

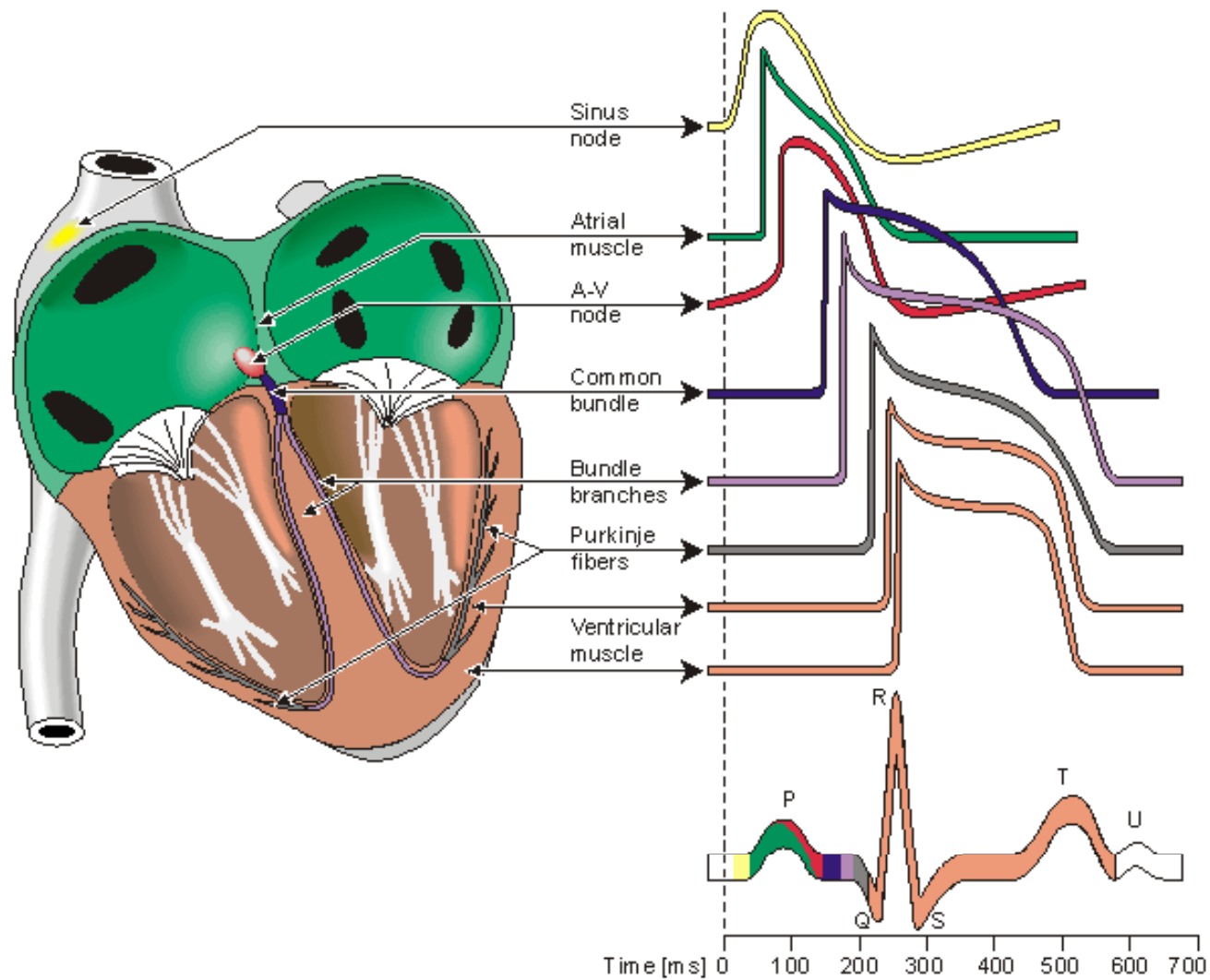


# Electrocardiograph (ECG)

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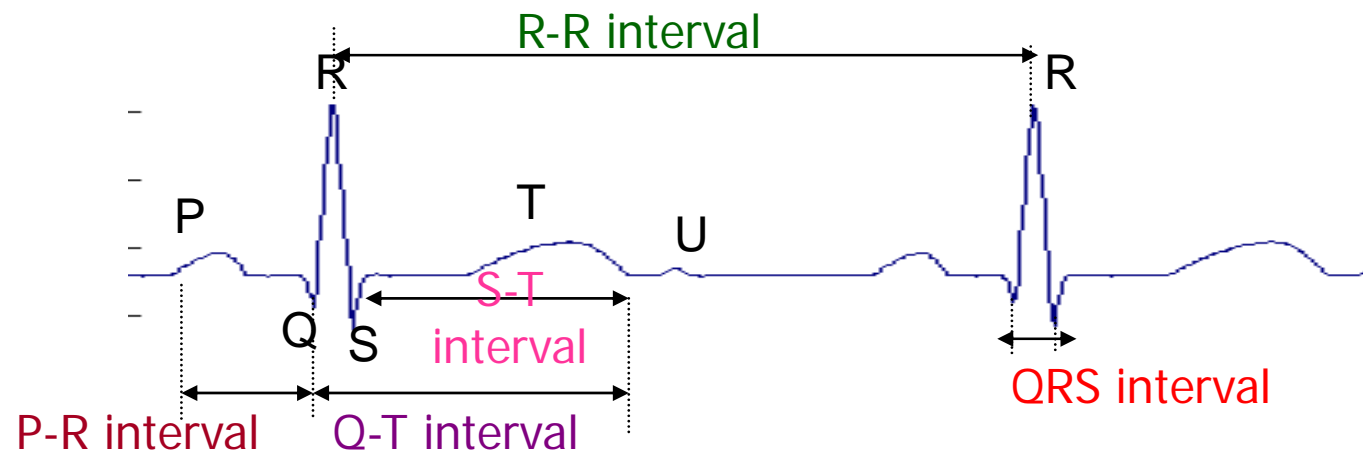
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Chang Gung University, Taiwan  
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# Heart and electrocardiogram (ECG, EKG)



# ECG features

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**P wave** : Atrial depolarization

**QRS complex** : Ventricular depolarization

**T wave** : Ventricular repolarization

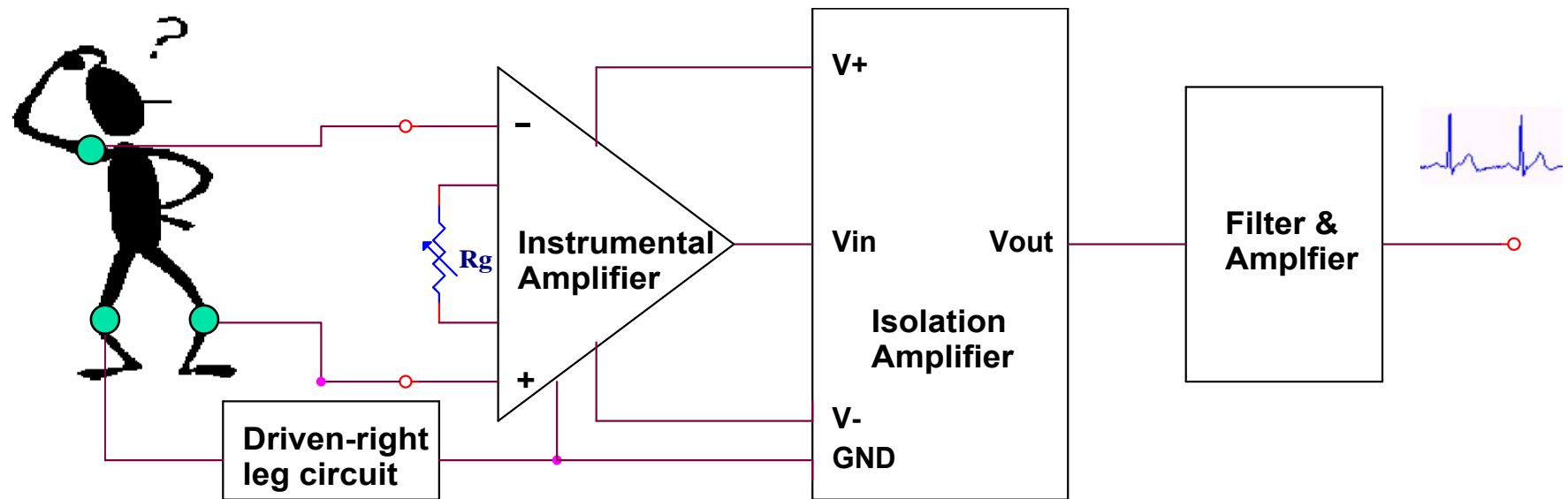
**U wave** : Slow repolarization of ventricular muscle

**R-R** : Heart period

**P-R** : Conduction delay in the AV-node

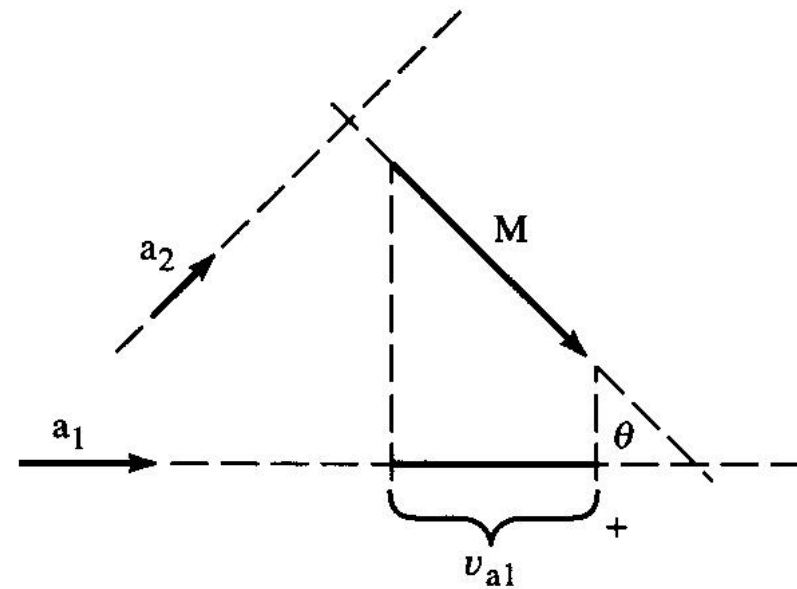
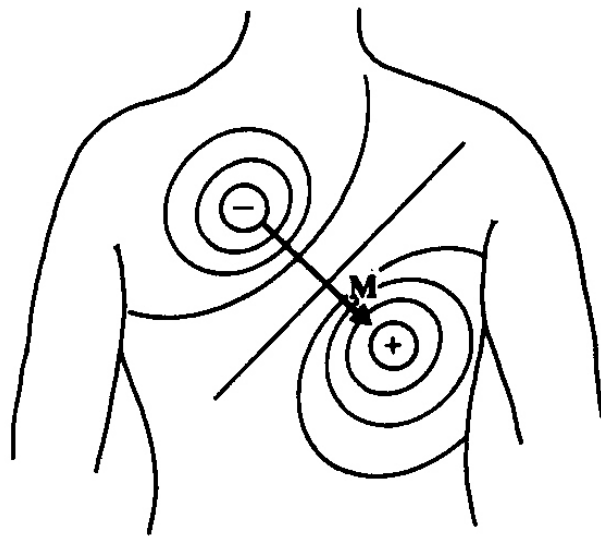
**S-T** : Ventricular repolarization time

# ECG amplifier



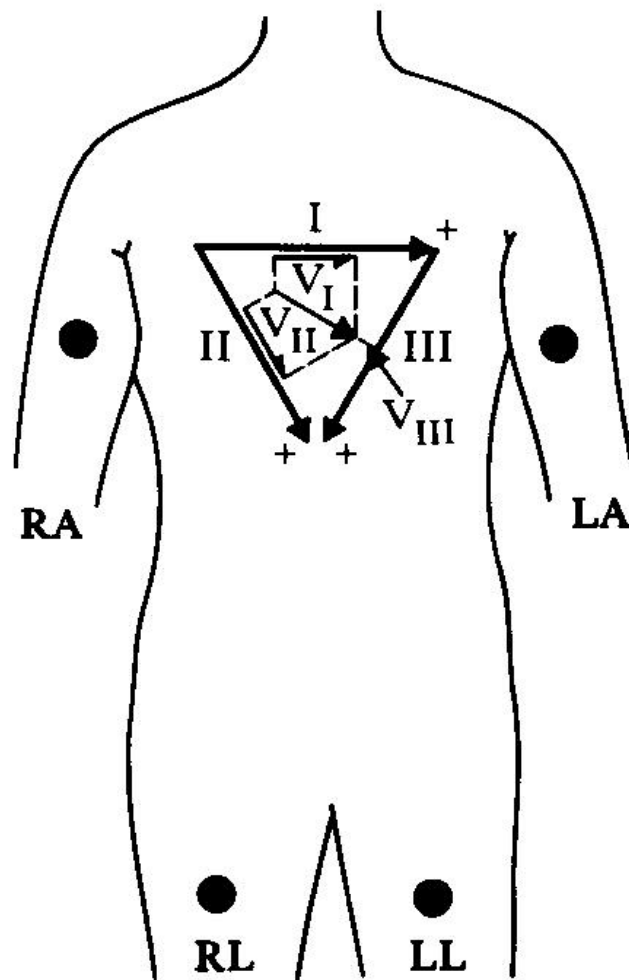
## Dipole field of heart when R is maximum

