### Attenuation-based Light Field Displays

#### Bachelorarbeit

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#### Abstract

Abstract goes here

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# Chapter 1

# Introduction

1.1 Related Work

## Chapter 2

## Capturing a Light Field

#### 2.1 The Plenoptic Function and the Light Field

The plenoptic function, as introduced by [AB91], is a 7D function that describes the intensity of light for every frequency, along every light ray in space, at any time. It is defined as

$$P \colon \mathbb{R}^3 \times [0, 2\pi) \times [0, \pi] \times \mathbb{R}^2 \to \mathbb{R}^+$$
$$(x, y, z, \theta, \phi, t, \lambda) \mapsto P(x, y, z, \theta, \phi, t, \lambda),$$

where the parameters (x,y,z) are the coordinates of a point in 3D space and the angles  $(\theta,\phi)$  describe the direction of an incoming light ray at time t. The light's intensity is given for every wavelength  $\lambda$  and thus, the plenoptic function not only captures the visible frequency spectrum but all electromagnetic waves. A commonly used measure for light is the radiance, which is obtained from P by integrating over all wavelengths:  $R(x,y,z,\theta,\phi,t) = \int_{\mathbb{R}} P(x,y,z,\theta,\phi,t,\lambda) \, d\lambda$ .

In practice, it is impossible to acquire all the data needed to model the 7D plenoptic function and hence it is reasonable to consider only a subset of the parameters. Dropping the time parameter t in  $R(x, y, z, \theta, \phi, t)$  yields a 5D function for the radiance in a static scene. As described by [LH96], this five dimensional representation can further be reduced to four dimensions in the following way. The radiance along a line is constant in free space and so, the 5D plenoptic function holds redundant information for the points on this line. Ignoring this redundancy leads to the equivalent 4D parameterization of the ray space. [LH96] propose a parameterization by two parallel planes, as seen in figure 2.1, where the coordinates of the lines (rays) are given by the intersections with the two planes. The 4D light field L(u, v, s, t) is therefore defined as the radiance along the line intersecting the two planes at coordinates (u, v) and (s,t). This two-plane parameterization of the light field is the most common one seen in literature, but there are many ways to choose a parameterization. For instance, one can use a plane and two angles to define each ray passing this plane, which would result in a light field  $L(u, v, \theta, \phi)$  where  $\theta, \phi \in (0, \pi)$ .

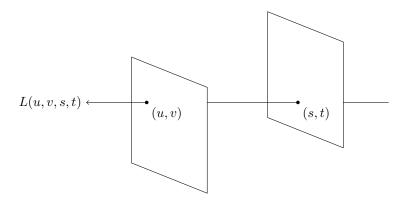


Figure 2.1: Parametrization of the light field with two planes.

#### 2.2 Light Field Acquisition

For practical applications, the light field must be discretized and so, an appropriate sampling method needs to be chosen. This means that only a slice of the actual light field can be captured and the two planes are clipped to form rectangles. In this work, the term *light field* is used for both the infinite, continuous light field as well as the discrete collection of data samples.

#### **Oblique Projection**

Oblique projection, as shown in figure 2.2(a), is a special case of orthographic projection: The parallel rays do not need to be perpendicular to the image plane of the camera. The advantage is that there is a one-to-one correspondence between camera position and ray angle, since all rays in one camera are parallel. This means that the angular resolution is simply the number of cameras, and the spatial resolution is the number of pixels in the image plane. The angular extent from  $\theta_{\min}$  to  $\theta_{\max}$  is called the **field of view** (FOV) of the light field and should not be confused with the field of view of a conventional camera. For a uniform angular sampling with resolution  $N_{\theta} \times N_{\phi}$ , the angles  $\theta_i$  and  $\phi_j$  are

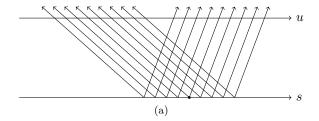
$$\theta_i = \theta_{\min} + (i-1) \frac{\text{FOV}_{\theta}}{N_{\theta} - 1}, \qquad \phi_j = \phi_{\min} + (j-1) \frac{\text{FOV}_{\phi}}{N_{\phi} - 1},$$
 (2.1)

where  $i = 1, 2, ..., N_{\theta}$  and  $j = 1, 2, ..., N_{\phi}$ .

