

# Medical Image Analysis and Processing

## Image Noise Filtering

### Anisotropic Diffusion Filter

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# Motivation

- › Edge Preserving Filtering
- › Edge-Aware filtering

# Mathematical Background

- › Let  $u(x_1, x_2)$  is 2D scalar function and  $J \in \mathbb{R}^2$  a 2D vector function:
- › Gradient of  $u$ ,  $\nabla u$ :

$$\nabla u = \begin{bmatrix} \frac{\partial u}{\partial x_1} & \frac{\partial u}{\partial x_2} \end{bmatrix}^t, \text{ } t: \text{Transpose}$$

- › Divergence of vector  $\vec{J}$ ,  $\nabla \cdot \vec{J}$ :

$$\vec{J} = [J_1 \quad J_2]^t \Rightarrow \nabla \cdot \vec{J} = \frac{\partial J_1}{\partial x_1} + \frac{\partial J_2}{\partial x_2}$$

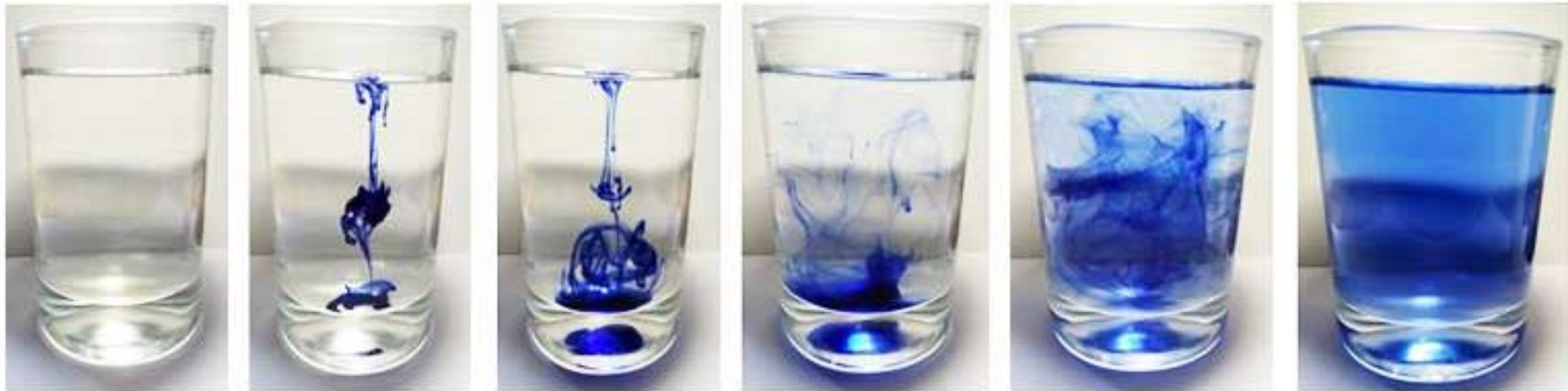
- › Laplacian of  $u$ ,  $\nabla^2 u$ :

$$\nabla^2 u = \nabla \cdot (\nabla u) = \frac{\partial^2 u}{\partial x_1^2} + \frac{\partial^2 u}{\partial x_2^2}$$

# Physical Background

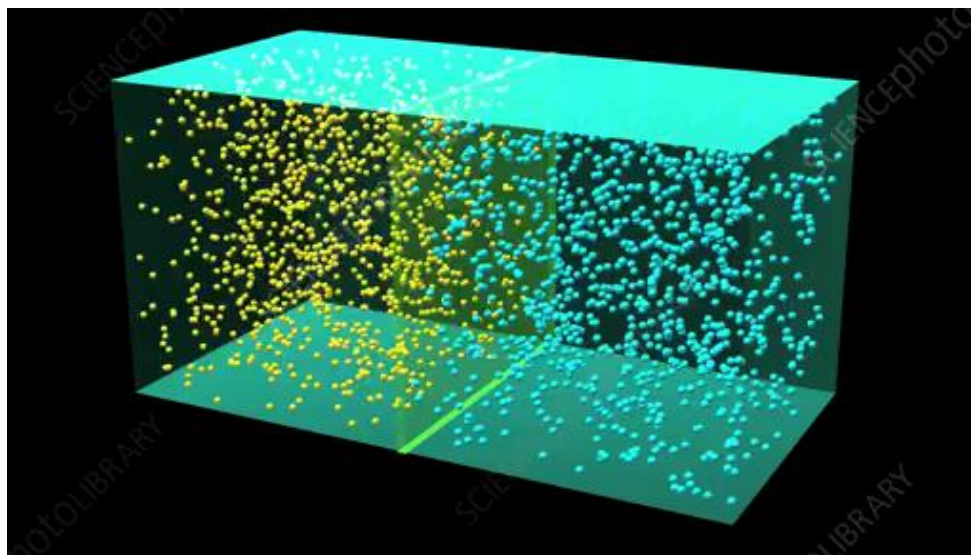
## › Diffusion:

