

Lecture 4 –X ray Imaging Application

This lecture will cover:

- Characteristics of X-ray images (CH2.8)
 - SNR
 - Resolution
 - CNR
- Digital Subtraction Imaging (*CH2.9-2.10.1*)
 - X-ray contrast agents
 - Digital Subtraction Angiography
 - Dual-energy Subtraction
- Specialized X-ray imaging techniques (CH2.10.2-2.10.3)
 - Digital Fluoroscopy
 - Digital mammography
- Clinical applications

Signal-to-noise ratio



N X-ray strike the detector per unit area (Poisson distribution)

$$P(N) = \frac{\mu^N e^{-\mu}}{N!}$$

Where variation $\sigma = \sqrt{\mu}$

SNR
$$\propto \sqrt{N}$$

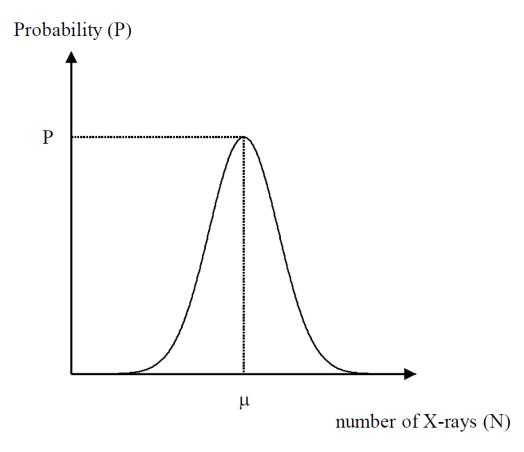


Figure. The probability of a certain number of X-rays striking a unit area of the detector. The statistical uncertainty in this number is represented by the standard deviation (r) of the Poisson distribution.

Signal-to-noise ratio



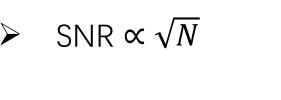
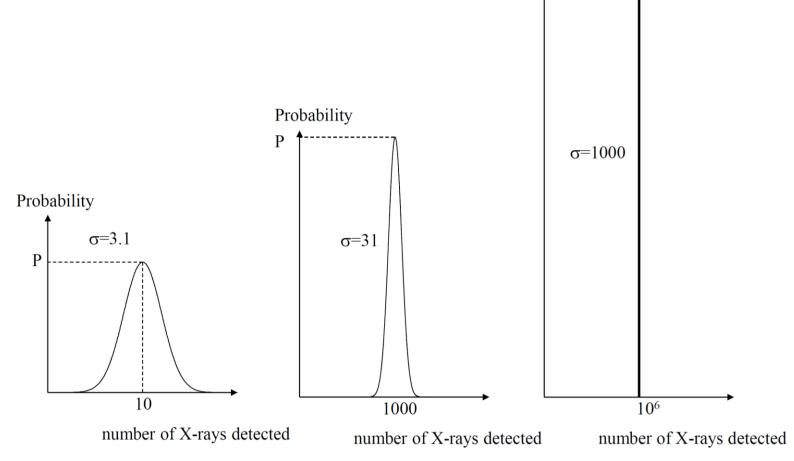


Figure. Plots of a Poisson distribution with increasing number of X-rays produced. As the number increases, the distribution becomes narrower, with the mean number of events and the total number of events converging to the same value.



Probability





- The tube current and exposure time: square root of the product of these two quantities
- The tube kVp: increase SNR with higher voltage, non-linear effect
- The patient size and part of the body being images: the bigger, the lower SNR
- The geometry of the anti-scatter grid: large grid ratio, lower SNR.
- The efficiency of the detector: detector quantum efficiency (DQE)

$$DQE = \left[\frac{SNR_{out}}{SNR_{in}}\right]^2$$





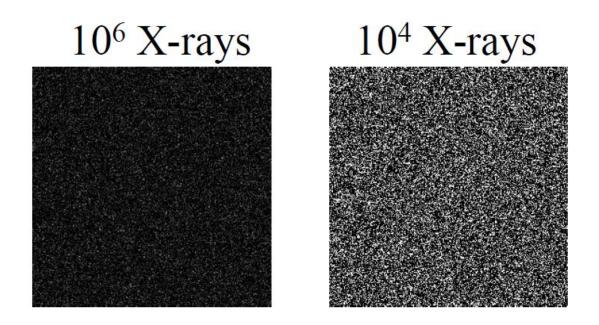


Figure. The effect of radiation dose (total number of incident X-rays) on the SNR of a planar image with no patient in place. The image on the left has 100 times the number of X-rays per pixel, and so has 10 times higher SNR.

