







A clinical and research 3T MRI protocol under 30 minutes

(Yes, it's possible!)

SK Larroque, M Carrière, C Martial, S Laureys github.com/LRQ3000/mri_protocol

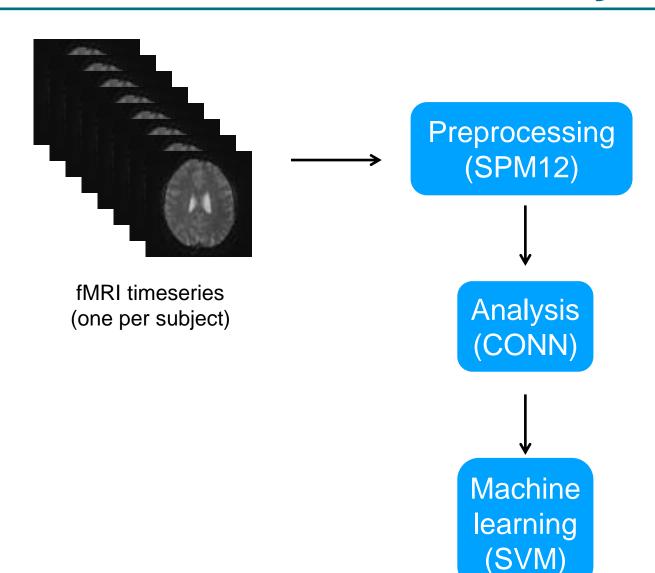


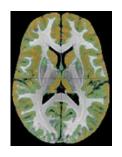
Coma Science Group GIGA Consciousness University & Hospital of Liège, Belgium

