Bayesian model selection & averaging

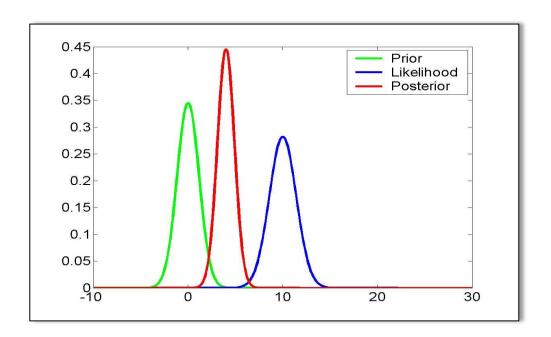
Klaas Enno Stephan







Bayes' theorem



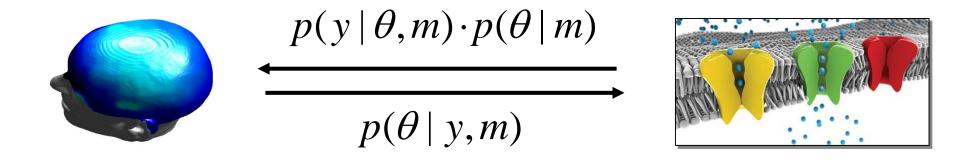


The Reverend Thomas Bayes (1702-1761)

$$p(\theta \mid y, m) = \frac{p(y \mid \theta, m) p(\theta \mid m)}{p(y \mid m)}$$

posterior = likelihood • prior / evidence

Generative model



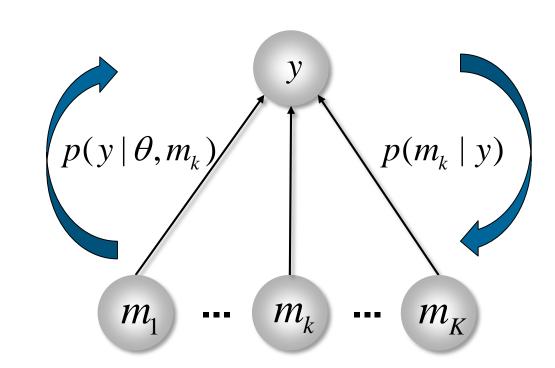
- 1. enforces mechanistic thinking: how could the data have been caused?
- 2. generate synthetic data (observations) by sampling from the prior can model explain certain phenomena at all?
- 3. inference about parameters $\rightarrow p(\theta|y)$
- 4. inference about model structure: formal approach to disambiguating mechanisms $\rightarrow p(y|m)$ or p(m|y)

Long-term goal: Differential diagnosis based on generative models of disease symptoms

SYMPTOM

(behaviour or physiology)

HYPOTHETICAL MECHANISM



Model comparison and selection

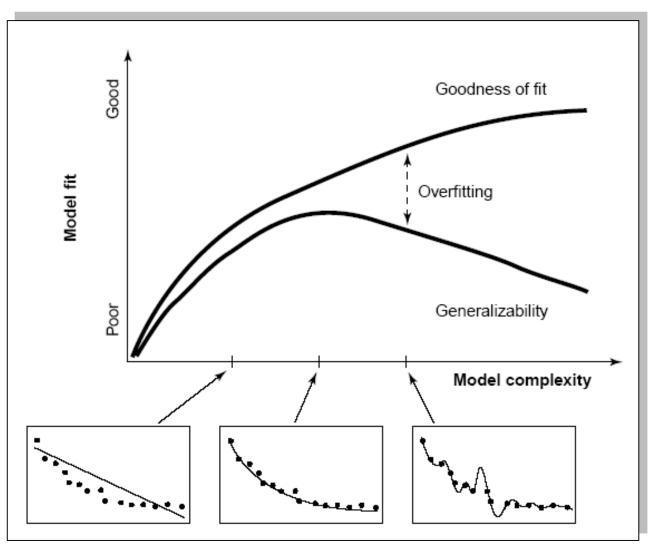
Given competing hypotheses on structure & functional mechanisms of a system, which model is the best?



Which model represents the best balance between model fit and model complexity?



For which model m does p(y|m) become maximal?



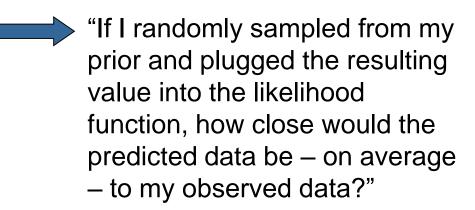
Pitt & Miyung (2002) TICS

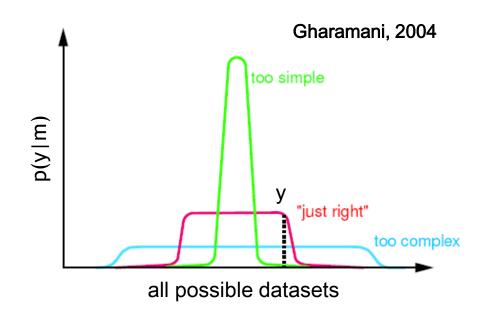
Bayesian model selection (BMS)

Model evidence (marginal likelihood):

$$p(y | m) = \int p(y | \theta, m) p(\theta | m) d\theta$$

accounts for both accuracy and complexity of the model





Various approximations, e.g.:

- negative free energy, AIC, BIC

Model space (hypothesis set) M

Model space M is defined by prior on models.

