



Electrochemically changing potential

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Abstract

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Introduction

Since the help of single-molecule fluorescence detection methods, optical studies have made many breakthroughs in the field of science. Single-molecule fluorescence resonance energy transfer (FRET) is one of the most general accepted techniques. Different kind of kinetics of proteins, such as redox switching [?], have been revealed. In the past, Biswajit Pradhan has taken a closer look at the time traces and autocorrelation of azurin labelled with ATTO 655 under different potentials. Here the potential was changed chemically: different solutions with different concentrations of ascorbate were used to achieve different potentials. The goal of this thesis is to make an experimental set up which can measure the time traces and autocorrelation of single molecules in different potentials. However, a key difference with the set up of B. Pradhan is that the potentials are not changed chemically, but rather electrochemically. With the help of a electrochemical analyser different potentials are achieved.

In general the setup on its own is meaningless and rather a first step to scientific success. The results are way more important. To discuss the measurements made with the new setup, the autocorrelations of labelled azurin measured with the two different set ups are compared.

Chapter 2

Theory

In this chapter, the fundamental physics and electrochemistry are explained which are used in the set up.

2.1 Fluorescence

Fluorescence is the property of certain atoms and molecules to absorb light at particular wavelengths and emit light at longer wavelengths. These type of atoms and molecules are called fluorophores or fluorescent dyes. A brief interval after absorption - the fluorescence lifetime - the atoms or molecules will emit light of less energy (longer wavelengths). Fluorescence is a process governed by three events. All these events occur on different timescales separated by several orders of magnitude. These events are summarised in Figure 2.1.

2.1.1 Excitation

The first event is excitation. For any molecule, several electronic states exist depending on the total electron energy and the symmetry of the electron spin states. Each state is divided in sub-states - a number of vibrational and rotational energy levels associated with the atomic nuclei and the bonding orbitals. At room temperature, most molecules lack the internal energy to exist in any other state than the lowest vibrational level of the ground state. This ground state is usually an electronic singlet in which all electrons are spin-paired (opposite spins). With the help of a laser, photons with energy $E_{photon} = h\nu_{laser}$ are absorbed by the fluorophores. The absorption of energy happens to any of the closely spaced

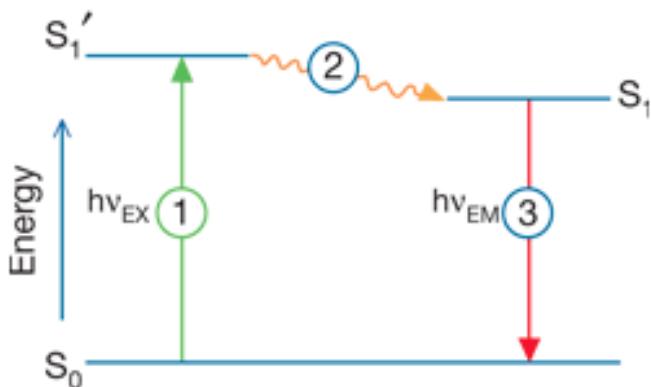


Figure 2.1: The three major events in fluorescence: excitation (1), relaxation (2) and emission (3).

vibrational and rotational energy levels of the excited states. Absorption of light occurs in a few femtoseconds ($10^{-15}s$). It will only occur for specific wavelengths known as the absorption bands. If a photon contains more energy than necessary for an electronic transition, the excess energy is converted into vibrational and rotational energy via non-radiative processes. If the energy of a photon is too low, no transition occurs. Excitation of a molecule by absorption normally happens without a change in electron spin-pairing. Therefore, the excited state is also a singlet. Usually the fluorophores are excited to higher vibrational levels of the first or second singlet electronic energy state. Certain transitions have higher probability than others and combined they form an absorption spectrum of the molecule.

2.1.2 Vibrational relaxation

After absorption, several processes occur with varying probabilities. The most likely is relaxation to the lowest vibrational energy level of the first excited state, a process known as internal conversion or vibrational relaxation. This is a loss of energy in a non-radiative manner and has a timescale of a picosecond ($10^{-12}s$) or less. Since a significant number of vibration cycles happen during the excited lifetimes, molecules undergo complete vibrational relaxation. The excess vibrational energy is converted into heat, which is transferred to the neighbouring solvent molecules.

2.1.3 Emission

The excited molecule exists in the lowest excited singlet state for a period in the order of nanoseconds ($10^{-9}s$) before relaxing to the ground state. During this relaxing, a photon will be emitted. Because the ground state consist of closely spaced vibrational energy levels, the resulting emission intensity is distributed over a band of wavelengths rather than a sharp line. Most fluorophores can repeat the excitation and emission cycle a lot of times. However, the excited state is more reactive with the surrounding which can result in photobleaching: the molecule is permanently unable to fluoresce.

Other relaxation pathways compete with the fluorescene emission process. The excited state energy can be dissipated as heat, the excited molecule can collide with another molecule to transfer energy (for example quenching) or intersystem crossing to the lowest excited triplet state can occur. The latter will result in emission of a photon through phosphorescence or a transition back to the excited singlet state that yields delayed fluorescence. Molecules who exhibit the triplet state have a high degree of chemical reactivity, often resulting in photobleaching.

2.2 Fluorescence Resonance Energy Transfer

Fluorescence resonance energy transfer (FRET) permits determination of two molecules within several nanometers, the distance close to where molecular interactions occur. The process of resonance energy transfer can take place when the donor fluorophore in an electronically excited state transfer its excitation energy to a nearby chromophore (the acceptor). If the fluorescence emission spectrum of the donor molecule overlaps the absorption spectrum of the acceptor molecule and the two are within minimal spatial radius, the donor can transfer its excitation energy in a non-radiative fashion through dipole-dipole intermolecular coupling. Treating an excited fluorophore as an oscillating dipole, it can undergo energy exchange with a second dipole having a similar resonance frequency. If the acceptor itself is a fluorochrome, increased or sensitised fluorescence emission is observed. By exciting the donor and acceptor molecules with light of wavelengths centred near the absorption maximum of the donor, the detected light will be emitted at wavelengths centred near the emission maximum of the acceptor if FRET has taken place. This resonance energy transfer is not sensitive to the surroundings of a fluorophore. The FRET

efficiency is given by:

$$E = \frac{1}{1 + (r/R_0)^6} \quad (2.1)$$

where r is the distance between the donor and acceptor molecule and R_0 is the Förster distance - the distance at which the energy transfer efficiency is 50%. Related to this efficiency is the lifetime (τ'_D in presence of an acceptor and τ_D with the absence of an acceptor) and the fluorescence intensity (F'_D in presence of an acceptor and F_D with the absence of an acceptor) via the formulas

$$E = 1 - \frac{\tau'_D}{\tau_D} \quad (2.2)$$

and

$$E = 1 - \frac{F'_D}{F_D}. \quad (2.3)$$

2.3 FluRedox principles and labelled azurin

In contrast to FRET, FluRedox is based on the change of the overlap integral associated with a change in the optical properties of the redox-active centre upon oxidation and reduction. The optical read-out responds exclusively to the redox state of the protein [?].

Azurin is a blue copper protein with an active copper site (see Figure 2.2). The active centre of azurin has strong characteristic features in its optical absorption spectrum which is dependent on the redox state. It may occur in oxidised (Cu^{2+}) or reduced (Cu^+) form. Oxidised azurin exhibits a strong absorption band around 600 nm (blue). Fluorescent labelling of this protein makes it suitable for single molecule studies. ATTO-655 is a fluorescence dye with an emission band around 680 nm. The emission band of the dye and the absorption band of the azurin overlap (see Figure 2.3). When azurin is oxidised, FRET between the dye and the centre quenches the dye fluorescence. This quenching is absent when the protein is in reduced state because its 600 nm absorption has vanished [?].