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# Electrocardiogram (ECG) measurements

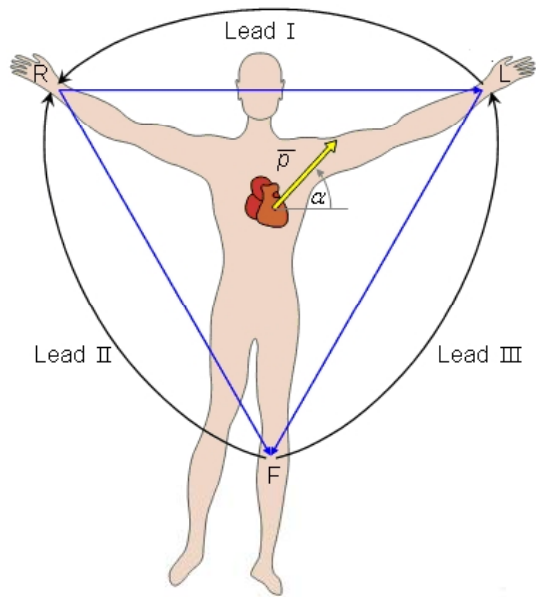
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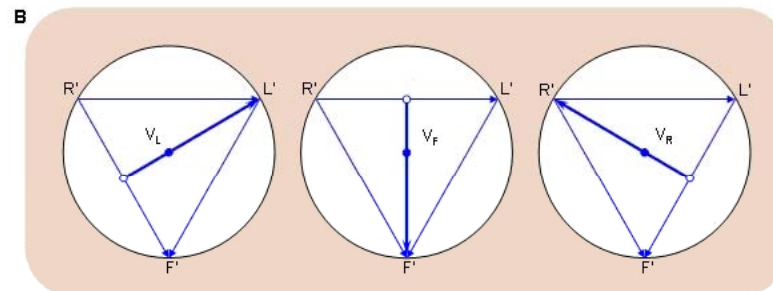
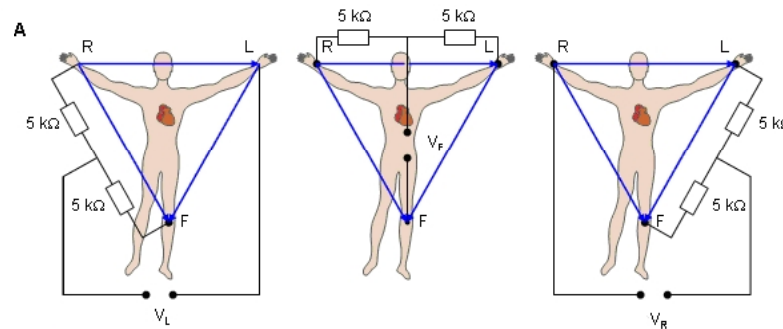
$$I - II + III = 0$$

# 12-Lead ECG

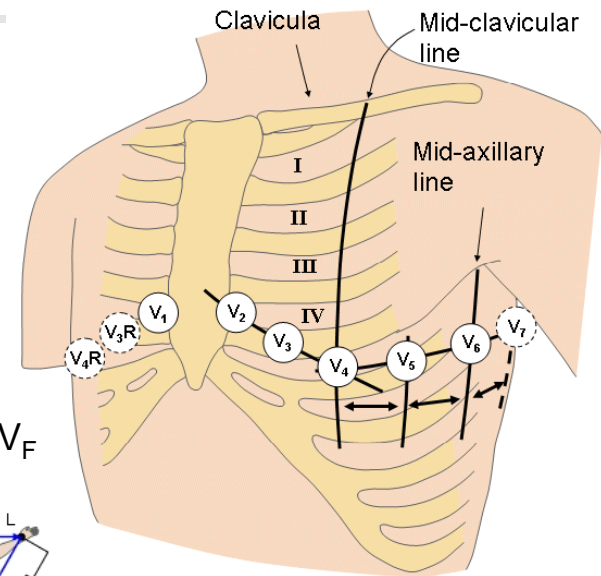
Einthoven leads: I, II & III



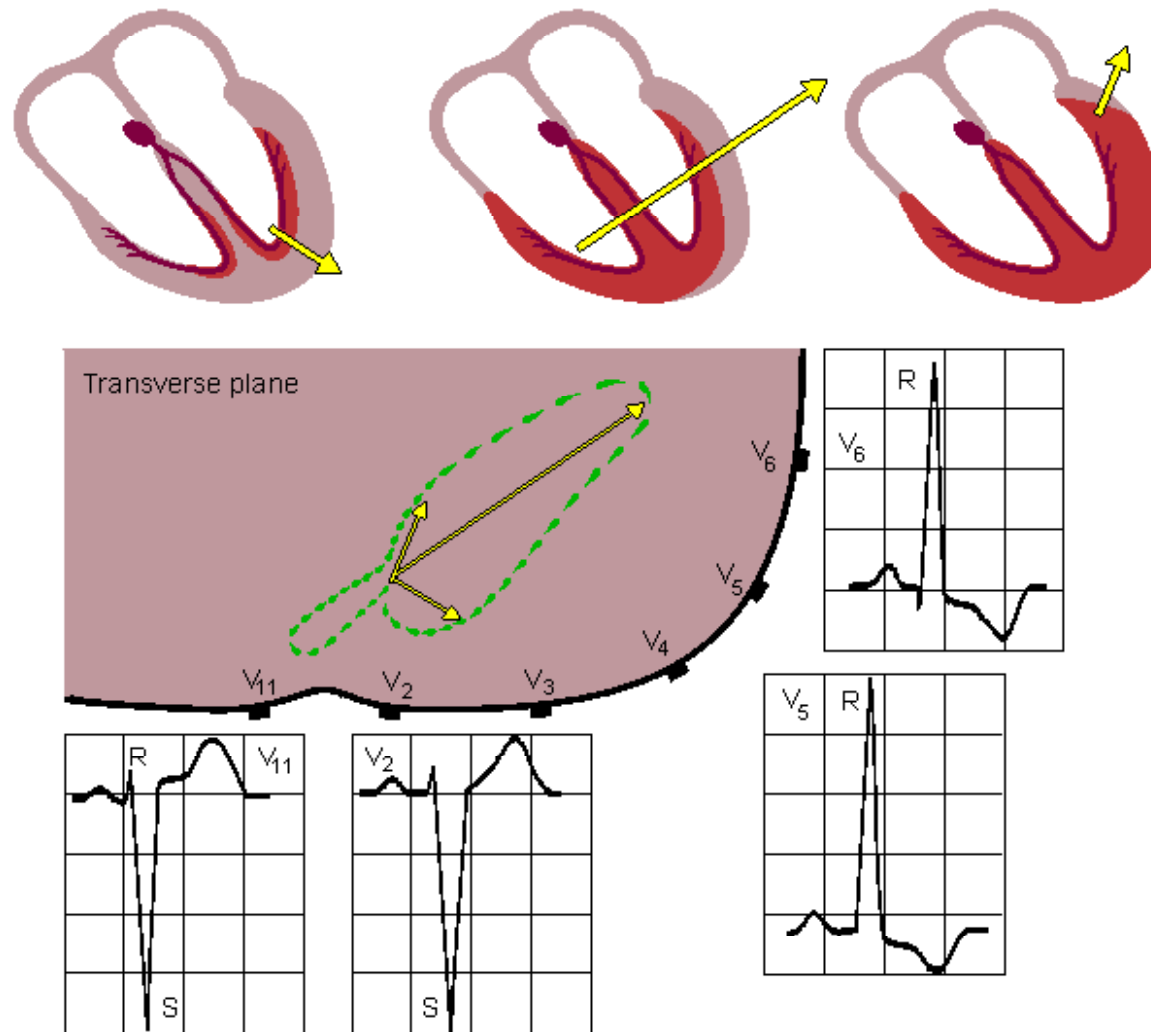
Goldberger augmented leads:  $V_R$ ,  $V_L$  &  $V_F$



Precordial leads:  $V_1$ - $V_6$

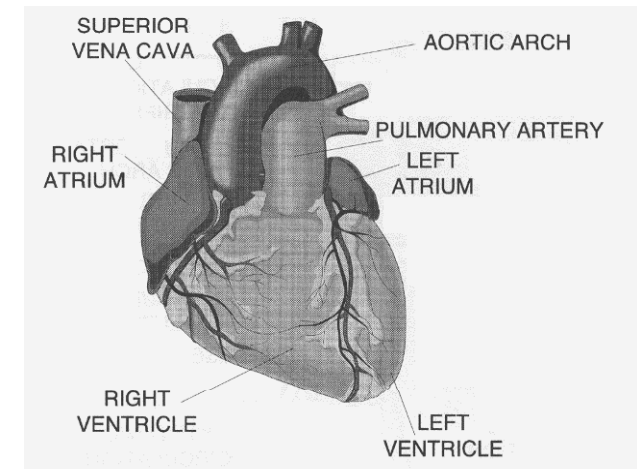
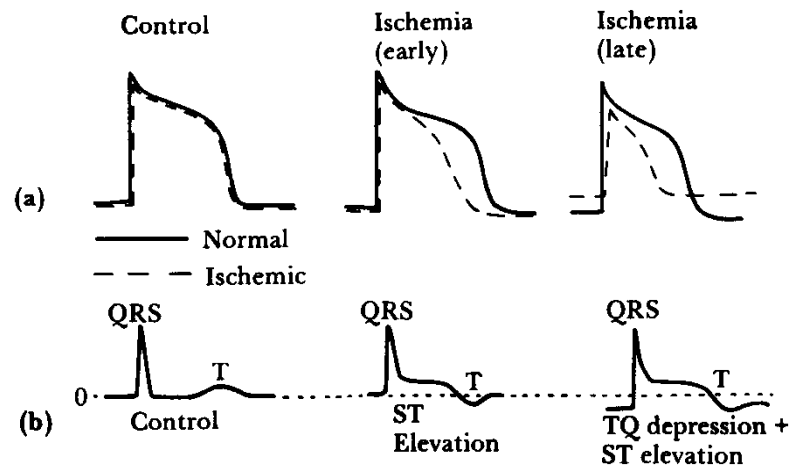


