

Network analysis in EEG data with principal Hessian directions and Ricci flow

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Abstract

The high-dimensional nature of EEG data—especially multichannel EEG—poses major challenges for downstream classification. Uncovering connectivity and network structure between EEG channels can help mitigate the curse of dimensionality when it comes to EEG signal recovery, whether via identifying redundant channels or informing interchannel feature selection. In this paper, we present two complementary methods for inferring network structure and connectivity in EEG data: (1) a new supervised algorithm for inferring classification-relevant community structure based on principal Hessian directions (pHd), and (2) a discrete Ricci flow-based unsupervised community detection algorithm. We demonstrate these systematic methods on both small-scale and larger-scale high-dimensional EEG datasets involving classifying imagined digits versus non-digits and detecting emotional valence. Beyond inferring underlying connectivity structure, we show that combining the information extracted via Ricci flow and pHd can enable improvements in downstream EEG signal recovery.

All supporting code stored in personal GitHub repository — also viewable at bit.ly/feb3_meeting.

1. Introduction

EEG data often exhibits high-dimensionality due to fast electrode sampling rates, substantial channel counts, and the time-intensive process of EEG data collection [1-3]. As a result, the number of features per sample in an EEG signal recovery context can far outstrip the number of samples themselves (i.e., $d >> n$) [4][5]. This high-dimensionality introduces several significant challenges in signal recovery and classification tasks. Overfitting, a well-documented problem when training classification models on neural data [6][7], can be particularly severe in high-dimensional settings; models can capture noise and spurious training data patterns, leading to poor generalization on unseen data [8]. This overfitting risk is even further exacerbated in the context of EEG, where the signal-to-noise ratio is already low due to various physiological and external artifacts [9-13]. Moreover, the redundant and highly-correlated features common in multichannel EEG data can obscure meaningful patterns, making it difficult to isolate the signals that are truly indicative of different cognitive states or conditions [14][15]. Model interpretability also suffers in high-dimensional settings [16-18], making it challenging to derive meaningful neuroscientific insights from the classification models. Ideal EEG classification systems not only perform well but also provide clear explanations of feature importance and interactions [19-21], which is difficult to achieve when dealing with thousands of (potentially collinear) features [17][18]. Uncovering structure in high-dimensional EEG data is thus crucial for many practical applications.

Beyond classical algorithms for general dimensionality reduction and feature selection like Principal Component Analysis (PCA) and minimum-redundancy-maximum-relevance (MRMR) [22][23], several studies have presented methods for creating effective embeddings of high-dimensional EEG by exploiting the underlying relationships between different EEG channels [24][25]. By detecting redundancy and collinearity among EEG channels while elucidating interchannel features carrying signal, developing methods to analyze network structure in EEG can lead to meaningful low-dimensional embeddings—and more robust downstream classification. In this vein, Behrouzi et al., 2022 and Choi, 2024 demonstrated that feeding graph embeddings of EEG data into downstream graph convolutional network (GCN)-based architectures led to superior test classification performance [26][27]. Similarly, Wang et al., 2022 showed that integrating graph topology information into EEG features led to performance increases on EEG classification tasks [28].

These recent strides in systematic, automated frameworks for graph-based EEG embeddings [26-28] build upon a significant body of literature on functional connectivity (FC) [29-35]. Traditional methods for inferring relationships between EEG channels exploit conventional hemispheric relationships [36-38]; for example, several studies present methods grounded in hemispheric asymmetry for informing classification model features [38-42]. However, traditional connectivity methods reliant on established EEG electrode placements may fail in cases of electrode displacement or dislocation, to which traditional EEG setups are

highly susceptible [43][44]. Similarly, preprogrammed models that rely on fixed assumptions about EEG relationships may overlook transient or task-specific patterns, which can be critical for understanding neural dynamics in real-world and clinical settings [45-47]. These shortcomings highlight the need for data-driven approaches that can adaptively capture connectivity structures.

Conventional data-driven methods for inferring functional connectivity in EEG include pairwise correlation [48], coherence [49], and Granger causality (in directed cases) [50]. While effective, these methods can fail to account for broader network topology in EEG and evolving dynamic patterns [51-54]—recent studies have shifted toward more elaborate algorithms for functional connectivity inference. For example, Pellegrini et al., 2023 proposed a flexible approach using beamforming for identifying EEG connectivity [53], while Xu et al., 2024 demonstrated EEG network-based preprocessing methods using a wavelet transform on musical EEG data [54]. These studies provide promising evidence for the utility of EEG connectivity and network analysis. Notably, we mark a distinction between versatile embedding or preprocessing methods designed to be applied to various settings and different downstream model architectures [55-57], and efforts aimed at developing state-of-the-art (SOTA) models themselves; the latter category includes many notable studies that focus on the development of SOTA neural network classification architectures rather than solely on upstream network analysis methods [58-60]. As opposed to building neural networks for EEG classification, the focus of this research is on demonstrating useful network analysis and embedding techniques.

In this vein, we propose two complementary methods for inferring network structure in EEG data. First, we present a novel application of the principal Hessian directions (pHd) method, first proposed by Li in 1992 [61], geared toward signal-relevant community detection among EEG channels. The pHd method, which identifies directions in the input space that exhibit significant curvature of a response surface, has been demonstrated on many applications involving dimensionality reduction, signal recovery, and visualization [61-64]. In this study, we extend the existing body of pHd literature by applying pHd to a novel community detection context. Our proposed method computes the pHd for each individual EEG channel with respect to the signal (here, in a classification setting) and evaluates the alignment of the principal Hessian direction across channels to identify signal-relevant communities. Though originally formulated for dimensionality reduction, we hypothesize that the pHd-based network analysis method presented herein can offer supplemental information that improves downstream signal recovery performance and can be applied systematically across different EEG preprocessing and connectivity contexts.