2.4 Single molecules techniques

It is impossible to open newspapers without stumbling over words that reflect the impact of life sciences to the modern world. Many speculations and discussions suffer from vagueness since many biological mechanisms

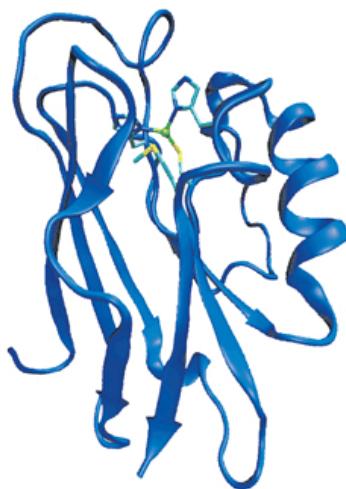


Figure 2.2: Three dimensional structure of azurin. The green sphere is the copper centre of the protein. Picture is taken from [?].

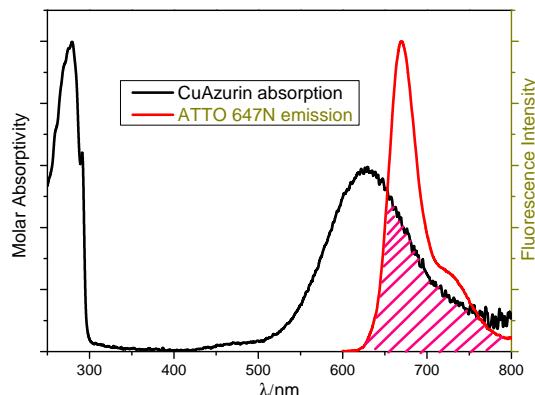


Figure 2.3: Absorption spectrum of CuAz (black) and the emission spectrum of the fluorescence dye ATTO-655 (red). The overlapping parts are purple marked. The absorption band around 600 nm is absent when azurin is reduced.

are barely known to exist and even less mechanisms are fully understood. New and more precise techniques have made this field grow quickly. With new synthetic fluorophores, the ability to study single proteins at a time is exploited to investigate a variety of dynamics. One of the ways to get a better understanding of these single proteins is the usage of fluorescence correlation spectroscopy and the usage of confocal microscopes.

2.4.1 Fluorescence Correlation Spectroscopy

The instrumentation of Fluorescence Correlation Spectroscopy (FCS) is based on an inverted confocal microscope. A laser beam is directed into a microscope objective via dichroic mirrors and focused on the sample. High numerical aperture are used. Fluorescence light from the sample is collected and passed through the dichroic and emission filter. A pinhole in the image plane blocks the light not originating from the focal region. When concentrations in order of a few - or less - nanomolar of fluorescent particles are applied, single particles can be monitored at a given time. A more detailed description can be found in reference ??.

The fluorescence intensity collected during the experiments were elaborated using the normalized autocorrelation (AC) function, defined by:

$$G'(\tau) = \frac{\langle I(t)I(t + \tau) \rangle}{\langle I(t) \rangle^2}. \quad (2.4)$$

Substracting the normal offset of value 1, this leads to

$$G(\tau) = G'(\tau) - 1 = \frac{\langle \delta I(t) \delta I(t + \tau) \rangle}{\langle I(t) \rangle^2} \quad (2.5)$$

where the brackets denotes temporal averaging and $\delta I(t) = I(t) - \langle I(t) \rangle$. The autocorrelation function is used to compute the self-similarity after lag-time τ .

2.4.2 Confocal Laser Scanning Microscopy

Confocal Laser Scanning Microscopy (CLSM) is the setup we used in this experiment. The CLSM is used to scan a sample. In contrast to the FCS, the detection of the signal from the sample depends on strategic choices. The sample is mounted on a moving piezoelectric scanning stage. This allows sub-micrometer movements. The scanning stage is moved along the confocal volume and the fluorescent signal is collected for each position sampled. Together with the fluorescence intensity, the setup is equipped to record the lifetime of the fluorescence and time traces with the help of a time-correlated single-photon counting (TCSPC) board. A more detailed description of the setup is found in sections 3 and ??.

For this thesis, the Cu-azurin and Zn-azurin were labeled and immobilized on the sample slide. Surrounded by an electron mediator, different potentials were applied on areas of $(20 \times 20) \mu\text{m}^2$, which have around 30 -

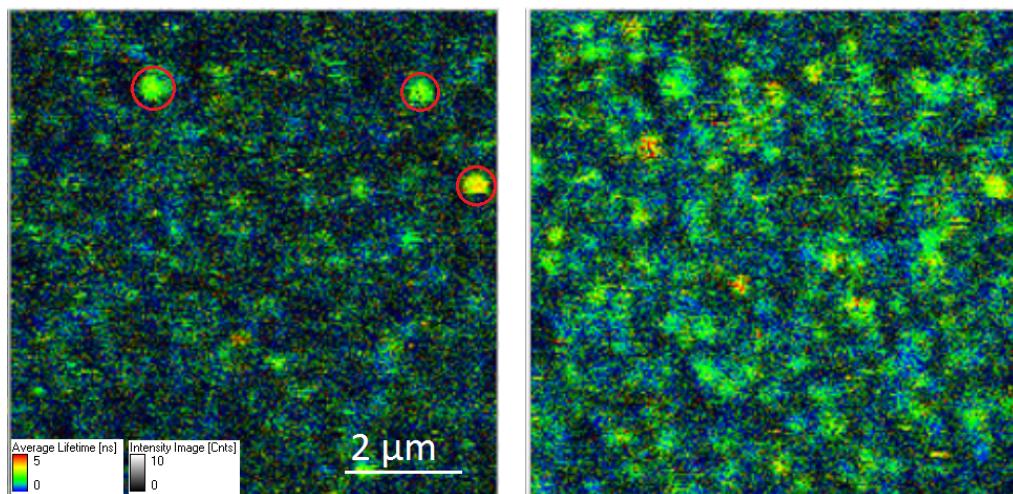


Figure 2.4: A $(10 \times 10) \mu\text{m}^2$ area filled with immobilized Cu-azurin at different potentials. On the left: potential of 100mV, here the Cu-azurin is oxidized. The bright spots (red circles) are either bleached proteins or impurities. A way to get rid of these impurities is by focussing the laser with slightly more power on these spots. On the right: same area, but with -100mV potential. All the proteins are reduced. Comparing these two pictures show immediately the active protein and the non active proteins/impurities.

40 immobilized proteins. Initially applying a positive and negative potential, by means of lifetime analysis and intensity, the active azurin and inactive azurin/impurities can be pointed out directly after taking the images, since the FRET effect affects directly the lifetime of the dye (see Figure 3.4). Once we select the working proteins, the signal of the proteins is recorded for different time intervals (usually 30 seconds) resulting in time traces as showed in Figure 2.5.

