Crustal Deformation Modeling Tutorial PyLith Version 3

Brad Aagaard Matthew Knepley Charles Williams



June 27, 2017

PyLith v3.0

- Multiphysics through pointwise integration kernels
- Higher order spatial and temporal discretizations
- Adaptive time stepping via PETSc TS
- Improved fault formulation for spontaneous rupture (v3.1)



Solve governing equation in integrated sense:

$$\int_{\Omega} \psi_{trial} \cdot PDE \, d\Omega = 0,\tag{1}$$

by minimizing the error with respect to the unknown coefficients.

This leads to equations of the form:

$$\int_{\Omega} \psi_{trial} \cdot f_0(x,t) + \nabla \psi_{trial} \cdot f_1(x,t) \, d\Omega = 0. \tag{2}$$



Governing Equations

We want to solve equations in which the weak form can be expressed as

$$F(t, s, \dot{s}) = G(t, s) \tag{3}$$

$$s(t_0) = s_0 \tag{4}$$

where F and G are vector functions, t is time, and s is the solution vector.

Using the finite-element method and divergence theorem, we cast the weak form into

$$\int_{\Omega} \vec{\psi}_{trial} \cdot \vec{f}_{0}(t, s, \dot{s}) + \nabla \vec{\psi}_{trial} : \boldsymbol{f}_{1}(t, s, \dot{s}) d\Omega =$$

$$\int_{\Omega} \vec{\psi}_{trial} \cdot \vec{g}_{0}(t, s) + \nabla \vec{\psi}_{trial} : \boldsymbol{g}_{1}(t, s) d\Omega, \quad (5)$$

where $\vec{f_0}$ and $\vec{g_0}$ are vectors, and f_1 and g_1 are tensors.



Explicit Time Stepping

Explicit time stepping with the PETSc TS requires $F(t, s, \dot{s}) = \dot{s}$.

Normally $F(t, s, \dot{s})$ contains the inertial term $(\rho \ddot{u})$.

Therefore, when using explicit time stepping we transform our equation into the form:

$$F^*(t, s, \dot{s}) = \dot{s} = G^*(t, s)$$
 (6)

$$\dot{s} = M^{-1}G(t,s). \tag{7}$$



Solving the Equations

Explicit time stepping requires a subset of the terms used in implicit time stepping.

- PETSc TS object provides time-stepping and solver implementations
 - Application code provides functions for computing RHS and LHS residuals and Jacobians
- Explicit time stepping
 - Compute RHS residual, G(t,s)
 - Compute lumped inverse of LHS, M^{-1}
 - No need to compute LHS residual, because $F(t, s, \dot{s}) = \dot{s}$
- Implicit time stepping (Krylov solvers)
 - Compute RHS residual, G(t,s)

 - Compute LHS residual, $F(t, s, \dot{s})$ Compute RHS Jacobian, $J_G = \frac{\partial G}{\partial s}$
 - Compute LHS Jacobian, $J_F = \frac{\partial \vec{F}}{\partial z} + t_{shift} \frac{\partial F}{\partial z}$



Example: Elasticity

$$\rho \frac{\partial^2 \vec{u}}{\partial t^2} = \vec{f}(\vec{x}, t) + \nabla \cdot \boldsymbol{\sigma}(\vec{u}) \text{ in } \Omega, \tag{8}$$

$$\sigma \cdot \vec{n} = \vec{\tau}(\vec{x}, t) \text{ on } \Omega_{\tau},$$
 (9)

$$ec{u} = ec{u}_0(ec{x},t) ext{ on } \Omega_u,$$
 (10)

Implicit Time Stepping without Inertia

Displacement \vec{u} is the unknown, $\vec{s} = \vec{u}$.

$$\underbrace{0}_{\vec{f}_0^u} = \int_{\Omega} \vec{\psi}_{trial}^u \cdot \underbrace{\vec{f}(\vec{x}, t)}_{\vec{g}_0^u} + \nabla \vec{\psi}_{trial}^u : \underbrace{-\boldsymbol{\sigma}(\vec{u})}_{\boldsymbol{g}_1^u} d\Omega + \int_{\Omega_{\tau}} \vec{\psi}_{trial}^u \cdot \underbrace{\vec{\tau}(\vec{x}, t)}_{\vec{g}_0^u} d\Omega_{\tau} \tag{11}$$

Different constitutive models are encapsulated in alternative kernels for $\sigma(\vec{u})$.