Usual choice: flat prior over a small set of models.

$$p(m) = \begin{cases} 1/|M| & \text{if } m \in M \\ 0 & \text{if } m \notin M \end{cases}$$

In this case, the posterior probability of model i is:

$$p(m_i \mid y) = \frac{p(y \mid m_i) p(m_i)}{\sum_{j=1}^{|M|} p(y \mid m_j) p(m_j)} = \frac{p(y \mid m_i)}{\sum_{j=1}^{|M|} p(y \mid m_j)}$$

Approximations to the model evidence in DCM

Logarithm is a monotonic function



Maximizing log model evidence

= Maximizing model evidence

Log model evidence = balance between fit and complexity

$$\log p(y|m) = accuracy(m) - complexity(m)$$
$$= \log p(y|\theta,m) - complexity(m)$$

No. of parameters

$$AIC = \log p(y \mid \theta, m) - p$$

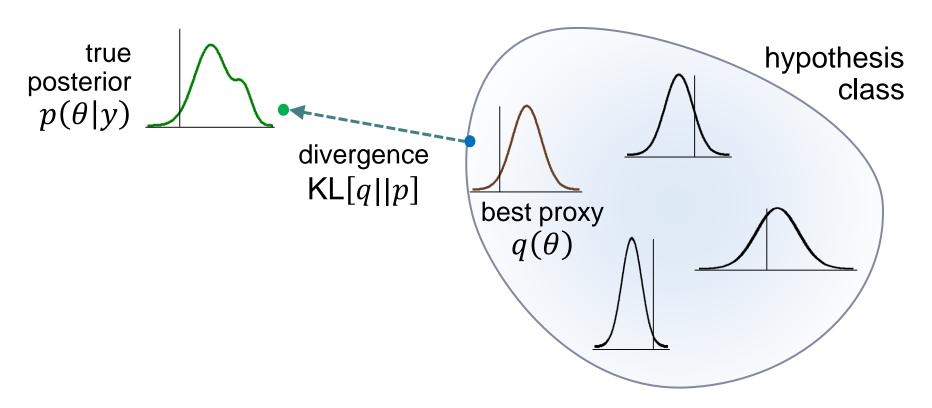
data points

Akaike Information Criterion:
$$AIC = \log p(y \mid \theta, m) - p$$
Bayesian Information Criterion: $BIC = \log p(y \mid \theta, m) - \frac{p}{2} \log N$

Variational Bayes (VB)

Idea: find an approximate density $q(\theta)$ that is maximally similar to the true posterior $p(\theta|y)$.

This is often done by assuming a particular form for q (fixed form VB) and then optimizing its sufficient statistics.



The (negative) free energy approximation $oldsymbol{F}$

$$\ln p(y) = \text{KL}[q||p] + F(q,y)$$
divergence
 ≥ 0
energy

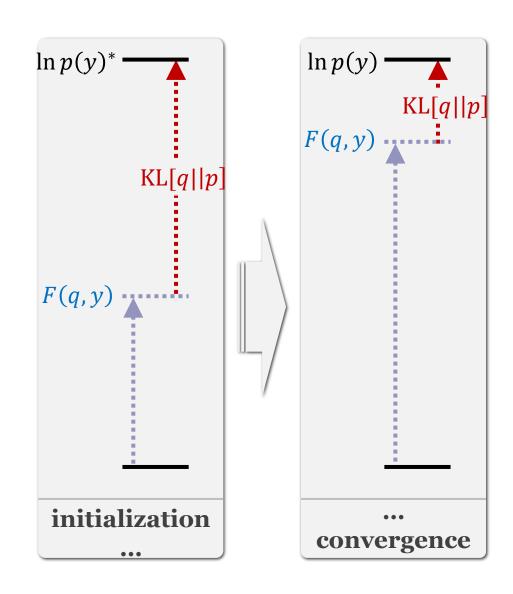
(unknown) (easy to evaluate for a given q)

F(q, y) is a functional wrt. the approximate posterior $q(\theta)$.

Maximizing F(q, y) is equivalent to:

- minimizing KL[q||p]
- tightening F(q, y) as a lower bound to the log model evidence

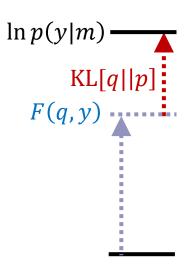
When F(q, y) is maximized, $q(\theta)$ is our best estimate of the posterior.



The (negative) free energy approximation F

F is a lower bound on the log model evidence, where the bound is determined by the KL divergence between an approximate posterior q and the true posterior::

$$\log p(y | m) = F + KL[q(\theta), p(\theta | y, m)]$$



Like AIC/BIC, F is an accuracy/complexity tradeoff:

$$F = \underbrace{\langle \log p(y \mid \theta, m) \rangle}_{accuracy} - \underbrace{KL[q(\theta), p(\theta \mid m)]}_{complexity}$$

The complexity term in *F*

In contrast to AIC & BIC, the complexity term of the negative free energy F
accounts for parameter interdependencies.

$$KL[q(\theta), p(\theta \mid m)]$$

$$= \frac{1}{2} \ln |C_{\theta}| - \frac{1}{2} \ln |C_{\theta|y}| + \frac{1}{2} \left(\mu_{\theta|y} - \mu_{\theta}\right)^T C_{\theta}^{-1} \left(\mu_{\theta|y} - \mu_{\theta}\right)$$

- determinant = measure of "volume" (space spanned by the eigenvectors of the matrix)
- The complexity term of F is higher
 - the more independent the prior parameters (↑ effective DFs)
 - the more dependent the posterior parameters
 - the more the posterior mean deviates from the prior mean

mpdcm: Computing the evidence by sampling



Bayes factors

To compare two models, we could just compare their log evidences.

But: the log evidence is just some number – not very intuitive!