2.5 Binding protein to the surface

In a variety of different applications the biotin-avidin system has been used [?]. Living organisms develop highly specific defence mechanisms to help survive in unfriendly environments. Avidin, a protein found in egg white, has the ability to bind with very high affinity to vitamin biotin. This interaction is thought to represent the natural defence mechanism: the binding of avidin with biotinylated enzymes inactivates the enzymes and thus inhibits the growth of bacteria. Compared to other ligand-binder interactions, biotin-avidin has unique characteristics. The noncovalent in-

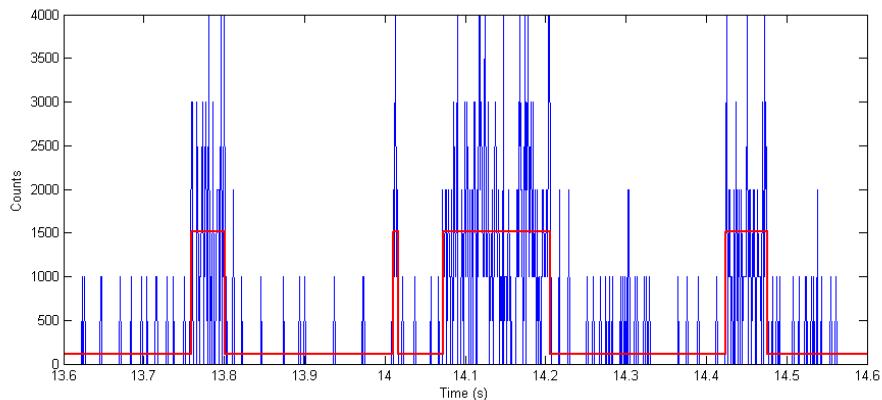


Figure 2.5: Example of a small part of a 30 sec timetrace of an immobilised Cu-Azurin in a -100mV potential, taken with a CLSM. The blue line is the raw data, the red line is the fitted on and off magnitude and changepoint times. This is calculated using a specific program which is in more details described in the Data section.

teraction of avadin with biotin has a formation constant of $10^{15} \text{ L} \cdot \text{mol}^{-1}$, much greater than the interaction of ligands with their specific antibodies (about $10^3 - 10^6$ times greater). Also the avidin to biotin binding is specific enough to ensure the binding direct to the target of interest. Finally, the avidin possesses four binding sites per molecule.

The NeutrAvidin is used unlabelled and serves as a link between the biotinylated binder (the biotin on the glass slide) and the biotinylated molecule (labeled Cu-azurin). This is illustrated in Figure 2.6

2.6 Oxidation-reduction reactions

Electron transfer (ET) is the movement of electrons and can be generated by movements of electrons from one element to another in a oxidation-reduction (redox) reaction. Oxidation is the loss of electrons, reduction is the acquisition of electrons. The species being oxidized is called the reductant and the species being reduced is called the oxidant. The oxidation-reduction reaction can occur spontaneously. This is due to the difference in potential energy between the two substances. This difference is called the cell potential, denoted as E_{cell} . This cell potential depends upon the concentration of species as well as temperature. The greater the cell potential the greater is the driving force of the electrons. Since the standard state cell potential E_{cell}^0 is measured under standard states (1 Molar and 1

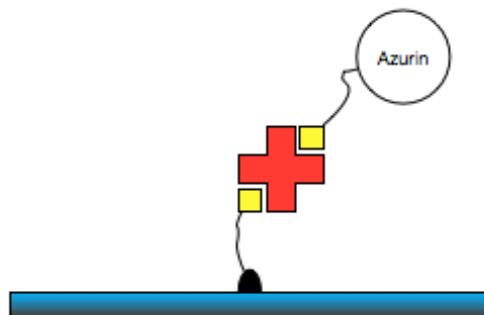


Figure 2.6: Illustration of the sample slide - NeutrAviding - protein binding. The red cross is the NeutrAvidin, with the four corners representing the binding spots for biotin. The yellow rectangles represent the biotin. One side is bound to the glass surface while the other side is connected to the azurin

atmospheric pressure), it differs from the non-standard state cell potential. The two are closely related via

$$E_{cell} = E_{cell}^0 - \frac{RT}{nF} \ln Q \quad (2.6)$$

or in terms of \log_{10}

$$E_{cell} = E_{cell}^0 - \frac{0.0592}{n} \log_{10} Q \quad (2.7)$$

where Q is the reaction quotient. This equation is referred to as the Nernst equation. For a reversible reaction (which is usually the case in redox reactions) $aA + bB \rightleftharpoons cC + dD$ where a , b , c and d are the stoichiometric coefficients for the balanced reaction, we can calculate the reaction quotient using:

$$Q = \frac{[C]^c [D]^d}{[A]^a [B]^b} \quad (2.8)$$

2.7 Electrochemical detection

Electrochemical detection instruments can be used for monitoring the current passing through a flow cell in liquid electrochemistry and flow injection analysis, but they can also be used for other electroanalytical applications. The potential control range of these instruments is $\pm 10V$. To

reach certain potentials, a constant potential is applied and the current is recorded as function of time (amperometric i - t curve), as is shown in Figure 2.7. Once the current in the i - t Curve is constant (i.e flat), the solution has reached the demanded potential. The data sample interval is chosen according to the length of the experiment.

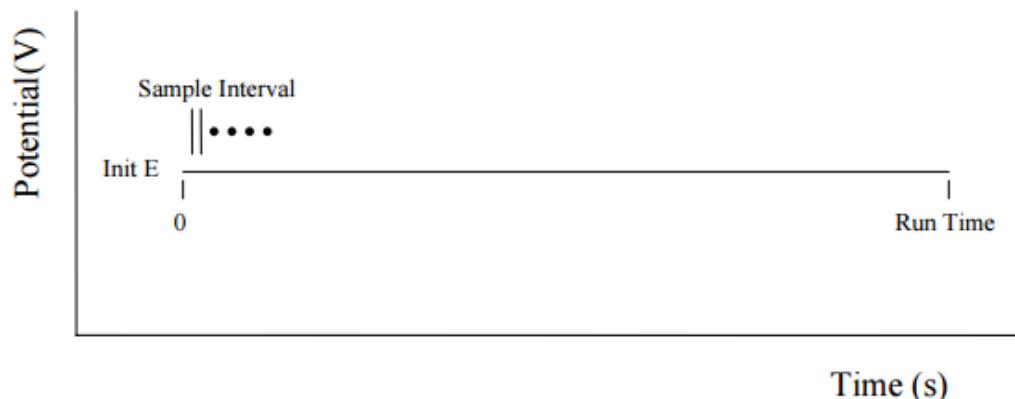


Figure 2.7: The amperometric i - t curve.

Chapter **3**

Experimental setup

This chapter covers the establishment of the setup from the start till the end. In papers and publications, it is not common to describe how the experiment was built from the start till the end, but considered the duration and effort it took during this project it cannot be excluded from this thesis. The chapter is divided in three parts: the first part describes the previously used setup in which the potential changed chemically by increasing or decreasing the concentration of electron donor. The second part of this chapter covers the progress from scratch to the final setup including the experimental successes and experimental failures. The final part of this chapter discusses the final setup and how it operates. It is this setup with which the data is acquired.

Some parts and techniques such as the confocal microscope and functionalizing of the glass slides is used in both setups. Therefore these are described below.

In this chapter and the rest of the thesis: the blue copper azurin used in the experiments is labelled with ATTO665 at binding site K122 (lysine at position 122). When copper azurin (CuAzu) is mentioned, it is referred to the one with ATTO665 label. The potentials measured and mentioned in this thesis are always with respect to the calomel electrode.

Confocal microscope

To perform the experiment, a home built confocal microscope used previously for similar experiments [?] was used. A 639 nm pulsed laser, controlled by a PDL 800-B (PicoQuant) laser driver at 40MHz repetition rate, is passed through a narrow band filter (LD01-640/8-25, Semrock). To

collimate the beam to the desired diameter an aspheric lens of suitable focal length was used. The beam then got reflected via a dichroic mirror (ZT640RDC, Chroma) to the high numerical aperture (NA) oil immersion objective (1.4 NA, 100X oil, Zeiss). The stage on which the sample was mounted was controlled by a nanopositioning piezo element (P517.3CD, Physic Instrumente). The emission was collected and filtered through an emission filter (ET655LP, Chroma) and focused onto a 50 μ m pinhole to filter the background. Once the beam got focused on the active area of a single photon counting module (SPCM-AQR-14, Perkin Elmer) data acquisition was performed by a photon counting PC-board (TimeHarp 200 PicoQuant). A schematic set up is shown in Figure 3.1.

