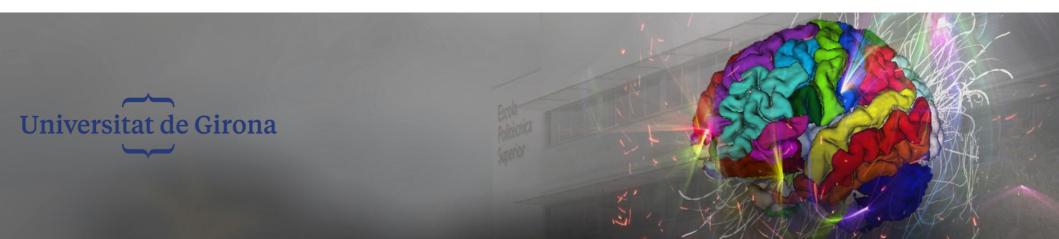


E-Health Visualization

Robert Martí robert.marti@udg.edu





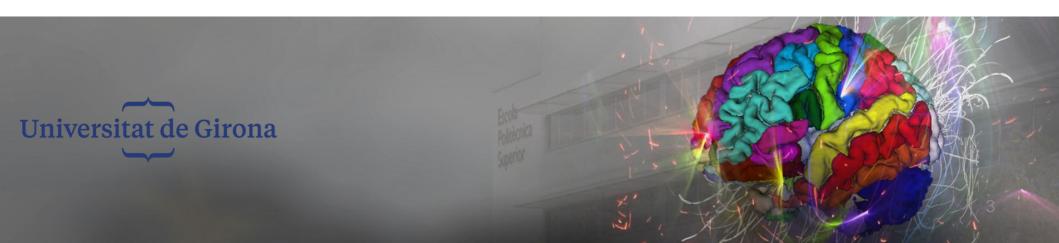
Displaying information

- Resolution
- Bit depth (aka. Bits per pixel): from 8 to 16 bits (integer).
- How can we display a given intensity range?
- Have the same tissues the same intensities in different patients? In MRI? In CT? In US?
- Best way to display information: 2D, 3D, rendering, cineview.



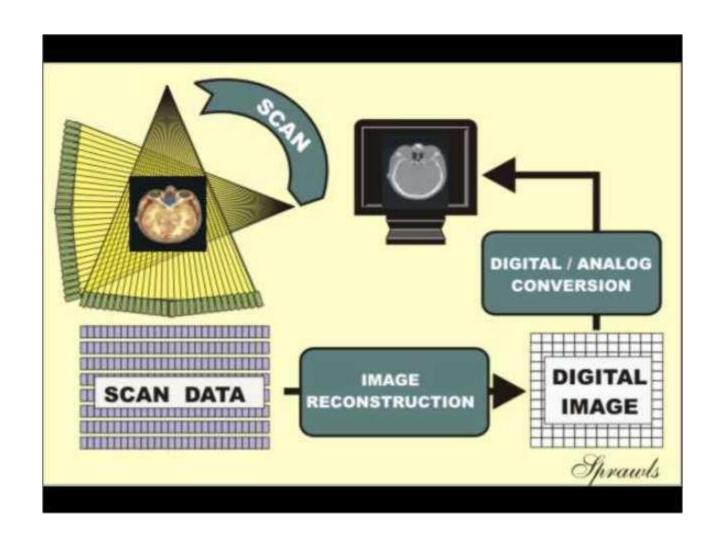


CT





CT image formation

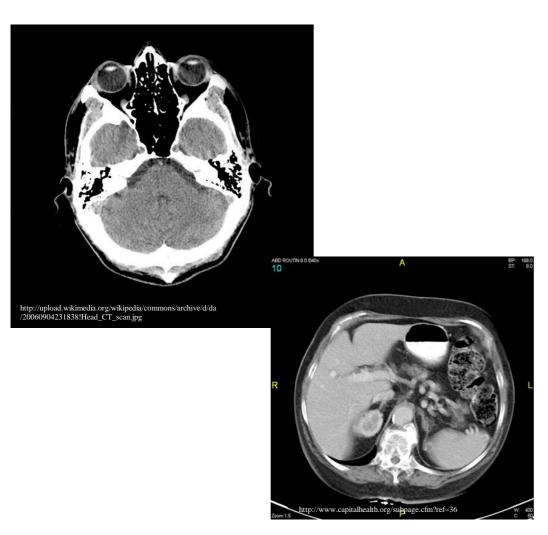




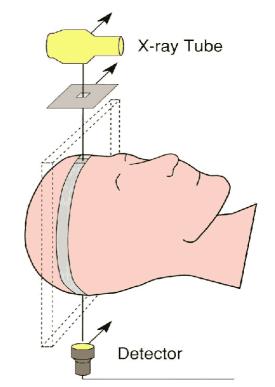


CT information

• CT acquisition.





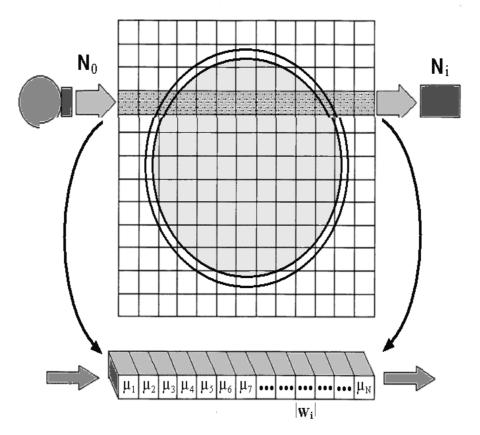


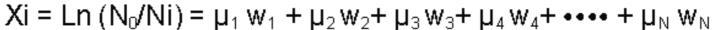




Houndsfield Units

- Also known as CT units.
- Final intensity Ni: weighted sum of tissue attenuation