A more intuitive interpretation of model comparisons is made possible by Bayes factors:

positive value, $[0; \infty[$

$$B_{12} = \frac{p(y | m_1)}{p(y | m_2)}$$

Kass & Raftery classification:

B ₁₂	p(m₁ y)	Evidence
1 to 3	50-75%	weak
3 to 20	75-95%	positive
20 to 150	95-99%	strong
≥ 150	≥ 99%	Very strong

Fixed effects BMS at group level

Group Bayes factor (GBF) for 1... K subjects:

$$GBF_{ij} = \prod_{k} BF_{ij}^{(k)}$$

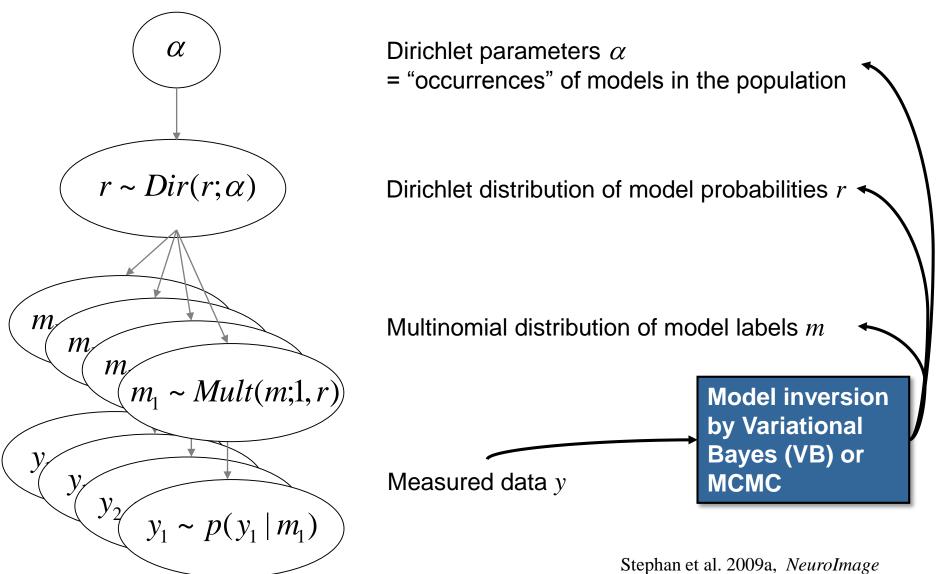
Average Bayes factor (ABF):

$$ABF_{ij} = \sqrt{\prod_{k} BF_{ij}^{(k)}}$$

Problems:

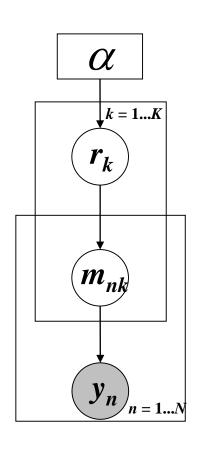
- blind with regard to group heterogeneity
- sensitive to outliers

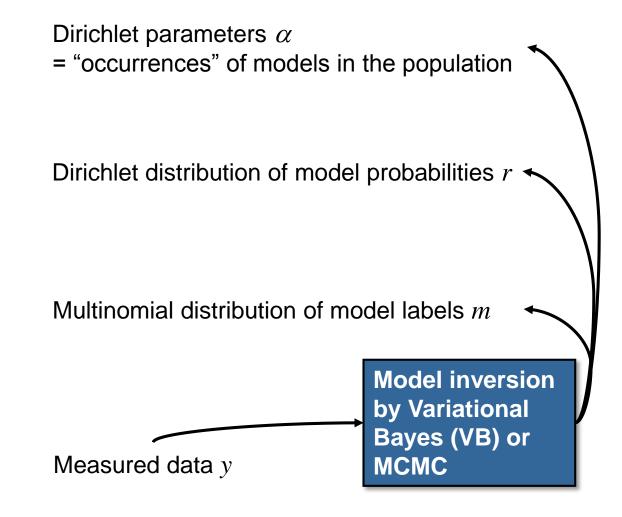
Random effects BMS for heterogeneous groups



Stephan et al. 2009a, *NeuroImage* Penny et al. 2010, *PLoS Comp. Biol.*

Random effects BMS for heterogeneous groups





Stephan et al. 2009a, *NeuroImage* Penny et al. 2010, *PLoS Comp. Biol.*

Reminder: VB in a nutshell (mean-field approximation)

Neg. free-energy approx. to model evidence.

$$\ln p(y|m) = F + KL[q(\theta,\lambda), p(\theta,\lambda|y)]$$

$$F = \langle \ln p(y,\theta,\lambda) \rangle_{q} - KL[q(\theta,\lambda), p(\theta,\lambda|m)]$$

Mean field approx.

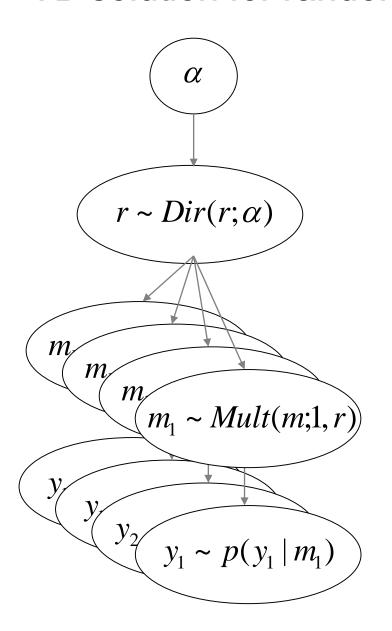
$$p(\theta, \lambda \mid y) \approx q(\theta, \lambda) = q(\theta)q(\lambda)$$

Maximise neg. free energy wrt. q = minimise divergence, by maximising variational energies

$$q(\theta) \propto \exp(I_{\theta}) = \exp\left[\left\langle \ln p(y, \theta, \lambda) \right\rangle_{q(\lambda)}\right]$$
$$q(\lambda) \propto \exp(I_{\lambda}) = \exp\left[\left\langle \ln p(y, \theta, \lambda) \right\rangle_{q(\theta)}\right]$$

Iterative updating of sufficient statistics of approx. posteriors (e.g., by gradient ascent).

