setting

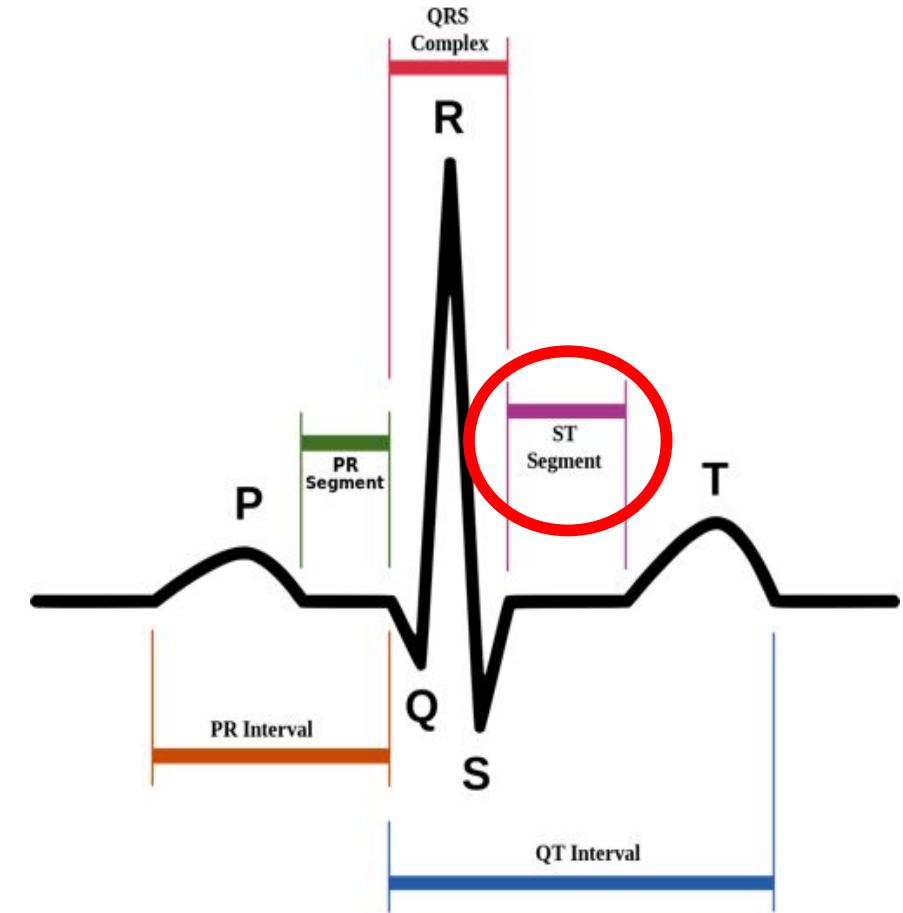
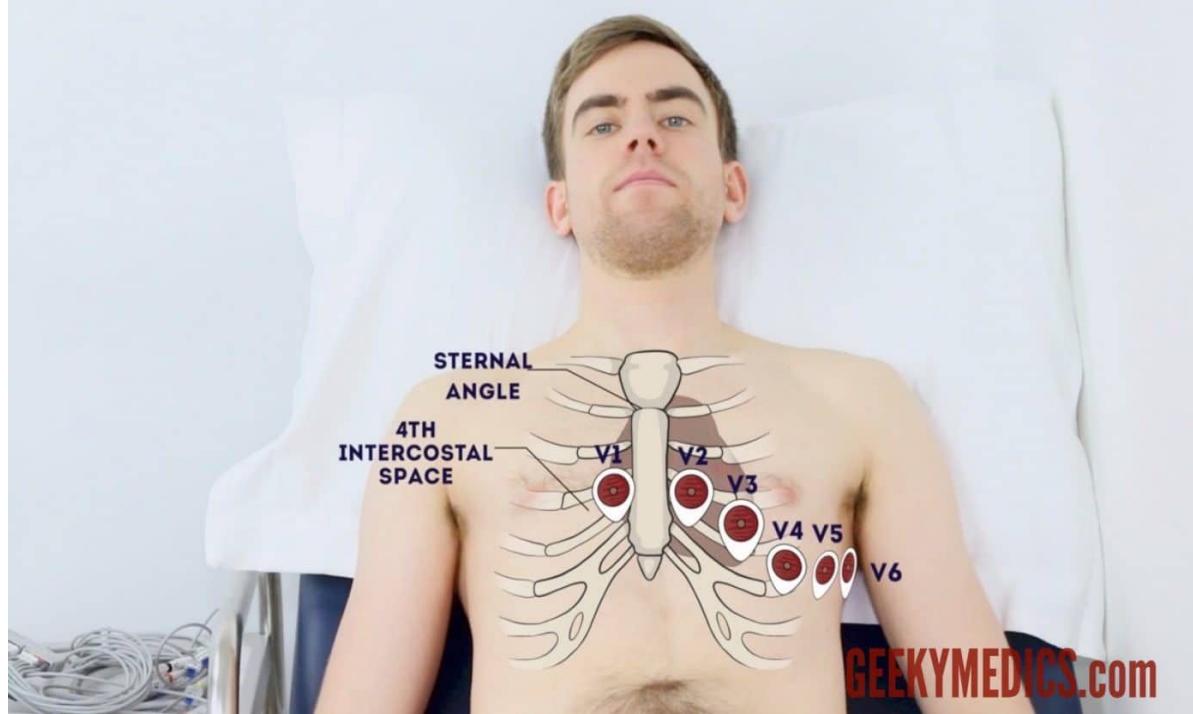
## Subtypes of Myocardial Infarction

**Ischemic?**  
Deficient supply of blood to a body part that is due to obstruction of the inflow of arterial blood.



# 1.1 Problem Setting

How can we detect MI? - ECG data



STEMI: ST-elevation myocardial infarction

NSTEMI: heart attack that usually happens when your heart needs oxygen can't be met

# 1.1 Problem Setting

## How can we detect MI?

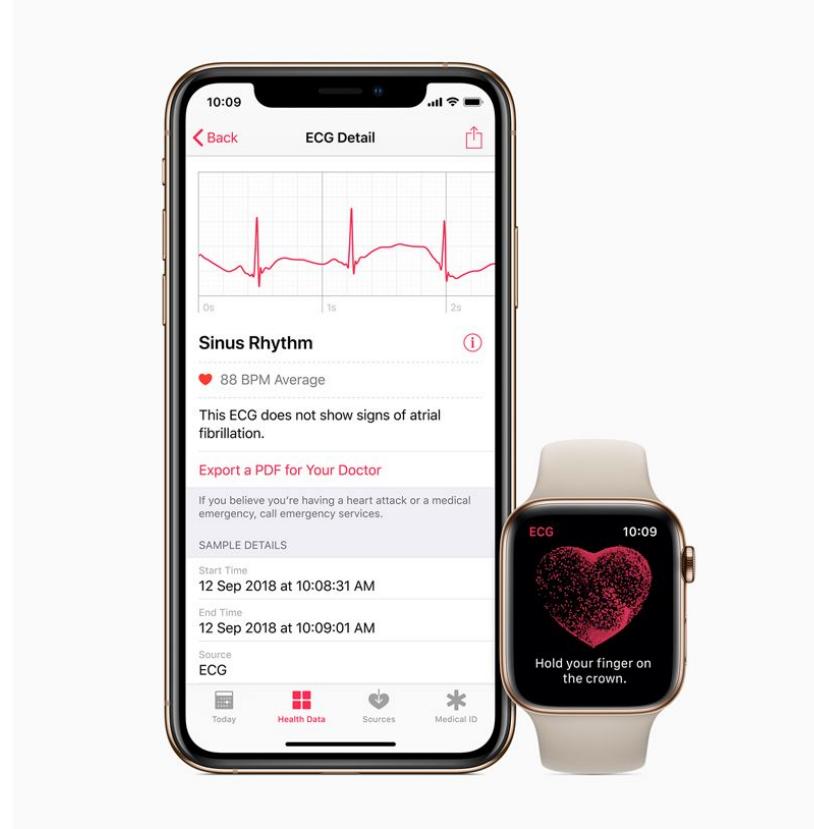


Figure 1) <http://what-when-how.com/paramedic-care/the-monitoring-ecg-clinical-essentials-paramedic-care-part-1>

Figure 2) <https://www.samsung.com/global/galaxy/galaxy-watch4/>

Figure 3) <https://www.apple.com/uk/newsroom/2019/03/ecg-app-and-irregular-rhythm-notification-on-apple-watch-available-today-across-europe-and-hong-kong/>

# 1.2 Project Idea

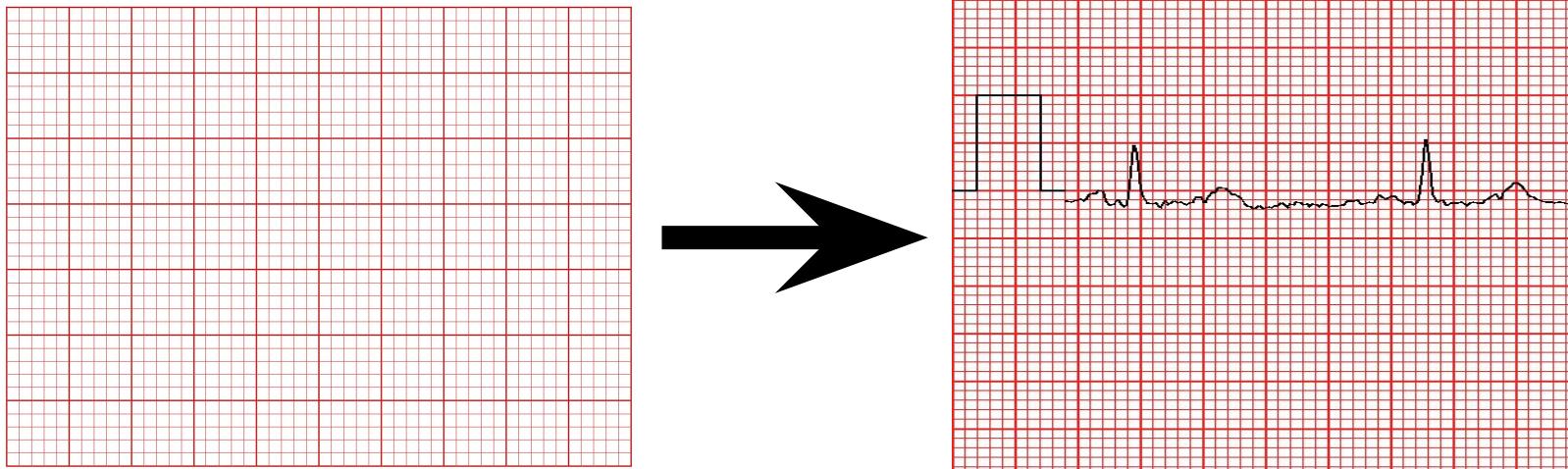
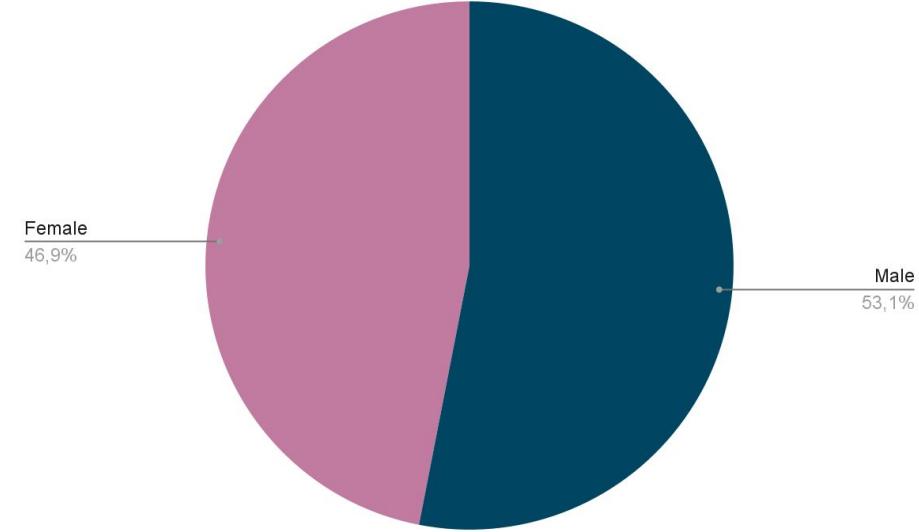
## Why do we need a reliable ECG assessment?



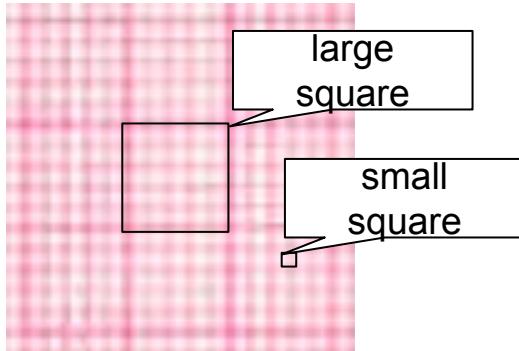
**“In Tanzania, I was involved in training and equipping taxi drivers in the place of ambulances and using motorcycle taxi riders as first responders.”**

## 2.1 Datasets

- PTB-XL ECG dataset
  - 21837 clinical 12-lead ECGs
  - 18885 patients, between 0 and 95 years old
  - 10 second length
  - 71 total different ECG statements conform to the SCP-ECG standards
- Generate new “**PTB-V**” (“PTB-Visualized”) dataset
  - From time series to images
  - Python library “PIL” (Pillow) and the classes `Image` and `ImageDraw`

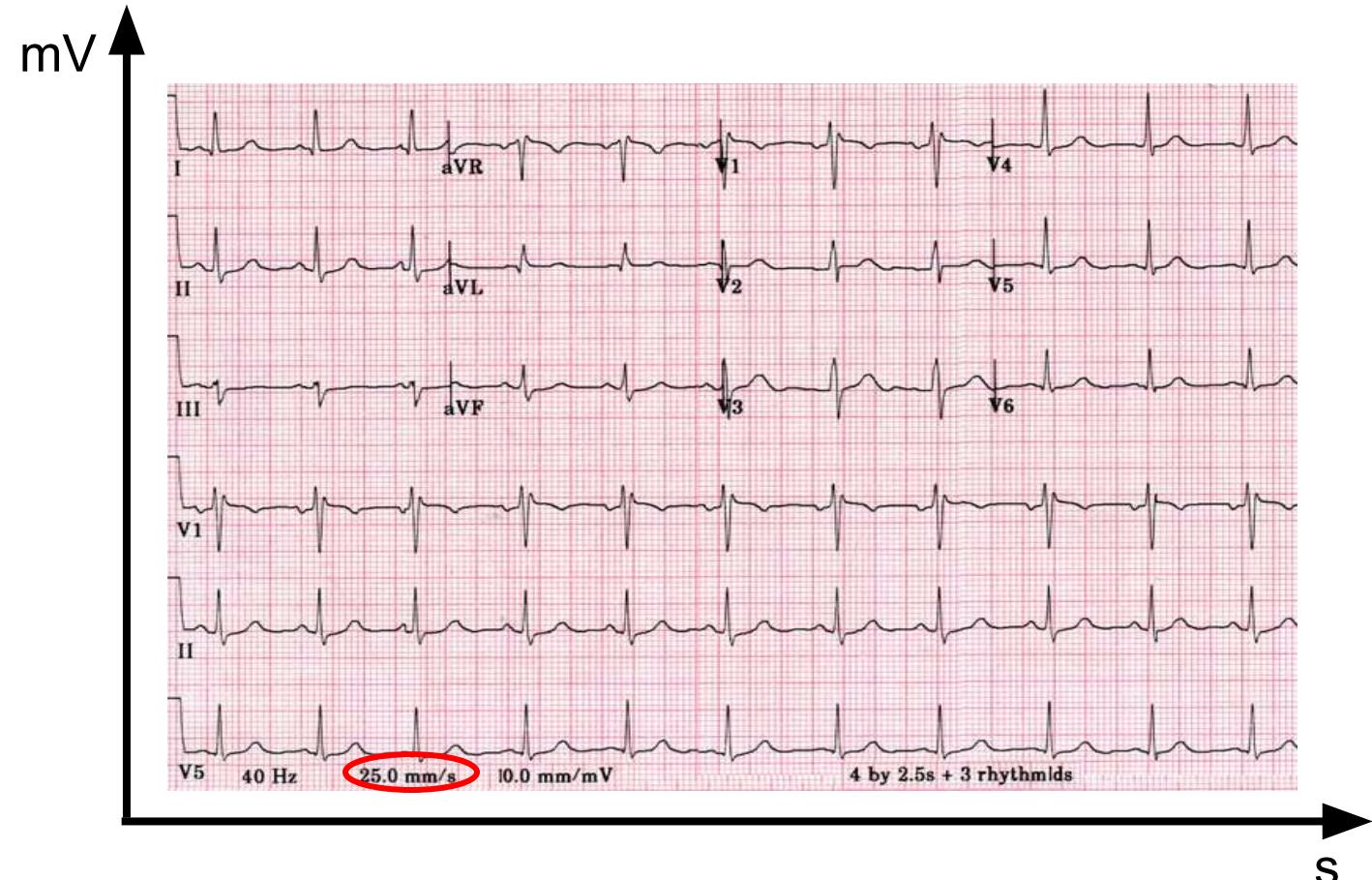


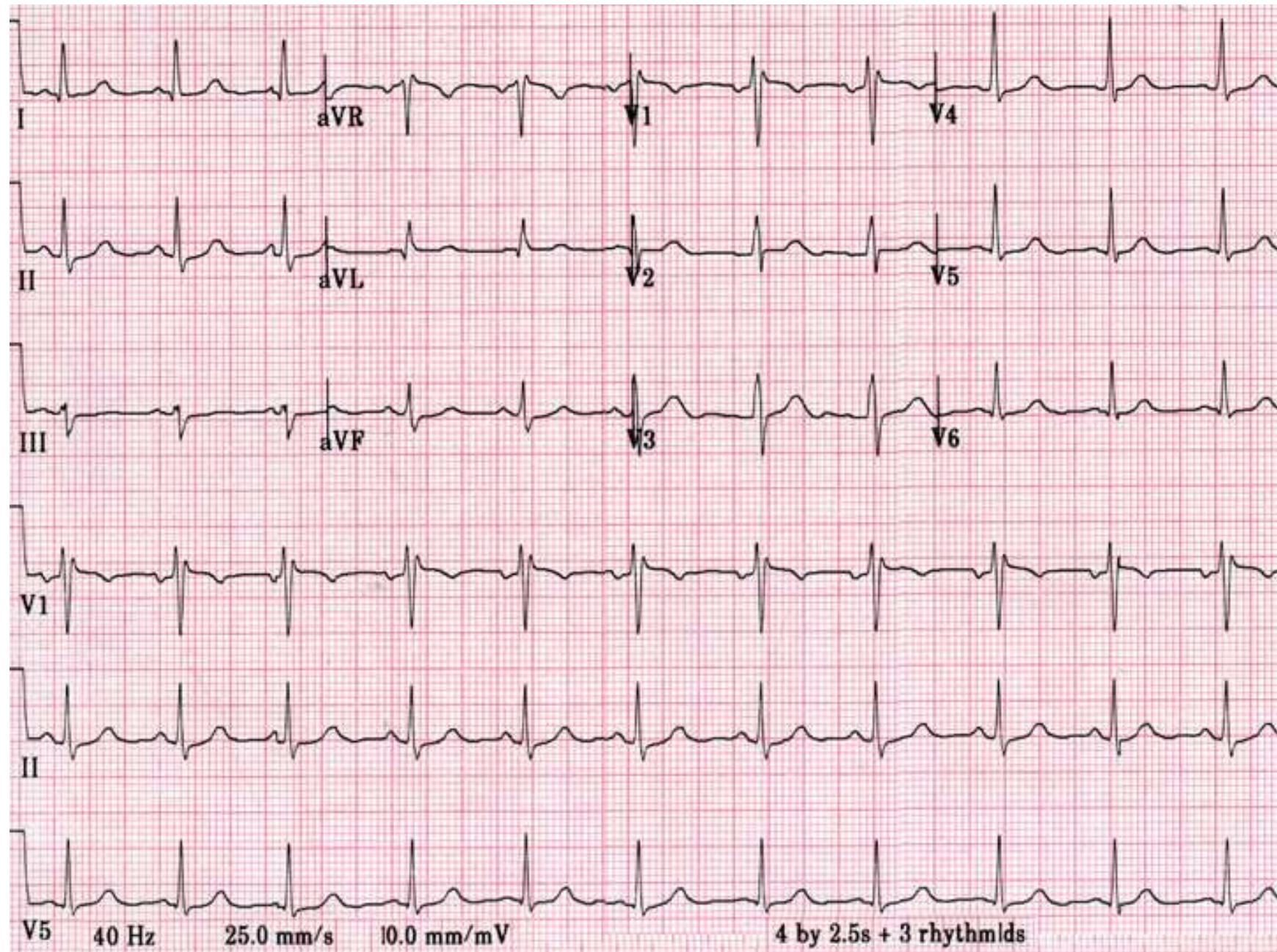
## 2.2 How to Read an ECG



**Default paper speed of 25mm/s:**

- Each small square is  $1 \text{ mm}^2$
- Each small square represents 0.04 s
- Each large square represents 0.2 s
- 5 large squares = 1 s
- 10 squares high = 1 mV