Given a light field L(u,v,s,t) and the distance d between the two planes, a re-parameterization  $L'(\theta,\phi,s,t)$  can be obtained according to figure 2.2(b) by the transformation

$$\theta = \arctan\left(\frac{u-s}{d}\right), \qquad \phi = \arctan\left(\frac{v-t}{d}\right).$$
 (2.2)

Note that uniform sampling in angular dimension does not yield a uniform grid in the (u, v)-plane. Despite the simplicity of this projection type, it is not feasible to build cameras of this type and so, oblique projection is left to be used exclusively by computers for rendering synthetic scenes.



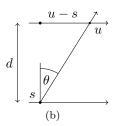


Figure 2.2: (a) Light field aquisition using oblique projection. (b) Reparameterization of the two-plane representation to angular coordinates.

#### Perspective Projection

Another way to capture the light field is with a grid of optical systems, e.g. cameras. Typically, the (u,v)-plane is sampled on a grid  $G_{uv}=\{(u_i,v_j)\mid i=1,\ldots,n,j=1,\ldots,m\}$  on the (u,v)-plane with a resolution  $n\times m$ . The extent in horizontal (vertical) direction is called the horizontal (vertical) baseline. Although it is strictly speaking not correct, the resolution of the (u,v)-plane is often referred to as the angular resolution. The angles of the rays in a light field captured by perspective projections are determined by the focal length, the sensor size and the sensor resolution of the camera. For a camera light field, typically it is expected that

- All cameras are placed at grid positions in  $G_{uv}$  on the same plane, called the (u, v)-plane,
- The optical axes of the cameras are orthogonal to the (u, v)-plane,
- All cameras have the same intrinsic parameters (e.g. focal length).

In this case, the focal planes of all cameras coincide with a common focal plane, the (s,t)-plane. Figure 2.3(a) shows this scenario for three cameras in two dimensions. Given images  $I_{uv}(x,y)$  with respect to a coordinate system centered at the camera position (u,v), the coordinates on the (s,t)-plane are s=u+x, and t=v+y. Thus, the light field in continuous coordinates is obtained by

$$L(u, v, s, t) = L(u, v, u + x, v + y) = I_{uv}(x, y).$$
(2.3)

In the discrete case, each camera captures sample points on the (s,t)-plane, but not everyone of these sample points on the (s,t)-plane is captured by every camera. So, as demonstrated in figure 2.3(b), the camera images need to be rectified such that all discrete coordinates (u,v,s,t) correspond to valid rays. This rectification process is equivalent to a re-parameterization L' of the continuous light field L, given by the formula

$$L'(u, v, s', t') = L(u, v, \gamma(s' - u) + u, \gamma(t' - v) + v), \qquad (2.4)$$

where  $\gamma=\frac{d}{d'}$  and d' is the distance between the (u,v)-plane and the new (s',t')-plane. As derived by [IMG00], this re-parameterization is equivalent to a 4D shear.

A different way to understand this coordinate change is to imagine the (u, v)and (s, t)-plane being the aperture and sensor planes respectively, resulting in

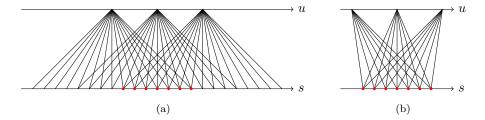


Figure 2.3: Perspective projections of a scene. (a) Projections with three pinhole cameras. (b) Discarding unused rays corresponds to cropping the camera images.

one big camera in which a light field is formed. Changing the distance between the two planes is now equivalent to changing the focal length of this one camera. The effect on the light field inside is similar to refocusing, except that in a conventional camera, the image on the sensor is formed by a weighted integral over u and v such that the angular information vanishes. Objects at focal distance from the camera would appear sharp and objects away from the focal point would become blurred.

From stereo vision, it is known that the displacement of the projections in the image planes of two cameras is only dependent on the focal length f, the baseline  $\Delta u$  and the distance z, and the relation is given by  $\Delta s = f\Delta u/z$ . This knowledge can directly be applied to the two-plane parameterization. For the continuous light field, it amounts to

$$ds = -\frac{d}{z} du$$
 and  $dt = -\frac{d}{z} dv$ . (2.5)

In the discrete case, the displacement  $\Delta s$  or  $\Delta t$  is also called the **disparity** and is often given in pixel units.