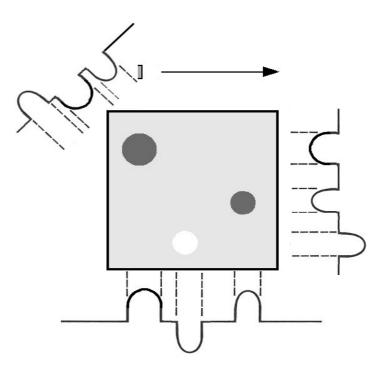






Houndsfield Units

Reconstruction of the 3D volume: backprojection

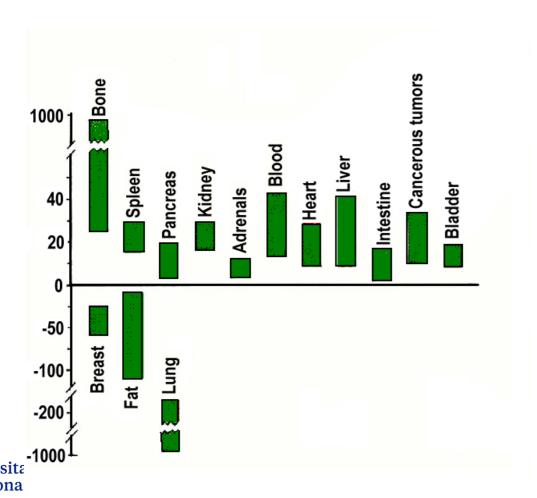






Houndsfield Units

- CT Units or Houndsfield units
- % of the difference with the attenuation of the voxel and the attenuation of water x 1000.



$$CT\# = \left(\frac{\mu_{tissue} - \mu_{water}}{\mu_{water}}\right) \times 1000$$



Windowing

- Windowing: Window width and window level to optimize the contrast of the viewer.
- Level: the midpoint of the window range (Low level: contrast in the lungs or high levels in the bones).
- Width: intensity range

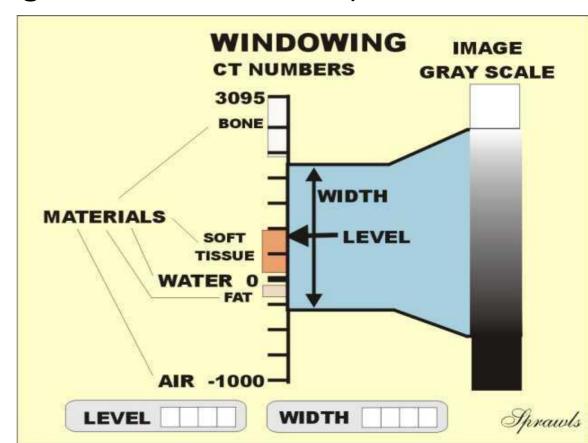






Image quality

- Contrast resolution. Ability to differentiate between different tissue densities.
- High contrast. Ability to see small objects and details with high density compared with the background.
 - Lung nodules/lesions
- Low contrast. Ability to visualise objects with little difference in density.
 - Example: differentiating white matter and grey matterd in CT.

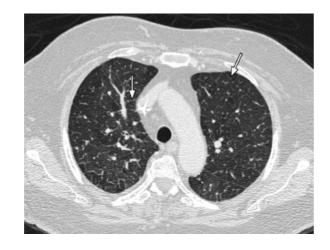








Image quality

- Artifacts: degrade image quality and perception of details.
- Streaks: patient motion or metal and noise
- Rings: problems with the detector
- Shading: problems with the reconstruction (not enough views).







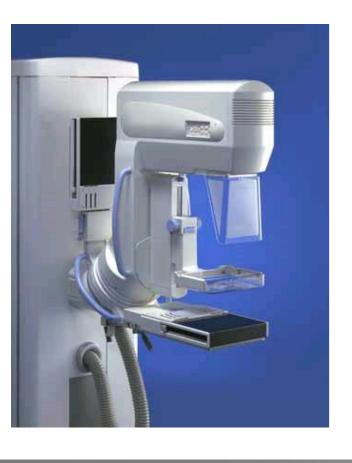


Streaks

Rings and bands

Shading





Mammography





Mammography

"RAW" to "For Presentation"









Grayscale Transforms

- Aplication of lookup tables (LUT) to change grayscale.
- Highest diagnostic information content should be displayed with optimal contrast
- DICOM standard of displays
 - Medical displays should be perceptually linear.
 - DICOM Grayscale Standard Display Function
- If properly calibrated, similar differences in pixel values should be perceived as similar differences in luminance, regardless of the luminance level.

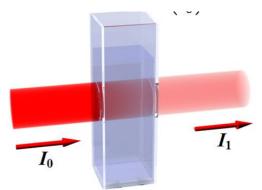




- Film screen response to a x-ray exposure E is determined by its characteristic curve: the relation between the log of the exposure and optical density.
- Exposure (E): concentration of radiation (ionization in a given volume of air) (Roetgens).
- Optical density (D or OD): is a measure of the degree of film darkening (measure of light transmitted through the film-It- with respect to the incident IO)

$$D = \log \frac{I_0}{I_t}$$

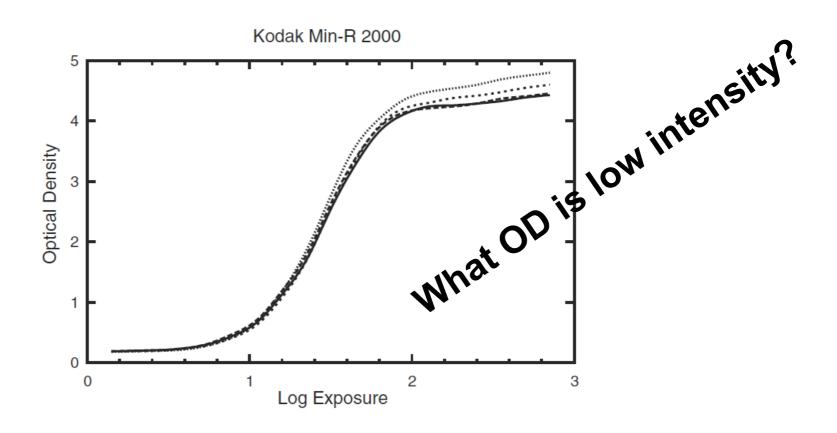
Transmittance (I _t /I ₀)	Percent Transmittance	Inverse of Transmittance (I ₀ /I _t)	Film Density (Log(I ₀ /I _t))
1.0	100%	1	0
0.1	10%	10	1
0.01	1%	100	2
0.001	0.1%	1000	3
0.0001	0.01%	10000	4
0.00001	0.001%	100000	5
0.000001	0.0001%	1000000	6
0.0000001	0.00001%	10000000	7







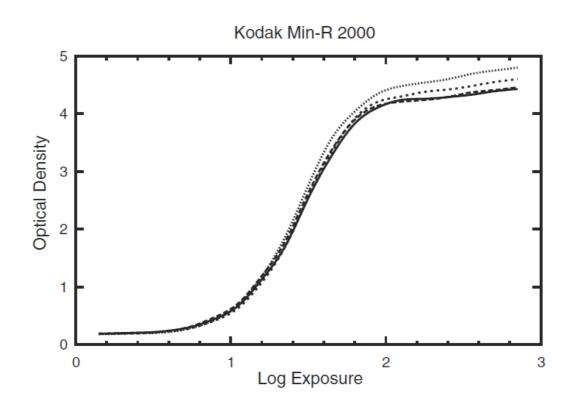
 Film screen response to a x-ray exposure E is determined by its characteristic curve: the relation between the log of the exposure and optical density.