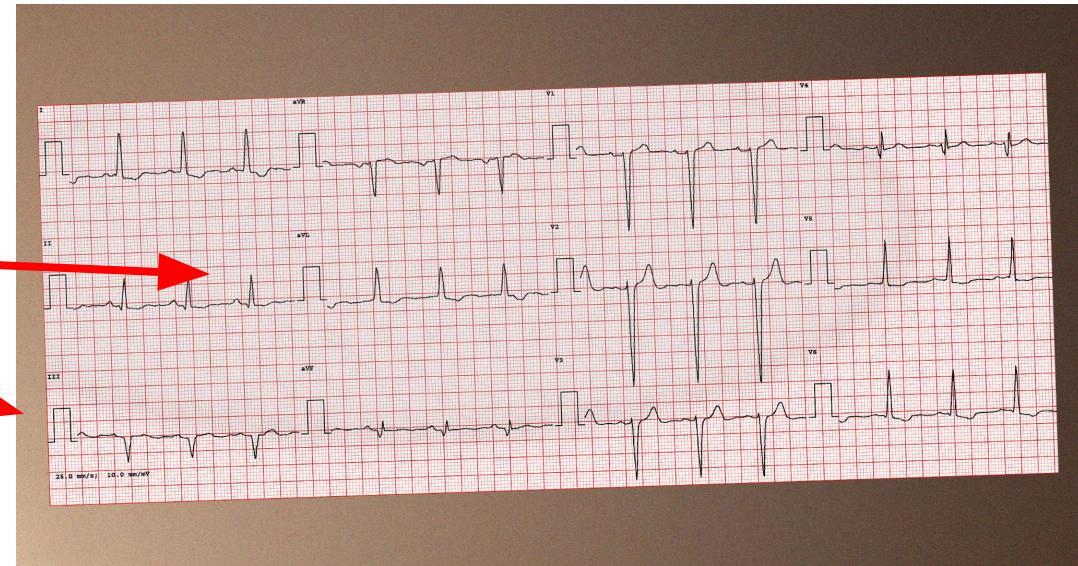
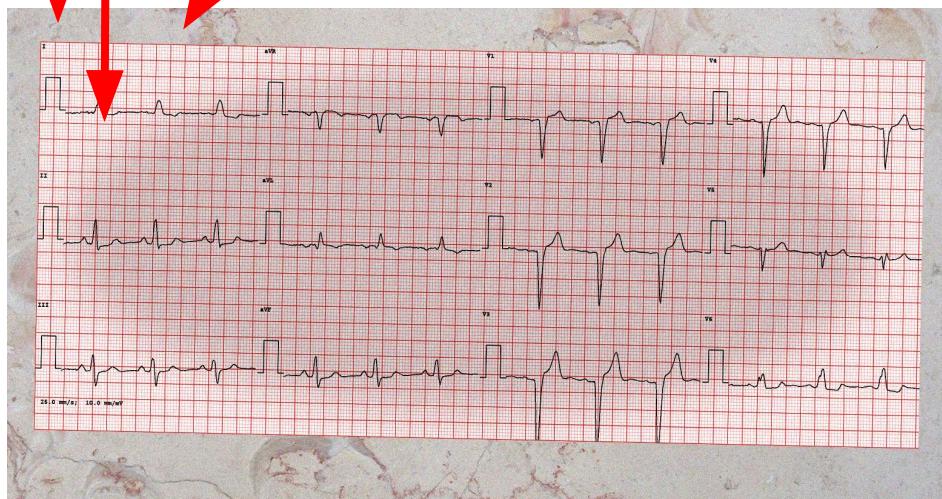




## 2.3 Data augmentation

**Goal** : making the segmentation network more robust to different kinds of inputs

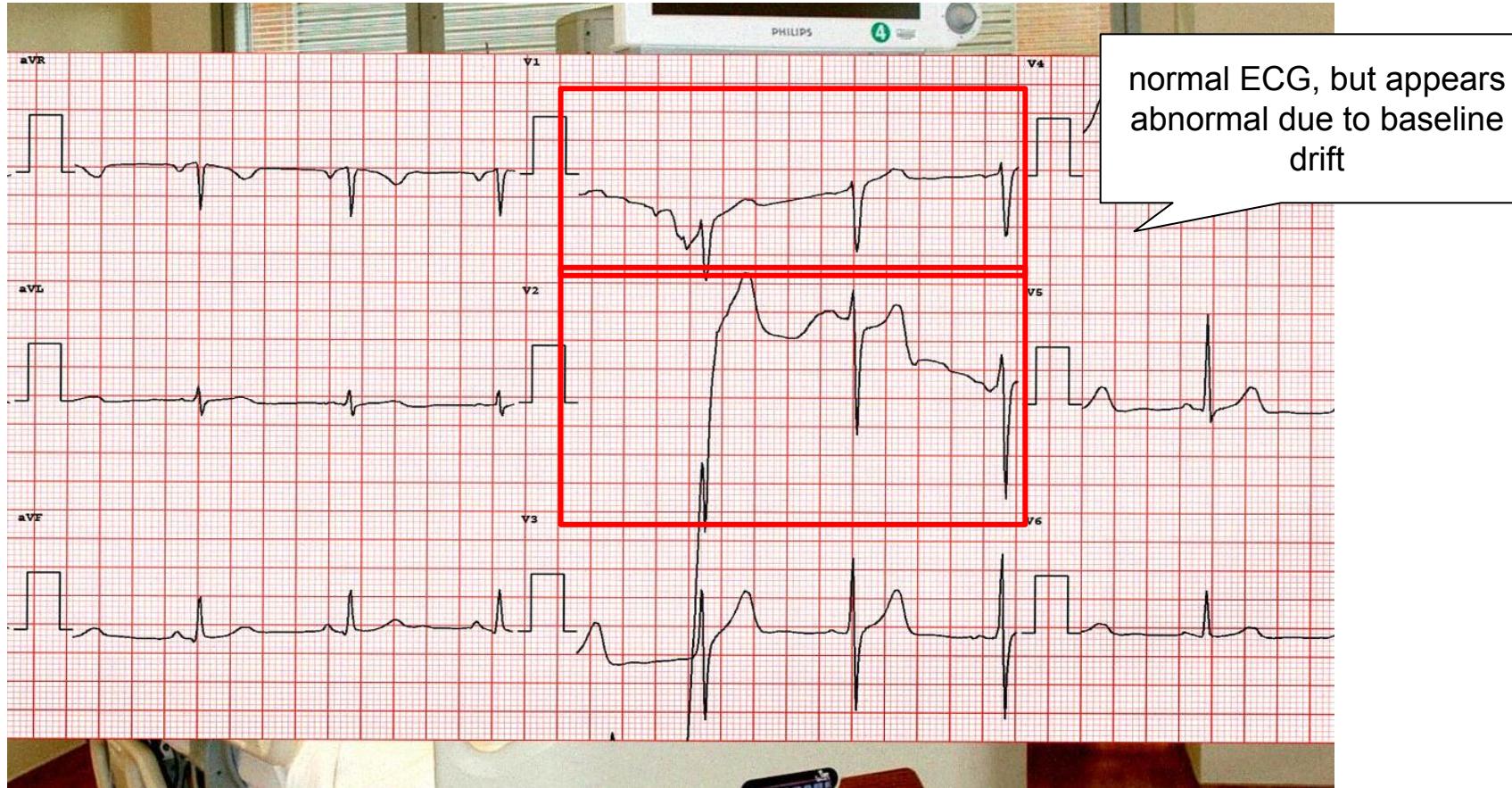
- shearing
- rotation
- blurring
- noise
- shadows and flashes
- different backgrounds



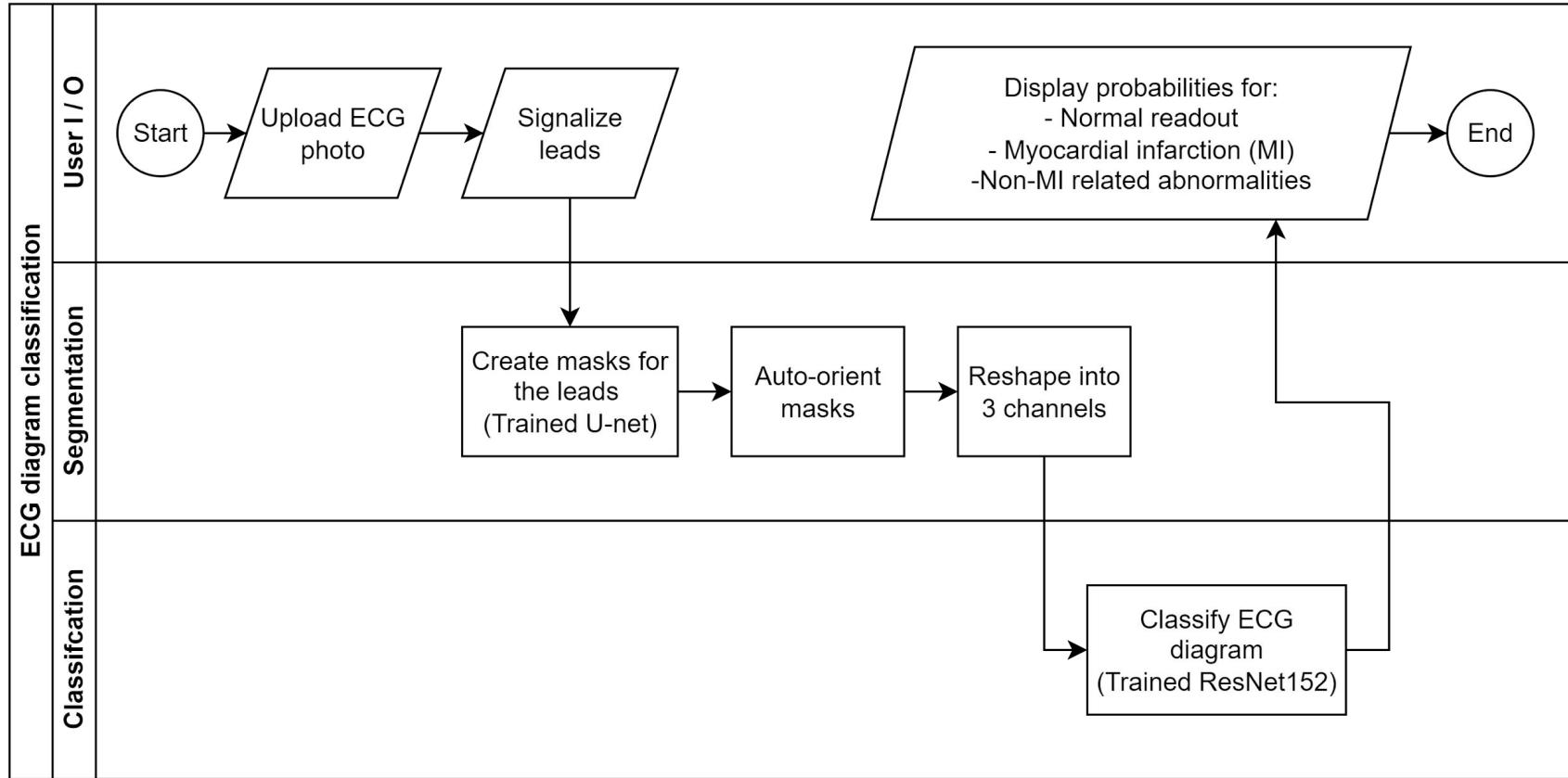
→ as a result we also generate more pictures

## 2.4 Problems with the data

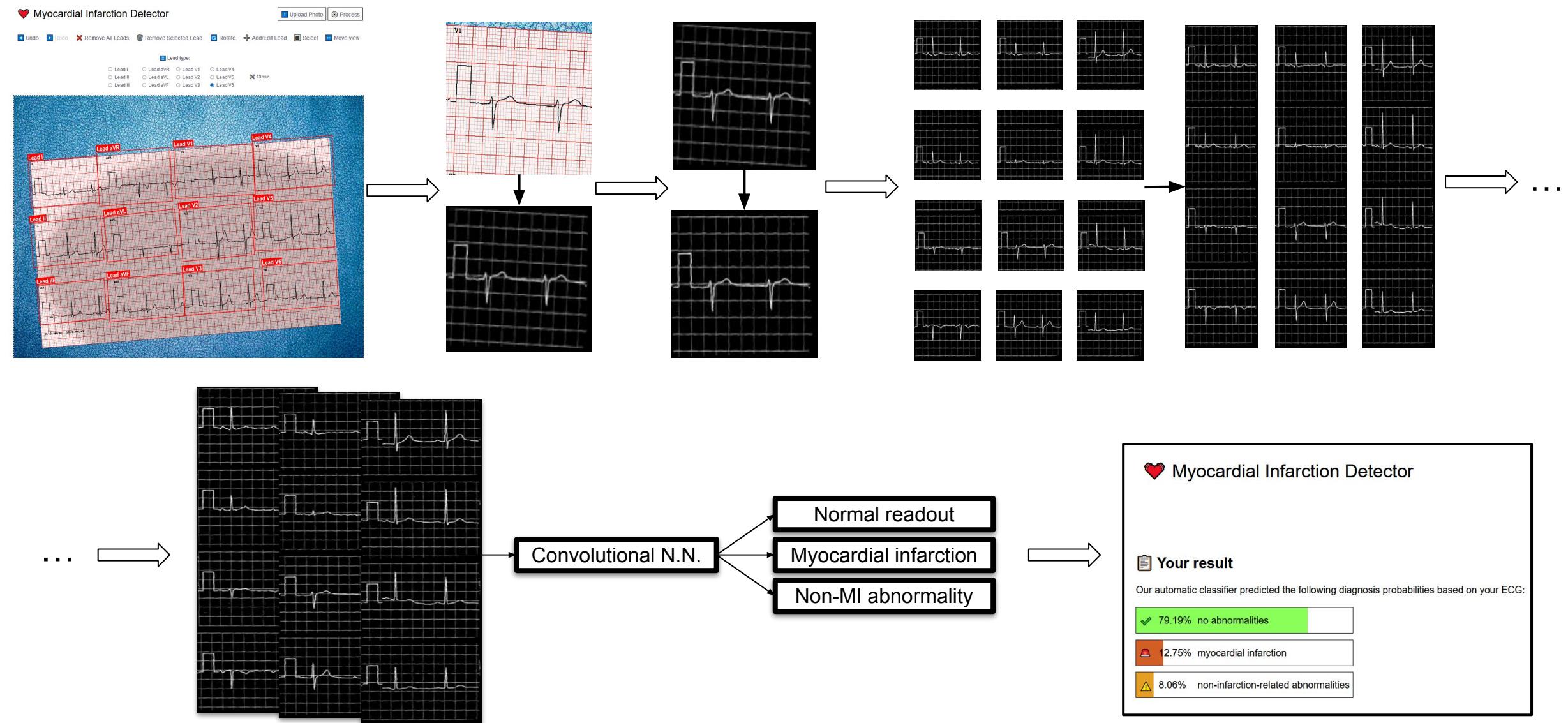
- **Baseline drift:** Patient moving during the measurement