VB solution for random effects BMS



$$p(r \mid \alpha) = Dir(r, \alpha) = \frac{1}{Z(\alpha)} \prod_{k} r_{k}^{\alpha_{k}-1}$$

$$Z(\alpha) = \prod_{k} \Gamma(\alpha_{k}) / \Gamma\left(\sum_{k} \alpha_{k}\right)$$

$$p(m_n \mid r) = \prod_k r_k^{m_{nk}}$$

$$p(y_n | m_{nk}) = \int p(y | \theta) p(\theta | m_{nk}) d\theta$$

Write down joint probability and take the log

$$p(y,r,m) = p(y|m)p(m|r)p(r|\alpha_0)$$

$$= p(r|\alpha_0) \left[\prod_n p(y_n|m_n)p(m_n|r) \right]$$

$$= \frac{1}{Z(\alpha_0)} \left[\prod_k r_k^{\alpha_{0k}-1} \right] \left[\prod_n p(y_n|m_n) \prod_k r_k^{m_{nk}} \right]$$

$$= \frac{1}{Z(\alpha_0)} \prod_n \left[\prod_k p(y_n|m_n) r_k \right]^{m_{nk}} r_k^{\alpha_{0k}-1}$$

$$\ln p(y, r, m) = -\ln Z(\alpha_0) + \sum_{n} \sum_{k} ((\alpha_{0k} - 1) \ln r_k + m_{nk} (\log p(y_n | m_{nk}) + \ln r_k))$$

Mean field approx.

$$q(r,m) = q(r)q(m)$$

Maximise neg. free energy wrt. q = minimise divergence, by maximising variational energies

$$q(r) \propto \exp(I(r))$$

$$q(m) \propto \exp(I(m))$$

$$I(r) = \langle \log p(y, r, m) \rangle_{q(m)}$$

$$I(m) = \langle \log p(y, r, m) \rangle_{q(r)}$$

Iterative updating of sufficient statistics of approx. posteriors

$$\alpha = \alpha_0$$

$\alpha_0 = [1, \ldots, 1]$

Until convergence

$$u_{nk} = \exp\left(\ln p(y_n \mid m_{nk}) + \Psi(\alpha_k) - \Psi\left(\sum_k \alpha_k\right)\right)$$

$$g_{nk} = \frac{u_{nk}}{\sum_{k} u_{nk}}$$

$$\beta_k = \sum_n g_{nk}$$

$$\alpha = \alpha_0 + \beta$$

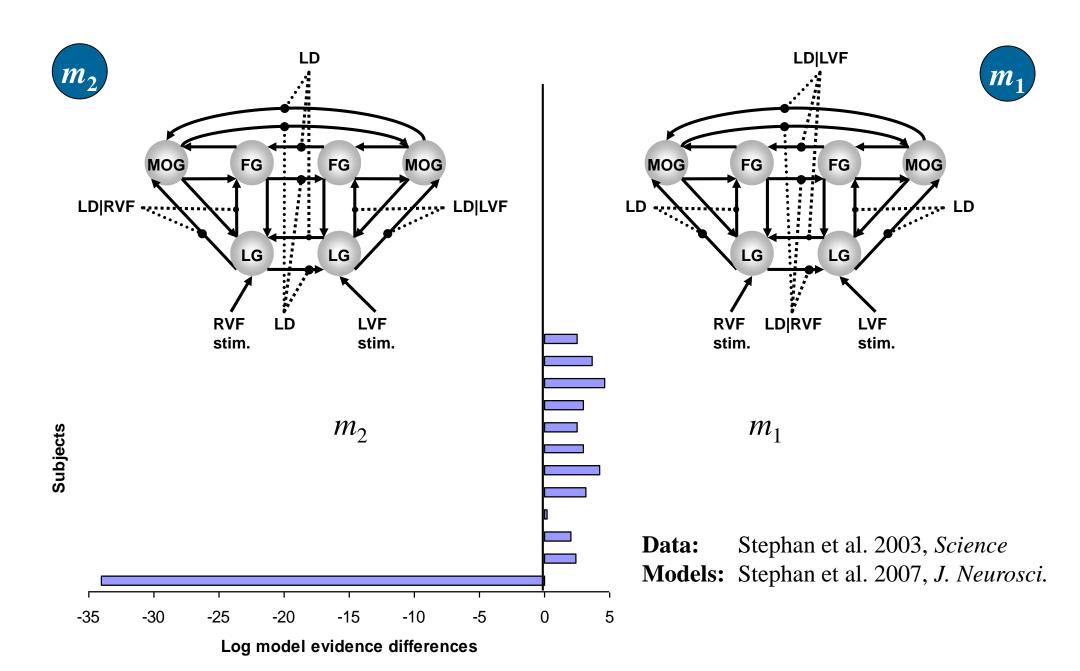
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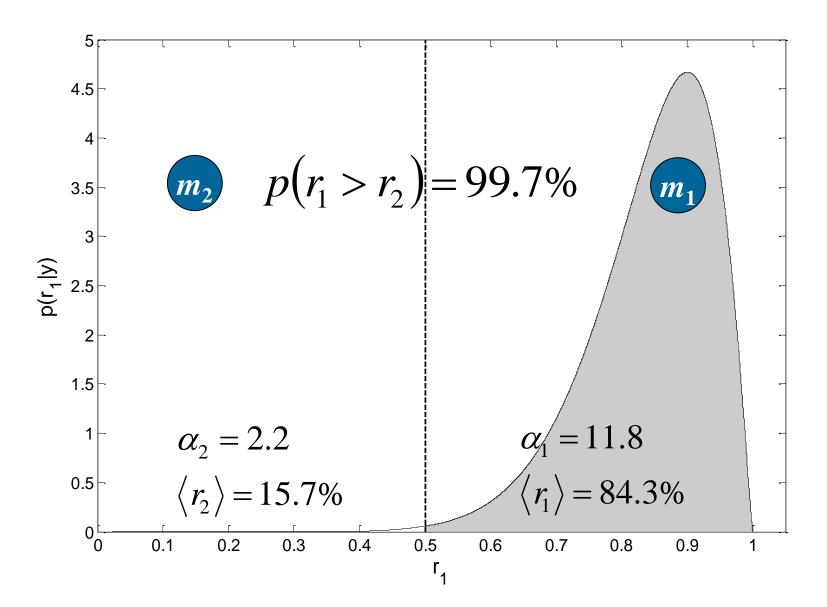
$$g_{nk} = q(m_{nk} = 1)$$

our (normalized)
posterior belief that
model *k* generated the
data from subject *n*

$$\beta_k = \sum_n g_{nk}$$

expected number of subjects whose data we believe were generated by model *k*





How can we report the results of random effects BMS?