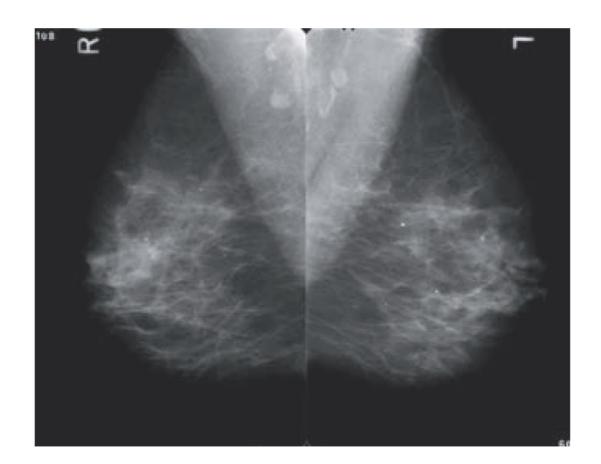
- When viewed in a light box (with luminance I0), the transmitted light is $I = I_0 \log_{10}(-D)$
- Hence applying a similar function to the exposure of FFDM we can estimate the intensity of the image.







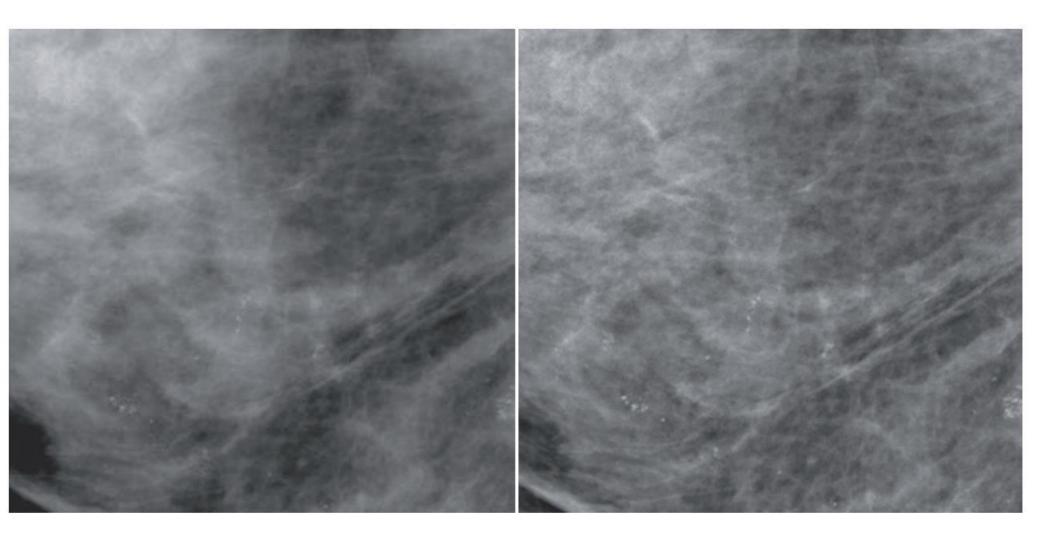
- FFDM images to give them a film like appearance
- With the characteristic curve we can obtain the LUT
- Other LUTs can be applied (linear, non-linear, sigmoid).







Is that enough? Spatial enhancement.





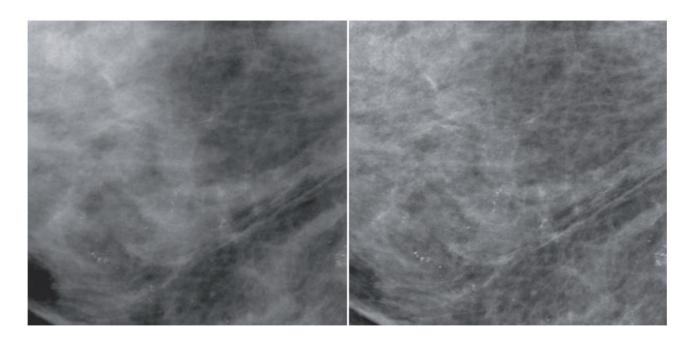


Unsharp masking

$$y_i' = y_i + f(y_i - s_i(\sigma))$$

New image yi' (si, smoothing, f amount of enhancement)

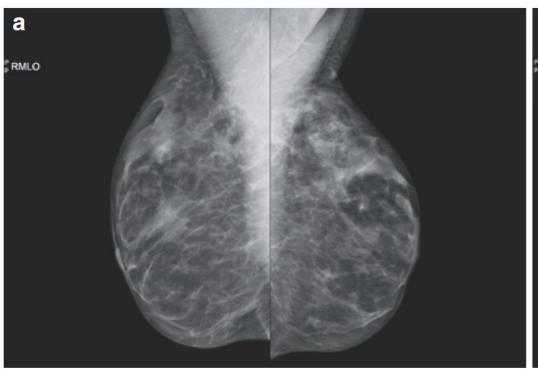
- Basically, subtracting a smoothed version of the image.
- Matlab: B = imsharpen(A)
- Enhances high frequency: edges (and noise!).