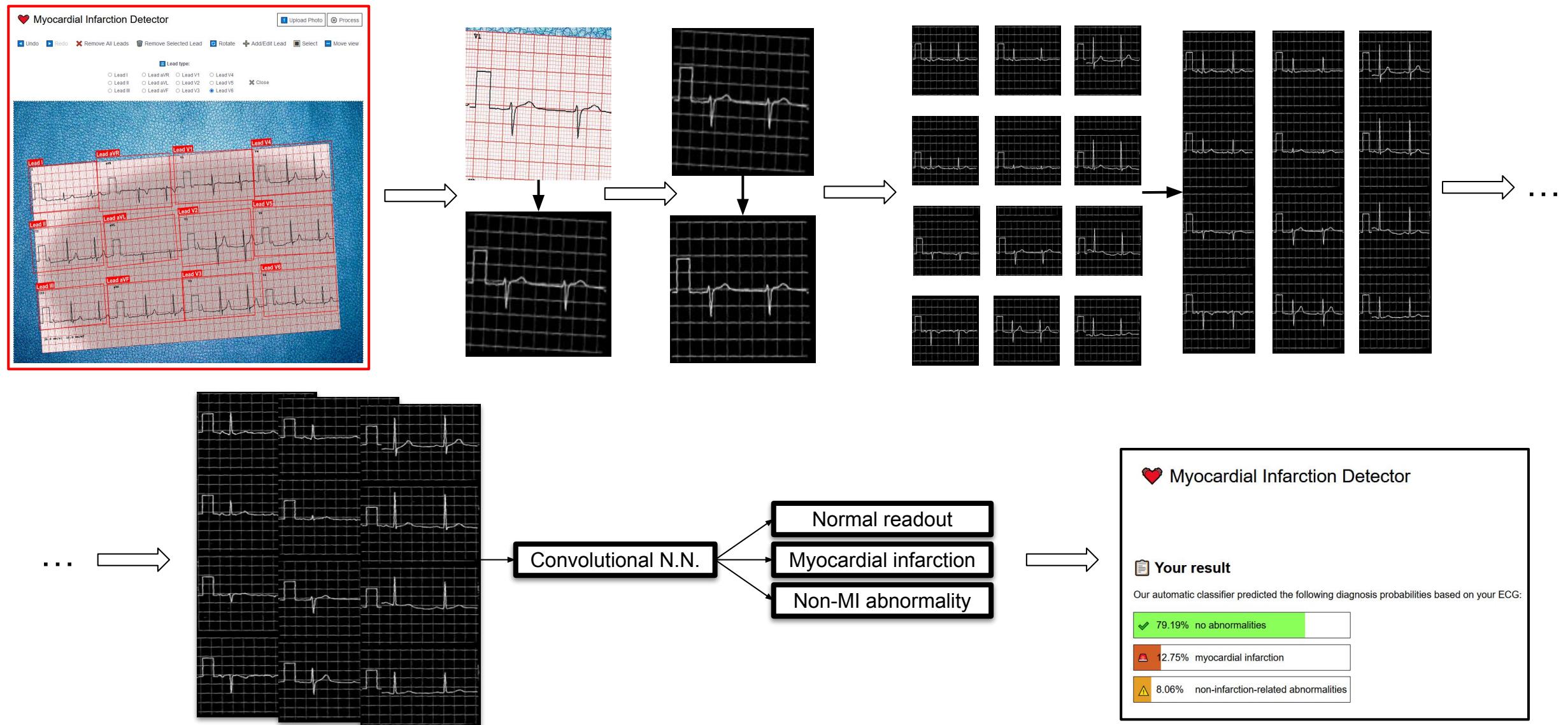
# 3 ECG Processing Overview



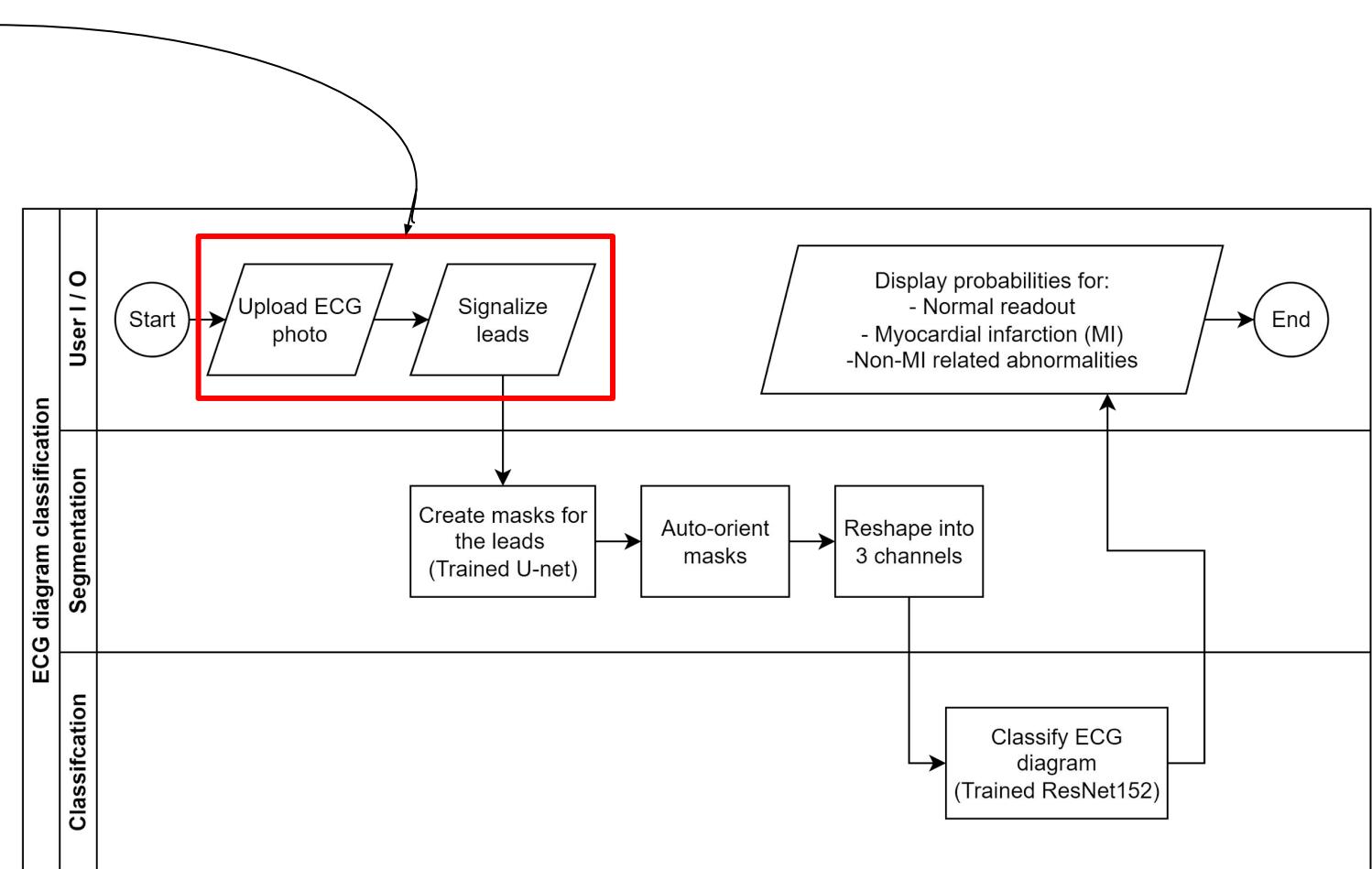
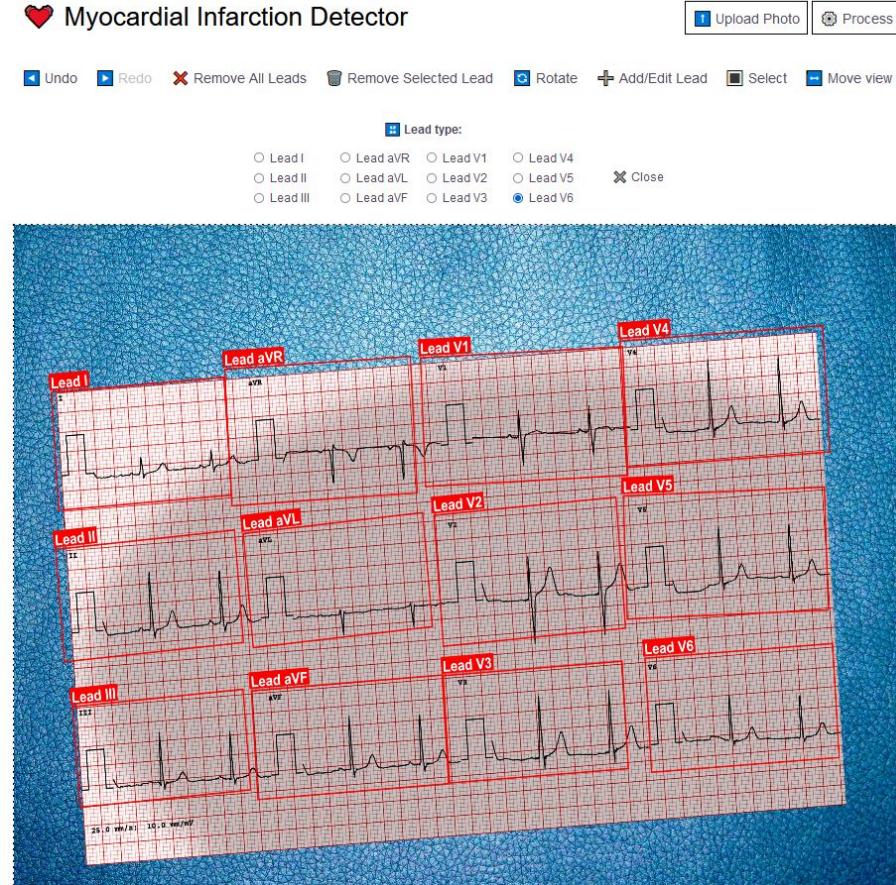
# 3 ECG Processing Overview



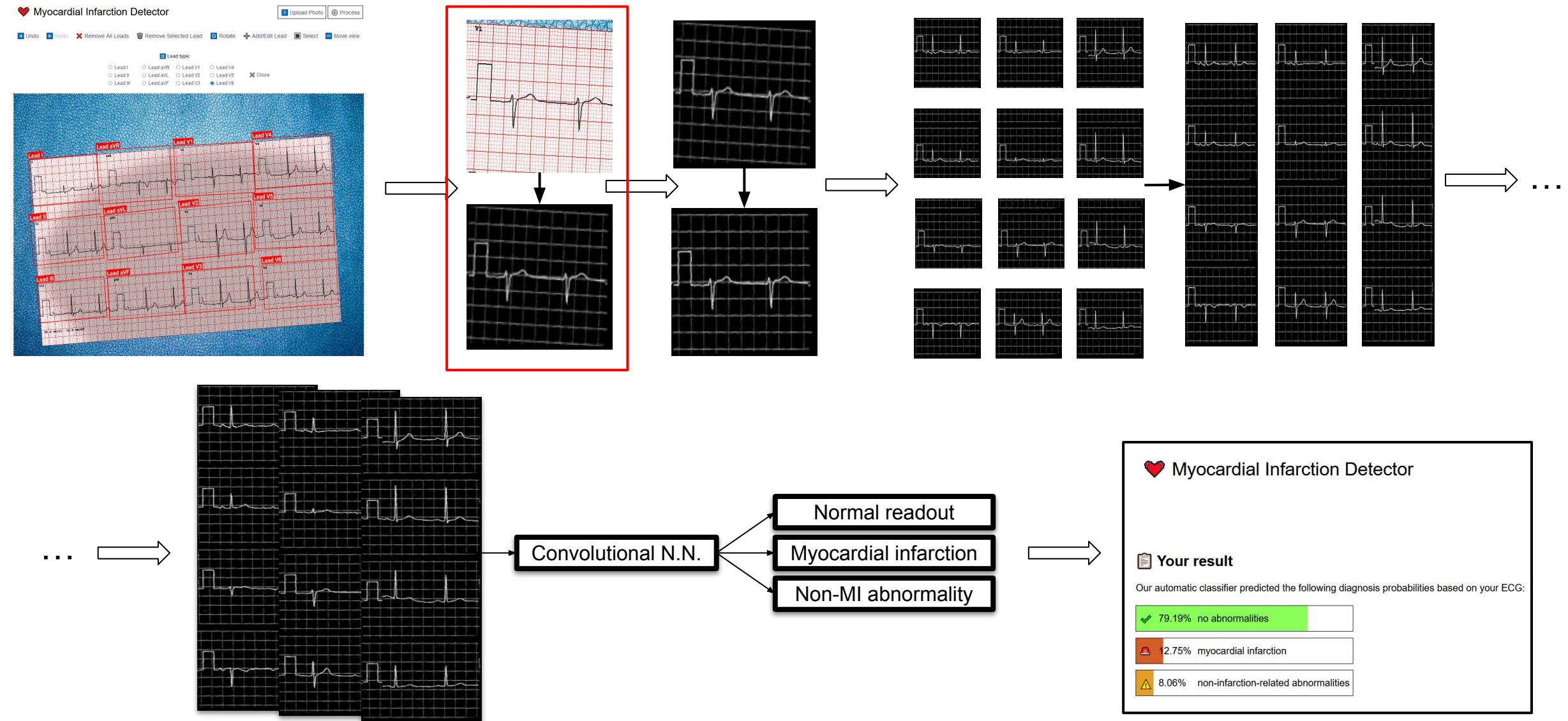
# 3 ECG Processing Overview



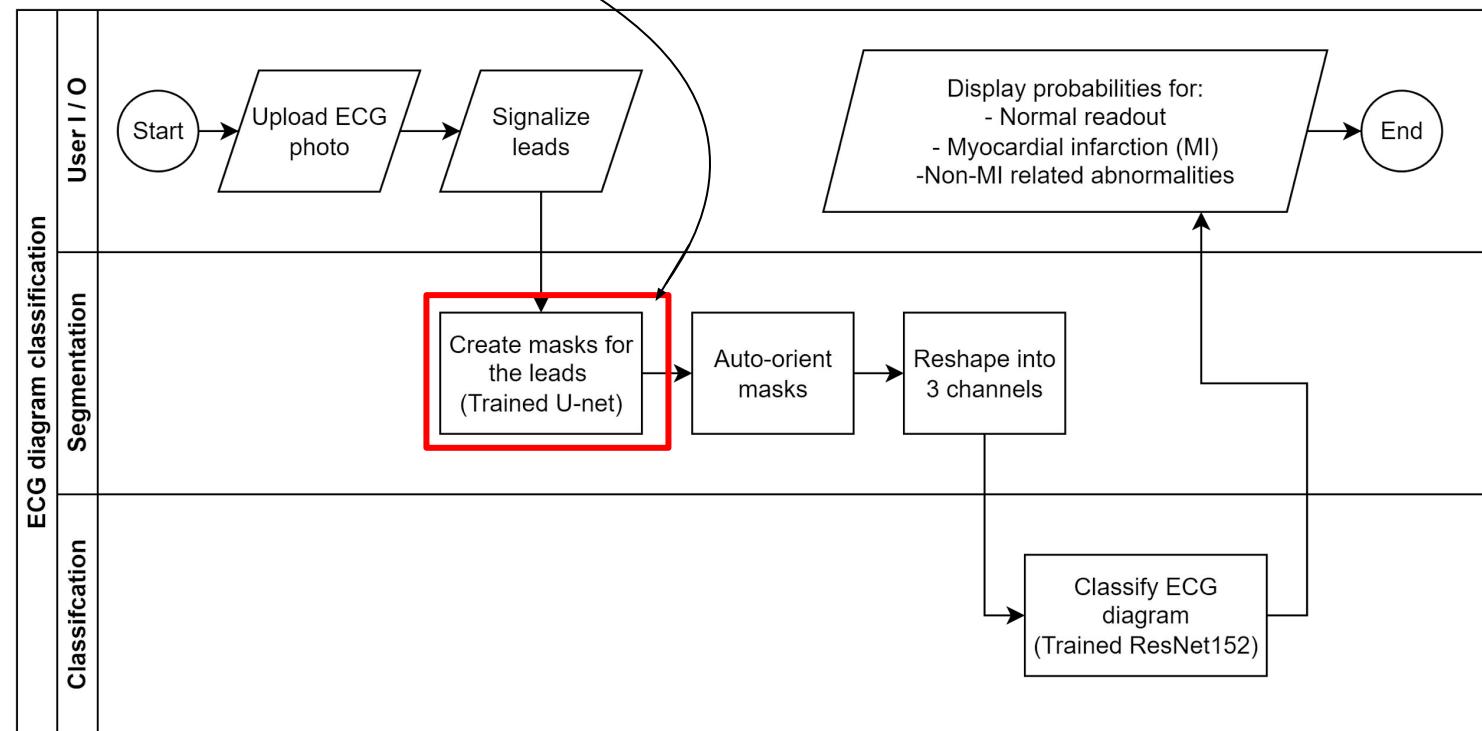
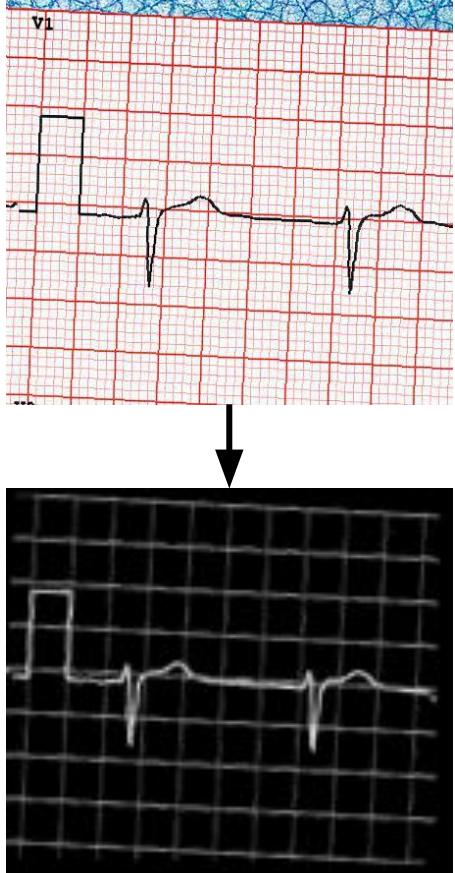
# 3 ECG Processing Overview



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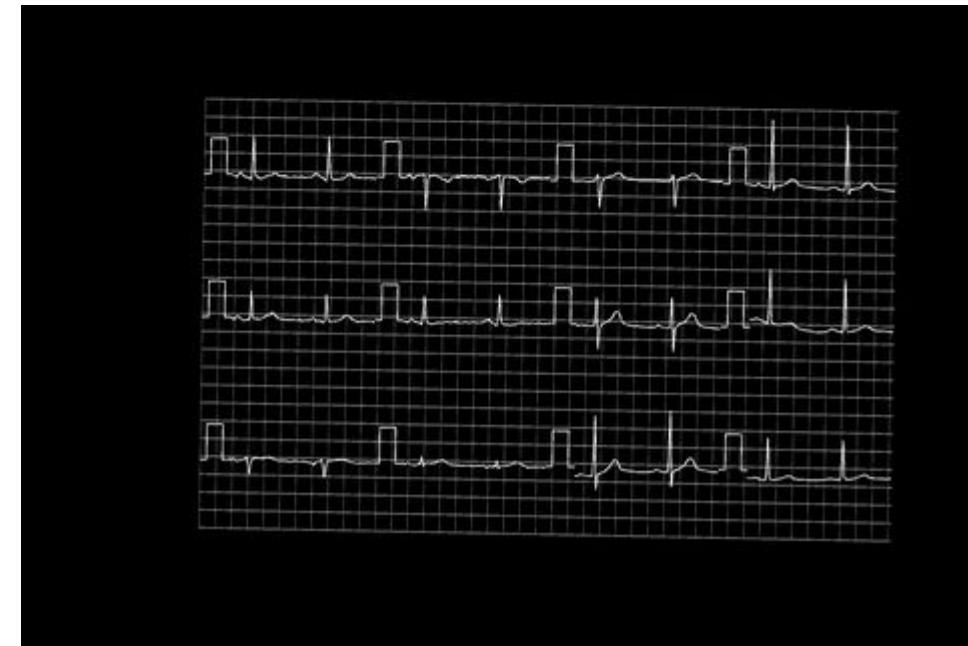
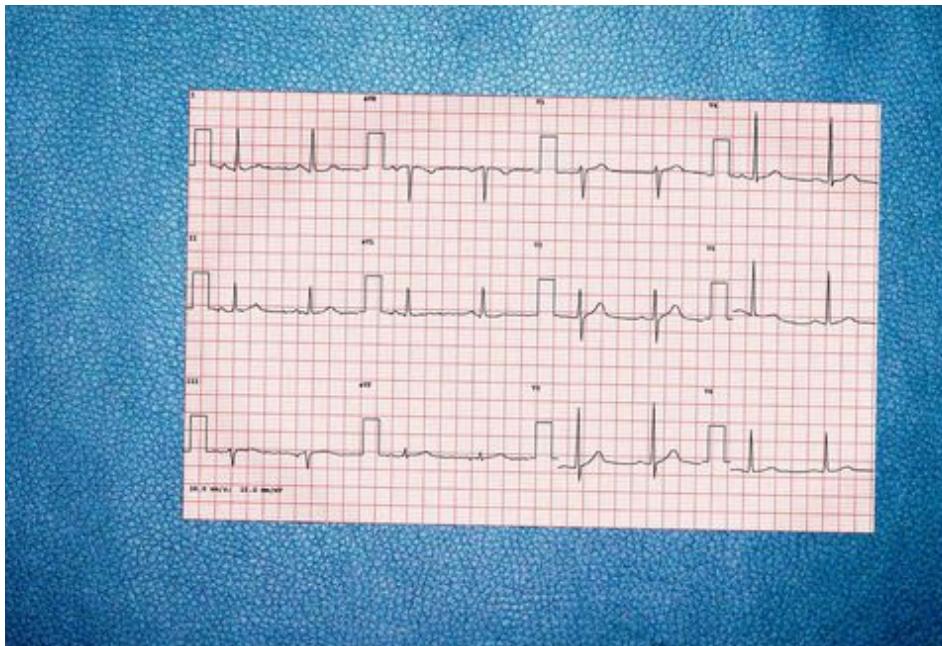