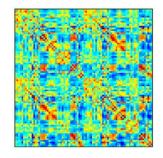
CME 2019 Dortmund, September 23th 2019

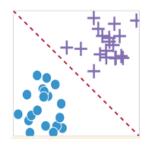
What we do: MRI analyses





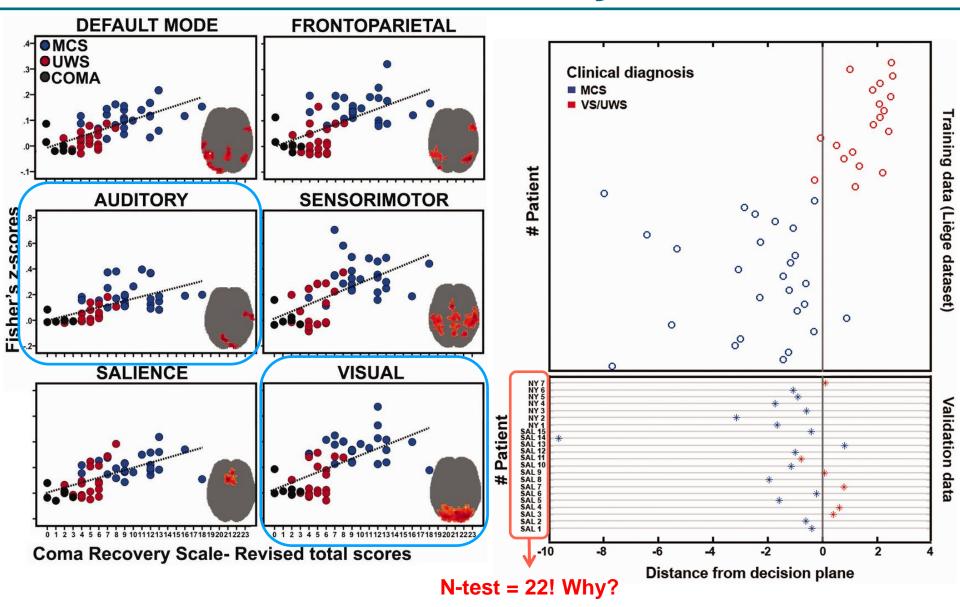






What we do: MRI analyses

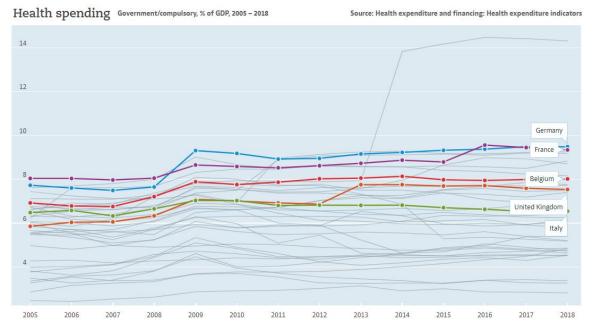




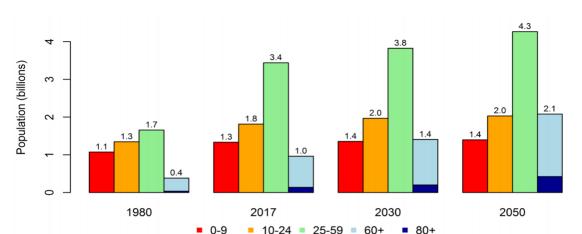
Limitations to sample size



Time Cost



Global population by broad age group, in 1980, 2017, 2030 and 2050



Fee-for-service, Diagnosis-relatedgroup payment^[4]

Limitations to sample size



1. Time & Cost

Healthy volunteers: compliant, cognitively autonomous

2. Motion & Sedation



Patients: uncontrolling or non-compliant, discomfort, monitoring vital parameters

Admitted

With MRI

Analyzable Non-sedated

Over 10 years (%):

676 (100%)

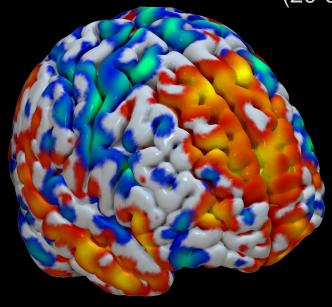
465 (69%)

256 (38%) ~110 (16%)

→ Overcome limitations by optimizing acquisition?

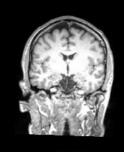
A 30 min cutting-edge, motion-resilient MRI protocol

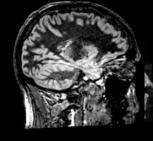
(20-channel coil, 3T Siemens Vida)

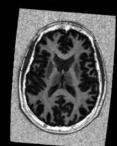


Sub-second BOLD TR 728ms 500 vols in 6:13

T1 FLAWS 5:02



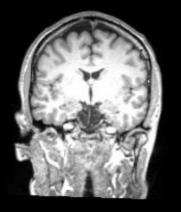


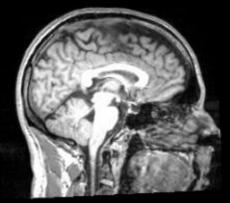




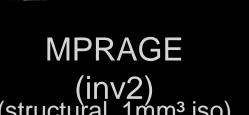
3-shells DWI 13:25

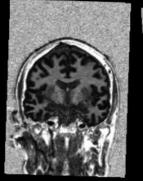
T1 FLAWS^[1] produces simultaneously:

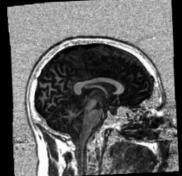


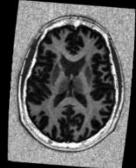


(inv2) (structural, 1mm³ iso)

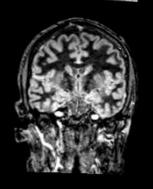


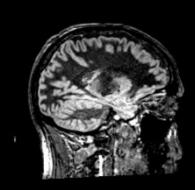






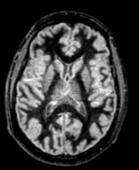
White Matter (uni)





→ Physiological segmentation:

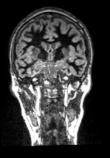
- No approximation (not computational!)
- In subject-space
- Always coregistered (even with motion)
- All in 5 min (on 3T), voxel size: 1mm iso
- More clinical infos (complement FLAIR) [1] Tanner et al, 2012

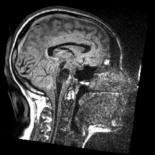


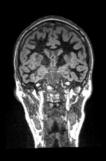
Grey Matter (inv1)

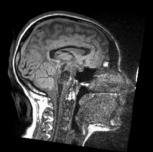
Our T1 FLAWS enhancements:

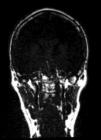
(see also alternatives in [1])

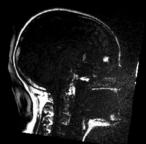


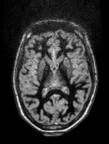




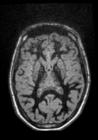




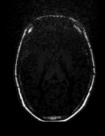




GM min(inv1, inv2)



GM mIP (inv1 .* inv2) ./ (inv1 + inv2)

