

ECI End

5<sup>th</sup> module

Brain signals  $\rightarrow$  ~~analog~~ AC to DC  $\rightarrow$

Set of features  $\rightarrow$  feature vectors

Two steps of feature extraction:-

- (i) Signal conditioning to reduce noise
- (ii) Extraction of features
- (iii) Feature conditioning to properly prepare the feature vector for the feature translation stage

First step: Signal condition

$\rightarrow$  removing noise

Signal conditioning can include a number of diff procedures:-

- (i) frequency range prefiltering
- (ii) data decimation & resampling
- (iii) Spatial filtering

Second step: Block processing

$\rightarrow$  For BCI applications, it is highly desirable for the processing

Time (Temporal) features  $\rightarrow$  Peak Picking  
Correlation Template matching

### Peak Picking

$\rightarrow$  determines minimum and maximum value of the signal samples in a specific block of time and uses that value as feature for the time block.

$\rightarrow$  Signal can be averaged or integrated over all or part of the time block to yield features of the block.

### Extracting the features

1) Correlation and template matching

### Frequency features

Band pass, FFT, autoregressive modeling

Transformation algorithms  $\rightarrow$  feature condensation

Normalization, log normal transforms, feature smoothing

PCA & ICA; removing irrelevant and redundant features

(Maximum relevant Minimum redundant)

## Feature Translation

Third step : feature engineering

translation algorithms

## feature translation

Discriminant functions, regression functions

## Regression analysis

The regression analysis is a statistical method to deal with formulation of mathematical model depicting relationship among variables which can be used for purpose of prediction.

## Classification of regression analysis models

Linear regression models.

Simple linear regression

multiple linear regression

## Least square method

$$SSE = \sum_{i=1}^n e_i^2 = \sum_{i=1}^n (y_i - \hat{y}_i)^2 = \sum_{i=1}^n (y_i - a - bx_i)^2$$

We are to minimize the value of SSE and hence to determine parameters of  $a$  &  $b$

$$\frac{\partial(SSE)}{\partial a} = -2 \sum_{i=1}^n (y_i - a - bx_i)$$

$$\frac{\partial(SSE)}{\partial b} = -2 \sum_{i=1}^n (y_i - a - bx_i) \cdot x_i$$

for minimum value of SSE

$$\frac{\partial(SSE)}{\partial a} = 0$$

$$\frac{\partial(SSE)}{\partial b} = 0$$

$$a = \bar{y} - b\bar{x} \quad b = \frac{\sum_{i=1}^n (x_i - \bar{x})(y_i - \bar{y})}{\sum_{i=1}^n (x_i - \bar{x})^2}$$

$R^2$  : measure of quality of fit  $\rightarrow$  coefficient of determination

SST  $\rightarrow$  total corrected sum of squares

$$= \sum_{i=1}^n (y_i - \bar{y})^2$$

$$R^2 = 1 - \frac{SSE}{SST} \quad ; \quad R^2 = 1 \text{ means good fit}$$

$$a = \bar{y} - b\bar{x}$$

$$b = \frac{\sum_{i=1}^n (x_i - \bar{x})(y_i - \bar{y})}{\sum_{i=1}^n (x_i - \bar{x})^2}$$



## Bayesian classifier

statistical classifier

(assumptions : mutually exclusive & exhaustive)

Bayesian classifier is an approach for modelling probabilistic relationships between the attribute set & the class variable.

## M estimate

$$P(A_j = a_j | C_i) = \frac{n_{C_i} + m p}{n + m}$$

$n$  = total number of instances from class  $C_i$

$n_{C_i}$  = number of training samples from class  $C_i$  that takes  $A_j = a_j$

$m$  = it is a parameter known as the equivalent sample size,

$p$  = it is a unspecified parameters.

## ~~Vote~~rate Classification

### Entropy

To deal with classification jobs, entropy ~~be~~ is an important concept.

an information-theoretic measure of uncertainty contained in training data.

$$E = - \sum_{i=1}^m p_i \log_2 p_i$$

$$= \frac{4}{24} \log_2 \frac{4}{24} - \frac{5}{24} \log_2 \frac{5}{24} - \frac{15}{24} \log_2 \frac{15}{24}$$

Decision tree induction is top-down, recursive, divide & conquer approach.