# ECG at chest leads



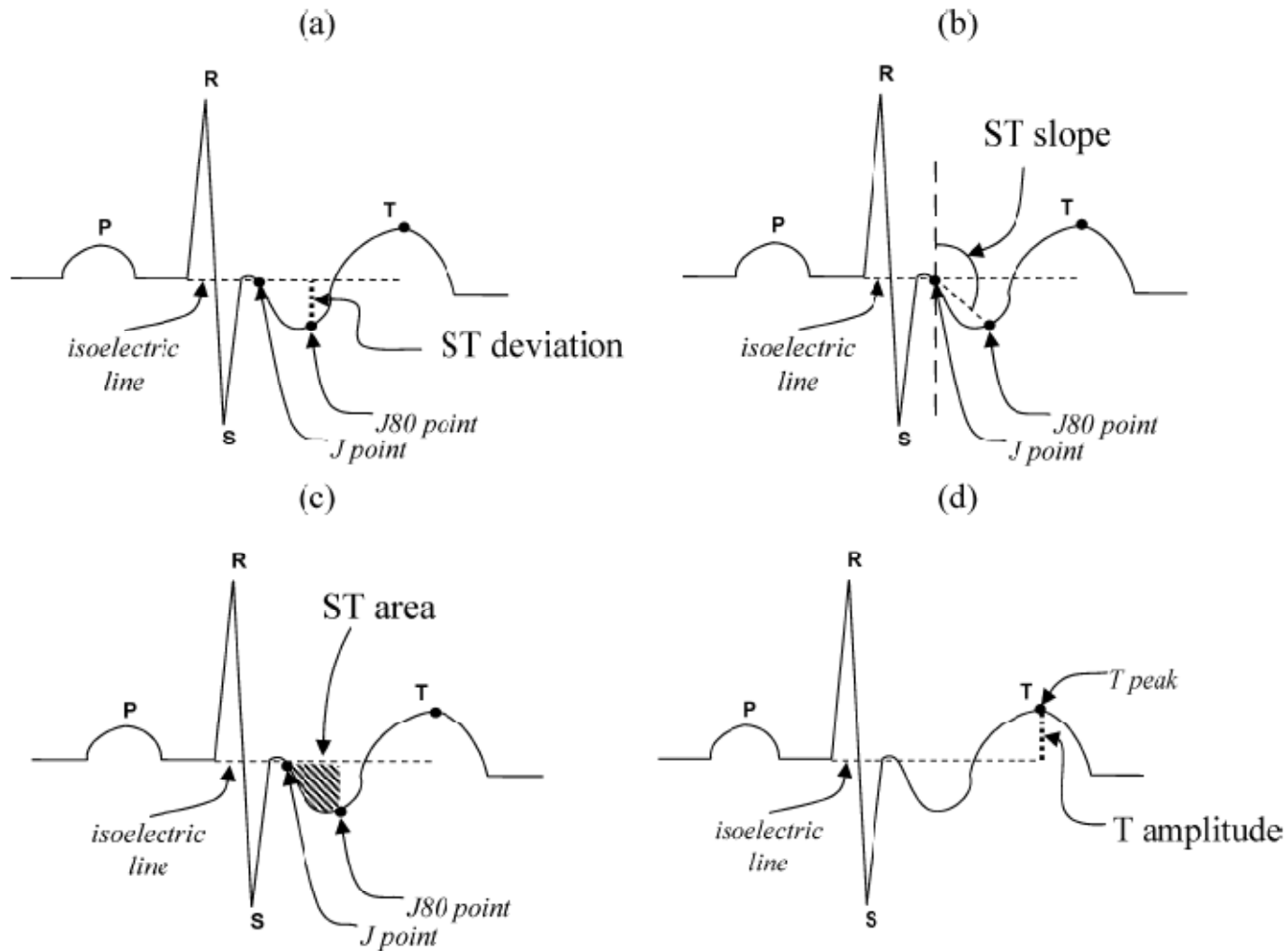


# ST-segment elevation

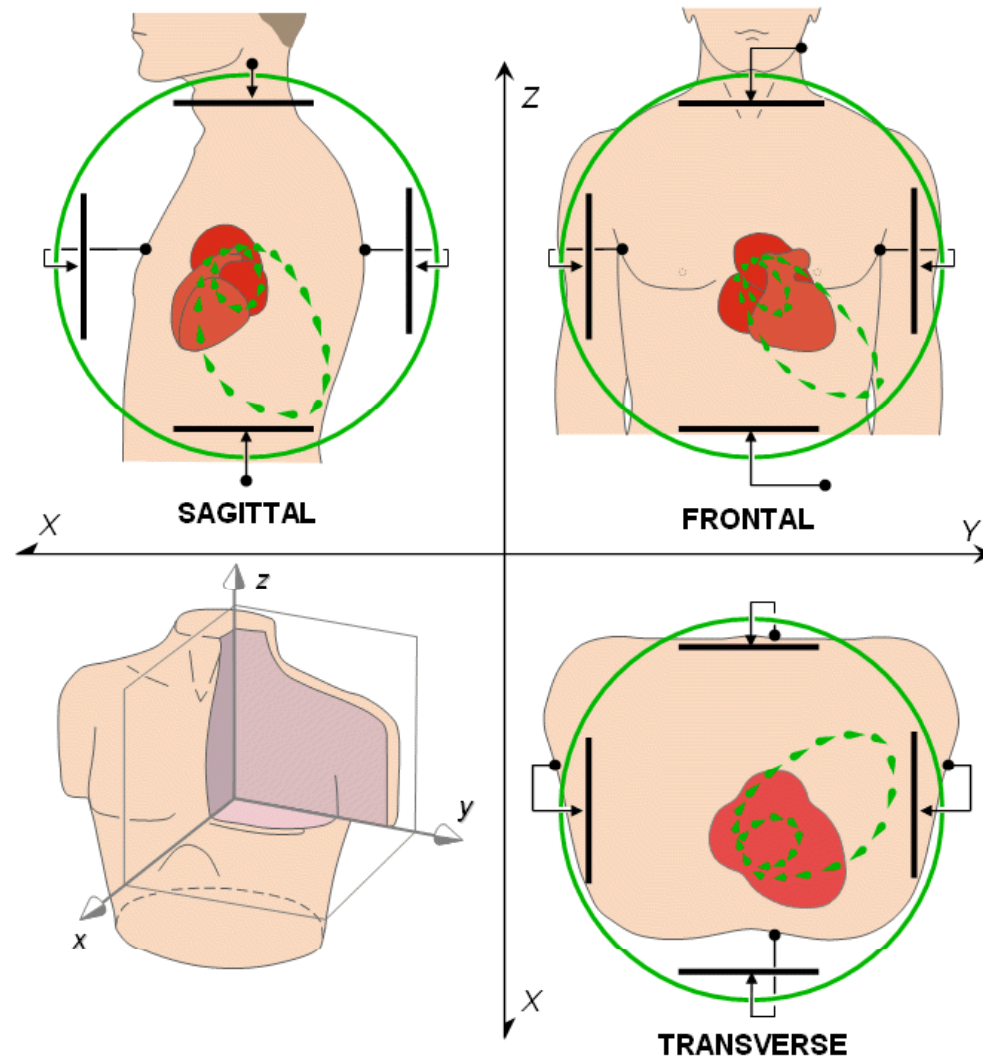


**Figure 4.21** (a) Action potentials recorded from normal (solid lines) and ischemic (dashed lines) myocardium in a dog. Control is before coronary occlusion. (b) During the control period prior to coronary occlusion, there is no ECG S–T segment shift; after ischemia, there is such a shift. (From Andrew G. Wallace, “Electrophysiology of the Myocardium,” in *Clinical Cardiopulmonary Physiology*, 3rd ed. New York: Grune & Stratton, 1969; used with permission of Grune & Stratton. Based on data by W. E. Sampson and H. M. Scher, “Mechanism of S–T Segment Alteration During Acute Myocardial Injury,” 1960, *Circulation Research*, 8, by permission of The American Heart Association.)

## ST-segment depression (mostly in myocardial ischemia)

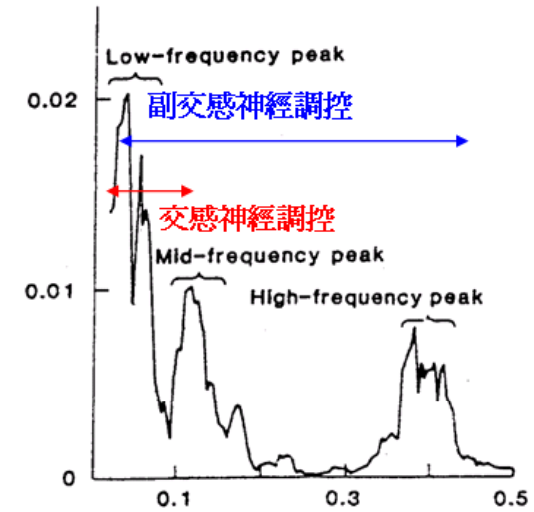
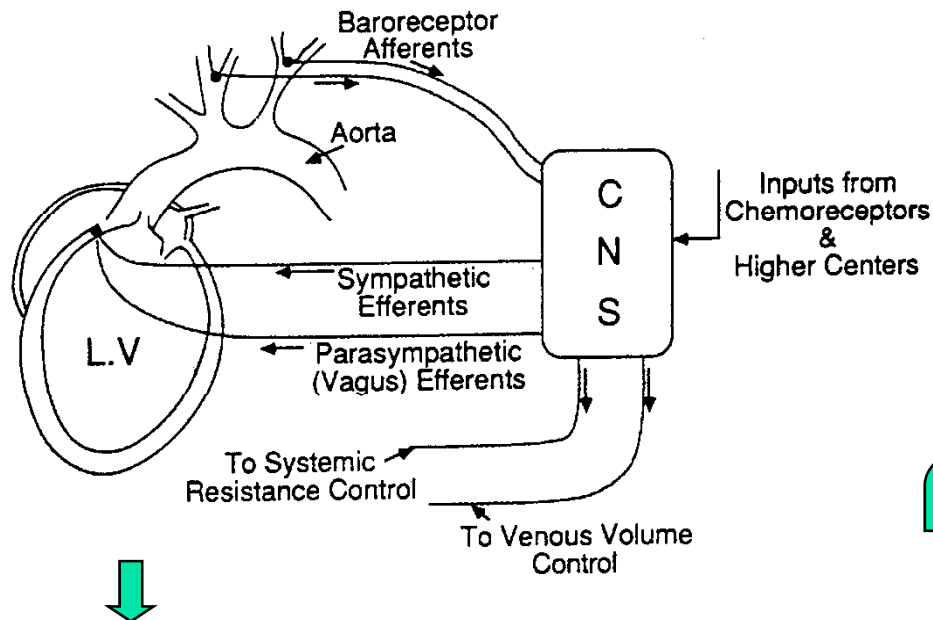


# Vectorcardiogram (VCG)

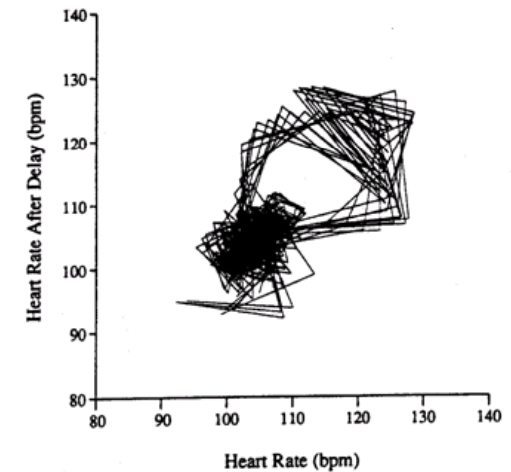
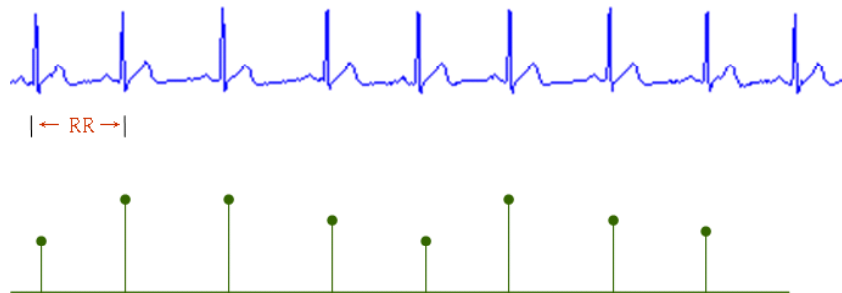