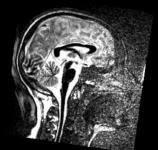


Skull inv1 .* uni

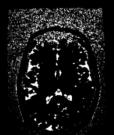




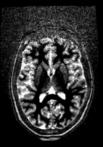




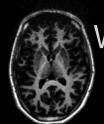




CSF inv1 - GM



CSF mIP inv1 - GM mIP

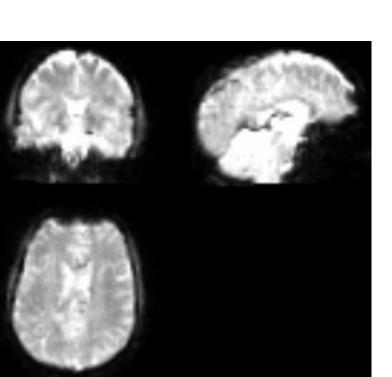


WM denoised inv2 .* uni

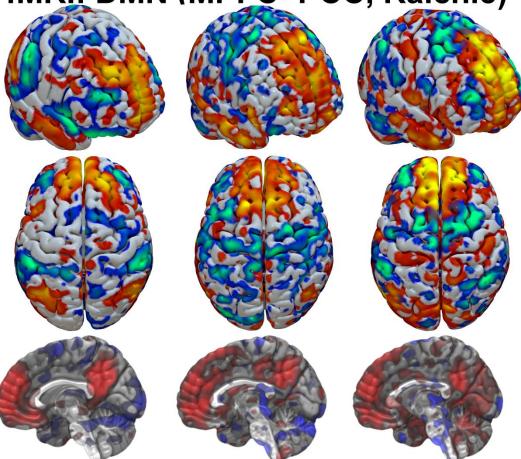
Sub-second EPI Bold fMRI

(728 ms, SMS x3, PI x2, 3mm³ iso)





First-level seed-based fMRI: DMN (MPFC+PCC, Raichle)



- Dynamic connectivity
- Bypass HRF (<1.5s)
- Motion resilient

NEW MRI OLD MRI 300 vols (10:00) 300 vols (3:47) 500 vols (6:13)

TR: 2s

TR: 728ms TR: 728ms

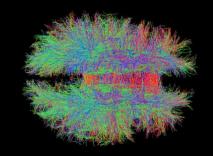
NEW MRI

OLD MACHINE DTI (SINGLE-SHELL B1000, WITH ACT)



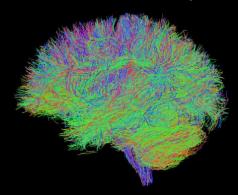




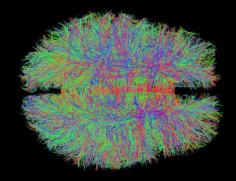


NEW MACHINE DTI (MULTI-SHELL 3-SHELLS, NO ACT) [1]









Optimizations:

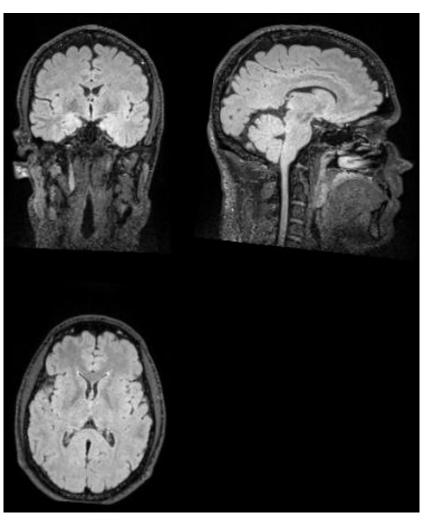
- 3 shells: b700 30dir, b1000 64dir, b2000 64dir.
- b1000 is high quality (small TE),
 others: higher TE → faster TR.
- SMS x4.
- Partial fourier 7/8 (warning: prevents mrdegibbs!)

