



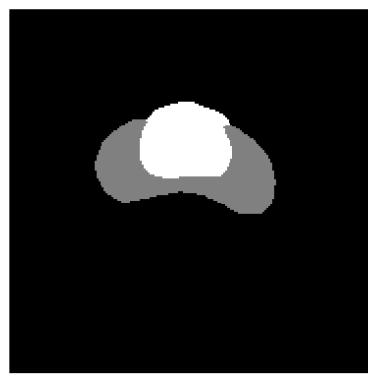
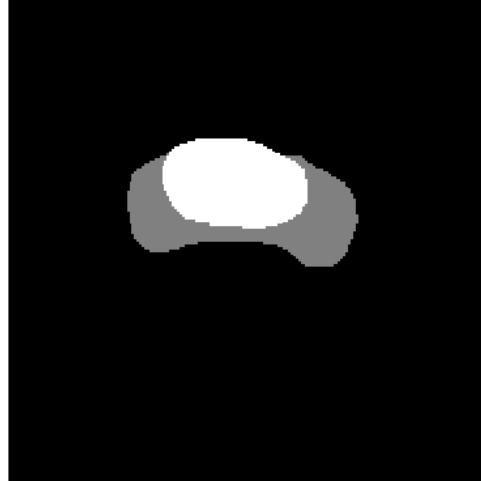
MAKING AI MAKE SENSE: CONCEPT-BASED PATHOLOGY DIAGNOSIS AND UNCERTAINTY-AWARE MRI

Asst. Prof. Christian Baumgartner

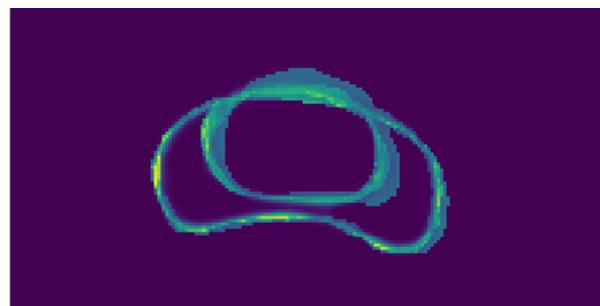
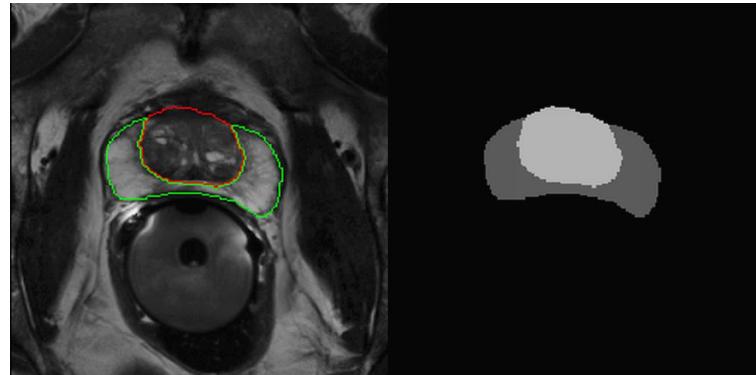
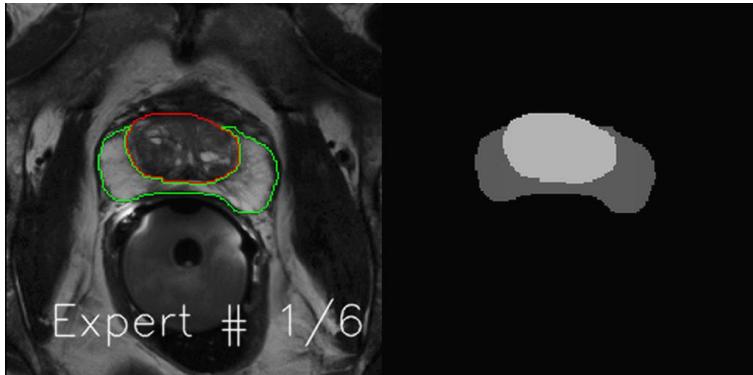
The background image is a wide-angle aerial photograph of the city of Lucerne, Switzerland. It captures the historic Old Town in the foreground, characterized by its dense cluster of buildings with red-tiled roofs and traditional architecture. A prominent feature is the Chapel Bridge (Kapellbrücke) spanning the Reuss River. To the left, the lake Lucerne (Vierwaldstättersee) is visible, with the town of Weggental across it. In the distance, the towering peaks of the Swiss Alps rise against a clear blue sky.

Lucerne Medical AI Group

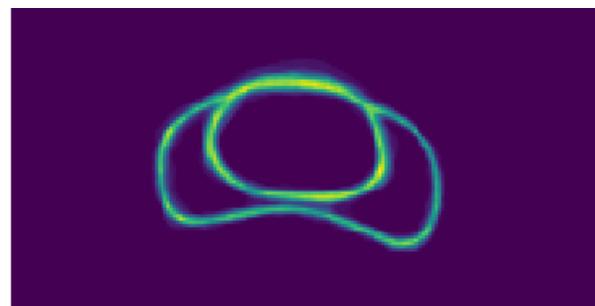
MEDICAL IMAGING IS FULL OF UNCERTAINTIES



RESEARCH FOCUS: ESTIMATING UNCERTAINTIES



Annotator variance



Predicted variance

RESEARCH GAPS

- 1) Usefulness of uncertainty of regarded as “self-evident”
→ *Uncertainty is only useful if influences some **downstream** clinical task*
- 2) Clinical decisions of rely on a cascade of clinical steps: how can we propagate uncertainty?



- 3) Could we use uncertainty to do something useful?
→ Personalise image acquisitions



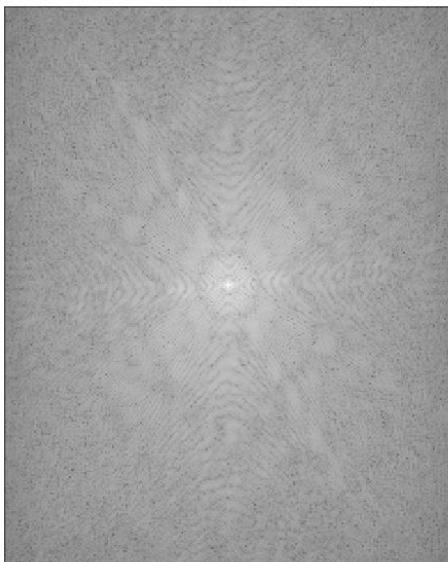
FAST UNCERTAINTY-GUIDED MR ACQUISITION



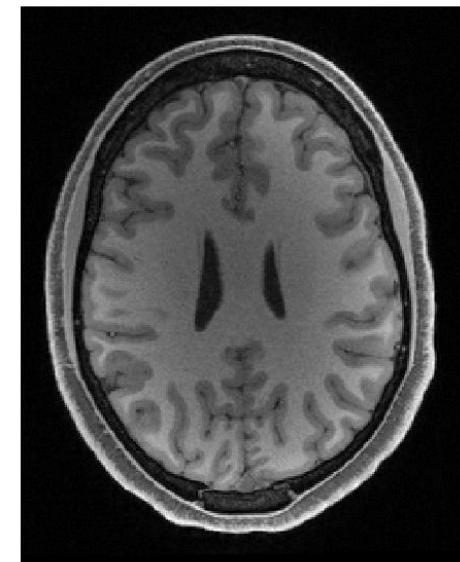
Paul Fischer
PhD Student/
Post-doc Uni Basel

QUICK PRIMER ON MRI RECONSTRUCTION

Measurement data (k-space)