Example: Elasticity (continued)

Explicit Time Stepping with Inertia

Form a first order equation using displacement \vec{u} and velocity \vec{v} as unknowns,

$$\vec{s}^{T} = \begin{pmatrix} \vec{u} & \vec{v} \end{pmatrix}^{T}$$

$$\int_{\Omega} \vec{\psi}_{trial}^{u} \cdot \underbrace{\frac{\partial \vec{u}}{\partial t}}_{i} d\Omega = \int_{\Omega} \vec{\psi}_{trial}^{u} \cdot \underbrace{\vec{v}}_{\vec{g}_{0}^{u}} d\Omega, \tag{12}$$

$$\int_{\Omega} \vec{\psi}_{trial}^{v} \cdot \underbrace{\frac{\partial \vec{v}}{\partial t}}_{v} d\Omega = \frac{1}{\vec{m}} \left(\int_{\Omega} \vec{\psi}_{trial}^{v} \cdot \underbrace{\vec{f}(\vec{x}, t)}_{\vec{g}_{0}^{v}} + \nabla \vec{\psi}_{trial}^{v} : \underbrace{-\boldsymbol{\sigma}(\vec{u})}_{\boldsymbol{g}_{1}^{v}} d\Omega + \int_{\Omega_{\tau}} \vec{\psi}_{trial}^{v} \cdot \underbrace{\vec{\tau}(\vec{x}, t)}_{\vec{g}_{0}^{v}} d\Omega_{\tau} \right), \tag{13}$$

$$\vec{m} = \int_{\Omega} \vec{\psi}_{trial}^{v} \cdot \underbrace{\rho}_{J_{f0}^{vv}} \vec{\psi}_{basis}^{v} d\Omega \tag{14}$$



Example: Elasticity (continued)

Implementing the governing equations involves a small set of simple kernels.

	Implicit	Explicit
$ec{v}$	_	$ec{g}_0^v$
$ec{f}(ec{x},t) \ -oldsymbol{\sigma}(ec{u}) \ ec{ au}(ec{x},t)$	$egin{aligned} ec{g}_0^u \ oldsymbol{g}_1^u \end{aligned}$	$ec{g}^v_0$
$-oldsymbol{\sigma}(ec{u})$		\boldsymbol{g}_1^v
$ec{ au}(ec{x},t)$	$ec{ar{f}_0^u} \ ec{f}_0^u$	$ec{g}_0^v$
$\vec{0}$	$ar{f_0^u}$	_
ho	_	$J^{uv}_{f_0}$

We also have simple kernels for the Jacobians needed in implicit time stepping.



Example: Elasticity Stress Kernels for Residual

Volumetric Stress

```
for (i=0; i < _dim; ++i) {
    trace += disp_x[i] - initialstrain[i*_dim+i];
    meanistress += initialstress[i*_dim+i];
}
meanistress /= (PylithReal) _dim;
for (i = 0; i < _dim; ++i) {
    stress[i*_dim+i] += lambda * trace + meanistress;
}</pre>
```

Deviatoric Stress



Example: Poroelasticity Neglecting Inertia

We assume a compressible fluid completely saturates a porous solid undergoing infinitesimal strain.