Spatial resolution



- ➤ A combination of the contributions from each part of imaging process:
 - Size of focal spot:

$$f = F \sin \theta$$

• Distance between X-ray tube and the patients (S_0) and distance between X-ray tube and detector (S_1)

$$P = \frac{f(S_1 - S_0)}{S_0}$$

 The properties of X-ray detector: number of pixels in the images

Figure. A finite effective spot size as well as the tube—patient (S0) and tube—detector (S1) distances determine the spatial resolution of the image. The 'geometric unsharpness' or penumbra (P) causes features and edges in the image to become blurred, as shown on the right..

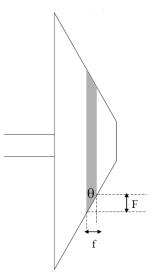
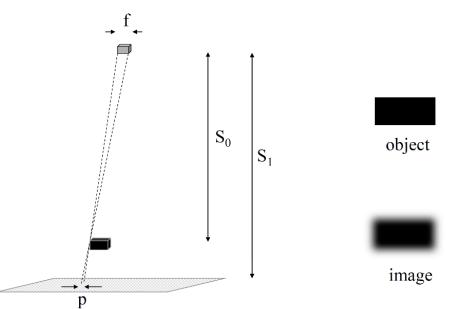


Figure. The effect of the bevel angle h on the effective focal spot size (f) as a function of the width of the electron beam (F).



Contrast-to-noise ratio



Factors affecting CNR

- Compton scattered X-ray
 - X-ray energy spectrum
 - The field of view (FOV, 视野) of X-ray image linear in 10-30cm, constant above 30cm
 - The thickness of the body being imaged
 - The geometry of the anti-scatter grid
- \triangleright SNR: $CNR_{AB} = |SNR_A SNR_B|$
- Spatial resolution



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Contrast agent (造影对比剂)



Referring to the chemical substance introduced into the body

- Orally or injected into the bloodstream;
- Accumulated in a particular organ or structures
- Enhance the contrast between the structure and surrounding tissue
- Used in X-ray, Ultrasound, MRI, entirely for nuclear medicine
- Provide maximum contrast for the minimum administered dose
- Adverse side-effect: give the maximum contrast for the minimum administered dose

X-ray Contrast agent



- ➤ Efficient at absorbing X-ray strong contribution from photoelectric interaction
- > Two classes of X-ray contrast agent
 - Gastrointestinal (GI) tract (胃肠道疾病)
 - ✓ Orally, rectally, nasal cannula
 - Iodine-based agent
 - ✓ Water-soluble iodinated compounds (水溶性碘化物)
 - ✓ Injected into the bloodstream
 - ✓ For visualization of vasculature

Agent for the GI tract



- ➤ Barium sulphate (硫酸钡)
- Orally (upper GI tract), rectally(lower GI tract), nasal cannula
- With agent white; without agent (low absorption) dark

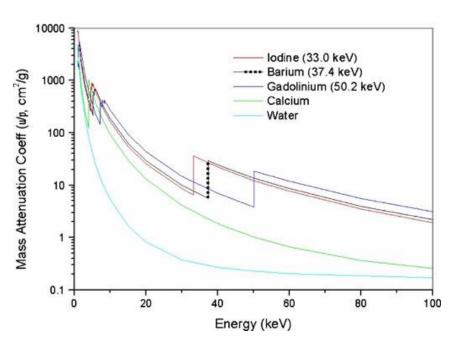


Figure. The mass attenuation coefficient of Iodine, Barium sulphate, and Gadolinium as a function of X-ray energy.

