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The electroencephalogram was recorded using tin electrodes embedded in a nylon mesh cap (Quik-cap, Neuromedical Supplies, Sterling, Virginia, USA), with a left mastoid reference and a forehead ground. An average mastoid reference was derived off-line. EEG data were corrected for ocular movement artifacts using the Gratton algorithm (1). Data were recorded from 0.01 to 70 Hz (half-amplitude cutoffs) and digitized at 400 Hz, using a SynAmps data acquisition system (Neuroscan Labs, Sterling, Virginia, USA). Prior to analysis the data were filtered with a 9-point Chebyshev type II low-pass zero-phase shift digital filter (Matlab 5.3, Mathworks, Inc., Natick, Massachusetts, USA), with a half-amplitude cutoff at 12 Hz.

ERP activity was quantified as the mean amplitude in the 200-300 ms epoch following the onset of the stimulus, relative to a 100 ms pre-stimulus baseline. A 2 (gain/loss) \times 38 (electrode location) repeated-measures analysis of variance (ANOVA) revealed a significant gain vs. loss effect, $F(1, 11) = 9.71$, $P = 0.0098$, $MSE = 28.54$, and a significant gain/loss \times location interaction, $F(37, 407) = 8.21$, $P = 0.00022$, $MSE = 0.56$. When necessary, in this and all analyses, P-values were adjusted using the Greenhouse-Geisser correction for violations of the ANOVA assumption of sphericity. All figures show error bars consisting of 2 standard errors of the mean, derived from the corresponding mean squared error (MSE) from the ANOVA.

In the analysis dissociating gain/loss from correct/error effects on the amplitude of the MFN (Figure 3), the 2 (gain/loss) \times 2 (correct/error) ANOVA showed a significant effect of gain/loss status, $F(1, 11) = 21.19$, $P = 0.00076$, $MSE = 9.22$. The error/correct effect was not significant $F(1, 11) = 1.63$, $P = 0.23$, $MSE = 4.58$.

To analyze the effect of position within the block on the proportion of risky responses, we used a repeated-measures ANOVA with a single four-level factor representing the quarter within a block. The effect of block quarter was significant, $F(3, 33) = 4.24$, $P = .038$, $MSE = 0.0049$, and a separate test contrasting the first quarter to the last quarter was also significant, $F(1, 11) = 6.74$, $P = 0.024$, $MSE = 0.0089$. The means for the quarters were (first to last): 0.58, 0.51, 0.53, 0.48.

The analysis of the effects of previous outcome on the proportion of risky choices and on the MFN effect (Figure 4) distinguished between two kinds of trials: trials where the alternatives were different ([5][25] or [25][5]) and trials where alternatives were equal ([5][5] and [25][25]). We refer to the former case as "choice" trials (where subjects had the opportunity to make a risky or cautious choice),

and the latter case as "no-choice" trials. In the analysis of proportion of risky choices, a 2 (gain vs. loss) $\times 2$ (25 vs. 5) $\times 2$ (choice vs. no-choice) repeated measures ANOVA showed a significant effect of the gain/loss status of the previous trial, $F(1, 11) = 23.54$, $P = 0.00051$, $MSE = 0.018$. The significant gain/loss \times 25/5 interaction $F(1, 11) = 5.59$, $P = 0.038$, $MSE = 0.021$, showed that the proportion of risky choices was affected by the gain/loss status of the previous trial more when the outcome was a gain or loss of 25 cents than when it was 5 cents. The MFN effect was also affected by the gain/loss status of the previous trial, $F(1, 11) = 6.38$, $P = .028$, $MSE = 5.17$, with a greater MFN effect following losses than following gains. The gain/loss \times 25/5 interaction was not significant, $F(1, 11) = 0.94$, $P = 0.35$, $MSE = 5.71$. The linear trend apparent in Figure 4 was significant for both the probability of a risky choice and for the MFN effect ($F(1, 11) = 17.05$, $P = 0.0017$, $MSE = 0.032$ and $F(1, 11) = 5.04$, $P = 0.046$, $MSE = 7.56$, respectively). Standard error bars are derived from the gain/loss \times 25/5 interaction MSE .

Using the Brain Electrical Source Analysis (BESA) software (2), we derived a best-fit single-dipole model of the MFN, based on the amplitude of the gain-loss difference waveform computed at its peak, 265 ms following the stimulus. Then, with BESA's coordinates for the dipole solution, we located the dipole within a canonical magnetic resonance imaging template of the human head, derived from an average of scans from 152 individual heads (file avg152T1.img, available as part of the SPM99 software at <http://www.fil.ion.ucl.ac.uk/spm>, Wellcome Department of Cognitive Neurology, London). We aligned the spherical geometry of BESA with the MRI template by fitting a sphere to a convex hull circumscribing the average head defined in the MRI image, using a least-square best-fit criterion. The origin of the sphere within the voxel coordinates of the template was, $x = 46.1$, $y = 55.8$, $z = 39.8$, and the radius of the sphere was 47.5 voxels. The spherical coordinates of the dipole in BESA's coordinate system were $\theta = 67.0$, $\phi = 83.4$, eccentricity = 40.9%. Figure 2 depicts the dipole solution using a sphere with a radius of 5 voxels, centered at those coordinates. The residual (unaccounted-for) variance associated with the best-fit dipole model shown in Figure 2 was less than 5%.

References

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