

Direct Estimation of Differential Functional Graphical Models

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Abstract

Background: In many applications, it is more natural to consider data as random function vectors rather than multivariate scalars; e.g., electroencephalography (EEG) data are more appropriately treated as functions of time. As in the multivariate scalar case, undirected graphs can be used to encode conditional independence relationships between the random functions.

What we do: We directly estimate the difference of structures between two functional graphs without estimating the individual graphs. The direct estimation approach allows better computational efficiency and statistically consistent results in a high-dimensional setting even when individual graphs are dense.

Algorithm contribution: We propose an efficient proximal gradient-descent algorithm to estimate the differential graph.

Theoretical result: We show that our method recovers the differential graph structure with high probability even in high-dimensional setting with dense individual graphs as long as the underlying differential structure is sparse.

Experiments: We demonstrate the benefits of our method by simulations and an analysis of real EEG data. We also provide a setting where the functional data approach is not ideal.

Our Method

Functional PCA: Estimate the covariance function $K_{jj}^X(t, s) = \text{Cov}(X_{ij}(t), X_{ij}(s))$ with $\bar{X}_j(t) = n_X^{-1} \sum_{i=1}^{n_X} X_{ij}(t)$:

$$\hat{K}_{jj}^X(s, t) = \frac{1}{n_X} \sum_{i=1}^{n_X} (X_{ij}(s) - \bar{X}_j(s))(X_{ij}(t) - \bar{X}_j(t)).$$

For each $j \in [p]$, an eigen-decomposition of $\hat{K}_{jj}^X(s, t)$ gives estimated eigenfunctions $\hat{\phi}_{jk}^X$ and scores $\hat{a}_{ij}^X = \{\hat{a}_{ijk}^X\}_{k \in [M]}$ with

$$X_{ij} \approx \sum_{k=1}^M \hat{\phi}_{jk}^X \hat{a}_{ijk}^X.$$

FuDGE (Functional Differential Graph Estimation):

Suppose $\hat{a}_i^{X,M} = \{\hat{a}_{i1}^X, \dots, \hat{a}_{ip}^X\}$ has sample covariance S^X and population precision matrix

$$\Theta_X^M = \begin{bmatrix} \text{Cov}(\hat{a}_{i1}^T \hat{a}_{i1}) & \dots & \text{Cov}(\hat{a}_{i1}^T \hat{a}_{ip}) \\ \dots & \dots & \dots \\ \text{Cov}(\hat{a}_{ip}^T \hat{a}_{i1}) & \dots & \text{Cov}(\hat{a}_{ip}^T \hat{a}_{ip}) \end{bmatrix}^{-1} \quad \text{with } \text{Cov}(\hat{a}_{ij}^T \hat{a}_{il}) \in \mathbb{R}^{M \times M}.$$

Roughly speaking, if the (j, l) block of Θ_X^M only contains 0, then $X_{ij} \perp X_{il} \mid \{X_{ik}\}_{k \neq l}$. Thus, we estimate $\hat{\Delta}^M \approx \Theta_X^M - \Theta_Y^M$ with block sparsity by solving

$$\hat{\Delta}^M \in \underset{\Delta \in \mathbb{R}^{pM \times pM}}{\text{argmin}} L(\Delta) + \lambda_n \sum_{\{i,j\} \in V^2} \|\Delta_{ij}\|_F,$$

$$\hat{E}_\Delta = \{(j, l) \in V^2 : \|\hat{\Delta}_{jl}^M\|_F > \epsilon_n \text{ or } \|\hat{\Delta}_{lj}^M\|_F > \epsilon_n\}.$$

Algorithm 1 FuDGE: Proximal gradient-descent

Input $S^X, S^Y, \lambda_n, \epsilon_n$; **Output** $\hat{\Delta}$

Initialize $\Delta^{(0)} = 0_{pM}$

repeat

$$A = \Delta - \eta \nabla L(\Delta) = \Delta - \eta \left(S_X^{(M)} \Delta S_Y^{(M)} - (S_Y^{(M)} - S_X^{(M)}) \right)$$

for $1 \leq i, j \leq p$ **do**

$$\Delta_{jl} \leftarrow \left(\frac{\|A_{jl}\|_F - \lambda_n \eta}{\|A_{jl}\|_F} \right)_+ \cdot A_{jl}$$