*Diffusion* is the net movement of anything (for example, atom, ions, molecules, and etc.) from a region of **higher concentration** to a region of **lower concentration**.



# Physical Background

- › Diffusion: A distinguishing feature of diffusion is that it depends on particle **random walk** (Brownian Motion), and results in mixing or mass transport without requiring **directed bulk motion**.



# Physical Background

› Fick First Law:

$$\vec{J} = -D\nabla u$$

›  $u$ : Particle Concentration

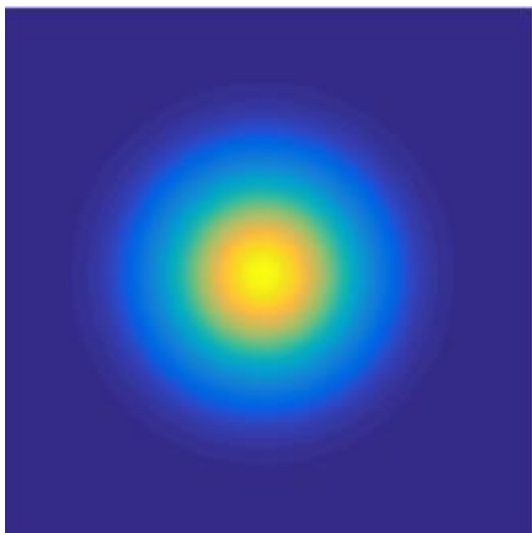
›  $\vec{J}$ : Diffusion flux vector, amount of substance per unit area per unit time in each direction

›  $D$ : is the diffusion coefficient (Tensor):

*A Positive Definite Symmetric Matrix*

# Physical Background

- › Isotropic vs Anisotropic Diffusion:
- › Isotropic: Diffusion Coefficient is the same in every direction.



$$\vec{J} \parallel \nabla u$$

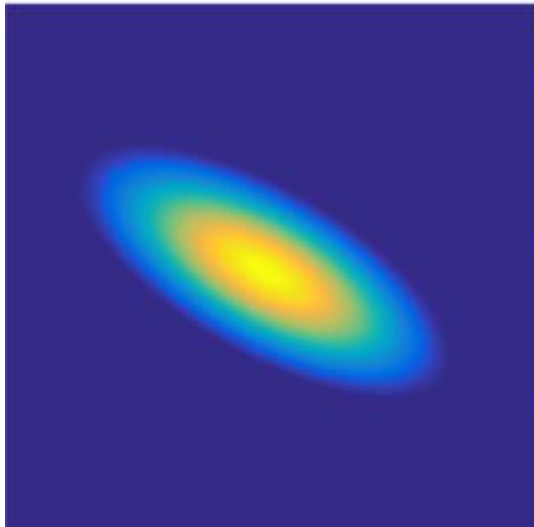
$$\mathcal{D} = \begin{bmatrix} D & 0 \\ 0 & D \end{bmatrix}$$



# Physical Background

- › Isotropic vs. Anisotropic Diffusion:
- › Anisotropic: Different diffusion coefficients along different directions.

$$\vec{J} \nparallel \nabla u$$



$$\mathcal{D} = \begin{bmatrix} D_{x_1 x_1} & D_{x_1 x_2} \\ D_{x_2 x_1} & D_{x_2 x_2} \end{bmatrix}, D_{x_1 x_2} = D_{x_2 x_1}$$

# Physical Background

- › Inhomogeneous vs. homogeneous diffusion:
- › Homogeneous Diffusion:  $D = D_0$  is constant tensor
- › Inhomogeneous Diffusion:  $D = D(x_1, x_2)$  is spatial variant tensor.