# Heart rate variability (HRV, 心率變異度)

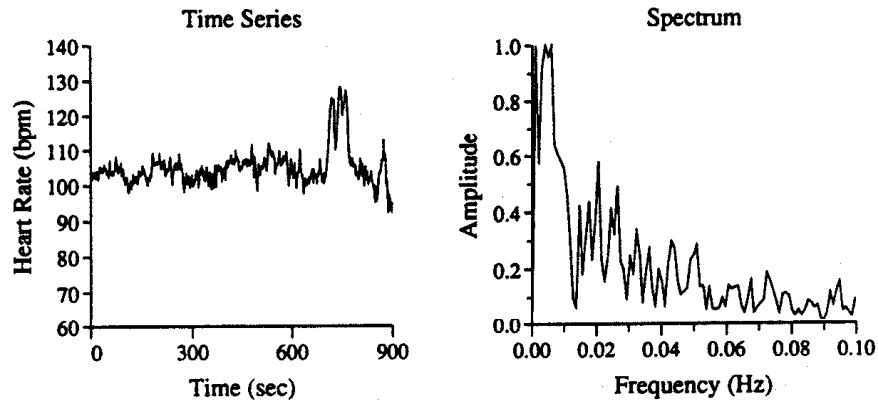
線性分析



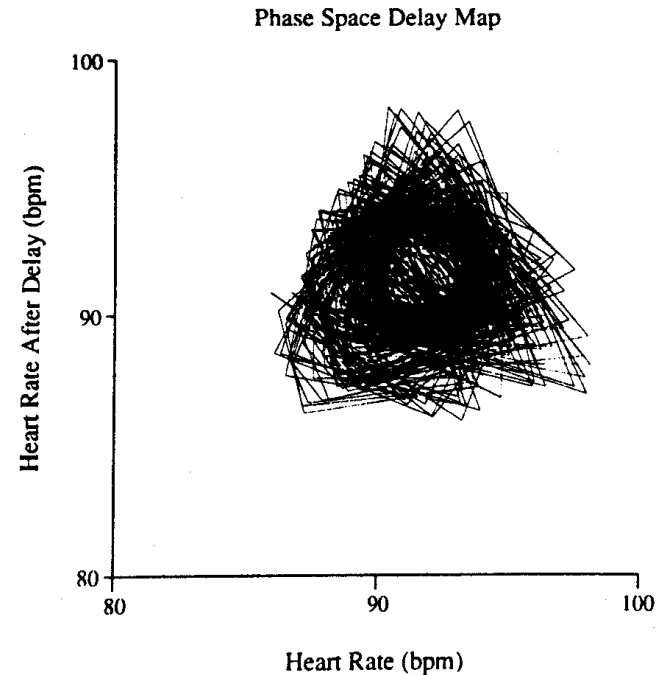
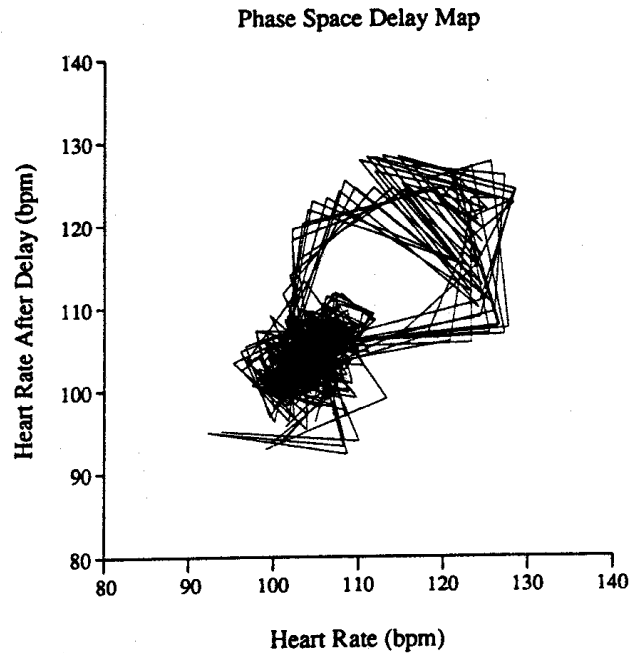
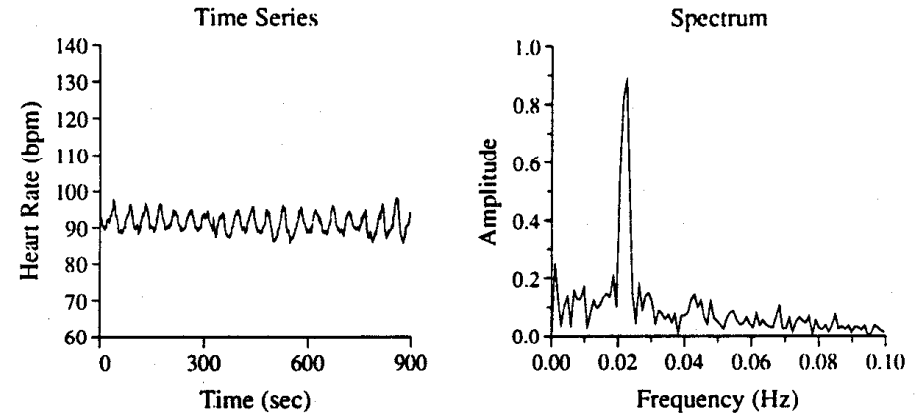
非線性分析



## Normal Subject



## Cardia arrest due to ventricular tachyarrhythmia 8 days later

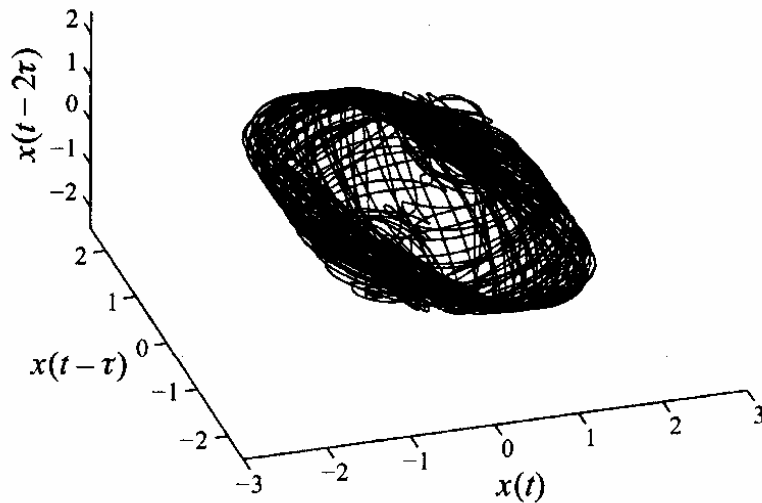


Goldberger *et al*, , Scientific American, 1990.

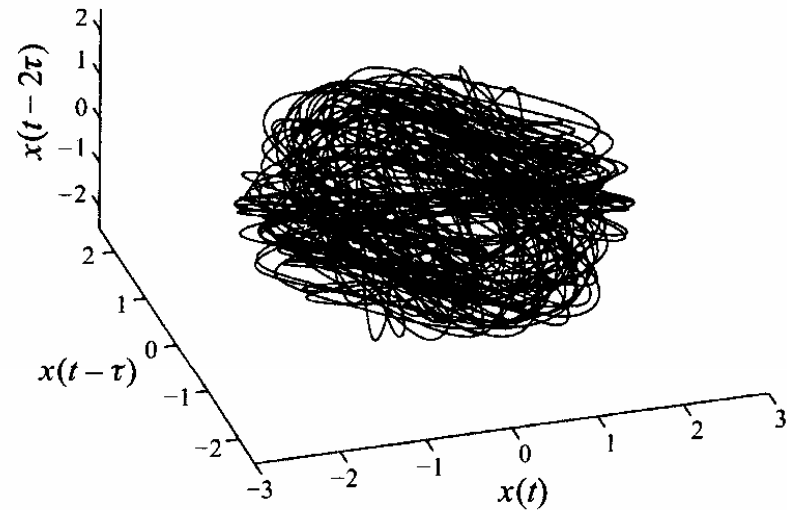
# Is HRV chaotic (渾沌)?

- Chaotic: 隱含一種亂中有序
- Random: 隨機

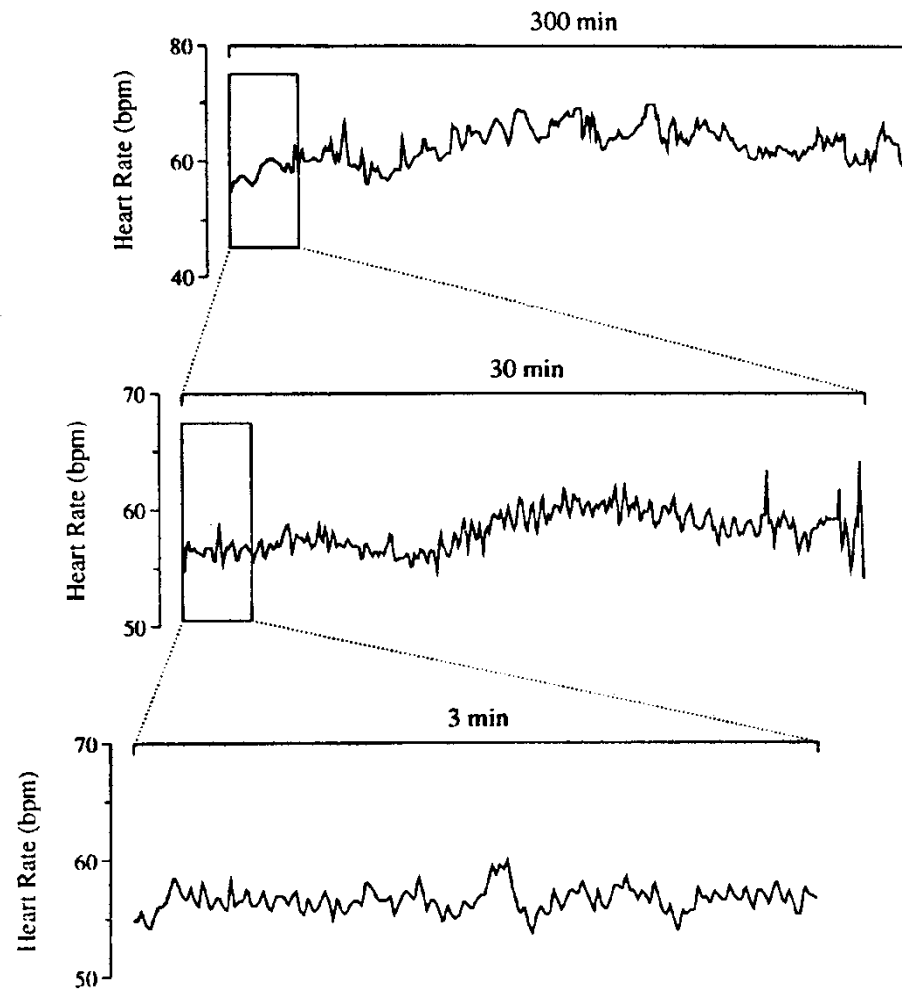
Chaotic



Near random



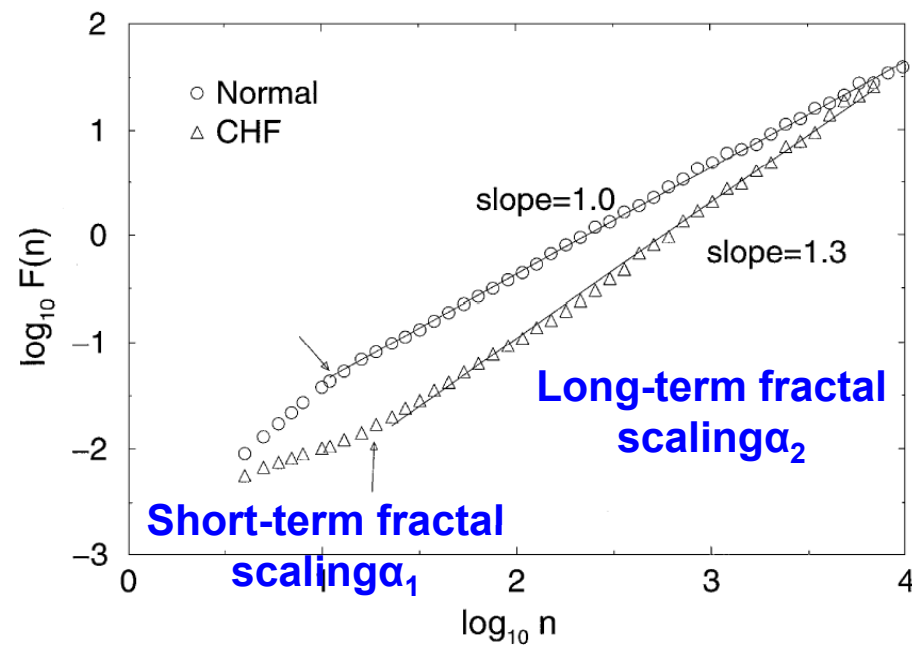
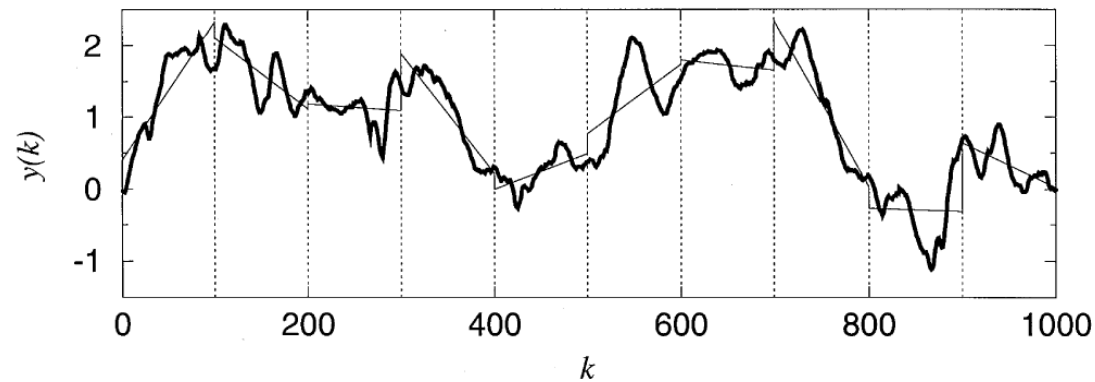
# Self-similarity (自我相似性) in HRV



It would be better  
delineated by fractal (碎型)  
characteristics

Goldberger *et al*, Scientific American, 1990.

