

433 Final Report

1. Abstract

Skin cancer remains one of the most critical global health concerns due to its potentially fatal consequences if left undetected. This project addresses the challenges of automated skin cancer detection using deep learning models trained on dermoscopic images and tabular metadata. The proposed system integrates image features extracted using ResNet50 with patient-specific metadata features selected through a multi-model feature selection process involving LightGBM, XGBoost, and CatBoost.

To tackle the severe class imbalance between benign and malignant cases, various strategies were employed, including data augmentation, weighted loss functions, and hyperparameter optimization. Multiple model configurations were tested, and the best-performing model achieved a recall of 54% for malignant cases with an overall accuracy of 94%. This result represents a significant improvement over previous models, emphasizing the effectiveness of multi-modal data integration and advanced model training techniques. The system's promising performance highlights its potential for real-world clinical applications in dermatological diagnostics.

2. Introduction

Skin cancer, particularly melanoma, is one of the most severe and potentially fatal forms of cancer, responsible for a significant number of cancer-related deaths worldwide. Its prevalence has been steadily increasing due to factors such as prolonged ultraviolet (UV) radiation exposure, harmful chemical exposure, and environmental changes driven by shifting lifestyles. Early and accurate detection of skin cancer is essential, as it dramatically improves survival rates and minimizes the severity of treatment. However, diagnosing skin cancer accurately remains challenging, as traditional methods rely on manual examination of dermoscopic images by dermatologists. This process is time-consuming, resource-intensive, and susceptible to human error, particularly in regions with limited access to specialized healthcare professionals. These limitations underscore the urgent need for automated diagnostic solutions to supplement dermatological assessments.

Advancements in artificial intelligence (AI) and machine learning (ML) have emerged as promising approaches

to addressing this issue. Convolutional Neural Networks (CNNs), a class of deep learning models, have achieved state-of-the-art performance in image analysis tasks by learning complex, non-linear patterns from large datasets. These models have demonstrated the ability to surpass human-level performance in specific medical applications, including skin lesion classification. Motivated by this potential, this project aims to develop a robust deep learning-based system capable of classifying skin lesions as benign or malignant. This effort seeks to enhance diagnostic accuracy, reduce the burden on healthcare systems, and improve patient outcomes globally by offering a scalable, automated diagnostic tool.

2.1. Challenges

Developing a reliable deep learning-based diagnostic system for skin cancer detection presents multiple challenges. One of the most critical issues is the severe class imbalance in the dataset, where malignant cases are significantly underrepresented compared to benign cases. This imbalance causes models to become biased toward the majority class, reducing sensitivity in detecting malignant lesions. False negatives in cancer detection pose a considerable risk, as they can lead to delayed treatment and worsen patient outcomes. Addressing this challenge requires thoughtful data preprocessing, augmentation strategies, and model design choices to ensure balanced learning.

Additionally, skin lesion images exhibit considerable variability due to differences in lesion size, shape, texture, and color, often influenced by patient-specific factors such as age, gender, and skin tone. This variability complicates the model's ability to generalize across diverse patient populations. Therefore, designing a model capable of capturing such heterogeneity is critical for ensuring clinical reliability and fairness in real-world applications.

Another major challenge arises from limited computational resources. The project relied on the free tier of Google Colab, which imposed constraints such as limited GPU access, capped memory, and restricted session durations. These limitations affected the scope of experimentation, reducing the dataset size, limiting the number of epochs, and restricting the ability to explore more complex model architectures or advanced training techniques. Overcoming these constraints required efficient resource man-