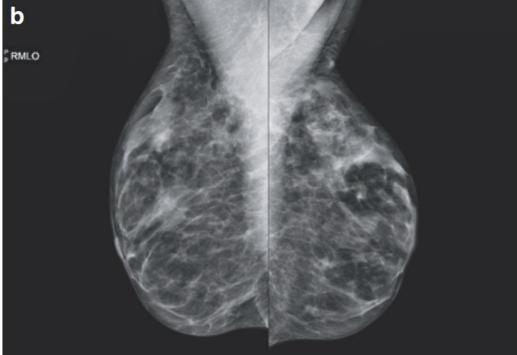






- Adaptative Histogram Equalization (CLAHE)
 - Locally (patches) equalise the histogram to a given statistical distribution (parameter).
 - Matlab: J = adapthisteq(I)

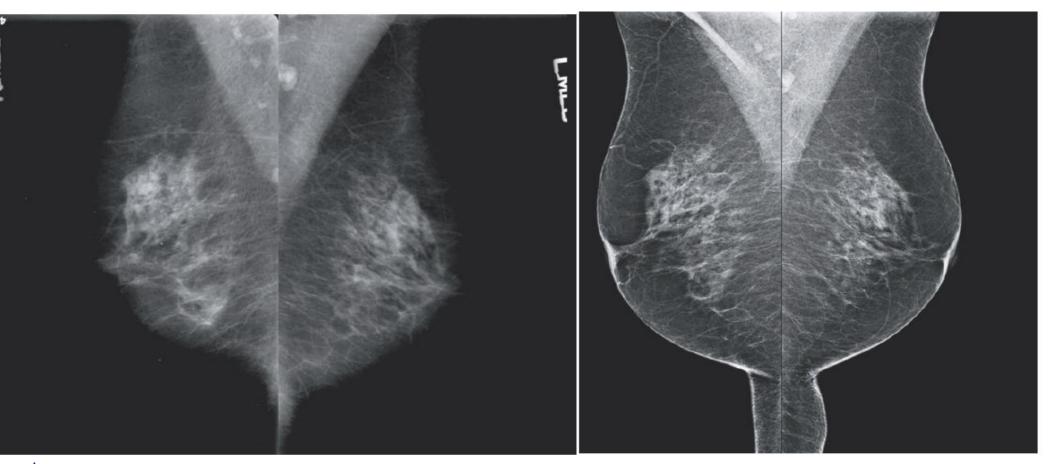








- Other (vendor specific) post-processing approaches.
- Application specific: Breast Peripherial Enhancement.







Breast Peripherial Enhancement.

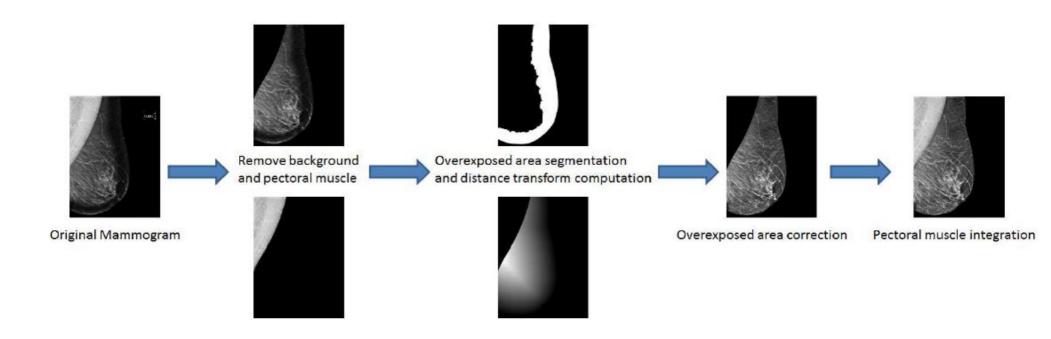








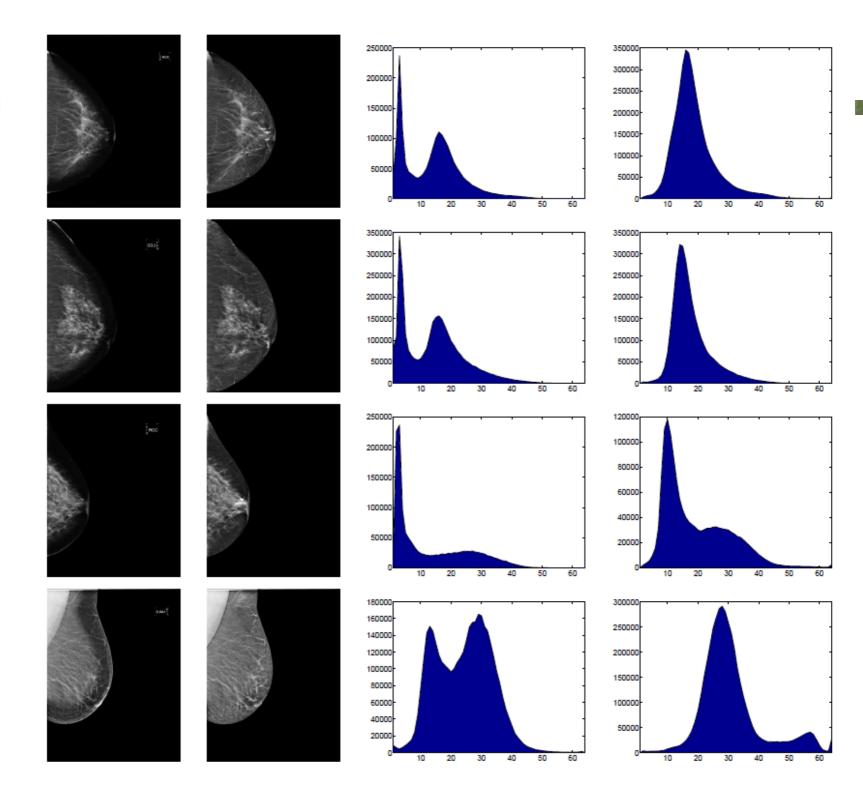
Breast Peripherial Enhancement.



$$I'(x) = I(x) \frac{\overline{I}_{N_{in}(x)}}{\overline{I}_{N(x)}}$$



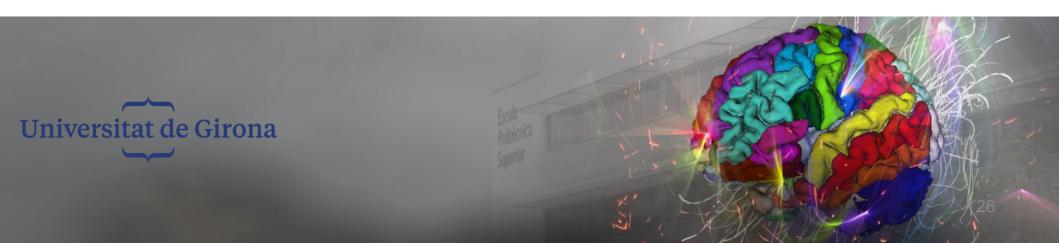








Medical Displays & Calibration

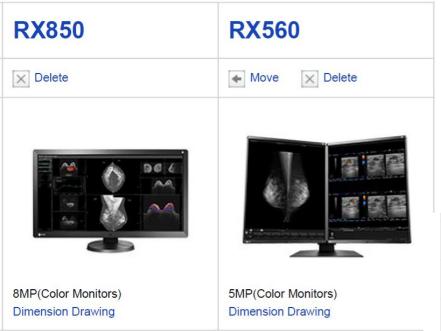




Medical Displays

Brightness (typical)

Several Manufacturers (Eizo, Totoku, Barco, ...)