Great for:

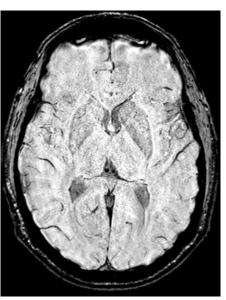
- Clinical tissue assessment under varying diffusion bvals
- Worst case: degrades to single-shell
- Standalone (structural unnecessary)

Clinical sequences: FLAIR, SWI, T2, ASL 🐸

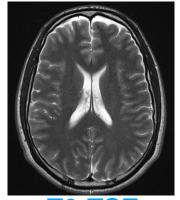




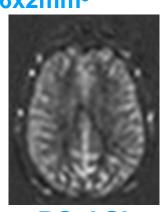
FLAIR 3:12, 1mm³



SWI SWI/mIP 3:57, 0.6x0.6x2mm³



T2-TSE 1:21, 0.4x0.4x4.0mm³



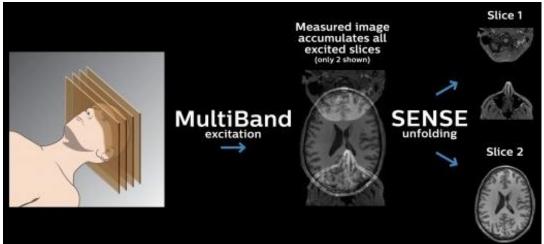
PC-ASL 2:17, 3mm³

How did we make it?



1) Technological optimizations:

- Modern acceleration: GRAPPA + multiband (SMS)[1]



- Literature
 MP2RAGE FLAWS, multi-shell DTI, multi-band BOLD
- Fine-tuning: calculations + trial-and-error
 BOLD flip angle, time of inversion, bandwidth, filters, ...

How did we make it? - 2



2) Meta-protocol optimizations:

- Protocol programming:
 - Maximize speed (motion resilience, avoids sedation & reacquisitions)
 - Acquire BOLD first (unlikely sedated)
 - Conditional naming
- Physical devices:
 - > Head immobilizer



(here: Pearltec MultiPad)





Take home message



- Cutting-edge research MRI under clinical constraints possible
- Quality-speed trade-off can be an opportunity
- New analyses opportunities in clinical populations (dynamic connectivity, multi-tissues unconstrained DTI, ...)
- Reduce risks & ethical issues by avoiding sedation

Future: compressed sensing, quantitative MRI, thermoplastic

mask^[1], AI reconstruction



(a) T₁ map, μ







(e) T_1 map, σ (f) T_2 map, σ (g) T_2^* map, σ (h) ρ^* map, σ Figure: Mean and standard deviation templates of the T_1 , T_2 , T_2^* and ρ^* map

Full protocol for Siemens Vida (need SMS license)
 & bibliography: github.com/lrq3000/neuro_slides/cme2019



Thank you for your attention!

github.com/LRQ3000/mri_protocol

Basic analysis scripts: github.com/LRQ3000/csg_mri_pipelines

Huge thanks to Jean-Marc Léonard at Siemens Healthineers, Nathalie Maquet and the Liège Hospital's radiology department team and Pearltec for their support!







Bonus slides

MRI: the time-quality conundrum



- Great polyvalence, for both research and clinical purposes
- Wide array of imaging contrasts: structural/function anatomy/connectivity, blood flow, lesions, etc.
- But clinical vs research needs are different:
 - Limited acquisition time (30 to 60 min) vs virtually unlimited (2h+)
 - Clinical pertinence (eg, lesions) vs cutting-edge (multi-shell DTI)
 - Uncooperative/uncontrolling patients (motion, discomfort, panic!)
 vs healthy volunteers (instruction compliance, no motion, calm)
- Usually results in a compromise: most sequences are clinical, some are for research with sub-optimal outdated (but faster) parameters

→ Can we make a MRI protocol both with cutting-edge research sequences and under clinical constraints?

How did we make it?



1) Technological optimization:

- Modern acceleration technologies:
 GRAPPA parallel imaging + simultaneous multi-slice
 (SMS aka multi-band).
 Beware of speed-quality trade-off!
- Literature for base sequences (MP2RAGE FLAWS, multi-shell DTI, multi-band BOLD)
- Calculations + trial-and-error to fine-tune parameters (BOLD flip angle, time of inversion, bandwidth)

How did we make it? - 2



2) Meta-protocol optimization:

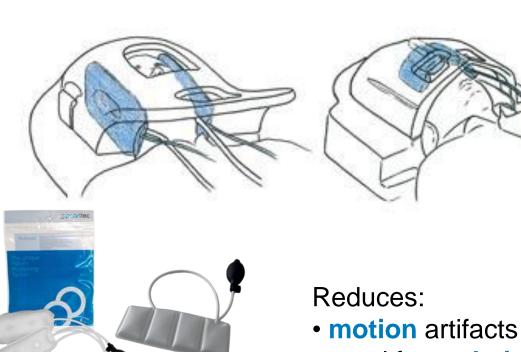
- Careful protocol programming:
 - Maximize speed of sequence acquisition (reduces risk of motion and need for sedation)
 - Place BOLD first, structural/rest after (ensures patient is awake, less distressed, always guarantees a non-sedated BOLD)
 - Sequence renaming depending on choices (eg, sedated or not?) for automatic documentation stored in DICOMs (bypass lack of conditional custom data storage in MRI software)

Physical devices:

- Head immobilizer
- Comfort knee pillow (reduces back pain), blanket, etc.