#### 2.3 Visualization

The epipolar-plane image (EPI) allows for a very intuitive visualization of depth from a 4D light field. It was first defined by [BBM87] as follows. Consider a point P in 3D space and a pair of cameras with the optical axis pointing in the same direction. The plane passing through P and the two centers of projection is called the **epipolar plane**. The epipolar plane projects to a line on each of the camera image planes, named the **epipolar line**. This line represents a constraint for the projection of P in each of the images and it is used to solve the correspondance problem in computer vision. The notion of epipolar lines can be directly applied to a multiple camera setup. In figure 2.4, a synthetic scene is rendered in 500 different positions along a horizontal baseline. Since the camera movement is in horizontal direction only, the epipolar lines correspond to a fixed pixel row in each image. The EPIs shown in figures 2.4(b) and 2.4(c) are created by collecting the chosen pixel row (scanline) in every image and stacking it up.

As described in the previous section, the depth component of P occurs as a displacement of the projections in consecutive images Under the assumption

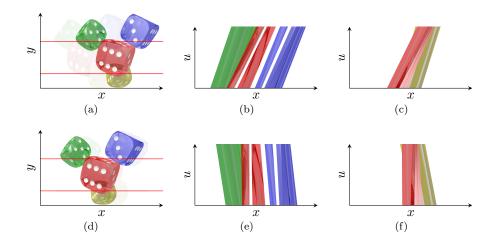


Figure 2.4: (a) Raw 3D light field rendered from 500 positions along a horizontal baseline. Two scanlines are extracted from every image. (b) The feature paths of the blue and green dice have a steeper slope than those of the red die. (c) Feature paths of the yellow die have an even steeper slope, indicating greater depth. (d) The light field is rectified according to figure 2.3(b) such that the disparities of the red die are approximately zero. (e) - (f) EPIs from the same scanlines. The slopes of the feature paths stay the same relative to each other.

that the (u, v)-plane is sampled uniformly, the disparity D with respect to P is stays constant from one image to the next. Thus, following the projection of the point P in every image corresponds to a line in the EPI with slope 1/D. [BBM87] refer to this line as the **feature path**. This means that points farther away from the camera will appear as a feature path in the EPI with steeper slope than points close to the camera. Note that the depth range in the light field can immediately be determined by identifying the maximum and minimum slope in the EPI. Also, for a perfectly Lambertian scene, each line in the EPI has a uniform color.

## Chapter 3

## Light Field Tomography

#### 3.1 A Model for Light Attenuation

The light field display is modeled by a volumetric attenuator  $\mu(x, y, z)$  that attenuates the light traveling through its material. According to the Beer-Lambert law, the intensity of a light ray  $\mathcal{R} \subset \mathbb{R}^3$  passing through the material decreases exponentially over distance:

$$I = I_0 e^{-\int_{\mathcal{R}} \mu(r) \, \mathrm{d}r}. \tag{3.1}$$

The incident intensity  $I_0$  is the intensity of the ray before it enters the attenuator. Equation 3.1 can be rewritten into

$$\bar{I} := \log\left(\frac{I}{I_0}\right) = -\int_{\mathcal{P}} \mu(r) \, \mathrm{d}r.$$
 (3.2)

Now, let the attenuator  $\mu(x,y,z)$  be a cubic slab of height d in Z-direction and let L(u,v,s,t) be the two-plane parameterization of the light field such that the (s,t)-plane coincides with the (x,y)-plane of the attenuator and the (u,v)-plane is at distance d. The set of points describing the ray defined by the coordinates (u,v,s,t) is

$$\mathcal{R} = \left\{ \lambda a + b \mid a = \begin{pmatrix} u - s \\ v - t \\ d \end{pmatrix}, b = \begin{pmatrix} s \\ t \\ 0 \end{pmatrix}, \lambda \in \mathbb{R} \right\}. \tag{3.3}$$

A point  $p = (x, y, z)^T$  is part of the ray  $\mathcal{R}$  if and only if

$$\exists \lambda \in \mathbb{R} : p = \lambda a + b \qquad \Longleftrightarrow \qquad a \times (p - b) = 0, \tag{3.4}$$

where  $\times$  denotes the cross product. Now, I can be replaced with the light field L and the right hand side of equation 3.2 can be written as an integral over  $\mathbb{R}^3$ :

$$\bar{L}(u, v, s, t) = -\int_{\mathbb{R}^3} \mu(p)\delta(a \times (p - b)) \,\mathrm{d}p. \tag{3.5}$$

Here,  $\delta$  denotes the Dirac delta function on  $\mathbb{R}^3$  and  $\mu$  is zero outside the boundaries of the slab. This means that the integrand is only non-zero for points on the ray with coordinates (u, v, s, t).