086	agement while maintaining model reliability and perfor-	
087	mance.	
088	2.2. Proposed Solution	
089	To address these challenges, this project employed a multi-	
090	faceted approach that combines data augmentation, feature	
091	reduction, multimodal learning, and hyperparameter opti-	
092	mization. Addressing the class imbalance, data augmenta-	
093	tion techniques were applied exclusively to the underrep-	
094	resented malignant class using PyTorch. Transformations	
095	such as random rotations, flips, brightness adjustments, and	
096	zoom operations were used to create diverse synthetic sam-	
097	ples, enhancing the model's ability to learn discriminative	
098	features for malignant lesions.	
099	In parallel, the tabular metadata associated with the der-	
100	moscopic images was refined by reducing the number of	
101	features from approximately 60 to 20 through a feature se-	
102	lection process. This reduction minimized noise and en-	
103	hanced the model's computational efficiency by retaining	
104	only the most relevant features. Models such as LightGBM,	
105	XGBoost, and CatBoost were employed to determine fea-	
106	ture importances, with the top-ranked features forming the	
107	final dataset used during training.	
108	To extract visual features, ResNet50 and EfficientNetB0	
109	architectures were employed due to their strong perfor-	
110	mance in medical imaging tasks. These models were trained	
111	from scratch to learn dataset-specific features instead of re-	
112	lying on pre-trained weights, as transfer learning was found	
113	to be less effective given the unique nature of the dataset.	
114	Additionally, a multimodal learning approach was im-	
115	plemented, combining extracted image features with the re-	
116	efined tabular metadata. This strategy enabled the model to	
117	leverage both visual and contextual information, enhancing	
118	its overall diagnostic performance. Key hyperparameters	
119	such as learning rate, batch size, and the number of epochs	
120	were carefully tuned through iterative experimentation to	
121	ensure model stability and optimal performance.	
122	2.3. Earlier Results and Model Evolution	
123	Initial experiments encountered considerable difficulties	
124	due to resource limitations and severe class imbalance.	
125	Early models trained on the full dataset suffered from sig-	
126	nificant overfitting, with near-perfect performance on the	
127	training set but zero sensitivity toward malignant cases in	
128	the testing phase. To address these issues, the dataset was	
129	reduced to 10,000 samples to ensure manageability, and ad-	
130	vanced data augmentation techniques were employed to im-	
131	prove minority class representation.	
132	Subsequent models demonstrated notable improve-	
133	ments, achieving a classification accuracy of 94% for be-	
134	nign cases. However, the sensitivity toward malignant	
135	cases remained low, highlighting the persistent challenge of	
136	handling class imbalance. Additional techniques, includ-	
	ing weighted loss functions and cross-validation, were in-	137
	troduced to mitigate these issues, ultimately enabling the	138
	model to achieve a recall of 54% for malignant cases in the	139
	final iteration—a significant improvement over earlier at-	140
	tempts.	141
	2.4. Related Works	142
	The application of deep learning in medical imaging has	143
	been extensively studied, yielding promising results in skin	144
	cancer detection. Yadav and Jadhav (2019) highlighted the	145
	potential of CNN-based architectures for disease diagno-	146
	sis, demonstrating superior performance in extracting and	147
	interpreting complex image features. Similarly, Dahou et	148
	al. (2023) achieved high diagnostic accuracy through trans-	149
	fer learning using architectures such as EfficientNet and	150
	ResNet, combined with novel optimization techniques.	151
	Recent advances also include the Derm-T2IM frame-	152
	work, which addressed dataset limitations by generating	153
	synthetic data, improving model robustness and reducing	154
	overfitting. While these studies have explored individual as-	155
	pects of deep learning in medical imaging, few works have	156
	effectively addressed the combined challenges of class im-	157
	balance, feature selection, and computational constraints.	158
	This project builds on these previous studies by integrat-	159
	ing data augmentation, multimodal learning, and model tun-	160
	ing into a cohesive framework tailored to the specific chal-	161
	lenges of skin cancer detection. The proposed system rep-	162
	resents a scalable and adaptive approach to automated skin	163
	cancer diagnosis, providing a valuable contribution to the	164
	growing body of research in AI-driven healthcare.	165
	3. Methodology	166
	The methodology employed in this project was structured	167
	to address the significant challenges of imbalanced data and	168
	computational constraints while ensuring the development	169
	of an effective deep learning-based diagnostic tool for skin	170
	cancer detection. This section provides a comprehensive	171
	explanation of the steps undertaken, from data preprocess-	172
	ing to model development and evaluation, highlighting the	173
	rationale behind each decision.	174
	3.1. Data Collection and Preprocessing	175
	The dataset for this project was sourced from a Kaggle chal-	176
	lenge, containing a severe imbalance between benign and	177
	malignant cases, with 400,666 benign and only 393 malig-	178
	nant samples. This imbalance presented a significant chal-	179
	lenge for training a model capable of accurately identifying	180
	malignant cases, as the model could easily overfit to the ma-	181
	jority class while neglecting the minority class. Addressing	182
	this issue required several preprocessing steps designed to	183
	balance the data distribution and enhance the model's abil-	184
	ity to learn meaningful features.	185
	Two primary training datasets were derived from the	186