Recommended Brightness for Calibration	500 cd/m ²	500 cd/m ²
Contrast Ratio (typical)	1450:1	1500:1
Response Time (typical)	20 ms (on / off)	12 ms (on / off)
Туре	Color (IPS)	Color (IPS)
Backlight	LED	LED
Size	79 cm / 31.1"	54.1 cm / 21.3"
Native Resolution	4096 x 2160 (17:9 aspect ratio)	2048 x 2560 (4:5 aspect ratio)
Viewable Image Size (H x V)	697.9 x 368.0 mm	337.9 x 422.4 mm
Pixel Pitch	0.1704 x 0.1704 mm	0.165 x 0.165 mm
Display Colors	10-bit colors (DisplayPort) : 1.07 billion (maximum) colors 8-bit colors: 16.77 million from a	10-bit colors (DisplayPort) : 1.07 billion (maximum) colors 8-bit colors: 16.77 million from a

palette of 68 billion colors

850 cd/m²



palette of 68 billion colors

1100 cd/m²



Medical Displays



Momentum QHD LCD display with a M Line, 32 (31.5" / 80 cm diag.), Quad HD (2560 x 14 ers (Eizo, Totoku, Barco, ...) similar products >

	_
Overview	Specifications
Backlight type	W-LED system
Panel Size	31.5 inch / 80 cm
Color gamut (typical)	NTSC 108%*, sRGB126%*
Effective viewing area	698.11 (H) x 392.69 (V)
Aspect ratio	16:9
Optimum resolution	2560 x 1440 @ 60 Hz
Pixel Density	93 PPI
Response time (typical)	5 ms (Gray to Gray)*
Brightness	250 cd/m²
Contrast ratio (typical)	1200:1
SmartContrast	50,000,000:1
Pixel pitch	0.273 x 0.273 mm
Viewing angle	• 178º (H) / 178º (V)
	• @ C/R > 10
Flicker-free	Yes
Picture enhancement	SmartImage
Display colors	1.07G (8bits + FRC)
Scanning Frequency	30 - 83 kHz (H) / 48 - 76 Hz (V)
sRGB	Yes

Brightness (typical)	850 cd/m ²	1100 cd/m ²
Recommended Brightness for Calibration	500 cd/m ²	500 cd/m ²
Contrast Ratio (typical)	1450:1	1500:1
Response Time (typical)	20 ms (on / off)	12 ms (on / off)
Туре	Color (IPS)	Color (IPS)
Backlight	LED	LED
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a/producta/radifa	roo/ry050/inday html	28



Medical Displays

See

http://www.eizoglobal.com/products/radiforce/rx850/index.html

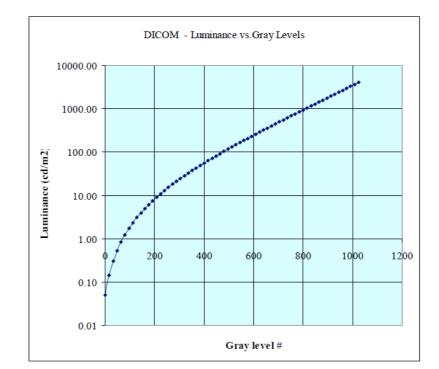
Study on the Efficiency of RadiForce RX850 in Mammography





- DICOM standard part 14. Grayscale Standard Display Function (GSDF).
- http://dicom.nema.org/dicom/2004/04 14pu.pdf
- The way human eye responds to contrast in light levels is not linear. At higher luminance, the change needs to be much greater before we perceive the difference from one

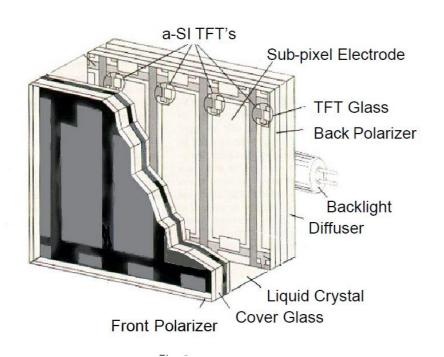
level to the next.

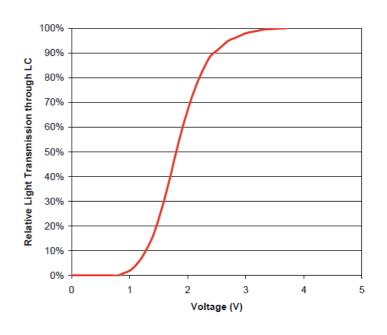






- Need to calibrate medical displays.
- The amount of light to control pixels is also non linear



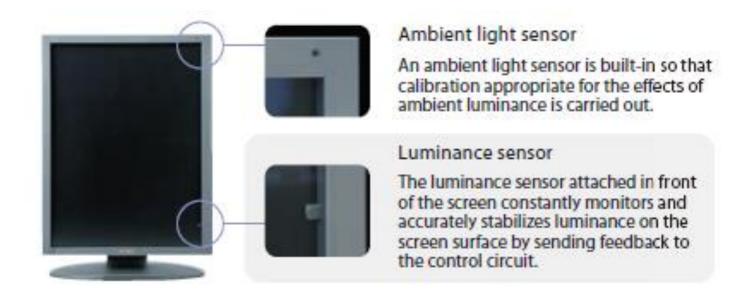






- Two variables involved
 - Peak luminance. Maintain a constant maximum luminance (declines with time) of the backlight.
 - Gray level separation. Provide the accurate voltage to obtain the accurate level of light to achieve the DICOM standard.