1. Dirichlet parameter estimates

 α

2. **expected posterior probability** of obtaining the k-th model for any randomly selected subject

$$\langle r_k \rangle_q = \alpha_k / (\alpha_1 + \ldots + \alpha_K)$$

3. **exceedance probability** that a particular model *k* is more likely than any other model (of the *K* models tested), given the group data

$$\exists k \in \{1...K\}, \forall j \in \{1...K \mid j \neq k\}:$$

$$\varphi_k = p(r_k > r_j \mid y; \alpha)$$

4. **protected exceedance probability**: see below

Overfitting at the level of models

- ↑ #models ⇒ ↑ risk of overfitting
- solutions:
 - regularisation: definition of model space = choosing priors p(m)
 - family-level BMS
 - Bayesian model averaging (BMA)

too simple

"just right"

too complex

posterior model probability:

$$p(m|y)$$

$$= \frac{p(y|m)p(m)}{\sum_{m} p(y|m)p(m)}$$

$$p(\theta | y)$$

$$= \sum_{m} p(\theta | y, m) p(m | y)$$

Model space partitioning or: Comparing model families

- partitioning model space into K subsets or families:
- pooling information over all models in these subsets allows one to compute the probability of a model family, given the data
- effectively removes uncertainty about any aspect of model structure, other than the attribute of interest (which defines the partition)

$$M = \left\{ f_1, ..., f_K \right\}$$

$$p(f_k)$$

Family-level inference: fixed effects

- We wish to have a uniform prior at the family level:
- This is related to the model level via the sum of the priors on models:
- Hence the uniform prior at the family level is:
- The probability of each family is then obtained by summing the posterior probabilities of the models it includes:

$$p(f_k) = \frac{1}{K}$$

$$p(f_k) = \sum_{m \in f_k} p(m)$$

$$\forall m \in f_k : p(m) = \frac{1}{K|f_k|}$$

$$p(f_k \mid y_{1..N}) = \sum_{m \in f_k} p(m \mid y_{1..N})$$

Family-level inference: random effects

 The frequency of a family in the population is given by:

$$S_k = \sum_{m \in f_k} r_m$$

• In RFX-BMS, this follows a Dirichlet distribution, with a uniform prior on the parameters α (see above).

$$p(s) = Dir(\alpha)$$

 A uniform prior over family probabilities can be obtained by setting:

$$\forall m \in f_k : \alpha_{prior}(m) = \frac{1}{|f_k|}$$

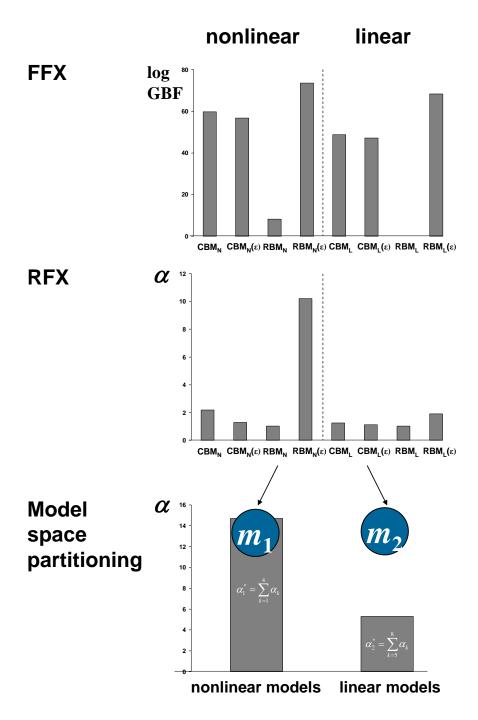
Family-level inference: random effects – a special case

 When the families are of equal size, one can simply sum the posterior model probabilities within families by exploiting the agglomerative property of the Dirichlet distribution:

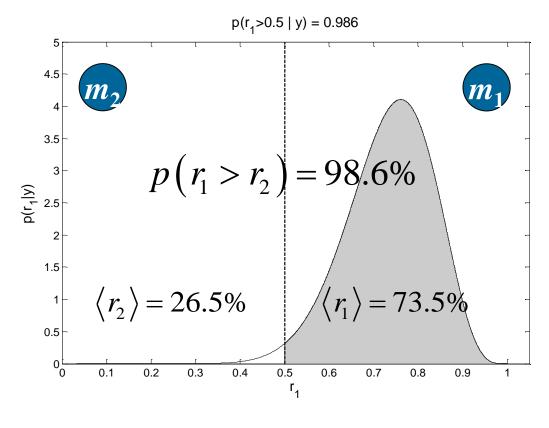
$$(r_1, r_2, ..., r_K) \sim Dir(\alpha_1, \alpha_2, ..., \alpha_K)$$

$$\Rightarrow r_1^* = \sum_{k \in N_1} r_k, r_2^* = \sum_{k \in N_2} r_k, ..., r_J^* = \sum_{k \in N_J} r_k$$

$$\sim Dir(\alpha_1^* = \sum_{k \in N_1} \alpha_k, \alpha_2^* = \sum_{k \in N_2} \alpha_k, ..., \alpha_J^* = \sum_{k \in N_J} \alpha_k)$$