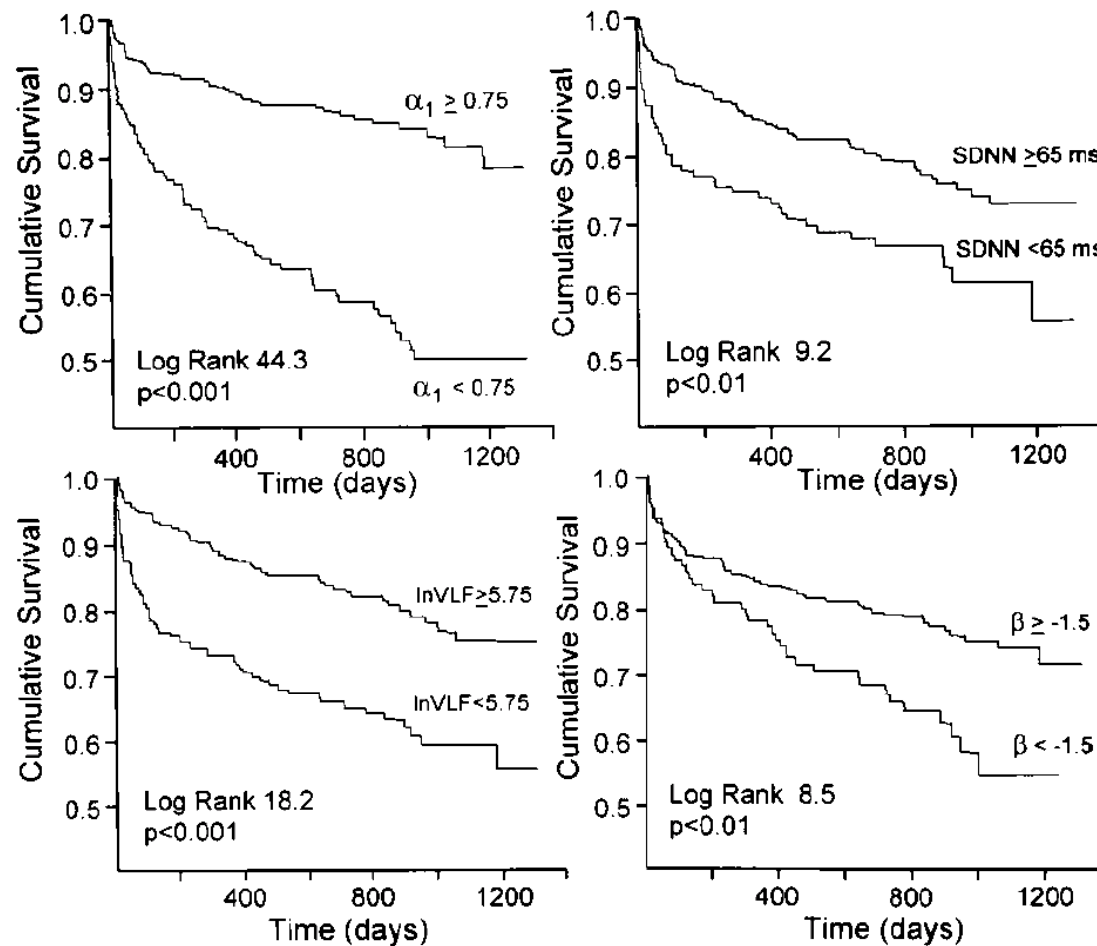
# Detrend fluctuation analysis (DFA)



HE Stanley *et al*, , Physica A, 1999



# Survival curves after acute myocardial infarction using HRV

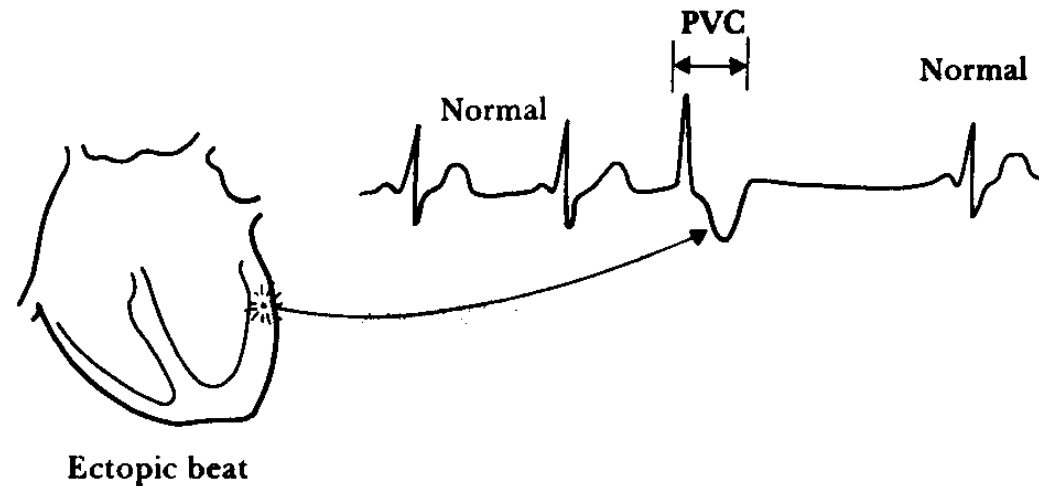


# ECG classification

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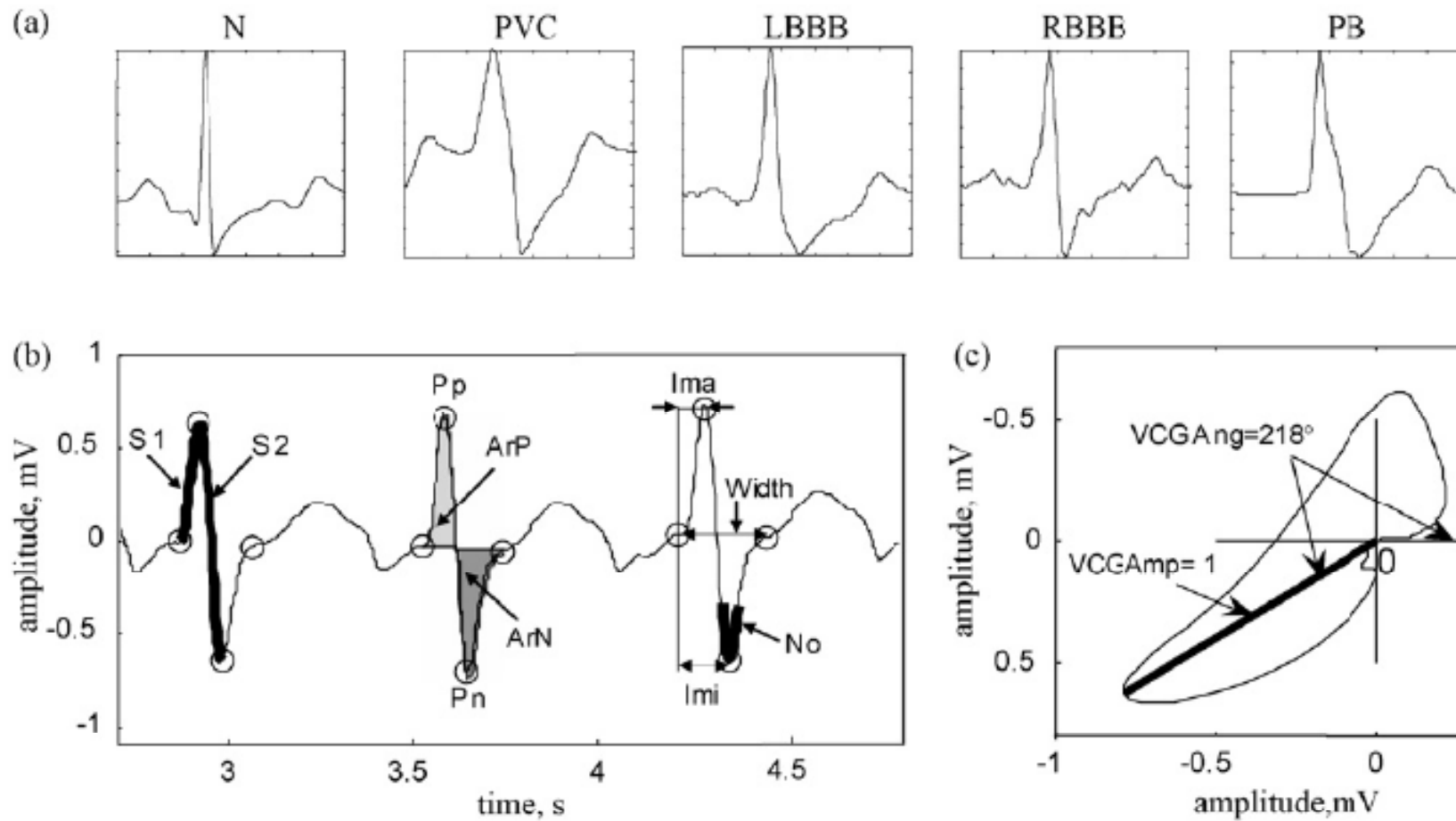
- Premature ventricular contraction
- Ventricular tachycardia, ventricular fibrillation
- Human identification

## Cardiac arrhythmia: premature ventricular contraction (PVC)



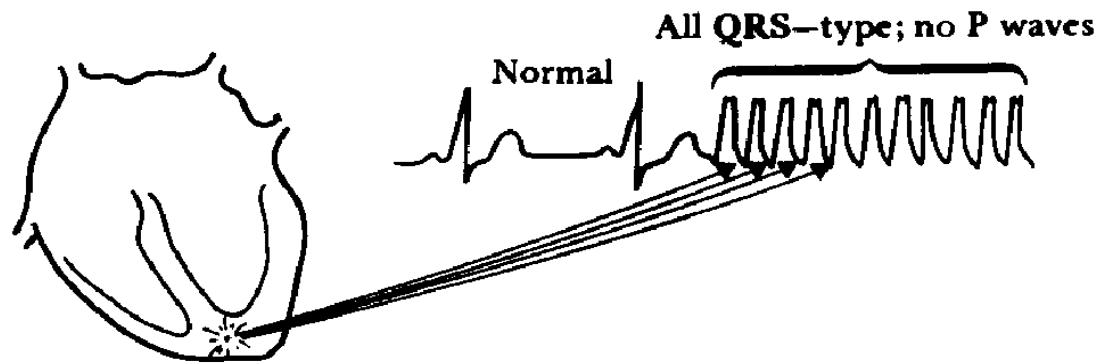
**Figure 4.18** Normal ECG followed by an ectopic beat An irritable focus, or *ectopic pacemaker*, within the ventricle or specialized conduction system may discharge, producing an extra beat, or *extrasystole*, that interrupts the normal rhythm. This extrasystole is also referred to as a premature ventricular contraction (PVC). (Adapted from Brendan Phibbs, *The Human Heart*, 3rd ed., St. Louis: The C.V. Mosby Company, 1975.)