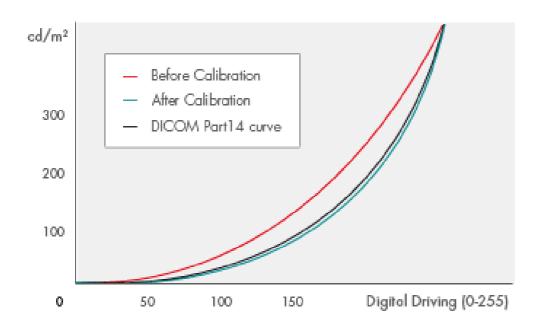








- Two variables involved
 - Peak luminance. Maintain a constant maximum luminance (declines with time) of the backlight.
 - Gray level separation. Provide the accurate voltage to obtain the accurate level of light to achieve the DICOM standard.









Home > Products > RadiForce > RadiCS UX2

RadiCS UX2

Quality Control Software & Calibration Sensor

RadiCS provides total support for the quality maintenance and control of client monitors, covering everything from calibration to acceptance and constancy tests, calibration asset, and historical management. Complying with AAPM, DIN, IEC and other standards, RadiCS enables precise QC with easy-to-follow procedures.

Contact EIZO



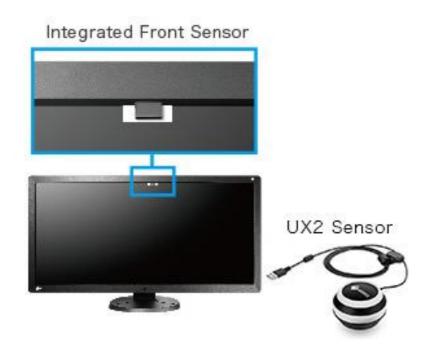








Support for different display functions: DICOM Part 14
GSDF, CIE, Exponential (gamma value), Log Linear, Linear,
User definition.







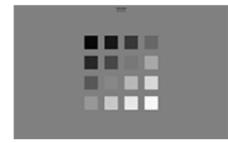
QC standards



"Assessment of Display Performance for Medical Imaging Systems" formulated by Task Group (TG) 18 of American Association of Physicists in Medicine.

ACR-AAPM-SIIM "Practice Guideline for Determinants of Image Quality in Digital Mammography"

This guideline was formulated collaboratively by specialists in mammography and medical physics who represent the American College of Radiology (ACR), the American Association of Physicists in Medicine (AAPM), and the Society for Imaging Informatics in Medicine (SIIM).



New York State Department of Health Bureau of Environmental Radiation Protection

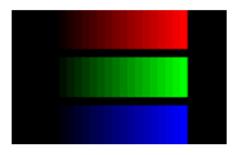
Guide for Radiation Safety / Quality Assurance Program Primary Diagnostic Monitors

The guidelines describe the types and extension of information and criteria used by the New York State Department of Health Bureau of nvironmental Radiation Protection to evaluate Primary Diagnostic Monitor (PDM) in facilities as a part of the radiation safety and quality assurance program.

NYC Quality Assurance Guidelines for Primary Diagnostic Monitors

Refers to the "Guidance related to quality assurance for Primary Diagnostic Monitor (PDM)" based on the health regulations of New York city provided by the New York City Health Department's Office of Radiological Health.





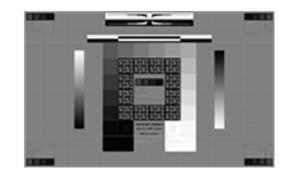


Calibration and QC

QC standards

EUREF "European Guidelines for Quality Assurance in Breast Cancer Screening and Diagnosis Fourth Edition"

This guideline was issued by the European Commission in cooperation with EUREF (European Reference Organization for Quality Assured Breast Screening and Diagnostic Services), EBCN (European Breast Cancer Network), and EUSOMA (European Society of Mastology).

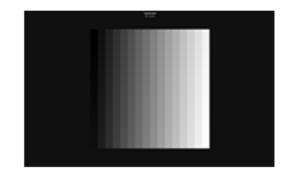


IPEM Report 91

"Recommended Standards for the Routine Performance Testing of Diagnostic X-ray Imaging Systems" formulated by the Institute of Physics and Engineering in Medicine in the UK.

DIN 6868-157

"Image quality assurance in diagnostic X-ray departments – Part 157: X-ray ordinance acceptance and constancy test of image display systems in their environment" formulated by the German Institute for Standardization (Deutsches Institut für Normung e.V).





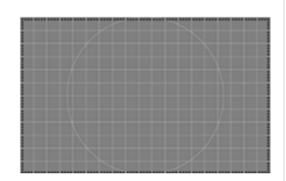


Calibration and QC

QC standards



"Image Quality Assurance in X-ray Diagnosis - Part 20: Acceptance test and consistency test for image display devices" formulated by the Austrian Standards Institute).



JESRA X-0093 * B-2017

"Quality Assurance (QA) Guideline for Medical Imaging Display Systems" formulated by Japan Industries Association of Radiological Systems (JIRA).

Quality Control Manual for Digital Mammography

A quality control manual for digital mammography systems written by the

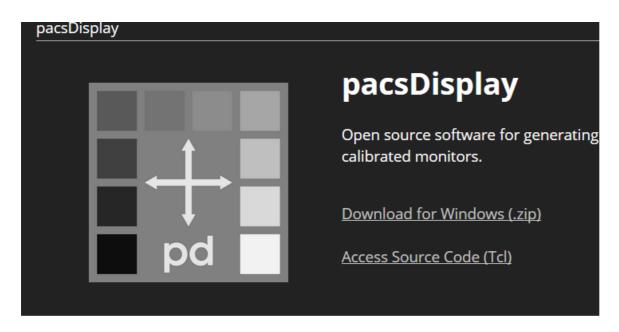
Japan Central Institute on Quality Assurance of Breast Cancer Screening, a nonprofit organization, in

Japan. This NPO studies and manages quality control of mammography.