original data to experiment with different strategies for handling class imbalance. The first dataset was created by undersampling the benign cases to achieve a training set of 8,000 benign and 315 malignant samples without data augmentation. The second dataset applied data augmentation techniques to increase the representation of malignant cases, resulting in a training set with 8,000 benign and 629 malignant samples. Augmentation included random rotations, flips, brightness adjustments, and zooming, generating diverse variations of malignant lesions while preserving their diagnostic characteristics.

The testing dataset, consistent across all experiments, contained 2,000 benign and 80 malignant samples. This separate test set ensured a fair evaluation of model performance and allowed for comparative analysis across experiments.

3.2. Feature Selection

A multi-model feature selection process was implemented using three state-of-the-art gradient boosting algorithms: LightGBM, XGBoost, and CatBoost. Each model was trained on the metadata, and feature importances were computed based on their contributions to the prediction task. The importance scores from all three models were averaged to mitigate biases from individual algorithms. The top 20 features with the highest average importance scores were selected, forming the final metadata feature set.

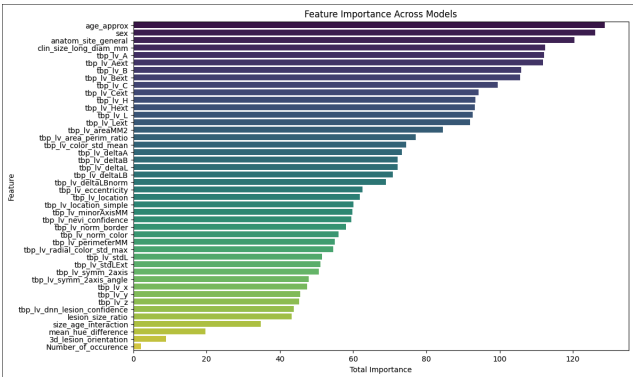


Figure 1. Feature importance across models

3.3. Model Selection and Design

Model selection was guided by the need for a scalable, accurate, and resource-efficient solution. Two deep learning architectures, ResNet50 and EfficientNetB0, were chosen based on their robust performance in medical image analysis tasks. Their feature extraction capabilities enabled precise classification despite limited computational resources.

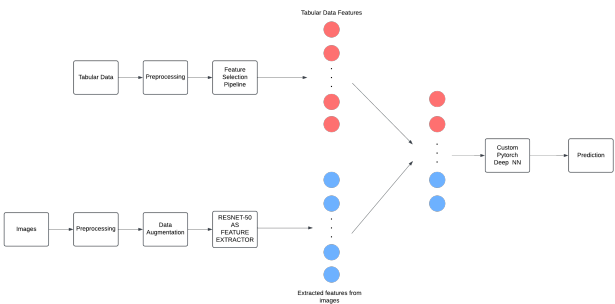


Figure 2. Full architecture

Three experimental setups were tested: 1. No data augmentation with a weighted loss function. 2. Data augmentation without a weighted loss function. 3. Both data augmentation and a weighted loss function.