Second, emerging literature on graph processing [65-67] has highlighted the discovery of Ricci flow as a new SOTA technique for community detection that outperforms classical Louvain and Spectral Clustering counterparts [67-69]. Recent studies leveraging discrete analogs of the Ricci flow tailored toward graphs based on Ollivier’s notion of Ricci curvature have demonstrated promising results on applied clustering problems [67-71], and in this study, we present the first large-scale application of the Ricci flow for community detection

on EEG data. Beyond inferring mere adjacency relationships, we anticipate that unsupervised partitioning of EEG channels into communities will enable the discovery of complementary structure in conjunction with the aforementioned pHd method. More specifically, by exploring where the pHd communities overlap with and depart from the Ricci flow communities, we can identify both redundant (in the overlapping case) and subtly informative (in the departure case) interchannel relationships for signal recovery.

2. Methods & Results

We demonstrate our network analysis methods on two real-world EEG datasets: a small-scale EEG dataset on imagined digits (*MindBigData*) from Vivancos et al., 2022 [72] and a larger-scale EEG dataset on emotional valence (*SEED*) from Duan et al., 2013 [42, 73]. Both datasets are high-dimensional, and for the purposes of demonstrating our pHd method, center around classification tasks: we explore classifying imagined digits versus non-digits in a preliminary *MindBigData* setting, and later extend our methods to detect positive versus negative emotional valence in the *SEED* dataset.

2.1 Initial Demonstration

As a proof-of-concept, we first apply our proposed network analysis methods to imagined digit versus non-digit classification on small-scale 14-channel (Emotiv EPOC) data from Vivancos et al., 2022 [72]. This initial dataset was selected due to its high-dimensional nature and relative simplicity; we employed balanced digit and non-digit classes of two-second segments ($n=300$) with 14 channels at 128 Hz.

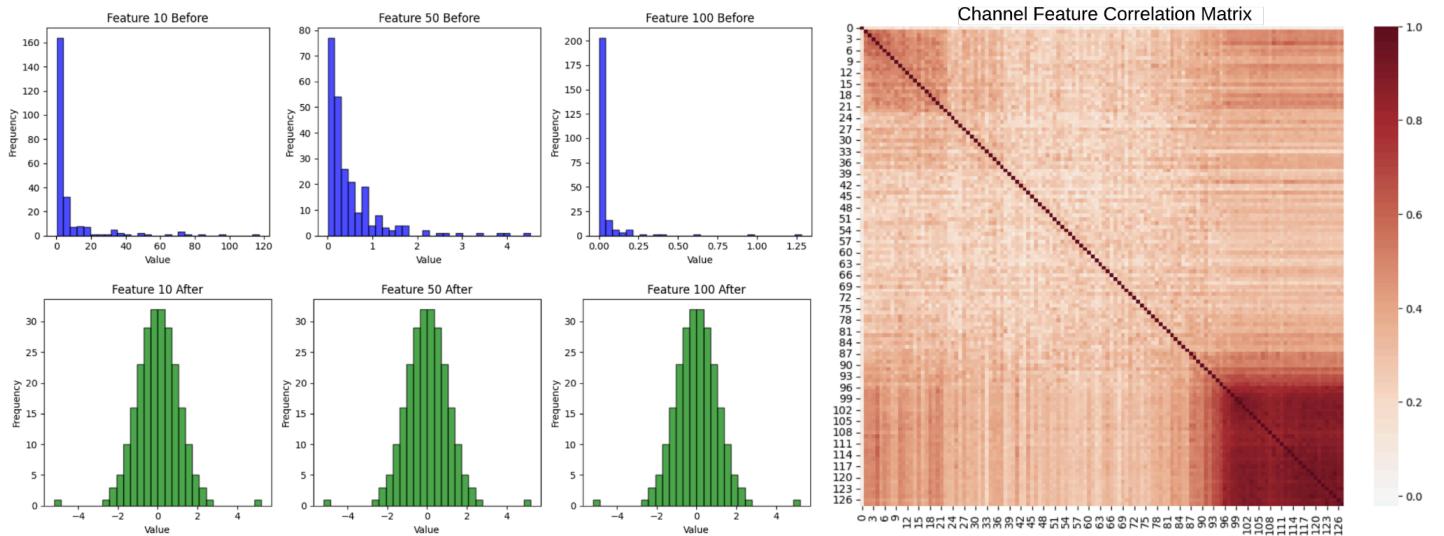


Figure 1: Power spectrum features before (upper left) and after Gaussianization (lower left); feature correlation matrix (right).

Here, we present a first-of-its-kind pipeline for implementing principal Hessian directions on multichannel EEG data. As our aforementioned notion of pHd alignment relies on the assumption of meaningful

features with respect to the classification problem, we cannot leverage our initial data existing in the temporal domain as arbitrary timestamps on temporally-invariant signals convey no classification-relevant information. Thus, we apply a fast Fourier transform (FFT) to obtain a power spectrum (selecting only positive frequencies to avoid redundancy) for each channel in every sample. Since each individual EEG channel now conveys comparable class-relevant frequency data, we can viably apply our alignment notion. Note that all network analysis methods are performed on a partitioned training dataset (in this case, with a 4:1 train-test split) in order to prevent data leakage.