end for

until Converge

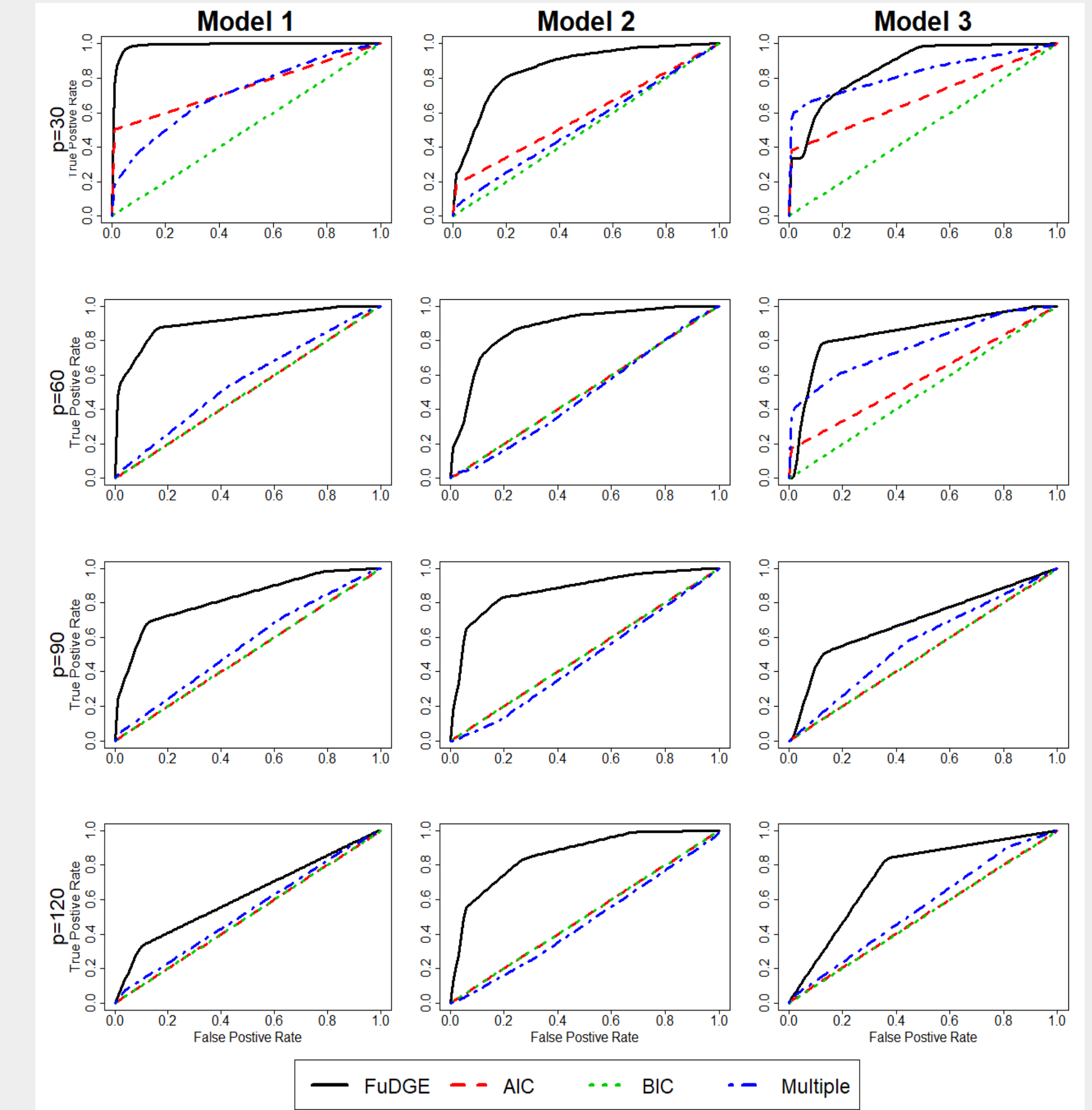
Theoretical Guarantees

Under mild conditions, for n and M large enough and appropriately selected ϵ_n , we have $P(\hat{E}_\Delta = E_\Delta) \geq 1 - 2c_2/n^2$.

For fixed M , the sample complexity is $O(s \log(p))$, where s is the number of differential edges. Thus, the method is consistent even in the high-dimensional case when the differential graph is sparse.

Simulation Results

Detailed simulation settings and more simulation results are given in the paper.



EEG Data Application

We use FuDGE to analyze electroencephalogram (EEG) data obtained from an alcoholism study, which included 122 total subjects; 77 in an alcoholic group and 45 in the control group. The EEG data was measured by placing $p = 64$ electrodes on various locations on the subject's scalp and measuring voltage values across time. The estimated differential graph for the two groups is below.