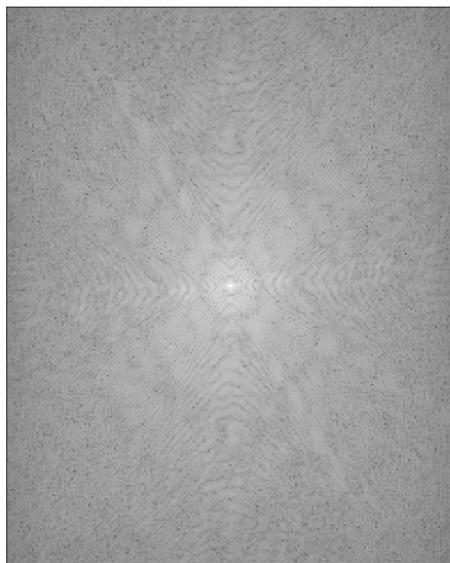


Image

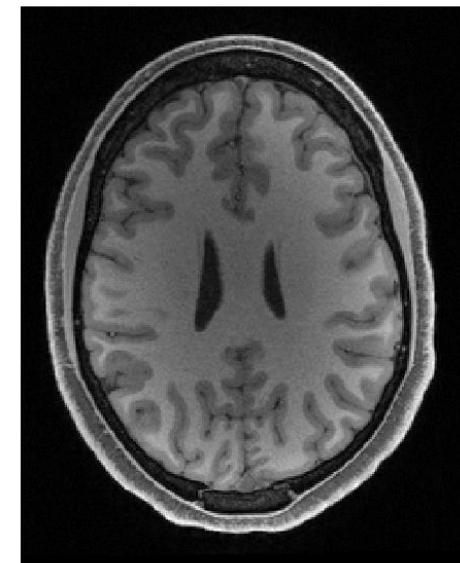


QUICK PRIMER ON MRI RECONSTRUCTION

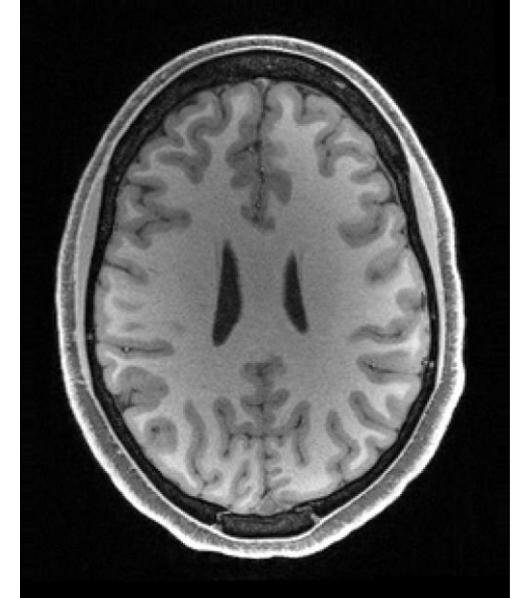
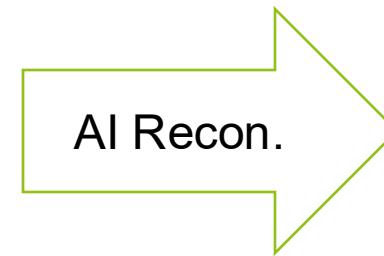
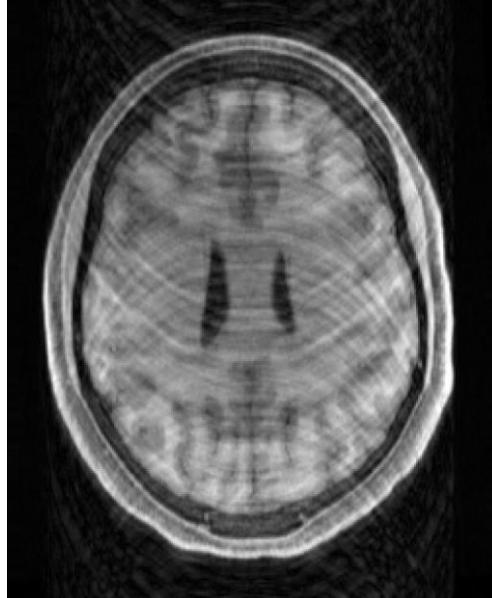
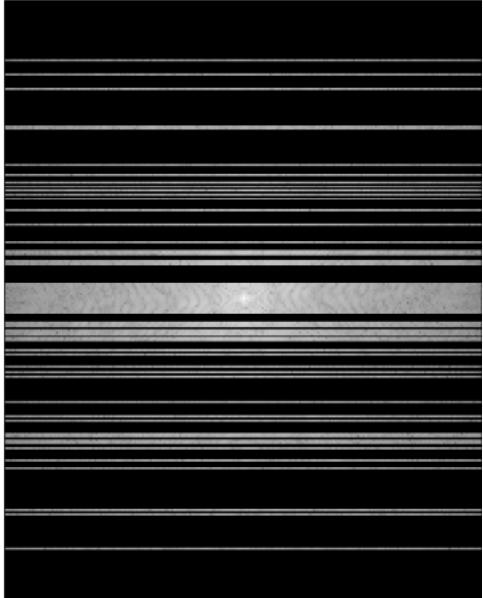
Measurement data (k-space)



Image



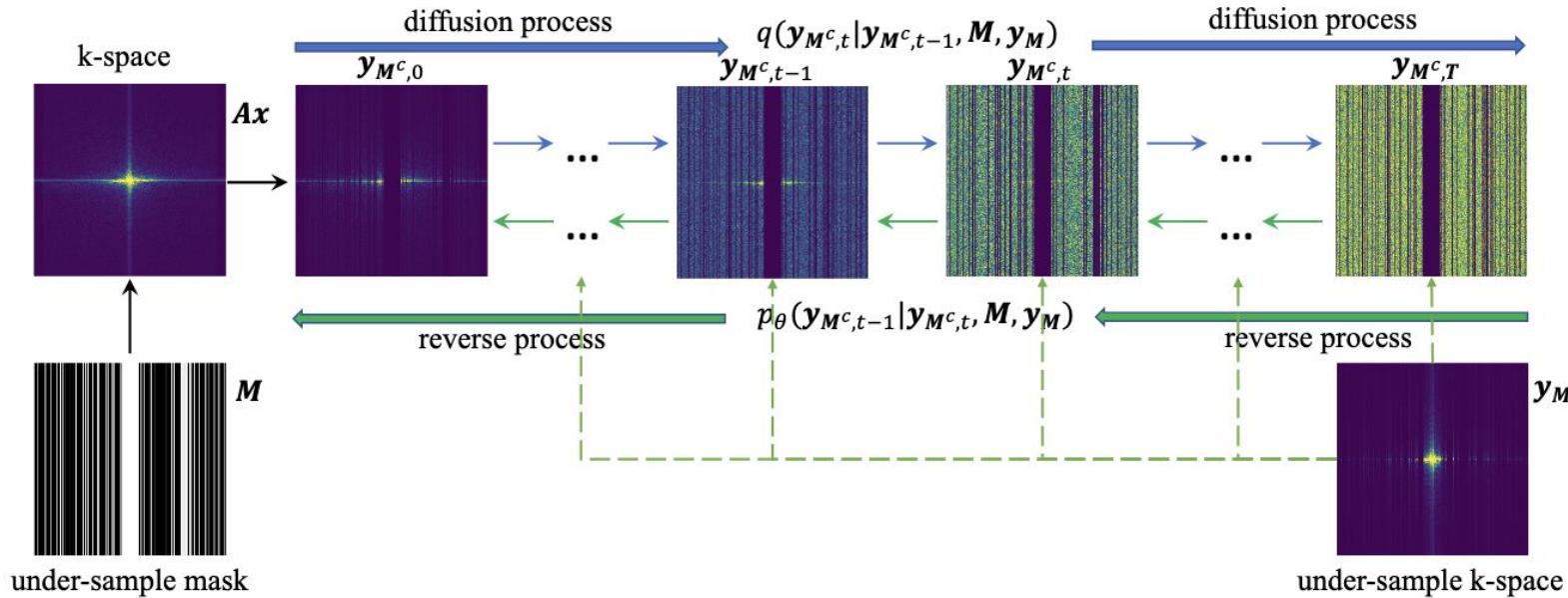
IMAGES CAN BE RECONSTRUCTED USING AI



Infinitely many solutions! Some more likely than others.

FIRST CONTRIBUTION: PROBABILISTIC MR RECONSTRUCTION

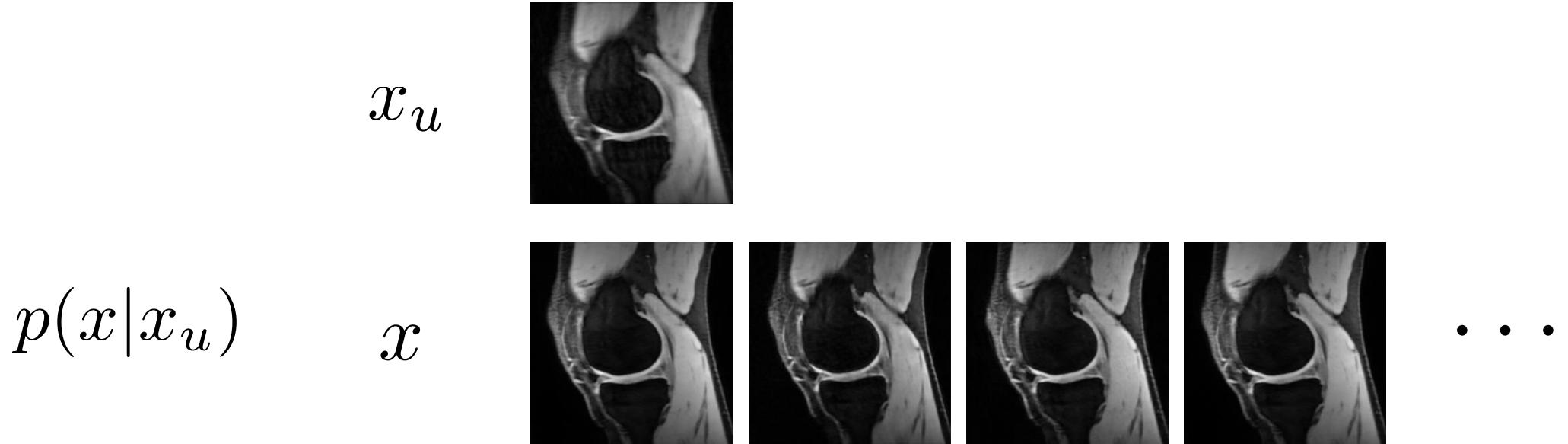
State-of-the-art: MR Reconstruction based on Diffusion Models



Xie, Yutong, and Quanzheng Li. "Measurement-conditioned denoising diffusion probabilistic model for under-sampled medical image reconstruction." *International Conference on Medical Image Computing and Computer-Assisted Intervention*. Cham: Springer Nature Switzerland, 2022.

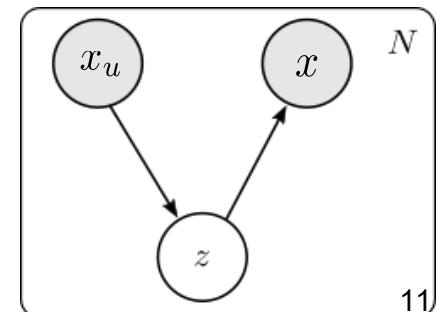
Best reconstructions, but **very slow inference** (~10 seconds per slice)