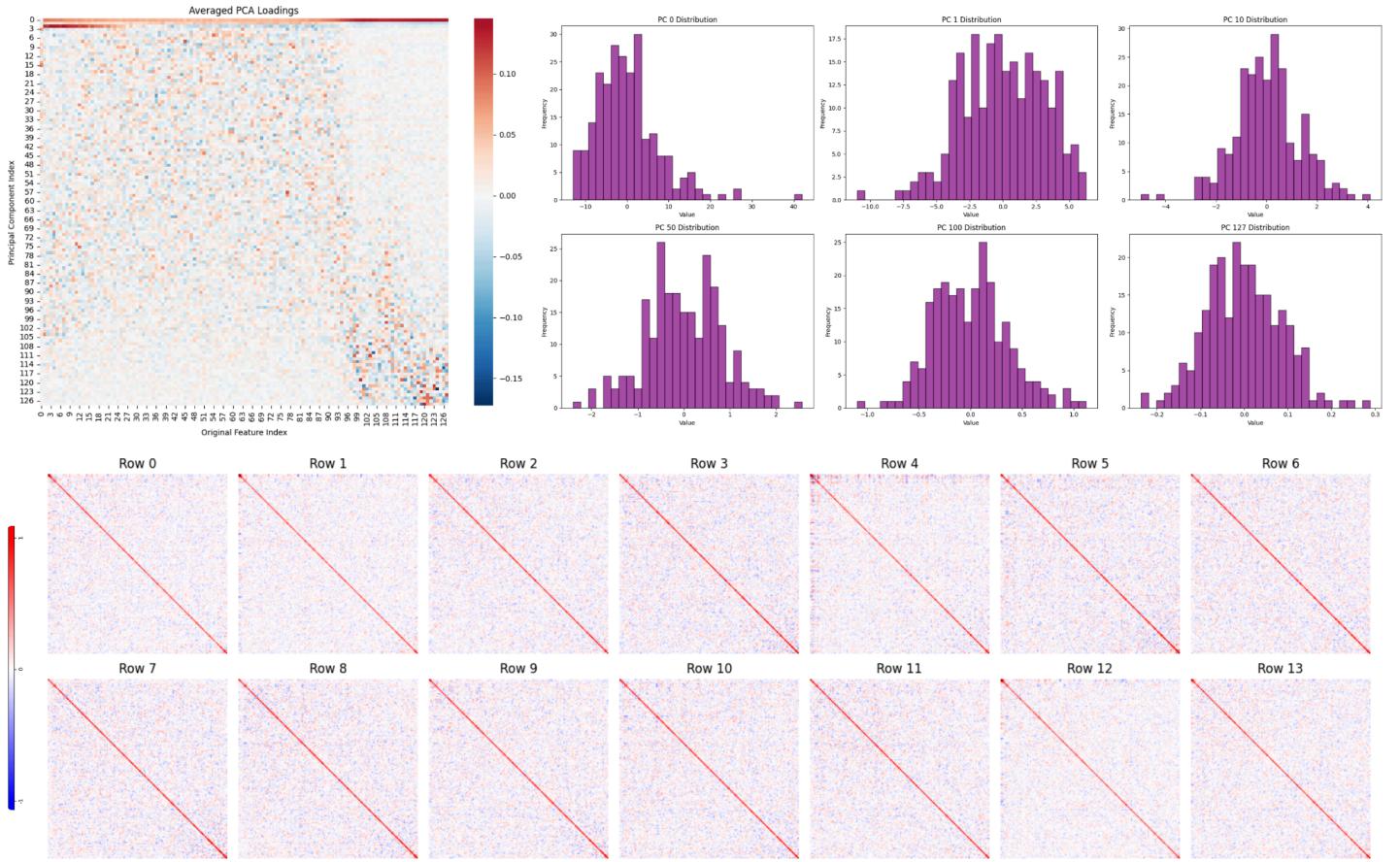


Figure 2: Averaged principal component loading matrix (upper left), feature distributions after principal component transformation (upper right), final feature correlation matrices for each EEG channel (bottom).

Notably, in order to leverage the classical technique with theoretical guarantees for estimating principal Hessian directions using Stein’s lemma [61], we also require features to be independent and identically distributed normal random variables with mean 0 and identity covariance. As shown in Figure 1, this is certainly not the case in our initial setting—power spectrum bins are not normally distributed across individual channels (Figure 1, left panel), nor are they empirically uncorrelated (Figure 1, right panel). We thus propose and demonstrate the following first-of-its-kind algorithm for pHd preprocessing in EEG data: (1) Gaussianize individual power spectrum features, (2) perform PCA with whitening on each individual channel, (3) aggregate and apply the same averaged set of PC loadings to transform every channel, and (4) renormalize the

transformed features using identical cross-channel parameters with a new optimization based on the Kolmogorov-Smirnov normality test. This systematic process is designed to enable downstream application of conventional pHd estimation leveraging the theoretical guarantees of Stein's lemma [61].

Initial Gaussianization is performed using a 100-bin quantile transformer on each power spectrum feature. While PCA could theoretically eliminate each channel's cross-feature correlation shown in Figure 1 (right panel), we cannot apply 14 different PC loadings to 14 different channels as this would disturb our goal to detect meaningful pHd alignment. Crucially, we must apply the same set of loadings to each channel so that the resulting PC-based features convey the exact same frequency information across different channels—otherwise, the pHd vectors would not have one-to-one comparable features. We rectify this concern by performing individual PCAs on each channel and then averaging the PC loadings (Figure 2, upper left panel) to form a single transformation matrix. This same averaged loading matrix is then applied to transform each EEG channel. While this does sacrifice the goal of perfectly uncorrelated features, we achieve our aim of ensuring meaningful comparability—and can observe empirically that this aggregated transformation yields approximately uncorrelated final features across each individual channel, as desired (Figure 2, lower panel).