# Physical Background

- › Mass Conservation (continuity equation):

$$\frac{\partial u}{\partial t} = -\nabla \cdot \vec{J} = -\text{div}(\vec{J})$$

- › Using Fick's first law:

$$\frac{\partial u}{\partial t} = -\nabla \cdot \vec{J} = -\nabla \cdot (-D\nabla u) = \nabla \cdot (D\nabla u)$$

- › For homogeneous (Constant D) diffusion:

$$\frac{\partial u}{\partial t} = \nabla \cdot (D\nabla u) = D\nabla \cdot (\nabla u) = D\nabla^2(u)$$

- ›  $\nabla^2(u)$ : Laplacian

# Physical Background

› Fick's second law:

$$\frac{\partial u}{\partial t} = \nabla \cdot (D \nabla u)$$

› For homogeneous (Constant D) diffusion:

$$\frac{\partial u}{\partial t} = D \nabla^2(u) = D \left( \frac{\partial^2 u}{\partial x_1^2} + \frac{\partial^2 u}{\partial x_2^2} \right)$$

› Similar to heat equation

# Homogeneous Linear Diffusion Filtering

› Consider the following isotropic diffusion problem:

$$\begin{cases} \frac{\partial u}{\partial t} = D \nabla^2 u & -\infty < x_1, x_2 < +\infty \\ u(x_1, x_2, t = 0) = u_0(x_1, x_2) \end{cases}$$

› A PDE with initial condition (not boundary condition)

›  $u_0(x_1, x_2)$ : Noisy image as initial condition

› It can be shown:

$$u(x_1, x_2) = u_0(x_1, x_2) ** h(x_1, x_2, t)$$

$$h(x_1, x_2, t) = \frac{1}{4\pi Dt} \exp\left(-\frac{x_1^2 + x_2^2}{4Dt}\right)$$

# Homogeneous Linear Diffusion Filtering

› Solution:

$$u(x_1, x_2) = u_0(x_1, x_2) ** h(x_1, x_2, t)$$

$$h(x_1, x_2, t) = \frac{1}{4\pi Dt} \exp\left(-\frac{x_1^2 + x_2^2}{4Dt}\right)$$

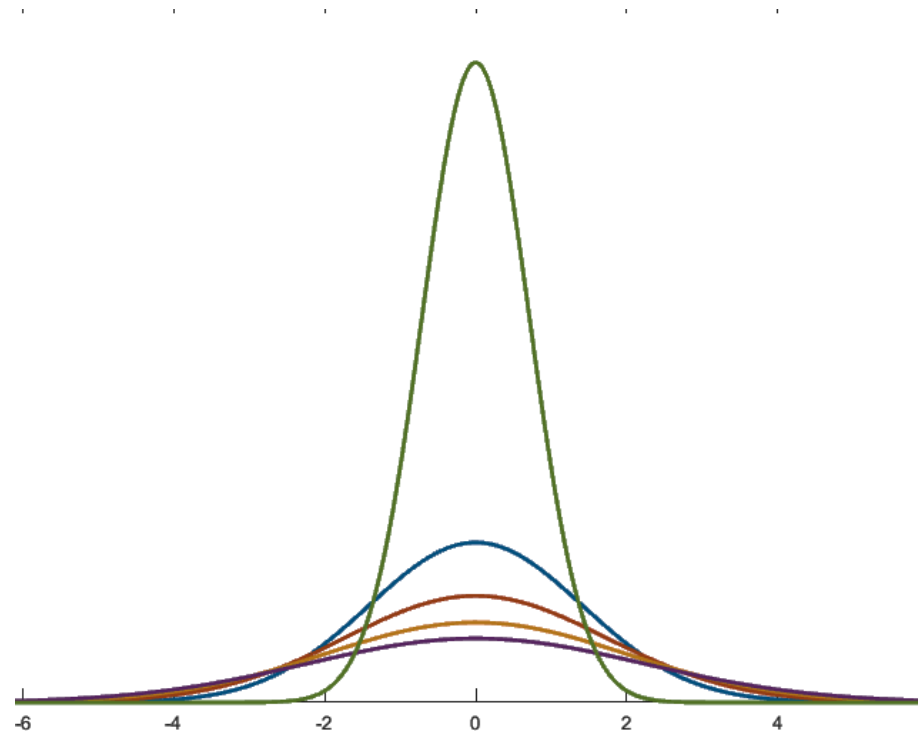
› Old fashion gaussian filtering ( $2Dt = \sigma^2$ )

$$h(x_1, x_2, t) = \frac{1}{2\pi\sigma^2} \exp\left(-\frac{x_1^2 + x_2^2}{2\sigma^2}\right)$$

› A scale-space filtering!