The weighted loss function assigned higher penalties to misclassifying malignant cases, compensating for class imbalance. Each experimental setup employed 5-fold cross-validation, ensuring that models were trained and validated on different subsets of the data to improve generalizability.

Additionally, the models were trained from scratch rather than using pre-trained weights. This decision was influenced by the unique nature of dermoscopic images, which differ significantly from common datasets like ImageNet. Training from scratch allowed the models to learn domain-specific features tailored to the skin lesion dataset.

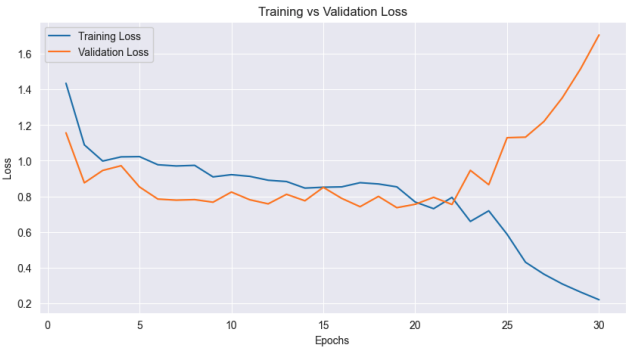


Figure 3. Training vs Validation Loss for Model 2 Iteration 2

The graph shows the training and validation loss trends for the model trained without data augmentation but with a weighted loss function. The training loss steadily decreased, indicating effective learning, while the validation loss stabilized around epoch 20, signaling the optimal stopping point to avoid overfitting. This configuration provided the best balance between learning and generalization, resulting in the most reliable model within the project's constraints.