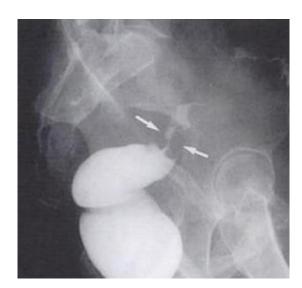


Figure. A barium sulphate enhanced image of the colon shows an adenocarcinoma (white arrows). The high attenuation of the barium sulphate produces a very high (white) image intensity.

lodine-based contrast agent



- Iodine: K-shell binding energy 33.2 KeV
- Small vessel of ~50μm diameter to be detected
- Lowest dose applied to minimize the side-effect

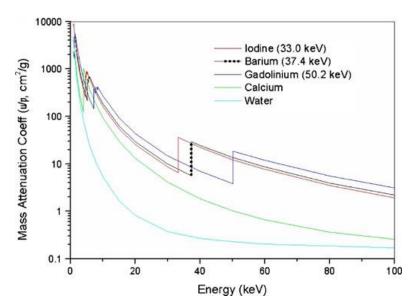


Figure. The mass attenuation coefficient of Iodine, Barium sulphate, and Gadolinium as a function of X-ray energy.

(a) (b)
$$I \xrightarrow{R_1} I \qquad I \xrightarrow{R_1} I \qquad I \xrightarrow{R_2} I \qquad R_3$$

$$R_1 = R_2 = R_3 = CONHCH_2CH(OH)CH_2OH$$

$$L = N(COCH_3)CH_2CH(OH)CH_2N(COCH_3)$$

Figure. (a) Generic formula for a monomeric iodinated X-ray contrast agent. The side-groups R1, R2 and R3 can all be the same or different. (b) Generic form of a dimeric agent, in which the two benzene rings are joined by a chemical linker (L). The chemical structure of iodixanol, which is both iso-osmolar with blood and also non-ionic, is shown.

Digital Subtraction Angiography



Digital Subtraction Angiography (DSA, 数字减影血管造影):

- ➤ High resolution images of the vasculature
- Subtraction image between a regular image and an image acquired by injecting with lodine-based contrast agent

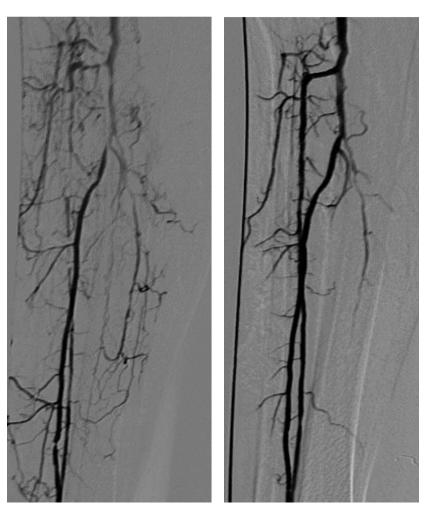


Figure. Digital subtraction angiograms showing fine vessel structures. The vessels containing iodinated contrast agent are shown as dark areas in the subtraction images

Digital Subtraction Angiography



The regular image:

$$I = I_0 e^{-(\mu_B d_B + \mu_T d_T)}$$

The injection image:

$$I_1 = I_0 e^{-[\mu_B d_B + \mu_T (d_T - d_I) + \mu_I d_I]}$$

The subtraction image

$$\ln I - \ln I_1 = (\mu_I - \mu_T)d_I$$

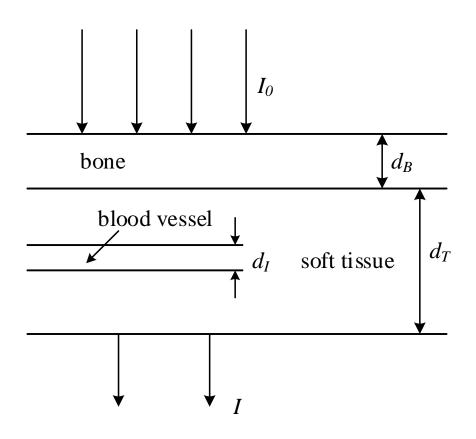


Figure. The schematic diagram of subtraction imaging.