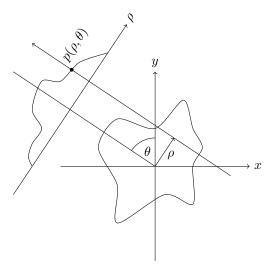


Figure 3.1: The 2D Radon transform of the ray  $(\rho, \theta)$  passing a material with density f(x, y).

Combining equation 3.1 and 3.5 gives the light field emitted by the attenuator. The goal is to produce such an attenuation display that emits a given target light field.

In computed tomography, the **Radon transform** of a real valued and compactly supported, continuous function f(x, y) on  $\mathbb{R}^2$  is defined as

$$p(\rho, \theta) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) \delta(x \cos \theta - y \sin \theta - \rho) dx dy,$$
 (3.6)

where  $(\rho, \theta) \in \mathbb{R} \times \left(-\frac{\pi}{2}, \frac{\pi}{2}\right)$  defines a ray as shown in figure 3.1. Because the Radon transform is essentially a line integral, it can be generalized to three or more dimensions. Adapting the notation from the two-plane parameterization, the Radon transform of the attenuation map  $\mu$  along ray  $\mathcal{R}$  becomes

$$p(u, v, s, t) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \mu(x, y, z) \delta\left(a \times \left((x, y, z)^{T} - b\right)\right) dx dy dz,$$
 (3.7)

which is equivalent to equation 3.5. This shows that

$$\bar{L}(u, v, s, t) = -p(u, v, s, t),$$
 (3.8)

or with the words of [WLHR11]: "The logarithm of the emitted light field is equivalent to the negative Radon transform of the attenuation map."

#### 3.2 Discrete Attenuation Layers

The previous section introduced a continuously varying attenuation map to model the display. [WLHR11] propose to represent the attenuator with a set of N two-dimensional layers, also called masks.

Let  $L_{ijkl} = L(u(i), v(j), s(k), t(l))$  be the matrix of samples from the light field and for simplicity, let m := m(i, j, k, l) be a linear index of the 4D indices. Equation 3.1 suggests a per-ray constraint in the form

$$L_m = L_0 \prod_{n=1}^{N} t^{(n)}(h(m,n)), \tag{3.9}$$

where h(m,n) is the (discrete) 2D coordinate of the intersection of the m-th ray with the n-th layer, and  $t^{(n)}(\xi)$  is the **transmittance** of layer n at that coordinate. Having a constraint for each ray, the goal is to solve for the transmittance t. However, the system of equations in 3.9 is non-linear and cannot directly be solved. One can obtain a linear system of equations by taking the logarithm in 3.9:

$$\bar{L}_m = \sum_{n=1}^N \log \left( t^{(n)}(h(m,n)) \right) = -\sum_{n=1}^N a^{(n)}(h(m,n)) = -P_m \alpha.$$
 (3.10)

Here,  $a^{(n)} := -\log t^{(n)}$  denotes the **absorbance** of layer n. This relation between transmittance and absorbance also directly follows from the Beer-Lambert law. Here,  $P_m = \left(P_m^{(1)}, \ldots, P_m^{(N)}\right)$  is a binary row vector, encoding the intersection of the ray with the pixels on each layer. The unknown absorbance is represented by the column vector  $\alpha = \left(\alpha^{(1)}, \ldots, \alpha^{(N)}\right)^T$ . Each  $\alpha^{(i)}$  is just a flattened representation of the absorbance matrix  $a^{(i)}$ . Note that equation 3.10 is the equivalent of the continuous version in 3.8, since  $P_m$  encodes the Radon transform. Finally, the above equations indexed by m can be combined into one large linear system  $P\alpha = -\bar{L}$ .