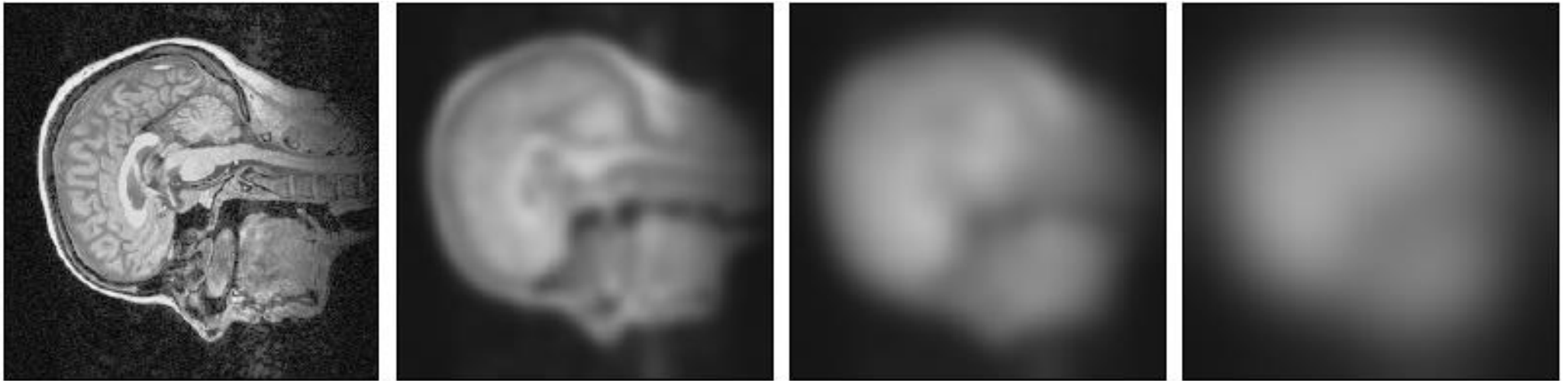
# Homogeneous Linear Diffusion Filtering

› A scale-space filtering,  $h(r, t)$ ,  $r = \sqrt{x_1^2 + x_2^2}$



# Homogeneous Linear Diffusion Filtering

› Scale-space filtering example:





# Homogeneous Linear Diffusion Filtering

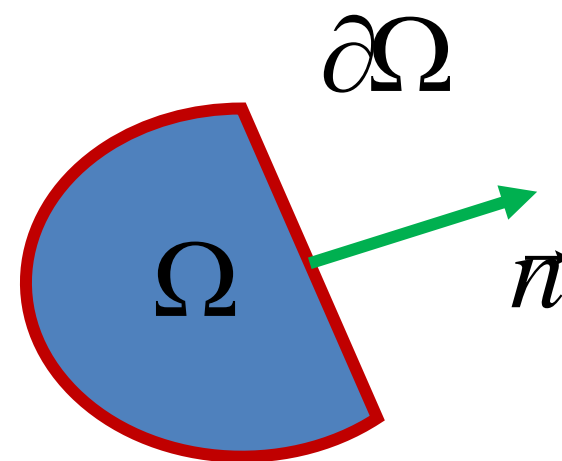
› A more realistic processing ( $\Omega$ : image domain)

$$\begin{cases} \frac{\partial u}{\partial t} = D \nabla^2 u & (x_1, x_2) \in \Omega \\ u(x_1, x_2, t = 0) = u_0(x_1, x_2) \\ \frac{\partial u}{\partial \vec{n}} \Big|_{\partial \Omega} = 0 \end{cases}$$