OUR APPROACH IS BASED ON CONDITIONAL VAES



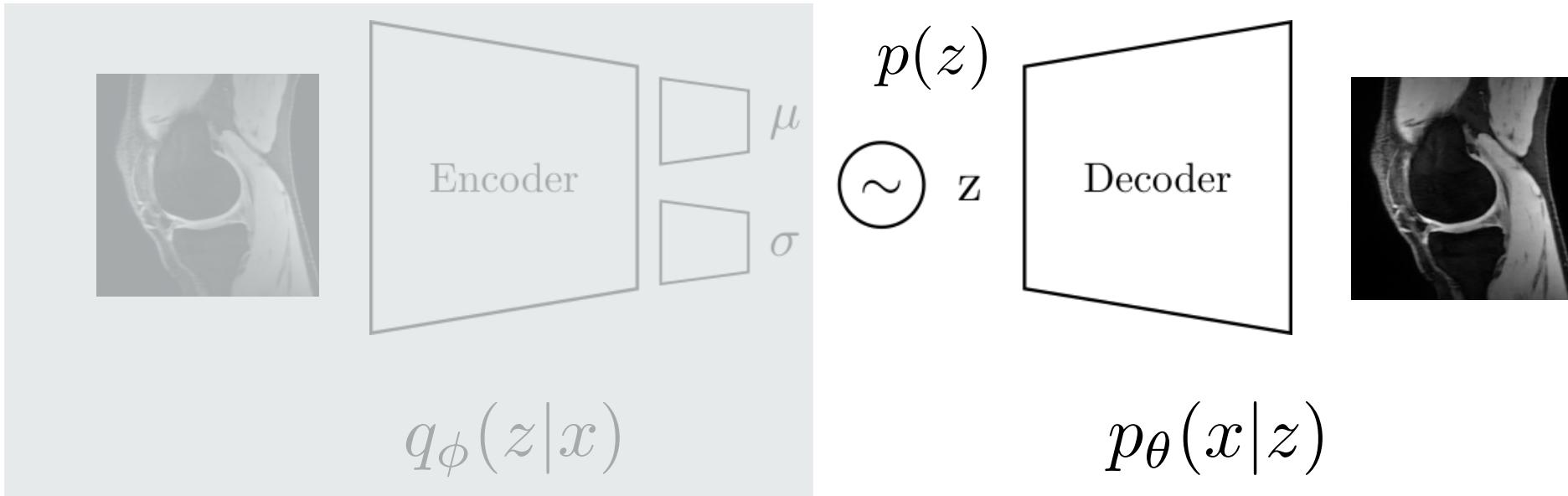
Assumption of cVAE: low-dimensional z explains all the variation

$$p(x|x_u) = \int p(x|z)p(z|x_u)dz$$



VARIATIONAL AUTOENCODERS: A BRIEF INTRO

$$\ln p(x) \geq \mathbb{E}_{q_\phi(z|x)} [\ln p_\theta(x|z)] - \text{KL} [p(z)||q_\phi(z|x)]$$



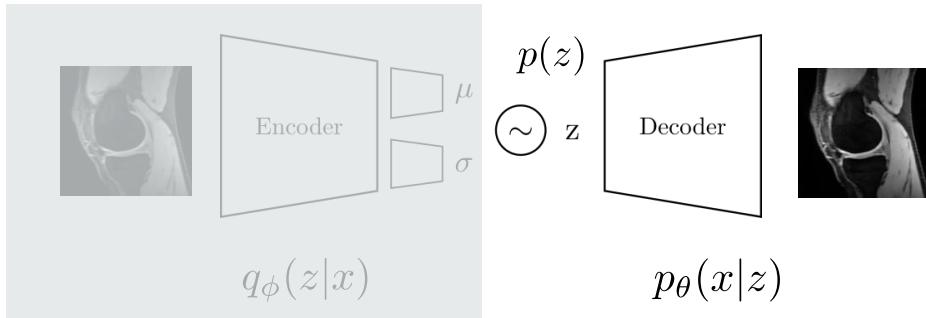
After training, discard posterior

CONDITIONAL VARIATIONAL AUTOENCODERS

VAE

$$p(s) = \int p(s|z)p(z)dz$$

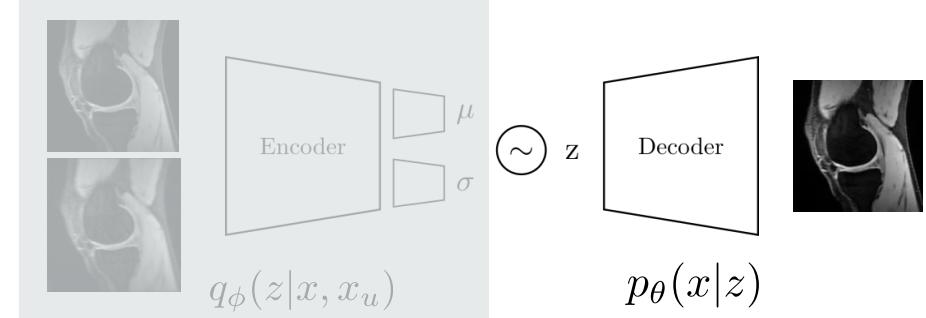
$$\ln p(x) \geq \mathbb{E}_{q_\phi(z|x)} [\ln p_\theta(x|z)] - \text{KL} [p(z)||q_\phi(z|x)]$$



cVAE

$$p(x|x_u) = \int p(x|z)p(z|x_u)dz$$

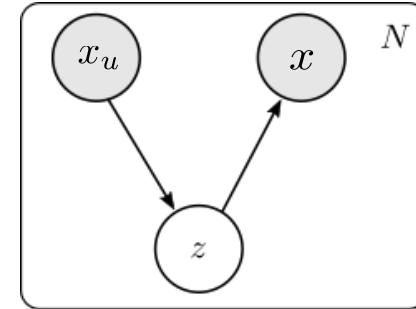
$$\ln p(x|x_u) \geq \mathbb{E}_{q_\phi(z|x,x_u)} [\ln p_\theta(x|z)] - \text{KL} [p(z|x_u)||q_\phi(z|x,x_u)]$$