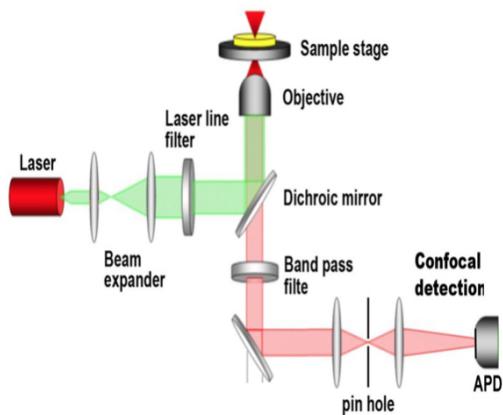


Figure 3.1: Schematic drawing of the confocal microscope used in the chemical and electrochemical set up.

Functionalizing glass slides

Not only the same confocal microscope was used in both setups, also the immobilization of the proteins is similar. The functionalization of the cover glass is based on the process used in [?]. $\varnothing 25\text{mm}$ #1 thickness glass coverslips (Menzel-Glaser) were used for all immobilizations. The coverslips were rinsed several times with milliQ water and treated with a $\text{H}_2\text{O}/\text{NH}_4\text{OH}/\text{H}_2\text{O}_2$ (5:1:1) bath at 70° C. The coverslips were then rinsed again but with water and finally with ethanol. The result of this process is the coverslips contain active silanol groups which can react with silanes and thus providing capability to functionalize the surface. The coverslips were stored in ethanol.

Before usage, the coverslips were flamed and then ozone cleaned for 15 minutes. Then the coverslips were treated for 30 min with a 1% solution of 3-(2-aminoethyl)aminopropyl trimethoxysilane in methanol containing 5% glacial acetic acid. After washed extensively with methanol, the coverslips were sonicated with intervals of 10 minutes. Dried with clean nitrogen, it was left in the desiccator overnight or kept in the oven at 65° C for 3 hours. The next day they were treated with a 5 mg/mL solution of methoxy-peg-NHS (MW 2000, Laysan Bio) and 0.05 mg/mL biotin-peg-N-hydroxysuccinimide (MW 3400, Laysan Bio) in 50mM phosphate buffered saline (PBS) with pH 7.4. To ensure enough biotin functionalities are present the ratio of biotin peg to methoxy was kept at 1:100 in the final experiments.

3.1 Changing the potential chemically

A small glass slide is functionalized in a similar way explained previously. A syringe is used to suck solution through the tubes onto the glass slide. One side is connected to the syringe, the other side is connected to the desired solution. First a mixture of proteins is put on the glass slide. After sufficient time, the proteins will bind to the glass slide. A new mixture consistent of buffer HEPES (pH = 7) is then sucked through the tube onto the glass slide to remove non-bound proteins. Once the proteins are removed, a new mixture consistent of ascorbate ($C_6H_8O_6$) and potassium ferricyanide ($[Fe(CN)_6]^{4-}$) is incubated into the flow cell. Ascorbate is an antioxidant and exists predominantly as the ascorbate monoanion $AschH^-$. The standard potential of ascorbate is around 40mV (pH = 7) with respect to a colomel electrode, which is close to the standard potential of the proteins. Oxidation of ascorbate forms ascorbyl radical $Asc^{\bullet-}$, the equivalent of ascorbate but with one less proton and one less electron. Upon further oxidation this becomes dehydroascorbate ($C_6H_6O_6$) [?]. Schematically this becomes:

At equilibrium, using the Nernst equation (Formula 2.6), the potential can be written as

$$E = E^0 - \frac{RT}{F} \log_{10} \frac{[C_6H_6O_6][Fe(CN)_6]^{3-}}{[C_6H_8O_6][Fe(CN)_6]^{4-}}. \quad (3.1)$$

Thus by adjusting the concentration of ascorbate (in this case adding ascorbate) or ferri-/ferrocyanide, different potentials will be achieved in the solution. The final redox potentials of the solution were measured

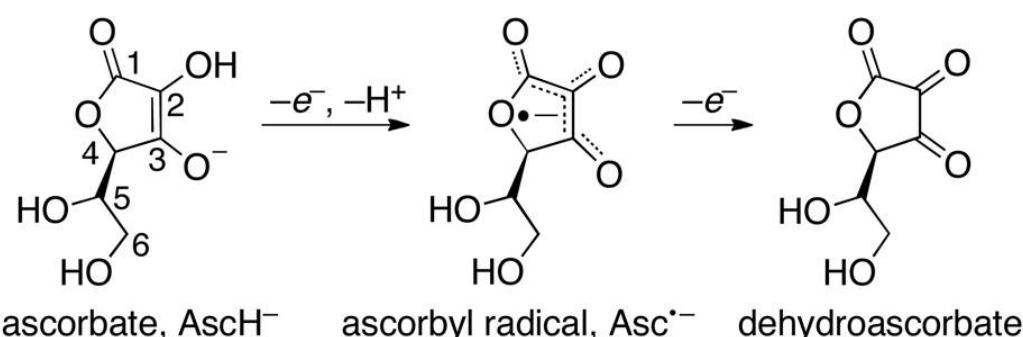


Figure 3.2: Redox of ascorbate

with a reference electrode (standard calomel, SCE) and a platinum counter electrode connected to a voltmeter.

Some of the downsides to this setup are summed below:

- The change of potential is induced by adjusting the concentration of ascorbate or ferri/ferrocyanide. By adding or removing substances, the solution will be disturbed. The chance of losing the monitored proteins is substantial if this is not done carefully.
- Reaching specific potentials is only possible by adding or removing the exact amount of redox participants. A small mistake and the wanted potential will not be reached.

These downsides lead ultimately to the desire of a better controllable and reliable setup.

3.2 Process to the final setup

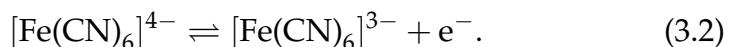
In the previous setup the potential was controlled by adding different concentration of chemicals. In the new setup, these changes are achieved electrically. Beside the confocal microscope, a new instrument has to be introduced: the electrochemical analyzer (Model 800B Series Electrochemical Detector, CH Instruments). Instead of using different concentrations of ascorbate, a cell with a working electrode, counter electrode and reference electrode in a buffer is used. During the process of getting to the final setup, the same working electrode, counter electrode and reference electrode is used: a $\varnothing 250\mu\text{m}$ golden wire acts as the working electrode, the counter electrode is a $\varnothing 0.5\text{mm}$ thin platinum wire and the reference electrode is a saturated calomel electrode. All the potentials throughout this work are reported relative to the SCE.

3.2.1 Electron mediator

When looking at single molecule level, it is expected to see the molecule spend half the time reduced and half of the time oxidized when the potential is set to the mid-point potential of the molecule. This is evidenced by equal on- and off-times for the blinking. For reducing potentials the molecule will spend more time in the off state and for oxidizing potentials the molecule will spend more time in the on state. It is therefore important to have a range of potentials that are below and above the mid-point potential of the molecule of interest. In the case of Cu-azurin, the midpoint potential is around 25mV. A solution consistent of a buffer and a redox-pair is needed to act as an electron mediator to obtain the potentials around the mid-point potential of Cu-azurin. A good way to check what range of potentials such solution can reach is the use of cyclic voltammetry (CV) measurement. This is a plot of the current versus the potential. Since the previous setup did not use the potentiostat, the first thing we did for this experiment was using this device to obtain the CV of different solutions to find the one solution that suits this experiment the best.

To obtain the CV of different solutions, a small setup was made. A volume of around 200mL was put on top of magnetic mixer and the working, reference and counter electrode were lowered into the solution and connected to the potentiostat. With this setup, three different solutions were chosen based on its midpoint potential (see below). It is useful to choose a solution with its midpoint potential close to the midpoint potential of the CuAz, since it is easier to reduce or oxidize near the midpoint potential. For obvious reasons, the interesting potentials in this thesis are the potentials around the midpoint potential of CuAz.