The subtraction image can be acquired

- By sequencing
 - 1. The mask (掩模、蒙片) image at t=0
 - 2. Producing images of the same area at a set rate (1 to 7.5 frames per second)
 - 3. Finding the subtraction image with the highest contrast.
- By energy
 - K-edge: acquire two images at lower and higher K-shell energy (33KeV) of iodine
 - **Dual energy**: subtract bone or soft tissue effect
- > By combination of sequencing and energy

Dual-energy Subtraction



For lower energy:

$$\ln I_L = \ln I_{0L} - (\mu_{BL} d_B + \mu_{TL} d_T)$$

For higher energy:

$$\ln I_{H} = \ln I_{0H} - (\mu_{BH} d_{B} + \mu_{TH} d_{T})$$

The subtraction image

$$S = K_H \ln I_H - K_L \ln I_L$$

= $K_H \ln I_{0H} - K_L \ln I_{0L} + (K_L \mu_{BL} - K_H \mu_{BH}) d_B + (K_L \mu_{TL} - K_H \mu_{TH}) d_T$

- For bone subtraction: $\frac{K_H}{K_L} = \frac{\mu_{BL}}{\mu_{BH}}$
- For tissue subtraction: $\frac{K_H}{K_L} = \frac{\mu_{TL}}{\mu_{TH}}$

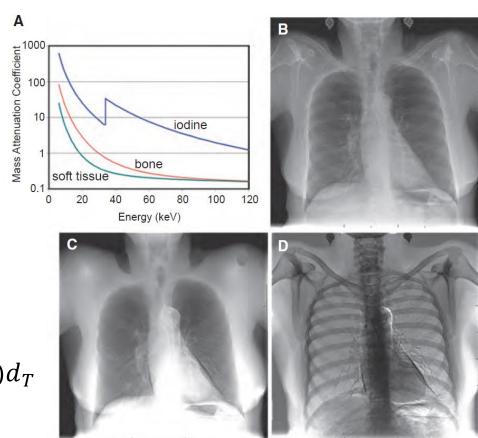


Figure. Dual-energy chest radiography is illustrated. A. The linear attenuation coefficients for soft tissue, bone, and iodine are shown. B. The single-energy (120 kV) radiograph is shown. C. The bone-subtracted, soft tissue—only image is illustrated. This image shows the lung parenchyma and mediastinum, which are the principal organs of interest on most chest radiographs. D. The soft tissue-subtracted, bone-only image is illustrated. Note that the earrings, which are made of metal and are more similar to bone than soft tissue in terms of composition, show up on the bone-only image.





The subtraction image can be acquired

> By combination of sequencing and energy

- Energy subtraction for soft tissue
- Sequencing subtraction for hard tissue (bone)

 I_{0L} : regular image from low energy

 I_{0H} : regular image from high energy

 I_{1L} : contrast image from low energy

 I_{1H} : contrast image from high energy

 S_{0T} : regular tissue subtraction image derived from I_{0L} and I_{0H}

 S_{1T} : contrast tissue subtraction image derived from I_{1L} and I_{1H}

S: final subtraction image where $S = S_{0T} - S_{1T}$



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Digital Fluoroscopy



Digital Fluoroscopy (荧光透视,数字透视):

- ➤ Continuous X-ray imaging for monitoring interventional surgery or dynamic studies of contrast agent
- Minor modification of DR
 - Increase thickness of detector for higher detection efficiency
 - Short pulse of X-ray: ~5-20ms
 - 30 frame/second
 - Low dose for each frame, lower SNR and CNR



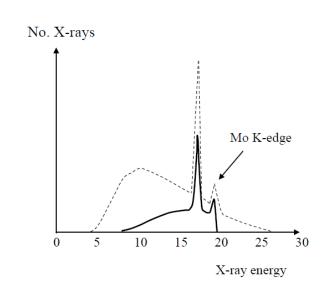
Figure. A neurointerventional unit, with a C-arm digital fluoroscopy unit.

Digital mammography



Digital mammography (乳腺X线摄影):

- > Detecting small tumors or microcalcifications in breast
- ➤ Technique specification
 - High spatial resolution and CNR
 - Low radiation dose: Molybdenum anode (钼靶)
 - Small focal spot (≤0.3mm): (1) flat cathode (2) small bevel angle
 - Molybdenum filter: reduce high energy X-ray
 - Large focal-spot-to-detector distance (45-80cm)
 - Compression of breast during exam: to improve transmission and reduce Compton scatter.