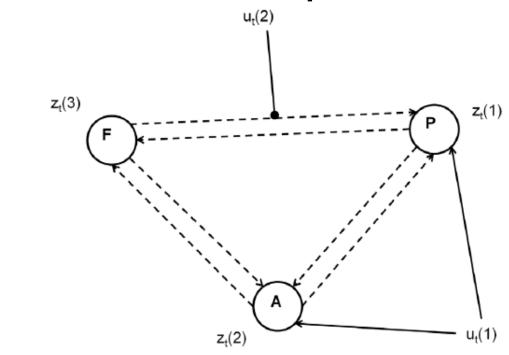
Model space partitioning: comparing model families

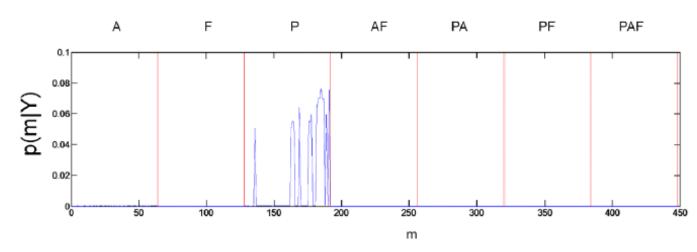


Stephan et al. 2009, NeuroImage

Comparing model families – a second example

- data from Leff et al.
 2008, J. Neurosci
- one driving input, one modulatory input
- 2⁶ = 64 possible modulations
- 2³ 1 input patterns
- $7 \times 64 = 448 \text{ models}$
- integrate out uncertainty about modulatory patterns and ask where auditory input enters





Bayesian Model Averaging (BMA)

- abandons dependence of parameter inference on a single model and takes into account model uncertainty
- uses the entire model space considered (or an optimal family of models)
- averages parameter estimates, weighted by posterior model probabilities
- represents a particularly useful alternative
 - when none of the models (or model subspaces) considered clearly outperforms all others
 - when comparing groups for which the optimal model differs

single-subject BMA:

$$p(\theta | y)$$

$$= \sum_{m} p(\theta | y, m) p(m | y)$$

group-level BMA:

$$p(\theta_n | y_{1..N})$$

$$= \sum_{m} p(\theta_n | y_n, m) p(m | y_{1..N})$$

NB: $p(m|y_{1..N})$ can be obtained by either FFX or RFX BMS

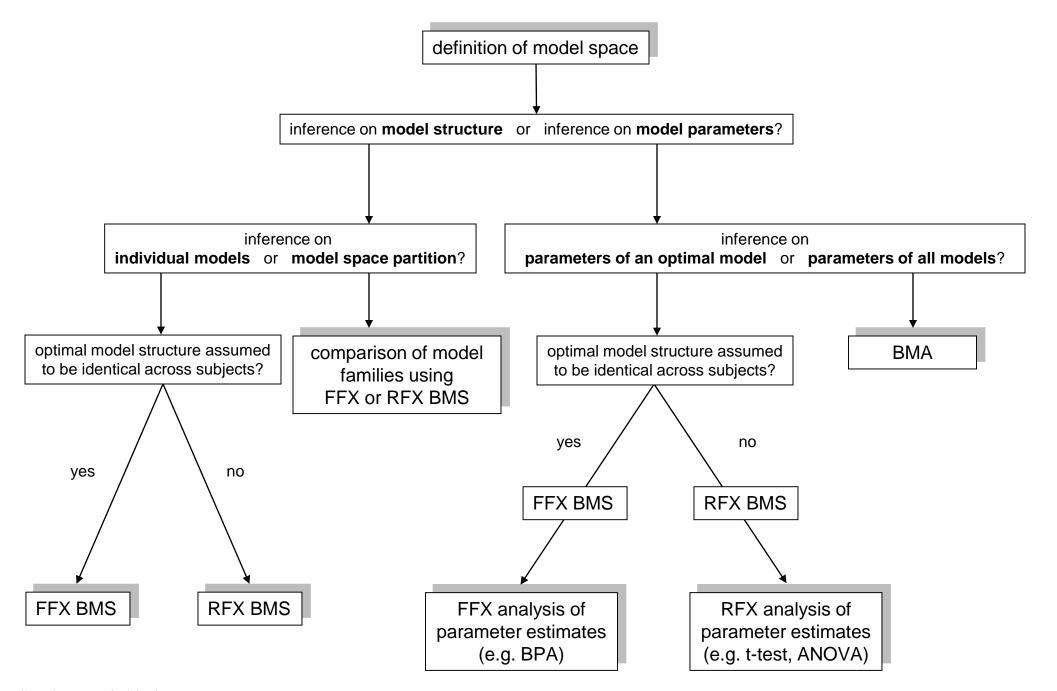
Protected exceedance probability: Using BMA to protect against chance findings

- EPs express our confidence that the posterior probabilities of models are different – under the hypothesis H₁ that models differ in probability: r_k≠1/K
- does not account for possibility "null hypothesis" H₀: r_k=1/K
- Bayesian omnibus risk (BOR) of wrongly accepting H₁ over H₀:

$$P_{o} = \frac{1}{1 + \frac{p(m|H_{1})}{p(m|H_{0})}}$$

protected EP: Bayesian model averaging over H₀ and H₁:

$$\begin{split} \widetilde{\varphi}_k &= P(r_k \! \geq \! r_{k' \neq k} | y) \\ &= P(r_k \! \geq \! r_{k' \neq k} | y, H_1) P(H_1 | y) + P(r_k \! \geq \! r_{k' \neq k} | y, H_0) P(H_0 | y) \\ &= \varphi_k (1 \! - \! P_0) + \frac{1}{K} P_0 \end{split}$$