1. A solution with ascorbate. Ascorbate, together with ferricyanide, is used in the chemically-induced redox switching setup. The details of the redox of ascorbate is described in more detail in section 3.1.
2. With a midpoint potential of 6mV, the redox couple potassium ferricyanide ($[Fe(CN)_6]^{4-}$)/ferrocyanide ($[Fe(CN)_6]^{3-}$) is a close to perfect candidate for this experiment. The oxidation of ferrocyanide, resulting in ferricyanide is given by

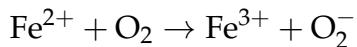


Following the Nernst equation:

$$E = E_{FeCN}^0 - \frac{RT}{F} \log_{10} \frac{[Fe(CN)_6]^{3-}}{[Fe(CN)_6]^{4-}} \quad (3.3)$$

3. The last solution tested was phenazine ethosulfate (PES). Its mid-point potential is 55mV and very close to the documented midpoint potential of CuAz. PES in oxidized state may receive electrons from the electrode to get reduced and in closed vicinity the redox potential is controlled by the concentration ratio of $[PES]_{ox} / [PES]_{red}$.

In the final setup, the total volume of the solution is 4mL. When tried to measure the potential of the ferri/ferro redox couple, a volume of 200-300mL was used. While stirring, oxidizing the redox couple was a fast process. Reducing the ferricyanide, however, took much longer. One explanation could be oxidative stress. Water contains hydrogen in the oxidation state +1 and oxygen in the oxidation state -2. Because of that, the reaction



can occur [?]. This will slow down the production of Fe^{2+} and thus according to the Nernst equation, lower potentials will be reached slower or not at all. Also the setup is not sealed from the air which contains oxygen. In previous voltage-induced redox switching experiments[?] measurements in anaerobic conditions were performed to reduce (in some cases it was reduced to an extend the interaction with oxygen was considered non-existent) the interactions with oxygen. This problem occurred for the other solutions too, but for PES in a lesser extend. Therefore a 200 μM PES in PBS with a total volume of 4mL was chosen as electron mediator in the follow-up experiments.

3.2.2 Proteins on the surface

Having functionalized sample slides and a fitting electron mediator, the next phase in the process to the final setup is to get the right amount of proteins on the sample slide. As mentioned in section 2.5, NeutrAvidin is used as a link between the sample slide and the proteins and has four possible bind spots (Figure 3.3). Before the proteins were applied on the sample slide, they were mixed together with the NeutrAvidin. Different ratios between proteins and NeutrAvidin were tried to find the right ratio. When more proteins bind to the same NeutrAvidin, the proteins will quench due to collisional quenching. The quencher diffuses to the protein during the lifetime of the excited state. Upon contact, the proteins returns to the ground state, without emission of a photon. The protein and quencher must be in contact [?]. The quenched proteins visualizes as blue spots on the sample slide (their lifetime is shorter), as is clearly the case when the ratio between proteins and NeutrAvidin was 1:1 (see Figure

3.4). Lowering the ratio of proteins to the same amount of NeutrAvidin ensures the fact that less protein will bind to the same NeutrAvidin. At some point the probability that the NeutrAvidin is bound to more than one protein is very slim. This is the case when the ratio between protein and NeutrAvidin 1:40 (Figure ??) and this ratio is used in further experiments.

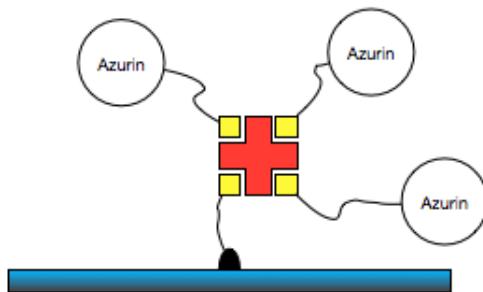


Figure 3.3: Illustration of NeutrAvidin (red cross) bound to three azurin molecules via biotin (yellow). This is likely the cause of collisional quenching.

3.2.3 The working electrode

In an electrochemical system, the working electrode is the electrode of interest. In this case the working electrode is made of gold, since gold is one of the best electron conductors. The reaction of interest is occurring on and near the working electrode in conjunction with the counter electrode and reference electrode. Since the establishment of the redox potential relies on the diffusion of the electron mediator, the actual redox sensed by the molecule is dependent on the distance between the working electrode and the molecule as well as on the time after an external potential is applied. One way to keep the distance between the molecule and working electrode as small as possible is by creating a gold layer on top of the functionalized sample slides with the help a sputtering machine. This gold layer is in touch with the electrochemical analyzer via a $\varnothing 250\text{mm}$ golden wire. By creating transparent areas where proteins are immobilized such that the distance between the gold border and proteins are sufficient small and assuring to apply an external potential long enough, it can be assumed that the potential on the gold is equal to the one in the near surrounding. Using a 20nm thin gold layer gave a lot of problems, however.

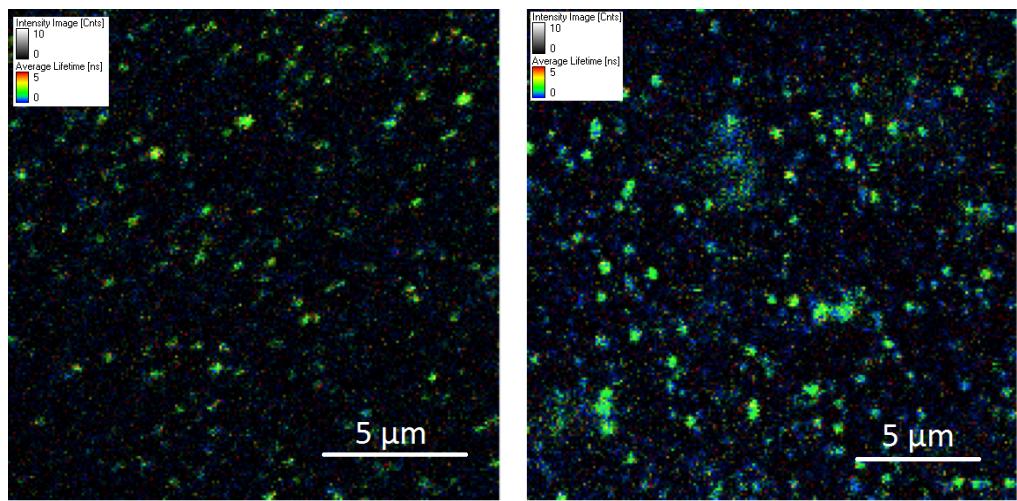


Figure 3.4: A $(20 \times 20) \mu\text{m}^2$ image of immobilised azurin on the sample slide with different ratios of protein to NeutrAvidin. Left: the ratio between protein and NeutrAvidin is 1:1. Right: the ratio between protein and NeutrAvidin is 1:5. When the amount of proteins to NeutrAvidin is decreased, a decreased amount of quenched proteins (blue spots) is observed.

One of the problems to overcome was to find a proper way to create transparent areas in the gold. These areas need to meet some requirements such as a size (usually a cross section of several tens of micrometer) big enough to monitor multiple (20-30) proteins at the same time. Several different methods were tried (see Figure 3.5) and some of them are described hereafter.