FROM NORMAL CVAE TO HIERARCHICAL CVAE

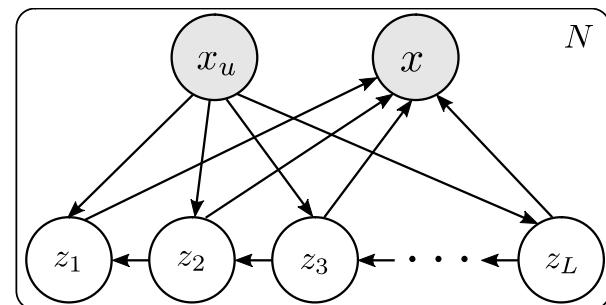
One level cVAE

$$p(x|x_u) = \int p(x|z)p(z|x_u)dz$$

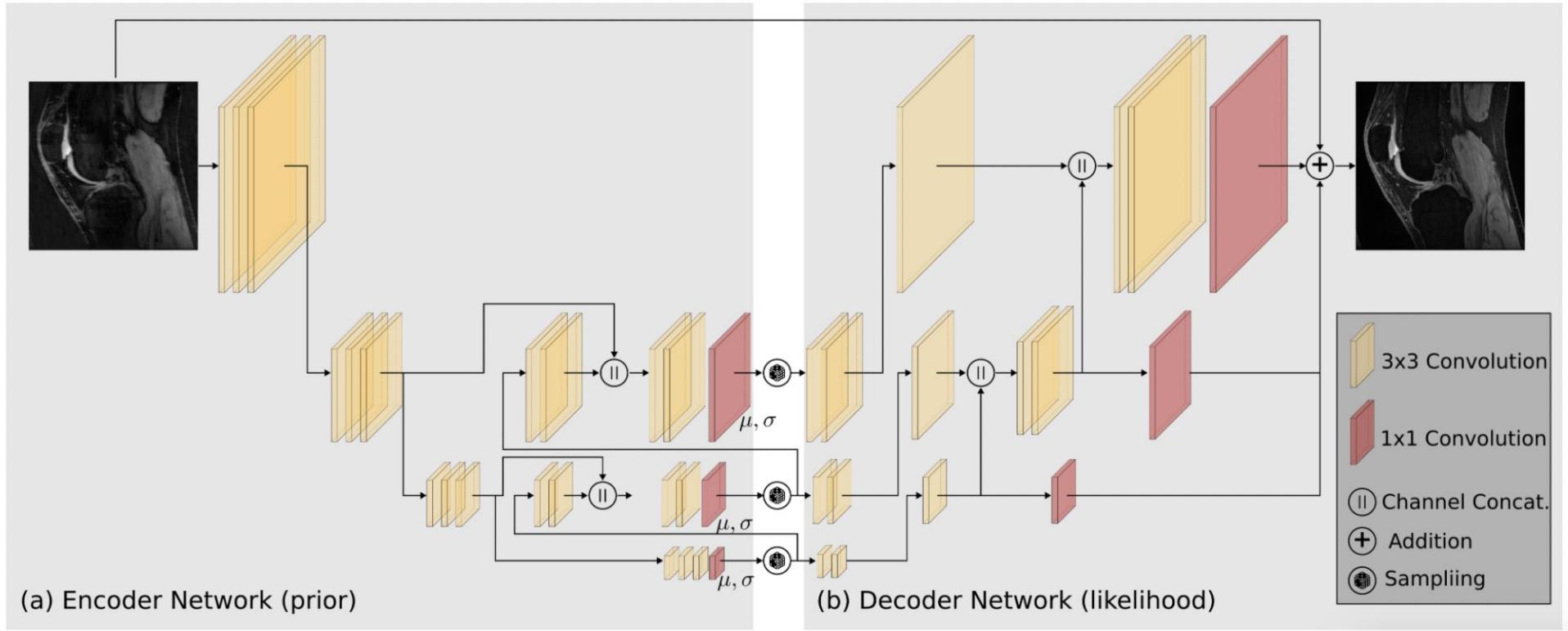


Hierarchical cVAE

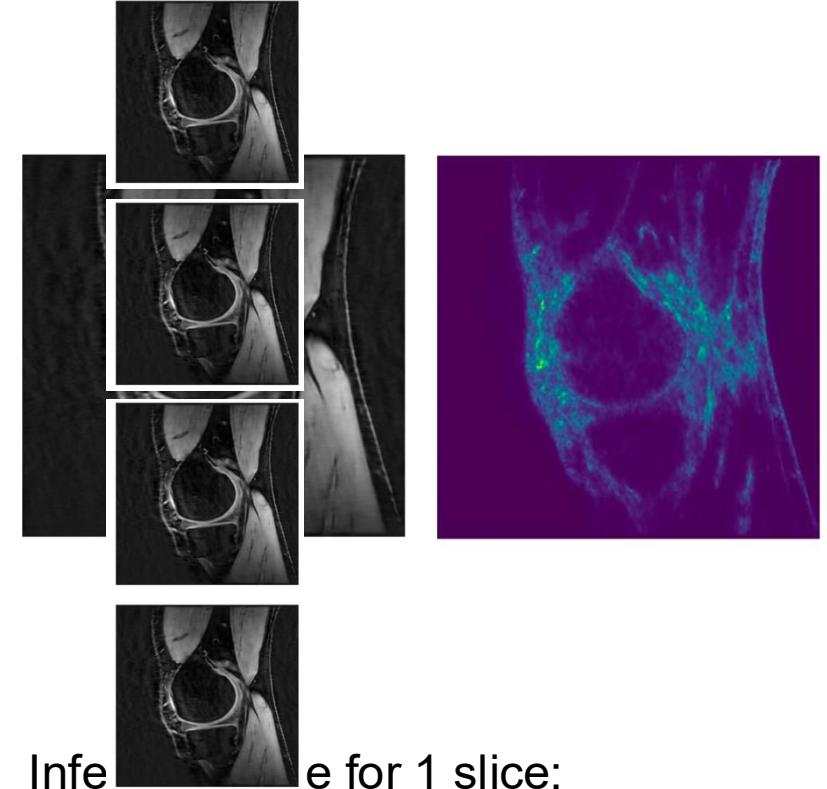
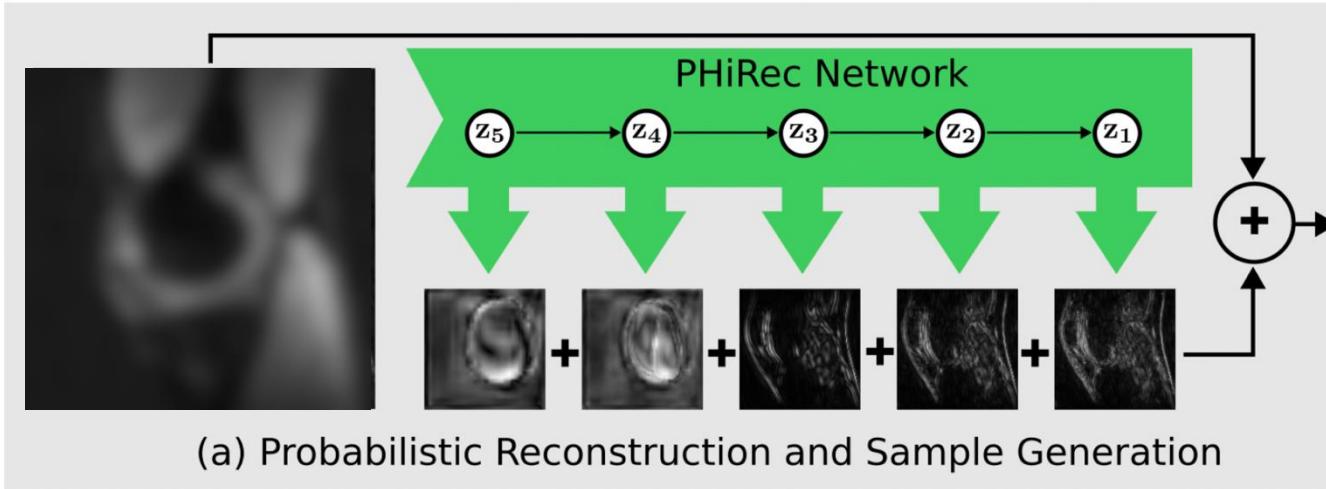
$$p(x|x_u) = \int p(x|z_1, \dots, z_L)p(z_1|z_2, x_u) \cdots p(z_{L-1}|z_L, x_u)p(z_L|x_u)dz_1 \cdots dz_L$$



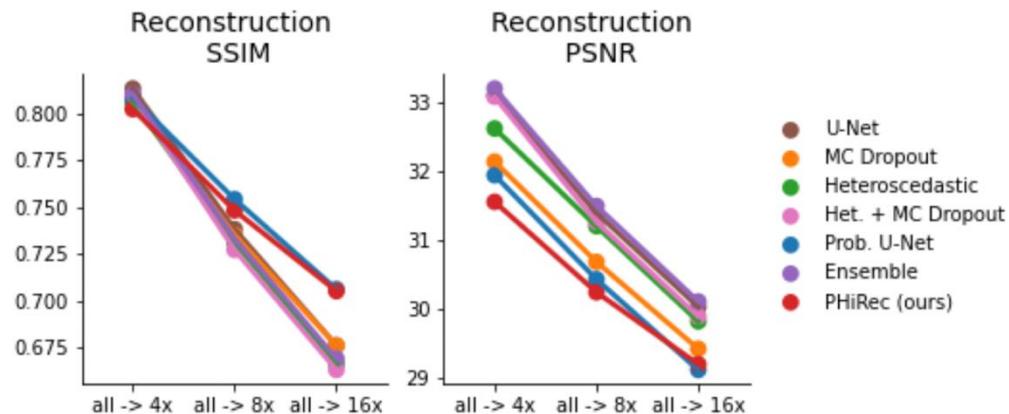
PROBABILISTIC HIERARCHICAL RECONSTRUCTION (PHIREC)



PHIREC FOR ACCELERATED MR IMAGING AND UNCERTAINTY PROPAGATION

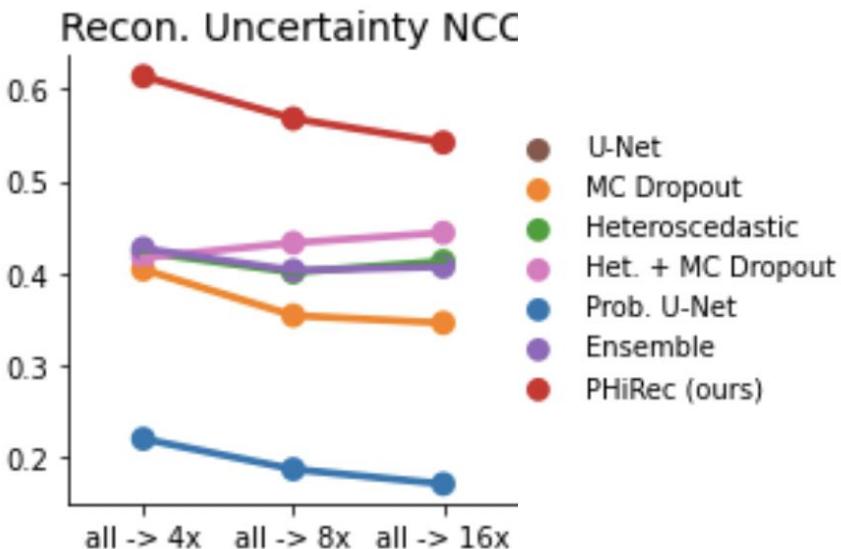
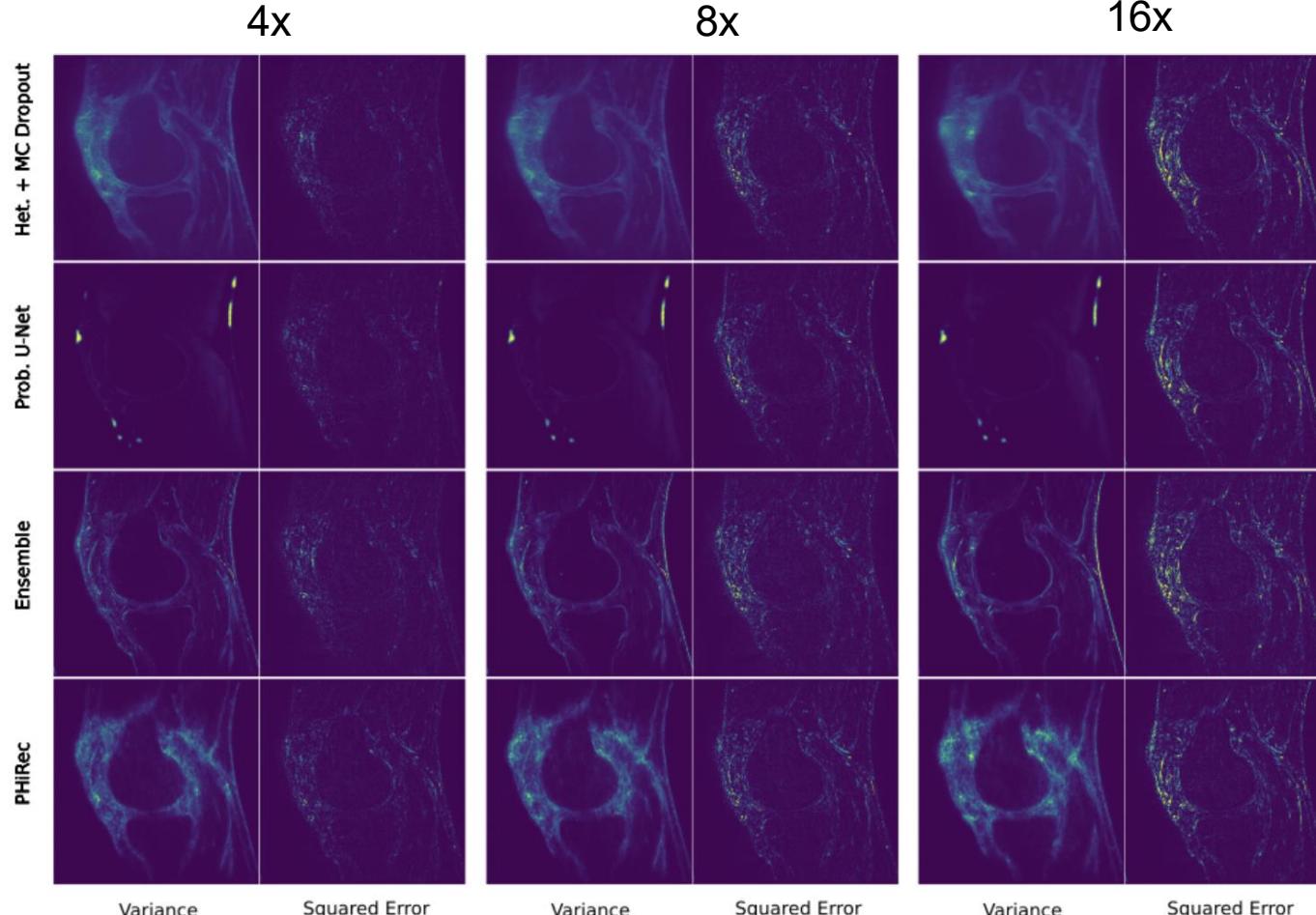