# 3 ECG Processing Overview



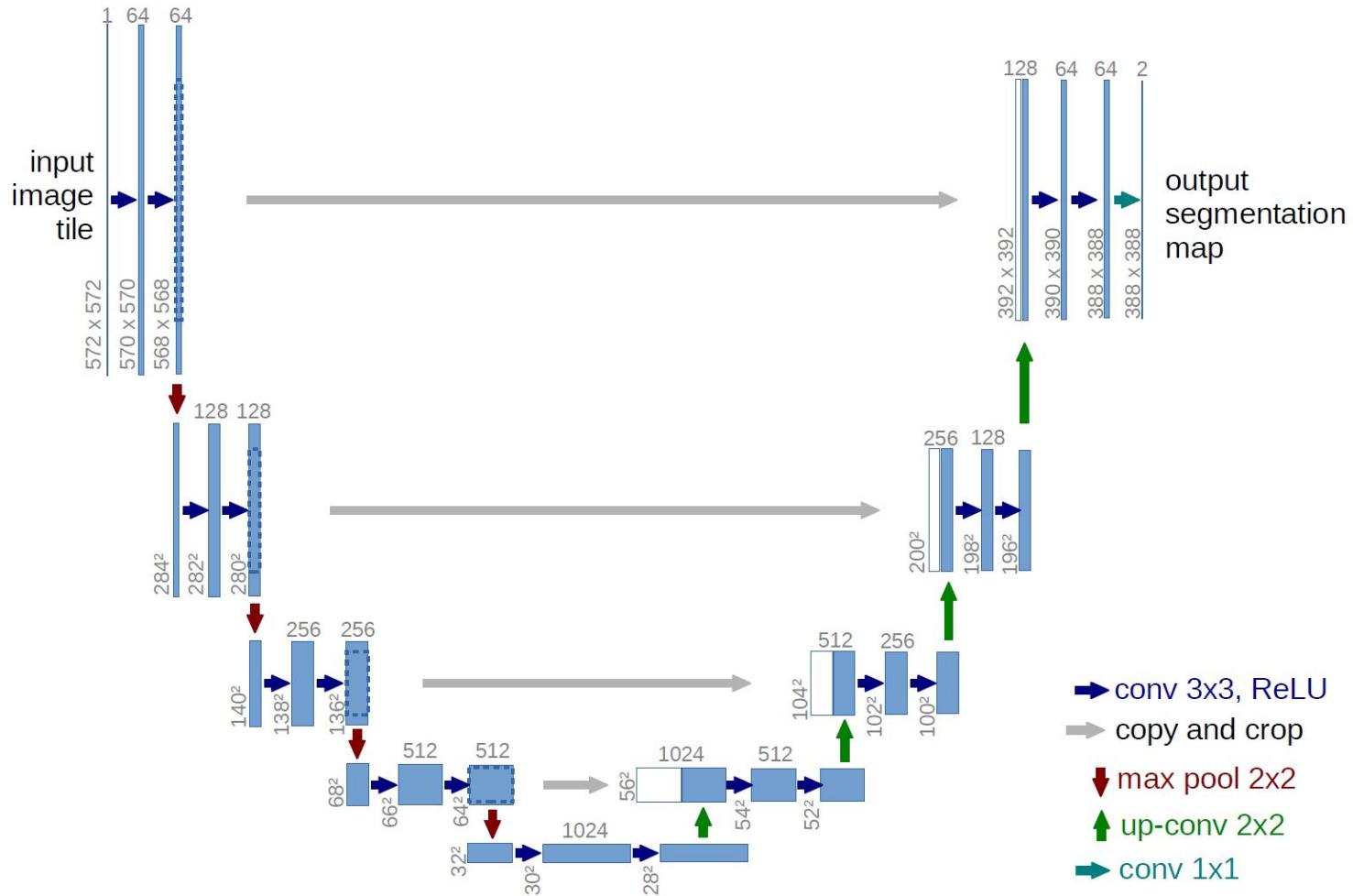
## 3.1 ECG Segmentation

The U-Net was trained with pairs of masks and generated ECG diagrams with data augmentation applied to them, notice that the mask corresponds to the training label.

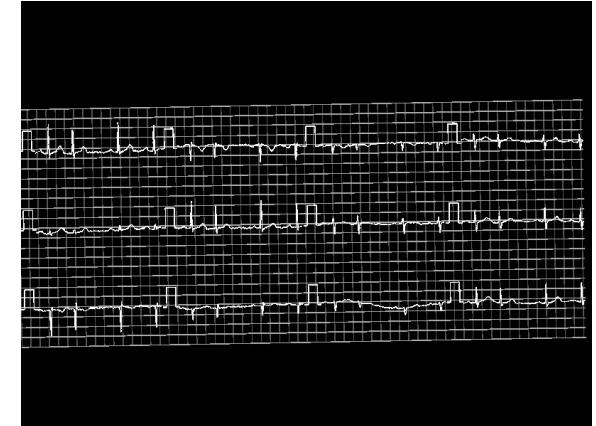
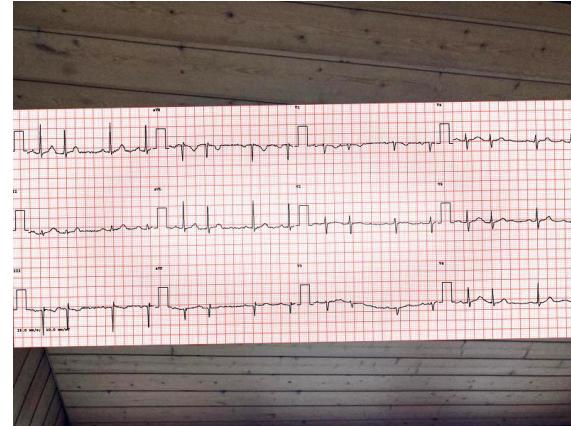
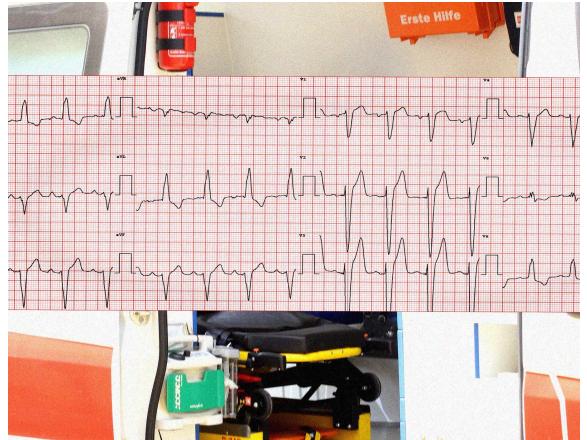
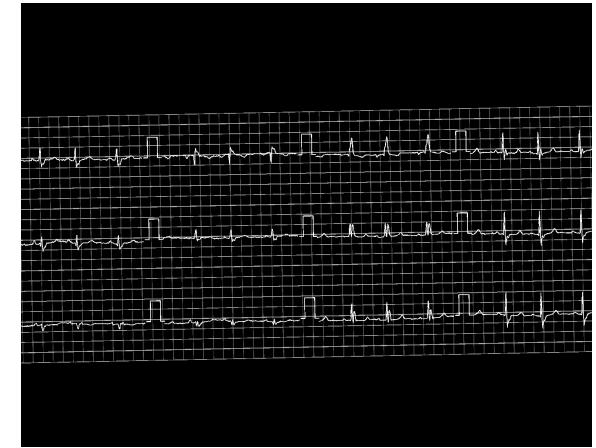
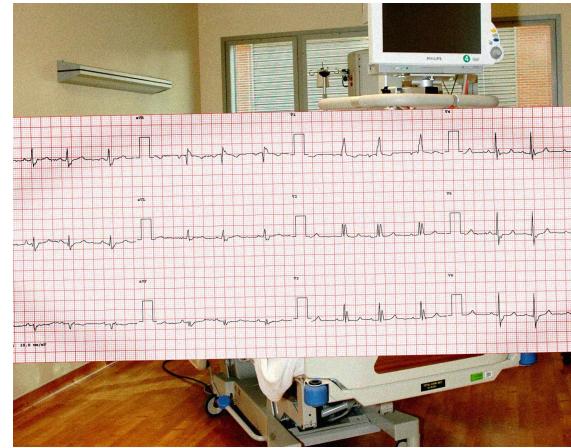
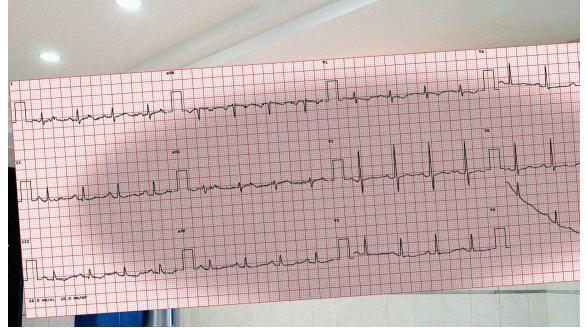


Grid-lines are also captured in the training to be used for auto-orienting of diagrams during processing.

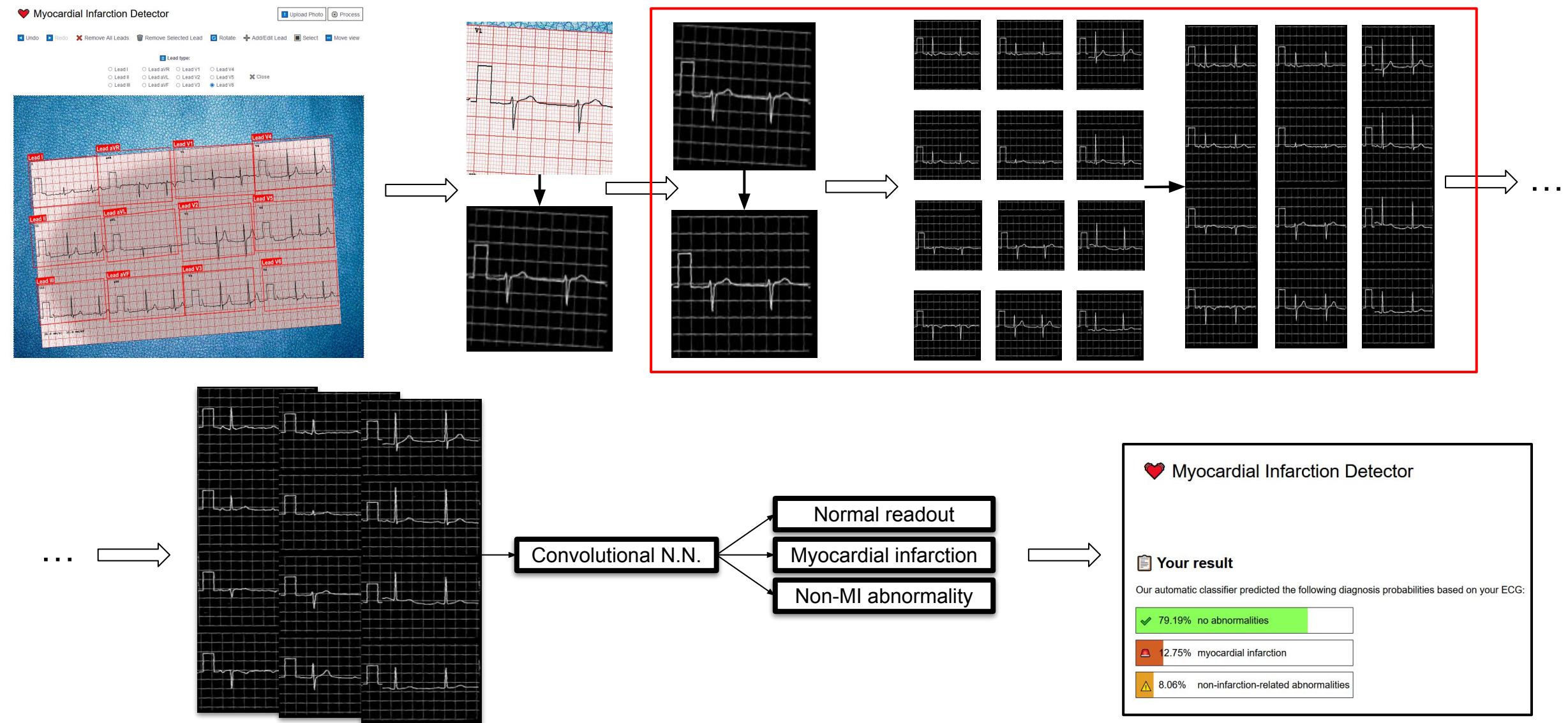
# 3.1 ECG Segmentation



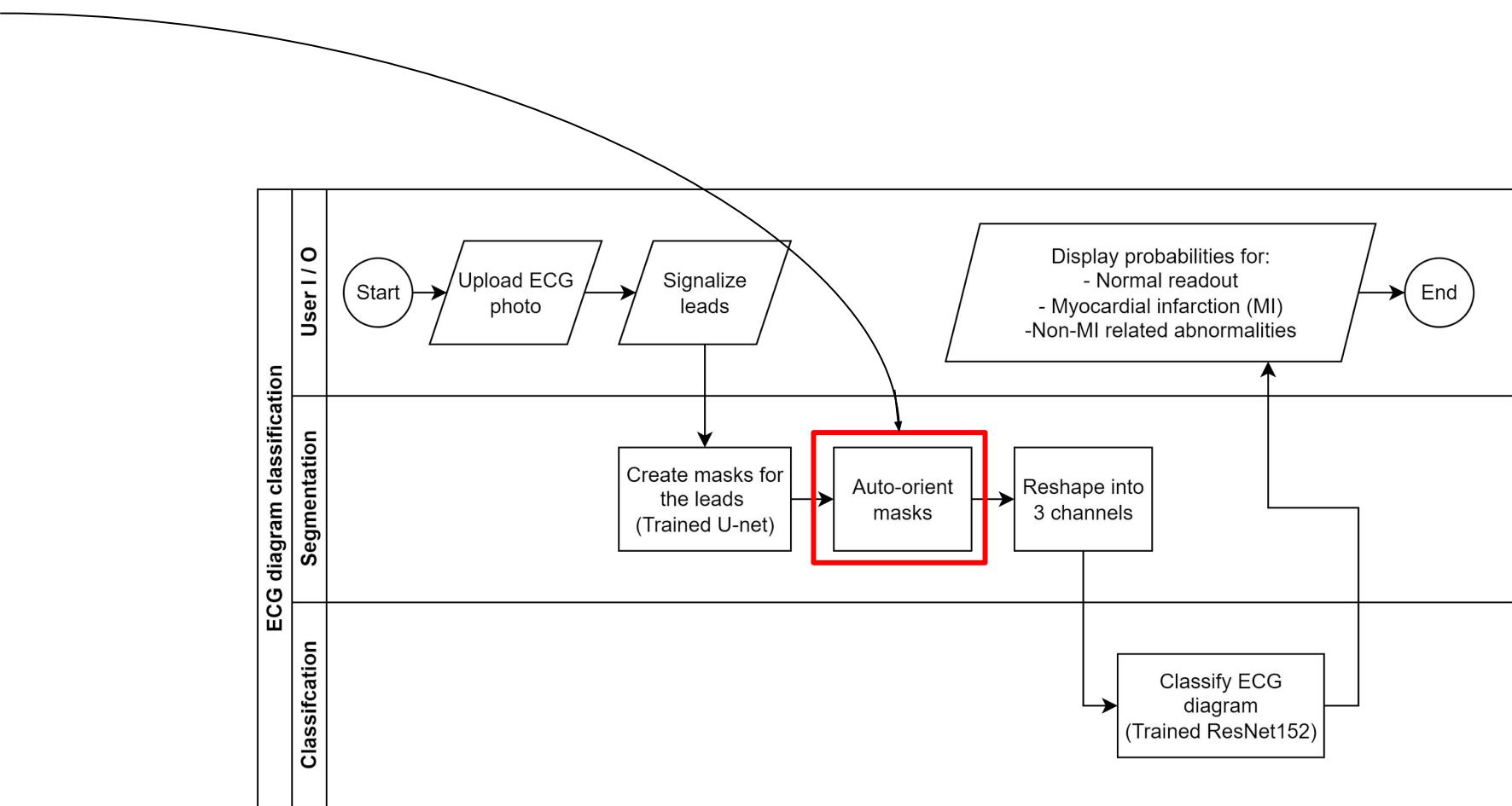
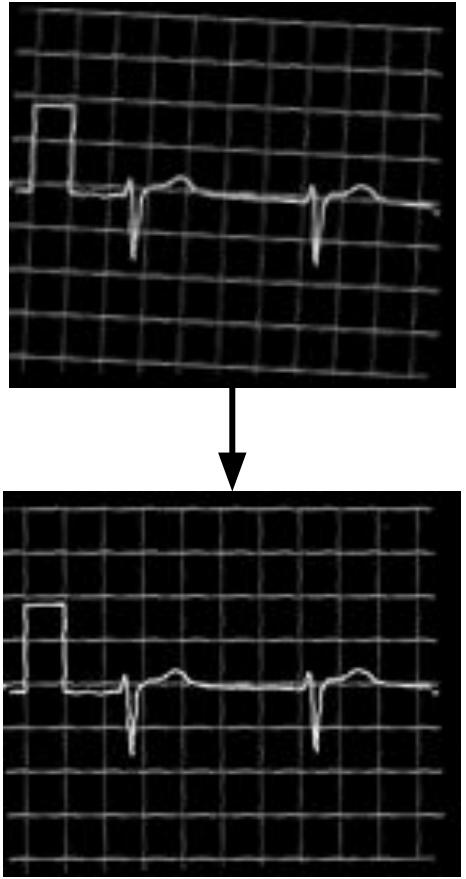
# 3.1 ECG Segmentation