1. **Scratches.** The first attempt was sputtering the whole glass slide with a 20nm thin layer of gold. With a needle scratches were made and imaged. When making scratches it is of big importance to not cross other scratches. Once the scratches cross each other, areas of gold that are isolated from the gold layer that is in touch with the wire can be created. The gold will not be connected to the working electrode in that case and no electrochemical changes will be seen near those edges. Once the scratches were made and put under the microscope it was easy to locate the transparent areas. However, the transparent areas created in this way were often too monitor multiple proteins at once. Beside that, the functionalised sample slide happened to get damaged along this process: when making scratches it is difficult to apply the same pressure along the scratches resulting in different depth of scratches. The dimension of proteins are in the nanometers. Different deepness make it impossible to focus on mul-

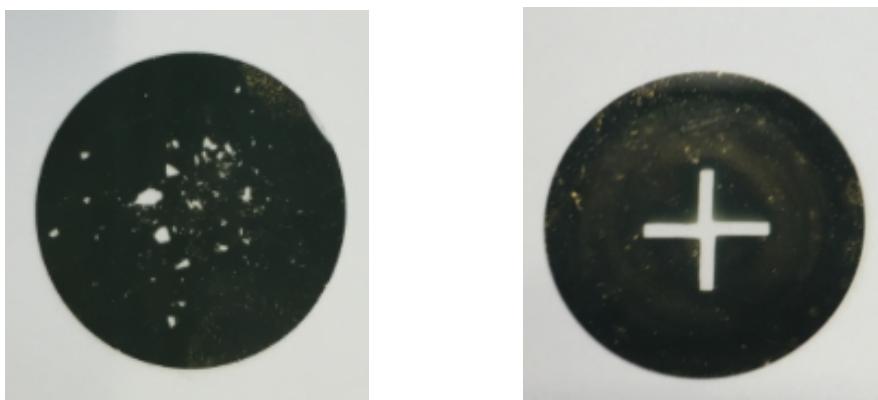


Figure 3.5: A few examples of the $\varnothing 25\text{mm}$ glass slides with a golden layer on top of it. Left: the transparent areas created with the help of small pieces of glass. Right: with the use of small iron crosses a transparent area with the form of a cross was created.

multiple proteins in the same area at once.

2. **Small pieces of glass.** To get areas with the same depth, small pieces of smashed glass were laying on top of the immobilised glass slide before they were sputtered with gold. Once the sputtering was finished, the pieces of glass were removed resulting in small transparent areas (see the left side of Figure 3.5). The borders between glass and gold were sharp (the borders were 'slim' on the images), but again a lot of areas formed via this method were too small to monitor multiple proteins. Later it was done with only a few bigger pieces of glass to avoid these small areas. This showed some improvement.
3. **Metal crosses.** Small metal crosses on top of the glass before sputtering, resulting in cross-like transparent areas (see Figure 3.5). These transparent areas were easy to locate, the edges were straight and the borders were sharp as long as the gold layer was 30 nm thick, see Figure 3.6. If a certain $(80 \times 80) \mu\text{m}^2$ area didn't suit single protein experiments, it is easy to slide along the border to find an area that suits better.

The latter method to create reliable areas is used in the next phase of the experiment: the combination of the electron mediator, proteins and the gold layer. Individually these parts worked as intended. However, a combination of the parts lead to two serious problems:

1. Damaged gold layer. The longer the experiment continued, the more clear it was that the border of the goldlayer would slowly separate.

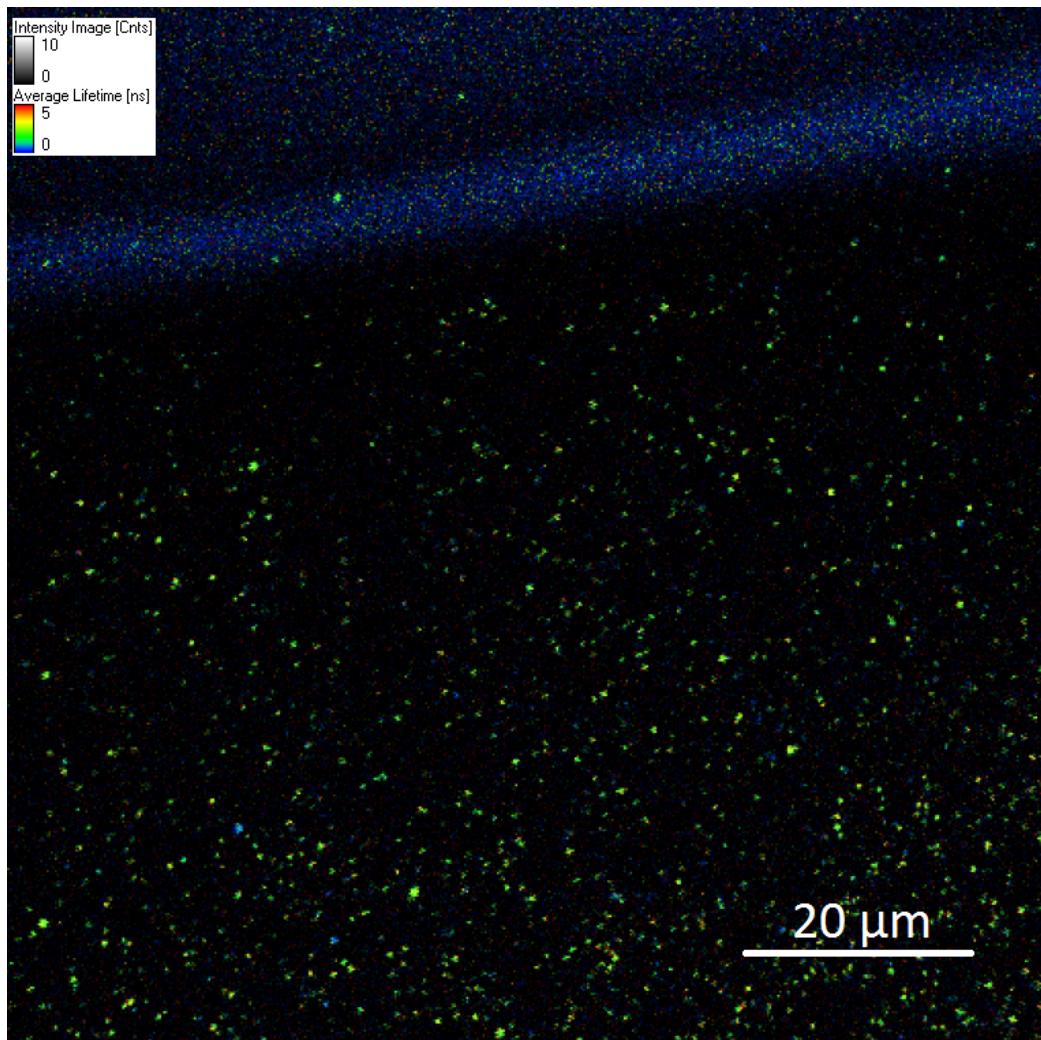


Figure 3.6: $(80 \times 80) \mu\text{m}^2$ image of the slim border. The top part of the image is gold, the bright blue line is the border between the gold and the glass and the green spots below the border is azurin.

At the end of a day of experiments, the gold layer was damaged to such an extend that it would simply separate from the sample slide. The PES is most likely the reason for this. Though the exact reason for this was never clear - when a golden layer was exposed to a different electron mediator (ferricyanide or ascorbate) the gold layer seemed to be not damaged. The damage caused by PES can be seen if you compare the border of the gold layer (bright blue) of Figure 3.8 - taken at the start of the experiment - with the border of Figure 3.7 (this picture was taken towards the end of a day of exper-

iments). One way to tackle this problem, as suggested by one of the professors, would be a protective layer on top of the gold layer. This protective layer is 4-Mercaptobutanoic acid ($C_4H_8O_2S$). This kind of protective layer has been used in similar experiments [?] where it has been shown that the length of the carbon chain can vary without effecting the electron exchange between the gold and the single molecule. In these experiments, however, usually the molecules were on top of the gold layer whereas in our case the proteins are next to the gold layer. The result of using this protective layer was that the proteins did not show any redox, even when different potentials were applied. Since the protective layer did not work, the other way to tackle the damaged gold layer is an increase in thickness of the gold layer. This will not solve the problem, but delay it long enough to do proper experiments. In all previous experiments, the thickness of the gold layer was 20nm. Increasing the thickness of the gold layer led to the second problem.