Inference for 1 slice:

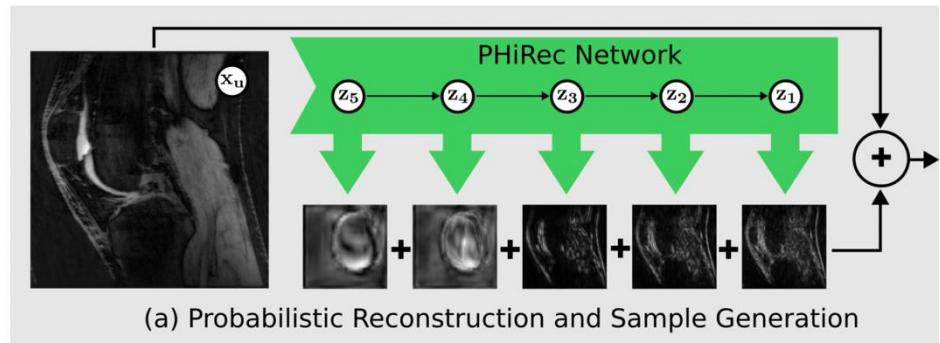


PHiRec: 1ms
Diffusion Model: ~10s

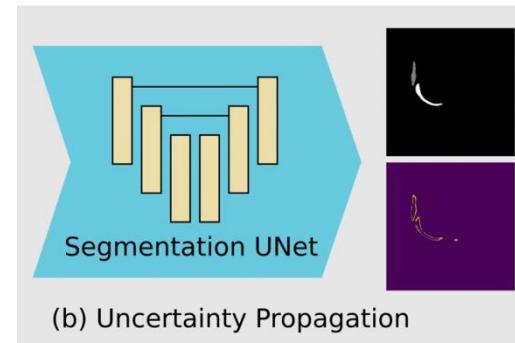
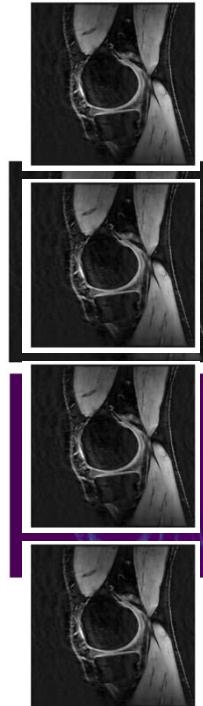
UNCERTAINTY QUANTIFICATION PERFORMANCE



PART 2: UNCERTAINTY PROPAGATION



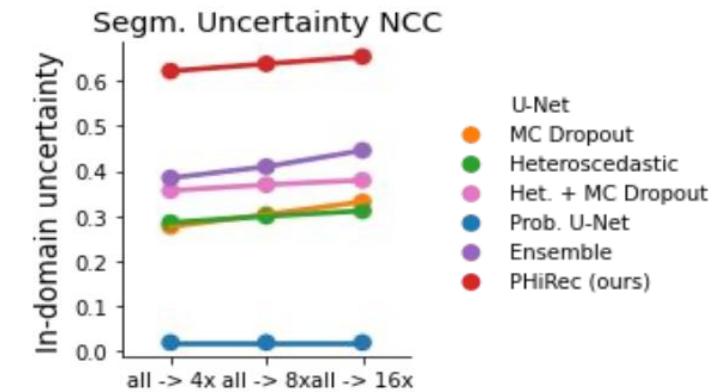
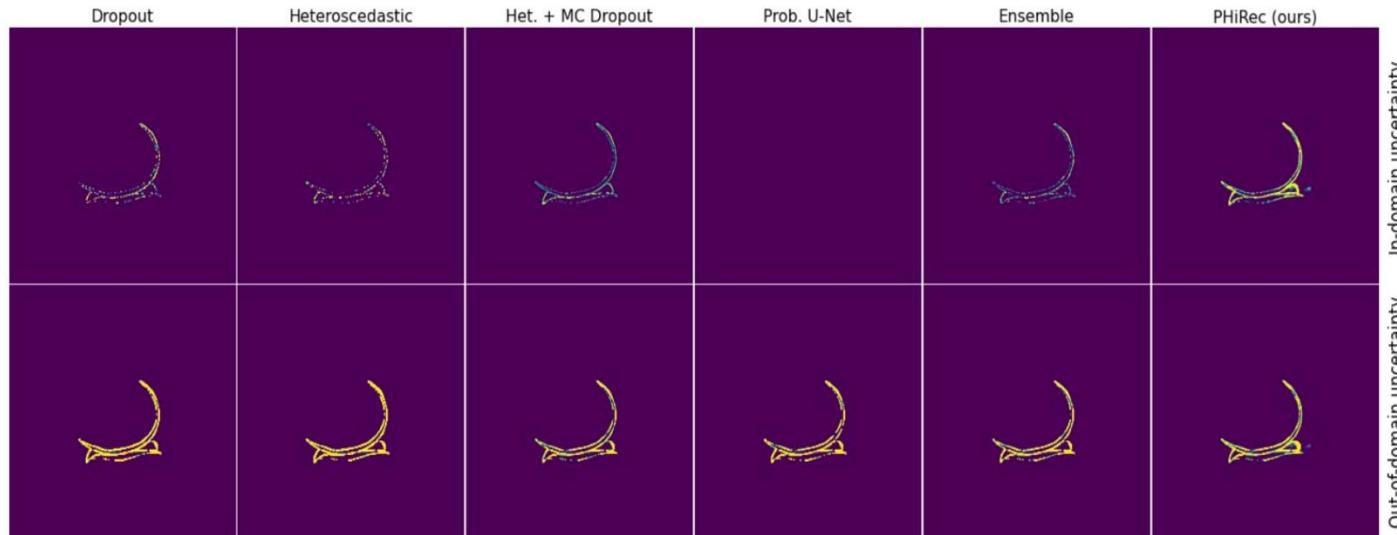
$$p(x|x_u)$$



$$f : x \mapsto s$$

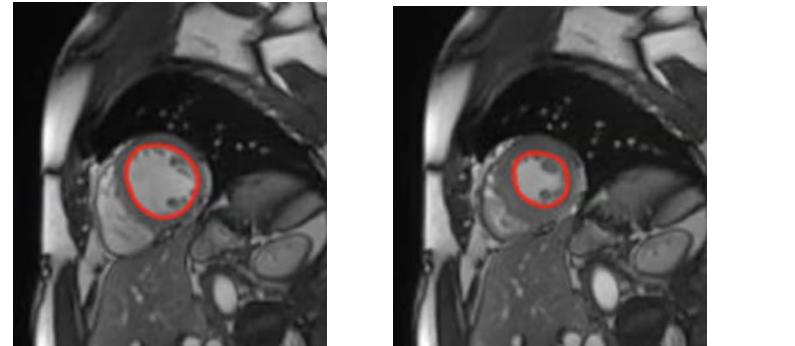
$$p(s|x_u) \approx \frac{1}{N} \sum_i^N \delta(s - f(X_i)), \quad X_i \sim p(x|x_u)$$

RESULTS: UNCERTAINTY PROPAGATION



PERSONALISED ADAPTIVE MR AQUISITIONS

Goal: Use patient-specific uncertainty to stop the scan early if the certainty is high enough for a downstream decision



$$\text{LVEF} = [(\text{End-Diastolic Volume} - \text{End-Systolic Volume}) / \text{End-Diastolic Volume}]$$

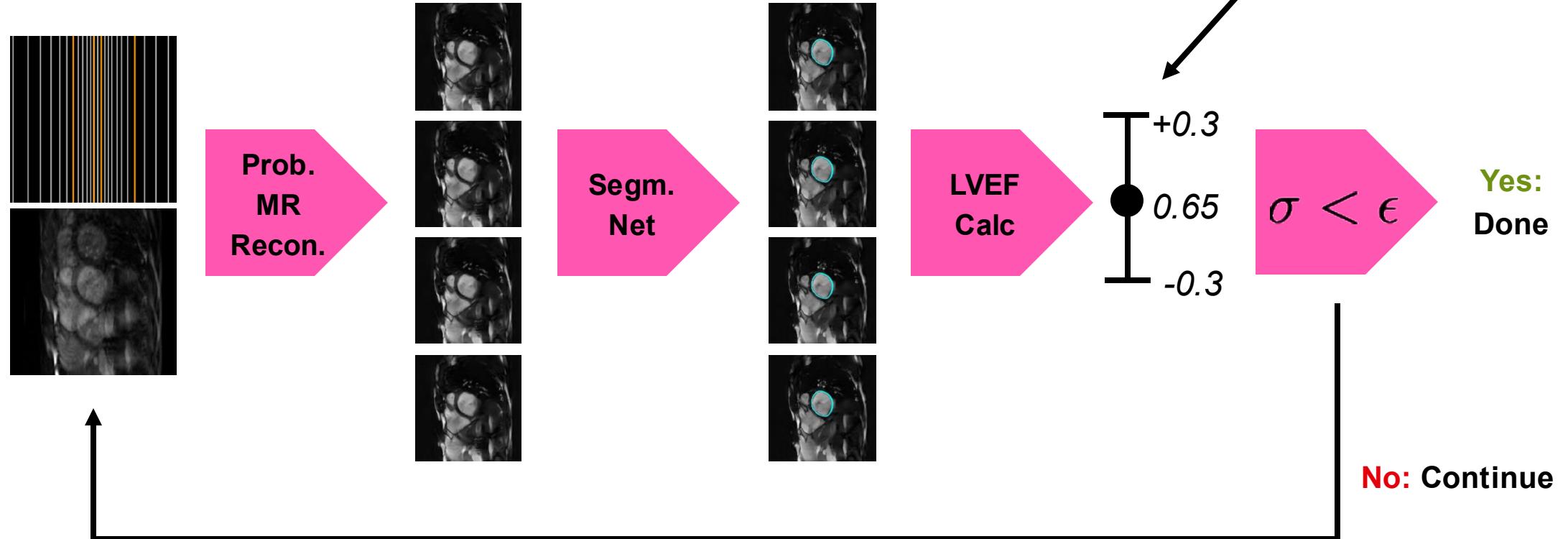


Alice: Young healthy subject with normal cardiac anatomy. Faster acceleration possible.