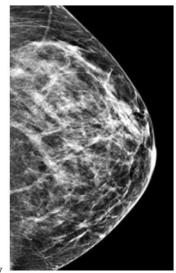


Figure. (Top) The X-ray spectrum used for digital mammography. The kVp of the X-ray tube is 26 keV. The anode is made from molybdenum and produces a substantial number of low energy X-rays (dashed line). A 30 μm thickness molybdenum filter is used to reduce the contribution from very low energy X rays (solid line). (Bottom) Example of a digital mammogram, showing very high spatial resolution.



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Bone fracture



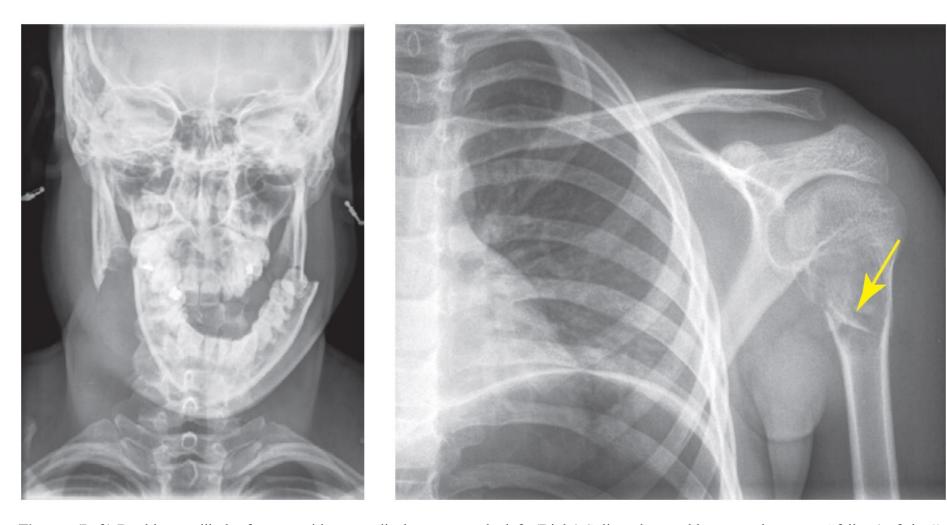


Figure. (Left) Double mandibular fracture with strong displacement to the left. (Right) Solitary humeral bone cyst known as "fallen leaf sign".

Lung metastases



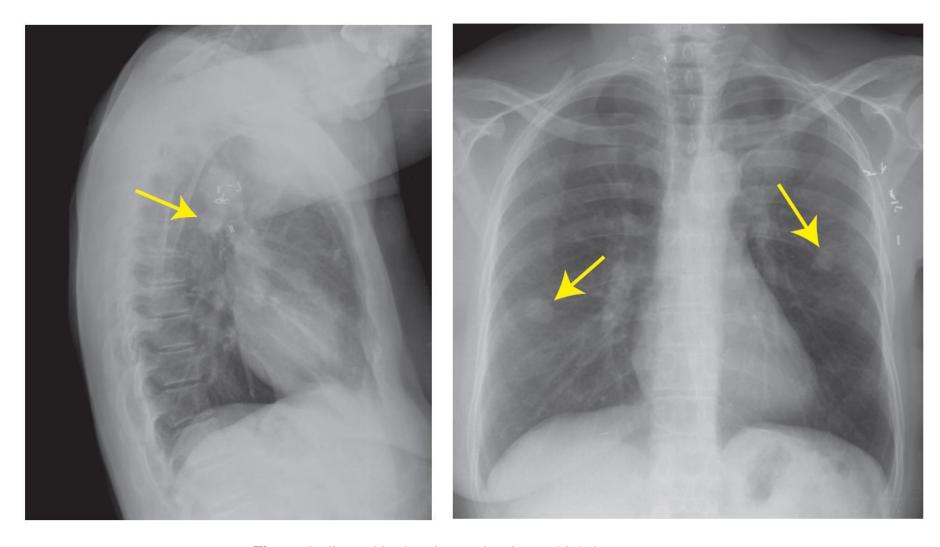


Figure. Radiographic chest image showing multiple lung metastases.