2. Missing proteins. Near the edges of the working electrode, a much lower density of proteins was observed (see Figure 3.8) once the gold layer thickness was increased. The reason for this could be that during the sputtering of the gold layer, the metal crosses would slightly move a little bit and thus damaging the methoxy-peg-NHS layer. This would make it harder for proteins to bind near the surface. Another explanation could be the fact that some gold-particles might have slipped under the metal cross and taking the spots where the proteins usually would bind.

The final setup: platinum grid

At this point of the process it was clear that the gold-layer as a working electrode in the current setup gave too many problems and a final solution was attempted. Instead of using a gold layer, a single golden wire was kept on the sample slide to see if this would give any good results. This can be seen in Figure 3.9. The green color are the proteins showing switching and blinking. This was the first sign that instead of the golden layer, a (golden) wire as working electrode could do the trick. Finding a single wire with the microscope and keeping it on the sample slide is a tough task and is not controllable and thus a change was needed. Instead of one golden wire, a platinum rectangular grid (the total length/width of the grid is around 2.5cm) is used and pressed on the sample slide with the help of a small glass slide. Not only is the pressure evenly applied on

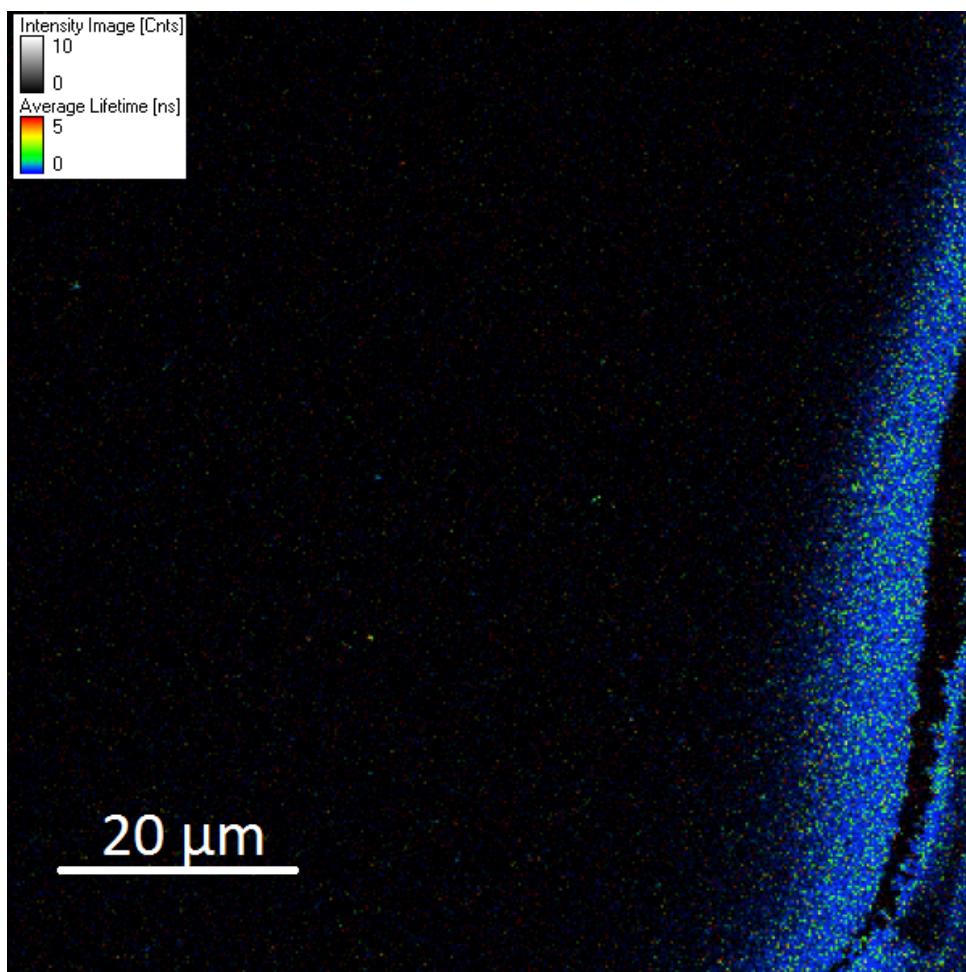


Figure 3.7: $(80 \times 80) \mu\text{m}^2$ of the bright blue border between gold (far right) and glass (left), showing the fractured border due to PES damaging the golden layer.

the grid when pressure is applied on the glass slide on top of the grid, but also small confined volumes are formed where the sample slide and glass slide form the 'floor' and 'roof' and the platinum grid the 'walls'. These confined volumes are in the order of nanoliters, which makes switching possible in a matter of minutes. On top of changing the working electrode, also the electron mediator was changed. Once the setup worked, PES showed more disadvantages such as its very high autofluorescence which makes the ratio signal-to-noise very low. PES is hydrophobic and is difficult to mix with the PBS: it will get stuck on the surface and interacts with the proteins. To avoid these problems a different electron mediator is used in the final experiments. A mixture of 200 μM ferricyanide and 100 μM ascorbate mixed with PBS to a total volume of 4mL. This was the