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At each node, the splitting attribute is selected to be the most informative among the attributes not yet considered in path starting from the root.

Weighted entropy

$E_A(D)$   $\rightarrow$  expected information gain required to classify a tuple from  $D$  based on splitting of  $A$ .

$$E_A(D) = \sum_{j=1}^m \frac{|D_j|}{|D|} E(D_j)$$

$\frac{|D_j|}{|D|}$  denotes the weight of the  $j^{\text{th}}$  training set.

## Info gain

$$\alpha(A, D) = E(D) - E_A(D)$$

✓  
Total dataset

✓  
For  $A=1, A=2, \dots, A=n^{\text{th}}$  class

The ID3 strategy of attribute selection is to choose to split on the attribute that gives greatest reduction in the weighted average entropy.

## Frequency table

$$\text{Info gain} \geq 0$$

→ When the entropy of training set takes largest value ( $\log_2 k$ ) (this occurs when the classes are balanced) then the info gain will be zero.

## CART Algorithm

CART is a technique that generates a binary decision tree

Gini index of diversity known as  $V$

$$\text{Weighted average gain index} = G_A(D) = \frac{|D_1|}{D} G(D_1) + \frac{|D_2|}{D} G(D_2)$$

$$V(A, D) = G(D) - G_A(D)$$

$$1 - \sum p_i^2$$

CR2 for node class

Algorithm C4.5

No limitation of ID3

If attribute has distinct values for all tuples, then it would result in large number of partitions, each one containing just one tuple.

ID3 may suffer from overfitting problem.

$$\text{Gain ratio} = \frac{\text{Information gain}}{\text{split information}}$$



## Linear regression

min Least squares estimation

$$\min \sum_{i=1}^m (y_i - \hat{y}_i)^2 = \sum_{i=1}^m (y_i - (w \cdot x_i + b))^2$$

$$\hat{w} = (X^T X)^{-1} X^T y$$

$$\text{LASSO} \rightarrow \min \sum_{i=1}^m (y_i - w \cdot x_i - b)^2 + \underbrace{\left( c \sum_{j=1}^n |w_j| \right)}_{\text{regularization term}}$$

$$\text{Ridge regression} \rightarrow \min \sum_{i=1}^m (y_i - w \cdot x_i - b)^2 + c \sum_{j=1}^n |w_j|^2$$

Soft margin

$$(x_i, y_i) \quad i = 1 \dots m$$

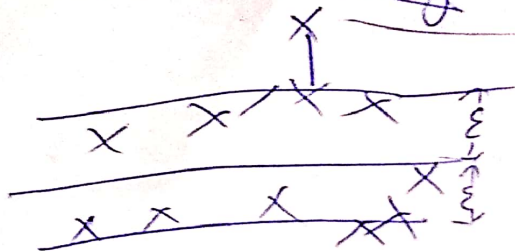
minimize

$$\frac{1}{2} \|w\|^2 + c \sum_{i=1}^m \left( \xi_i + \frac{\xi_i^+}{2} \right)$$

Under constraints

$$\begin{cases} y_i - (w \cdot x_i) - b \leq \varepsilon + \xi_i \\ (w \cdot x_i) + b - y_i \leq \varepsilon + \xi_i^+ \\ \xi_i, \xi_i^+ \geq 0, i = 1 \dots m \end{cases}$$