244	3.4. Multimodal Data Integration	294
245	To enhance diagnostic accuracy, the project integrated	295
246	metadata from tabular data with image features extracted	296
247	using deep learning. Metadata features, such as age, lesion	297
248	location, and lesion dimensions, were reduced to the top 20	298
249	features through the feature selection process.	299
250	Simultaneously, a 2048-dimensional feature vector was	300
251	extracted from the final convolutional layer of ResNet50,	301
252	representing dermoscopic image features. The two feature	302
253	sets were concatenated into a unified vector, which served	303
254	as input to a fully connected neural network for the final	304
255	classification task. This multimodal integration allowed the	305
256	model to leverage both visual and contextual information,	306
257	improving its ability to detect malignant lesions.	307
258	3.5. Training and Optimization	308
259	Model training required balancing resource constraints with	309
260	the need for optimal performance. Hyperparameters such as	310
261	learning rate, batch size, and number of epochs were care-	311
262	fully tuned based on empirical testing and validation set per-	312
263	formance.	313
264	The final hyperparameter configuration for the best	
265	model (Model 2 Iteration 2) was as follows: Learning	
266	Rate: 0.00001, selected to allow gradual weight adjust-	
267	ments and prevent unstable updates caused by larger learn-	
268	ing rates. Batch Size: 128, chosen to stabilize gradient up-	
269	dates while maximizing GPU utilization. Epochs: 200, de-	
270	termined through early stopping-like observations from the	
271	training vs. validation loss graph, where performance gains	
272	plateaued beyond 200 epochs.	
273	Additionally, weighted loss functions were employed to	
274	assign greater importance to malignant cases during train-	
275	ing. Data augmentation and undersampling techniques fur-	
276	ther addressed class imbalance, reducing false negatives—a	
277	critical concern in cancer detection.	
278	Performance metrics such as precision, recall, F1-score,	
279	and ROC-AUC were monitored during training. Since ac-	
280	curacy alone would be misleading due to class imbalance,	
281	recall for malignant cases was prioritized, given its signifi-	
282	cance in reducing missed cancer diagnoses.	
283	3.6. Implementation and Reproducibility	
284	The project was implemented using PyTorch for deep learn-	
285	ing model development and scikit-learn for data prepro-	
286	cessing and performance evaluation. Matplotlib was used	
287	for generating visualizations of metrics and model perfor-	
288	mance.	
289	Reproducibility was ensured by setting a fixed random	
290	seed (42) and saving model weights after each training ses-	
291	sion. These measures provided consistent results across	
292	multiple runs and allowed future researchers to replicate the	
293	experiments reliably.	
	3.7. Improvement and New Approaches	294
	The project introduced several improvements over previous	295
	attempts. First, the multi-model feature selection process	296
	ensured a reliable and unbiased ranking of features, reduc-	297
	ing noise and improving performance. Additionally, an ex-	298
	tensive feature engineering process generated context-rich	299
	features such as lesion size ratios, age-size interaction, av-	300
	erage hue difference, and three-dimensional lesion orienta-	301
	tion.	302
	The adoption of a multimodal architecture was the most	303
	notable innovation, as it combined image-based and tabular	304
	features, providing a comprehensive understanding of each	305
	case. Compared to earlier models that used only image fea-	306
	tures, this integrated system significantly improved recall	307
	and generalization.	308
	Lastly, class imbalance was addressed through data aug-	309
	mentation, weighted loss functions, and undersampling.	310
	These strategies improved the model’s ability to detect ma-	311
	lignant cases while minimizing overfitting, resulting in a	312
	scalable and accurate diagnostic tool.	313
	4. Results	314
	This section provides a comprehensive analysis of the ex-	315
	periments conducted, focusing on the performance of var-	316
	ious iterations of the trained models. Key results, includ-	317
	ing performance metrics, training and validation trends, and	318
	confusion matrices, are presented to evaluate and compare	319
	the models. The findings highlight the best-performing	320
	model and analyze its performance on both the training and	321
	testing datasets, while also comparing these outcomes to	322
	prior attempts.	323
	4.1. Model Performance Across Iterations	324
	After training and testing each model across eight itera-	325
	tions, the results were summarized in Table 1. The models	326
	varied in terms of learning rate (LR), batch size (BS), and	327
	number of epochs, allowing for a systematic evaluation of	328
	the impact of these hyperparameters on model performance.	329
	Model 1 iterations employed a higher learning rate of 0.001,	330
	with batch sizes of either 32 or 64, and epochs ranging from	331
	25 to 100. These configurations struggled with overfitting	332
	and failed to generalize effectively, achieving recall values	333
	between 0.25 and 0.33 when detecting malignant cases.	334
	Model 2 demonstrated significantly improved recall per-	335
	formance across iterations, particularly in Iteration 2, which	336
	used a learning rate of 0.00001, a batch size of 128, and 200	337
	epochs. This setup achieved a test recall of 0.54, the highest	338
	among all iterations. Model 3 iterations also reached a re-	339
	call of 0.54 in Iteration 2; however, further analysis showed	340
	that Model 2 Iteration 2 provided superior generalization	341
	due to more stable validation performance, as described be-	342
	low.	343

Model	LR	BS	Epoch	Test Recall
Model 1 Itr.1	0.001	64	100	0.32
Model 1 Itr.2	0.001	32	50	0.25
Model 1 Itr.3	0.001	64	25	0.33
Model 2 Itr.1	0.00001	128	100	0.46
Model 2 Itr.2	0.00001	128	200	0.54
Model 2 Itr.3	0.00001	64	200	0.24
Model 3 Itr.1	0.00001	64	200	0.25
Model 3 Itr.2	0.00001	128	200	0.54

Table 1. Model iterations with hyperparameters and test recall results.

4.2. Model Selection and Evaluation of Model 2 Iteration 2

Among all iterations, Model 2 Iteration 2 emerged as the best-performing configuration due to its high recall of 0.54 for the Positive class (malignant cases). This setup used a learning rate of 0.00001, a batch size of 128, and 200 epochs, enabling the model to learn effectively without overfitting. The training vs. validation loss graph (Figure 4) illustrates the stability of the model, with validation loss converging without significant divergence from the training loss, even at higher epochs.



Figure 4. Training vs. validation loss for Model 2 Iteration 2.