Breast carcinoma



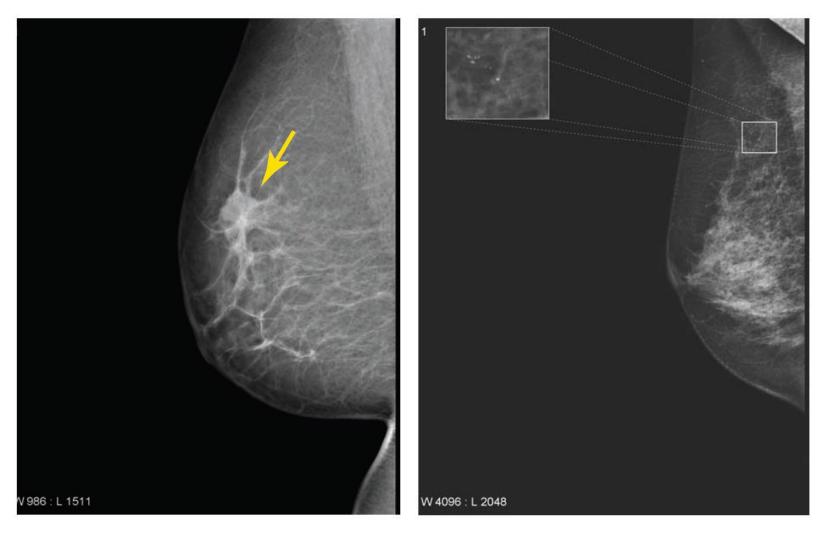


Figure. (Left) Dense opacity with spicular border in the cranial part of the right breast; histological proven invasive ductal carcinoma. (Right)Cluster of irregular microcalcifications suggesting a low differentiated carcinoma.

Bone fixation





Figure. (Left) Postoperative fluoroscopic control of bone fixation with plate and screws after a complete fracture of the humerus. (Right) Spine radiograph of scoliosis before and after surgical treatment.





Cerebral angiogram





Figure. Cerebral angiogram showing an aneurysm or saccular dilation of a cerebral artery.

GI tract



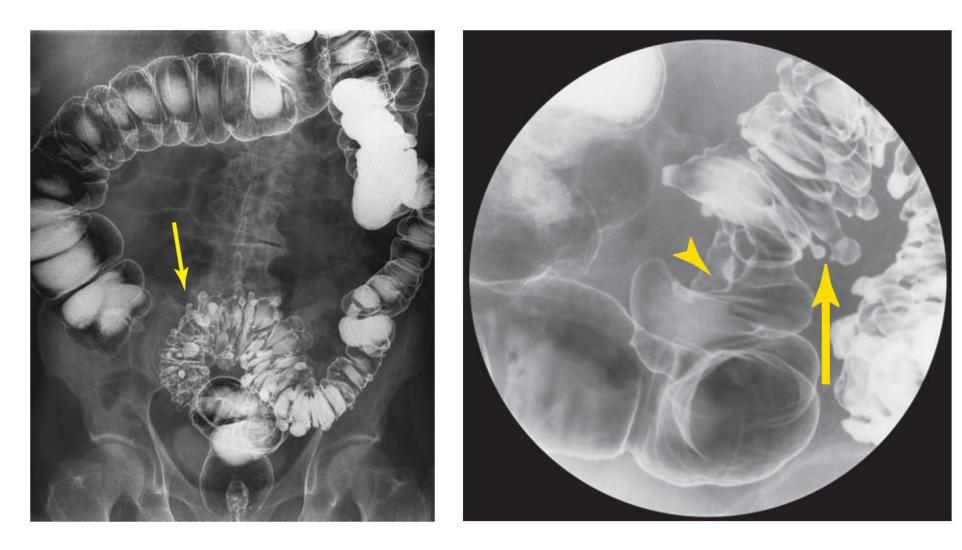


Figure. (Left) Double contrast (barium + gas insufflation) enema with multiple diverticula in the sigmoid colon (arrows). (Right) Polypoid mass proliferating intraluminally (arrowhead on the spotview).