›  $\Omega$ : image domain

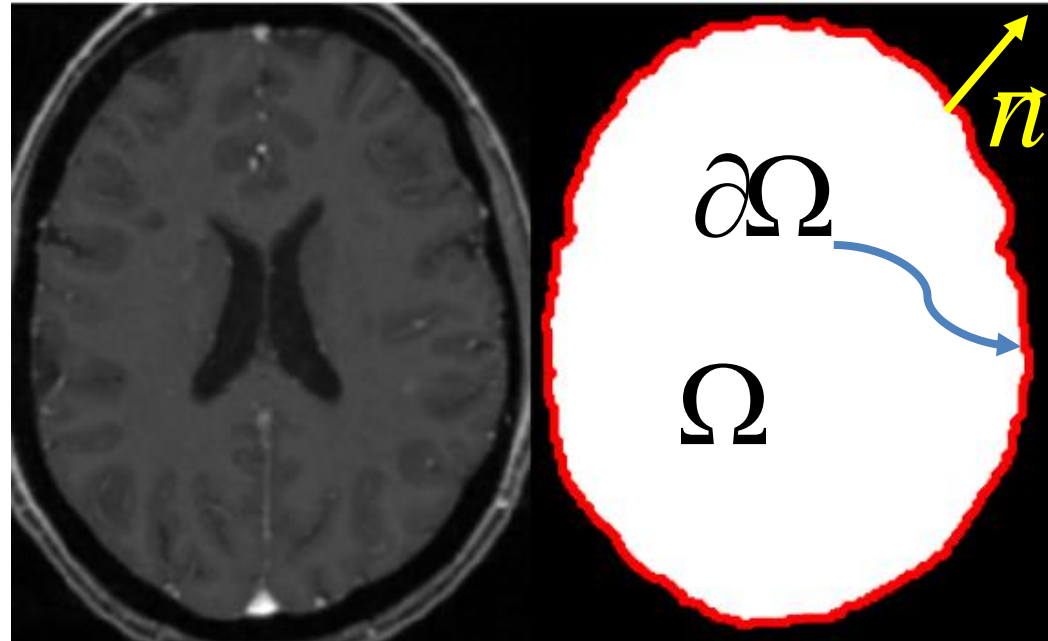
›  $\partial \Omega$ : image boundary

›  $\vec{n}$  : image normal vector



# Homogeneous Linear Diffusion Filtering

- › Boundary extraction to avoid unnecessary image blurring



# Inhomogeneous Linear Diffusion Filtering

› An Edge-Aware diffusion filter (version #1)

$$\text{› } \frac{\partial u}{\partial t} = \nabla \cdot (g(|\nabla f|^2) \nabla u), \quad (x_1, x_2) \in \Omega$$

$$\text{› } u(x_1, x_2, t = 0) = f(x_1, x_2)$$

$$\text{› } \left. \frac{\partial u}{\partial \vec{n}} \right|_{\partial \Omega} = 0$$

›  $f(x_1, x_2)$ : Noisy image as initial condition

›  $g(s)$ : A monotonically decreasing function

# Inhomogeneous Linear Diffusion Filtering

- › Diffusion Coefficient function
- ›  $g(s^2)$ : A monotonically decreasing function
- ›  $g(s^2) = \frac{g_0}{\sqrt{1+s^2/\lambda^2}}$ , Charbonnier
- ›  $g(s^2) = \frac{g_0}{1+s^2/\lambda^2}$ , Perona-Malik
- ›  $g(s^2) = g_0 \exp(-s^2/\lambda^2)$ , Gaussian

# Inhomogeneous Linear Diffusion Filtering

- › An Edge-Aware diffusion filter (version #2)
- ›  $f$  is too noisy for gradient estimation, try smoothing (regularization)
- ›  $\frac{\partial u}{\partial t} = \nabla \cdot (g(|\nabla f_\sigma|^2) \nabla u), (x_1, x_2) \in \Omega$
- ›  $u(x_1, x_2, t = 0) = f(x_1, x_2), \quad \frac{\partial u}{\partial \vec{n}} \Big|_{\partial \Omega} = 0$
- ›  $f(x_1, x_2)$ : Noisy image as initial condition
- › where,  $f_\sigma = f * G_\sigma$  (Gaussian Smoothing)

# Inhomogeneous Nonlinear Diffusion Filtering

- › An Edge-Aware diffusion filter (version #3)
- › Use  $u$  for gradient smoothing,
- ›  $\frac{\partial u}{\partial t} = \nabla \cdot (g(|\nabla u|^2) \nabla u), (x_1, x_2) \in \Omega$
- ›  $u(x_1, x_2, t = 0) = f(x_1, x_2), \quad \frac{\partial u}{\partial \vec{n}} \Big|_{\partial \Omega} = 0$
- ›  $f(x_1, x_2)$ : Noisy image as initial condition
- › This PDE is nonlinear, inhomogeneous, but isotropic

# Inhomogeneous Nonlinear Diffusion Filtering

- › An Edge-Aware diffusion filter (version #4)
- ›  $u$  is noisy in early steps, try smoothing (regularization):
- ›  $\frac{\partial u}{\partial t} = \nabla \cdot \left( g \left( |\nabla u_{\sigma(t)}|^2 \right) \nabla u \right), \quad (x_1, x_2) \in \Omega$
- ›  $u(x_1, x_2, t = 0) = f(x_1, x_2), \quad \frac{\partial u}{\partial \vec{n}} \Big|_{\partial \Omega} = 0$
- ›  $f(x_1, x_2)$ : Noisy image as initial condition
- › where,  $u_{\sigma(t)} = u * G_{\sigma(t)}$  (Gaussian Smoothing), and  $\sigma(t)$  is a decreasing function of time steps.