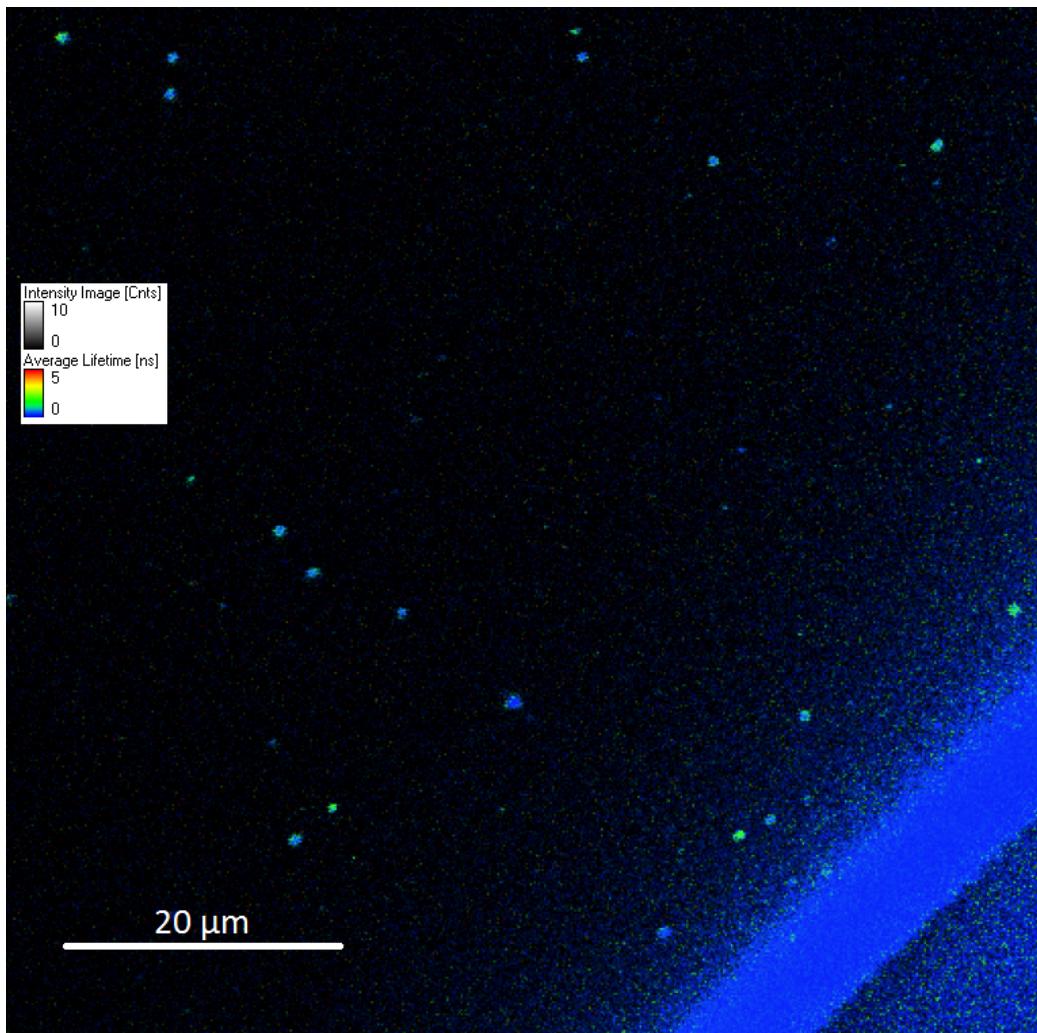


Figure 3.8: The $(80 \times 80) \mu\text{m}^2$ of the glass surface near the 200nm thick golden layer. As can be seen, almost no proteins are present despite using the same molecule densities.

last step in order to make the whole setup work as intended. The setup is schematically drawn in Figure 3.10 with a short description of its parts.

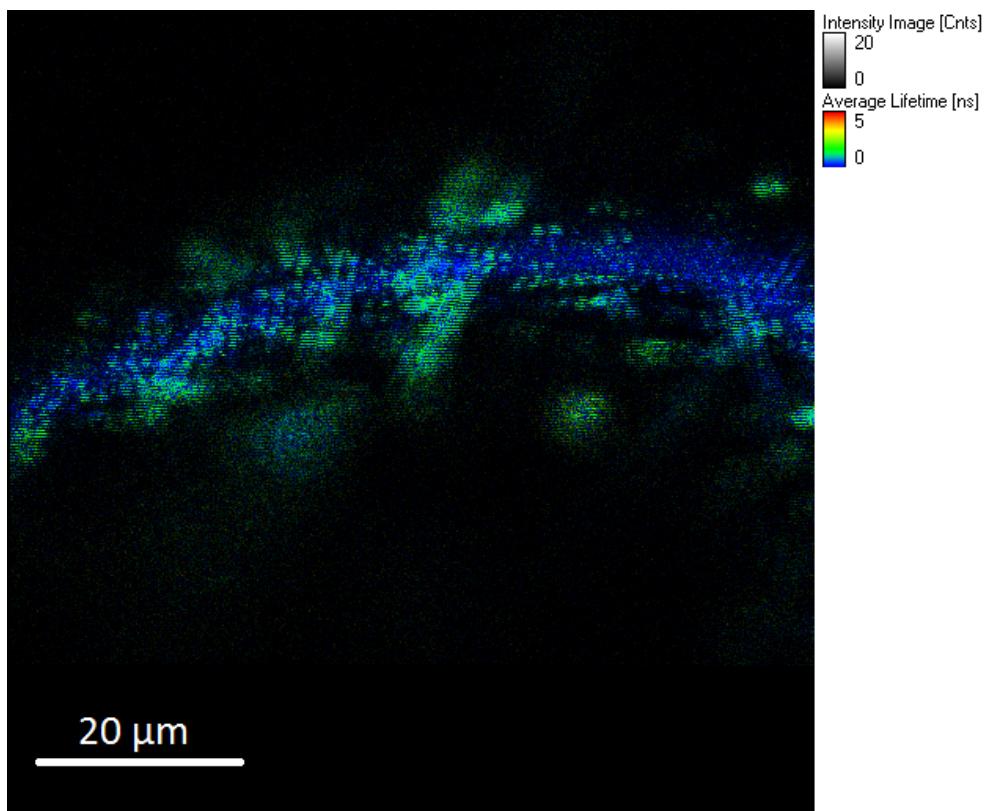


Figure 3.9: A $(80 \times 80) \mu\text{m}^2$ area of the sample slide with immobilized proteins. The blue 'snake' is the golden wire that touches the sample slide. The green spots represent the oxidized proteins. This is the first proof that proteins near the wire show oxidation.

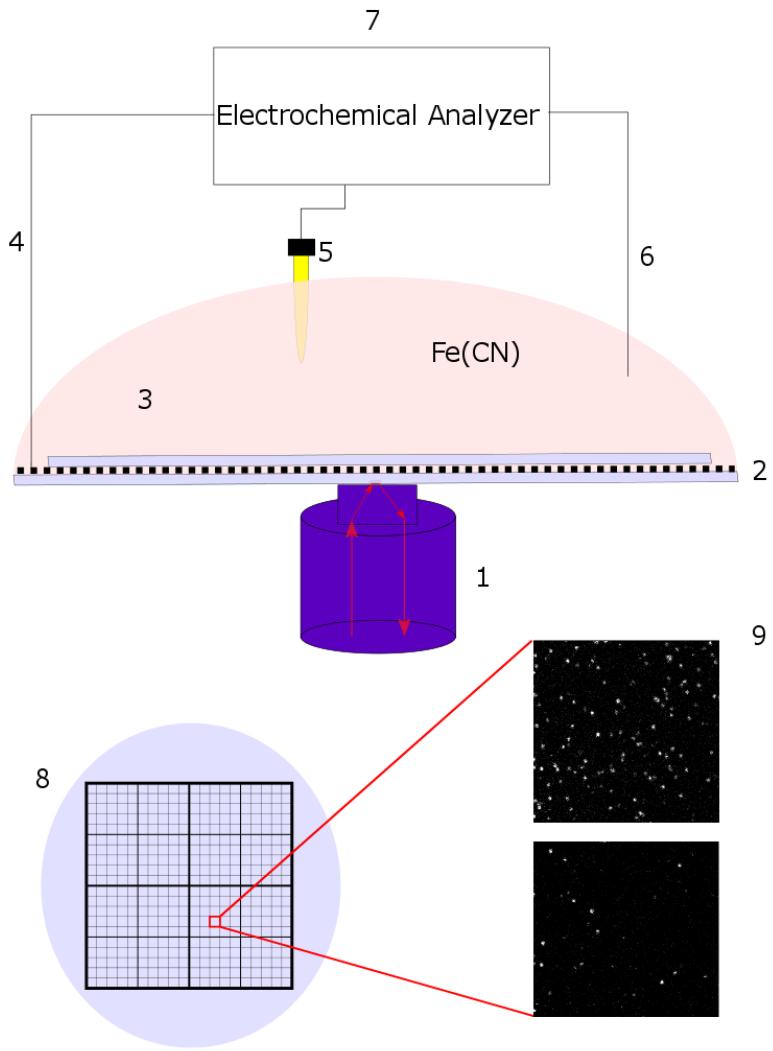


Figure 3.10: Not to scale schematic picture of the final setup in which the potential is changed electrically. (1) The confocal microscope as described at the beginning of this chapter. (2) The functionalized sample slide with on top the platinum grid and another small glass slide to press the grid on the sample slide, resulting in small confined volumes in the order of nanoliters. (3) The electron mediator consistent of $200\mu\text{M}$ ferricyanide, $100\mu\text{M}$ ascorbate and PBS (PH 7.4) with a total volume of 4mL . (4) The working electrode (golden wire) in connection with the platinum grid (section 3.2.3). (5) The saturated calomel reference electrode. (6) A platinum wire, not touching the grid, as the counter electrode. (7) The electrochemical analyzer (Model 800B Series Electrochemical Detector, CH Instruments) to which the electrodes are connected. (8), (9) Top view of the sample slide and two pictures of the same area showing the same CuAz reduced and oxidized.