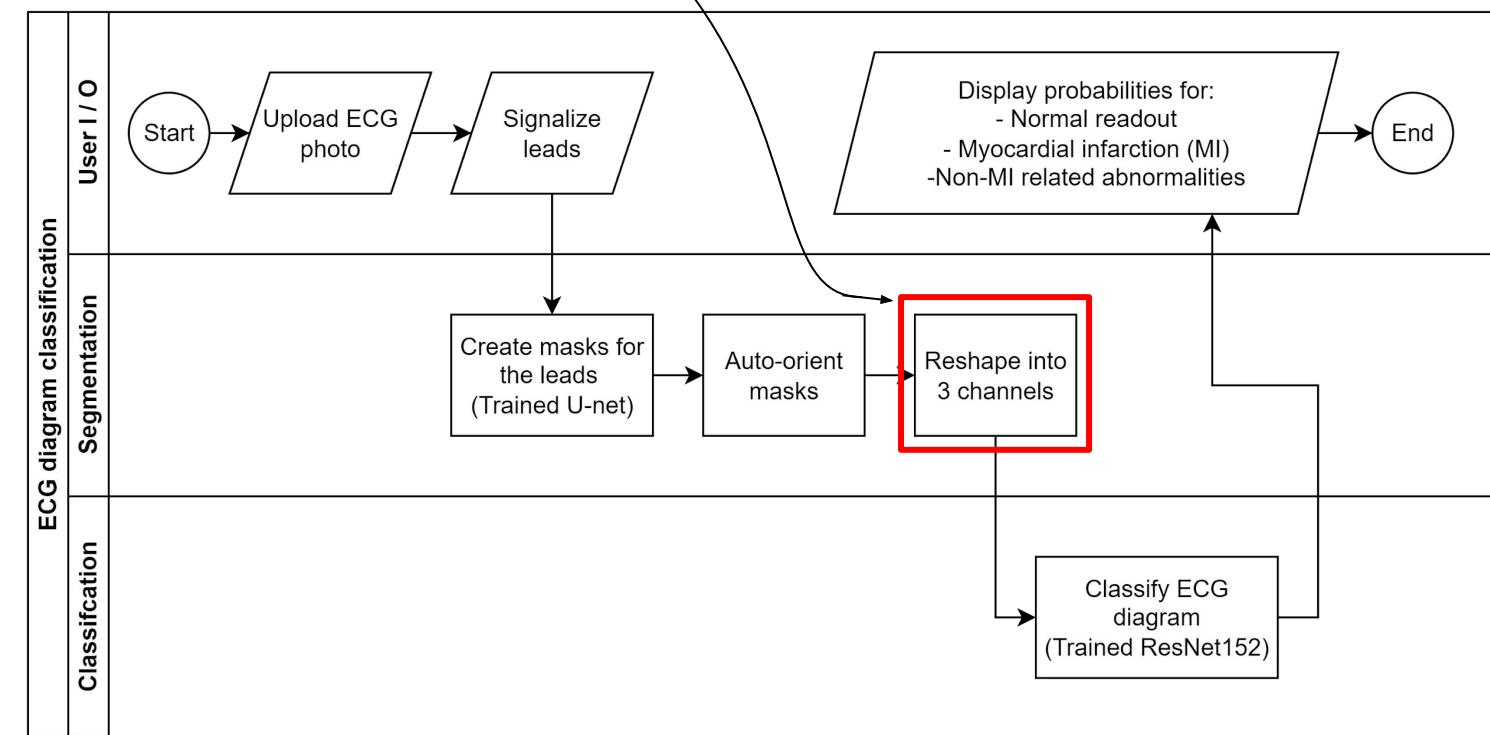
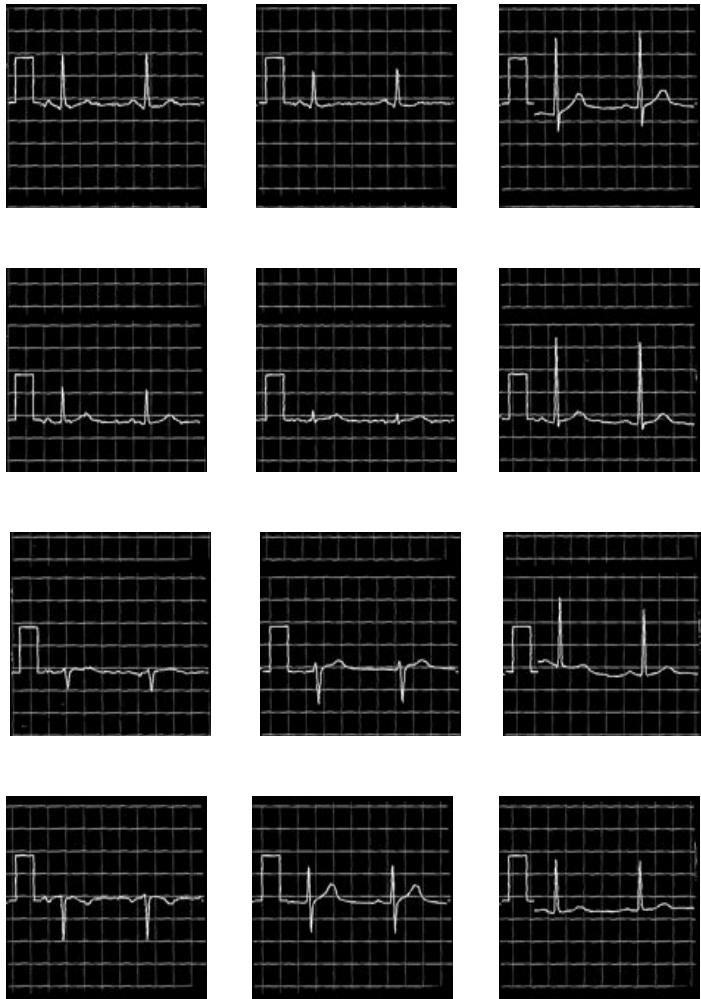
# 3 ECG Processing Overview



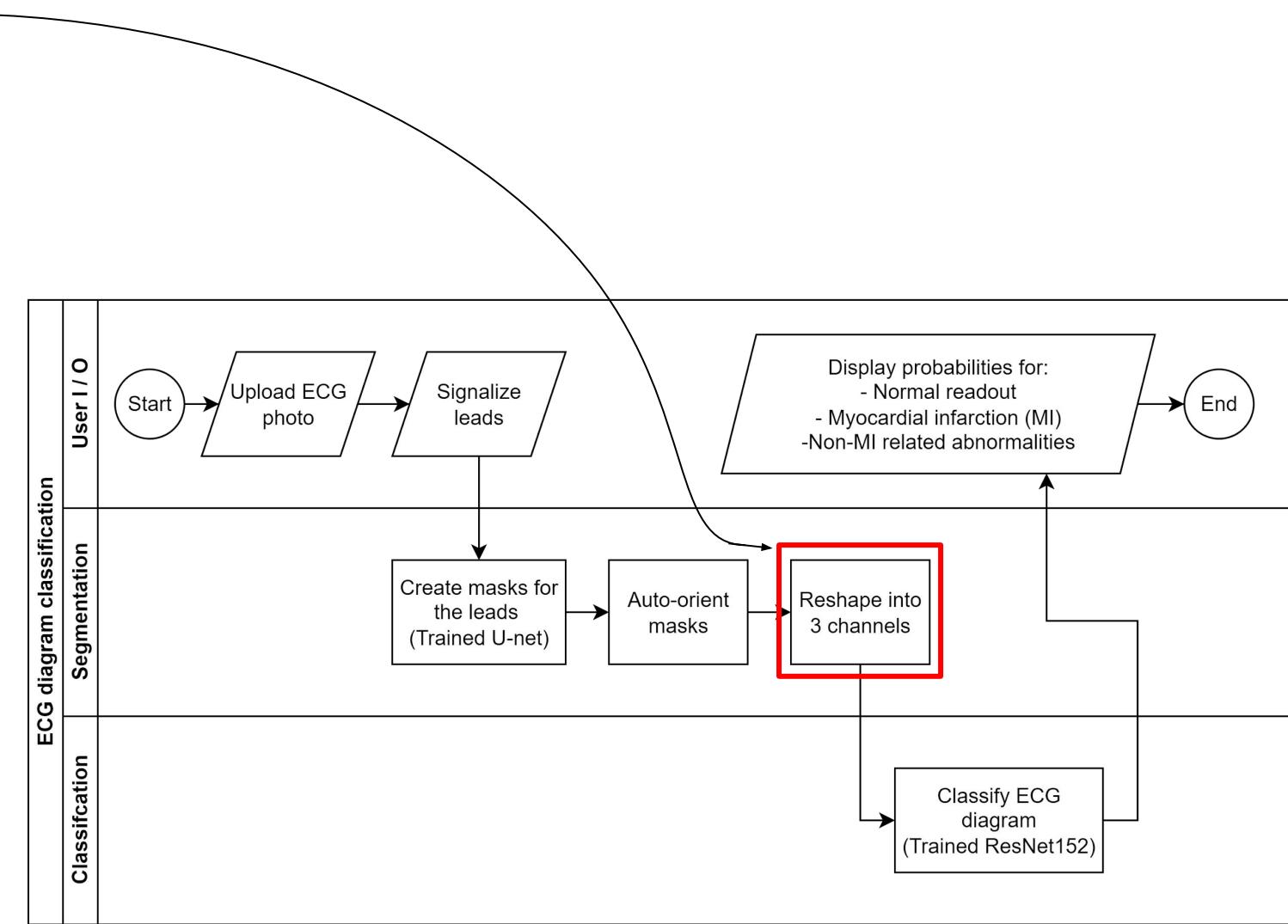
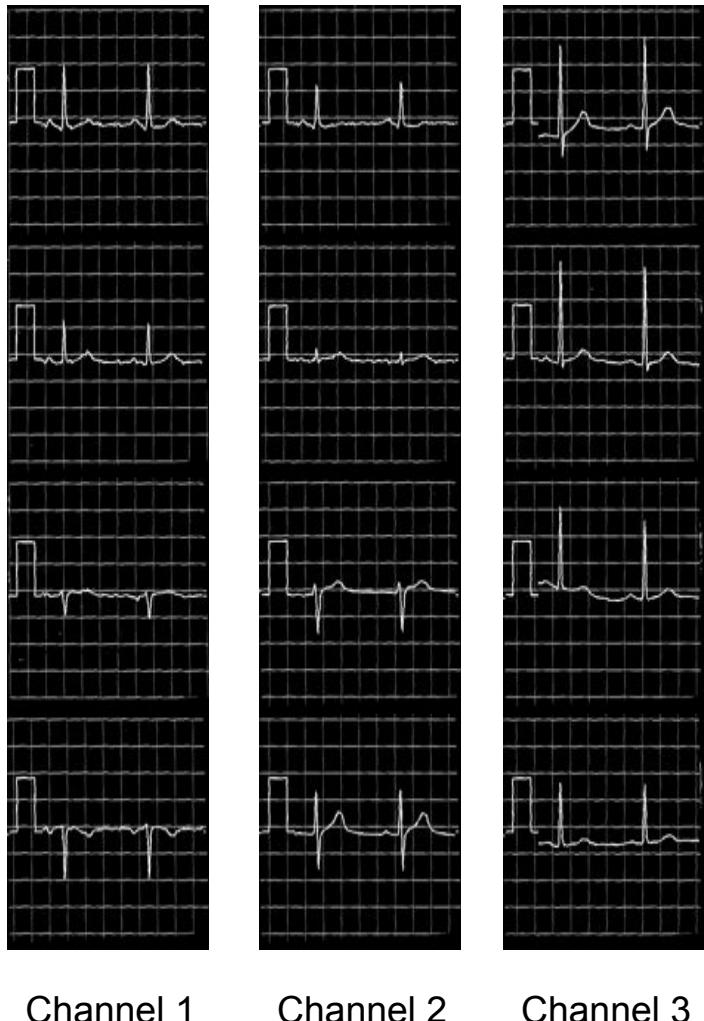
# 3 ECG Processing Overview



# 3 ECG Processing Overview

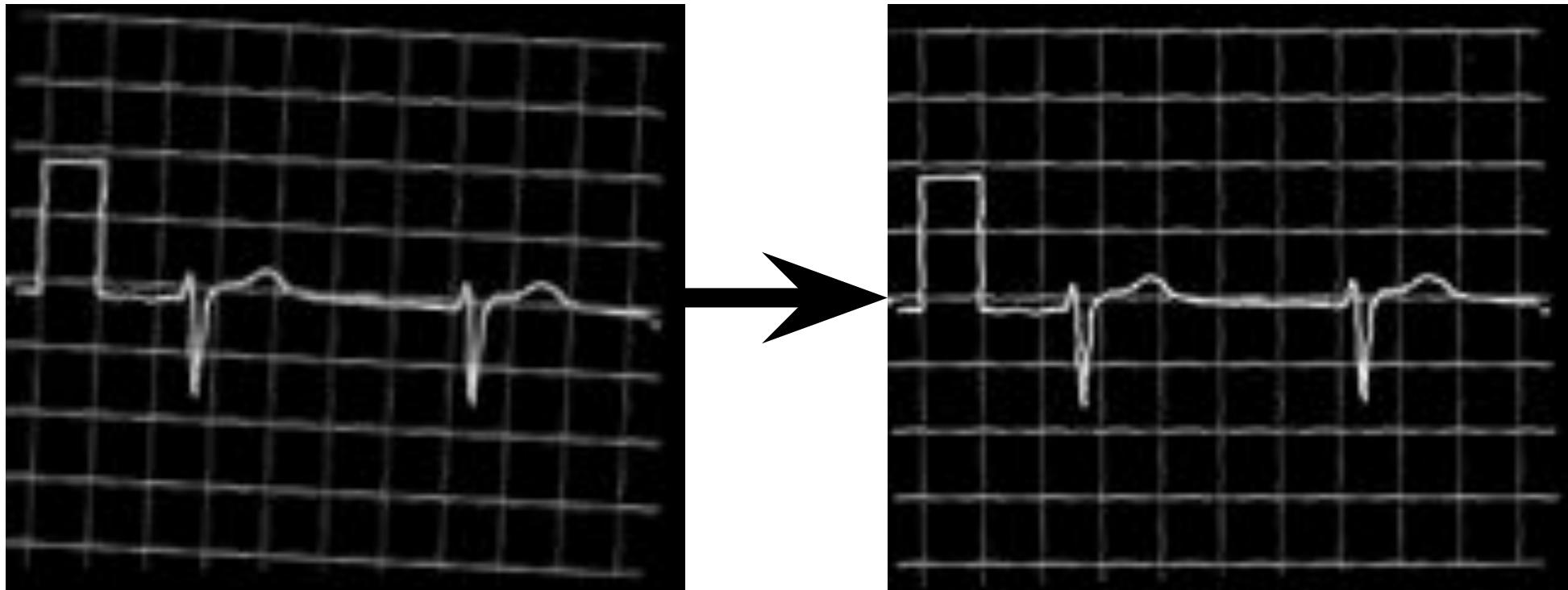


# 3 ECG Processing Overview



## 3.1 ECG Segmentation

The straightening algorithm is based on detecting horizontally the grid-lines on several heights and then correct the rotation

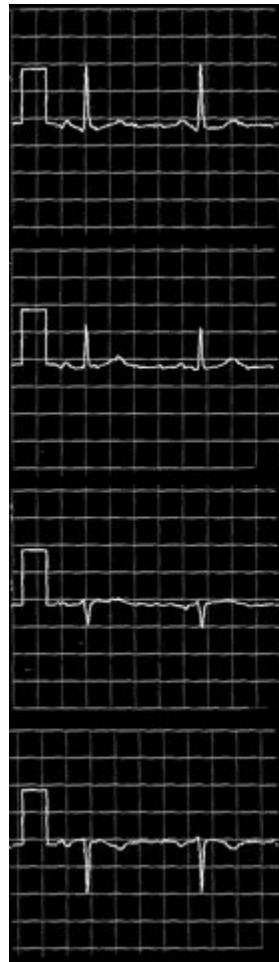


# 3.1 ECG Segmentation

The 12 leads are divided in 3 groups, one for each channel fed into the convnet for classification.

If more leads are inserted, they are added in a **consistent way** to the different channels. **This is important because certain types of myocardial infarctions result in characteristic changes to certain leads.**

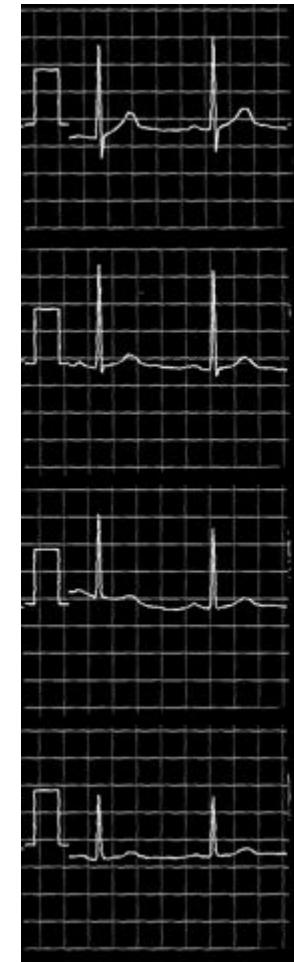
The grid lines are kept also fed to the classifying convnet. We expect that this helps with detecting correlations of different lead values at equal times.