Some examples of empirical BMS/BMA applications

Behavioral/Systems/Cognitive

Effective Connectivity Determines the Nature of Subjective Experience in Grapheme-Color Synesthesia

Tessa M. van Leeuwen, Hanneke E. M. den Ouden, and Peter Hagoort^{1,2}

¹Donders Institute for Brain, Cognition and Behaviour, Centre for Cognitive Neuroimaging, Radboud University Nijmegen, 6500 HB, Nijmegen, the Netherlands, and ²Max Planck Institute for Psycholinguistics, 6500 AH, Nijmegen, the Netherlands

Network dysfunction of emotional and cognitive processes in those at genetic risk of bipolar disorder

Michael Breakspear, 1,2,3,* Gloria Roberts, 3,4,* Melissa J. Green, 3,4,5,6 Vinh T. Nguyen, 1 Andrew Frankland, 3,4 Florence Levy, 3 Rhoshel Lenroot 3,6 and Philip B. Mitchell 3,4

Original Investigation

Brain Connectivity Abnormalities
Predating the Onset of Psychosis
Correlation With the Effect of Medication

André Schmidt, PhD; Renata Smieskova, PhD; Jacqueline Aston, MD; Andor Simon, MD; Paul Allen, PhD; Paolo Fusar-Poli, MD, PhD; Philip K. McGuire, MD, PhD; Anita Riecher-Rössler, MD, PhD; Klaas E. Stephan, MD, PhD; Stefan Borgwardt, MD, PhD

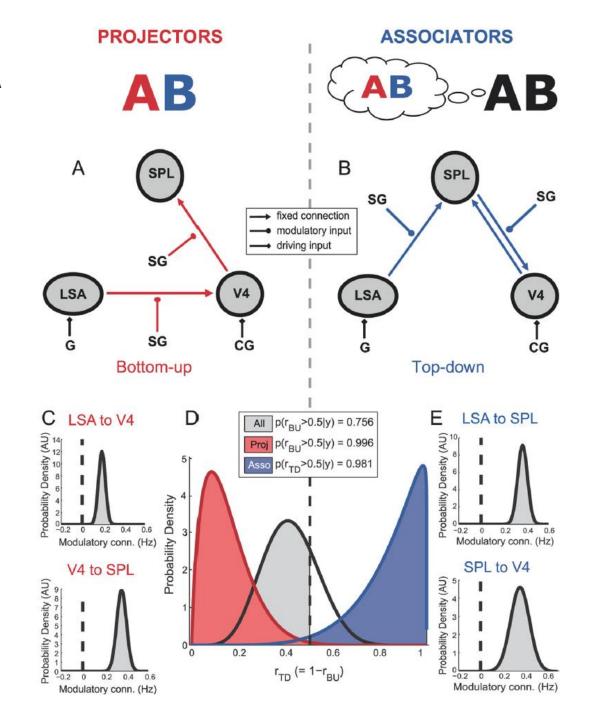
van Leeuwen et al. 2011, *J. Neurosci*.

Breakspear et al. 2015, *Brain*

Schmidt et al. 2013, JAMA Psychiatry

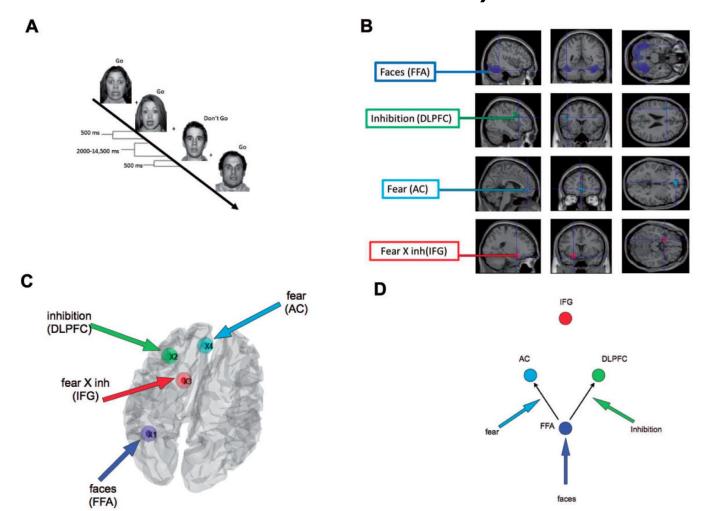
Application: Synaesthesia

- "projectors" experience color externally colocalized with a presented grapheme
- "associators" report an internally evoked association
- across all subjects: no evidence for either model
- but BMS results map precisely onto projectors (bottom-up mechanisms) and associators (top-down)



Go/No-Go task to emotional faces (bipolar patients, at-risk individuals, controls)

- interaction of motor inhibition and fear perception
- hypoactivation of left IFG in the at-risk group during fearful distractor trials
- What is the most likely circuit mechanism explaining the fear x inhibition interaction in IFG?



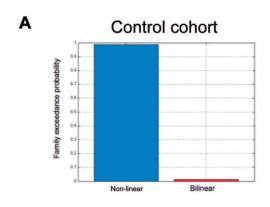
Model space

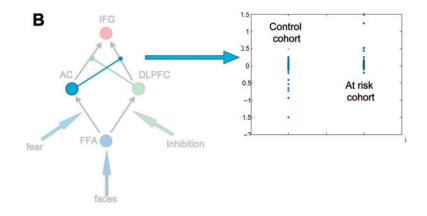
 models of serial (1-3), parallel (4) and hierarchical (5-8) processes

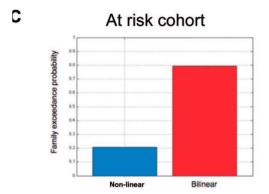
A: Bilinear models DLPFC Inhibition **B**: Non-linear models 5 6 DLPFC