Inflatable 3D head immobilizer

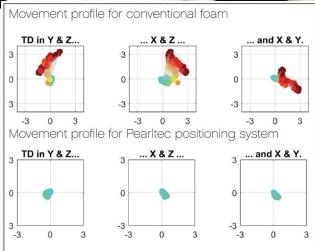




(here: Pearltec MultiPad)

- need for sedation (see infants studies, eg, Yamamura & Inatomi et al, 2018)







Future: Thermoplastic masks?





(Mandija, Agata et al 2019)

Take home message



- Possible to have a cutting-edge research MRI protocol under clinical constraints, through careful optimization
- Don't need perfection, just something that works with sufficient quality (speed-quality trade-off always applies)
- New analyses opportunities in clinical populations (dynamic connectivity, multi-tissues unconstrained DTI, accurate subject-level segmentation)
- Reduce risks & ethical issues by avoiding sedation
- Future: compressed sensing, quantitative MRI, thermoplastic mask^[1]
- → Full protocol for Siemens Vida (req SMS): github.com/lrq3000/neuro_slides/cme2019

Additional advices



- Enable 3D distortion correction, for all!
- Use alternate streams, allows to save uncorrected versions at no cost! Eg, distortion correction + motion can mess FLAWS, nice to have the original!

TODO Add example FLAWS messed

- Enable Prescan Normalize for subcortical analysis (all sequences), disable other filters (Hamming etc)
- Disable PACE (prospective motion correction), as this prevents retrospective motion correction (ie, with external softwares such as ART)
- If lots of Gibbs noise (eg, in FLAWS or MP2RAGE), lower GRAPPA acceleration!
- For multi-shell DTI, acquire 3 different DTI sequences and bundle together with a Copy Reference to copy the acquisition parameters automatically (necessary for the multishell DTI to be valid)

Additional advices



- With uncooperative/uncontrollable populations, the speed-quality trade-off might be simpler: better to speed up and have a more stable (but lower resolution) image, than have a high-resolution image that fails most of the time to be acquired because of motion!
- Acquire with interpolation and rescale, eg: acquire at 0.5x0.5x1.0mm and rescale to 1.0mm³, slight increase in SNR
- Increasing bandwidth reduces susceptibility to metal and chemical artifacts, useful for patients with potentially blood or metal infarcts

About free experimentation



- Feel free to experiment with your protocol, often the sequences are not optimized for your machine and/or needs.
- How to proceed: no necessary need for calculations, trial and error is still the best approach (use bisection approach), but where available, calculations can save you some time instead.
- Try on a dummy or a healthy volunteer, under supervision from radiologists or MRI brand engineer to ensure no risks notably of tissue over-heating. Normally most modern machines implement safeguards that should in any case prevent these issues by warning the operator and change adequately the protocol.

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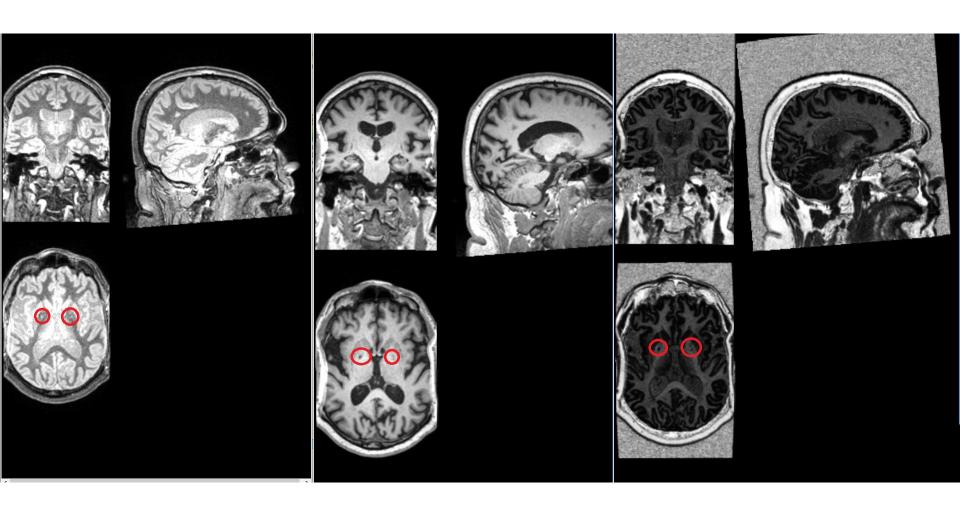
Clinical T1 FLAWS vs FLAIR