Calibration



http://pacsdisplay.org/

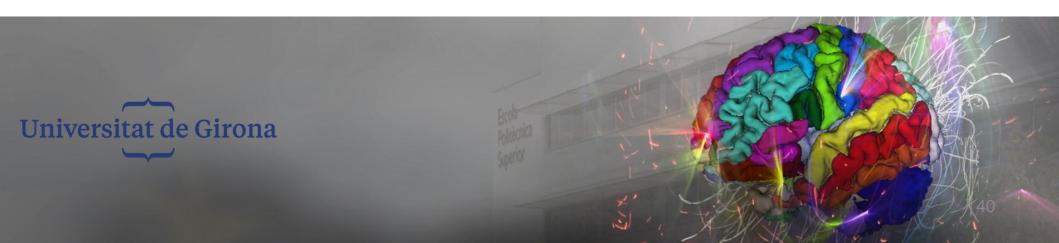


http://perfectlum.com/





Types of visualization



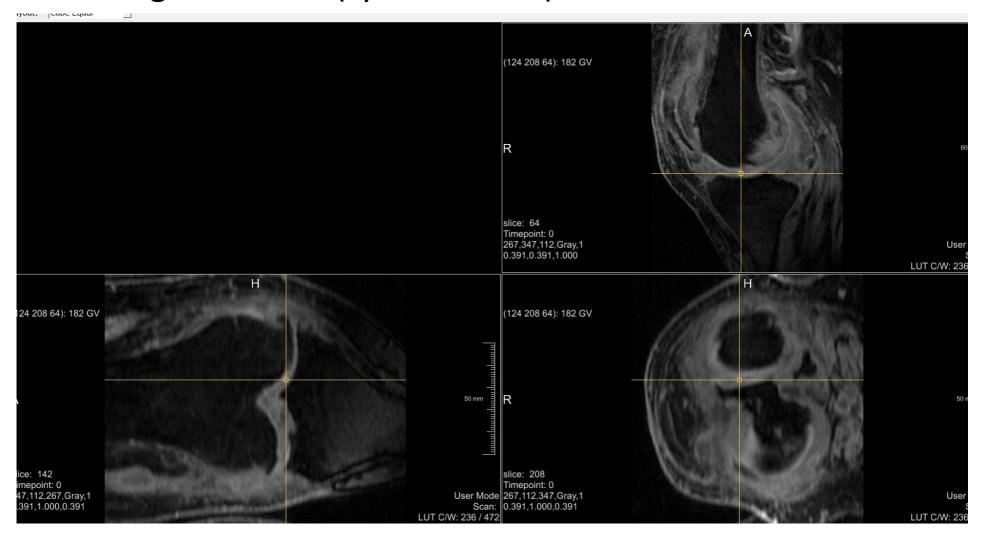


Hanging protocols





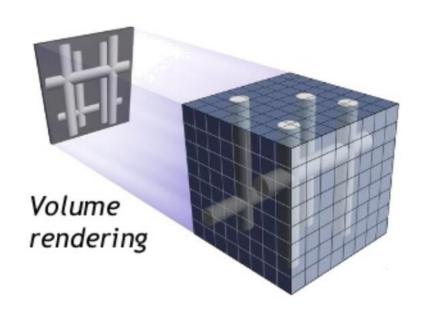
Orthogonal views (synchronised).

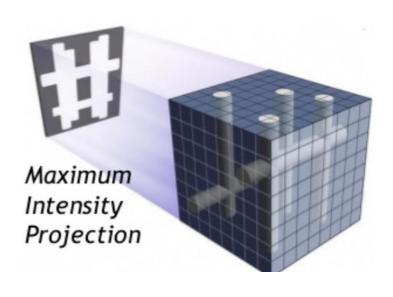






In addition to slice by slice display









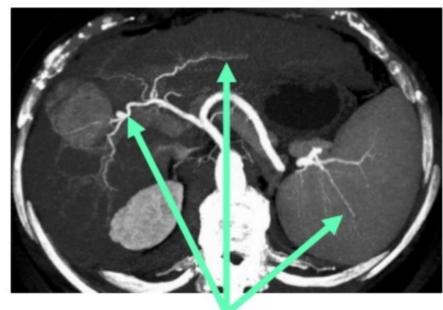
In addition to slice by slice display

Volume Rendering



Provides more 3D feel by accounting for occlusion

Maximum Intensity Projection

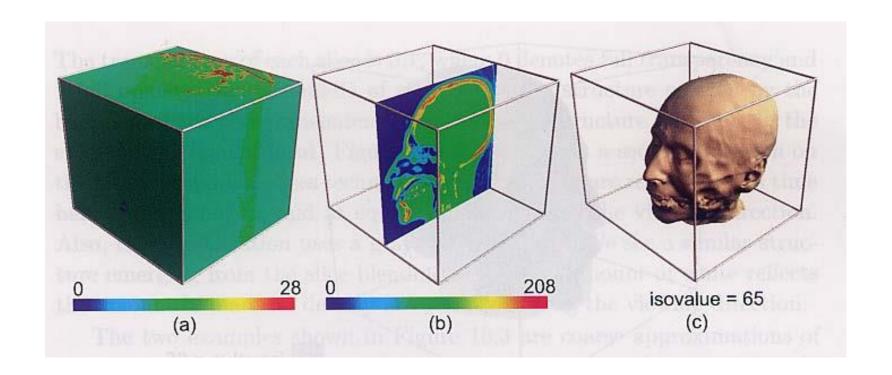


Good at mapping arterial structure, despite occlusion





- Displaying scalar values (3D image)
 - Surface, slice, or isosurface.

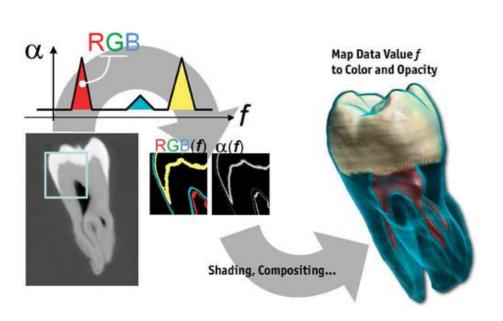


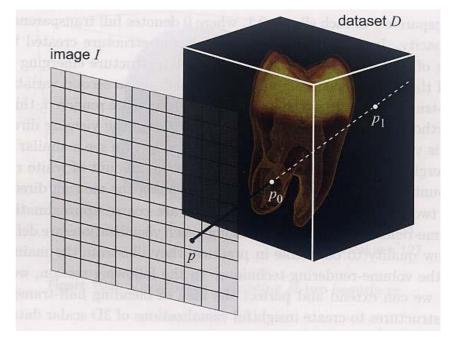




Volume rendering

- Transfer function (s): Mapping for each tissue type (scalar value) a colour and opacity.
- Image projection (Ray casting): take into account (integrate) the voxels that each ray casts. Ray function (F)