Channel 1

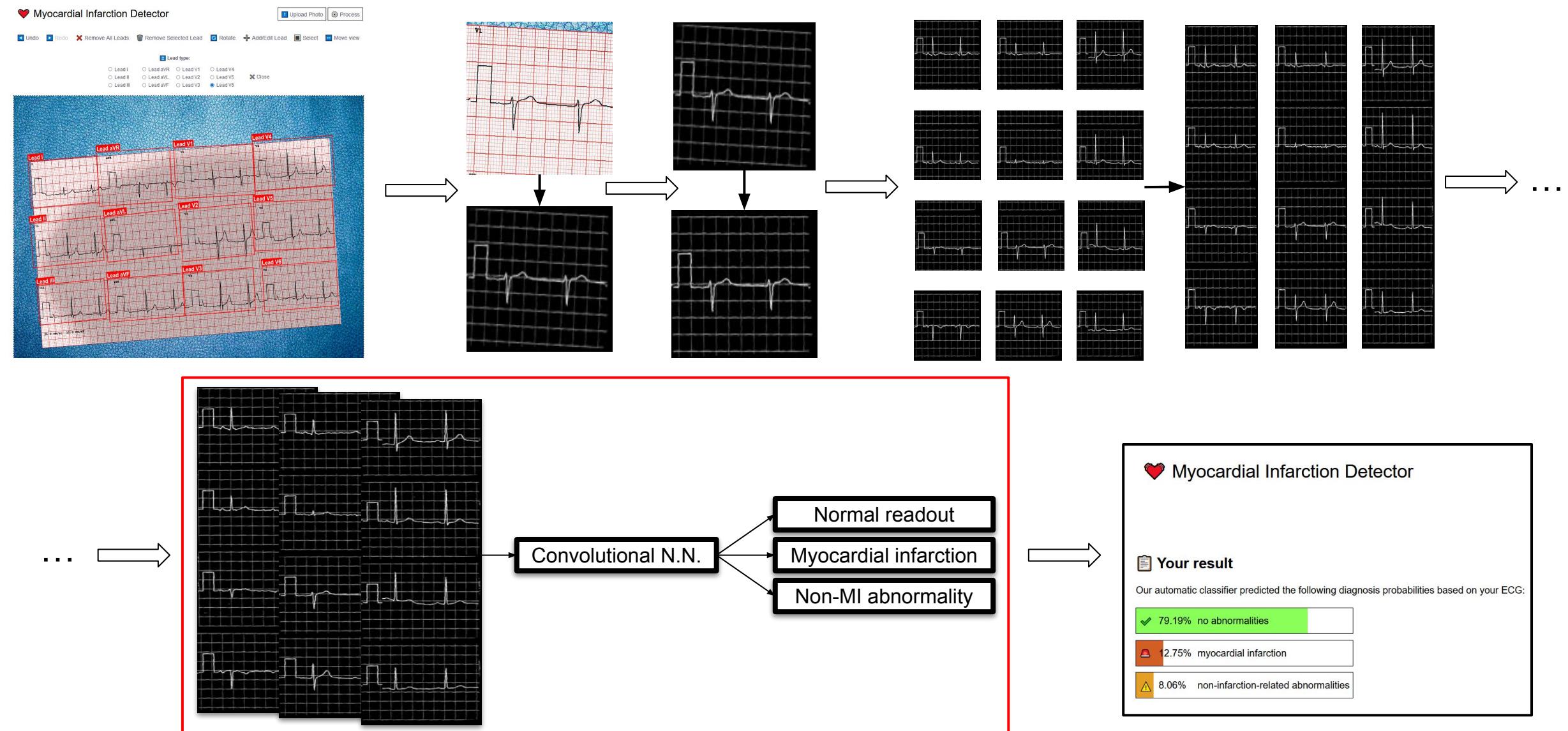


Channel 2



Channel 3

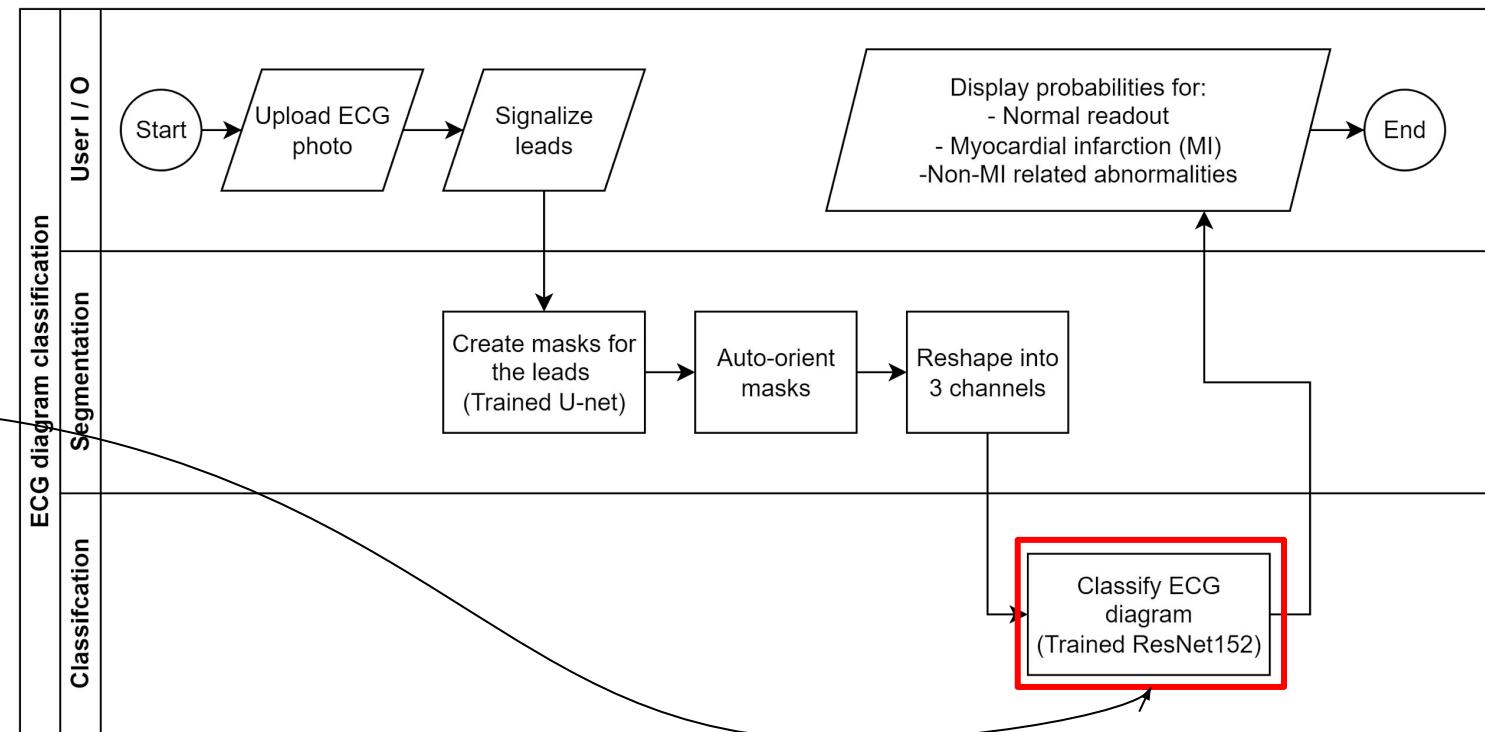
# 3 ECG Processing Overview



# 3 ECG Processing Overview



→ ResNet152



## 3.2 ECG Classification



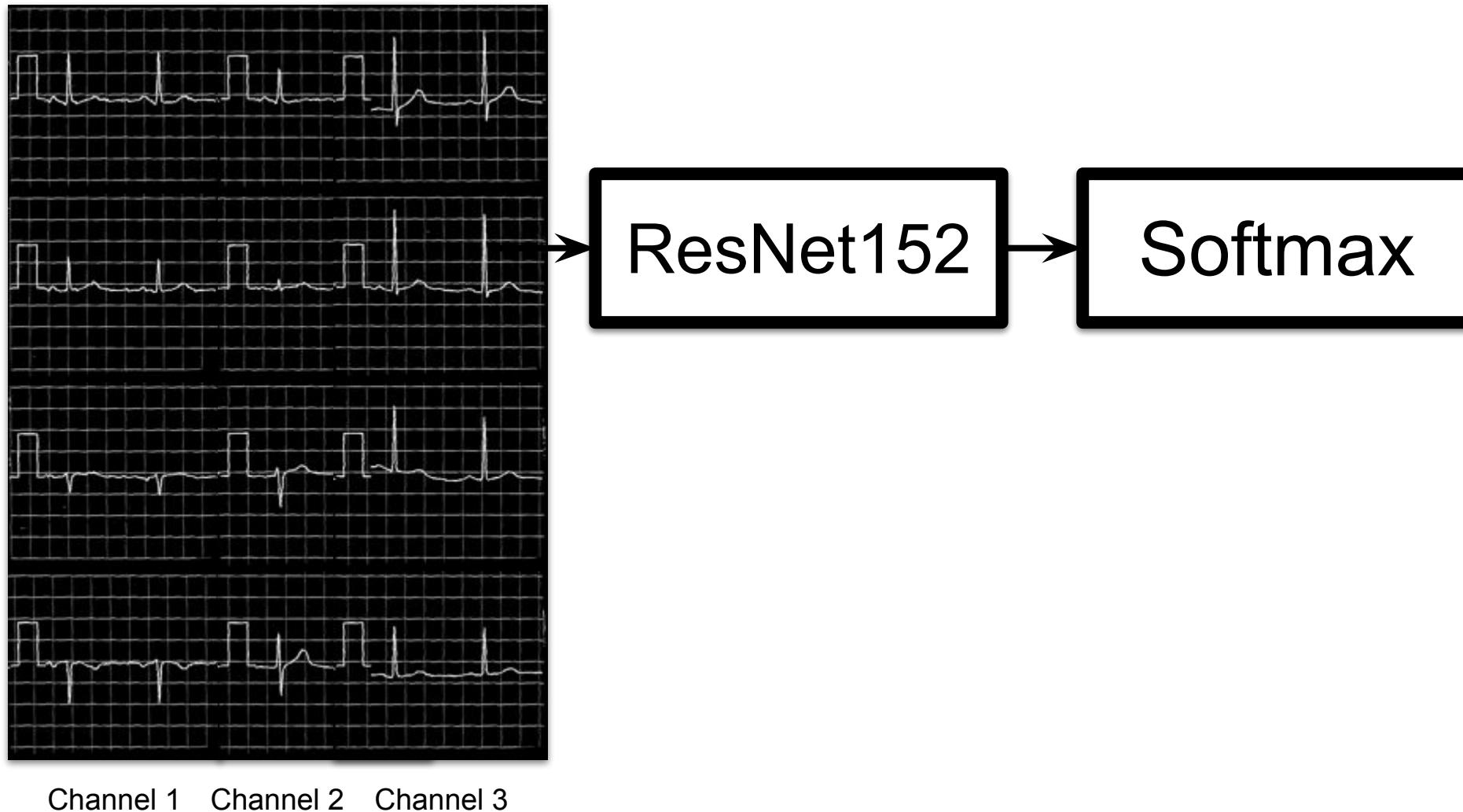
Channel 1   Channel 2   Channel 3

## 3.2 ECG Classification

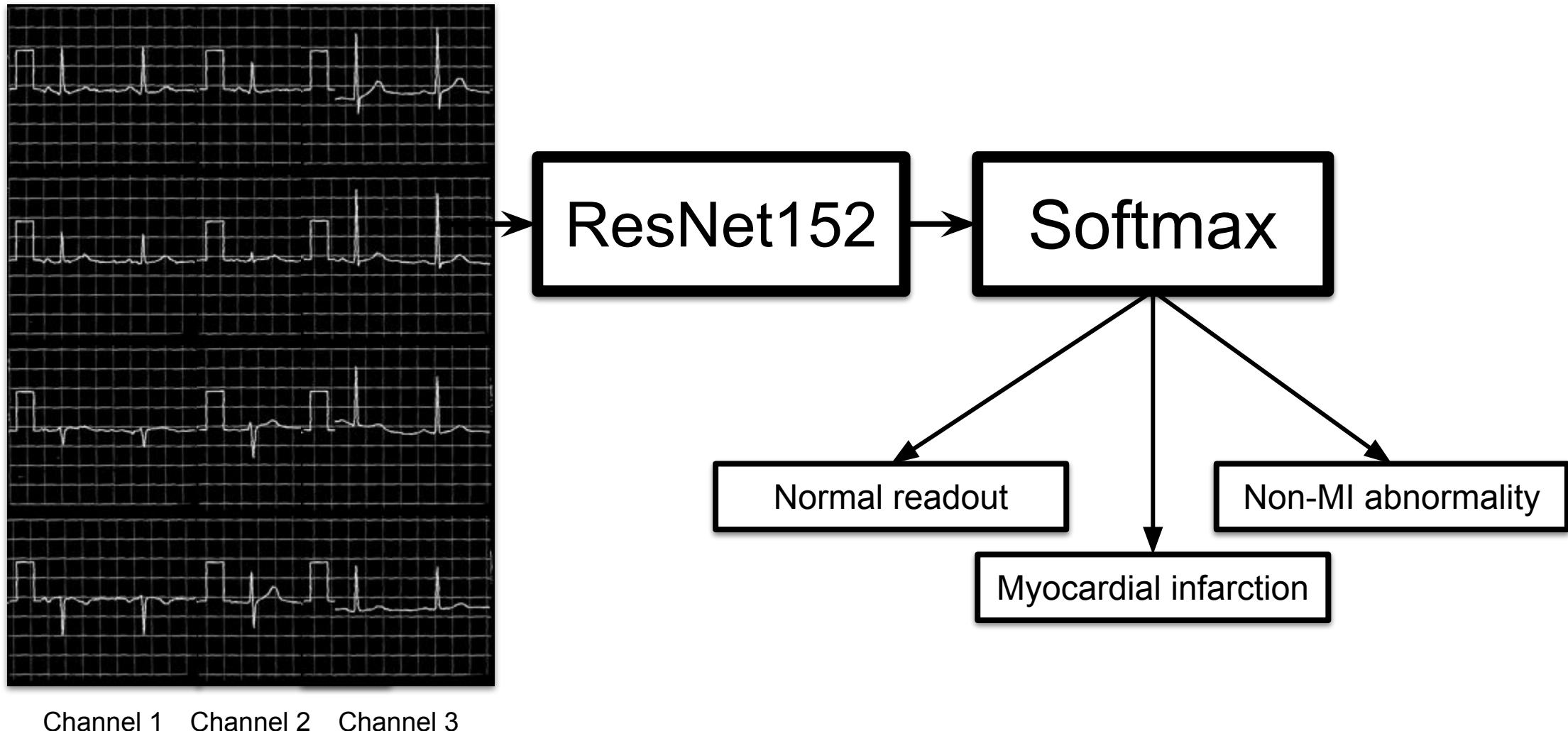


Channel 1   Channel 2   Channel 3

## 3.2 ECG Classification



## 3.2 ECG Classification



## 3.2 ECG Classification: ResNet152 architecture

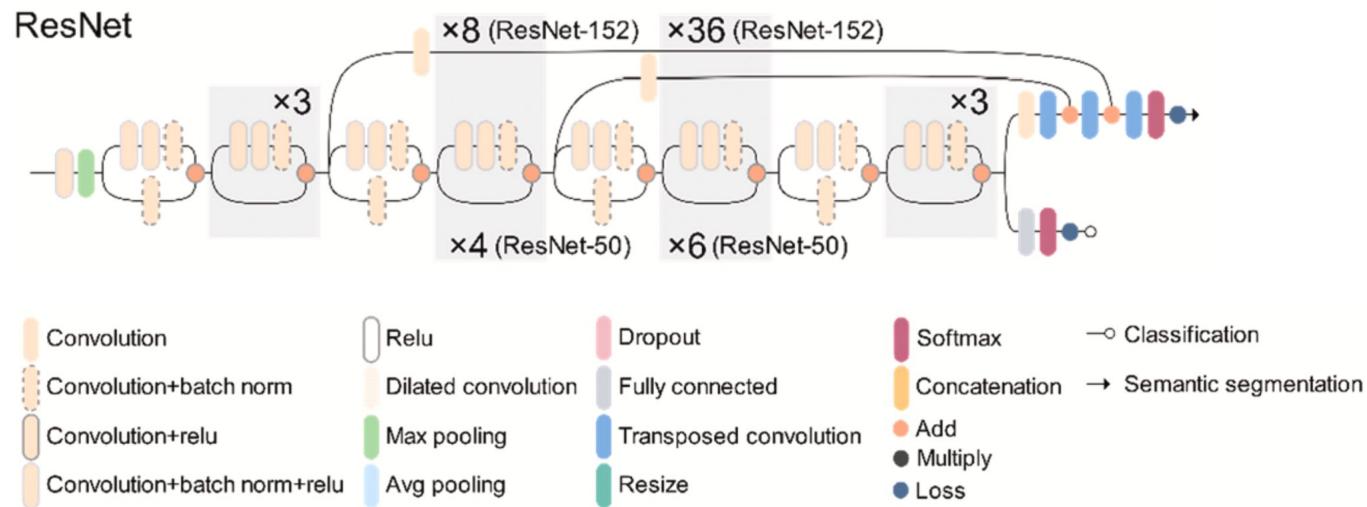


Figure 1: ResNet152 architecture diagram

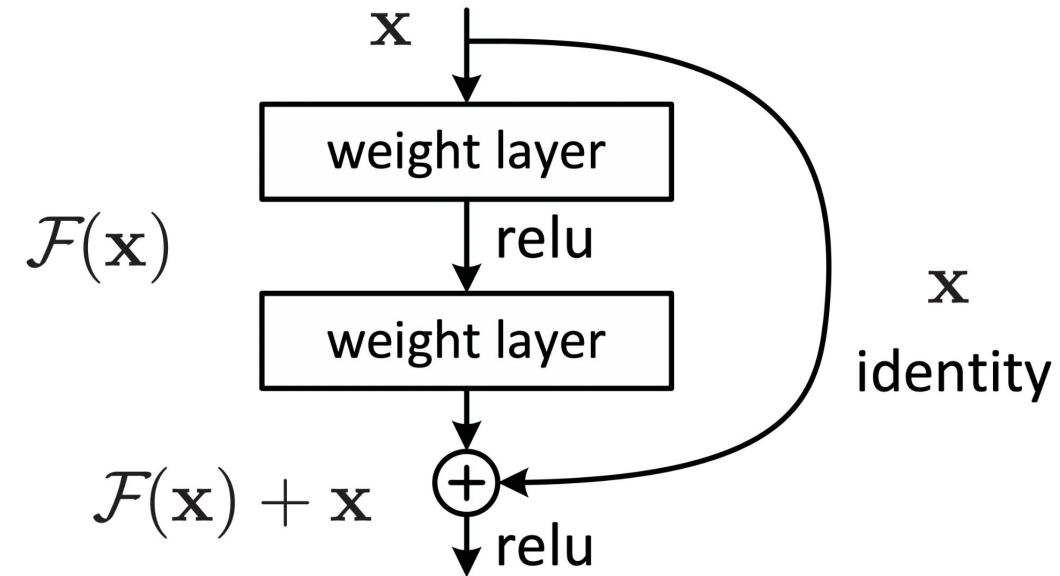
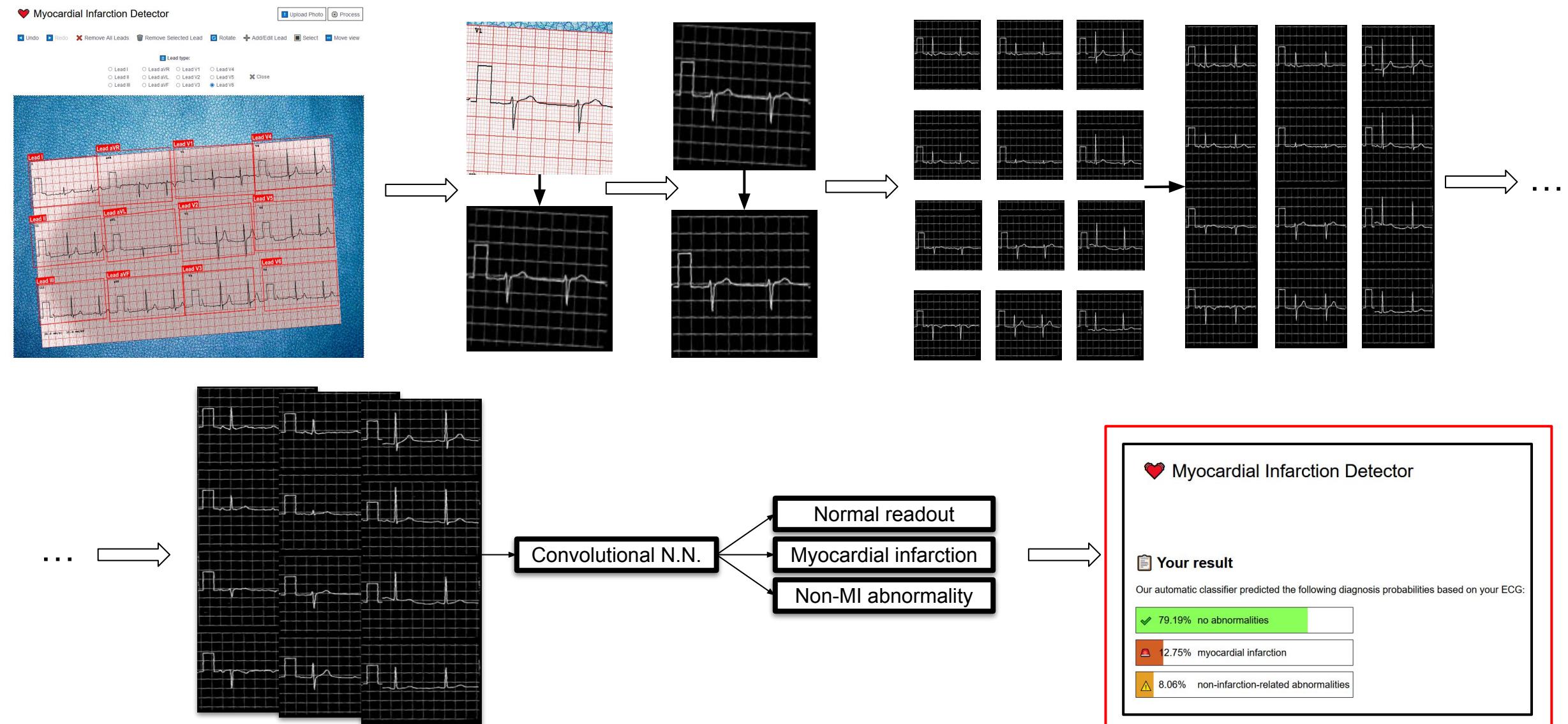


Figure 2: Residual learning building block

Figure 1 taken from: Zhouxin Xi, Chris Hopkinson, Stewart B. Rood, & Derek R. Peddle (2020). See the forest and the trees: Effective machine and deep learning algorithms for wood filtering and tree species classification from terrestrial laser scanning. *ISPRS Journal of Photogrammetry and Remote Sensing*, 168, 1-16.