However, we also empirically observe that the PC transformation has perturbed the gaussianity of our original features (Figure 2, upper left panel). Again, we cannot merely transform each channel's features individually as our features now represent combinations of frequencies as determined by the PC loadings—each feature must undergo the same transformation across all 14 channels in order to preserve our alignment notion. To rectify this concern, we developed a new Kolmogorov-Sminrov (KS)-based optimization method.

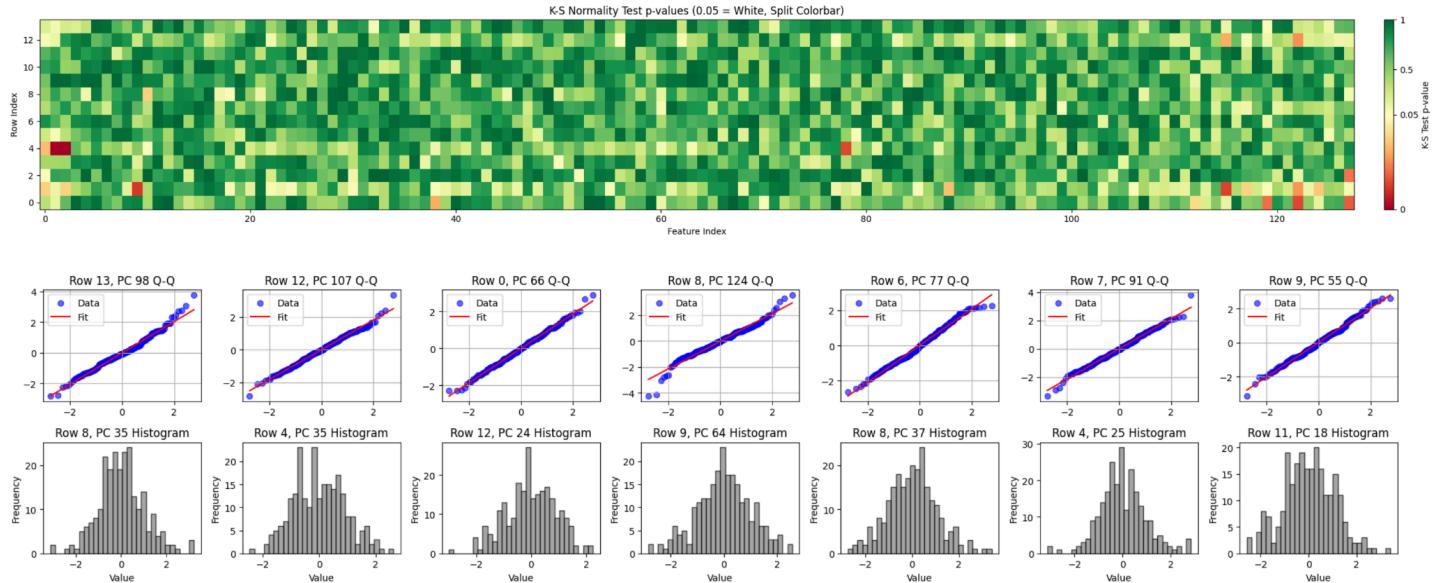


Figure 3: Results of the Kolmogorov-Smirnov normality optimization; p-values are plotted in the upper panel, with red denoting statistically significant deviations from normality while green denotes p-values above 0.05. The lower panel depicts quantile-quantile (Q-Q) normality plots and histograms for randomly selected features.

Our KS-based method attempts to achieve approximate standard normality across PC-perturbed feature distributions by applying a Z-score transformation for each feature across all 14 channels. As mentioned, the algorithm must apply the same two transformation parameters (mean μ and standard deviation σ) across all 14 channels—meaning that tradeoffs between channels when it comes to normality are inevitable. In order to ensure a systematic process maximizing overall normality, we attempt to maximize the average KS normality test p-value across all 14 channels for each PC-transformed feature using the L-BFGS-B optimization algorithm as proposed by Zhu et al., 1997 [74]. As shown in Figure 3 (upper panel), our optimization enables us to achieve a resulting feature set with relatively minimal statistically significant deviations from normality.

After completing our feature transformation, we then apply the pHd method by computing the principal Hessian direction with respect to the classification problem: labels are set to +1 for imagined digits and -1 for imagined non-digits. To obtain alignment information, we performed the pHd method on each individual channel. Per convention, we multiplied labels with the outer product of each feature vector and took the leading eigenvector of the resulting matrix. We then computed the correlation between each EEG channel's leading eigenvector to arrive at the final pHd alignment matrix for the dataset (Figure 4, upper left panel).