## ECG features (Jekova et al, 2007)

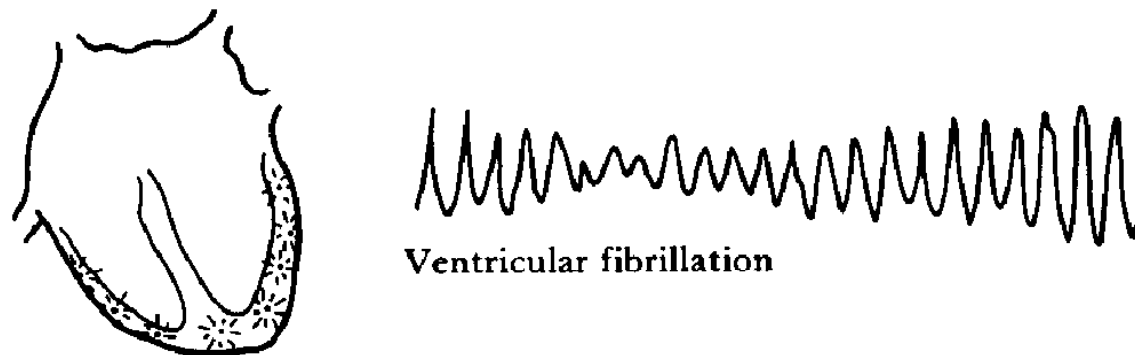


# Life-threatening arrhythmia

## Ventricular Tachycardia

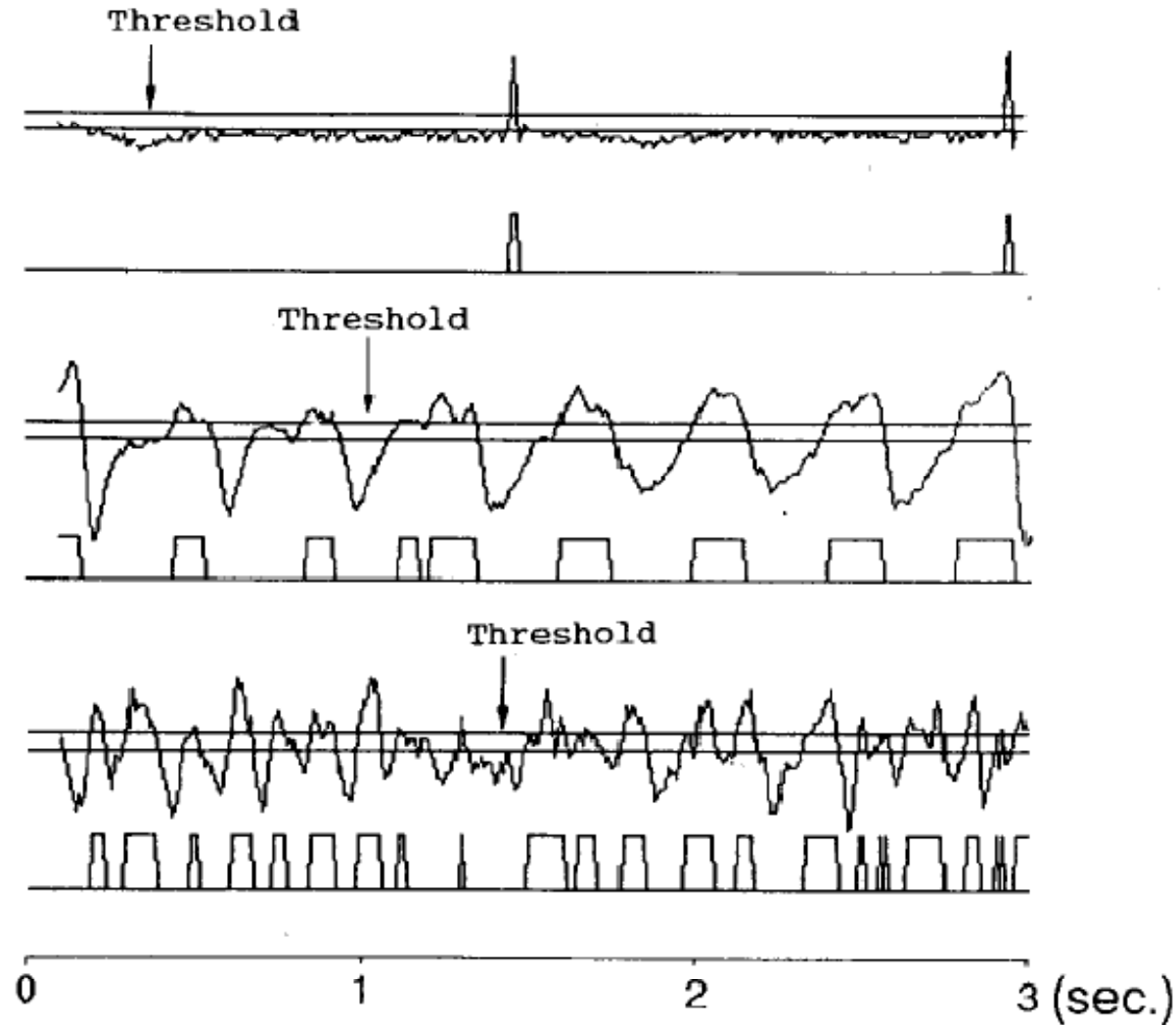


## Ventricular fibrillation

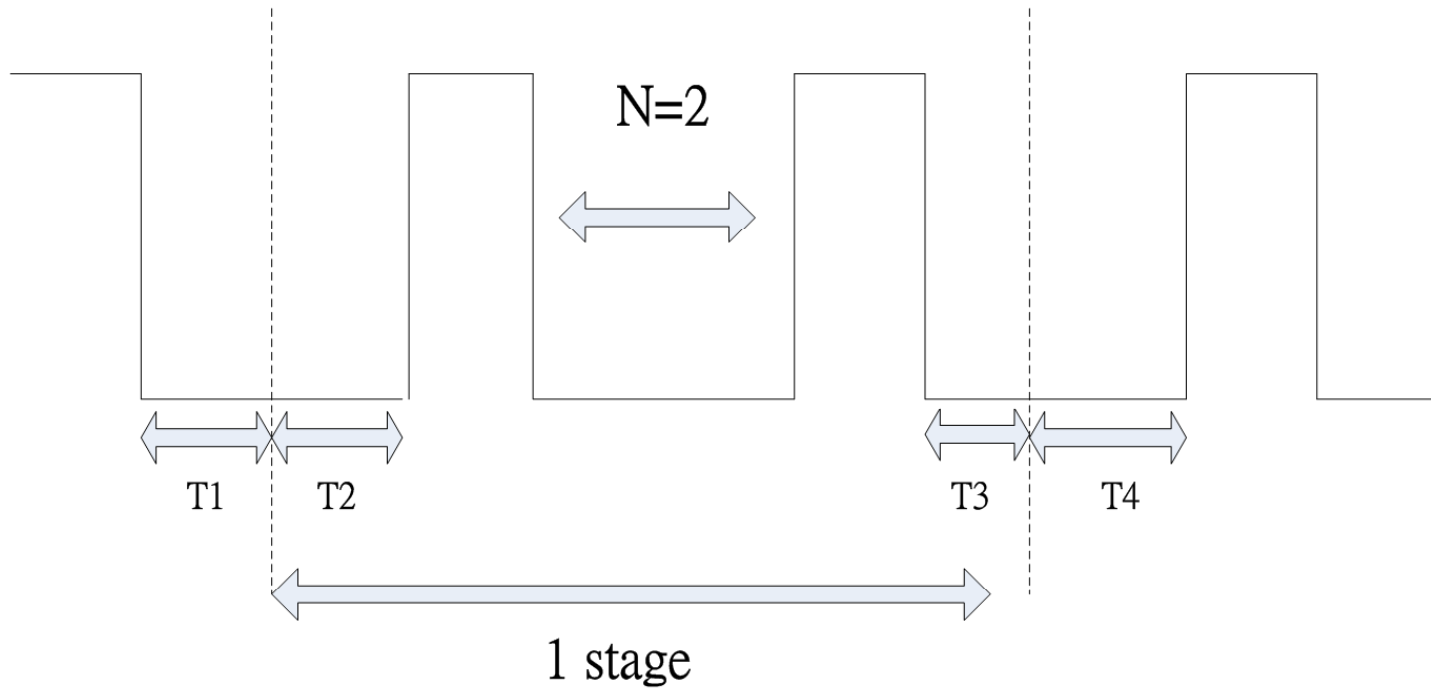


# Detecting VT and VF by TCI

Thaker et al, IEEE Trans. Biomed. Eng. 1990

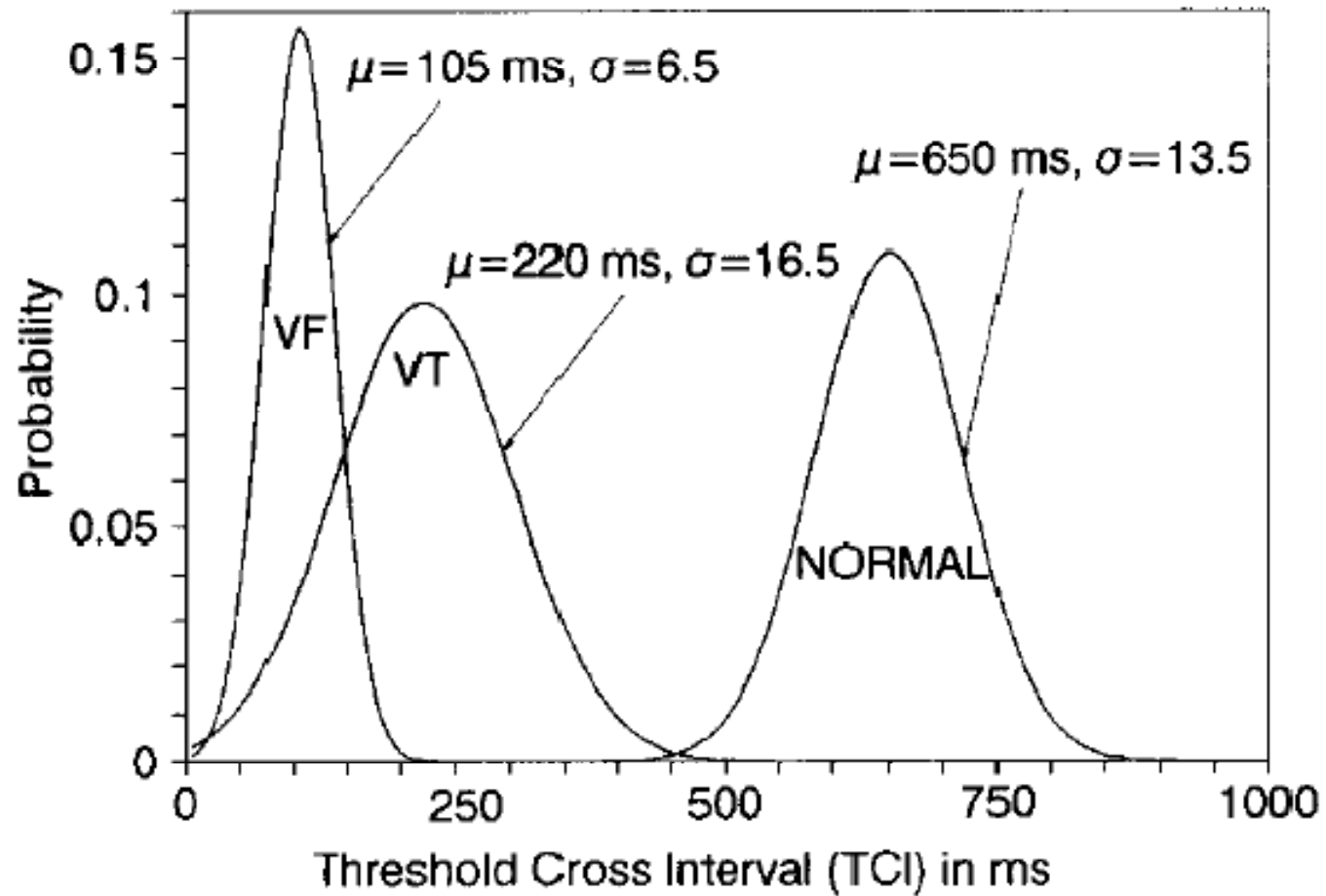


# Threshold crossing interval (TCI)



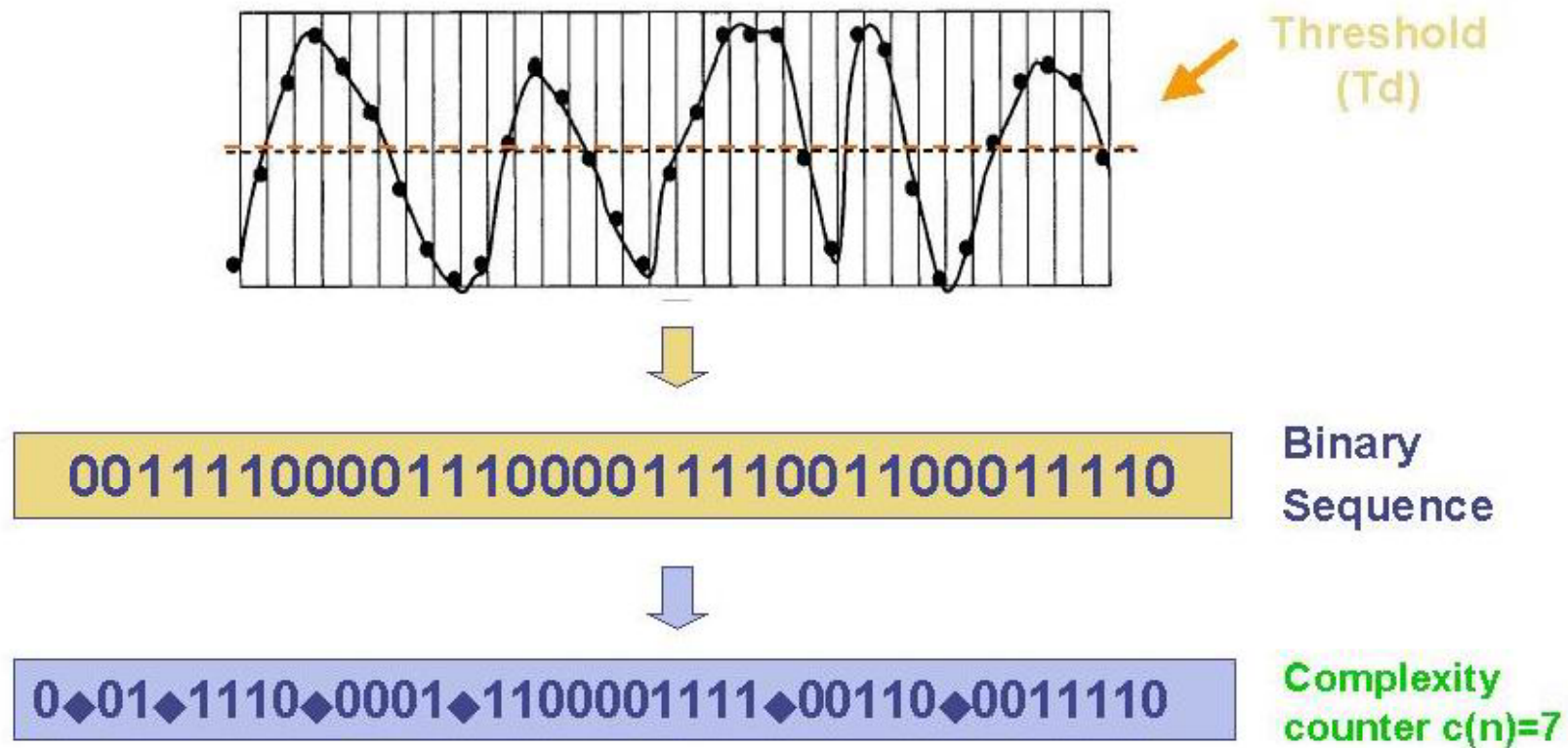
$$TCI = \frac{1000}{(N-1) + \frac{T2}{T1+T2} + \frac{T3}{T3+T4}}$$

## Detecting VT and VF by TCI

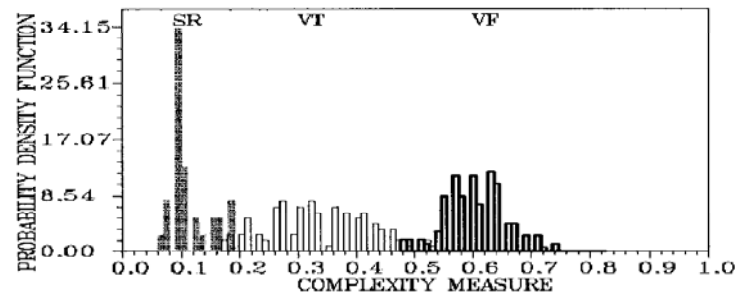