# Inhomogeneous Nonlinear Diffusion Filtering

› An Edge-Aware diffusion filter (version #5)

› Add smoothing factor to equation

$$\text{› } \frac{\partial u}{\partial t} = \nabla \cdot \left( g \left( |\nabla u_{\sigma(t)}|^2 \right) \nabla u \right) + \beta(f - u), \quad (x_1, x_2) \in \Omega$$

$$\text{› } u(x_1, x_2, t = 0) = f(x_1, x_2), \quad \frac{\partial u}{\partial \vec{n}} \Big|_{\partial \Omega} = 0$$

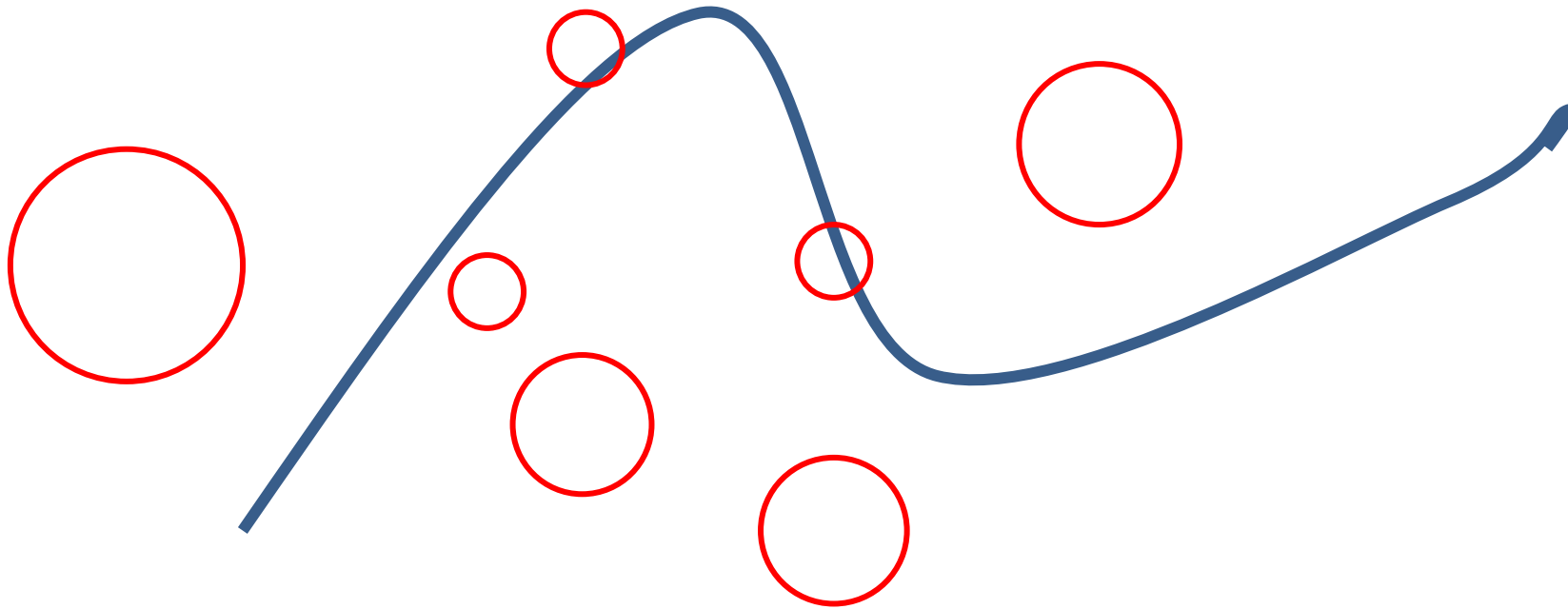
›  $f(x_1, x_2)$ : Noisy image as initial condition

›  $\beta$  : Adjust distance between initial,  $f$ , and final solution,  $u$ .



# Inhomogeneous Nonlinear Diffusion Filtering

› How it works, weak smoothing near the edges



# The End

› AnY QuEsTiOn?