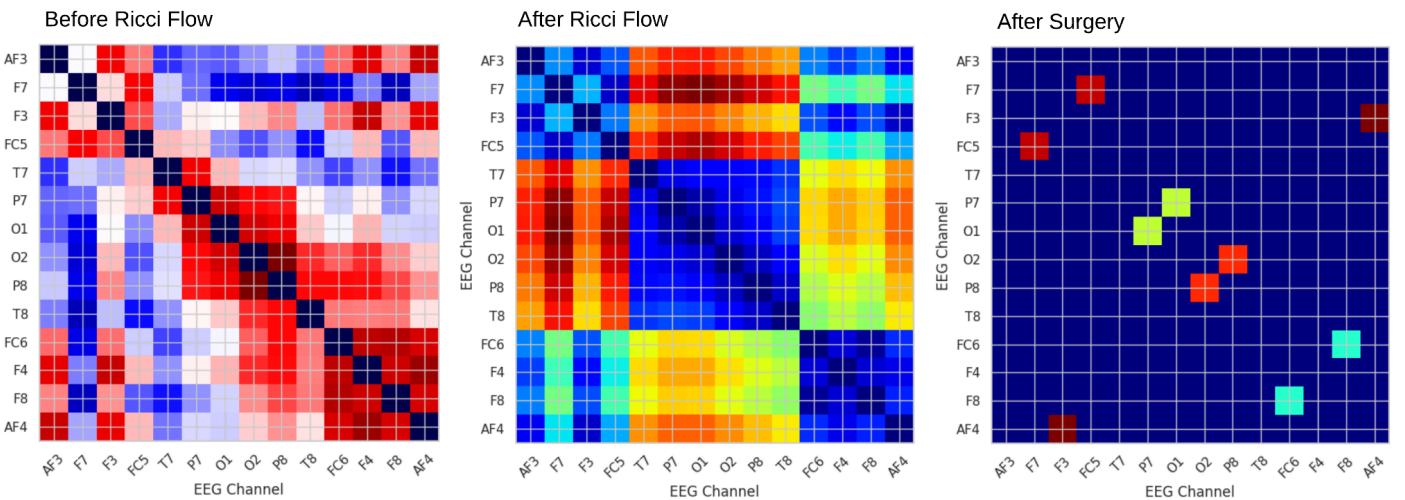
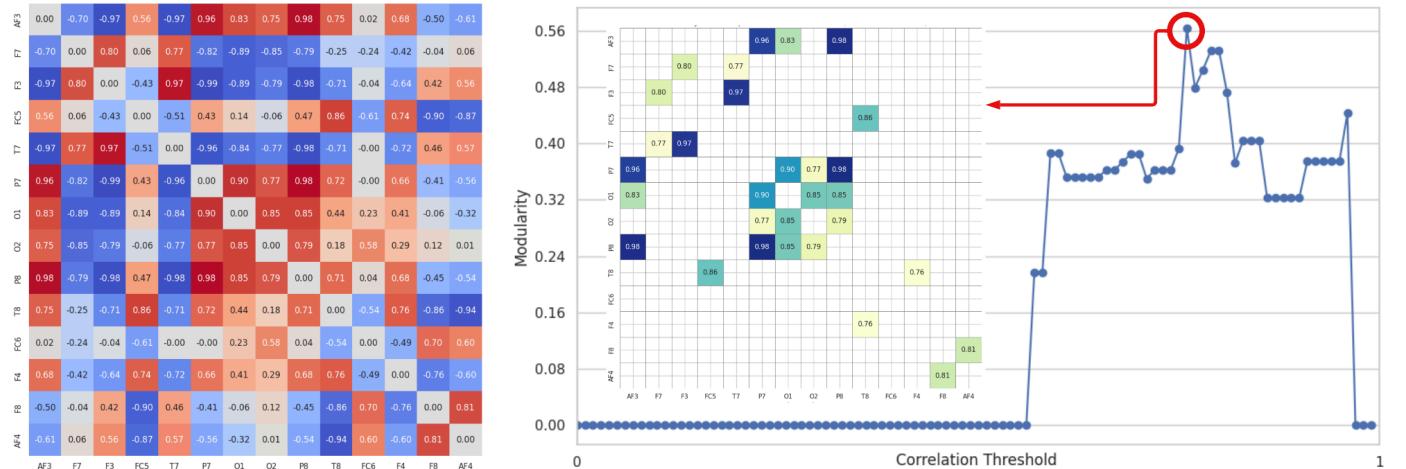


Figure 4: Results of both the principal Hessian directions-informed community detection algorithm (upper panels) and the Ricci flow-informed community detection algorithm (lower panels) on the initial 14-channel imagined digit versus non-digit dataset. The upper left panel depicts the pHd alignment matrix, while the upper right panel depicts the process of iteratively increasing the alignment (correlation) cutoff threshold and taking the adjacency matrix with maximum modularity. From left to right, the lower panels depict: (1) adjacency before Ricci flow, (2) adjacency after Ricci flow, and (3) partitioned communities after surgery.

To compute the pHd-informed community partitions, we started with the initial correlation-based adjacency matrix and iteratively increased the correlation cutoff value needed to maintain an edge between two channels. We then computed the modularity of all possible partitions and systematically took the set of communities with maximum modularity (as shown in Figure 4, upper right panel).

As discussed, we then shifted toward our complementary unsupervised community detection algorithm applying the Ricci flow. Building upon methods demonstrated in Sia et al., 2019 [67], Tian et al., 2023 [68], and Choi, 2024 [27], we used inter-channel correlation to initialize a weighted adjacency matrix and then applied the Ricci flow to the weighted graph using Ollivier’s notion of Ricci curvature [75]. We then evolved the weights of the graph using the Ricci flow and then performed “surgery” by cutting the graph’s heavily weighted edges [27, 67-68], using all unique cut ratios within two standard deviations of the total number of edges in order to obtain an exhaustive list of possible partitions while avoiding trivial scenarios (e.g., graphs with almost zero edges). We then obtained our final graph by selecting the community partition that maximized network modularity, as depicted in the bottom panel of Figure 4. Careful analyses and evaluations of the complementary pHd and Ricci flow community partitions are discussed in Section 2.3.

2.2 Higher-Dimensional Extension

After successfully demonstrating our network analysis methods on the 14-channel *MindBigData* case [72], we then applied our pHd and Ricci flow analyses to an even higher-dimensional setting: the 62-channel *SEED* dataset [42, 73], which we partitioned using a 9:1 train-test split. While our initial imagined digit versus non-digit demonstration involved two-second samples at 128 Hz, the SEED dataset enables network analysis across 130 seconds at 200 Hz. Our pHd-informed network analysis on SEED involves signal recovery related to positive versus negative emotional valence, with 450 total samples each containing 62-channel time series data obtained from 15 different subjects.