## Lempel-Ziv complexity (複雜度)

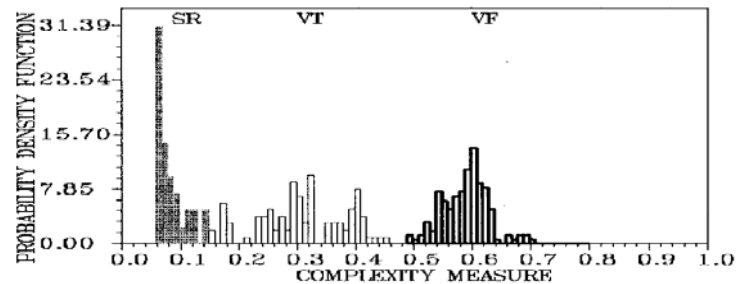


# Detecting Ventricular Tachycardia and Fibrillation by Complexity Measure (Xu-Sheng Zhang, et al, 1999)



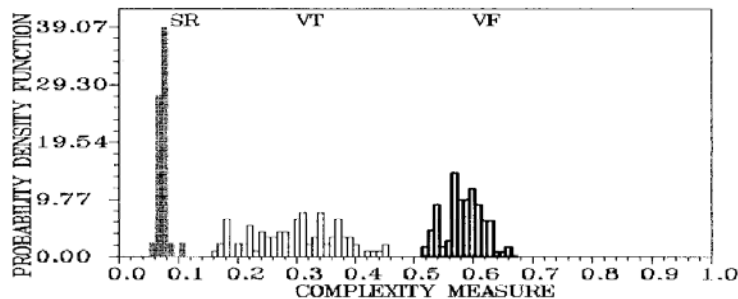
(a)

window length  
3 s



(b)

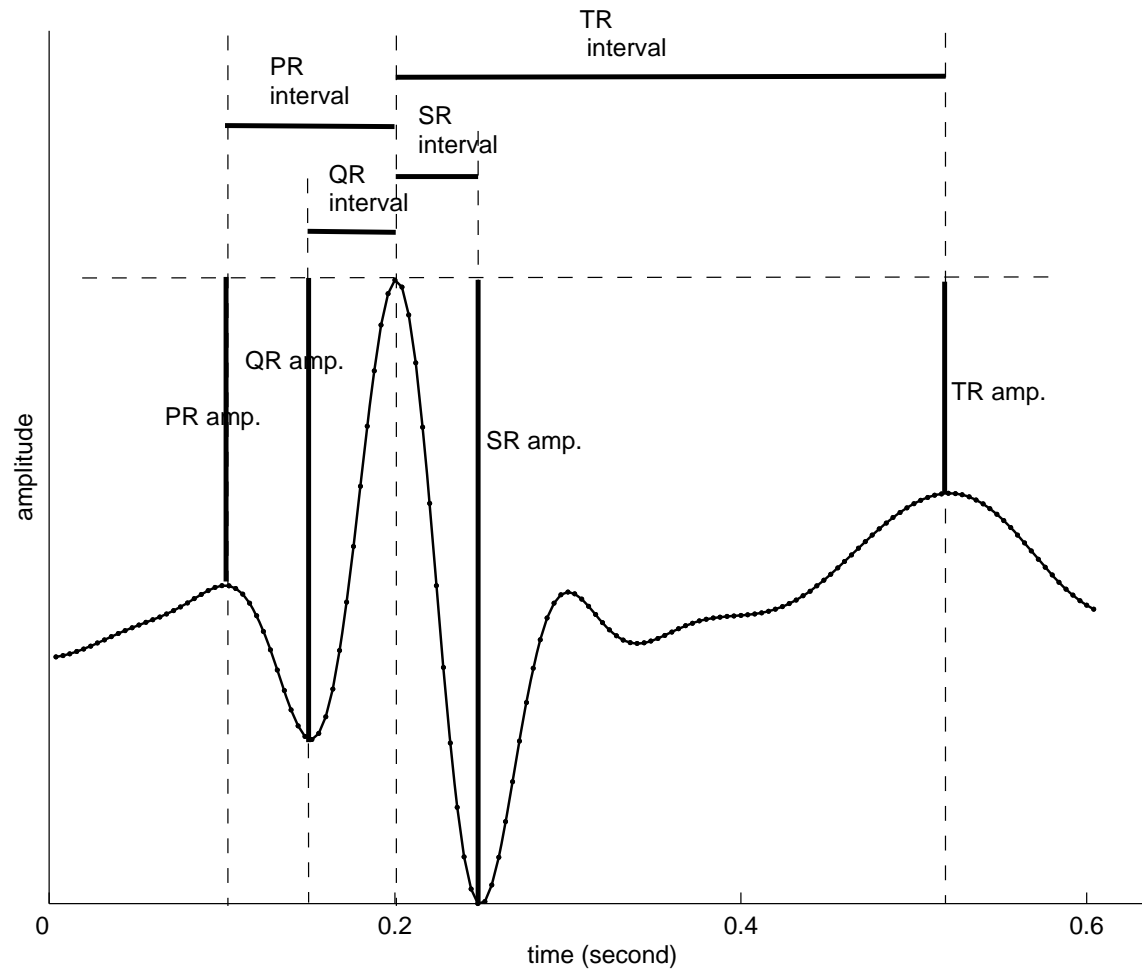
5 s



(c)

7 s

# Biometrics (生物辨識) by ECG features



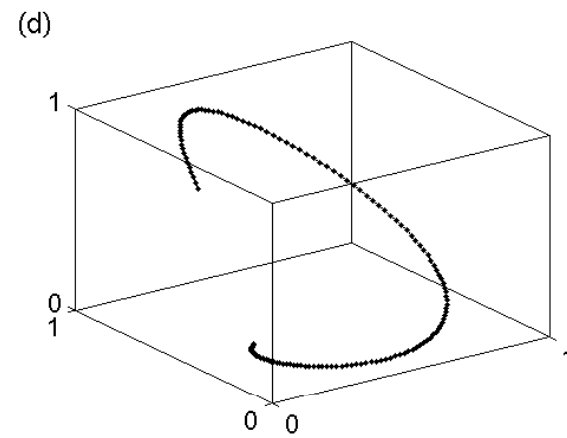
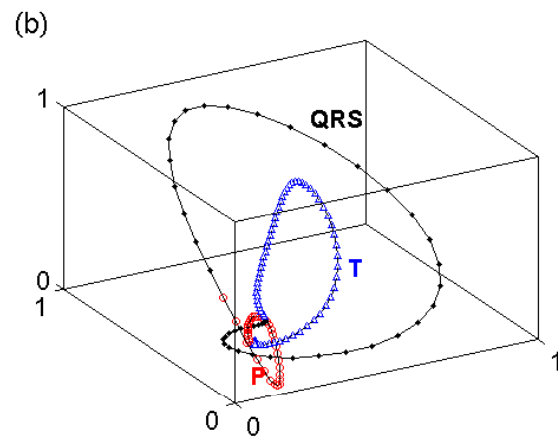
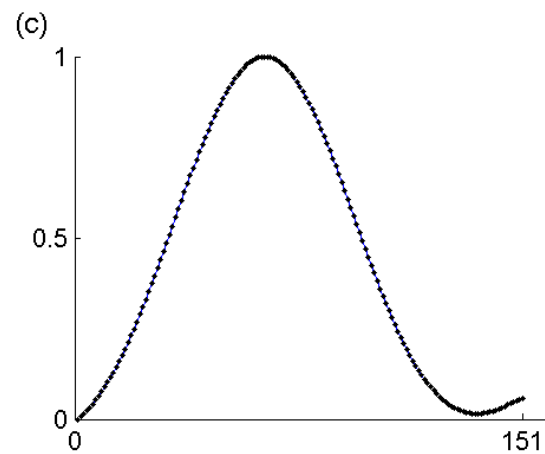
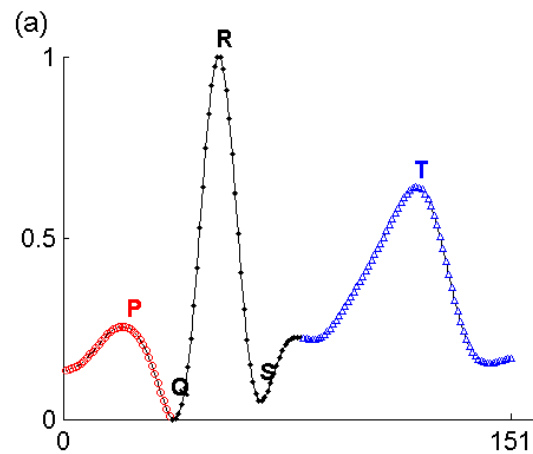
## Human identification (身份識別) by ECG features

Classification performance on various configurations in characteristic-point comparison methods.