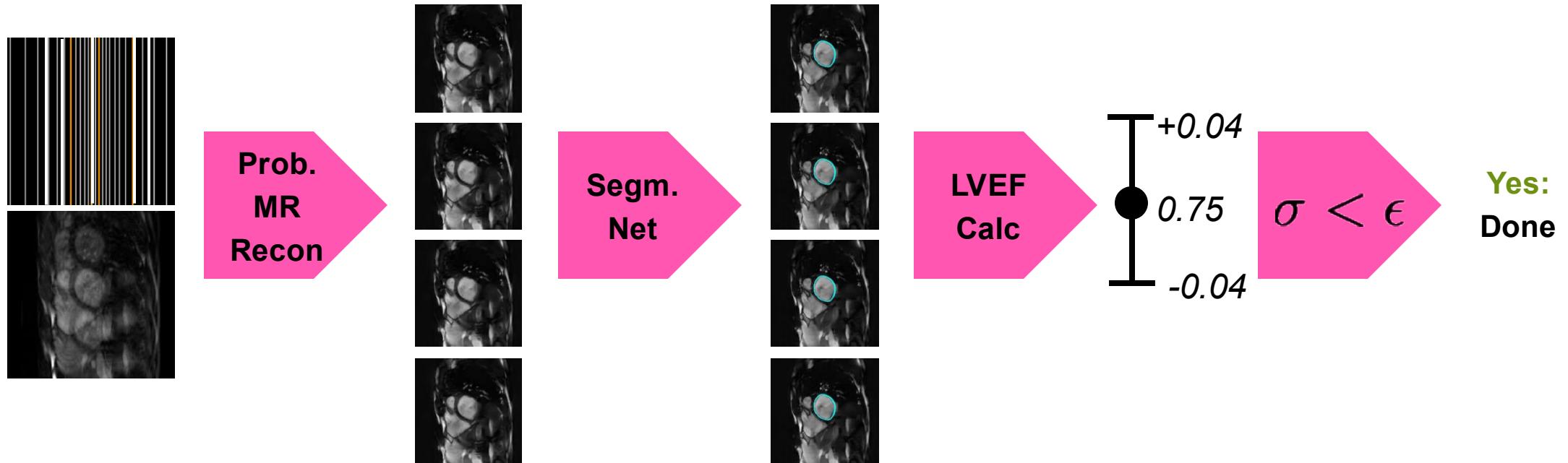
Bob: Unusual Cardiac Anatomy, irregular breathing. Only low acceleration possible.

UNCERTAINTY-GUIDED MR ACQUISITION



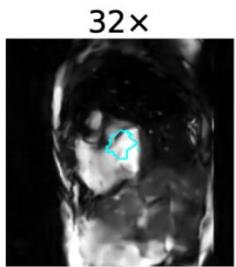
Paul Fischer, Jan Nikolas Morshuis, Thomas Küstner, Christian F Baumgartner, CUTE-MRI: Conformalized Uncertainty-based framework for Time-adaptivE MRI, Elsevier Medical Image Analysis (under review)

UNCERTAINTY-GUIDED MR ACQUISITION

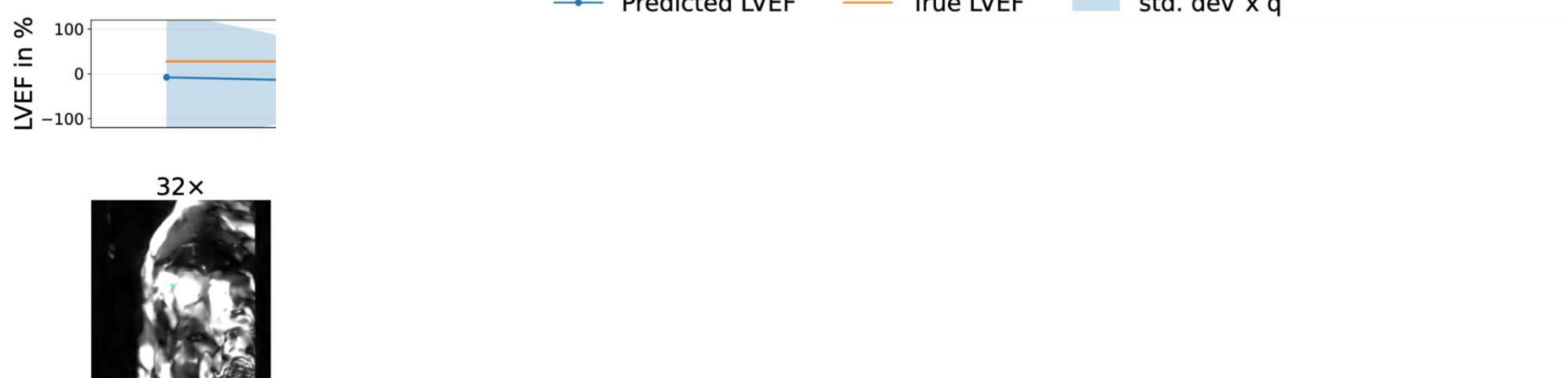


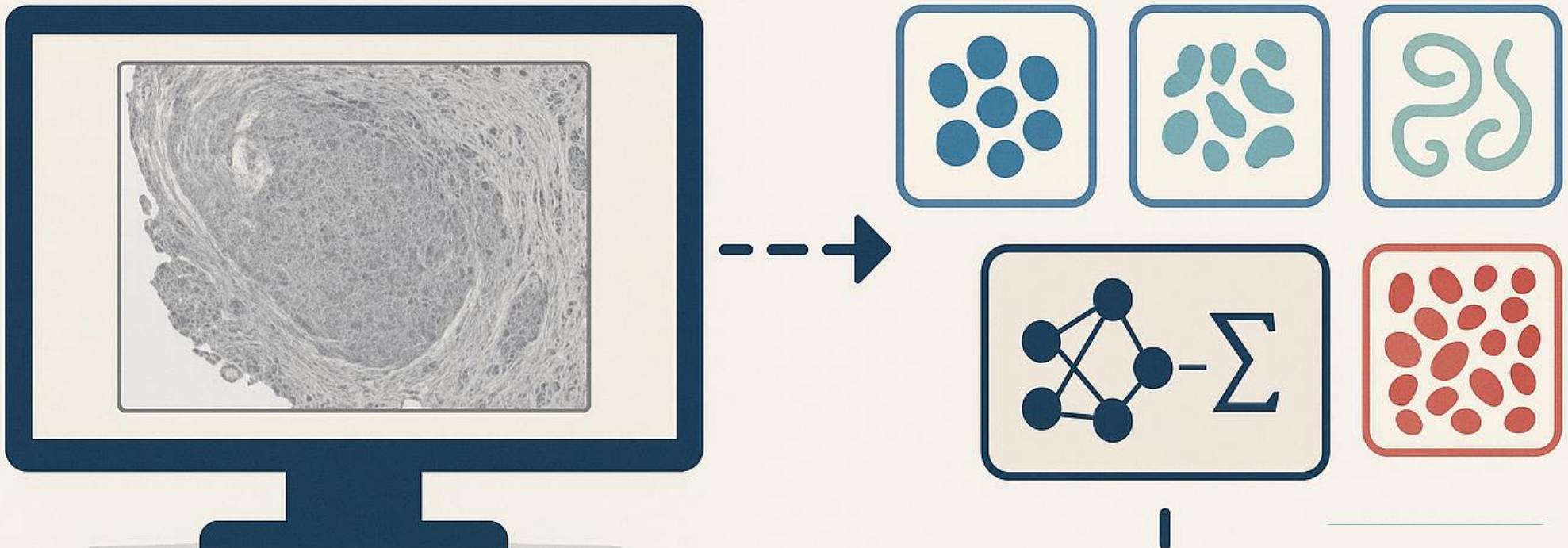
Paul Fischer, Jan Nikolas Morshuis, Thomas Küstner, Christian F Baumgartner, CUTE-MRI: Conformalized Uncertainty-based framework for Time-adaptivE MRI, Elsevier Medical Image Analysis (under review)

CASE EXAMPLE: “EASY” CASE

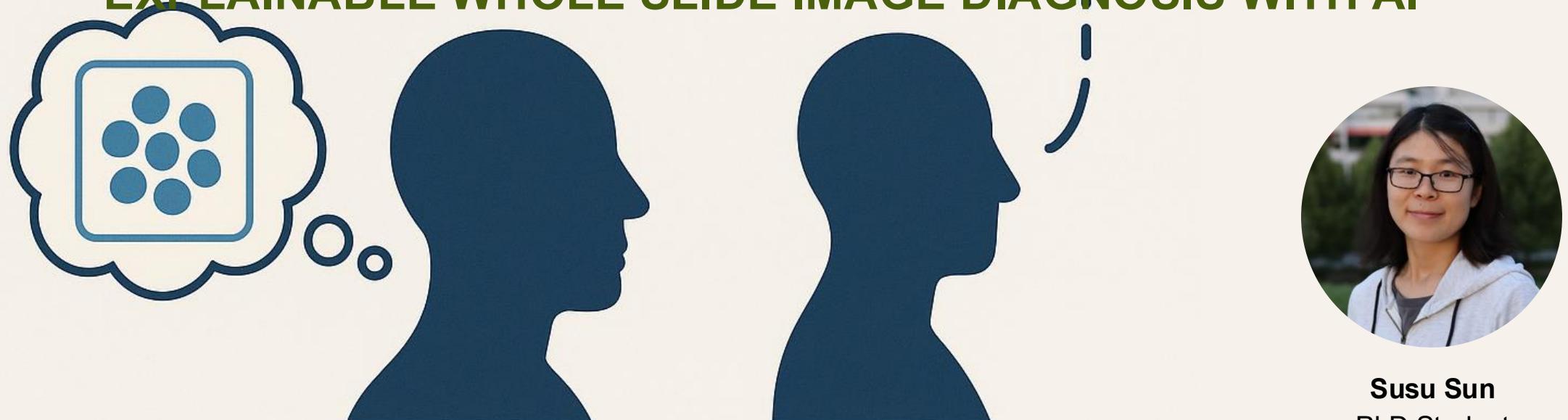


CASE EXAMPLE: “DIFFICULT CASE”