As with the 14-channel demonstration, we applied the same FFT, Gaussianization, and averaged PC loading pipeline. Notably, as the number of features per channel outstripped the total number of samples (13,000 versus 405), we reduced the dimensionality in the PC loading step to 405 frequency features before applying KS optimization. To further account for the high dimensionality of the dataset and the resulting high number of relatively uninformative features, we also harmonically weighted the pHd features when computing correlation—features based on prominent PCs were weighted higher when determining channel alignment to account for the $d \gg n$ nature of the dataset. The resulting pHd-informed community detection process is depicted in the upper panel of Figure 5. As before, we also systematically applied the discrete Ricci flow

algorithm for complementary unsupervised clustering, as depicted in Figure 5 (lower panel). An evaluation of the combined network analysis and community detection on SEED is explored in Section 2.3.

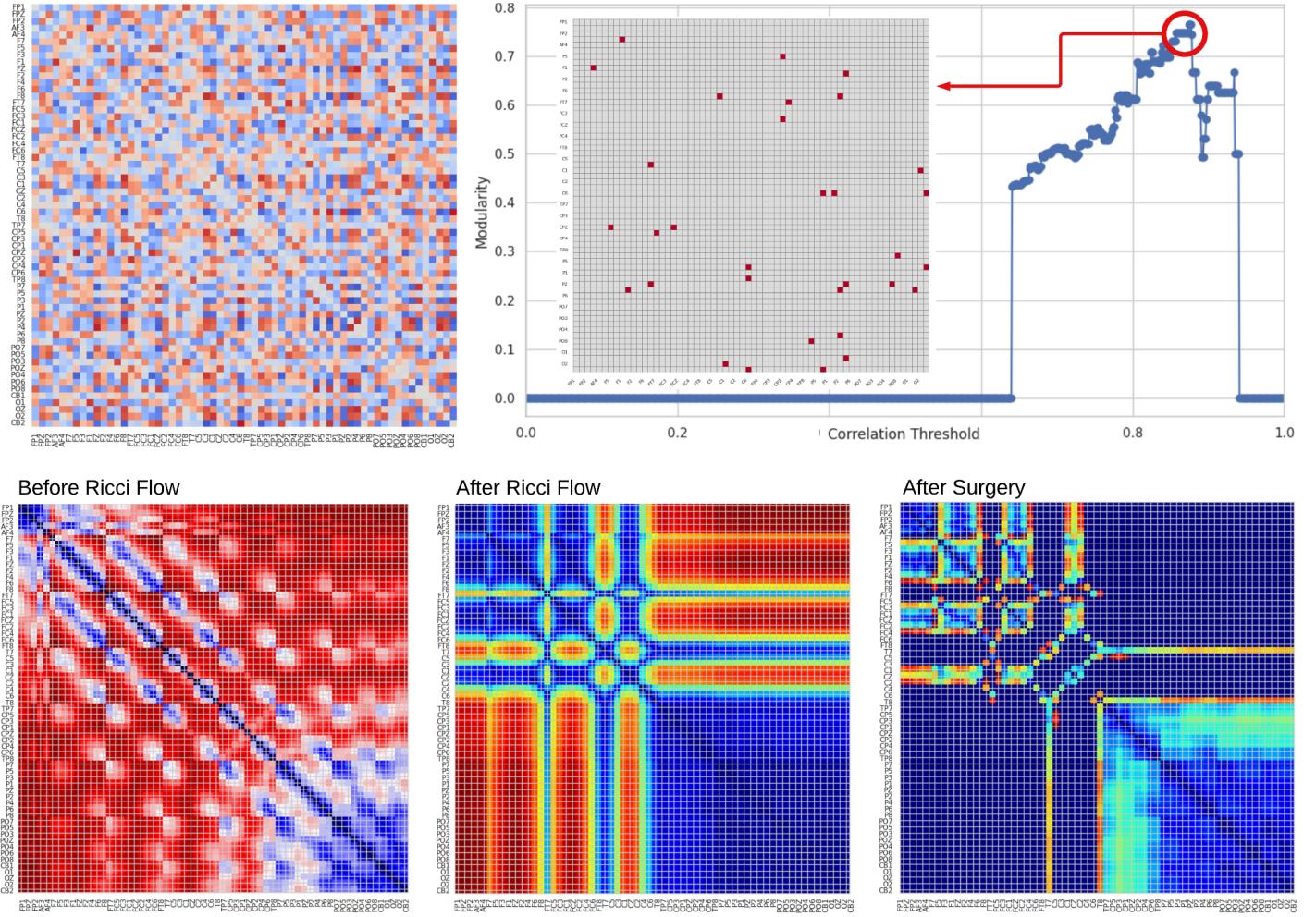


Figure 5: Results of both the principal Hessian directions-informed community detection algorithm (upper panels) and the Ricci flow-informed community detection algorithm (lower panels) on the 62-channel SEED dataset for emotional valence detection. The upper left panel depicts the pHD alignment matrix, while the upper right panel depicts the process of iteratively increasing the alignment (correlation) cutoff threshold and taking the adjacency matrix with maximum modularity. From left to right, the lower panels depict: (1) adjacency before Ricci flow, (2) adjacency after Ricci flow, and (3) partitioned communities after surgery.

2.3 Analyses

The pHD and Ricci flow-informed communities across all datasets and clustering methods were designed to maximize modularity in correspondence with conventional methods for optimal community detection [76-79]. Beyond merely providing interpretable insights into connectivity, however, we conduct a thorough demonstration of the comparative utility of our network analyses.