The confusion matrix for Model 2 Iteration 2 during testing (Figure 5) highlights the model’s classification performance. The model correctly identified 1585 benign cases (True Negatives) and 34 malignant cases (True Positives). However, 65 benign cases were misclassified as malignant (False Positives), and 29 malignant cases were missed (False Negatives). Despite these errors, the model achieved a recall of 54% for malignant cases, reflecting its effectiveness in identifying critical cases, a key priority for skin cancer diagnostics.

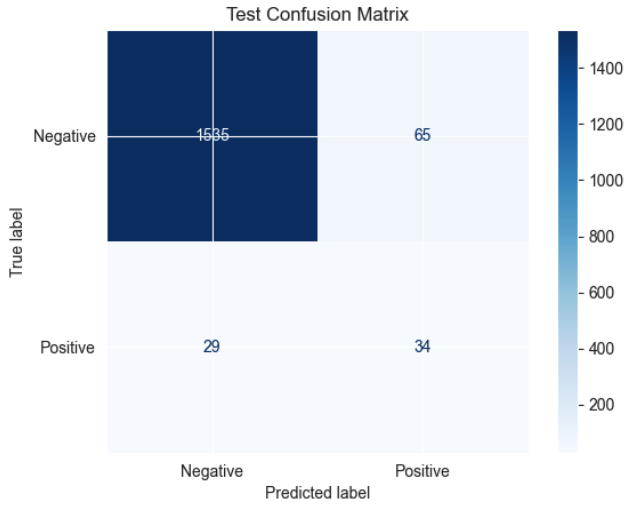


Figure 5. Confusion matrix for Model 2 Iteration 2 during testing.

4.3. Classification Metrics

Table 2 summarizes the classification metrics for Model 2 Iteration 2 on the test dataset. The Negative class (benign cases) exhibited high precision (0.98) and recall (0.96), contributing to an overall accuracy of 94%. The Positive class (malignant cases) achieved a precision of 0.34 and a recall of 0.54, resulting in an F1-score of 0.42. The macro-average recall was 0.75, indicating reasonable performance across both classes despite the severe class imbalance.

Class	Precision	Recall	F1-Score	Support
Negative	0.98	0.96	0.97	1600
Positive	0.34	0.54	0.42	63
Accuracy	0.94			1663
Macro Avg	0.66	0.75	0.70	1663
Weighted Avg	0.96	0.94	0.95	1663

Table 2. Classification metrics for Model 2 Iteration 2 during testing.

4.4. Discussion and Comparison to Previous Results

The results achieved in this study demonstrate significant improvements compared to previous models. The recall for malignant cases increased from under 40% in earlier attempts to 54%, highlighting the impact of weighted loss functions and multimodal data integration. This improvement reduced the number of false negatives—a crucial consideration given the life-threatening consequences of missing malignant cases.

The F1-score for the Positive class improved substantially as well, reflecting a better balance between precision and recall. This trade-off was deliberately accepted, as improving recall took precedence over precision in this context. While precision (0.34) for malignant cases remained

388 moderate, it was considered an acceptable trade-off, ensur-
389 ing the model was more sensitive to true malignant cases,
390 which are more critical in medical diagnostics.

391 Additionally, the stability of validation loss throughout
392 the training process reflected better generalization and a sig-
393 nificant reduction in overfitting compared to earlier models.
394 This improvement was driven by optimized hyperparame-
395 ter selection, effective feature engineering, and multimodal
396 integration.

397 **4.5. Limitations and Future Directions**

398 Despite the improvements, some limitations remain. The
399 moderate precision for malignant cases could lead to a
400 higher rate of False Positives, potentially causing unneces-
401 sary follow-up procedures in a clinical setting. Future work
402 could explore ensemble models and synthetic data genera-
403 tion to address class imbalance further. Additionally, im-
404 proving multimodal feature integration by incorporating at-
405 tention mechanisms could enhance the system’s ability to
406 learn feature relationships more effectively.

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