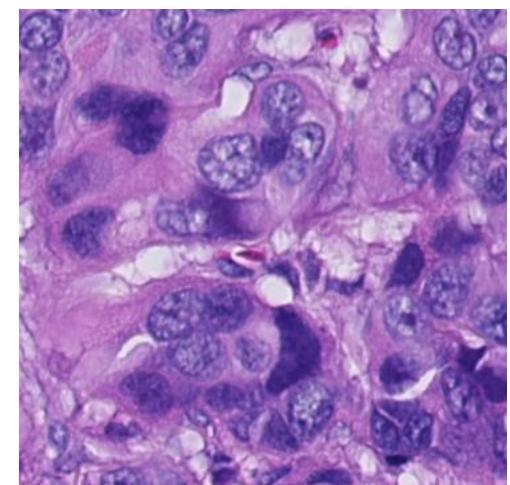
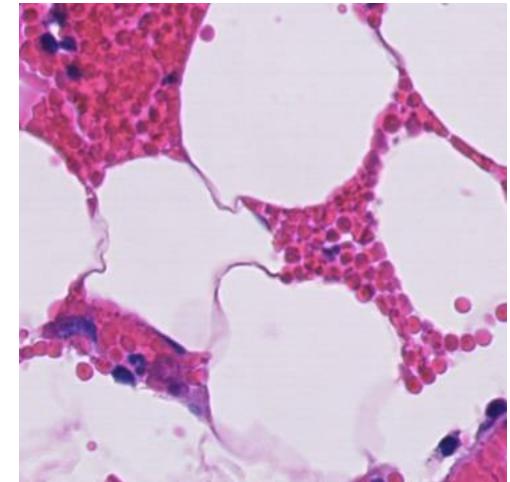
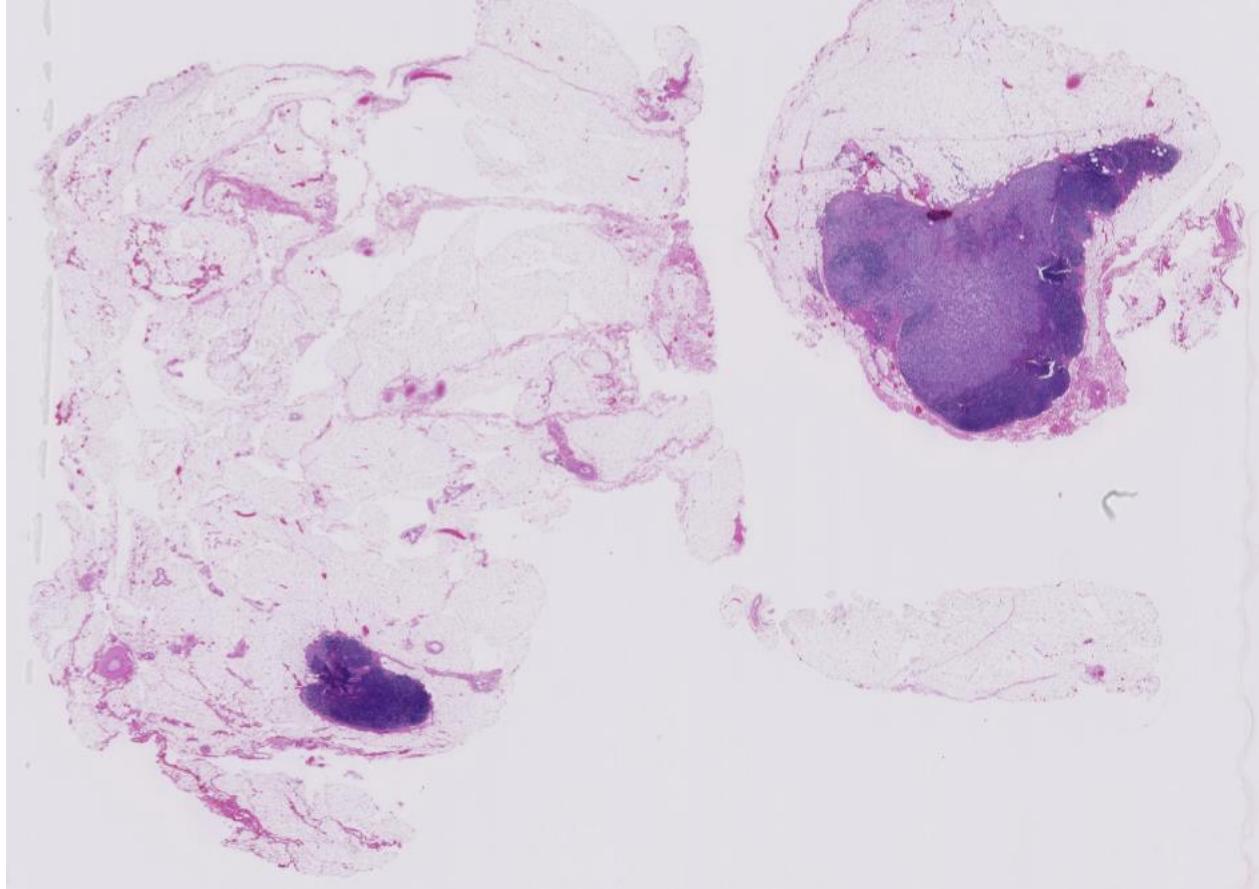


EXPLAINABLE WHOLE SLIDE IMAGE DIAGNOSIS WITH AI



Susu Sun
PhD Student

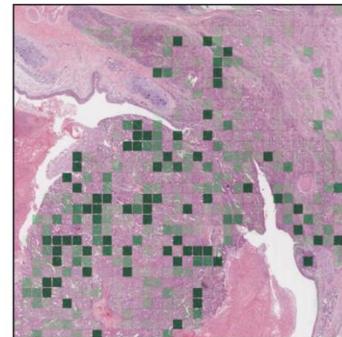
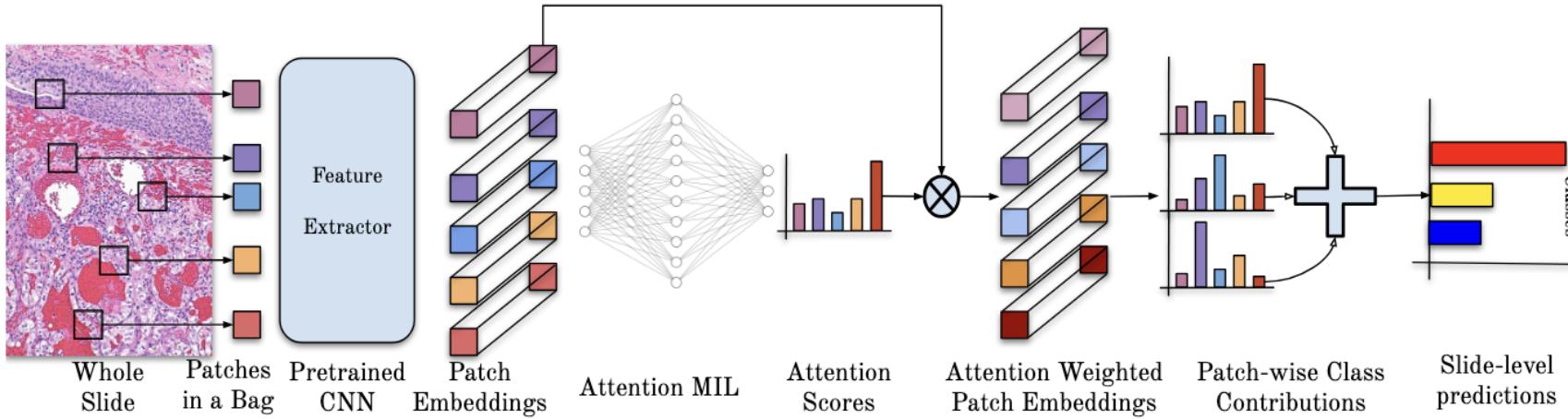
WHOLE SLIDE IMAGES (WSI)



Challenge for AI: WSI are huge (on the order of 100'000 x 100'000 pixels)

PRIOR STATE-OF-THE-ART

Multi-instance Learning (MIL)



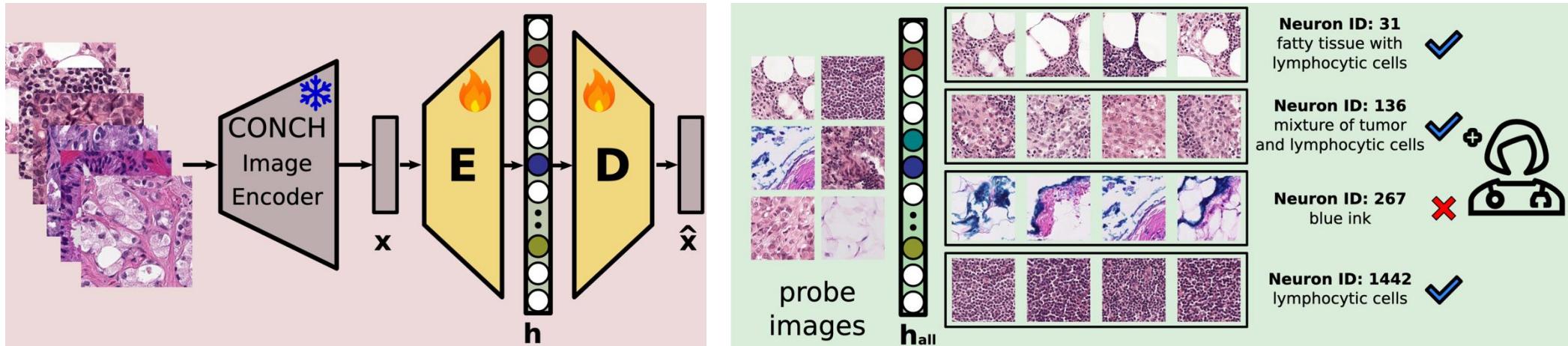
Attention Maps

Problems:

- Knowing *where* is not the same as knowing *why*
- Attention maps are known to not accurately reflect the model's decision

Javed, S. A., Juyal, D., Padigela, H., Taylor-Weiner, A., Yu, L., & Prakash, A. (2022). Additive mil: Intrinsically interpretable multiple instance learning for pathology. *Advances in Neural Information Processing Systems*, 35, 20689-20702.