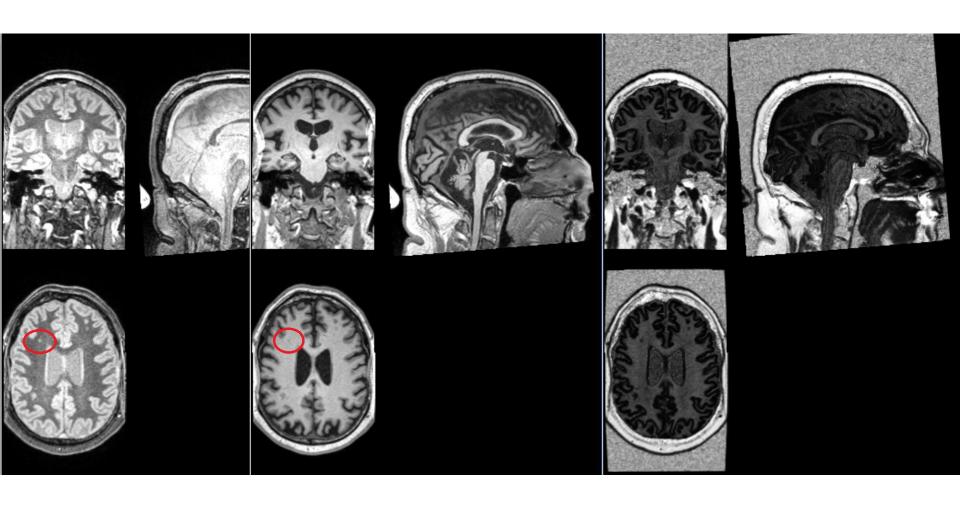
Clinical T1 FLAWS vs FLAIR





Clinical T1 FLAWS vs FLAIR





MRI protocol sequences list



- 1. AAhead_scout
- 2. Decision: Patient anesthetized?

Yes:

```
ep2d_bold_repos_moco_s3_p2_short avec AG
```

No:

```
ep2d_bold_repos_moco_s3_p2_short sans AG
```

3. Decision: Patient anesthetized?

Yes:

- AAhead_scout
- ep2d_bold_repos_moco_s3_p2_long_ avec_AG

No:

ep2d_bold_repos_moco_s3_p2_long_ sans_AG

- 4. gre_field_mapping
- 5. t1_mp2rage_sag_p3_iso
- 6. t1_mp2rage_sag_p2_iso_FLAWS_fast
- 7. ep2d_diff_mddw_30_p2_s3_b700
- 8. ep2d_diff_mddw_64_p2_s3_b1000
- 9. ep2d_diff_mddw_64_p2_s3_b2000
- 10. t2_space_FLAIR_sag_p3_iso
- 11. t2_swi_tra_p3_1.5mm
- 12. t2_tse_tra_512_p2
- 13. asl 3d tra fast

SIEMENS MAGNETOM TrioTim syngo MR B15

\\USER\Head Lg\Study Neuro Lg\MyGroup Lg\ep2d_bold_rest

Slice order: check in the machine's printout!