Elasticity equilibrium equation neglecting inertia:

$$0 = \vec{f}(\vec{x}, t) + \nabla \cdot \boldsymbol{\sigma}(\vec{u}, p_f) \text{ in } \Omega, \quad \boldsymbol{\sigma} \cdot \vec{n} = \vec{\tau}(\vec{x}, t) \text{ on } \Omega_{\tau}, \vec{u} = \vec{u}_0(\vec{x}, t) \text{ on } \Omega_u, \tag{15}$$

Mass balance of the fluid:

$$\frac{\partial \zeta(\vec{u}, p_f)}{\partial t} = \gamma(\vec{x}, t) - \nabla \cdot \vec{q}(p_f) \text{ in } \Omega, \quad \vec{q} \cdot \vec{n} = q_0(\vec{x}, t) \text{ on } \Omega_q, p_f = p_0(\vec{x}, t) \text{ on } \Omega_p, \quad (16)$$

Darcy's law:

$$\vec{q}(p_f) = -\kappa(\nabla p_f - \vec{f}_f), \quad \kappa = \frac{k}{\eta_f}$$
 (17)

Constitutive behavior of the fluid:

$$\zeta(\vec{u}, p_f) = \alpha(\nabla \cdot \vec{u}) + \frac{p_f}{M}, \quad \frac{1}{M} = \frac{\alpha - \phi}{K_c} + \frac{\phi}{K_f}, \tag{18}$$

Constitutive behavior of the solid (linear elasticity):

$$\sigma(\vec{u}, p_f) = C : \epsilon - \alpha p_f I$$
 (19)



Example: Poroelasticity Neglecting Inertia

Consider displacement \vec{u} and fluid pressure p_f as unknowns, $\vec{s}^T = \begin{pmatrix} \vec{u} & p_f \end{pmatrix}^T$

$$\underbrace{0}_{\vec{f}_{0}^{u}} = \int_{\Omega} \vec{\psi}_{trial}^{u} \cdot \underbrace{\vec{f}(\vec{x}, t)}_{\vec{g}_{0}^{u}} + \nabla \vec{\psi}_{trial}^{u} : \underbrace{-\boldsymbol{\sigma}(\vec{u}, p_{f})}_{\boldsymbol{g}_{1}^{u}} d\Omega + \int_{\Omega_{\tau}} \vec{\psi}_{trial}^{u} \cdot \underbrace{\vec{\tau}(\vec{x}, t)}_{\vec{g}_{0}^{u}} d\Omega_{\tau},$$
(20)

$$\int_{\Omega} \psi_{trial}^{p} \underbrace{\frac{\partial \zeta(\vec{u}, p_{f})}{\partial t}}_{f_{0}^{p}} d\Omega = \int_{\Omega} \psi_{trial}^{p} \underbrace{\gamma(\vec{x}, t)}_{g_{0}^{p}} + \nabla \psi_{trial}^{p} \cdot \underbrace{\vec{q}(p_{f})}_{f_{1}^{p}} d\Omega + \int_{\Omega_{q}} \psi_{trial}^{p} \underbrace{(-q_{0}(\vec{x}, t))}_{g_{0}^{p}} d\Omega_{q}.$$
(21)

Poroelasticity involves many of the same kernels as elasticity plus a few additional ones.



Finite-Element Discretization

Specify discretizations for solution fields and auxiliary fields

- Solution Fields
 Specify basis functions and quadrature for each field in solution.
- Auxiliary Fields
 - Fields associated with parameters and state variables for constitutive models & boundary conditions.
 - Populated from spatial databases.
 - Specify basis functions for each subfield in the auxiliary fields.
- PETSc DMPlex infrastructure unpacks/packs information to/from solution and auxiliary fields and calling finite-element kernels.



Summary of Multiphysics Implementation

We decouple the element definition from the fully-coupled equation, using pointwise kernels that look like the PDE.

- Flexibility The cell traversal, handled by the library, accommodates arbitrary cell shapes. The problem can be posed in any spatial dimension with an arbitrary number of physical fields.
- Extensibility The library developer needs to maintain only a single method, easing language transitions (CUDA, OpenCL). A new discretization scheme could be enabled in a single place in the code.
 - Efficiency Only a single routine needs to be optimized. The application scientist is no longer responsible for proper vectorization, tiling, and other traversal optimization.