OUR IDEA: FIRST STEP - DISCOVER AND NAME CONCEPTS

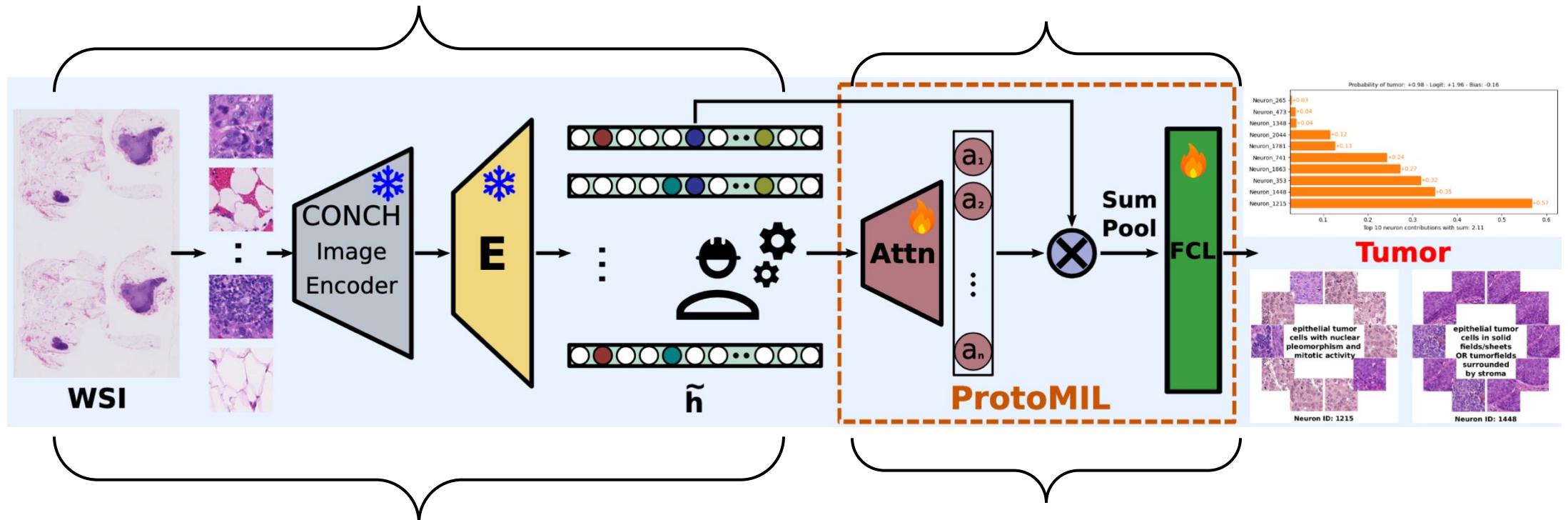


A **sparse autoencoder** is used to compress WSI patches to just a few informative neurons

We check what type of patch activates each neuron the most and ask a pathologist to name them

Susu Sun, Dominique van Midden, Geert Litjens, and Christian F. Baumgartner. "Prototype-Based Multiple Instance Learning for Gigapixel Whole Slide Image Classification." *Proc. MICCAI* (2025).

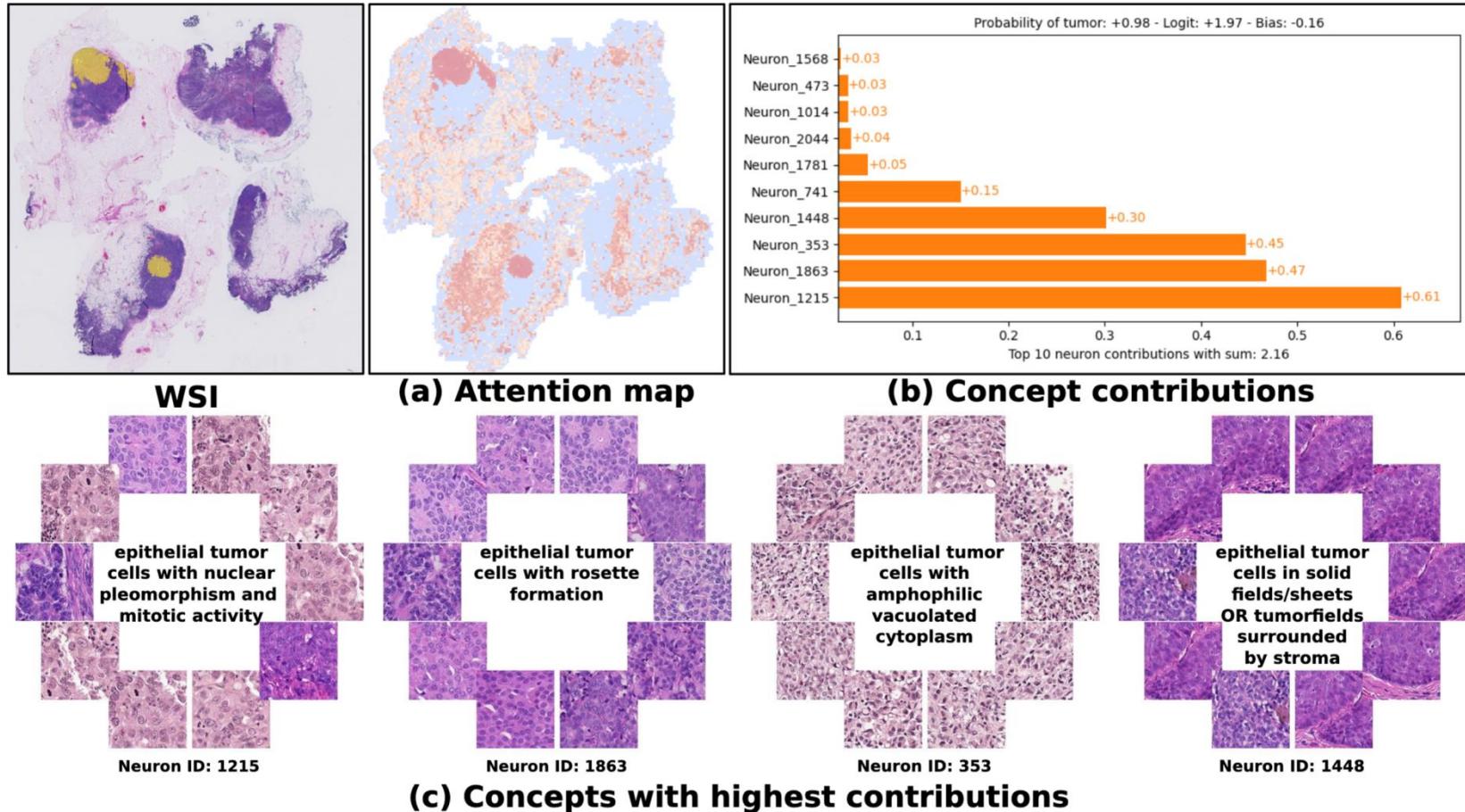
SECOND STEP: ENCODE TRAINING INTO NEURONS AND TRAIN A MIL APPROACH ON THEM



Applying the encoder part of the sparse autoencoder from before

Use a very simple MIL model for classification

OUTPUT OF OUR PROPOSED MODEL



MOVING UNWANTED SHORTCUT LEARNING

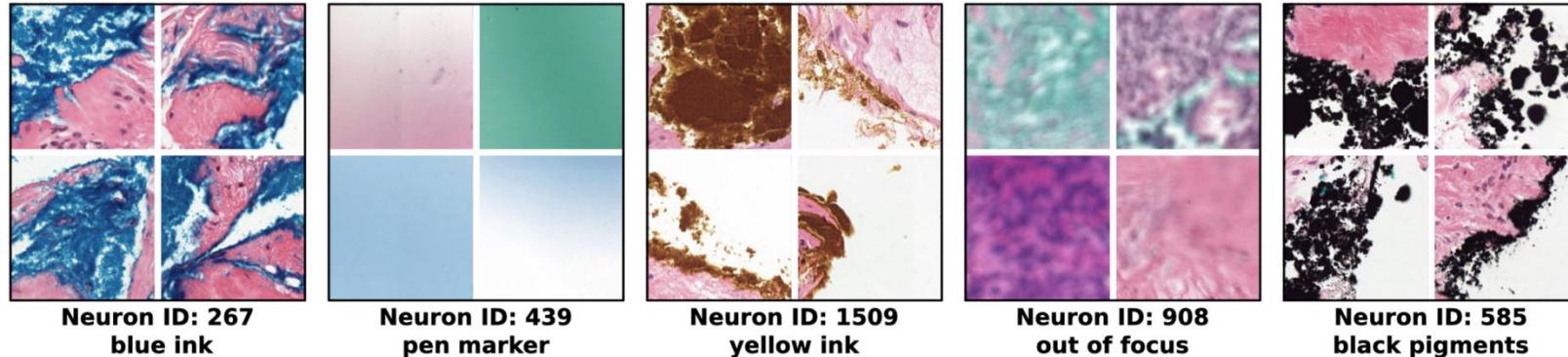


Table 1. Classification performance measured by Accuracy and AUC.

Model	Camelyon16		PANDA	
	Acc.	AUC	Acc.	AUC
ABMIL (image)	0.922	0.908	0.892	0.953
CLAM (image)	0.915	0.966	0.884	0.979
TransMIL (image)	0.938	0.950	0.939	0.977
AdditiveMIL (image)	0.875	0.883	0.905	0.958
ProtoMIL (concept)	0.907	0.918	0.916	0.970
ProtoMIL (intervened concepts)	0.926	0.913	0.916	0.964

THANK YOU FOR YOUR ATTENTION



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