Voxel size: 3.0×3.0×3.0 mm Rel. SNR: 1.00 Special sat. None Properties Prio Recon Off System Before measurement Body After measurement On Load to viewer On HEA On Inline movie Off REF Positioning mode Auto store images On Table position Load to stamp segments Table position 0 mm Load images to graphic Off MSMA S-C-T segments R>>L Sagittal Auto open inline display A >> P Coronal AutoAlign Spine Off Transversal F >> H Start measurement without On Adaptive Combine Coil Combine Mode further preparation Auto Coil Select Default On Wait for user to start single Standard Start measurements Shim mode Off Adjust with body coil Routine Off Confirm freq. adjustment Slice group 1 Assume Silicone Off 32 Slices 353.882 V ! Ref. amplitude 1H Dist. factor 25 % Adjustment Tolerance Auto Position Isocenter Adjust volume Orientation Transversal Position Isocenter A >> P Phase enc. dir. Orientation Transversal Rotation 0.00 deg 0.00 deg Rotation Phase oversampling 0 % R >> L 192 mm FoV read 192 mm A >> P 192 mm FoV phase 100.0 % F >> H 120 mm Slice thickness 3.0 mm TR 2000 ms ΤE 30 ms 1st Signal/Mode None Averages BOLD Concatenations GLM Statistics Off Prescan Normalize Filter Dynamic t-maps On Coil elements HEA;HEP Starting ignore meas 0 Contrast Ignore after transition 0 MTC Model transition states On 78 deg Flip angle Temp, highpass filter On Fat suppr. Fat sat 4.00 Threshold Paradigm size 30 Long term Averaging mode Meas[1] Baseline Reconstruction Magnitude Meas[2] Baseline Measurements 300 Meas[3] Baseline Delay in TR 0 ms Meas[4] Baseline Off Multiple series Meas[5] Baseline Resolution Meas[6] Baseline Base resolution Meas[7] Baseline 100 % Phase resolution Meas[8] Baseline Phase partial Fourier Meas[9] Baseline Off Interpolation Meas[10] Baseline Meas[11] Baseline PAT mode None Meas[12] Baseline Matrix Coil Mode Auto (CP) Meas[13] Baseline Meas[14] Baseline Distortion Corr. Off Off Meas[15] Baseline Unfiltered images Meas[16] Active On Prescan Normalize Meas[17] Active On Raw filter Meas[18] Active Elliptical filter Off Meas[19] Active Hamming Off Meas[20] Active Geometry Meas[21] Active Multi-slice mode Interleaved Meas[22] Active Series Ascending Meas[23] Active

5/+

This « interleaved » means nothing!

Geometry
Multi-slice mode Interleaved
Series Ascending

Ascending = sequential ascending. Else it would be «interleaved » here for interleaved ascending.

Manual

Automatic (mostly)

Typical fMRI processing steps



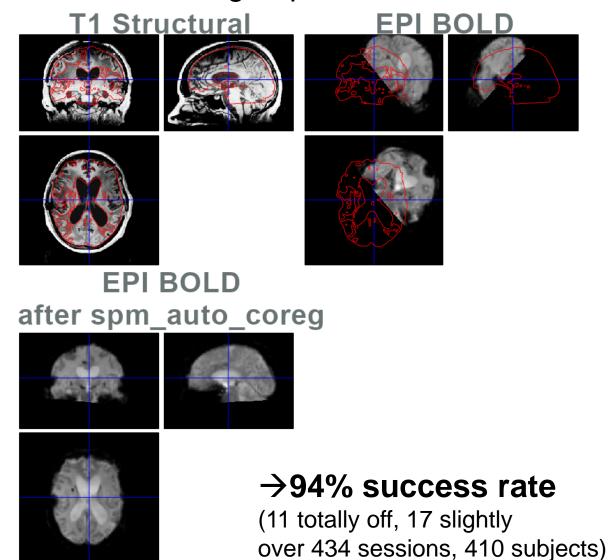
- Select subjects, prepare demographics (age, gender, etiology, sedation, etc)
- Convert from DICOM to NIfTI
- Exclude bad subjects (too much motion, artifacts, brain surgery, metallic prosthesis, etc)
- T1 reorient
- EPI/DTI manual coregistration
- Slice timing correction
- Realignment (motion correction)
- Auto coregistration
- Segmentation + Normalization (MNI 152)
- Smoothing
- Movement correction/rejection
- Denoising (PCA aCompCorr, ICA, etc.)

Takes > 90%
— of the analysis time!