Crucially, our pHD and Ricci flow methods are built to be complementary. The unsupervised community detection enabled via Ricci flow allows for the identification of channel groups with similar outward characteristics, while the signal-relevant pHD method identifies groups that convey similar information with

respect to the classification problem. By identifying nodes that are in the same Ricci flow-informed group but not in the same pHd-informed group, we can detect subtly-informative EEG channel relationships—channels that appear similar but fundamentally convey different information. To exploit this relationship, we can transform these subtly-informative channel pairs into new features describing the difference between the two channels in frequency space. Similarly, by identifying nodes that are in the same Ricci flow-informed group and in the same pHd-informed group, we can detect nodes that are fundamentally redundant and thus can be reduced without significant information loss by averaging their frequency content. Graphically, this combined analysis is depicted in the upper right panel of Figure 6; in the 14-channel imagined digit versus non-digit case, we identify two pairs of subtly informative nodes (third chart, in blue) and two pairs of redundant nodes (third chart, in red). To avoid information degradation, we do not replace standalone channels in singleton pHd communities with differential features; similarly, to ensure consistent application in the more complex 62-channel case, we average redundant nodes first before looking for subtly-informative pairings. Application of our combined analysis to the 62-channel case yielded two subtly informative channels and 19 channels with redundancies. This methodical combined framework allows for stable information to be derived across many EEG settings and signal recovery scenarios.

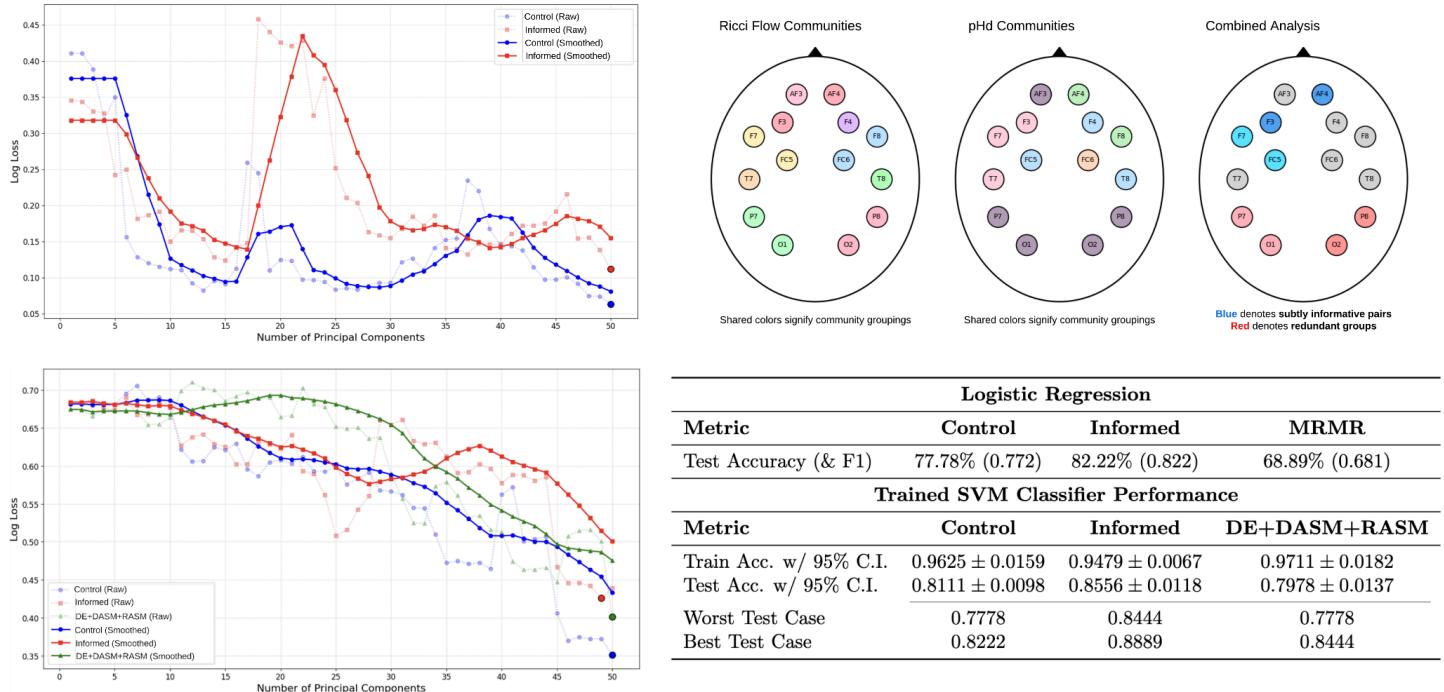


Figure 6: Supplemental results of our combined analysis methods across both datasets (*MindBigData* in the upper panels, *SEED* in the lower panels). The upper left panel depicts a performance (loss) comparison between an informed PC logistic regression (blue) and a control PC logistic regression (red). The upper right panel depicts Ricci flow- and pHd-informed communities and the resulting subtly informative and redundant relationships. A PC logistic regression on *SEED* is depicted in the lower left panel, with three depicted performance curves: control (red), informed (blue), and the conventional hemispheric DE+DASM+RASM method (green). SVM classification test results using the control, informed, and DE+DASM+RASM features are depicted in the lower right panel.

We conducted multiple careful analyses across both datasets to ensure that the derived relationships were legitimately informative. On the imagined digit dataset, we conducted two logistic regressions—one with the pHd and Ricci-informed features (reducing redundant and subtly-informative rows), and one without as a control. We found the control regression achieved a mean test log loss of 0.228 with standard error (SE) 0.144 (corresponding to a test accuracy of 95.0%), while the informed regression achieved a mean test log loss of 0.0474 with SE 0.0181 (and perfectly classified all test cases). Given the high dimensionality of the dataset, however, we also conducted principal component logistic regressions based on the informed vs. control feature sets (both with frequency domain features), plotting mean log loss on the test set versus the number of PC features used in the regression. As visualized in the upper left panel of Figure 6, we found that the pHd and Ricci flow-informed logistic regression demonstrated more stable test performance as the number of PC features increased compared to the control. The best global performance (marked by a colored dot in Figure 6, upper left panel) was also superior for the informed PC regression compared to the control.