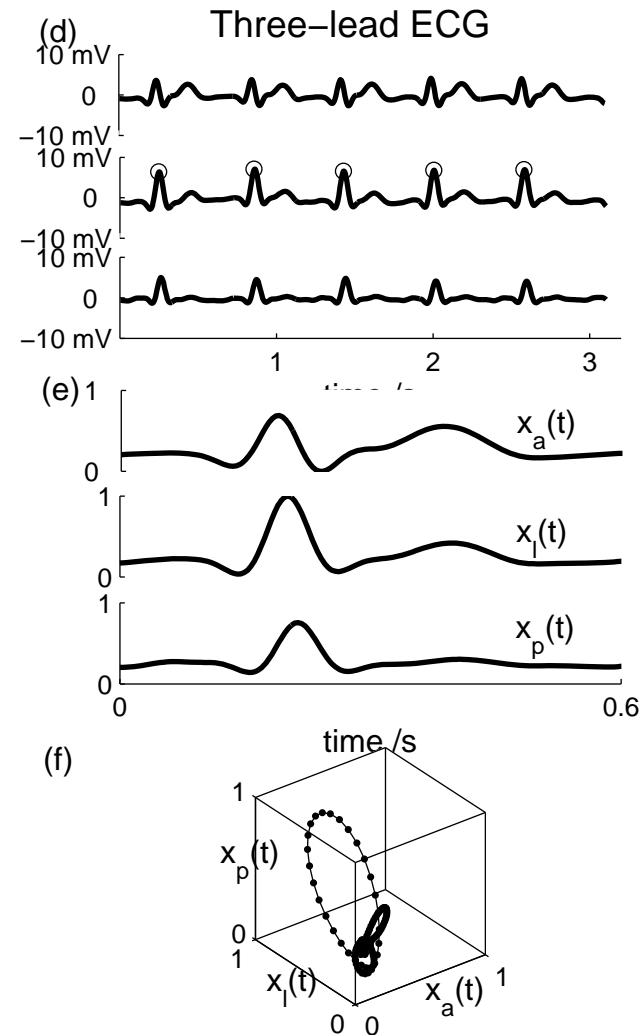
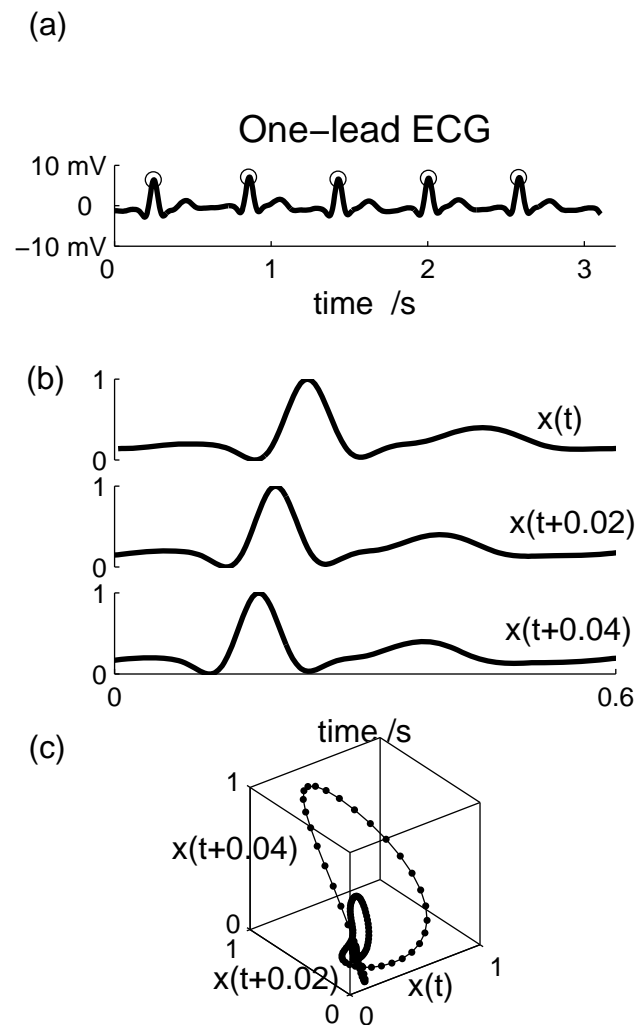
| ECG leads | ECG features | Comparison method | Sensitivity (%) | Specificity (%) | Accuracy (%) |
|-----------|--------------|-------------------|-----------------|-----------------|--------------|
| 1         | 8/4*         | BP20              | 89/95           | 86/67           | 87/81        |
| 3         | 24/9*        | BP20              | 95/94           | 95/86           | 95/90        |
| 1         | 8/4*         | RB10              | 86/74           | 91/81           | 89/77        |
| 3         | 24/9*        | RB10              | 97/100          | 98/93           | 98/96        |
| 1         | 8/4*         | PD                | 93/93           | 93/93           | 93/93        |
| 3         | 24/9*        | PD                | 100/100         | 95/95           | 98/98        |

For 1-channel anterior-lead ECG, input with eight extracted features or four major principal components (4\*). For 3-channel ECG, input with 24 extracted features or nine major principal components (9\*). BP 20: backpropagation with 20 hidden neurons; RB10: radial basis function with spread constant 10; PD: point distance in multi-dimensional space. Sensitivity, specificity and accuracy were defined as Fig. 6.

# Phase-space reconstruction of ECG



# Phase-space reconstruction of ECG



# Measures of differences between phase-space trajectories

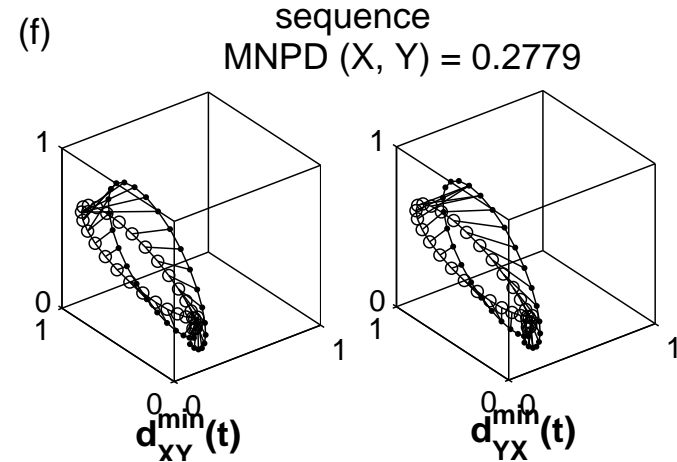
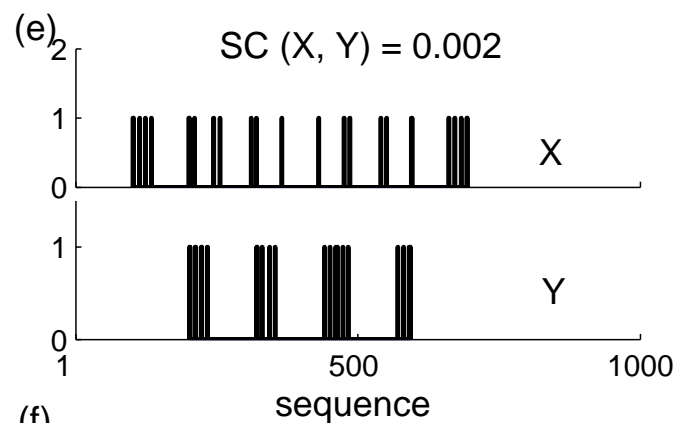
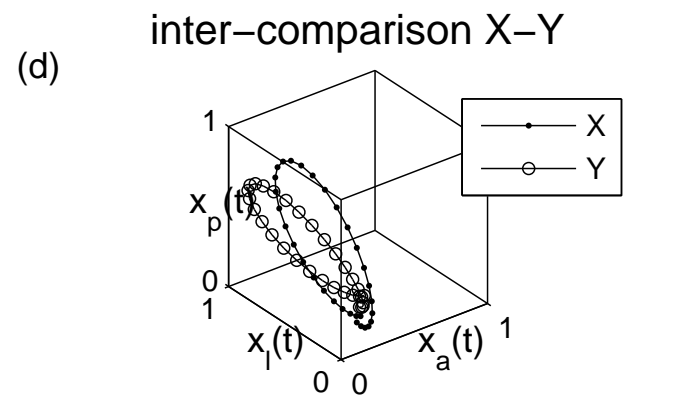
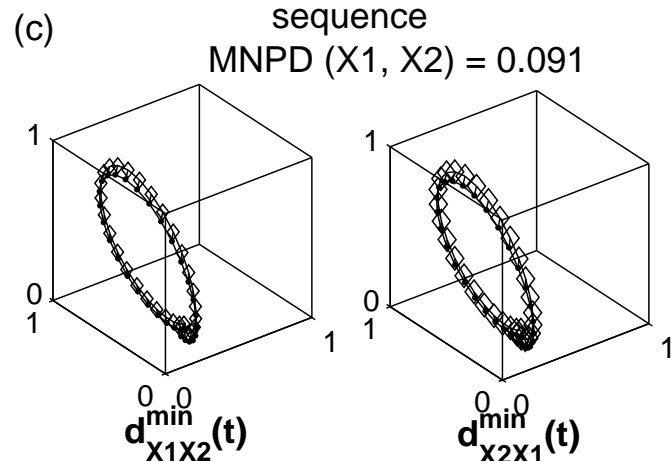
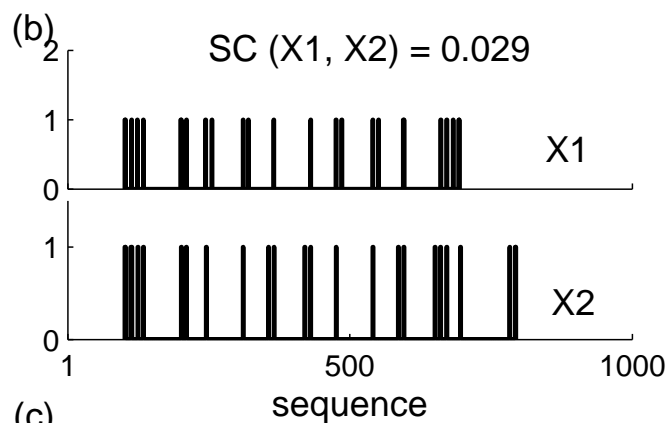
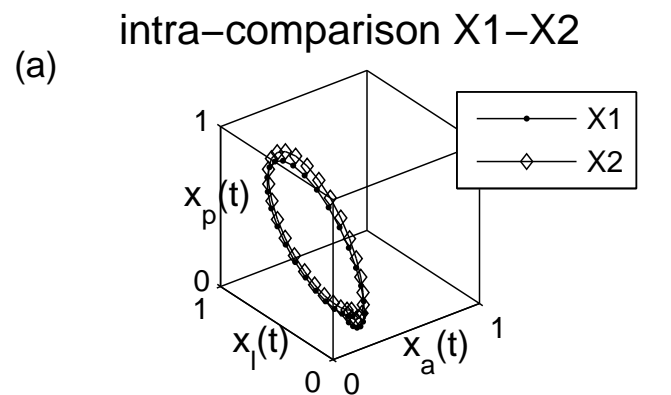
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## Spatial correlation (SC)

$$SC(\mathbf{X}, \mathbf{Y}) = \frac{\sum_{1 \leq i, j, k \leq M} N_{\mathbf{X}}(i, j, k) \times N_{\mathbf{Y}}(i, j, k)}{M^3 - 1}$$

## Mutual nearest point distance (MNPD)

$$MNPD(\mathbf{X}, \mathbf{Y}) = \frac{\sum_{t=t_1}^{t_P} d_{\mathbf{XY}}^{\min}(t) + \sum_{t=t_1}^{t_P} d_{\mathbf{YX}}^{\min}(t)}{2 \times P}$$





# Human identification over phase space of ECG

Classification performance on various configurations in portrait comparison methods.

| ECG leads | ECG points | Comparison method | Sensitivity (%) | Specificity (%) | Accuracy (%) |
|-----------|------------|-------------------|-----------------|-----------------|--------------|
| 1         | 31         | MNPD              | 98              | 88              | 93           |
| 1         | 151        | MNPD              | 95              | 89              | 92           |
| 3         | 31         | MNPD              | 99              | 98              | 99           |
| 3         | 151        | MNPD              | 98              | 95              | 97           |
| 1         | 31         | SC 10             | 96              | 87              | 92           |
| 1         | 151        | SC 10             | 89              | 75              | 82           |
| 3         | 31         | SC 10             | 97              | 96              | 97           |
| 3         | 151        | SC 10             | 98              | 86              | 91           |

Spatial correlations SC 10 computed upon  $10 \times 10 \times 10$  phase space partitions; MNPD: mutual nearest point distance. Sensitivity, specificity and accuracy were defined as Fig. 6.

## Reference

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- JJ.Carr, JM.Brown, Introduction to Biomedical Equipment Technology, 4nd Edition, Prentice-Hall, 2000.
- J. Enderle, Introduction to Biomedical Engineering, Academic Press, 2000.
- JG. Webster, Medical Instrumentation, application and design, 3rd, Houghton Mifflin, 2000.