In most cases, P is not a square matrix and the system can become overdetermined, which means that it has no solution in general. However, it is still possible to find values for  $\alpha$  such that the error  $\|P\alpha + \bar{L}\|$  is small. Thus, the objective becomes

$$\label{eq:continuous_equation} \begin{split} \underset{\alpha}{\operatorname{argmin}} & \quad \left\| P\alpha + \bar{L} \right\|^2 \\ \text{subject to} & \quad 0 \leq \alpha \leq \infty. \end{split} \tag{3.11}$$

Finally, when optimal values  $\alpha$  are found, the transmittance used to fabricate the layers is obtained by calculating  $e^{-\alpha}$ . Also note that the matrix P is very sparse because it is assumed that a ray passes through each layer at exactly one pixel no more than once and inter-reflections between the layers are not supported by the model. Thus, P can be efficiently stored using an appropriate data structure.

#### 3.3 Iterative Reconstruction

The optimization problem in equation 3.11 is essentially a fitting problem. Theoretically, it can be solved in a least squares sense using the normal equation  $P^T P \alpha = P^T \bar{L}$  and by inverting the matrix  $P^T P$ . For high resolution light fields, the matrix P becomes extremely large and it is unfeasible to compute the inverse of  $P^T P$ .

In general, the approach to solve these kind of problems is to use iterative methods. The choice of the method depends on the type of problem and the structure of the design matrix. In computed tomography, a variety of iterative solvers have been developed to solve the exact same problem. Among the different methods is the Simultaneous Algebraic Reconstruction Technique (SART) first proposed by [AK84]. The update rule of SART for iteration  $k=0,1,2,\ldots$  is

 $\alpha^{(k+1)} = \alpha^{(k)} + \lambda C P^T R \left( \bar{L} - P \alpha^{(k)} \right), \tag{3.12}$ 

where  $\lambda$  is a relaxation factor. R and C denote the diagonal matrices with entries  $R_{ii} = \frac{1}{r_i}$  and  $C_{ii} = \frac{1}{c_i}$ , where  $r_i$  and  $c_i$  are the sum of the elements in the i-th row and column of P respectively. The parts in 3.12 involving P and  $P^T$  are also referred to as the **forward**- and **back-projection** respectively.

The convergence of SART has been studied by [JW01]. They have proven that it converges to a weighted least squares solution.

#### 3.4 Ray Casting

To obtain the linear system P, the intersections between the rays and the attenuation layers have to be calculated. This calculation depends on the parameterization of the light field. For continuous light fields, it is always possible to apply a re-parameterization to get the desired representation (e.g. the two-plane parameterization) and then compute the intersection in a standard way. For discrete light fields however, this would require a suitable interpolation in ray-space, which gives poor results when the distribution of samples in the target space becomes too sparse.

What follows is a description of two methods to compute the indices for the non-zero entries in P. For simplicity, only a two-dimensional attenuator of size w is assumed, consisting of N layers at various depths  $Z_{\min} = z_1 < z_2 < \cdots < z_N = Z_{\max}$ . It is also assumed that the image plane s of the virtual cameras is bisecting the attenuator in the middle, at depth  $z_0 = \frac{Z_{\max} - Z_{\min}}{2}$ .

#### **Oblique Projection**

The setup for the oblique projection type is illustrated in figure 3.2(a). Let  $\theta_i$  denote the angle of the *i*-th oblique view from the light field. Following the notation in previous sections, the linear index m = m(i, k) indentifies the ray  $(\theta_i, s(k))$ . The intersection of ray m with the n-th layer is simply

$$h(m,n) = s(k) + \Delta z \tan(\theta_i), \tag{3.13}$$

where  $\Delta z = z_0 - z_n$  is the displacement of layer n from the image plane. The next step is to compute the pixel index at the point h(m, n). The shift in pixel units can directly be derived from the shift in equation 3.13 given the pixel size  $\Delta s$ , yielding

$$\Delta k = \left[ \frac{\Delta z \tan(\theta_i)}{\Delta s} \right], \tag{3.14}$$

and the new index is  $k' = k + \Delta k$ . The brackets in the above equation denote the rounding operation. Finally, this information is stored in the propagation matrix with the assignment  $P_{mk'}^{(n)} = 1$ .