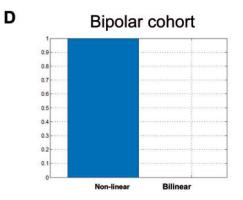
Family-level BMS

- family-level comparison: nonlinear models more likely than bilinear ones in both healthy controls and bipolar patients
- at-risk group: bilinear models more likely
- significant group difference in ACC modulation of DLPFC→IFG interaction





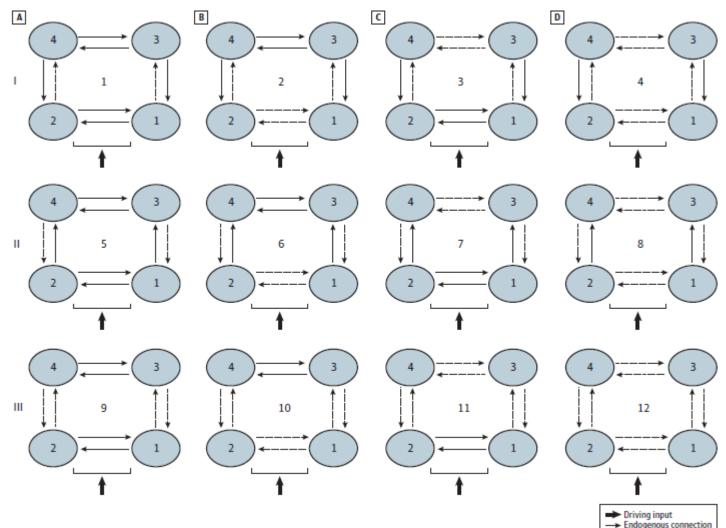




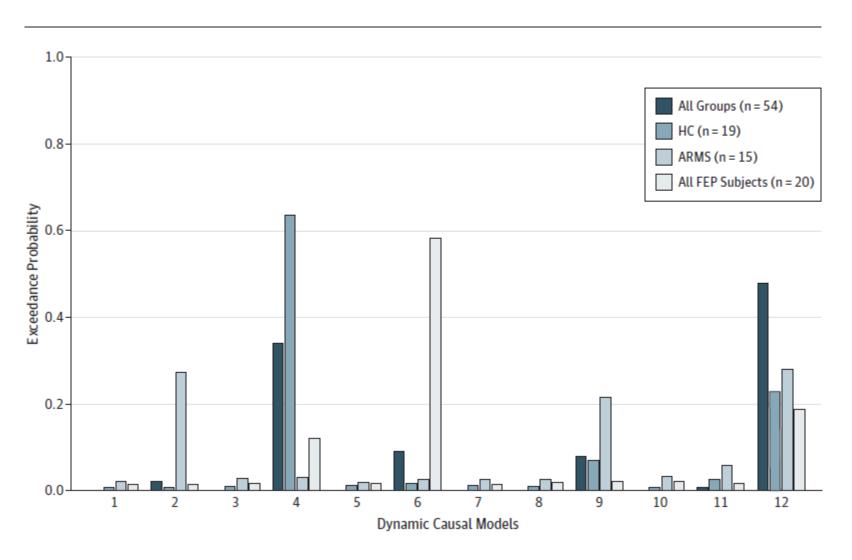


Prefrontal-parietal connectivity during working memory in schizophrenia

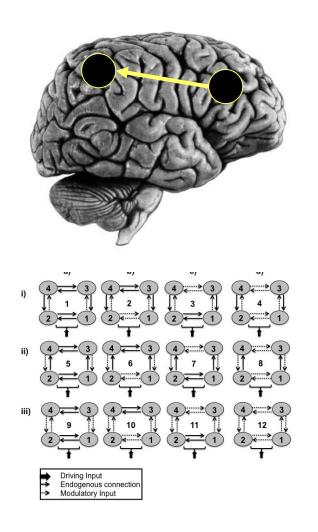
- 17 at-risk mental state (ARMS) individuals
- 21 first-episode patients (13 non-treated)
- 20 controls

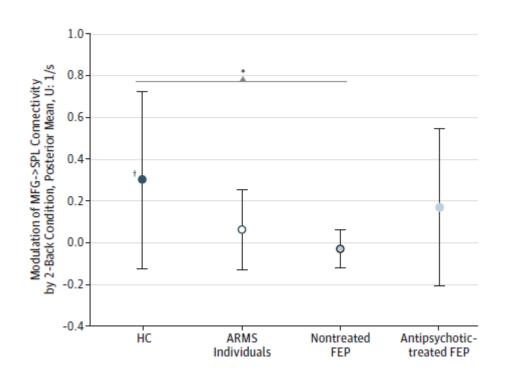


BMS results for all groups



BMA results: PFC → PPC connectivity





17 ARMS, 21 first-episode (13 non-treated), 20 controls

Further reading on BMS

- Penny WD, Stephan KE, Mechelli A, Friston KJ (2004a) Comparing dynamic causal models.
 Neurolmage 22:1157-1172.
- Penny WD, Stephan KE, Daunizeau J, Joao M, Friston K, Schofield T, Leff AP (2010) Comparing Families of Dynamic Causal Models. PLoS Computational Biology 6: e1000709.
- Penny WD (2012) Comparing dynamic causal models using AIC, BIC and free energy.
 Neuroimage 59: 319-330.
- Rigoux L, Stephan KE, Friston KJ, Daunizeau J (2014) Bayesian model selection for group studies – revisited. Neurolmage 84: 971-985.
- Stephan KE, Weiskopf N, Drysdale PM, Robinson PA, Friston KJ (2007) Comparing hemodynamic models with DCM. NeuroImage 38:387-401.
- Stephan KE, Penny WD, Daunizeau J, Moran RJ, Friston KJ (2009) Bayesian model selection for group studies. Neurolmage 46:1004-1017.
- Stephan KE, Penny WD, Moran RJ, den Ouden HEM, Daunizeau J, Friston KJ (2010) Ten simple rules for Dynamic Causal Modelling. NeuroImage 49: 3099-3109.

Thank you