## Support Vector regression



$$L_2(y, f(x, w)) = \max$$
$$= \max(|y - f(x, w)| - \epsilon, 0)$$

Given training data

$$(x_i, y_i) \quad i = 1, \dots, m$$

minimize

$$\frac{1}{2} \|w\|^2 + C \sum_{i=1}^m (\xi_i + \xi_i^*)$$

## Neural Networks

$$\delta_k \leftarrow y^k - w \cdot x^k$$

$$w_i \leftarrow w_i + \alpha \delta_k x_i^k$$

## Perceptron Node

$$\Delta w_i = (t - z) \times c \times x_i$$

↓

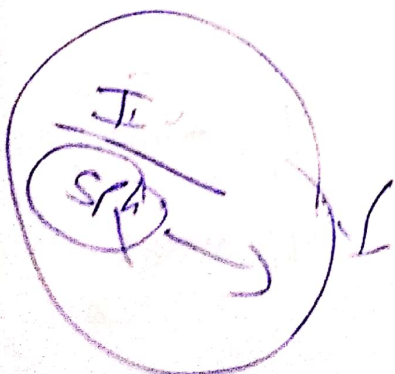
wt from input  $i$  to perceptron node,  $c$  is the learning rate,  
 $t$  is the target for the current instance,  $z$  is the current  
output, and  $x_i$  is  $i^{\text{th}}$  input.

Perceptron Convergence theorem: Guaranteed to find a solution in finite time if a solution ~~exists~~ exists

$$w_{\text{new}} = w_{\text{old}} + \underbrace{\alpha}_{\text{learning rate}} (y_i - \bar{y}_i)$$

weights will be updated <sup>error</sup> according to errors

$$\begin{array}{r} 10 \mu\text{m} \\ 12 \times 10^{-5} \text{m} \\ 1 \text{mm} \quad 12 \times 10^{-2} \text{mm} \\ \hline 0.12 \text{mm} \\ \hline 1 \text{mm} \end{array}$$



### 3<sup>rd</sup> module

#### Invasive

- microelectrodes → electrode made of tungsten, platinum or iridium alloy
- Intracellular recording → measures voltage or current across the membrane of the neuron.
- Tetrodes and multi-unit recording.
- The most common type of implantable arrays are microsilicon-based, and flexible microelectrode arrays.
- To record large number of neurons, microelectrodes can be arranged in a grid like structure to form a multielectrode array of  $m \times n$  electrodes.

#### Partially invasive

ECOG



ECOG electrodes can record the electrical fluctuations and lay coherent activity of large populations of neurons.

Micro ECoG



## Optical recording: Voltage sensitive dyes

→ Two photon calcium imaging

Based on the fact that electrical activity in neurons with ~~fluorescent~~ calcium - indicator dyes changes in Ca concentration.

Photon Ca imaging involves:

- (i) using pressure ejection to load neurons with fluorescent Ca - indicator dyes.
- (ii) Monitoring changes in Ca fluorescence during neural activity using two photon microscopy.

## Non Invasive

EEG signals reflect the summation of thousands of post synaptic potentials

Temporal resolution is good, spatial is poor

$\alpha \rightarrow 8 \text{ to } 13$  ;  $\beta \rightarrow 13 \text{ to } 30$

$\gamma \rightarrow 30 \text{ to } 100$  ;  $\delta \text{ waves} \rightarrow 0.5 - 4$  ;  $\theta$   
4-8

$\alpha - 8 - 13$  ,  $\beta - 13 \text{ to } 30$   $\gamma - 30 \text{ to } 100$

$\delta - 0.5 \text{ to } 4$   $\theta - 4 \text{ to } 8$

MEG  $\rightarrow$  magneto encephalography (better spatial resolution than EEG)

fMRI  $\rightarrow$  Bold  $\rightarrow$  paramagnetic properties

fNIR  $\rightarrow$  measures changes in blood oxygenation level. / Caused

by increased neural activity in brain.

Based on detecting near-infrared light absorbance of haemoglobin in the blood with & without oxygen

Positron Emission Tomography

measures emissions from radioactively ~~de~~ labeled, metabolically active chemicals that have been injected into the blood stream

$\rightarrow$  Transpiration to the brain.

The labelled compound is called radio tracers.

SPECT single photon emission Computed Tomography

$\downarrow$   
uses gamma rays

## Principles to discriminate artifacts from EEG signals

Physiological activity has a logical topographical field of distribution with an expected fall of voltage potentials. Artifacts have an illogical distribution that defies the principle of localization.

## Cognitive Workload

CWL is a demand placed upon humans for mental resources while performing a task.

mental resources include working memory, ability to process

Working memory ÷ is a cognitive system with a limited capacity to hold a small amount of information & process it.