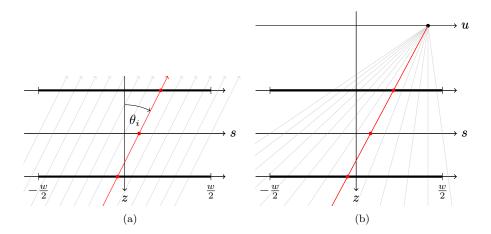


Figure 3.2: Computation of the ray-layer intersections from oblique (a) and perspective (b) projections. Two attenuation layers are drawn (top and bottom) with the virtual image plane in the center. Light rays intersect the layers at positions to be calculated.

#### Perspective Projection

For the perspective projection, it is assumed that the (u,v)-plane (or u-plane here) is at depth  $Z_u$ , with a distance  $z_0 - Z_u$  from the image plane. Again, let m = m(i,k) be the index that identifieds the ray (u(i),s(k)). Finding the coordinates of the ray (u,s) on a layer is similar to the re-parameterization in equation 2.4. Setting  $\gamma = \frac{z_0 - Z_u}{z_n - Z_u}$  for layer n, the formula for the intersection is

$$h(m,n) = \gamma(s(k) - u(i)) + u(i). \tag{3.15}$$

As before, the new pixel index  $k' = k + \Delta k$  is computed from the shift in the number of pixels

$$\Delta k = \left[ \frac{h(m, n) - s(k)}{\Delta s} \right], \tag{3.16}$$

and the assignment  $P_{mk'}^{(n)} = 1$  is made.

## Chapter 4

## Spectral Analysis

This chapter is intended to give an overview of the spectral properties and limitations specific to multiplicative light field displays. Spectral analysis is a crucial method for the quality assessment and it is the origin of a comprehensive understanding of 3D displays. A light field emitted by the display can be interpreted as a signal that is composed of sine waves with different amplitude, phase and frequency. Section 4.1 introduces the Fourier transform, an operation that decomposes such a signal into the frequencies that produce it. The spectral support, i.e. the range of frequencies the display is able to produce, is analyzed in section 4.3.

#### 4.1 Definitions

The Fourier transform  $\hat{f}$  of an integrable function  $f: \mathbb{R}^n \to \mathbb{C}$  is defined as

$$\hat{f}(\xi) = \mathcal{F}(f)(\xi) := \int_{\mathbb{D}_n} f(x)e^{-2\pi i x \cdot \xi} dx$$
(4.1)

for any  $\xi \in \mathbb{R}^n$ . According to the Fourier integral theorem, if both f and  $\hat{f}$  are absolutely integrable and f is continuous, then the inverse transform

$$f(x) = \mathcal{F}^{-1}(\hat{f})(x) := \int_{\mathbb{R}^n} \hat{f}(\xi) e^{2\pi i x \cdot \xi} d\xi$$
 (4.2)

is well defined. The domain of f is called the **spatial domain** and the domain of  $\hat{f}$  is referred to as the **frequency domain**. An important property of the Fourier transform is that a convolution in the spatial domain becomes a multiplication in the frequency domain, or in other words,

$$\widehat{(f * g)}(\xi) = \widehat{f}(\xi) \cdot \widehat{g}(\xi) \tag{4.3}$$

for integrable functions  $f,g:\mathbb{R}^n\to\mathbb{C}$ . On the other hand, a multiplication in the spatial domain becomes a convolution in the frequency domain after applying the Fourier transform, that is

$$\widehat{(f \cdot g)}(\xi) = (\hat{f} * \hat{g})(\xi). \tag{4.4}$$

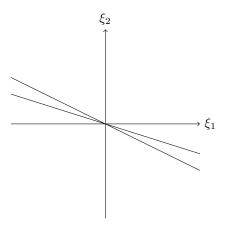


Figure 4.1:

#### 4.2 Spectral Support of Light Fields

#### 4.3 Spectral Support of Multiplicative Displays

Consider a scene with a bounded depth range  $Z_{\min} \leq Z \leq Z_{\max}$ . In section 2.3, it was shown that an object at a certain depth will be represented in the EPI as a line with a slope proportional to the depth.

Now, consider a single attenuation layer. The light field emitted by this layer has constant depth and thus, the lines in the EPI all have the same slope.

#### 4.4 The Fourier Slice Theorem

# Appendix A ap1

A.1 apsec1

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## <u>Erklärung</u>

gemäss Art. 28 Abs. 2 RSL 05

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