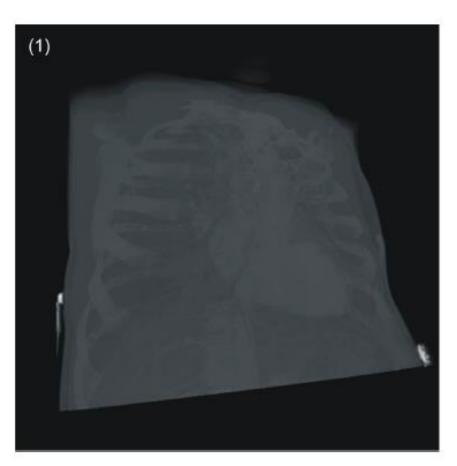


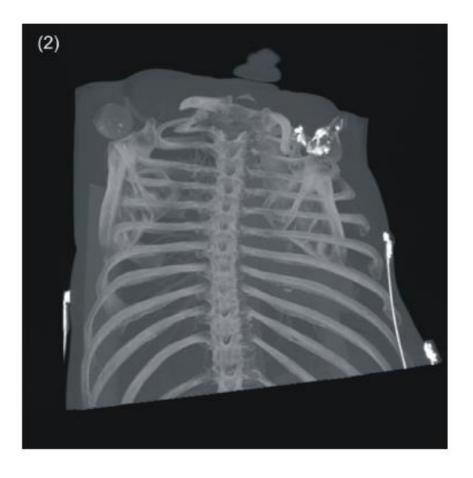
$$I(p) = F(s(t)), t \in [0,1]$$





- Volume rendering
 - Ray casting: maximum, mean and minimum intensity.

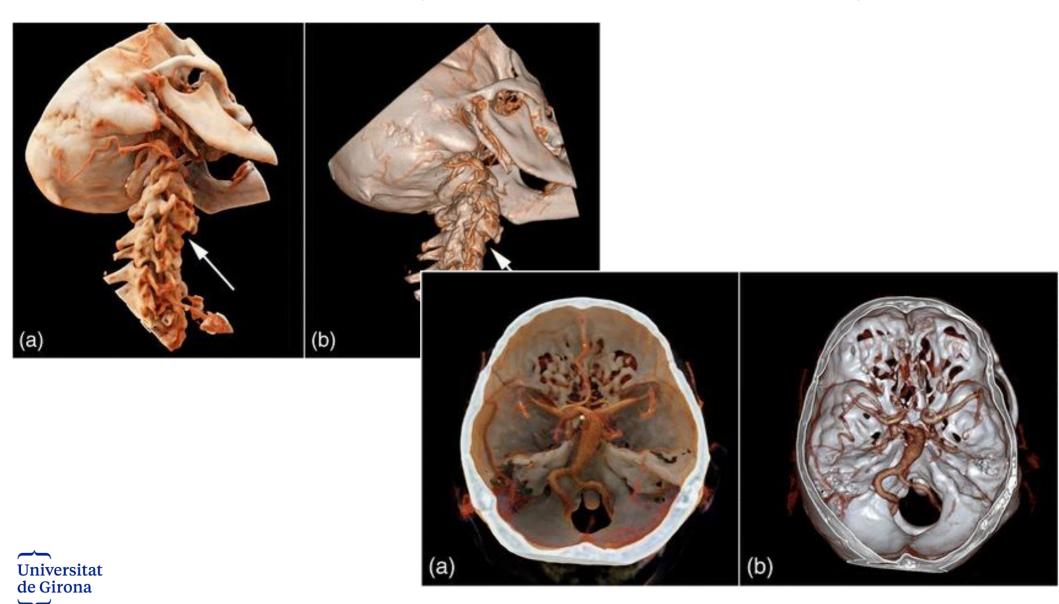






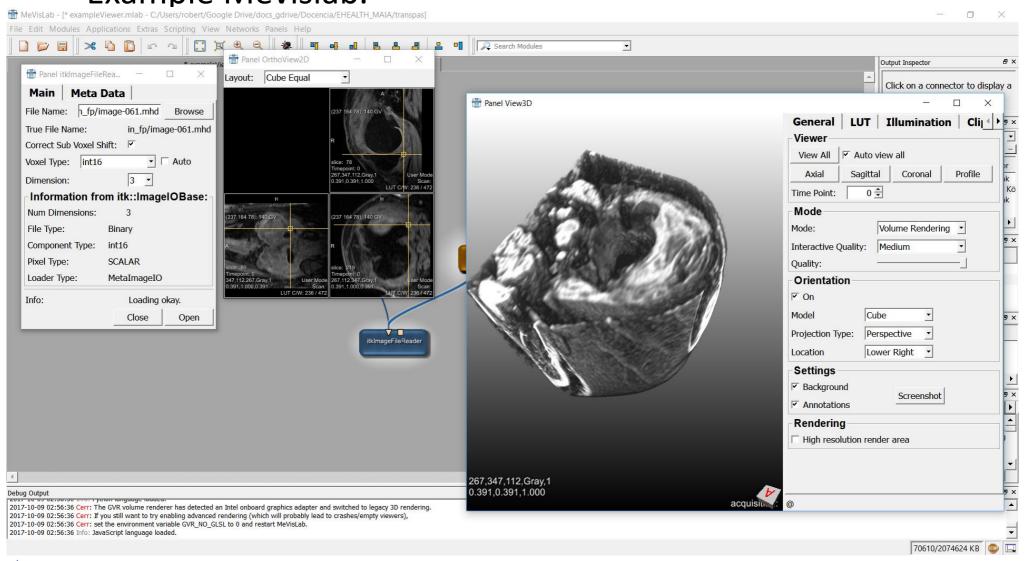


3D Volume Rendering (VR) vs Cinematic Rendering (CR)





• Example Mevislab.







Bibliography

- <u>www.aycan.com/applications/mammography/advanced-hanging-protocols.html</u>
- http://pacsdisplay.org/
- http://www.eizoglobal.com/products/radiforce/index.html
- Karssemeijer N., Snoeren P.R. (2010) Image Processing. In: Bick U., Diekmann F. (eds) Digital Mammography. Medical Radiology. Springer, Berlin, Heidelberg
- Digital Imaging and Communications in Medicine (DICOM)
- Part 14: Grayscale Standard Display Function.
 http://dicom.nema.org/dicom/2004/04_14pu.pdf
- Cinematic rendering an alternative to volume rendering for 3D computed tomography imaging. https://link.springer.com/article/10.1007%2Fs13244-016-0518-1