To corroborate these preliminary results achieved on the simpler MindBigData case, we conducted multiple analyses of the utility of the pHd- and Ricci flow-informed network analysis on the SEED dataset. Our initial logistic regression test revealed that our informed preprocessing method led to superior accuracy compared to both an uninformed control regression and a minimum-redundancy-maximum-relevance (MRMR)-informed regression (see Figure 6, lower right panel). The expanded channel count in SEED also enabled comparison with the highly-cited differential entropy (DE), differential asymmetry (DASM), and rational asymmetry (RASM) method for preprocessing [42]. When applied to the aforementioned PC logistic regression test, we found that the pHd- and Ricci flow-informed method again achieved the best global performance and empirically demonstrated relatively strong performance across PCs compared to the two alternatives (Figure 6, lower left panel).

To further assess the utility of our pHd- and Ricci-flow informed analysis and preprocessing, we trained ten kernel SVMs (via grid-searching identical parameter grids) on SEED on each of the three feature sets: control, informed, and DE+DASM+RASM. We found that our informed preprocessing method outperformed the other two methods by a statistically significant margin (Figure 6, lower right panel).

3. Discussion

We present a novel application of the principal Hessian directions method for community detection on EEG signals. It is important to note, however, that our use of pHd involves approximations and tradeoffs related to covariance and gaussianity; while we validate our method via the aforementioned studies on the utility of the pHd-informed network analysis, further testing will be required to determine the position of pHd within broader bodies of neural engineering and community detection literature. While our pHd application pipeline has the

advantage of being systematic, we note that the principal component vector computation may become intensive in settings with exceedingly large numbers of samples and features; they are, however, relatively suitable for high-dimensional applications with small n and thus fewer computable PCs. Further generalization to broader settings may require setting PC cutoffs via eigenvalue scree plots or iterative eigenvector estimation methods. The K-S optimization method used for preprocessing also introduces a potential bottleneck in large settings via its use of L-BFGS-B [74], as the number of features needed to be optimized is equivalent to the length of a channel and must be optimized over the number of channels. Follow-up studies may explore shortcut heuristics for computing constant normalization parameters across channels (e.g., taking simple or weighted averages of μ and σ parameters across channels).

Given that Ricci flow-based clustering algorithms have been shown to outperform SOTA clustering algorithms in recent literature [67-69], our use of Ricci flow for EEG network analysis is designed to be both a first-of-its-kind extended application and an intentional taxonomic choice for providing unsupervised clustering information in conjunction with pHd. As our Ollivier-Ricci curvature-based clustering algorithm is computed once across a single correlation-initialized graph (with node count equal to EEG channel count), the use of Ricci flow described herein is unlikely to prove prohibitively intensive for EEG applications, which rarely exceed 256 channels. However, we do note that the complexity of the Ricci flow community detection algorithm is typically quadratic due to the Sinkhorn-based computation [80] of Wasserstein distance for Ollivier Ricci curvature [68]; if necessary, potential linear-time approximations can be implemented as discussed in Tian et al., 2023 [68].

Our analyses in Section 2.3 demonstrate the utility of our complementary pHd and Ricci flow-informed network analysis methods. As mentioned in the Introduction, we emphasize that the objective of this study is not to build a SOTA classification model or to overperform EEG benchmarks for specific classification tasks. Rather, we aim to demonstrate useful preprocessing and analysis methods that can be used across diverse applications or combined with a variety of SOTA classifiers downstream. Our preprocessing methods are intentionally light and avoid thoroughly transforming features (instead averaging doubly-redundant channels, transforming subtly-informative relationships into differential features, etc.) in order to provide breathing room for subsequent combination with use-case-specific classification techniques. Through this study, we hope to expand the toolkit of EEG preprocessing methods by providing a systematic analytical framework for classification-relevant network analysis.

Though outside of the scope of this demonstration, we also note that as our derived relationships are grounded in terms of well-defined EEG channels, our methods confer potential advantages in the realm of interpretability. As opposed to methods like PCA, which may obscure direct interpretation of channel contributions by aggregating information into principal components, we instead establish plain, interpretable relationships that elucidate both channel-specific similarities and the roles of individual nodes in conveying

critical information. This explainability could potentially foster positive interactions with downstream regression coefficients; as an aside, we noted several shifts in regression coefficient weighting between control and informed models during testing. For example, FC6 features were heavily weighted in the 14-channel control model, while weights were more evenly distributed across transformed channels in the pHd- and Ricci flow-informed model (with the subtly-informative F3-AF4 relationship weighted strongest). It is crucial, however, to caveat this observation—there are strong limitations to coefficient interpretability given collinearity [81], and we make no formal assertions. Follow-up studies combining our methods with downstream explainable machine learning techniques could shed light on any hypothetical interpretability advantages.

We emphasize that while our study demonstrates potentially useful network analysis and preprocessing techniques for EEG data, results are preliminary and there are important limitations. While we evaluate our data on both 14-channel and 62-channel data across 45 subjects, further studies involving out-of-laboratory data collection will be necessary to assess whether the pHd- and Ricci flow-based methods remain useful in noisy real-world EEG conditions. Furthermore, collecting EEG data from human subjects across longer timeframes may also reveal whether the derived network relationships remain persistent or need to be continuously reevaluated. Moreover, we have no evidence on how these methods would perform in non-EEG neural signal recovery settings (e.g., fMRI or fNIRS data), nor do we investigate their effectiveness in cross-modal tasks involving the integration of multiple neural data types.

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