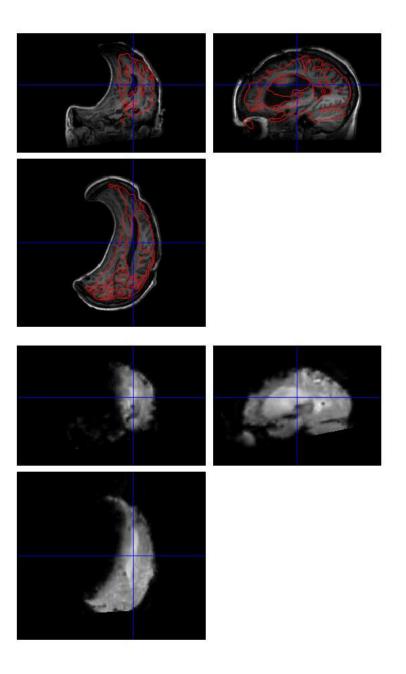
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spm_auto_reorient_coregister: Enhanced automatic reorientation and core

Enhanced automatic reorientation and coregistration on brain damaged patients with SPM12

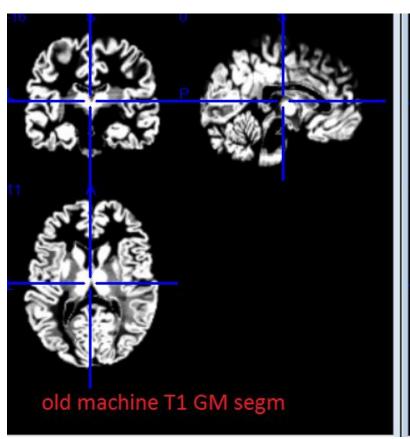


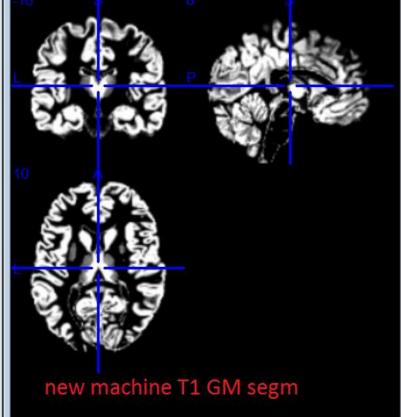
https://github.com/lrq3000/spm_auto_reorient_coregister



QA image example (same subject)







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QA image example (same subject)



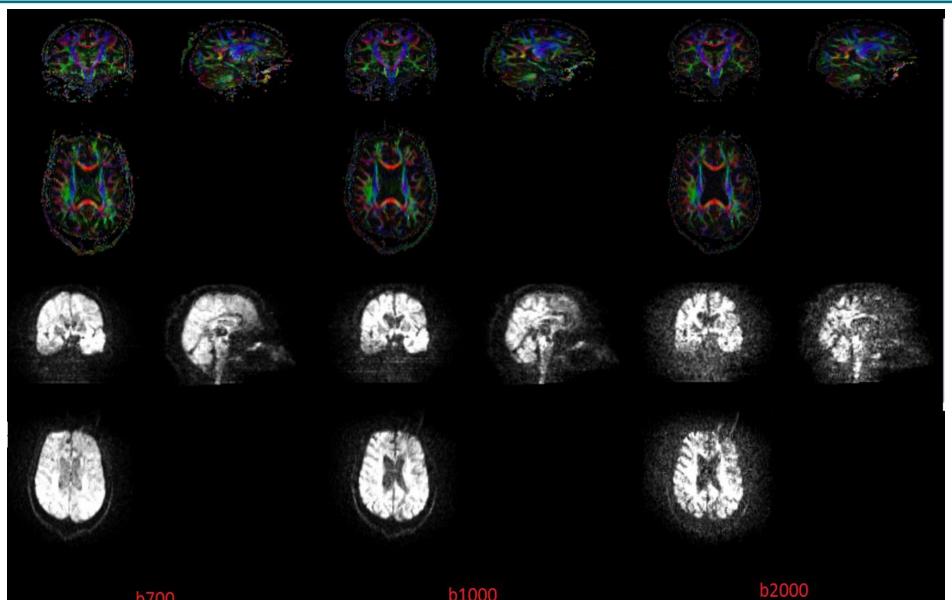




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Multi-shell DTI





A 30 min cutting-edge MRI protocol



(20-channel coil)



Short BOLD 3min47: Non-sedated! (except if really problematic patient) Better have motion than sedation! (we can correct motion, but not sedation!

Might be sedated if necessary, but please avoid

Structural: Sedation OK!

Note: If sedated, please choose « yes » in the boxes highlighted here in red.

Please do not delete or replace any sequence! (Sequence name will change according to sedation decision set here)

Note2: 3 DTI sequences go together ALWAYS! If you need to redo DTI, please redo them all!

All sequences can be implemented on any 3T Siemens with multiband and MP2RAGE (multi-echo T1) support (here Vida)