# 3 ECG Processing Overview

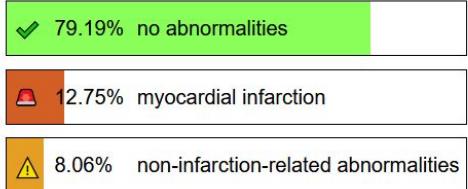


# 3 ECG Processing Overview

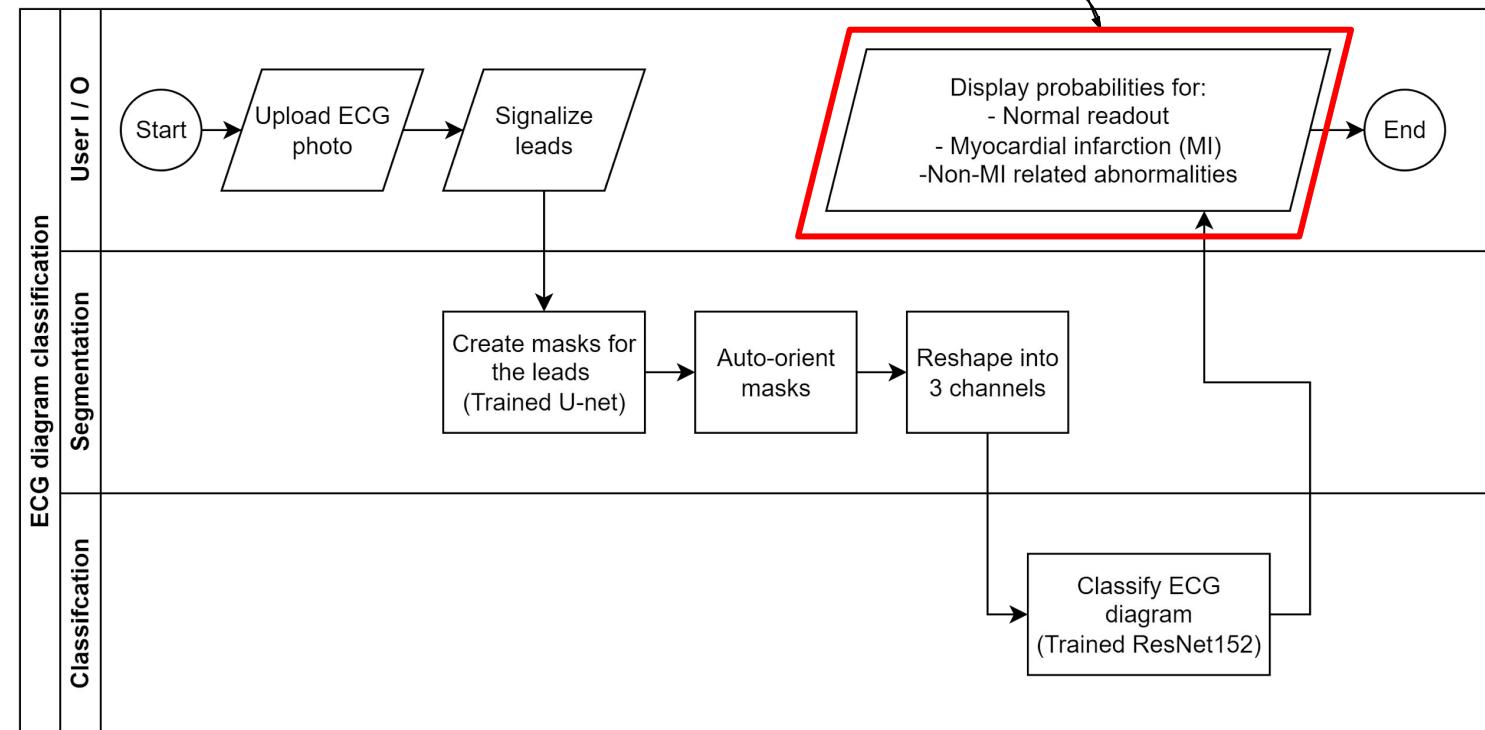
## Myocardial Infarction Detector

### Your result

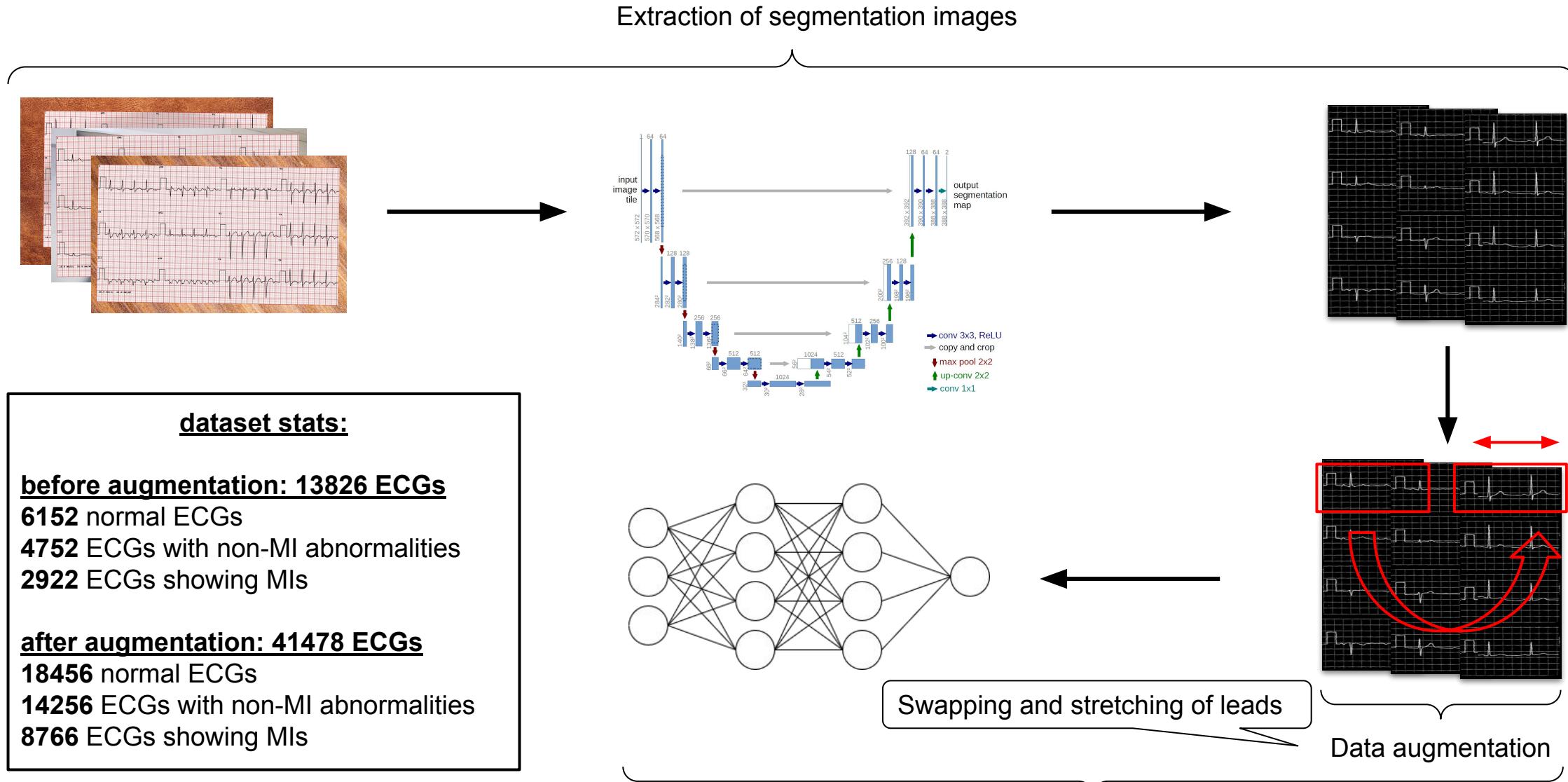
Our automatic classifier predicted the following diagnosis probabilities based on your ECG:



This will be presented with detail later on.



### 3.3 ECG Network Training



# 3.3 ECG Network Training: Training Environment



vast.ai

Account  
CLI  
FAQ

CLIENT  
Billing  
Instances  
Create

HOST  
Dashboard  
Machines  
Create Job  
Setup

ID	Machine ID	Host IP	Location	GPU Model	TFLOPS	Memory	CUDA Version	Network	Storage	Age	Remaining	Action Buttons
4450882	m:2293	host:6280	Taipei City, TW	1x RTX 3090	44.1	24.3 GB	Xeon® E5-2683 v4	↑88.8 Mbps ↓84.3 Mbps	Storage 661 MB/s 19.7 GB	verified Age: 6 days Remaining: 1 mon, 16d	<button>STOP...</button> <button>DESTROY...</button> <button>CONNECT</button>  <b>\$0.364/hr</b>	
4467564	m:2432	host:6280	Taipei City, TW	1x RTX 3090	44.1	24.3 GB	Xeon® E5-2696 V2	↑88.9 Mbps ↓87.9 Mbps	Storage 911 MB/s 24.5 GB	verified Age: 5 days Remaining: 1 mon, 15d	<button>START</button> <button>DESTROY...</button> <button>INACTIVE</button>  <b>\$0.337/hr</b>	
4520361	m:2308	host:6280	Taipei City, TW	1x RTX 3090	44.1	24.3 GB	Xeon® E5-2696 v2	↑512.1 Mbps ↓625.9 Mbps	Storage 945 MB/s 16.7 GB	verified Age: 2d 18h Remaining: 1 mon, 16d	<button>START</button> <button>DESTROY...</button> <button>INACTIVE</button>  <b>\$0.332/hr</b>	
4520517	m:2308	host:6280	Taipei City, TW	1x RTX 3090	44.7	24.3 GB	Xeon® E5-2696 v2	↑512.1 Mbps ↓625.9 Mbps	Storage 945 MB/s 16.7 GB	verified Age: 2d 18h Remaining: 1 mon, 16d	<button>STOP...</button> <button>DESTROY...</button> <button>CONNECT</button>  <b>\$0.332/hr</b>	

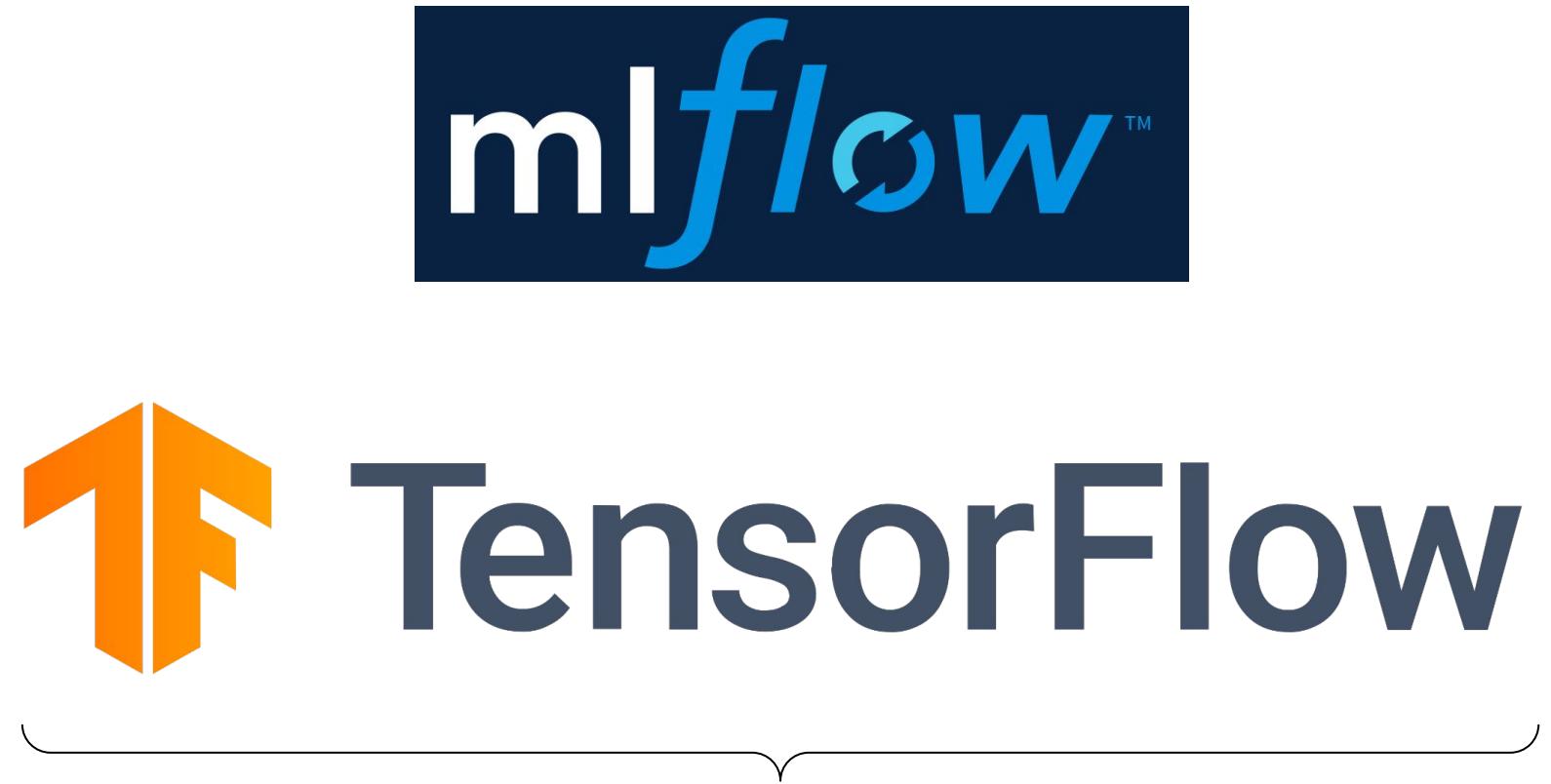
Remote development & training using [vast.ai](#)

### 3.3 ECG Network Training: Training Frameworks

Frameworks:



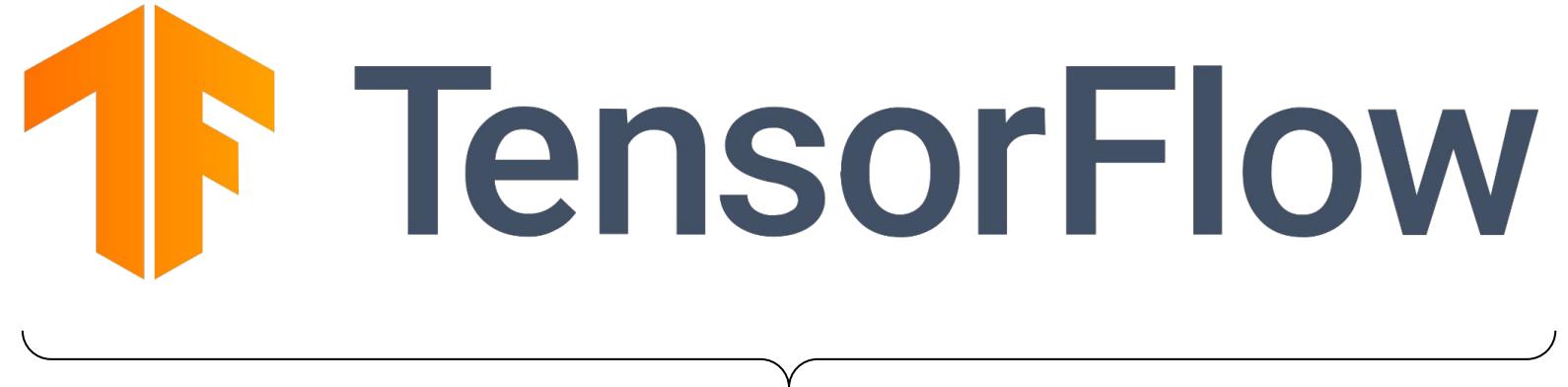
{ }  
For classification network



{ }  
For segmentation network

### 3.3 ECG Network Training: Training Frameworks

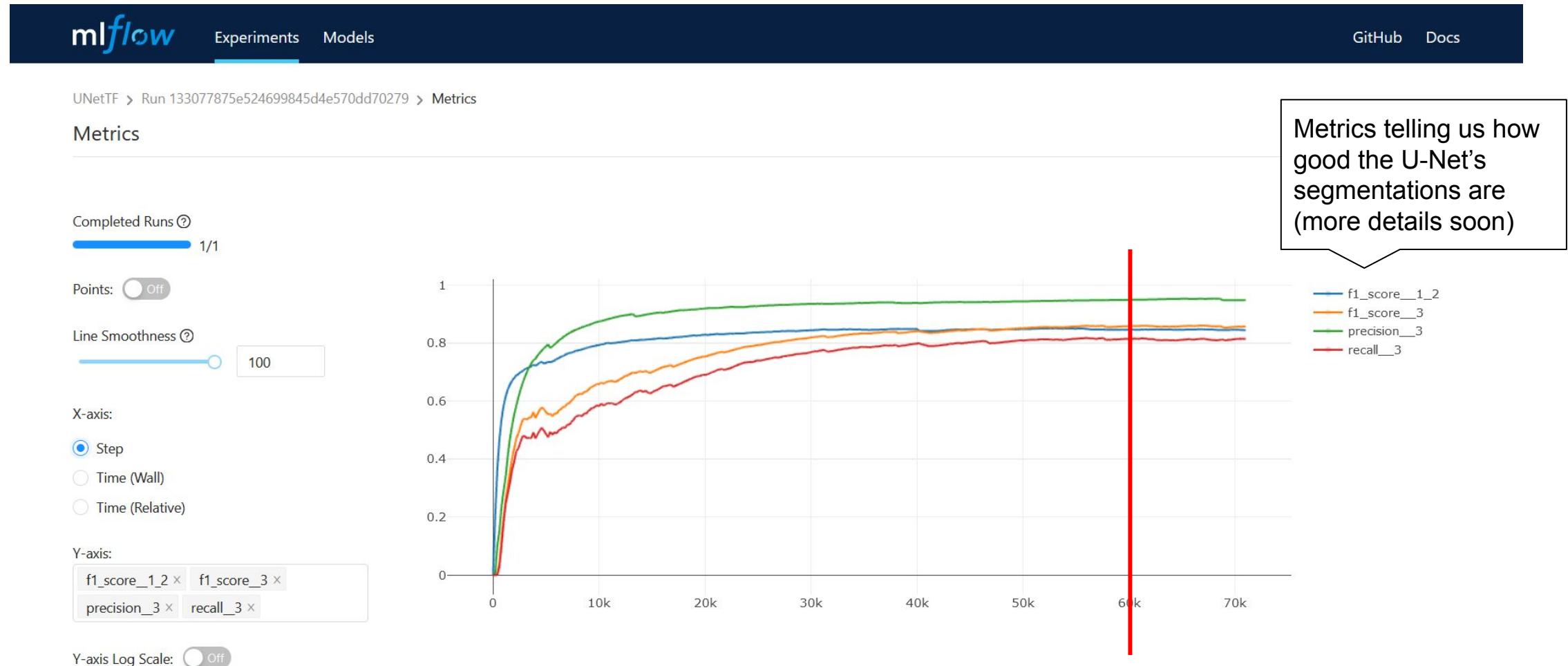
Frameworks:



For classification network

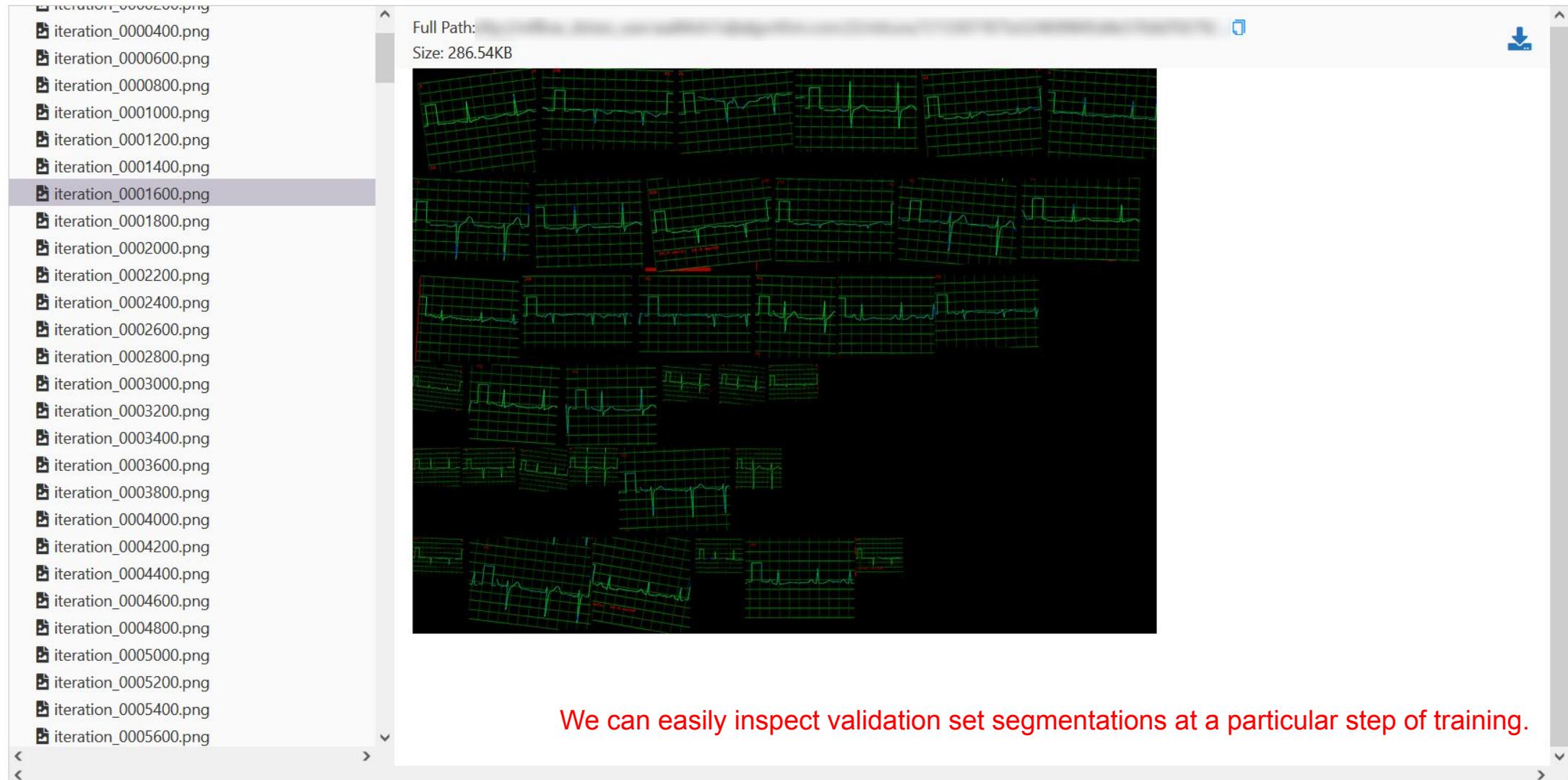
For segmentation network

# 3.3 ECG Network Training: Training Frameworks

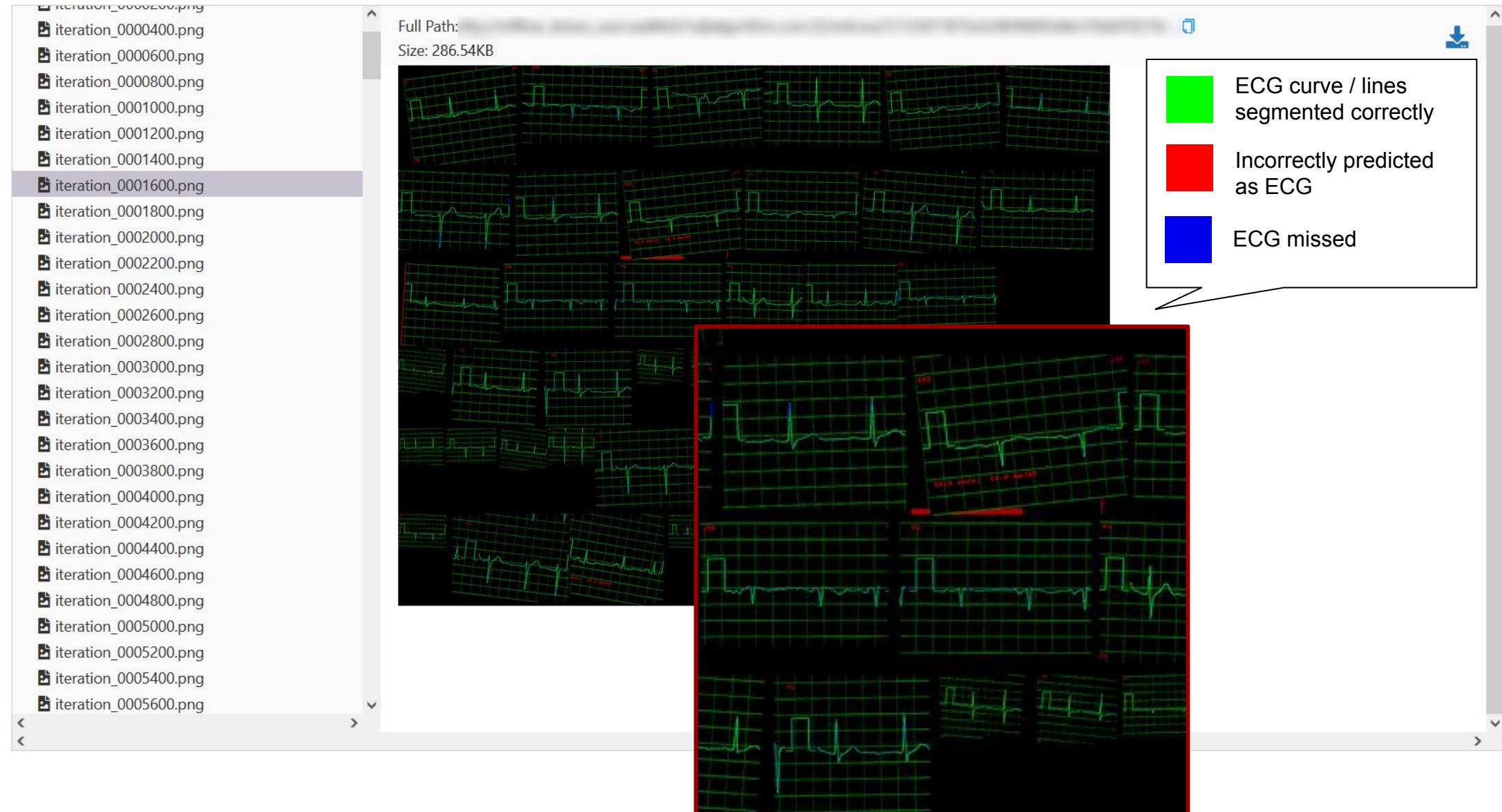


We can easily see (approximate) the step at which convergence is achieved.

### 3.3 ECG Network Training: Training Frameworks



### 3.3 ECG Network Training: Training Frameworks



### 3.3 ECG Network Training: Training Frameworks



### 3.3 ECG Network Training: Metrics

**Precision:**

$$\frac{\# \text{ True positives}}{\# \text{ True positives} + \# \text{ False positives}} \in [0, 1]$$

i.e. “if the classifier predicts an MI, how likely is it really an MI?”

**Recall:**

$$\frac{\# \text{ True positives}}{\# \text{ True positives} + \# \text{ False negatives}} \in [0, 1]$$

i.e. “if there is an MI, how likely is the classifier to say so?”

**F1 score:**

$$\frac{2 \times \text{Precision} \times \text{Recall}}{\text{Precision} + \text{Recall}} \in [0, 1]$$

harmonic mean of precision and recall; means to combine the two scores

### 3.3 ECG Network Training: Results

Class	Precision	Recall	F1 Score
Normal ECG	74.59%	86.40%	0.8006
Non-MI-related abnormalities	69.50%	56.70%	0.6246
<b>Myocardial Infarction</b>	<b>61.20%</b>	<b>53.12%</b>	<b>0.5688</b>

Results on validation dataset of augmented ECG segmentation images

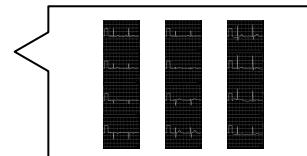
**Validation dataset:**  
**1331** ECG segmentations  
**581** normal ECGs  
**462** ECGs w/ non-MI abnormalities  
**288** ECGs w/ MI

### 3.3 ECG Network Training: Results

Class	Precision	Recall	F1 Score
Normal ECG	74.59%	86.40%	0.8006
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<b>Myocardial Infarction</b>	<b>61.20%</b>	<b>53.12%</b>	<b>0.5688</b>

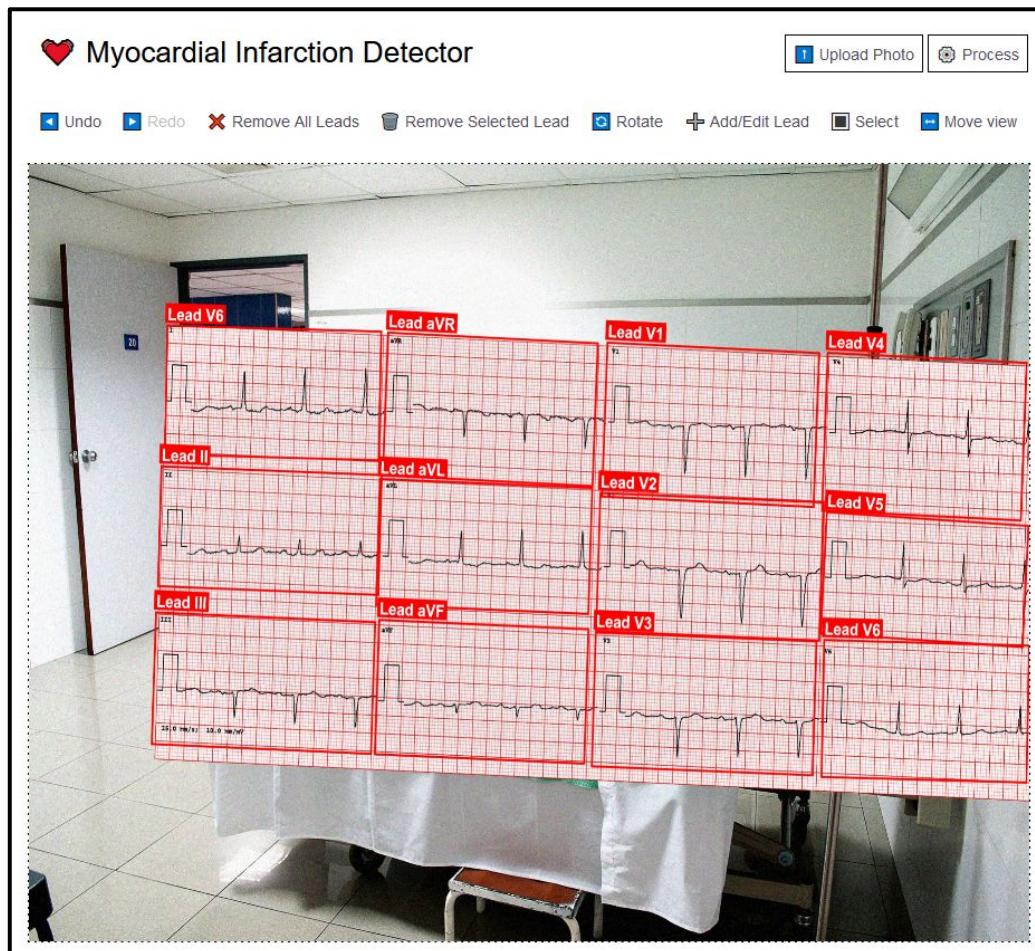
Results on validation dataset of augmented ECG segmentation images

- Big problem: **classification networks overfit!**
  - Cannot perform data augmentation on ECG segmentation images easily on-the-fly
    - Need to **synthesize new ECG photographs**
    - **Time-consuming** process!
- One study (<https://www.ncbi.nlm.nih.gov/pmc/articles/PMC8273385/>) using **10-second time series data** (raw PTB-XL dataset) achieved **precision of 78.9%, recall of 81.8%, F1 score of 0.825** on MIs
- We view our **result** as a **reasonable proof-of-concept**, considering we **only take snippets of ~3 seconds** for each lead and **use distorted image data** rather than pure time series, and did not perform hyperparameter tuning
  - **Shorter lead recordings** are much more **common in practice**

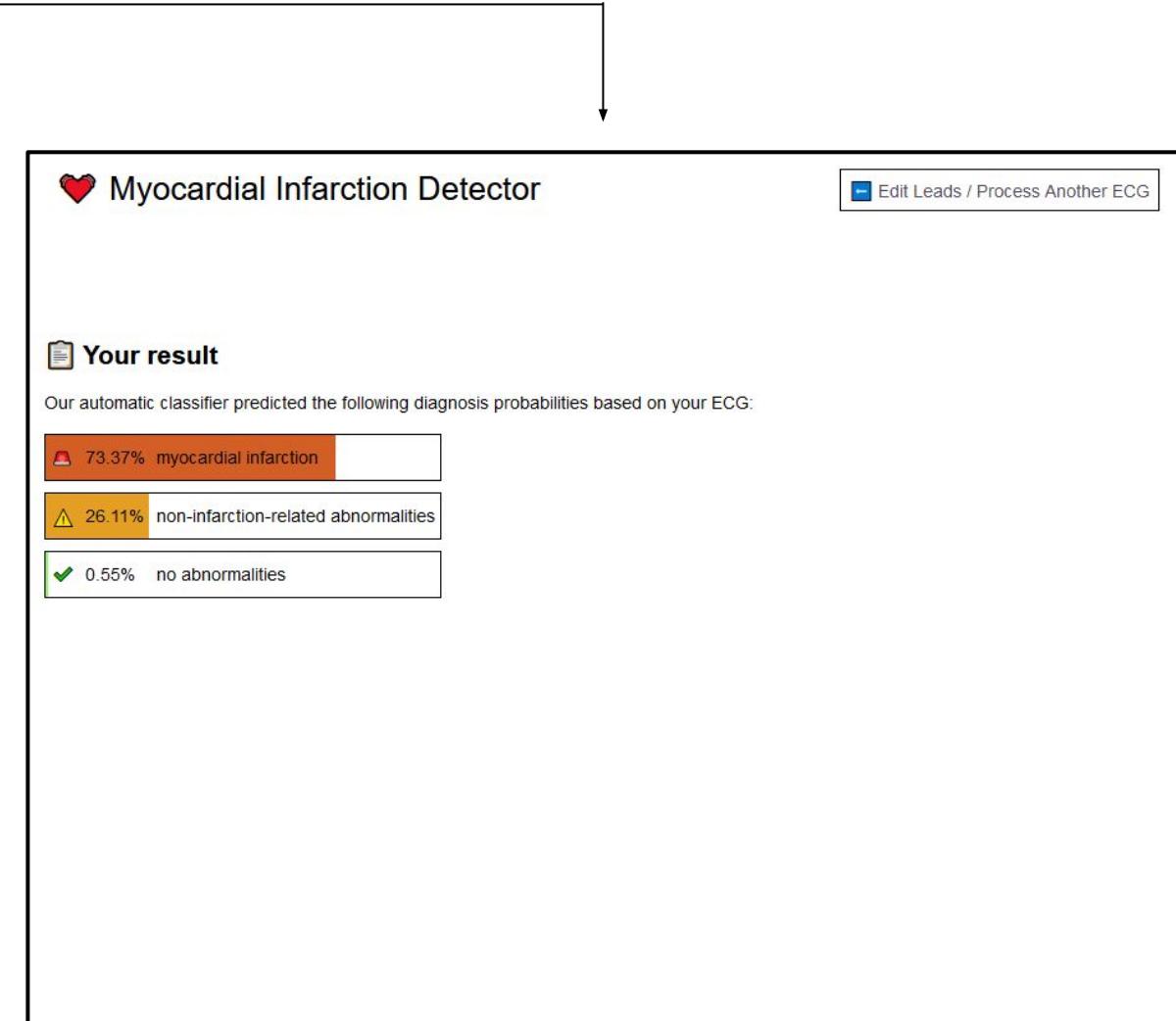


**Validation dataset:**  
**1331** ECG  
segmentations  
**581** normal ECGs  
**462** ECGs w/ **non-MI**  
**abnormalities**  
**288** ECGs w/ **MI**

# 3.4 Web Tool



Current address (temporary): <http://algrithm.com:8080/>



# 4. Future Work

- Use even more data!
  - Can generate nearly unlimited data, but: computationally expensive
  - Move image generation logic to GPU
- Diversify training set
  - Use different lead layouts & lengths
  - Use only subset of 12 leads
- Add support for paper speeds other than default 25mm/s
- Try other architectures for segmentation and classification
- Try to detect lead locations automatically, or provide initial suggestion for user to correct
- Implement noise removal algorithms
  - E.g. correction of baseline drift
- **Test using real ECGs!**

# DEMO



**THANK YOU!**



**Q&A**

